

# A Data Mining Approach for Determining Gait Abnormalities in Runners with Patellofemoral Pain Syndrome

**Ross Brancati, MS**

PhD Candidate

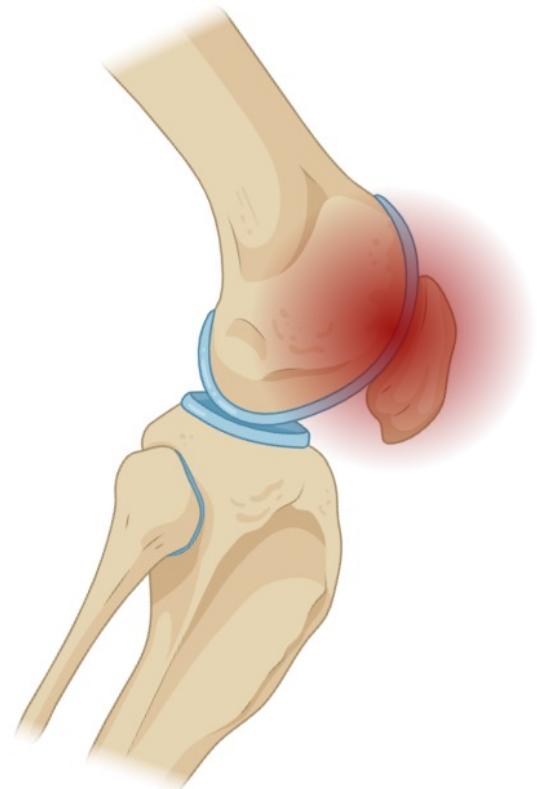
Musculoskeletal & Orthopedic Biomechanics Lab

November 28, 2022

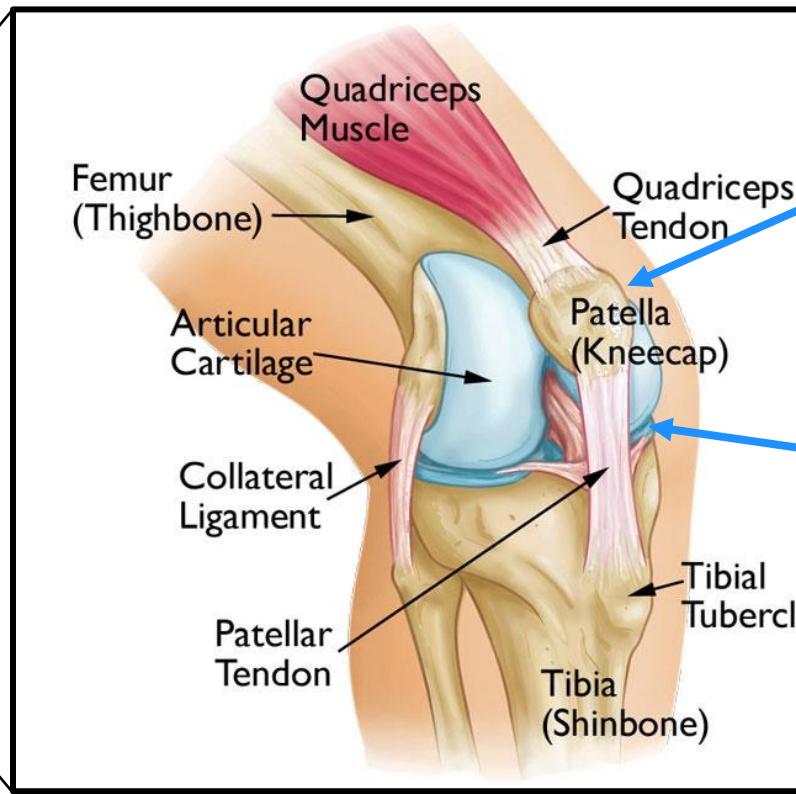
Seminar Presentation

# Patellofemoral Pain Syndrome

- Patellofemoral pain (PFP) is a common musculoskeletal pain disorder, often presenting as anterior knee pain
- Experienced by many recreational runners
- High prevalence (25%) and recurrence (up to 90%)
- Prolonged runs typically aggravate the pain
- Pathomechanical model highlights distal and proximal pathways to elevated patellofemoral joint stress



