

Granger Mediation Analysis for Multiple Time Series

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**Analytics for
Big Complex Data**

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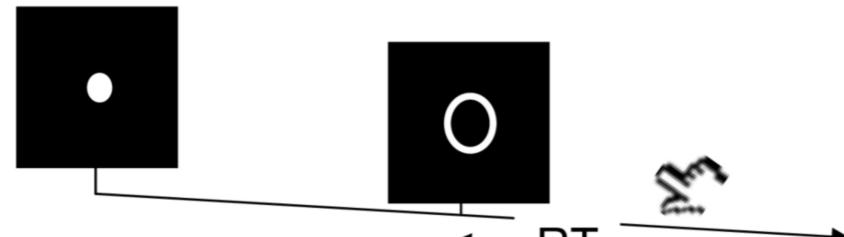
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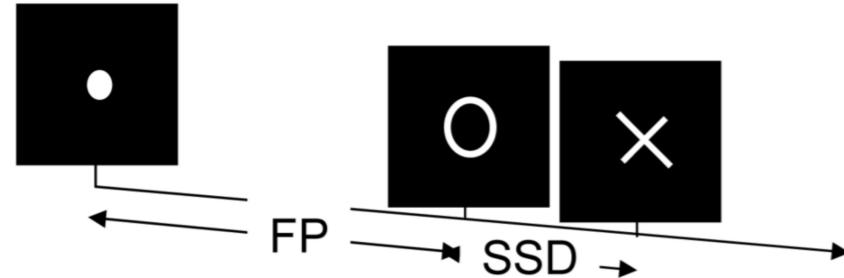
Slides viewable on web:
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fMRI Experiments

(a) GO trials: Success **G**; Error **F**



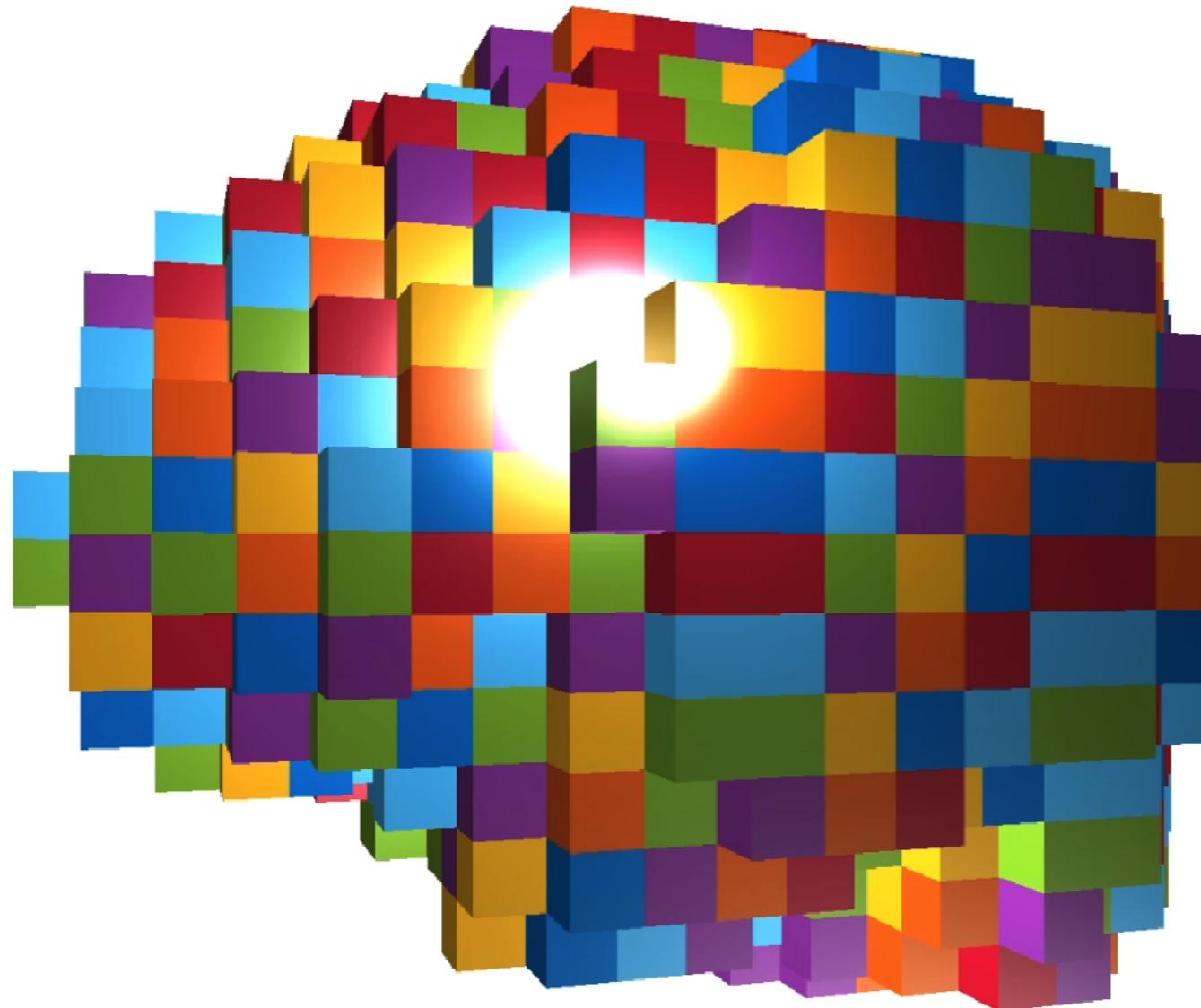
STOP trials: Success **SS**; Error **SE**



