

Stability analysis for a new model of multi-species convection-diffusion-reaction in poroelastic tissue

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Abstract

We perform the linear stability analysis of a new model for poromechanical processes with inertia (formulated in mixed form using the solid deformation, fluid pressure, and total pressure) interacting with diffusing and reacting solutes convected in the medium. We find parameter regions that lead to spatio-temporal instabilities of the coupled system. The mutual dependences between deformation and diffusive patterns are of substantial relevance in the study of morphoelastic changes in bio-materials. We provide a set of computational examples in 2D and 3D (related to brain mechanobiology) that can be used to form a better understanding on how, and up to which extent, the deformations of the porous structure dictate the generation and suppression of spatial patterning dynamics, also related to the onset of mechano-chemical waves.

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1. Introduction and problem statement

1.1. Scope and related work

We propose a new model for the interaction between diffusing species and an underlying poroelastic structure, focusing on detailing the physical aspects of the model, on deriving a spectral linear stability analysis, and on providing numerical examples dealing with growth and pattern formation, as well as with an application in traumatic brain injury. The permeability of soft tissue constituents, such as collagenous membranes, is typically in the orders of 10^{-14} to $10^{-12} \text{ [m}^2\text{N}^{-1}\text{s}^{-1}\text{]}$. If one considers membranes having a thickness of a few hundred microns, then fluid exchange occurs in the range of seconds and therefore this flow can affect physiological tissue deformations due to cardiac cycle or breathing [1]. This motivates the use of poroelasticity

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theory (confined to the regime of infinitesimal strains) in the characterisation of soft living tissues, and recent applications include the formation and development of brain oedema [2] and the poromechanical importance of pia matter [3].

Even if the present theoretical framework is motivated by a couple of examples in cell dynamics, other applications sharing a similar mathematical and mechano-chemical structure are numerous. We can cite, for instance, oxygen diffusivity in cartilage [4], drug delivery in arteries [5], tumour localisation and biomass growth [6], or chemically-controlled cell motion [7]. Two-way couplings are essential in this context. In some of the phenomena mentioned above, the consolidation of the porous media increases the flow of interstitial fluid which in turn contributes to the mechanically-induced transport of solutes [8]. Conversely, chemical solutes (in so-called active poroelastic materials) locally modify morphoelastic properties [9], and these processes occur on micro and macro-scales [10]. Therefore, in the general system we consider here, reaction-diffusion equations are coupled to the balances of mass and linear momentum of the fluid-solid mixture through convection (by the velocity of the poroelastic solid), as well as through a modification in the reaction, which is modulated by changes in volume. In turn, the solutes' concentration and the external forces drive the motion of the medium by means of contractile forces.

On the other hand, conducting a thorough stability analysis can contribute to reveal the essential physical mechanisms of these multiphysics systems with respect to selected parameter values. These tools are well-known and particularly useful in the context of patterning systems. However, the increasing complexity of current models implies that the spectral stability analysis is more and more analytically involved. In the context of the present work, related studies have been performed on particular sub-systems such as decoupled elasticity and diffusion [11]. More recent works tend to integrate further complexity by adding multi-layered coupled systems [12], incorporating domain or mechanical growth [13], the coupling between elasticity-diffusion [14], poroelasticity [15, 16], and also poroelasticity-diffusion [9], which resembles more the idea we advocate in this work.

The key contributions of this paper extend the work outlined above by including a new three-dimensional model for the two-way coupling between poroelasticity and reaction-diffusion, then deriving and discussing dispersion relations that indicate that the mechano-chemical feedback onsets Turing instabilities (with non-trivial wavenumber) for a range of coupling parameters. We also advance the formulation and numerical realisation of a locking-free finite element method, and a sample of numerical results including applications in brain injuries poromechanics. This work also generalises recent three-field models of poroelasticity using total pressure, and we demonstrate here the feasibility of the model and of the numerical method to reproduce a variety of coupling scenarios including pattern suppression, linear growth instability, and other morphological changes.

The remainder of this paper is laid out as follows. The governing equations proposed in [17] are recalled in what is left of this section. Then, in Section 2 we perform a linear stability analysis around a steady state with zero solid displacement, constant fluid pressure, and constant solute concentrations. To make the analysis as general as possible, we modify the momentum equilibrium that we present in our recent work [17] (which was oriented to the theoretical analysis of well-posedness of the coupled system), now including also an acceleration term. We use that to make some model comparisons. We proceed in Section 3 with recalling the mixed-primal finite element scheme from the companion paper [17]. Then we close with some illustrative numerical examples in 2D and 3D collected in Section 4.

1.2. Poroelasticity of soft tissue

Let us consider flow of interstitial fluid through a porous medium that is subject to elastic deformations. We will consider that the process occurs in either two- or three-dimensional domains $\Omega \subset \mathbb{R}^d$ with $d \in \{2, 3\}$, and that the fluid does not enter nor leaves the body. As common in the study of flow in porous media, we quantify the variation in fluid and solid states in terms of locally averaged variables. Then, for a given time $t \in (0, t_{\text{final}}]$, poromechanical quantities of interest are in this case the average displacement of the porous structure $\mathbf{u}^s(t) : \Omega \rightarrow \mathbb{R}^d$ and the pressure head associated with the fluid flowing through the pores,

$p^f(t) : \Omega \rightarrow \mathbb{R}$. We also suppose that gravitational forces have little effect in contributing to the momentum balances in comparison to inertia, or to other external body forces such as applied loads depending on space and time variables $\mathbf{b}(t) : \Omega \rightarrow \mathbb{R}^d$. In the classical theory of consolidation the system allows to describe physical loading of porous layers and the change of hydraulic equilibrium in a fluid-structure system. There, one assumes as well that the exerted stresses contain shear contributions by the solid phase whereas volumetric contributions appear from both solid and fluid phases (since the interstitial flow is considered governed by Darcy's law). This fact motivates the idea from [18, 19] to introduce an auxiliary scalar unknown

$$\psi = \alpha p^f - \lambda \operatorname{div} \mathbf{u}^s, \quad (1.1)$$

representing the total pressure, or the volumetric part of the total Cauchy stress $\boldsymbol{\sigma}$ (specified in the constitutive equation (1.3), below), where α is the so-called Biot-Willis consolidation (or pressure storage coupling) parameter.

Denoting by $\ell(t) : \Omega \rightarrow \mathbb{R}$ a given volumetric fluid source (or fluid sink, which is considered a datum in a system not necessarily in equilibrium), the conservation of total pore fluid content can be stated as an equation for the fluid pressure $p^f(t) : \Omega \rightarrow \mathbb{R}$

$$\left(c_0 + \frac{\alpha^2}{\lambda} \right) \partial_t p^f - \frac{\alpha}{\lambda} \partial_t \psi - \frac{1}{\eta} \operatorname{div} (\kappa \nabla p^f) = \ell, \quad (1.2)$$

where $\kappa(\mathbf{x})$ is the permeability (or hydraulic conductivity) of the porous medium which can be anisotropic, η is the constant viscosity of the pore fluid, and c_0 is the constrained specific storage coefficient (which encompasses both the porosity of the solid skeleton and the compressibility of the fluid or of the solid in the meso-scale).

The equations of motion (balance of linear momentum and the constitutive equation relating stress and strains) consist in finding solid displacements $\mathbf{u}^s(t) : \Omega \rightarrow \mathbb{R}^d$ such that

$$\boldsymbol{\sigma} = 2\mu \boldsymbol{\varepsilon}(\mathbf{u}^s) - \psi \mathbf{I}, \quad (1.3)$$

$$\rho \partial_{tt} \mathbf{u} - \operatorname{div} \boldsymbol{\sigma} = \rho \mathbf{b}, \quad (1.4)$$

where the total pressure is defined in (1.1), $\boldsymbol{\varepsilon}(\mathbf{u}) = \frac{1}{2}(\nabla \mathbf{u} + \nabla \mathbf{u}^\top)$ is the tensor of infinitesimal strains, \mathbf{I} is the identity tensor, ρ denotes the density of the saturated porous material, and μ, λ are the shear and dilation moduli associated with the constitutive law of the solid structure. These and all other model parameters are assumed constant, positive and bounded, except for the dilation modulus λ , which approaches infinity for fully incompressible materials. The analysis in [17] does not consider acceleration in the balance of linear momentum (1.4), as one typically supposes that solid deformations are much slower than the fluid flow rate. Nevertheless we keep that term here, as we will also explore the influence of inertial effects in the context of linear stability analysis.

1.3. Macroscopic description of two-species motion

Next we turn to the incorporation of two interacting species whose dynamics occurs by diffusion and reaction, as well as convection by the velocity of the moving domain. Alternatively, one could also suppose that the species are convected only by the fluid velocity (or by the filtration velocity). Simpler models are able to take advantage of one-dimensional geometries, or of a constant material density of the constituents (e.g., cells) in order to obtain closed-form expressions for the advecting velocity [14]. Instead, here we use the transient form of the equations of motion (1.4),(1.3) to determine such velocity.