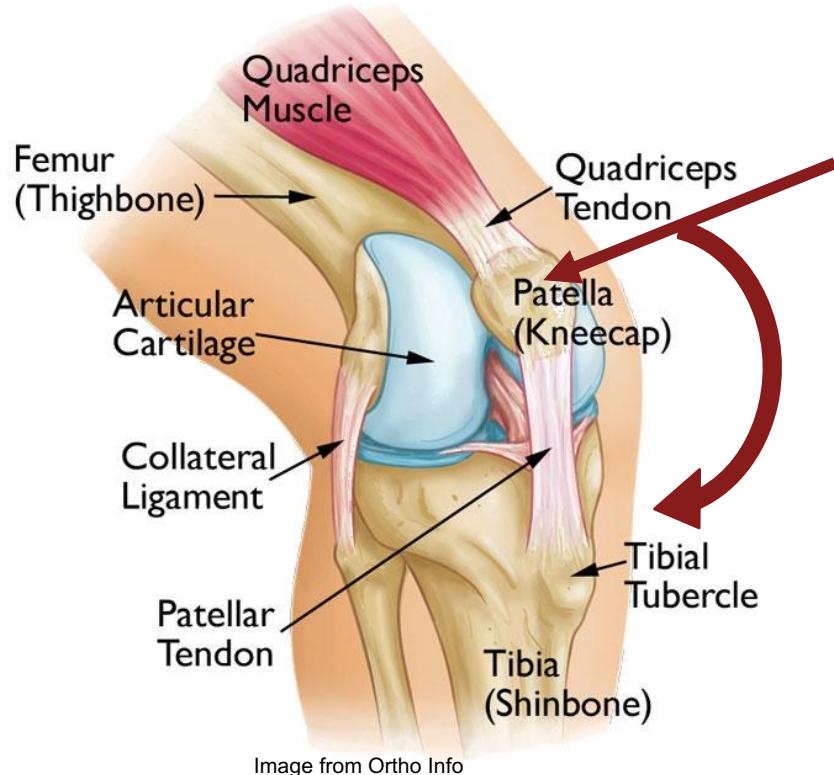
# Quick Anatomy Review



Patellofemoral Joint

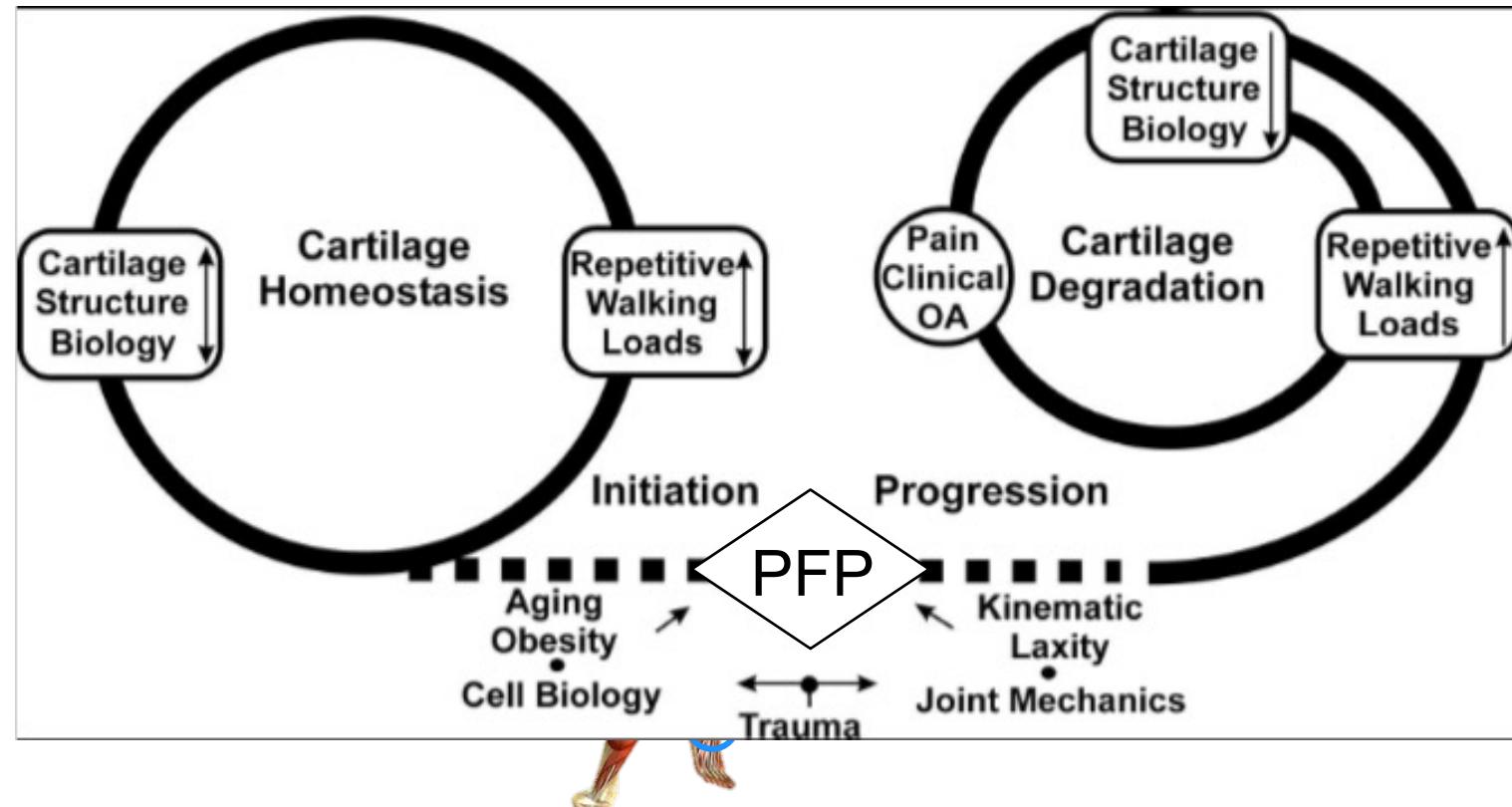
Tibiofemoral Joint

# Proposed Pain Mechanisms

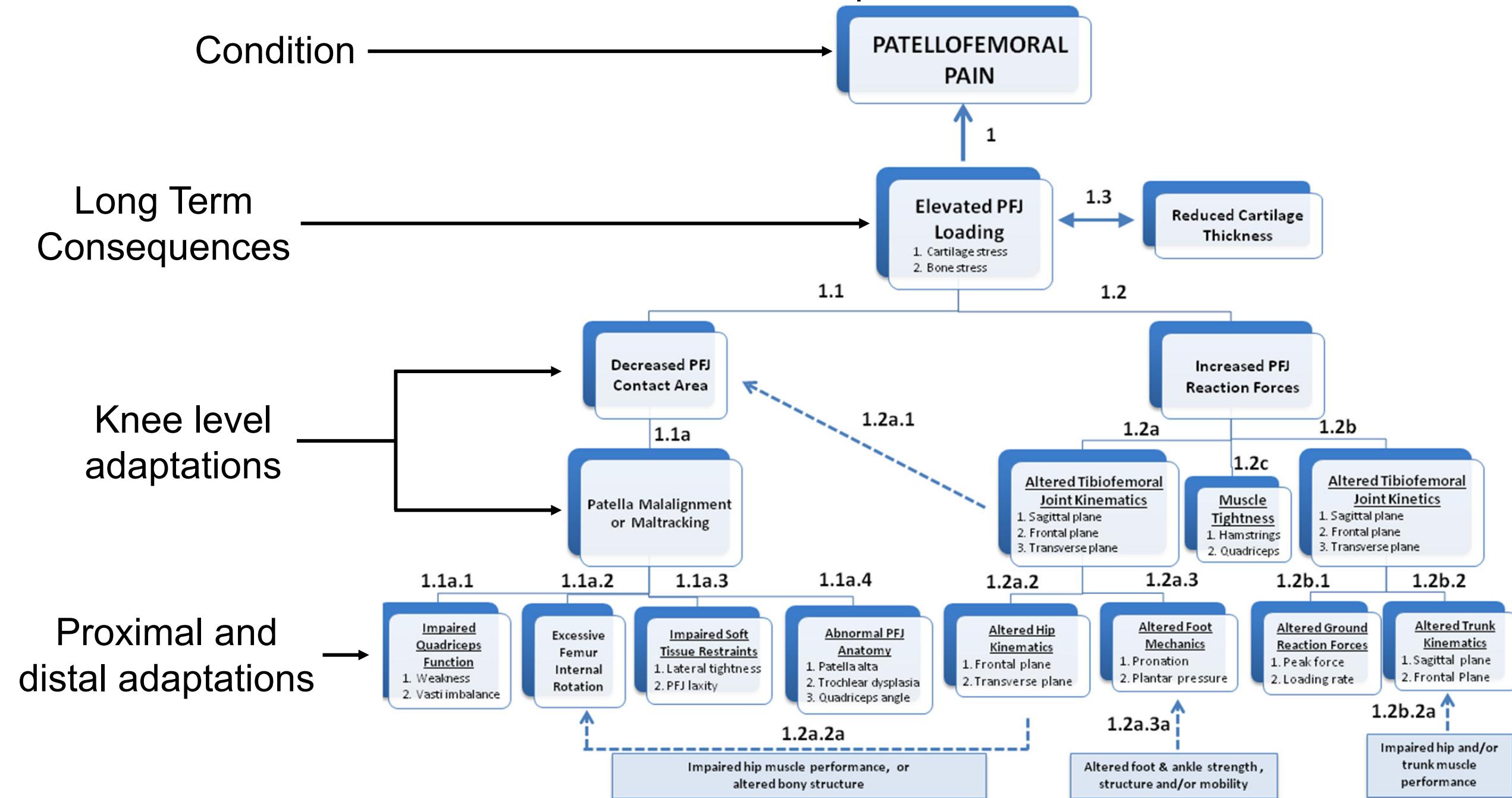


Elevated patellofemoral joint stress

Adaptations to patellofemoral cartilage

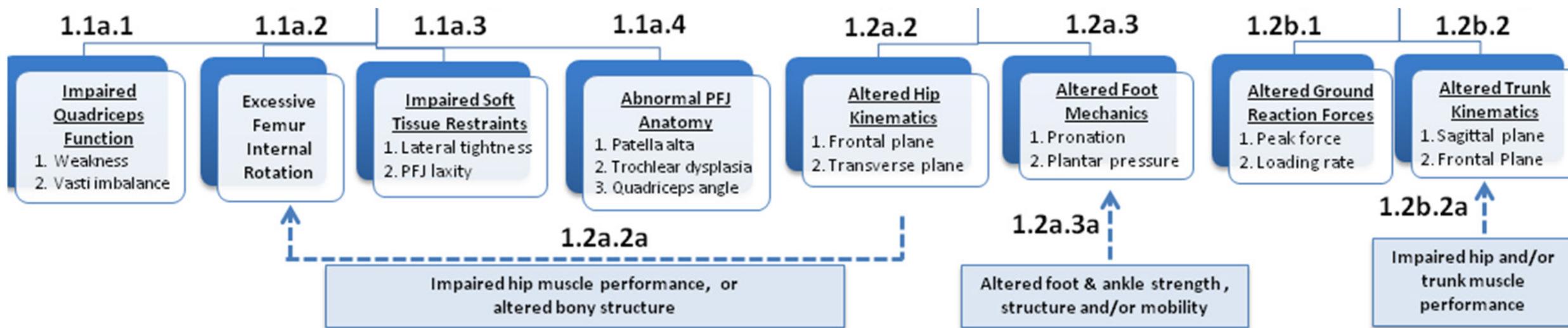


Willy et al. 2019, Powers et al. 2017, Andriacchi et al. 2009

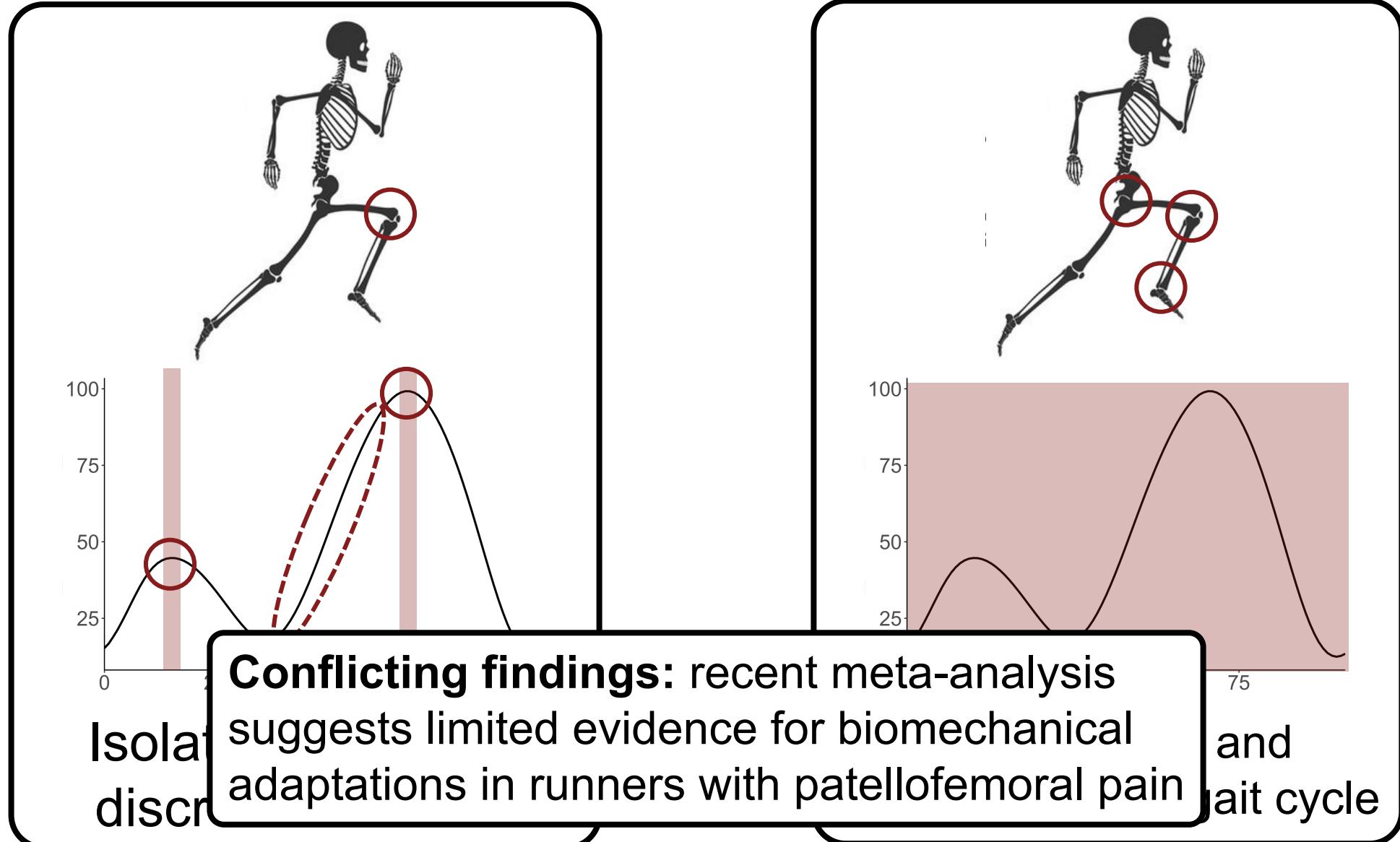


# Prior Work

- Many findings are conflicting due to heterogeneity of PFP
- Runners with PFP displayed:
  - Lower peak knee flexion angles
  - Lower peak knee extension moment
  - Prolonged soleus activation



# Prior Work



Review

## Machine learning in human movement biomechanics: Best practices, common pitfalls, and new opportunities

Eni Halilaj <sup>a,\*</sup>, Apoorva Rajagopal <sup>b</sup>, Madalina Fiterau <sup>c</sup>, Jennifer L. Hicks <sup>d</sup>, Trevor J. Hastie <sup>e,f</sup>, Scott L. Delp <sup>b,d,g</sup>