- Task fMRI: performs tasks under brain scanning
- **Randomized** stop/go task:
 - **press** button if "go";
 - **withhold** pressing if "stop"
- Not resting-state: "do nothing" during scanning

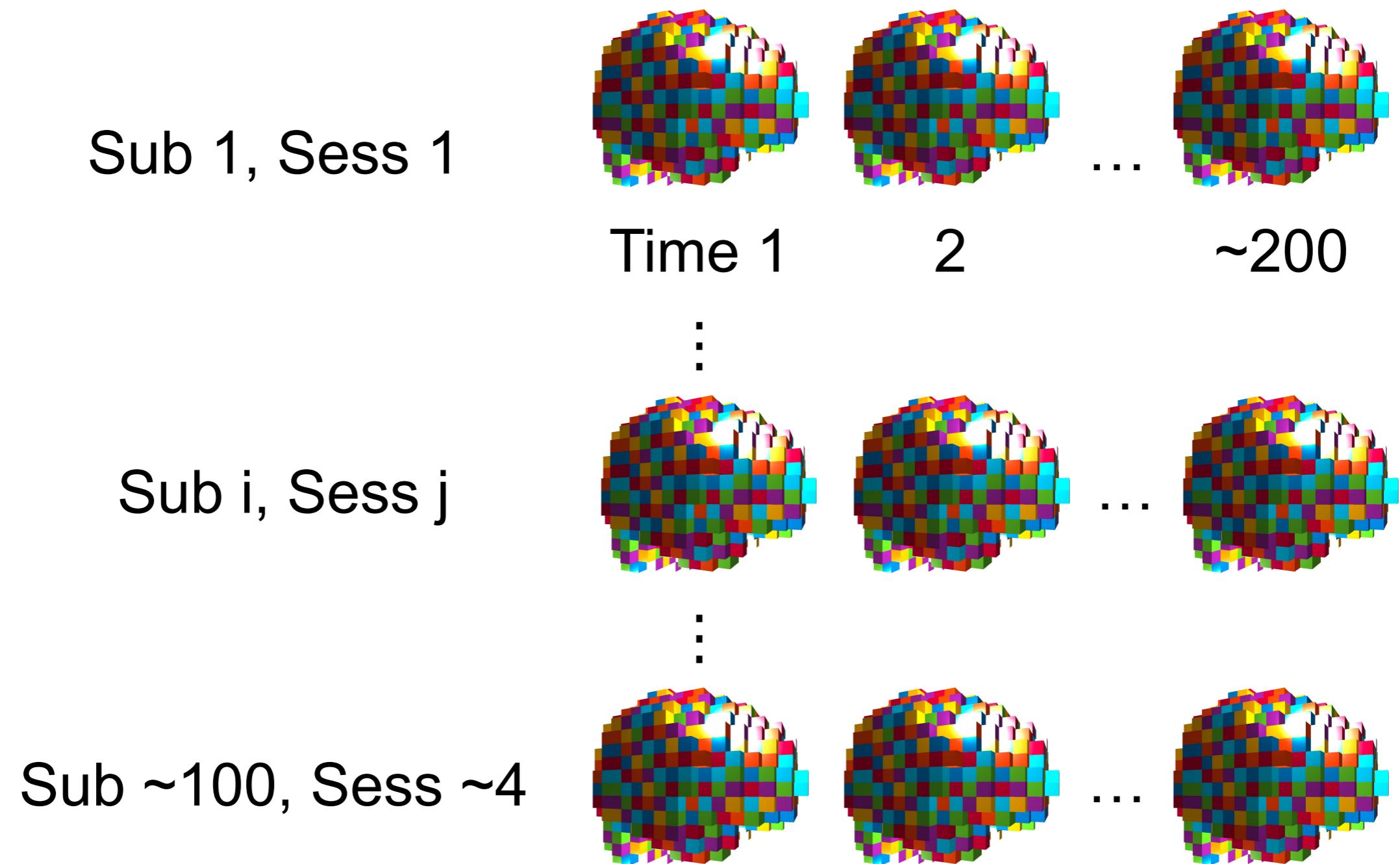
Goal: infer brain activation and connectivity