We therefore consider the propagation of a generic species with concentration w_1 , reacting with an additional species having a concentration w_2 . The problem can be written as follows

$$\partial_t w_1 + \partial_t \mathbf{u}^s \cdot \nabla w_1 - \operatorname{div} \{D_1(\mathbf{x}) \nabla w_1\} = f(w_1, w_2, \mathbf{u}^s), \quad (1.5)$$

$$\partial_t w_2 + \partial_t \mathbf{u}^s \cdot \nabla w_2 - \operatorname{div} \{D_2(\mathbf{x}) \nabla w_2\} = g(w_1, w_2, \mathbf{u}^s), \quad (1.6)$$

where D_1, D_2 are positive definite matrices containing possibly anisotropy of self-diffusion. The net reaction terms depend on parameters that account for the reproduction of species, the removal of species concentration due to reactive interactions, and the intrinsic changes from local modifications in volume (that is, how the pore microstructure evolves with deformation). For illustrative purposes, and as in [17, 14], we can simply consider hypothetical kinetic specifications, which can also simplify the exposition of the linear stability analysis of Section 2. We choose a modification to the classical Schnakenberg model

$$\begin{aligned} f(w_1, w_2, \mathbf{u}^s) &= \beta_1(\beta_2 - w_1 + w_1^2 w_2) + \gamma w_1 \partial_t \operatorname{div} \mathbf{u}^s, \\ g(w_1, w_2, \mathbf{u}^s) &= \beta_1(\beta_3 - w_1^2 w_2) + \gamma w_2 \partial_t \operatorname{div} \mathbf{u}^s, \end{aligned}$$

where $\beta_1, \beta_2, \beta_3, \gamma$ are positive rate constants. We emphasise again that the mechano-chemical feedback operates only by convection and by the last two terms defining f, g . These terms are modulated by the key parameter $\gamma > 0$, and therefore they act as a local source for a given species if the solid volume increases, otherwise the additional terms contribute to removal of species concentration [14].

1.4. Active stress

We assume that stresses are exerted by solid, by fluid, and by morphogens. Then the forces are condensed in a macroscopic balance equation for the mixture where we recall that the solid phase is simply considered as an isotropic deformable porous medium and that the fluid phase only contributes volumetrically to the stress through the hydrostatic fluid pressure at the interstitium. Microscopic tension generation is here supposed to occur due to active stresses (1.3) and

$$\boldsymbol{\sigma}_{\text{total}} = \boldsymbol{\sigma} + \boldsymbol{\sigma}_{\text{act}}, \quad (1.7)$$

where the active stress operates primarily on a given, constant direction \mathbf{k} , and its intensity depends on a scalar field $r = r(w_1, w_2)$ and on a positive constant τ , to be specified later on (see, e.g., [20])

$$\boldsymbol{\sigma}_{\text{act}} = -\tau r \mathbf{k} \otimes \mathbf{k}. \quad (1.8)$$

1.5. Initial and boundary conditions under different model configurations

We employ appropriate initial data at rest

$$w_1(0) = w_{1,0}, \quad w_2(0) = w_{2,0}, \quad \mathbf{u}^s(0) = \mathbf{0}, \quad \partial_t \mathbf{u}^s(0) = \mathbf{0}, \quad p^f(0) = 0, \quad \psi(0) = 0 \quad \text{in } \Omega \times \{0\}.$$

Regarding boundary conditions, the species concentrations will assume zero diffusive flux boundary conditions on the whole boundary

$$D_1(\mathbf{x}) \nabla w_1 \cdot \mathbf{n} = 0 \quad \text{and} \quad D_2(\mathbf{x}) \nabla w_2 \cdot \mathbf{n} = 0 \quad \text{on } \partial\Omega \times (0, t_{\text{final}}].$$

For the poromechanics we adopt either Robin conditions for the deformations (mimicking the presence of supporting springs) and zero fluid flux everywhere on the boundary,

$$[2\mu\varepsilon(\mathbf{u}^s) - \psi \mathbf{I} + \boldsymbol{\sigma}_{\text{act}}] \mathbf{n} + \zeta \mathbf{u}^s = \mathbf{0} \quad \text{and} \quad \frac{\kappa}{\eta} \nabla p^f \cdot \mathbf{n} = 0 \quad \text{on } \partial\Omega \times (0, t_{\text{final}}], \quad (1.9)$$

where $\zeta > 0$ is the (possibly time-dependent) stiffness of the spring; or as in [17] we can separate the boundary $\partial\Omega = \Gamma \cup \Sigma$ into two parts Γ and Σ where we prescribe clamped boundaries and zero fluid normal fluxes; and zero (total) traction together with constant fluid pressure, respectively

$$\mathbf{u}^s = \mathbf{0} \quad \text{and} \quad \frac{\kappa}{\eta} \nabla p^f \cdot \mathbf{n} = 0 \quad \text{on } \Gamma \times (0, t_{\text{final}}], \quad (1.10)$$

$$[2\mu\varepsilon(\mathbf{u}^s) - \psi \mathbf{I} + \boldsymbol{\sigma}_{\text{act}}] \mathbf{n} = \mathbf{0} \quad \text{and} \quad p^f = 0 \quad \text{on } \Sigma \times (0, t_{\text{final}}]. \quad (1.11)$$

Each case will be specified in the tests of Sections 2 and 4.

2. Linear stability analysis and dispersion relation

Next we proceed to derive a linear stability analysis following [14] (which gives insight about interaction mechanisms between tissue deformation and diffusing solutes). The present development is however more involved, since we are including acceleration effects in the momentum equilibrium equation. We skip as much as possible the lengthy details of the derivation, and concentrate only in the dispersion relation. Note that since the functions f and g are prescribed, we can specify a steady state given by $w_1 = w_{1,0} = \beta_2 + \beta_3$, $w_2 = w_{2,0} = \frac{\beta_3}{(\beta_2 + \beta_3)^2}$, $p = p_0$, $\psi = \psi_0$ and $\mathbf{u} = \mathbf{0}$. We will restrict the analysis to the case of an infinite domain in \mathbb{R}^d , with $d = \{2, 3\}$. We also maintain the dimensional form of the governing equations so that the analysis accommodates a large class of models.

2.1. General form of the dispersion relation

Following, for instance, [21] we can derive a dispersion relation that is eventually defined by the product of two distinct polynomials

$$P(\phi; k^2) = P_1(\phi; k^2)^{d-1} P_2(\phi; k^2),$$

where $P_1(\phi; k^2) = \rho\phi^2 + \mu k^2$, and where $d = \{2, 3\}$ is the spatial dimension of the infinite domain $\Omega = \mathbb{R}^d$, where the linear stability analysis of the coupled problem (1.2)-(1.4) is performed.

Since P_1 is a polynomial with pure imaginary roots, it does not have an influence on the stability of the steady state version of (1.2)-(1.4). Consequently, we can focus our attention on the fifth-order polynomial

$$P_2(\phi; k^2) = A_5(k^2)\phi^5 + A_4(k^2)\phi^4 + A_3(k^2)\phi^3 + A_2(k^2)\phi^2 + A_1(k^2)\phi + A_0(k^2), \quad (2.1)$$

defined by the terms

$$\begin{aligned} A_5(k^2) &= \rho c_0, \\ A_4(k^2) &= \rho \left(c_0(D_1 + D_2) + \frac{\kappa}{\eta} \right) k^2 - \rho c_0 \beta_1 \frac{\beta_3 - \beta_2 - (\beta_2 + \beta_3)^3}{\beta_2 + \beta_3}, \\ A_3(k^2) &= \rho \left(\frac{\kappa}{\eta} (D_1 + D_2) + c_0 D_1 D_2 \right) k^4 \\ &\quad + \left[c_0(2\mu + \lambda) + \alpha^2 - \rho c_0 \beta_1 \frac{D_2(\beta_3 - \beta_2) - D_1(\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} - \frac{\kappa \rho}{\eta} \beta_1 \frac{\beta_3 - \beta_2 - (\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \right] k^2 \\ &\quad + \rho c_0 \beta_1^2 (\beta_2 + \beta_3)^2 - i\gamma \left[\sum_{j=1}^d \widehat{\Upsilon}_j k_j \right] c_0 (w_{1,0}\theta_1 + w_{2,0}\theta_2), \\ A_2(k^2) &= \frac{\kappa \rho}{\eta} D_1 D_2 k^6 + \left[(c_0(2\mu + \lambda) + \alpha^2) (D_1 + D_2) + \frac{\kappa}{\eta} (2\mu + \lambda) - \frac{\kappa \rho}{\eta} \beta_1 \frac{D_2(\beta_3 - \beta_2) - D_1(\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \right] k^4 \\ &\quad + \left[\frac{\kappa \rho}{\eta} \beta_1^2 (\beta_2 + \beta_3)^2 - (c_0(2\mu + \lambda) + \alpha^2) \beta_1 \frac{\beta_3 - \beta_2 - (\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \right] k^2 \\ &\quad - i\gamma \left[\sum_{j=1}^d \widehat{\Upsilon}_j k_j \right] \left[\left(\frac{\kappa}{\eta} (w_{1,0}\theta_1 + w_{2,0}\theta_2) + c_0 (w_{1,0}\theta_1 D_2 + w_{2,0}\theta_2 D_1) \right) k^2 \right. \\ &\quad \left. + c_0 \left(-w_{1,0}\theta_2 \frac{2\beta_1\beta_3}{\beta_2 + \beta_3} + w_{2,0}\theta_1\beta_1(\beta_2 + \beta_3)^2 + w_{1,0}\theta_1\beta_1(\beta_2 + \beta_3)^2 - w_{2,0}\theta_2 \frac{\beta_1(\beta_3 - \beta_2)}{\beta_2 + \beta_3} \right) \right], \\ A_1(k^2) &= \left[\frac{\kappa}{\eta} (2\mu + \lambda) (D_1 + D_2) + (c_0(2\mu + \lambda) + \alpha^2) D_1 D_2 \right] k^6 \\ &\quad - \left[(c_0(2\mu + \lambda) + \alpha^2) \beta_1 \frac{D_2(\beta_3 - \beta_2) - D_1(\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} + \frac{\kappa}{\eta} (2\mu + \lambda) \beta_1 \frac{\beta_3 - \beta_2 - (\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \right] k^4 \\ &\quad + (c_0(2\mu + \lambda) + \alpha^2) \beta_1^2 (\beta_2 + \beta_3)^2 k^2 - i\frac{\kappa \gamma}{\eta} \left[\sum_{j=1}^d \widehat{\Upsilon}_j k_j \right] \left[(w_{1,0}\theta_1 D_2 + w_{2,0}\theta_2 D_1) k^2 \right] \end{aligned}$$