<sup>a</sup> Department of Mechanical Engineering, Carnegie Mellon University, United States

<sup>b</sup> Department of Mechanical Engineering, Stanford University, United States

<sup>c</sup> Department of Computer Science, Stanford University, United States

<sup>d</sup> Department of Bioengineering, Stanford University, United States

<sup>e</sup> Department of Statistics, Stanford University, United States

<sup>f</sup> Department of Health Research and Policy, Stanford University, United States

<sup>g</sup> Department of Orthopaedic Surgery, Stanford University, United States



Ina Fiterau Brostean



UMass InFusion Lab

## Data Mining: discover new patterns in data

## Feature Engineering: creating new features from existing ones to reduce dimensionality

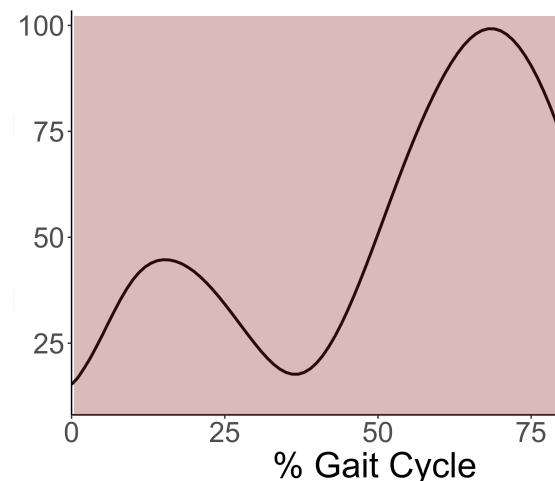
## Principal component analysis and machine learning models are becoming more popular in biomechanics research