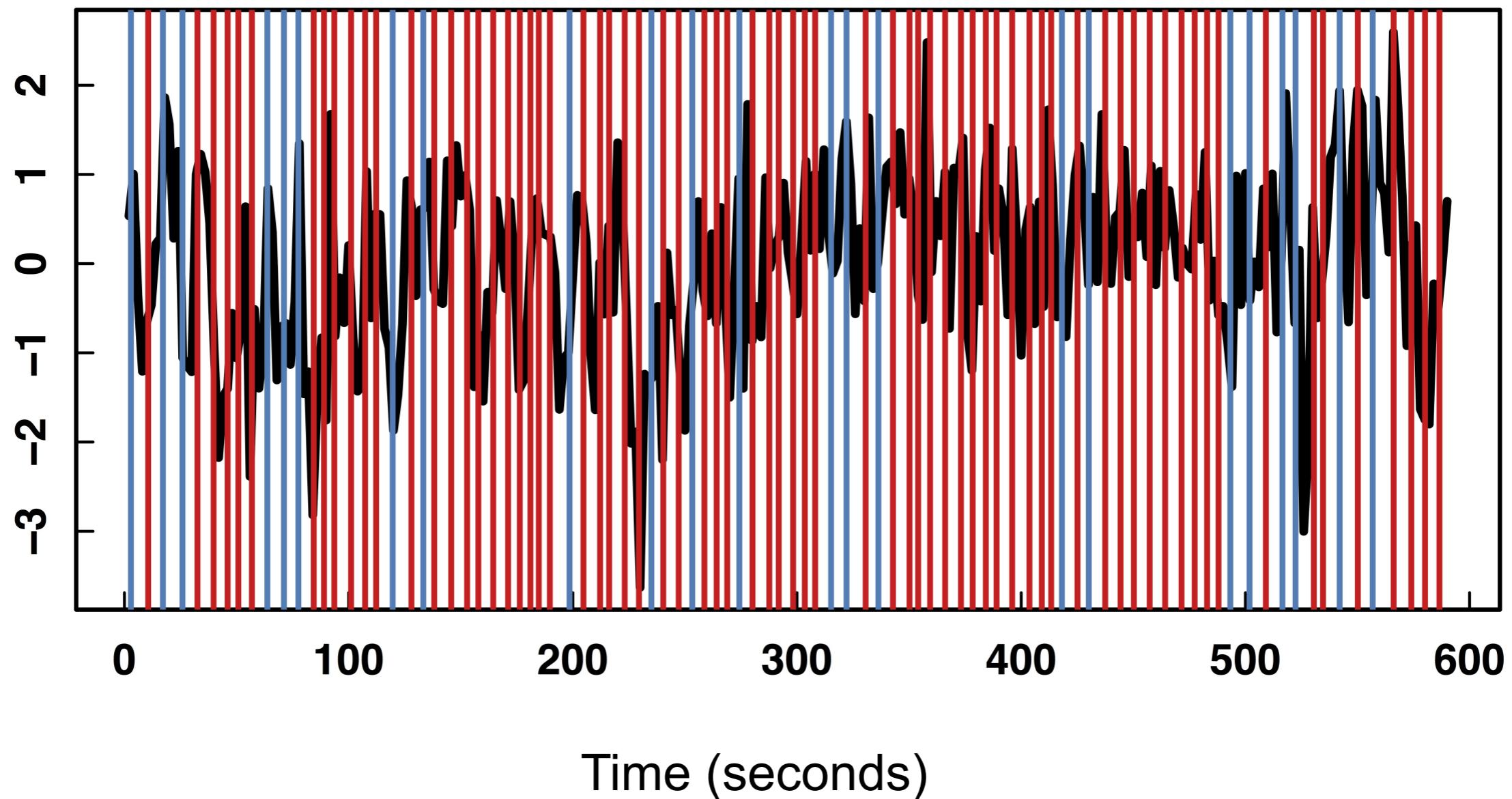
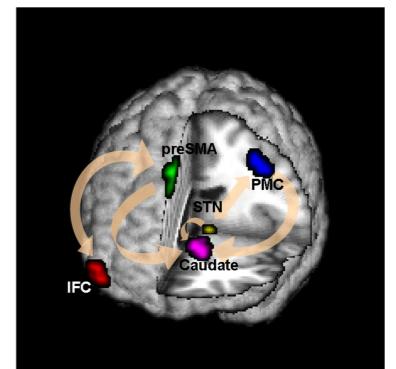
fMRI data: blood-oxygen-level dependent (BOLD) signals from
≡ each **cube**/voxel (~millimeters), $10^5 \sim 10^6$ voxels in total.

Multilevel fMRI Studies



Large, multilevel (subject, session, voxel) data
e.g. $1000 \times 4 \times 300 \times 10^6 \approx 1 \text{ trillion data points}$