$$-w_{1,0}\theta_2\frac{2\beta_1\beta_3}{\beta_2+\beta_3}+w_{2,0}\theta_1\beta_1(\beta_2+\beta_3)^2+w_{1,0}\theta_1\beta_1(\beta_2+\beta_3)^2-w_{2,0}\theta_2\frac{\beta_1(\beta_3-\beta_2)}{\beta_2+\beta_3}\Bigg]k^2,$$

$$A_0(k^2)=\frac{\kappa}{\eta}(2\mu+\lambda)k^4\left(D_1D_2k^4-\beta_1\frac{D_2(\beta_3-\beta_2)-D_1(\beta_2+\beta_3)^3}{\beta_2+\beta_3}k^2+\beta_1^2(\beta_2+\beta_3)^2\right),$$

where the coefficients $w_{j,0}$, for $j = \{1, 2\}$, are the steady state concentrations of generic species w_j , and

$$\theta_j = (\partial_{\mathbf{w}}\sigma_{act}(\mathbf{w}_0))_j, \quad \sigma_{act}(\mathbf{w}) = -\tau r(\mathbf{w}), \quad \hat{\Upsilon}_j = \Upsilon_{\cdot j} + i\tilde{\Upsilon}_j,$$

$$\Upsilon_{\cdot j} = \sum_k \partial_{\mathbf{x}_k} \Upsilon_{kj}, \quad \tilde{\Upsilon}_j = \sum_k k_k \Upsilon_{kj}, \quad \Upsilon = \mathbf{k} \otimes \mathbf{k}.$$

For the rest of the linear analysis, we impose that $\Upsilon = \mathbf{I}$, with \mathbf{I} the identity matrix, $r^{(1)}(\mathbf{w}) = w_1 + w_2$, $r^{(2)}(\mathbf{w}) = w_1^2$, and $\mathbf{b} = \mathbf{0}$. Under such conditions, only the coefficients A_3, A_2, A_1 are modified and they adopt the following forms

$$A_3(k^2) = \left[\rho \left(\frac{\kappa}{\eta} (D_1 + D_2) + c_0 D_1 D_2 \right) \right] k^4$$

$$+ \left[c_0 (2\mu + \lambda) + \alpha^2 - \rho c_0 \beta_1 \frac{D_2(\beta_3 - \beta_2) - D_1(\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} - \frac{\kappa \rho}{\eta} \beta_1 \frac{\beta_3 - \beta_2 - (\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \right.$$

$$\left. + \gamma c_0 \left((\beta_2 + \beta_3) \theta_1^{(i)} + \frac{\beta_3}{(\beta_2 + \beta_3)^2} \theta_2^{(i)} \right) \right] k^2 + \rho c_0 \beta_1^2 (\beta_2 + \beta_3)^2,$$

$$A_2(k^2) = \frac{\kappa \rho}{\eta} D_1 D_2 k^6 + \left[(c_0 (2\mu + \lambda) + \alpha^2) (D_1 + D_2) + \frac{\kappa}{\eta} (2\mu + \lambda) - \frac{\kappa \rho}{\eta} \beta_1 \frac{D_2(\beta_3 - \beta_2) - D_1(\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \right.$$

$$\left. + \gamma \left(\frac{\kappa}{\eta} \left((\beta_2 + \beta_3) \theta_1^{(i)} + \frac{\beta_3}{(\beta_2 + \beta_3)^2} \theta_2^{(i)} \right) + c_0 \left((\beta_2 + \beta_3) \theta_1^{(i)} D_2 + \frac{\beta_3}{(\beta_2 + \beta_3)^2} \theta_2^{(i)} D_1 \right) \right) \right] k^4$$

$$+ \left[\frac{\kappa \rho}{\eta} \beta_1^2 (\beta_2 + \beta_3)^2 - (c_0 (2\mu + \lambda) + \alpha^2) \beta_1 \frac{\beta_3 - \beta_2 - (\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \right.$$

$$\left. + \gamma \left(-2\beta_1 \beta_3 \theta_2^{(i)} + \beta_1 \beta_3 \theta_1^{(i)} + \beta_1 (\beta_2 + \beta_3)^3 \theta_1^{(i)} - \frac{\beta_1 \beta_3 (\beta_3 - \beta_2)}{(\beta_2 + \beta_3)^3} \theta_2^{(i)} \right) \right] k^2,$$

$$A_1(k^2) = \left[\frac{\kappa}{\eta} (2\mu + \lambda) (D_1 + D_2) + (c_0 (2\mu + \lambda) + \alpha^2) D_1 D_2 + \frac{\gamma \kappa}{\eta} \left((\beta_2 + \beta_3) \theta_1^{(i)} D_2 + \frac{\beta_3}{(\beta_2 + \beta_3)^2} \theta_2^{(i)} D_1 \right) \right] k^6$$

$$- \left[\frac{\gamma \kappa}{\eta} \left(2\beta_1 \beta_3 \theta_2^{(i)} - \beta_1 \beta_3 \theta_1^{(i)} - \beta_1 (\beta_2 + \beta_3)^3 \theta_1^{(i)} + \frac{\beta_1 \beta_3 (\beta_3 - \beta_2)}{(\beta_2 + \beta_3)^3} \theta_2^{(i)} \right) \right.$$

$$\left. + (c_0 (2\mu + \lambda) + \alpha^2) \beta_1 \frac{D_2(\beta_3 - \beta_2) - D_1(\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} + \frac{\kappa}{\eta} (2\mu + \lambda) \beta_1 \frac{\beta_3 - \beta_2 - (\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \right] k^4$$

$$+ (c_0 (2\mu + \lambda) + \alpha^2) \beta_1^2 (\beta_2 + \beta_3)^2 k^2.$$

As the characteristic polynomial (2.1) is of high order, it is challenging to determine analytically the main features of the coupled set of equations. We will therefore solve the eigenvalue systems numerically. Before that, we note that for the case without inertia ($\rho = 0$), the polynomial $P(\phi; k^2)$ is only of order 3. We concentrate on separate cases including or not the inertial term. Unless specified otherwise, throughout the analysis we will employ the following parameter values

$$D_1 = 0.05, \quad D_2 = 1.0, \quad \beta_1 = 170, \quad \beta_2 = 0.1305, \quad \beta_3 = 0.7695, \quad E = 3 \cdot 10^4, \quad \nu = 0.495,$$

$$\rho = 1, \quad c_0 = 1 \cdot 10^{-3}, \quad \kappa = 1 \cdot 10^{-4}, \quad \alpha = 0.1, \quad \eta = 1, \quad \gamma = 1 \cdot 10^{-4}, \quad \ell = 0,$$

which are relevant to the specifications in Tests 1-4 from Section 4. All the computations and graphs in the remainder of this section have been produced with an in-house MATLAB implementation.

2.2. Spatial homogeneous distributions

For the case $k^2 = 0$, the characteristic polynomial $P_2(\phi; 0) = 0$ reduces to

$$P_2(\phi; 0) = \phi^3 \left[\rho c_0 \phi^2 - \rho c_0 \beta_1 \frac{\beta_3 - \beta_2 - (\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \phi + \rho c_0 \beta_1^2 (\beta_2 + \beta_3)^2 \right].$$

Therefore its roots are either zero, or are defined by the second-order polynomial in square brackets. Owing to the Routh-Hurwitz theory, for any polynomial of order 2, a necessary and sufficient set of conditions can be stated so that the roots are in the space $\{z \in \mathbb{C} : \Re(z) \leq 0\}$. For a general polynomial $P(\phi) = a_2 \phi^2 + a_1 \phi + a_0$, we need to satisfy that all $a_i > 0$ (or all $a_i < 0$). In the present case, a_2 and a_0 are positive by definition, and consequently the spatial homogeneous case is stable, if and only if

$$\beta_3 - \beta_2 < (\beta_2 + \beta_3)^3. \quad (2.2)$$

Thus, the difference between the basal source rate β_3 with respect to β_2 might be smaller than $(\beta_2 + \beta_3)^3$, and a similar condition is provided in [22]. Additionally, we observe that the system is homogeneously stable irrespective of the parameter values, by simply removing the acceleration term in the momentum equilibrium.