# Our Approach

Teasing out the particularly important biomechanical adaptations instead of selecting them apriori could greatly improve our understanding of PFP

## Principal Component Analysis

finds important differences  
across the entire wave



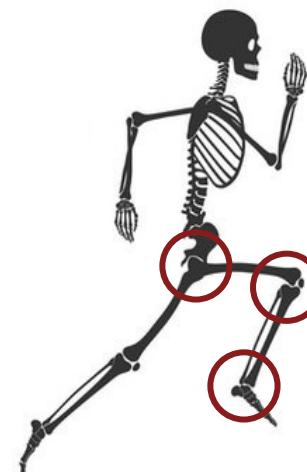
## Machine Learning Modeling

finds important differences  
across all variables

This “data mining” approach  
finds patterns that differentiate  
runners with and without PFP



Image from StichData



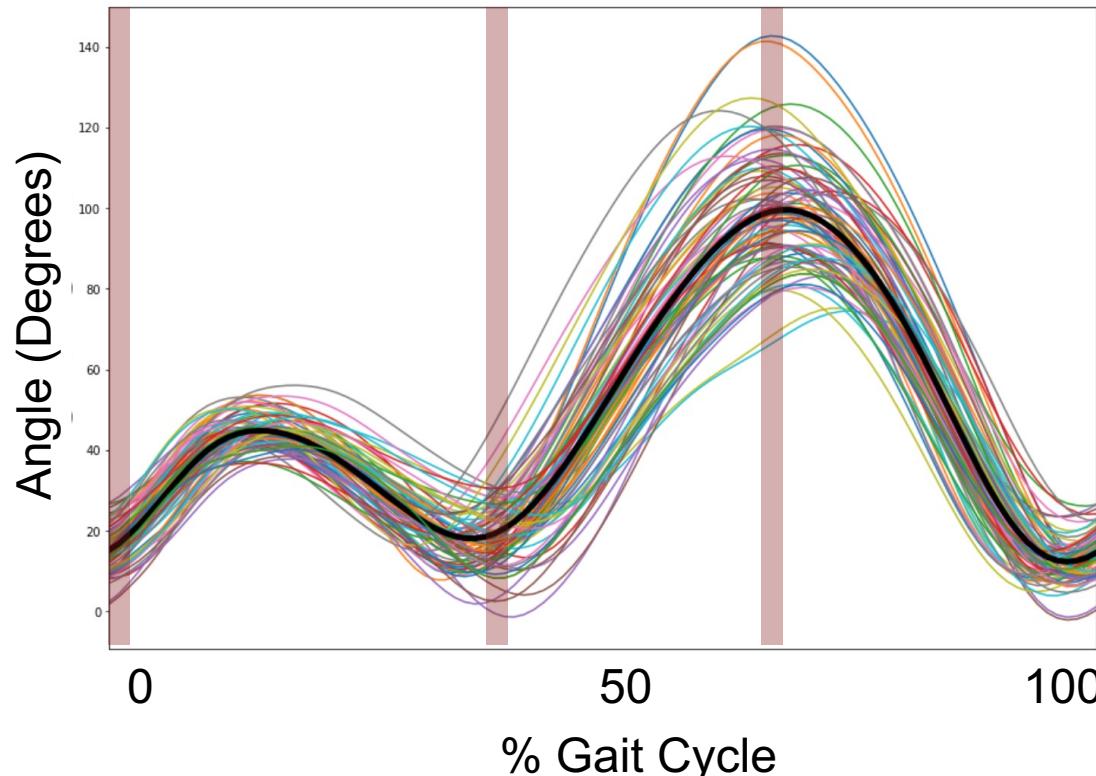
# Study Aims

**Aim 1:** Determine important biomechanical features that differentiate symptomatic for PFP and healthy runners at baseline

**Aim 2:** Determine important biomechanical features that differentiate symptomatic for PFP and healthy runners following a treadmill run that induces knee pain

**Aim 3:** Explore if runners recovered from pain still exhibit altered biomechanics by classifying them as either symptomatic for PFP or healthy

# Principal Component Analysis (PCA)



100 timepoints  
of the gait cycle

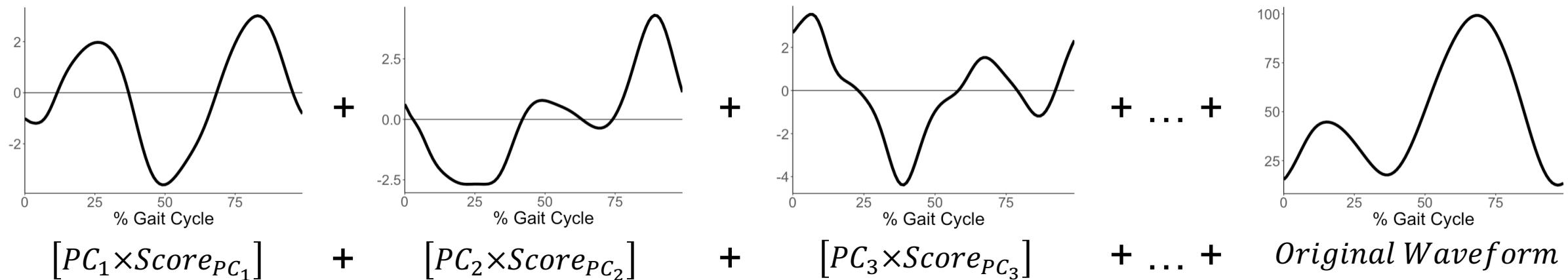


A few principal components  
explaining most of the  
variance in the data

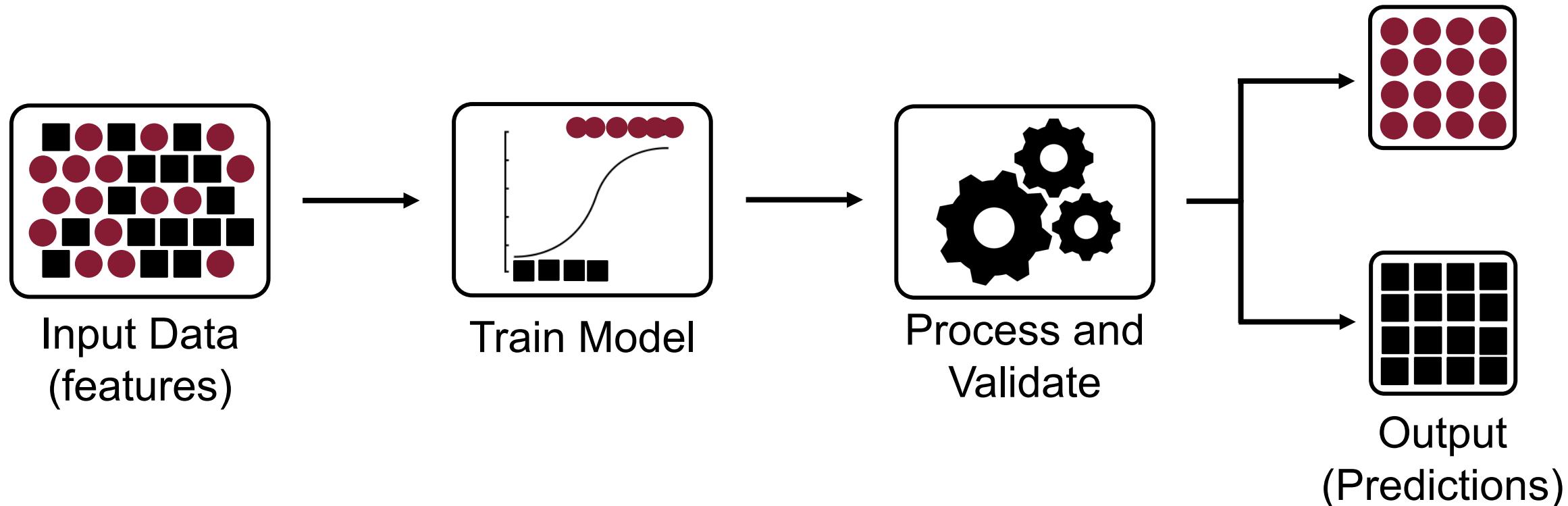
- PCA generates principal components (PCs) and scores for each observation associated with the respective PC