Raw Data: Motor Region

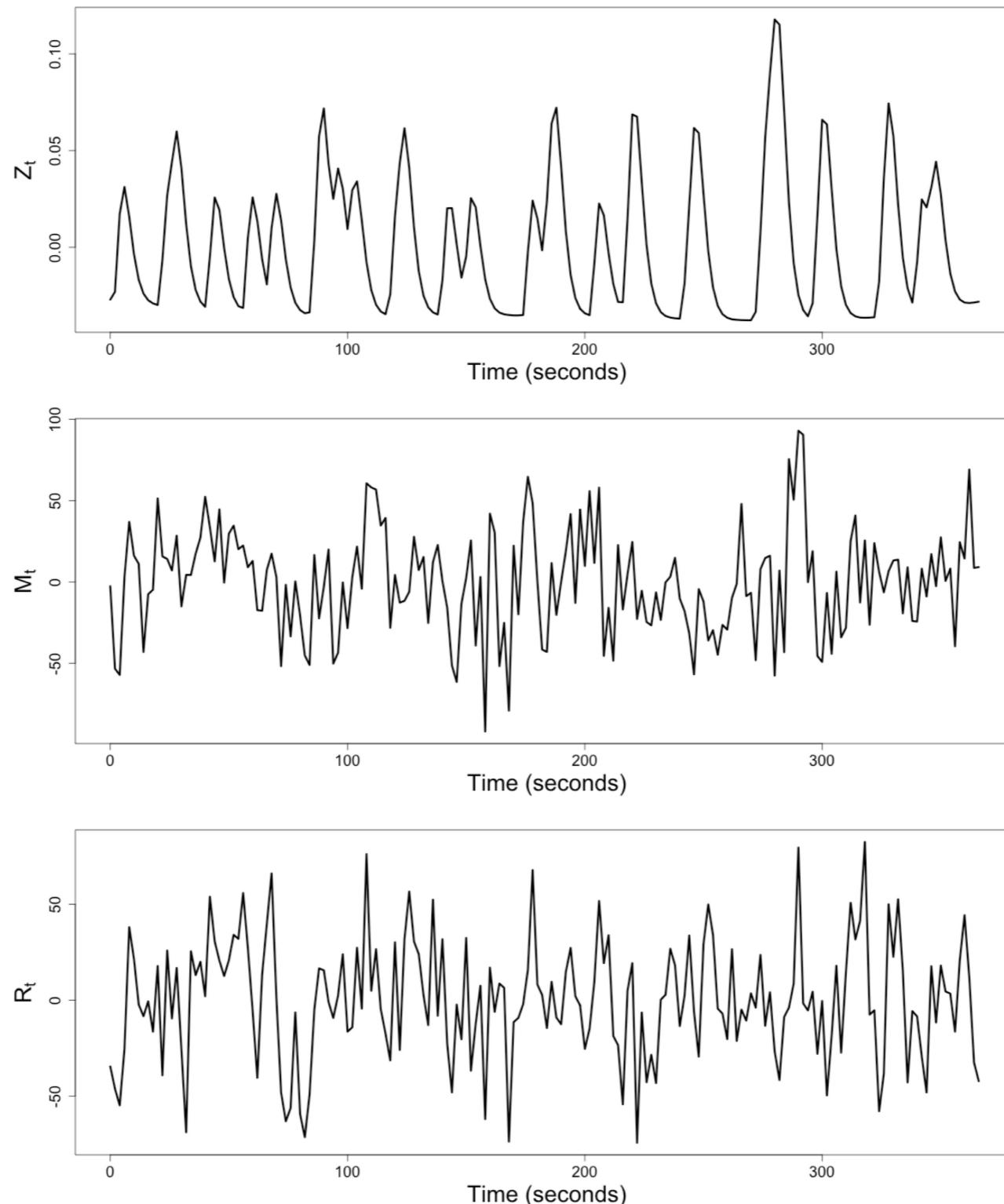


Time (seconds)

Black: fMRI BOLD activity

Blue: stop onset times; **Red:** go onset times





Z_t : Stimulus onsets convoluted with Canonical HRF

M_t, R_t : fMRI time series from two brain regions

Review: Granger Causality/VAR

- Given two (or more) time series x_t and y_t

$$x_t = \sum_{j=1}^p \psi_{1j} x_{t-j} + \sum_{j=1}^p \phi_{1j} y_{t-j} + \epsilon_{1t}$$

$$y_t = \sum_{j=1}^p \psi_{2j} y_{t-j} + \sum_{j=1}^p \phi_{2j} x_{t-j} + \epsilon_{2t}$$

- Also called vector autoregressive models
- y Granger causes x if $\phi_{1j} \neq 0$ [Granger, 69]
- Models **pair-wise** connections not **pathways**





Articles

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... Such data are generated by a wide range of **neuroimaging** and neurophysiological methods ... This paper introduced the operationalization of **Granger causality** in the form of linear vector autoregressive models ... Dynamic **causal** modeling of evoked responses in EEG and MEG ...

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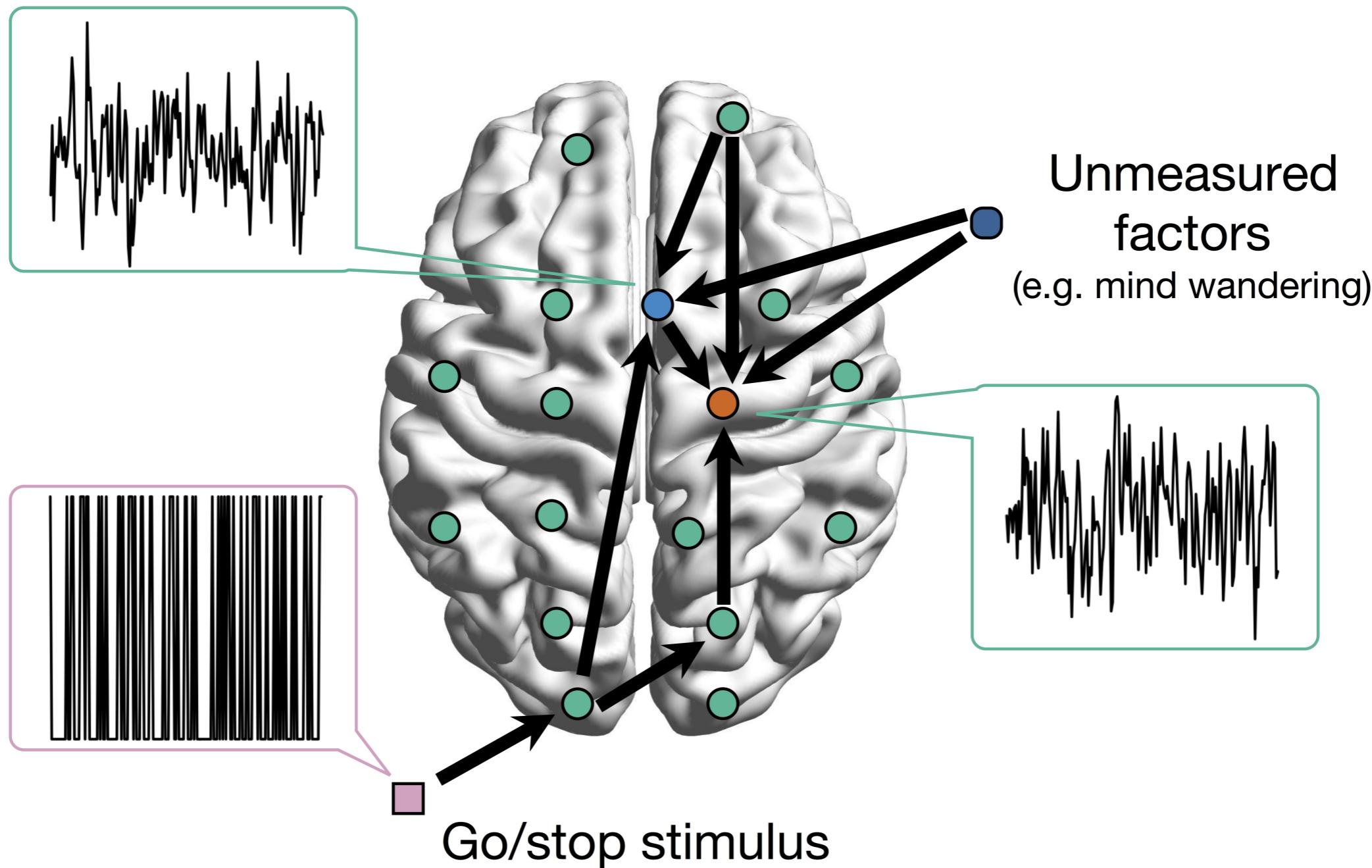