2.3. Uncoupled system

This scenario is reached if either γ or τ (or both) are zero. $P_2(\phi; k^2)$ is then a fifth-order polynomial defined as in (2.1) where the terms including γ or τ are dropped from the coefficients $A_i(k^2)$. For a polynomial of order 5, $P(\phi) = \sum_{j=0}^5 a_j \phi^j$, the Routh-Hurwitz conditions are given by

$$\forall_j \quad a_j > 0, \quad (2.3)$$

$$a_3 a_4 - a_2 a_5 > 0, \quad (2.4)$$

$$a_2 a_3 a_4 - a_2^2 a_5 - a_1 a_4^2 + a_0 a_4 a_5 > 0, \quad (2.5)$$

$$a_0 a_2 a_3 a_4 a_5 - a_0 a_3^2 a_4^2 + a_1 a_2 a_3 a_4^2 - a_1 a_2^2 a_4 a_5 - a_1^2 a_4^3 + 2a_0 a_1 a_4^2 a_5 - a_0^2 a_4 a_5^2 > 0. \quad (2.6)$$

Condition (2.2) indicates that β_2 and β_3 are both relevant. We decide to perform the analysis varying β_2 and fixing all the other parameters. The choice is justified by the influence of this parameter on the stability of the spatial homogeneous case and the direct relation of β_2 (or alternatively, β_3) on the sign of the conditions (2.3)-(2.6). Based on (2.2) and the parameter constraint, we can readily deduce that a_4 and a_5 are strictly positive, and they are rejected (they do not lead to patterning in the system). The complete analysis of (2.3)-(2.6) is analytically quite involved, however some information can already be drawn by looking at conditions that violate $a_0 > 0$. Note that a_1, a_2, a_3 can be written as affine functions of a_0 with positive coefficients, as long as $\rho \neq 0$. This leads, in the uncoupled system, to the property that if the conditions $a_i > 0$ are violated, then a_0 cannot be positive.

Figure 2.1(A) plots the contour lines of a_i , $i = 0, \dots, 4$. As we can observe for this specific parameter set, a_2, a_4 are negative only in the region below the magenta dot-dashed curve, corresponding to the limit given by condition (2.2). Consequently, these coefficients are strictly positive while (2.2) is true. Only a_0 and a_1 present Turing instability, and the latter is just a subset of the k - β_2 space defined by a_0 . Conditions (2.4)-(2.6) present a similar behaviour as that observed for a_0 (Figs. 2.1(B)-(D)), and therefore the analysis can be focused on a_0 only. For the case $\rho = 0$, the resulting polynomial is of order 3 and so the Routh-Hurwitz conditions are defined by

$$\forall_j \quad a_j > 0, \quad a_1 a_2 - a_0 a_3 > 0. \quad (2.7)$$

Note that, contrary to the general case, only a_1 can be written as an affine function of a_0 . As the condition (2.2) is no longer needed to obtain homogeneous stability, the coefficients of the affine description of a_1 are not necessarily strictly positive as before. Nevertheless, as illustrated in Figure 2.2, condition $a_0 > 0$ is the first to be broken with respect to the value of β_2 , and thus we proceed to analyse that coefficient.

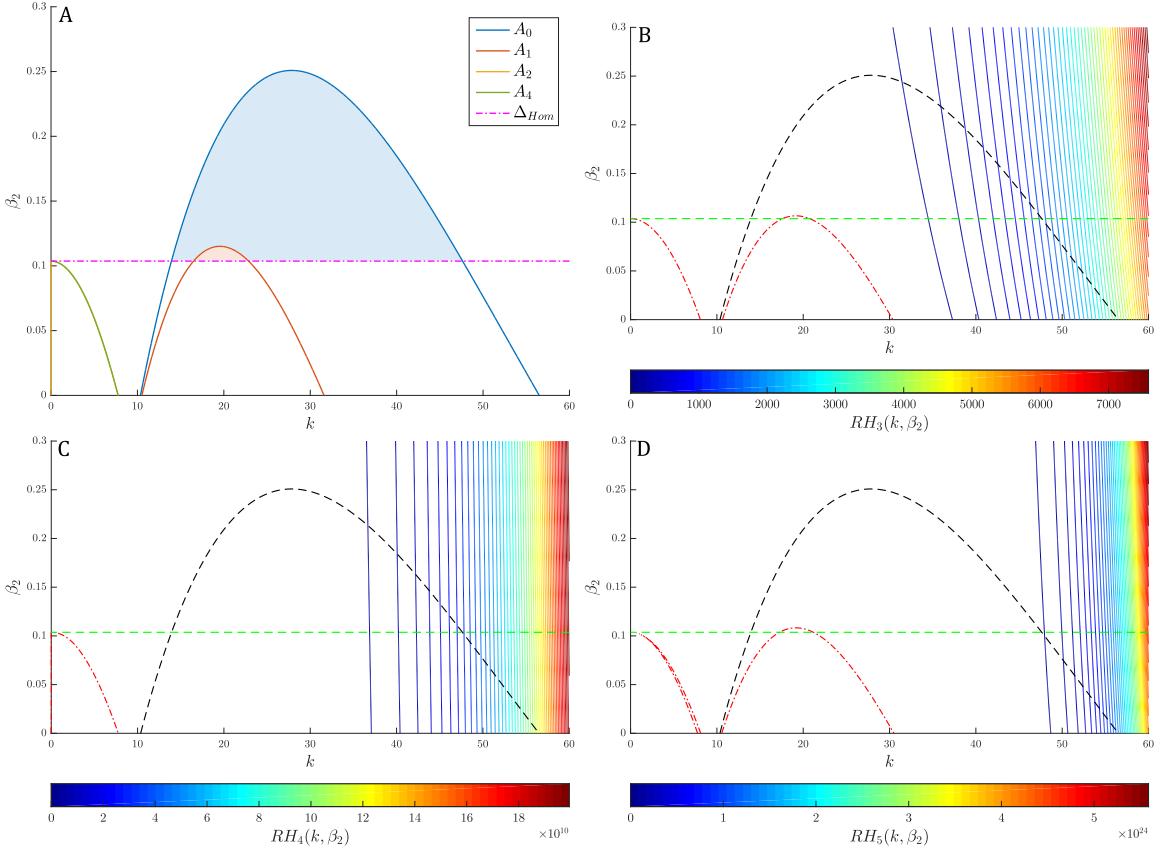


Figure 2.1: Contour plots of the Routh-Hurwitz conditions for the characteristic polynomial of uncoupled system (1.2)-(1.4) with $\rho = 1$. (A) Null level set of P_2 -polynomial coefficients a_i defined in (2.1). a_3 is strictly positive for the selected fixed parameters and so it is not presented. The magenta dot-dashed curve corresponds to the limit of condition (2.2) with fixed $\beta_3 = 0.7695$. (B) Level sets (100) of condition (2.4). Null levels of condition (2.4) (red dot-dashed); a_0 (black dashed); and condition (2.2) (green dashed) are added to locate Turing instability regions. (C-D) Similar analyses for the conditions (2.5) and (2.6) respectively. In all plots, colour-shaded regions correspond to a k - β_2 space that breaks the associated condition.

By definition, a_0 is a polynomial of even order with respect to k^2 , guaranteeing that there exists at least one local extremum. Therefore, we look for the critical wave number $k_c^2 > 0$, as the solution to $a'_0(k_c^2) = 0$ that substituting in a_0 will give $a_0(k_c^2, \varphi_c) = 0$, with φ_c being the critical parameter to analyse. In the present case a'_0 is a cubic polynomial with respect to k^2 . Then the following criteria may hold for a_0 to be negative

$$D_2(\beta_3 - \beta_2) - D_1(\beta_2 + \beta_3)^3 > 0, \quad (2.8)$$

$$36 \left(\beta_1 \frac{D_2(\beta_3 - \beta_2) - D_1(\beta_2 + \beta_3)^3}{\beta_2 + \beta_3} \right)^2 (\beta_1^2(\beta_2 + \beta_3)^2)^2 - 128D_1D_2 (\beta_1^2(\beta_2 + \beta_3)^2)^3 > 0. \quad (2.9)$$

Inequality (2.8) arises from the Routh-Hurwitz conditions, and it enforces that the coefficient has a real positive part. Combined with condition (2.2), it gives an interval for the ratio $(\beta_2 + \beta_3)^3/(\beta_3 - \beta_2)$ where Turing instabilities are reached. As the discriminant of a_0 is null, we look for the discriminant (2.9) of the derivative a'_0 to force $k^2 \in \mathbb{R}$. Figure 2.3 (panels (A)-(C)) presents the patterning space based on the implicit functions defined in (2.8) and (2.9) for the (β_2, β_3) space. The plots suggest that increasing the value of the production basal rate (β_3) of the inhibitor w_2 leads to a larger interval of possible basal rates (β_2) of the activator w_1 . The condition (2.2), represented by the blue-dot-dashed curve in Figure 2.3(A), is absent for the $\rho = 0$ scenario. This enlarges the patterning space, and therefore the presence of acceleration in the

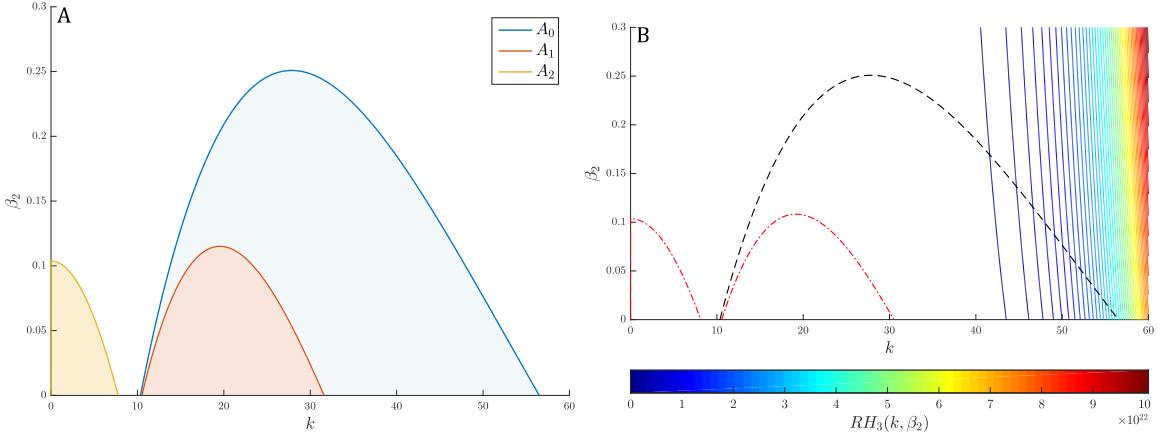


Figure 2.2: Contour plots of the Routh-Hurwitz conditions for the characteristic polynomial of uncoupled system (1.2)-(1.4) with $\rho = 0$. (A) Null level set of P_2 -polynomial coefficients a_i defined in (2.1). a_3 is strictly positive whatever the choice of the parameters and so it is not presented. (B) Level sets (100) of the second condition defined in (2.7). Null levels of condition (2.7) (red dot-dashed); and a_0 (black dashed) are added to locate Turing instability regions.