# Principal Component Analysis (PCA)

$$\text{Original Waveform} = \sum_{i=1}^n [PC_n \times Score_{PC_n}]$$



# Supervised Machine Learning Classification



● Healthy Runners  
■ Symptomatic Runners



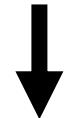
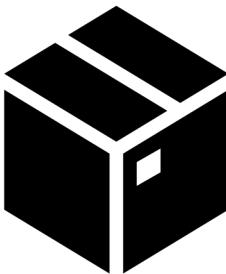
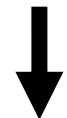
## Features that Differentiate Groups

- Kinetics
- Kinematics
- Muscle Activation Patterns (EMG)

# Interpretable Machine Learning Models

## Black Box Approaches

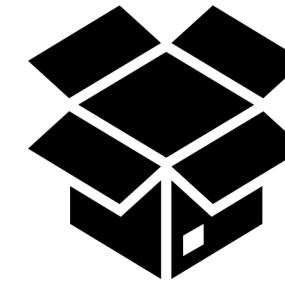
Inputs (features)



Outputs (predictions)

## Interpretable ML Approaches

Inputs



Outputs

- Informativeness
- Transferability
- Explainability
- Feature Importance

# Methods – Data Collection

41 recreational runners

- 15 healthy (H)
- 14 symptomatic PFP (S)
- 12 recovered from PFP (R)



Runners completed a 21-minute treadmill run at self-selected speed



- M1 ————— 21-minute treadmill run ————— M21 -



Kinetic, kinematic, electromyography (EMG), RPE, and subjective pain scores collected at 1<sup>st</sup> (M1) and 21<sup>st</sup> (M21) minutes

Variable	Healthy	Symptomatic	Recovered
Pain Level Change (M1 > M21)	0.06	3.00	0.33
RPE Change (M1 > M21)	4.80	3.64	2.79

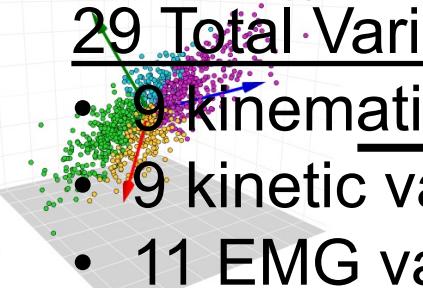
# Methods – Data Processing

## 1. Generate variable matrices

Subject ID	Group	t1	t2	...	t101
Subject 1 M1	H	Datapoint	Datapoint	...	Datapoint
Subject 1 M21	H	Datapoint	Datapoint	...	Datapoint
Subject 2 M1	S	Datapoint	Datapoint	...	Datapoint
...	...	Datapoint	Datapoint	...	Datapoint
Subject 29 M21	S	Datapoint	Datapoint	...	Datapoint

## 2. Principal Component Analysis

29 Total Variables

- 9 kinematic variables
  - 9 kinetic variables
  - 11 EMG variables
- 
- Generates Principal Component (PC) Scores

## 3. Logistic regression model: classify healthy and symptomatic runners

**Limitation:** nearly 100 principal components from all kinetic, kinematic, and EMG variables

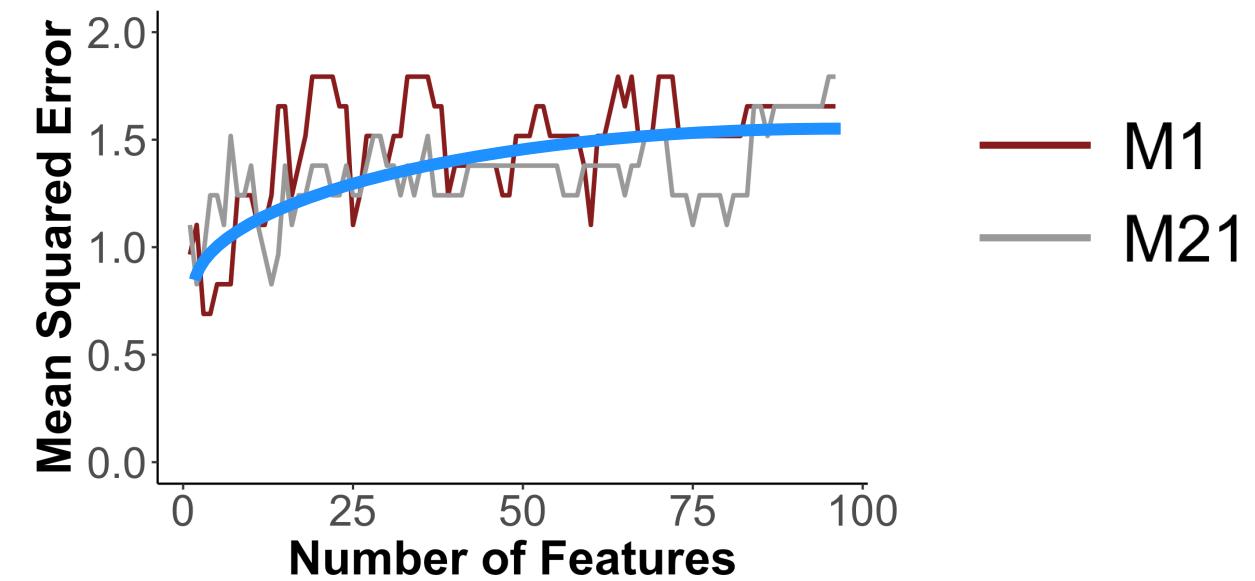
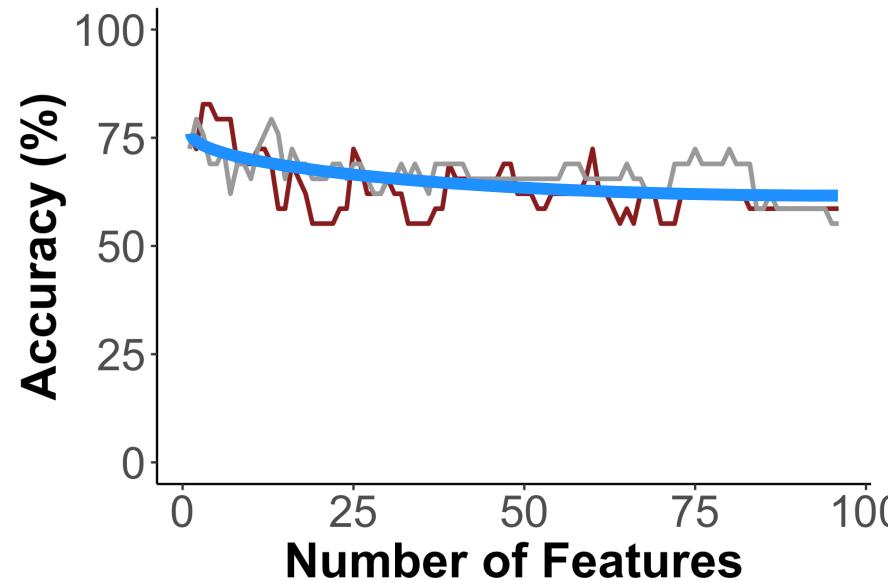
**Solution:** machine learning  
needed to determine the most important principal components