Granger Causality/VAR

- Granger Causality (VAR) popular for fMRI
 - About **8000** google scholar results on "granger causality neuroimaging"
- Models multiple **stationary** time series
- AR(p) (small p) fits fMRI well [Lingdquist, 08]
- **Not** for **non-stationary**/task fMRI
- **Cannot** model stimulus effects

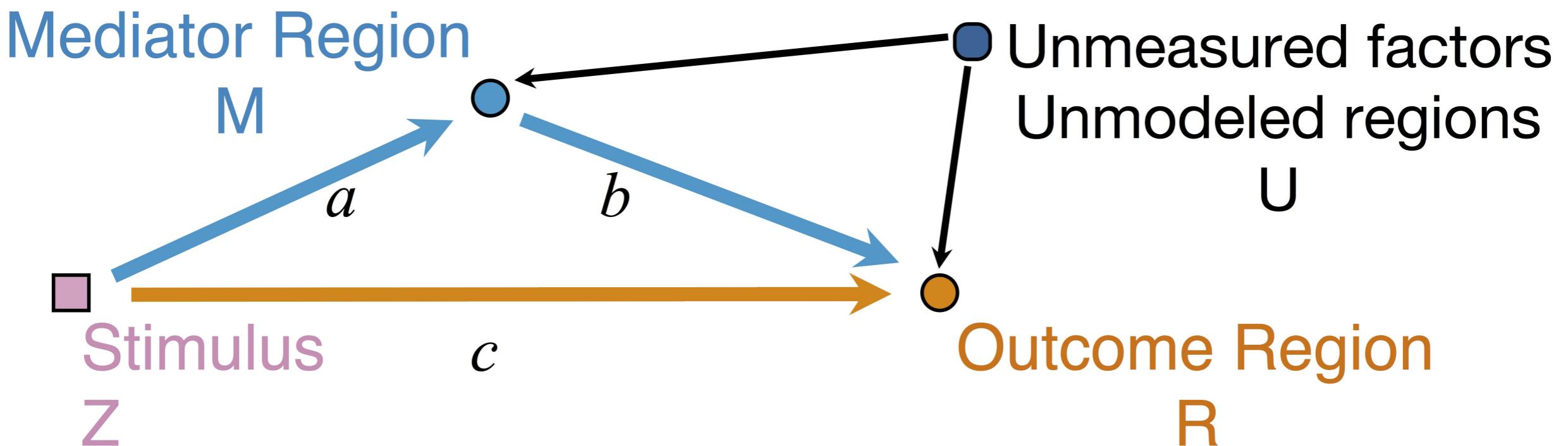


Conceptual Model with Stimulus



Goal: quantify effects **stimuli** → **preSMA** → **PMC regions**

Model: Mediation Analysis and SEM



$$M = Za + \underbrace{U}_{E_1} + \epsilon_1$$
$$R = Zc + Mb + \underbrace{Ug + \epsilon_2}_{E_2}, \quad \epsilon_1 \perp \epsilon_2$$

- **Indirect** effect: $a \times b$; **Direct** effect: c
- Correlated errors: $\delta = \text{cor}(E_1, E_2) \neq 0$ if $U \neq 0$

Mediation Analysis in fMRI

- Mediation analysis (usually assuming $U = 0$)

[Baron&Kenny, 86; Sobel, 82; Holland 88; Preacher&Hayes 08; Imai et al, 10; VanderWeele, 15;...]