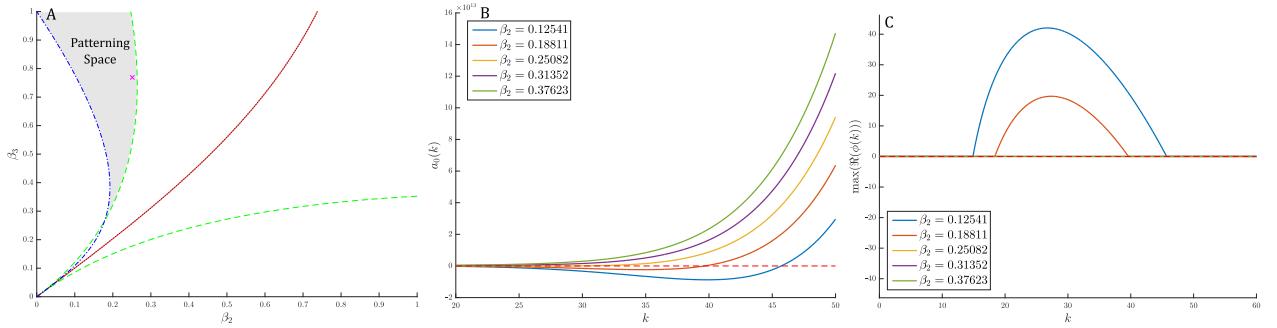


Figure 2.3: Patterning space, parameter condition and dispersion relations for the uncoupled poromechano-chemical model. (A) Predicted patterning space for a selected interval in (β_2, β_3) parameter space: boundary constructed from (2.8) (red plain); from (2.9) (green-dashed); and from (2.2) (blue-dot-dashed). (B) Parameter coefficient condition a_0 . Curves are drawn from the critical value $\beta_{2,c}$ (yellow) and for 25% and 50% increase/decrease of the parameter values. The critical parameter value is located in (A) and denoted by a magenta cross. (C) Associated dispersion relations, where the colour code is kept identical as in (B).

momentum equilibrium equation restricts the Turing space.

Taking into account the stability of the homogeneous spatial case, the constraint (2.8) is key for generating instabilities. If (2.8) is unsatisfied, all the dispersion relation coefficients are positive, whatever the choice of the parameter values. Figure 2.3(A) shows that condition (2.8) is not sufficient to onset instability, and the patterning space is smaller than the region delimited by the red curve in Figure 2.3(A). The question is then to check whether, after selecting a β_2 in the region delimited by the green-dashed and the red-solid curves in the patterning space, we can have instability by varying the value of β_1 only. Figures 2.4(A1)-(A2) display the behaviour of the uncoupled system for different values of β_1 and β_2 , fixing all other coefficients. When the system reaches the critical value for β_2 (magenta-dashed curve in Fig. 2.4(A1)), we see that a_0 tends to be strictly positive and prevents any instability from that condition (the other Routh-Hurwitz conditions are satisfied for the selected fixed parameters). Nevertheless, β_1 still has an influence by extending the space scale where instability can occur (see Fig. 2.4(A2)), without affecting the value of the critical value of β_2 (all the null level-sets do not exceed the reference magenta-dashed curve in Fig. 2.4(A2)). This confirms that β_2 (or eventually β_3) are appropriate parameters to analyse the stability of the system in the uncoupled scenario.

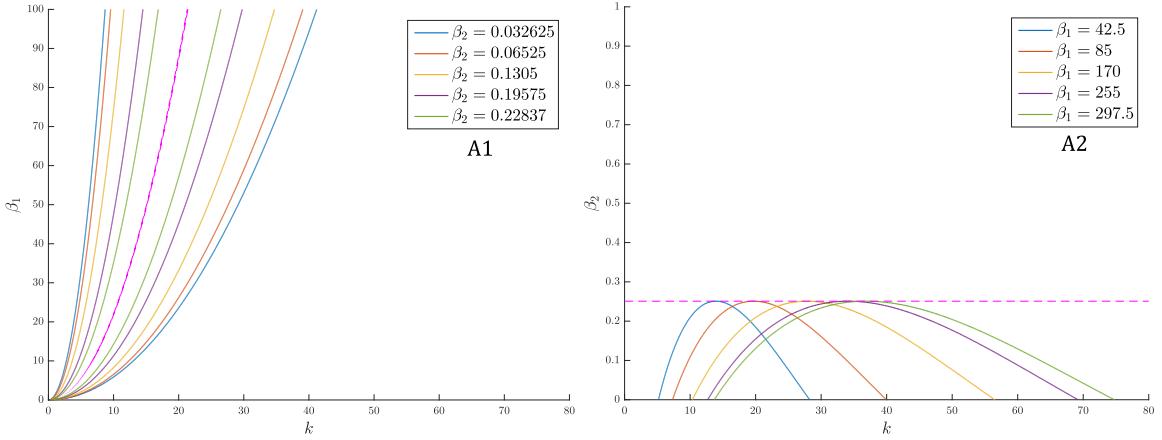


Figure 2.4: Contour plots of the Routh-Hurwitz conditions for the characteristic polynomial of the uncoupled system (1.2)-(1.4). (A1) Null level-set of \$P_2\$-polynomial coefficients \$a_0\$ defined in (2.1) for different \$\beta_2\$'s. (A2) Null level set of \$P_2\$-polynomial coefficients \$a_0\$ defined in (2.1) for different \$\beta_1\$'s. The magenta curve is used as reference for the critical \$\beta_2\$ value computed from \$a_0\$, setting \$\beta_1 = 170\$.

2.4. Coupled system - Null production/degradation rates

In contrast with classical reaction-diffusion systems, due to the coupling with the poroelastic deformations we can perfectly encounter cases where production/degradation rates are missing. For the first case of \$\beta_1 = 0\$ (corresponding to a pure convection-diffusion chemical system) the characteristic polynomial for \$\rho \neq 0\$ is still of order 5 with the new coefficients

$$\begin{aligned}
A_5^{(1)}(k^2) &= A_5(k^2), & A_4^{(1)}(k^2) &= \rho \left(c_0(D_1 + D_2) + \frac{\kappa}{\eta} \right) k^2, \\
A_3^{(1)}(k^2) &= \rho \left(\frac{\kappa}{\eta}(D_1 + D_2) + c_0 D_1 D_2 \right) k^4 + \left[c_0(2\mu + \lambda) + \alpha^2 + \gamma c_0 \left((\beta_2 + \beta_3)\theta_1^{(i)} + \frac{\beta_3}{(\beta_2 + \beta_3)^2}\theta_2^{(i)} \right) \right] k^2, \\
A_2^{(1)}(k^2) &= \frac{\kappa\rho}{\eta} D_1 D_2 k^6 + \left[(c_0(2\mu + \lambda) + \alpha^2)(D_1 + D_2) + \frac{\kappa}{\eta}(2\mu + \lambda) \right. \\
&\quad \left. + \gamma \left(\frac{\kappa}{\eta} \left((\beta_2 + \beta_3)\theta_1^{(i)} + \frac{\beta_3}{(\beta_2 + \beta_3)^2}\theta_2^{(i)} \right) + c_0 \left((\beta_2 + \beta_3)\theta_1^{(i)} D_2 + \frac{\beta_3}{(\beta_2 + \beta_3)^2}\theta_2^{(i)} D_1 \right) \right) \right] k^4, \\
A_1^{(1)}(k^2) &= \left[\frac{\kappa}{\eta}(2\mu + \lambda)(D_1 + D_2) + (c_0(2\mu + \lambda) + \alpha^2) D_1 D_2 + \frac{\gamma\kappa}{\eta} \left((\beta_2 + \beta_3)\theta_1^{(i)} D_2 + \frac{\beta_3}{(\beta_2 + \beta_3)^2}\theta_2^{(i)} D_1 \right) \right] k^6, \\
A_0^{(1)}(k^2) &= \frac{\kappa}{\eta}(2\mu + \lambda) D_1 D_2 k^8,
\end{aligned}$$

where each \$\boldsymbol{\theta}^{(i)}\$ (for \$i = 1, 2\$) is specified as

$$\boldsymbol{\theta}^{(1)} = \begin{pmatrix} \theta_1^{(1)} \\ \theta_2^{(1)} \end{pmatrix} = -\tau(1, 1)^\top, \quad \boldsymbol{\theta}^{(2)} = -2\tau(1, 0)^\top. \quad (2.10)$$

The spatially homogeneous case of \$k = 0\$ remains stable irrespective of the parameter values, by definition. Also note that for a general \$k\$, all the coefficients that do not include the coupling parameter \$\gamma\$ are strictly positive, and consequently they do not influence the stability of the coupled system. As there is no restriction on the parameter values for the homogeneous case, any parameter can be chosen as the critical one. In order to analyse the effect of poromechanics on the chemical system, we regard \$\tau\$ as the parameter of interest.