Extract Feature Coefficients

# Methods – Machine Learning Modeling

- Generated two models:
  1. Minute 1 Model (M1)
  2. Minute 21 Model (M21)
- Quasi-Forward Stepwise Feature Selection Algorithm:
  1. Select  $k$  best features
  2. Cross validate model
  3. Calculate model accuracy
  4. Repeat steps 1-3 for  $k = k + 1$  features derived from PCA
    - ~100 iterations for ~100 principal components
  5. Select the model with the highest classification accuracy

# Results – Machine Learning Modeling

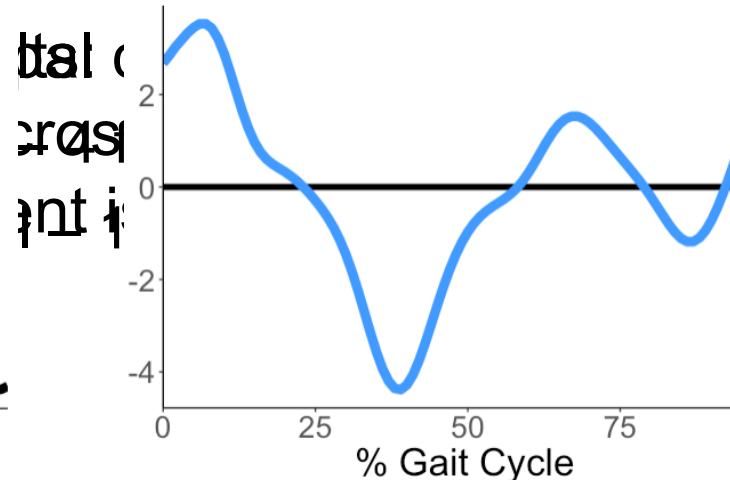
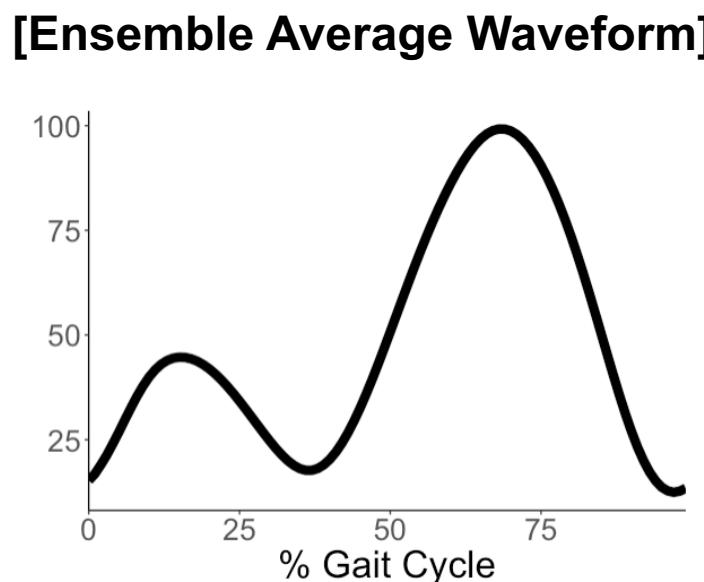
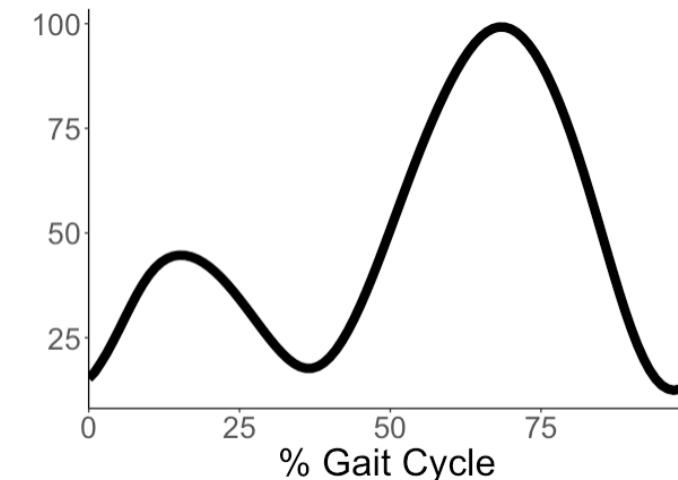


# Results

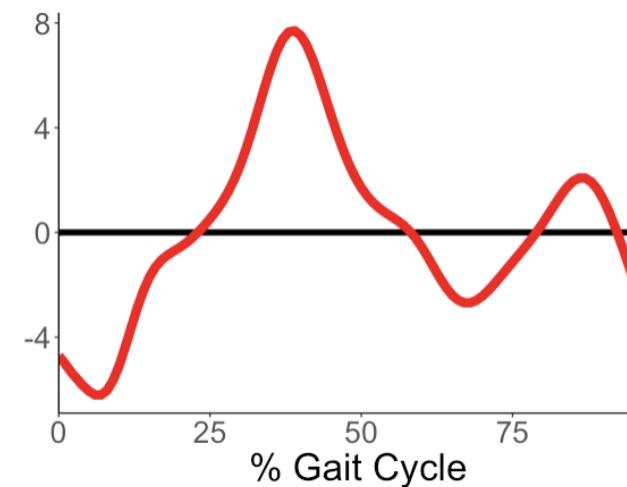
Variable	LR Coefficient	Explained Variance	Healthy Group Score	Symptomatic Group Score	p-value
<b>Minute 1 Model</b>					
Knee Flexion Angle PC3	3.617	8	-0.197 (0.564)	0.346 (0.48)	0.010*
Hip Adduction Moment PC3	1.301	13	-1.119 (2.554)	1.455 (2.988)	0.018*
Gluteus Maximus Activation PC2	0.929	33	1.578 (3.483)	-1.896 (4.415)	0.026*
Hip Adduction Moment PC1	0.801	49	3.731 (4.849)	-2.322 (5.298)	0.003*
<b>Minute 21 Model</b>					
Knee Flexion Moment PC2	2.341	14	-0.211 (0.333)	0.619 (1.831)	0.096
Hip Adduction Moment PC3	1.608	13	-0.66 (2.8)	1.784 (2.7)	0.024*
Knee Flexion Angle PC3	1.515	8	-0.241 (0.448)	0.385 (0.568)	0.003*
Knee Adduction Moment PC3	1.479	13	-0.619 (1.593)	1.32 (3.148)	0.044*
Biceps Femoris Activation PC1	1.452	37	0.934 (4.038)	-1.739 (4.206)	0.092
Ankle Flexion Angle PC3	1.342	13	-0.746 (0.961)	0.023 (1.262)	0.075
Soleus Activation PC2	1.272	23	-1.179 (1.856)	0.777 (3.344)	0.060
Ankle Abduction Moment PC1	0.934	52	-0.936 (2.802)	1.903 (4.285)	0.043*
Ankle Flexion Moment PC2	0.803	7	0.269 (0.604)	-0.186 (0.504)	0.037*
Hip Adduction Moment PC1	0.79	49	2.181 (5.434)	-1.785 (5.728)	0.066
Knee Rotation Angle PC4	0.705	8	0.872 (1.478)	-0.29 (1.299)	0.033*
Hip Rotation Angle PC4	0.604	6	0.977 (2.286)	-1.086 (1.516)	0.008*
Ankle Flexion Angle PC2	0.554	24	0.625 (1.441)	-0.358 (1.473)	0.080