- Parametric [Wager et al, 09] and functional [Lindquist, 12] mediation, under (approx.) independent errors
 - Stimulus → brain → **user reported ratings**, one brain mediator
 - Assuming $U = 0$ between ratings and brain
- Multiple mediator and multiple pathways
 - Dimension reduction by arXiv1511.09354 [Chen, Crainiceanu, Ogburn, Caffo, Wager, Lindquist, 15]
 - Pathway Lasso penalization [Zhao, Luo, 16]
- **This talk:** integrating Granger causality and mediation analysis



Model & Method



Our Mediation Model

$$M_t = Z_t a + E_{1t}, \quad R_t = Z_t c + M_t b + E_{2t}$$

- **Temporal** VAR errors

$$E_{1t} = \sum_{j=1}^p (\omega_{11_j} E_{1,t-j} + \omega_{21_j} E_{2,t-j}) + \epsilon_{1t}$$

$$E_{2t} = \sum_{j=1}^p (\omega_{12_j} E_{1,t-j} + \omega_{22_j} E_{2,t-j}) + \epsilon_{2t}$$

- **Spatial** errors: $\epsilon_{1t}, \epsilon_{2t}$

$$\begin{pmatrix} \epsilon_{1t} \\ \epsilon_{2t} \end{pmatrix} \sim \mathcal{N}(0, \Sigma), \quad \Sigma = \begin{pmatrix} \sigma_1^2 & \delta\sigma_1\sigma_2 \\ \delta\sigma_1\sigma_2 & \sigma_2^2 \end{pmatrix}$$



Equivalent Form

$$M_t = Z_t A + \sum_{j=1}^p (\phi_{1j} Z_{t-j} + \psi_{11j} M_{t-j} + \psi_{21j} R_{t-j}) + \epsilon_{1t}$$

$$R_t = Z_t C + M_t B + \sum_{j=1}^p (\phi_{2j} Z_{t-j} + \psi_{12j} M_{t-j} + \psi_{22j} R_{t-j}) + \epsilon_{2t}$$

- Nonzero ϕ 's and ψ 's denote the temporal influence from stimulus to mediator/outcome and etc
- A, B, C are causal following a similar proof in

[Sobel, Lindquist, 04]



Estimation: Conditional Likelihood

- The full likelihood for our model is too complex
- Given the initial p time points, the conditional likelihood is

$$\begin{aligned}\ell(\boldsymbol{\Theta}, \delta | \mathbf{Z}, \mathcal{I}_p) &= \sum_{t=p+1}^T \log f((M_t, R_t) | \mathbf{X}_t) \\ &= -\frac{T-p}{2} \log \sigma_1^2 \sigma_2^2 (1 - \delta^2) - \frac{1}{2\sigma_1^2} \|\mathbf{M} - \mathbf{X}\boldsymbol{\theta}_1\|_2^2 \\ &\quad - \frac{1}{2\sigma_2^2(1 - \delta^2)} \|(\mathbf{R} - \mathbf{MB} - \mathbf{X}\boldsymbol{\theta}_2) - \kappa(\mathbf{M} - \mathbf{X}\boldsymbol{\theta}_1)\|_2^2\end{aligned}$$



Multilevel Data: Two-level Likelihood

- Second level model, for each subject i

$$(A_i, B_i, C_i) = (A, B, C) + (\eta_i^A, \eta_i^B, \eta_i^C)$$

where errors η are normally distributed

- The two level likelihood is conditional convex
- Two-stage fitting: plug-in estimates from the first level
- Block coordinate fitting: jointly optimize first level likelihood + second level likelihood



Theorem: Assume assumptions (A1)-(A6) are satisfied.

Assume $E(Z_{i_t}^2) = q < \infty$, for $i = 1, \dots, N$. Let

$$T = \min_i T_i.$$

1. If Λ is known, then the two-stage estimator $\hat{\delta}$ maximizes the profile likelihood of model asymptotically, and $\hat{\delta}$ is \sqrt{NT} -consistent.
2. If Λ is unknown, then the profile likelihood of model has a unique maximizer $\hat{\delta}$ asymptotically, and $\hat{\delta}$ is \sqrt{NT} -consistent, provided that $1/\varpi = \bar{\kappa}^2/\varrho^2 = O_p(1/\sqrt{NT})$, $\kappa_i = \sigma_{i_2}/\sigma_{i_1}$, $\bar{\kappa} = (1/N) \sum \kappa_i$, and $\varrho^2 = (1/N) \sum (\kappa_i - \bar{\kappa})^2$.

Using the two-stage estimator $\hat{\delta}$, the CMLE of our model is consistent, as well as the estimator for $\mathbf{b} = (A, B, C)$.

Theory: Summary

- Under regularity conditions, N subs, T time points
- Our $\hat{\delta}$ is \sqrt{NT} -consistent
 - This relaxes the unmeasured confounding assumption in mediation analysis
- Our $(\hat{A}, \hat{B}, \hat{C})$ is also consistent