Figure 2.5 presents contour plots of the Routh-Hurwitz conditions with respect to the wave number \$k\$ and the parameter \$\tau\$, for both \$\boldsymbol{\theta}\$ defined in (2.10). From Figures 2.5(A1) and 2.5(B1), we observe that \$a_3\$ is the

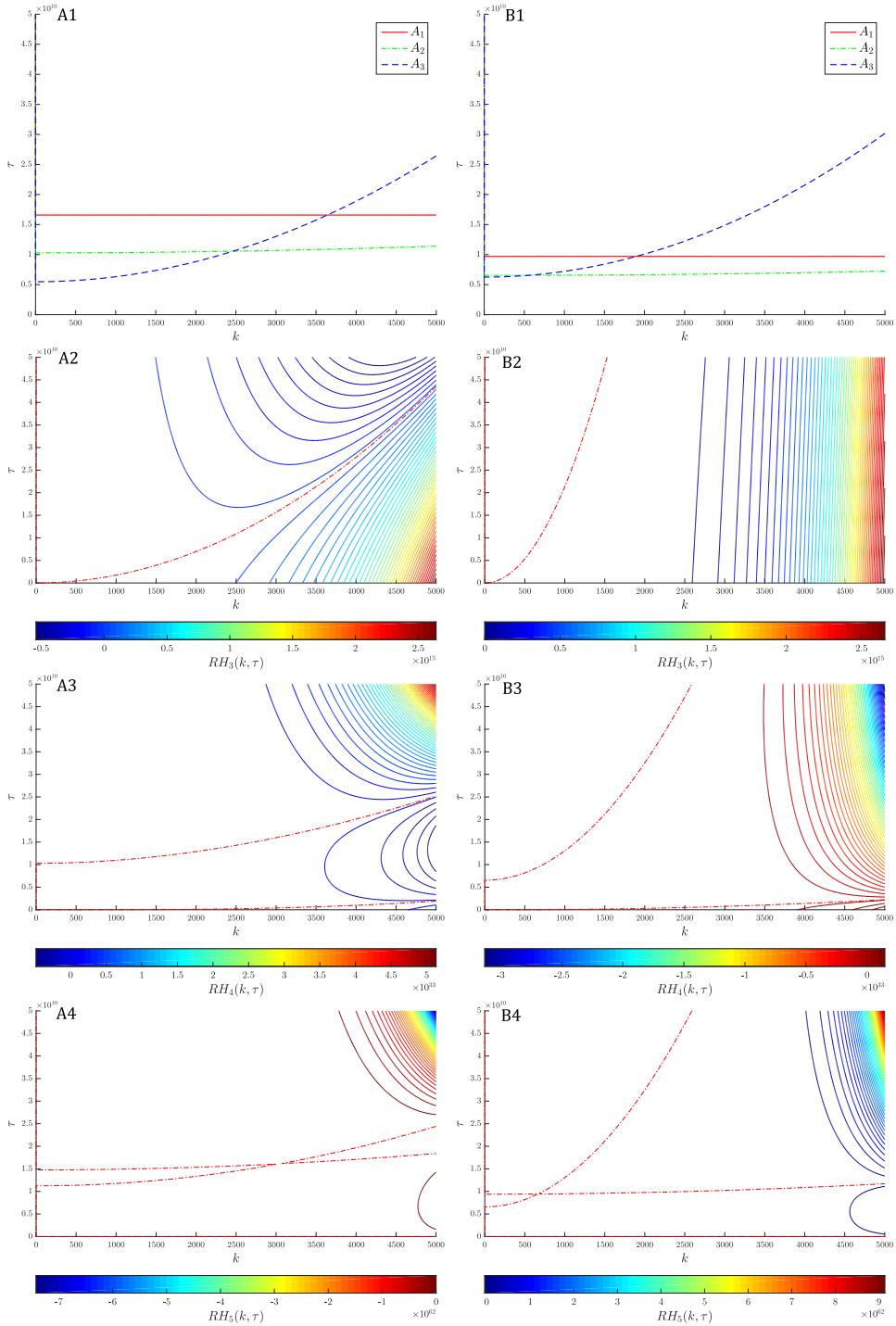


Figure 2.5: Contour plots of the Routh-Hurwitz conditions for the characteristic polynomial of system (1.2)-(1.4) for $\beta_1 = 0$ and $\rho = 1$. (A1) Null level set of P_2 -polynomial coefficients $a_i^{(1)}$ for the coupling term $\theta^{(1)}$. (A2) Level sets (100) of condition (2.4) with null level of the condition (2.4) (red dot-dashed) for the coupling term $\theta^{(1)}$. (A3-A4) Similar analysis for the conditions (2.5) and (2.6) respectively. (B1-B4) Similar analysis for the coupling term $\theta^{(2)}$.

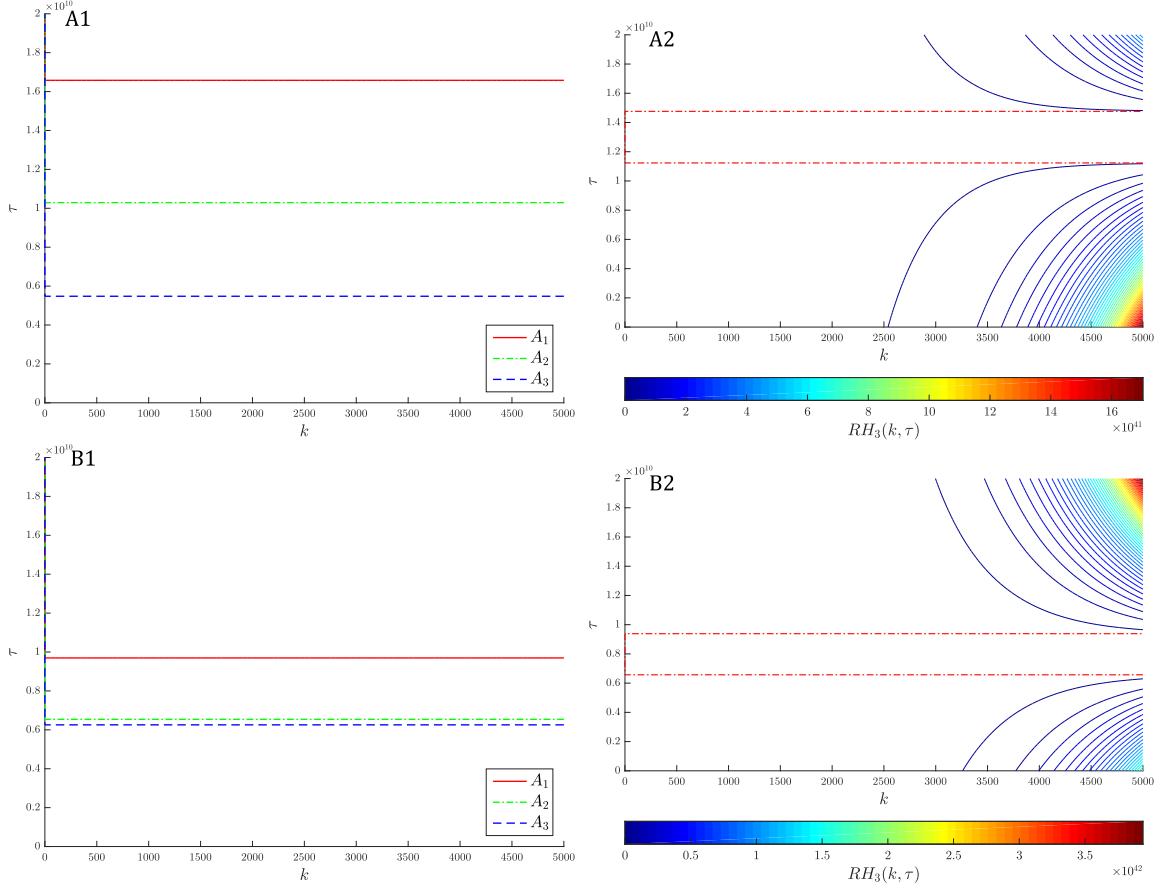


Figure 2.6: Contour plots of the Routh-Hurwitz conditions for the characteristic polynomial of system (1.2)-(1.4) for $\beta_1 = 0$ and $\rho = 0$. (A1) Null level set of P_2 -polynomial coefficients $a_i^{(1)}$ for the coupling term $\theta^{(1)}$. (A2) Level sets (100) of condition (2.7) with associated null level (red dot-dashed) for the coupling term $\theta^{(1)}$. (B1-B2) Similar analysis for the coupling term $\theta^{(2)}$.

first coefficient to break the inequality condition with respect to τ , and this occurs at a low wave number. Along k , the parabolic shape of the null levels shows how, depending on the size of the system, any of the three coefficients can break the Routh-Hurwitz inequality. Consequently, the coupled system presents complex instabilities and makes it difficult to choose only one coefficient to analyse the full patterning space. Nevertheless, patterns are reachable for large values of τ , irrespective of the wave number (at least in the presented interval). This is contrary to the uncoupled case, where all the a_i 's are strictly positive. Figures 2.5(A2)-(A4) and 2.5(B2)-(B4) depict the sign of the conditions (2.4)-(2.6) for $\theta^{(1)}$ and $\theta^{(2)}$, respectively. We readily see that the instability region starts already at a value of τ ($\sim 10^5$) lower than that provided by the a_i 's. This emphasises further the effects of the poromechanical coupling into pattern formation.