Mean (standard deviation), \*p<0.05

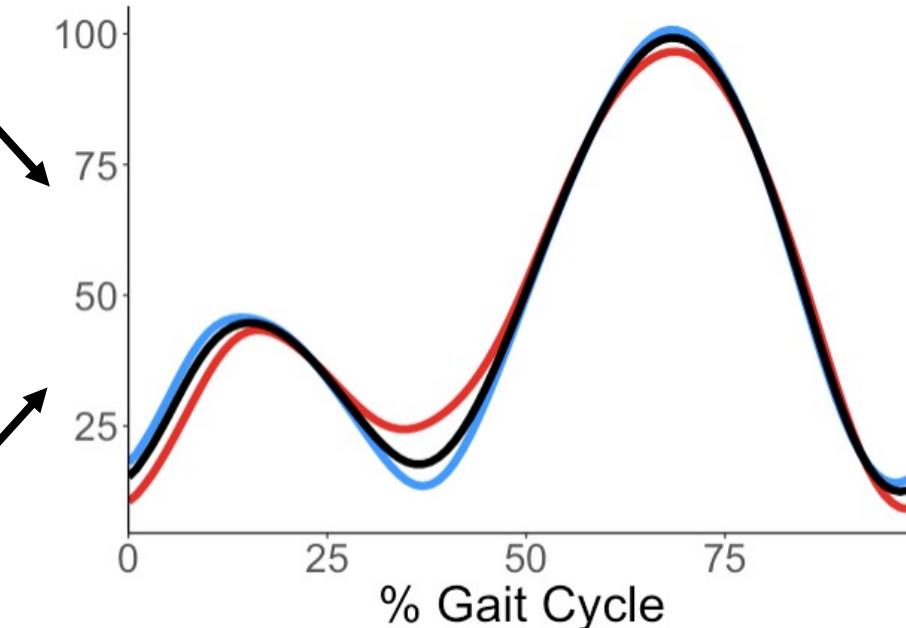
# Interpreting Principal Components



**[Group PC Score \* PC \* Scaling Factor]**



deviation from the mean at  
so we know what variance that



— Healthy Group — Symptomatic Group — Ensemble Average

# Results – Minute 1 Model (Aim 1)

Accuracy: 82.76% 20  
MSE: 0.670

Variable	Knee Flexion Angle PC3	Hip Adduction Moment PC1 + PC3	Gluteus Maximus Activation PC2
Principal Component Plot			
Interpretation of symptomatic group	<ul style="list-style-type: none"> <li>Larger magnitude of knee flexion angle at toe off.</li> </ul>	<ul style="list-style-type: none"> <li>Larger magnitude of hip abduction moment in mid-stance.</li> <li>Larger magnitude of hip adduction moment in late stance.</li> </ul>	<ul style="list-style-type: none"> <li>Lower pre- and mid-stance phase activation.</li> <li>Greater activation at heel strike and in late stance.</li> </ul>

# Discussion – Minute 1 Model (Aim 1)

- Symptomatic runners avoiding full range of knee flexion during stance
  - Smaller patellofemoral contact area?
  - Pain avoidance strategy?
- Altered frontal plane loading patterns at the hip joint
  - Proximal strategy
- Abnormal gluteus maximus activation patterns in pre-activation and stance phases
  - Potential alterations to patellofemoral joint kinematics

# Results – Minute 21 Model (Aim 2)

Accuracy: 79.31%

22

MSE: 0.828

Variable	LR Coefficient	Explained Variance
Knee Extension Moment PC2	2.341	14
Hip Adduction Moment PC3	1.608	13
Knee Flexion Angle PC3	1.515	8
Knee Adduction Moment PC3	1.479	13
Biceps Femoris Activation PC1	1.452	37
Ankle Flexion Angle PC3	1.342	13
Soleus Activation PC2	1.272	23
Ankle Abduction Moment PC1	0.934	52
Ankle Flexion Moment PC2	0.803	7
Hip Adduction Moment PC1	0.79	49
Knee Rotation Angle PC4	0.705	8
Hip Rotation Angle PC4	0.604	6
Ankle Flexion Angle PC2	0.554	24

Same features at M1  
model

# Results – Minute 21 Model (Aim 2)

Accuracy: 79.31%

23

MSE: 0.828

Variable	LR Coefficient	Explained Variance
Knee Extension Moment PC2	2.341	14
Hip Adduction Moment PC3	1.608	13
Knee Flexion Angle PC3	1.515	8
Knee Adduction Moment PC3	1.479	13
Biceps Femoris Activation PC1	1.452	37
Ankle Flexion Angle PC3	1.342	13
Soleus Activation PC2	1.272	23
Ankle Abduction Moment PC1	0.934	52
Ankle Flexion Moment PC2	0.803	7
Hip Adduction Moment PC1	0.79	49
Knee Rotation Angle PC4	0.705	8
Hip Rotation Angle PC4	0.604	6
Ankle Flexion Angle PC2	0.554	24

Ankle based strategy

# Results – Minute 21 Model (Aim 2)

Accuracy: 79.31%

24

MSE: 0.828

Variable	LR Coefficient	Explained Variance
Knee Extension Moment PC2	2.341	14
Hip Adduction Moment PC3	1.608	13
Knee Flexion Angle PC3	1.515	8
Knee Adduction Moment PC3	1.479	13
Biceps Femoris Activation PC1	1.452	37
Ankle Flexion Angle PC3	1.342	13
Soleus Activation PC2	1.272	23
Ankle Abduction Moment PC1	0.934	52
Ankle Flexion Moment PC2	0.803	7
Hip Adduction Moment PC1	0.79	49
Knee Rotation Angle PC4	0.705	8
Hip Rotation Angle PC4	0.604	6
Ankle Flexion Angle PC2	0.554	24

Frontal and transverse  
plane adaptations

# Discussion – Minute 21 Model (Aim 2)

- Same knee flexion and hip abduction patterns as minute 1
  - Key strategies regardless of pain status
- Abnormal hip rotation angles, knee extension moments, and knee rotation angles
  - Related to biceps femoris activation patterns
- Ankle-based strategy for maintaining running velocity
  - Potential strategy for mitigating pain