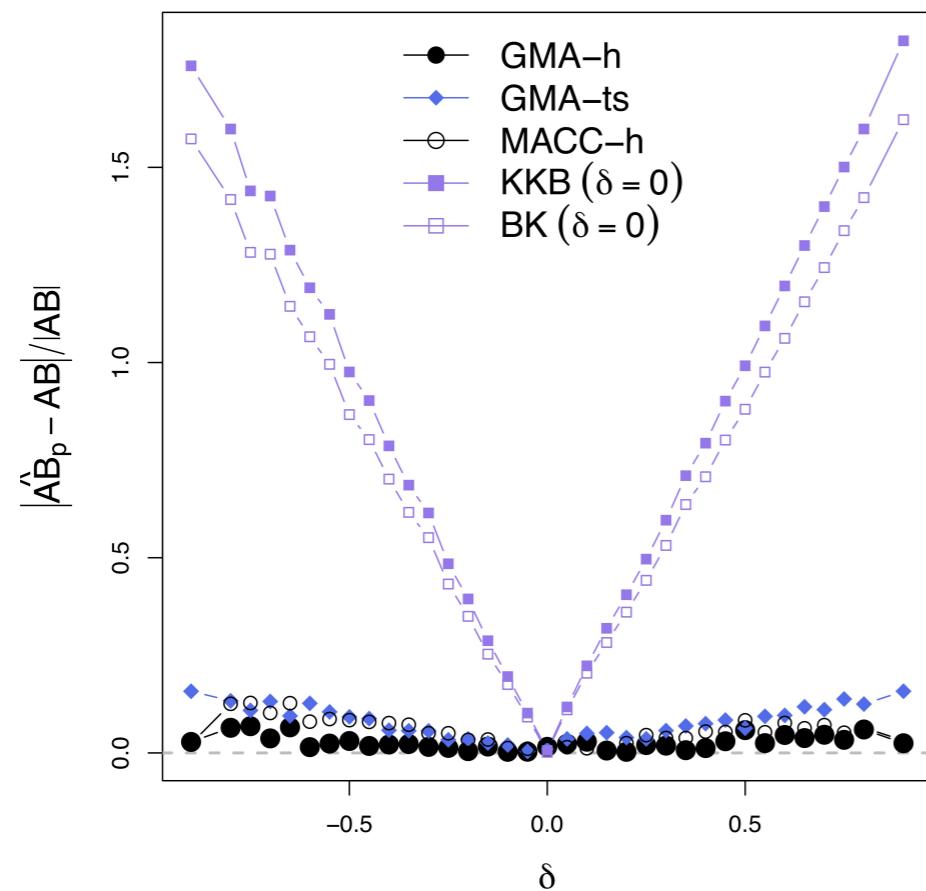
Simulations & Real Data

Comparison

- Our methods: **GMA-h** and **GMA-ts**
- Previous methods: BK [Baron & Kenny], MACC [Zhao and Luo], KKB [Kenny et al]
- Other methods do not model the temporal correlations or time series like ours