The choice of the coupling function θ has a non-intuitive influence on the Routh-Hurwitz conditions. While the area of the instability region for conditions (2.4) and (2.6) (cf. respectively Figs. 2.5(A2), (B2) and Figs. 2.5(A4), (B4)) is decreased, it is in turn increased for condition (2.5) (cf. Figs. 2.5(A3), (B3)). Proposing a patterning space based uniquely on the parameters can still be quite difficult due to the complexity of the Routh-Hurwitz conditions and by the evolution of the inequality constrain through the wave number. Nonetheless, we can still show how the poromechanics coupled to a pure convection-diffusion system may generate patterns. In the absence of acceleration, the analysis of the Routh-Hurwitz conditions is quite similar (see Figure 2.6) to the general case. We observe again that for a specific τ , the conditions can break for any

coupling function $\boldsymbol{\theta}$. Contrary to the case of $\rho = 1$, here the defect on the criteria occurs almost at one specific value of τ for any wave number k (see Figs. 2.6(A1), (B1)). The coupling function seems to move closer to each other the levels of the different coefficients a_i , and it also decreases the interval of τ that leads to breaking the second condition (2.7).

Secondly, we impose either the basal rate of the activator, β_2 , or the inhibitor, β_3 , to be zero. Again the characteristic polynomial $P_2(\phi, k^2)$ for $\rho \neq 0$ is still of order 5 with the new coefficients given by

$$\begin{aligned}
A_5^{(2)}(k^2) &= A_5^{(3)}(k^2) = A_5(k^2), \quad A_4^{(2,3)}(k^2) = \rho \left(c_0(D_1 + D_2) + \frac{\kappa}{\eta} \right) k^2 - \begin{cases} \rho c_0 \beta_1 (1 - \beta_3^2) \\ -\rho c_0 \beta_1 (1 + \beta_2^2), \end{cases} \\
A_3^{(2,3)}(k^2) &= \rho \left(\frac{\kappa}{\eta} (D_1 + D_2) + c_0 D_1 D_2 \right) k^4 \\
&\quad + \begin{cases} \left[c_0(2\mu + \lambda) + \alpha^2 - \rho c_0 \beta_1 (D_2 - D_1 \beta_3^2) - \frac{\kappa \rho}{\eta} \beta_1 (1 - \beta_3^2) + \Psi(\beta_3; \tau) \right] k^2 + c_0 \rho \beta_1^2 \beta_3^2 \\ \left[c_0(2\mu + \lambda) + \alpha^2 + \rho c_0 \beta_1 (D_2 + D_1 \beta_2^2) + \frac{\kappa \rho}{\eta} \beta_1 (1 + \beta_2^2) + \Psi(\beta_2; \tau) \right] k^2 + c_0 \rho \beta_1^2 \beta_2^2, \end{cases} \\
A_2^{(2,3)} &= \frac{\kappa \rho}{\eta} D_1 D_2 k^6 \\
&\quad + \begin{cases} \left[(c_0(2\mu + \lambda) + \alpha^2) (D_1 + D_2) + \frac{\kappa}{\eta} (2\mu + \lambda) - \frac{\kappa \rho}{\eta} \beta_1 (D_2 - D_1 \beta_3^2) + \Psi(\beta_3; \tau) \right] k^4 \\ \left[(c_0(2\mu + \lambda) + \alpha^2) (D_1 + D_2) + \frac{\kappa}{\eta} (2\mu + \lambda) + \frac{\kappa \rho}{\eta} \beta_1 (D_2 + D_1 \beta_2^2) + \Psi(\beta_2; \tau) \right] k^4 \end{cases} \\
&\quad + \begin{cases} \left[\frac{\kappa \rho}{\eta} \beta_1^2 \beta_3^2 - (c_0(2\mu + \lambda) + \alpha^2) \beta_1 (1 - \beta_3^2) + \Psi(\beta_3; \tau) \right] k^2 \\ \left[\frac{\kappa \rho}{\eta} \beta_1^2 \beta_2^2 + (c_0(2\mu + \lambda) + \alpha^2) \beta_1 (1 + \beta_2^2) + \Psi(\beta_2; \tau) \right] k^2, \end{cases} \\
A_1^{(2,3)} &= \begin{cases} \left[\frac{\kappa}{\eta} (2\mu + \lambda) (D_1 + D_2) + (c_0(2\mu + \lambda) + \alpha^2) D_1 D_2 + \Psi(\beta_3; \tau) \right] k^6 \\ \left[\frac{\kappa}{\eta} (2\mu + \lambda) (D_1 + D_2) + (c_0(2\mu + \lambda) + \alpha^2) D_1 D_2 + \Psi(\beta_2; \tau) \right] k^6 \end{cases} \\
&\quad - \begin{cases} \left[(c_0(2\mu + \lambda) + \alpha^2) \beta_1 (D_2 - D_1 \beta_3^2) + \frac{\kappa}{\eta} (2\mu + \lambda) \beta_1 (1 - \beta_3^2) + \Psi(\beta_3; \tau) \right] k^4 \\ - \left[(c_0(2\mu + \lambda) + \alpha^2) \beta_1 (D_2 + D_1 \beta_2^2) + \frac{\kappa}{\eta} (2\mu + \lambda) \beta_1 (1 + \beta_2^2) - \Psi(\beta_2; \tau) \right] k^4 \end{cases} \\
&\quad + \begin{cases} (c_0(2\mu + \lambda) + \alpha^2) \beta_1^2 \beta_3^2 k^2 \\ (c_0(2\mu + \lambda) + \alpha^2) \beta_1^2 \beta_2^2 k^2, \end{cases} \\
A_0^{(2,3)} &= \begin{cases} \frac{\kappa}{\eta} (2\mu + \lambda) k^4 [D_1 D_2 k^4 - \beta_1 (D_2 - D_1 \beta_3^2) k^2 + \beta_1^2 \beta_3^2] \\ \frac{\kappa}{\eta} (2\mu + \lambda) k^4 [D_1 D_2 k^4 + \beta_1 (D_2 + D_1 \beta_2^2) k^2 + \beta_1^2 \beta_2^2], \end{cases}
\end{aligned}$$

where Ψ is a generic function that summarises the appropriate coupling term defined precisely in (2.1) and the upper (resp. lower) line in braces exhibits the coefficient description for $\beta_2 = 0$ (resp. $\beta_3 = 0$). We observe from the new set of coefficients that the stability of the system behaves differently with respect to a zero basal rate. In an uncoupled scenario, the case $\beta_3 = 0$ implies that the a_i 's terms are strictly positive whatever the value of the coefficients. This indicates that removing the basal production of the inhibitor prevents any patterning (in the uncoupled scenario), and this occurs for any ρ and any wave number k . For $\beta_2 = 0$, the system can enter an instability region if and only if

$$0 < \beta_3 < \sqrt{\min \left(1, \frac{D_2}{D_1} \right)}.$$

Coupling the convection-reaction-diffusion system to the poromechanics enables both scenarios to reach an instability for some parameter values. We analyse again the coupled system focusing on τ . Figure 2.7 presents the null level set of the coefficients for both $\boldsymbol{\theta}$ (*cf.* (2.10)) and $\rho = 1$. The case $\beta_2 = 0$ (see Figs. 2.7(A1), (B1)) is significantly affected by the choice of $\boldsymbol{\theta}$. Going from a linear $\boldsymbol{\theta}^{(1)}$ to a nonlinear $\boldsymbol{\theta}^{(2)}$ coupling function, the instability region is clearly modified, especially for the coefficient a_2 , leading to a larger area. Furthermore, starting from a given wave number k , the system presents instability whatever the choice of the parameter τ