# Results – Recovered Runners (Aim 3)

**Aim 3:** Classify runners previously recovered from PFP as either symptomatic for PFP or healthy

Model Timepoint	# Healthy Classification	# Symptomatic Classification
Minute 1 Model	7	5
Minute 21 Model	5	7

- Recovered runners who experienced any pain classified as:
  - Symptomatic at both timepoints
  - Shifted from healthy at M1 to symptomatic at M21

# Summary & Conclusions

- Important adaptations with the onset of pain in runners at both the distal and proximal joints
- Ankle based strategy for maintaining velocity after 21 minutes of treadmill running
- Recovered runners respond heterogeneously
  - Onset of pain important for classification procedure

# Acknowledgements

## MOBL Group (and others):

- Dr. Katherine Boyer
- Erica Casto
- Skylar Holmes
- Aidan Gross
- Athulya Simon
- Ryan Gladfelter
- Andrew Bourguignon
- Kali Shamaly
- Kiichi Ash
- Carl Jewell
- Bill Johnson



Bailey

DE LUCA  
— FOUNDATION —

Funding from the De Luca Foundation

# References

- Crossley, K. M., Stefanik, J. J., Selfe, J., Collins, N. J., Davis, I. S., Powers, C. M., McConnell, J., Vicenzino, B., Bazett-Jones, D. M., Esculier, J.-F., Morrissey, D., & Callaghan, M. J. (2016). 2016 Patellofemoral pain consensus statement from the 4th International Patellofemoral Pain Research Retreat, Manchester. Part 1: Terminology, definitions, clinical examination, natural history, patellofemoral osteoarthritis and patient-reported outcome measures. *British Journal of Sports Medicine*, 50(14), 839–843. <https://doi.org/10.1136/bjsports-2016-096384>
- BAZETT-JONES, D. M., COBB, S. C., HUDDLESTON, W. E., O'CONNOR, K. M., ARMSTRONG, B. S. R., & EARL-BOEHM, J. E. (2013). Effect of Patellofemoral Pain on Strength and Mechanics after an Exhaustive Run. *Medicine & Science in Sports & Exercise*, 45(7), 1331–1339. <https://doi.org/10.1249/MSS.0b013e3182880019>
- Willy, R. W., Hoglund, L. T., Barton, C. J., Bolgia, L. A., Scalzitti, D. A., Logerstedt, D. S., Lynch, A. D., Snyder-Mackler, L., & McDonough, C. M. (2019). Patellofemoral pain clinical practice guidelines linked to the international classification of functioning, disability and health from the academy of orthopaedic physical therapy of the American physical therapy association. *Journal of Orthopaedic and Sports Physical Therapy*, 49(9), CPG1–CPG95. <https://doi.org/10.2519/jospt.2019.0302>
- Taunton, J. E., Ryan, M. B., Clement, D. B., McKenzie, D. C., Lloyd-Smith, D. R., & Zumbo, B. D. (2002). A retrospective case-control analysis of 2002 running injuries. *British Journal of Sports Medicine*, 36(2), 95–101. <https://doi.org/10.1136/bjsm.36.2.95>
- Powers, C. M., Witvrouw, E., Davis, I. S., & Crossley, K. M. (2017). Evidence-based framework for a pathomechanical model of patellofemoral pain: 2017 patellofemoral pain consensus statement from the 4th International Patellofemoral Pain Research Retreat, Manchester, UK: Part 3. *British Journal of Sports Medicine*, 51(24), 1713–1723. <https://doi.org/10.1136/bjsports-2017-098717>
- Andriacchi, T. P., Koo, S., & Scanlan, S. F. (2009). Gait Mechanics Influence Healthy Cartilage Morphology and Osteoarthritis of the Knee. *Journal of Bone and Joint Surgery*, 91(Supplement\_1), 95–101. <https://doi.org/10.2106/JBJS.H.01408>
- Bazett-Jones, D. M., Neal, B. S., Legg, C., Hart, H. F., Collins, N. J., & Barton, C. J. (2022). Kinematic and Kinetic Gait Characteristics in People with Patellofemoral Pain: A Systematic Review and Meta-analysis. *Sports Medicine*. <https://doi.org/10.1007/s40279-022-01781-1>
- Barton, C. J., Levinger, P., Crossley, K. M., Webster, K. E., & Menz, H. B. (2012). The relationship between rearfoot, tibial and hip kinematics in individuals with patellofemoral pain syndrome. *Clinical Biomechanics*, 27(7), 702–705. <https://doi.org/10.1016/j.clinbiomech.2012.02.007>
- Dierks, T. A., Manal, K. T., Hamill, J., & Davis, I. (2011). Lower extremity kinematics in runners with patellofemoral pain during a prolonged run. *Medicine and Science in Sports and Exercise*, 43(4), 693–700. <https://doi.org/10.1249/MSS.0b013e3181f744f5>
- Esculier, J. F., Roy, J. S., & Bouyer, L. J. (2015). Lower limb control and strength in runners with and without patellofemoral pain syndrome. *Gait and Posture*, 41(3), 813–819. <https://doi.org/10.1016/j.gaitpost.2015.02.020>
- Willson, J. D., Kerozek, T. W., Arndt, R. L., Reznicek, D. A., & Scott Straker, J. (2011). Gluteal muscle activation during running in females with and without patellofemoral pain syndrome. *Clinical Biomechanics*, 26(7), 735–740. <https://doi.org/10.1016/j.clinbiomech.2011.02.012>
- Noehren, B., Sanchez, Z., Cunningham, T., & McKeon, P. O. (2012). The effect of pain on hip and knee kinematics during running in females with chronic patellofemoral pain. *Gait and Posture*, 36(3), 596–599. <https://doi.org/10.1016/j.gaitpost.2012.05.023>
- Molnar, C. (2019). Interpretable Machine Learning: A Guide for Making Black Box Models Explainable. *Leanpub Publishing*.
- Halilaj, E., Rajagopal, A., Fiterau, M., Hicks, J. L., Hastie, T. J., & Delp, S. L. (2018). Machine learning in human movement biomechanics: Best practices, common pitfalls, and new opportunities. In *Journal of Biomechanics* (Vol. 81, pp. 1–11). Elsevier Ltd. <https://doi.org/10.1016/j.jbiomech.2018.09.009>
- Deluzio, K. J., & Ast Stephen, J. L. (2007). Biomechanical features of gait waveform data associated with knee osteoarthritis. An application of principal component analysis. *Gait and Posture*, 25(1), 86–93. <https://doi.org/10.1016/j.gaitpost.2006.01.007>
- Andriacchi, T. P., Koo, S., & Scanlan, S. F. (2009). Gait Mechanics Influence Healthy Cartilage Morphology and Osteoarthritis of the Knee. *Journal of Bone and Joint Surgery*, 91(Supplement\_1), 95–101. <https://doi.org/10.2106/JBJS.H.01408>
- Cheng, C. (2022) Principal Component Analysis (PCA) Explained Visually with Zero Math. *Towards Data Science*. n.d. Accessed: 8/2/2022
- Slide 2 image credit: Adobe Stock. Accessed 8/2/2022 <https://stock.adobe.com/ee/search?k=human+skel>