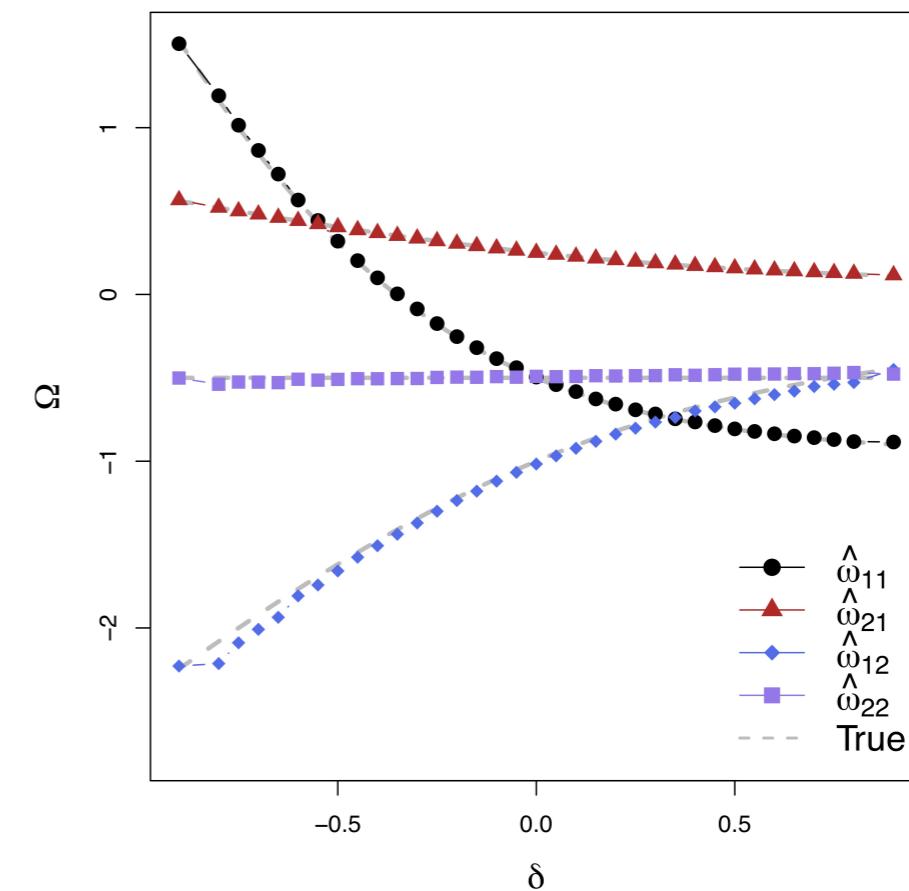


Simulations



Low bias for AB

Gray dash lines are the truth



Low bias for temporal cor

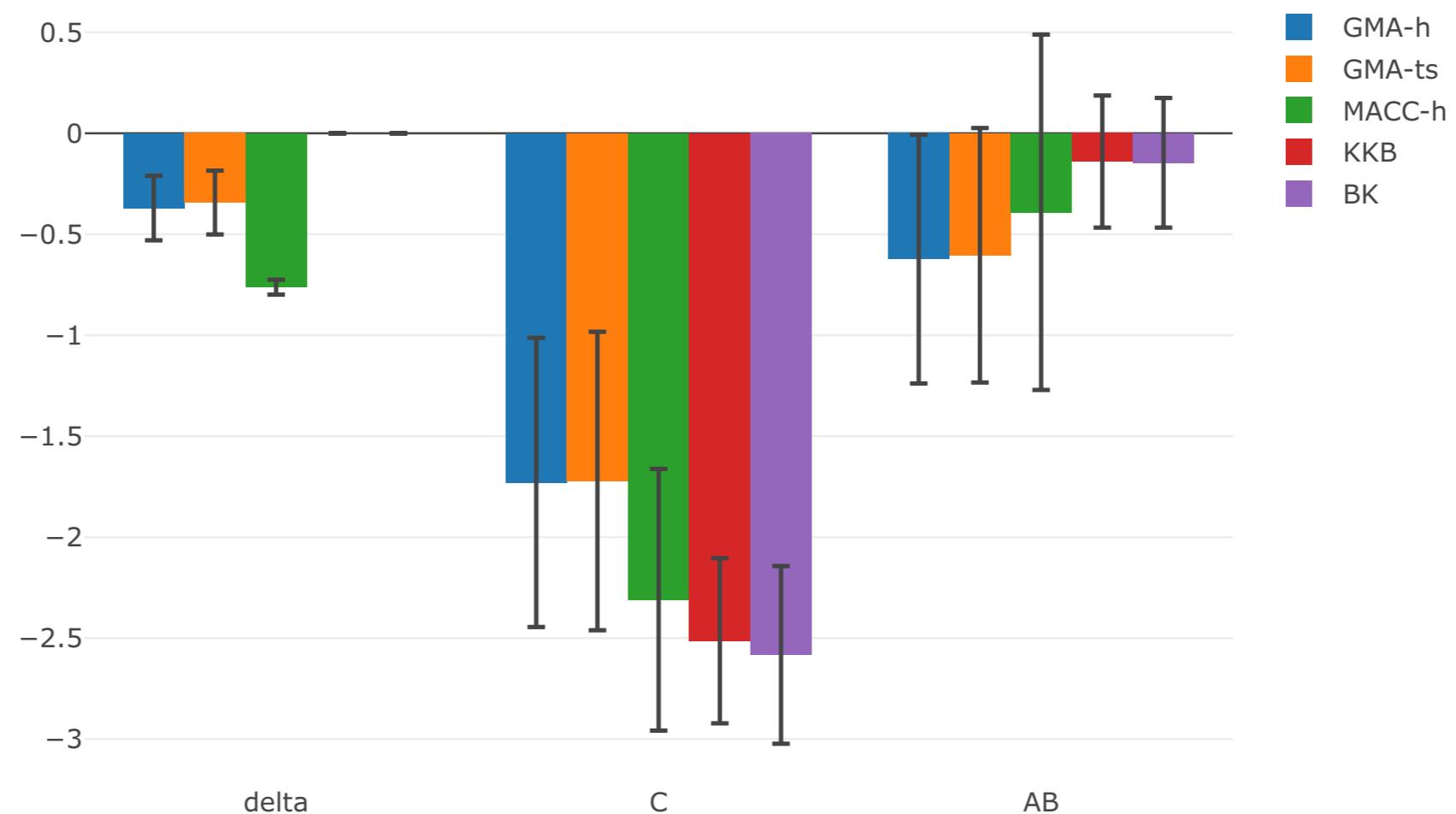
GMA performs the best, and recovers the temporal correlations

Real Data Experiment

- Public data: OpenFMRI ds30
- Stop-go experiment: withhold (STOP) from pressing buttons
- Expect "STOP" stimuli to deactivate brain region M1
- Goal: quantify the role of region preSMA



Result



Result

Method	δ	C	A	B	AB_p
GMA-h	-0.370 (-0.530, -0.156)	-1.729 (-2.445, -0.964)	-0.739 (-1.487, 0.035)	0.838 (0.644, 0.999)	-0.623 (-1.239, 0.033)
GMA-ts	-0.343 (-0.501, -0.163)	-1.722 (-2.461, -0.904)	-0.740 (-1.442, 0.080)	0.810 (0.656, 0.965)	-0.604 (-1.234, 0.055)
MACC-h	-0.762 (-0.799, -0.721)	-2.310 (-2.958, -1.641)	-0.259 (-0.810, 0.303)	1.511 (1.410, 1.619)	-0.391 (-1.271, 0.465)
KKB	-	-2.513 (-2.922, -2.073)	-0.225 (-0.772, 0.326)	0.617 (0.589, 0.647)	-0.140 (-0.467, 0.196)
BK	-	-2.583 (-3.023, -2.142)	-0.235 (-0.774, 0.352)	0.616 (0.588, 0.647)	-0.146 (-0.467, 0.211)

- STOP deactivates M1 directly (C) and indirectly (AB)
- preSMA mediates a good portion of the total effect
 - Help resolve the debates among neuroscientists
- Other methods under-estiamte the effects
- Novel feedback findings: M1 → preSMA after lag 1 and 2 (not shown)



Discussion

- Mediation analysis for multiple time series
- Method: Granger causality + mediation
 - Optimizing complex likelihood
- Theory: identifiability, consistency
- Result: low bias and improved accuracy
- Extension: functional mediation (Zhao, Function 37)
- CRAN pkg: **gma** and references within



Thank you!

Comments? Questions?

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