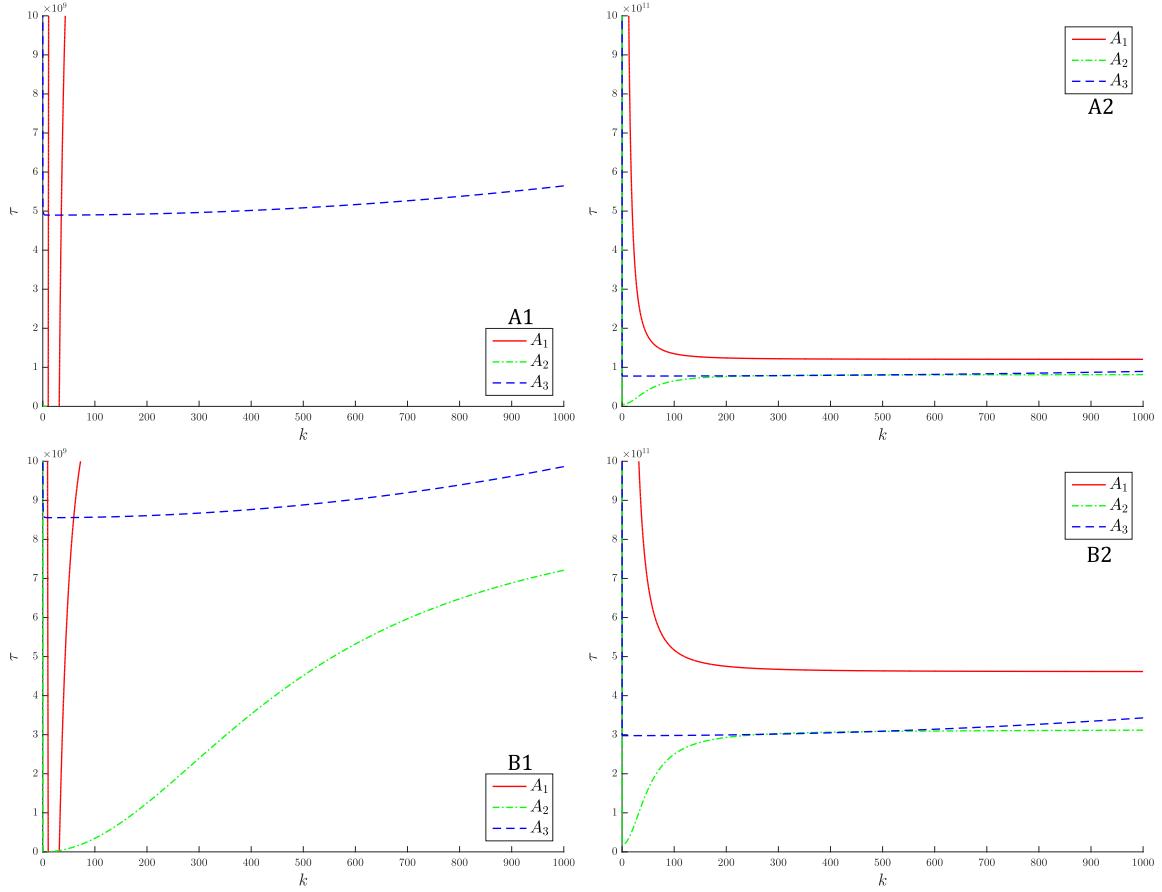


Figure 2.7: Null level set of the characteristic polynomial coefficients $a_i^{(2,3)}$ defined in (2.1) for different null basal rate and coupling term θ . (A1) $\beta_2 = 0$ with $\theta^{(1)}$. (A2) $\beta_3 = 0$ with $\theta^{(1)}$. (B1-B2) Similar analysis for $\theta^{(2)}$. In all plots we use $\rho = 1$.

(e.g., the red null level in Fig. 2.7(A1)). In $\beta_3 = 0$, instabilities can be produced using a large value of τ (see Figs. 2.7(A2), (B2)), implying that coupling the diffusion system to the poromechanics bypasses the intrinsic stability of an uncoupled system.

2.5. General coupled system

In a more general scenario, we look at how the strength of the coupling between the poromechanical and chemical systems modifies the linear stability properties. Figure 2.8 presents, for different values of the coupling parameter γ , the null levels of the dispersion relation coefficients. In order to reduce the complexity of the stability analysis, we fix $\beta_2 = 0.6319$ letting the other parameter values unchanged. This modification forces the coefficient a_0 to be strictly positive, reducing the complex pattern generated by the Routh-Hurwitz conditions (cf. (2.3)-(2.6)). Increasing γ reduces the critical value of τ needed to reach instability (compare with Figs. 2.8(A1), (A2)) without affecting the pattern generated by the null level-set. Additionally, the source terms in the modified Schnackenberg model depend also on β_1 . In order to compare the effectiveness of both parameters in stabilising or destabilising the system, we present in Figure 2.9 the null level-set of the coefficients a_i for different values of β_1 . In that case, we see that the critical value for τ is affected by increasing β_1 (see Fig. (2.9)(A1)-(A3)). Moreover, and contrary to what occurs with γ , it seems to affect significantly the pattern of the null level-sets (especially the one associated with the coefficient a_2) and therefore also the spatial scale where instabilities can occur. Analogous conclusions can be drawn even using a nonlinear

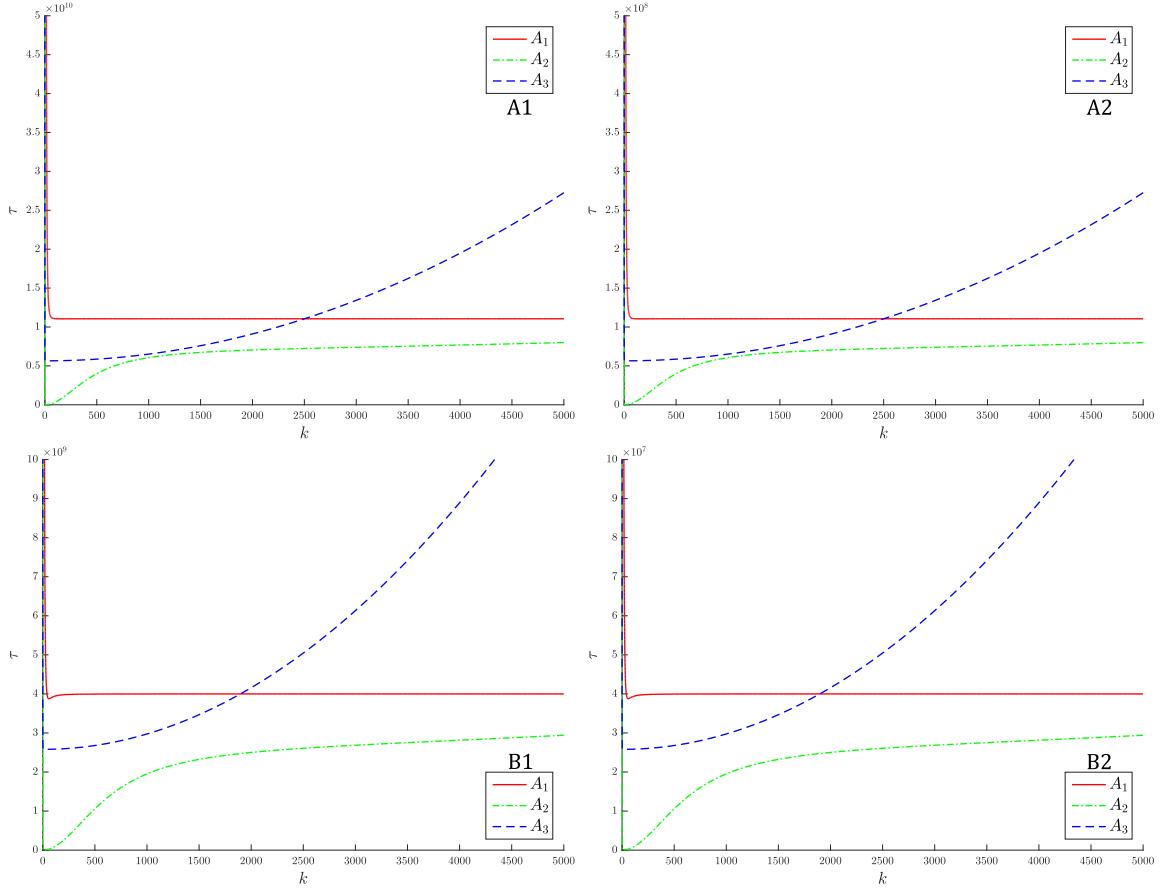


Figure 2.8: Null level set of the characteristic polynomial coefficients a_i with respect to τ defined in (2.1) for the general coupled system and for different coupling term $\boldsymbol{\theta}$. (A1) $\gamma = 10^{-4}$ with $\boldsymbol{\theta}^{(1)}$. (A2) $\gamma = 10^{-2}$ with $\boldsymbol{\theta}^{(1)}$. (B1-B2) Similar analysis for $\boldsymbol{\theta}^{(2)}$. In all plots we use $\rho = 1$, $\beta_2 = 0.6319$.

coupling function $r^{(2)}(\mathbf{w})$. As in the previous scenario, the different coefficients present a large interval where the Routh-Hurwitz conditions are not satisfied. In summary, the coupled system is able to produce non-trivial patterns at very different length scales.

Another way to show pattern generation is through dispersion relations related to the parameter τ , see Figure 2.10. These relations are computed using the implicit functions obtained from the coefficient a_2 when $\rho = 0$, and from condition (2.6), otherwise. The choice was made as they are the first coefficients to break the Routh-Hurwitz conditions with respect to τ in the explored space scale. We observe that if acceleration is present, a relatively small value of τ is sufficient (at a very low space scale) to induce instability, as seen in Figure 2.10(A1) (or (B1)). When $\rho = 0$, the system can still reach instability but it needs a larger value of τ , which shows again the effect of inertia on the system stability. Comparing Figures 2.10(A1)-(A2) with 2.10(B1)-(B2) we see that, for the selected parameters, the choice of the coupling function $\boldsymbol{\theta}$ affects the critical value of τ , but not the pattern of the dispersion relations.

To conclude this section, we analyse the sign of each a_i against the value of β_2 , and compare with the results from the uncoupled system studied above. Figure 2.11 displays the null level set when increasing the coupling strength (realised by augmenting τ and γ simultaneously). From Figures 2.11(A1) to 2.11(A3), we observe that a_2 is particularly affected by the choice of these two parameters. First, reducing the region of instability (see Fig. 2.11(A2)) we obtain, in a strongly coupled system, two instability regions delimited by

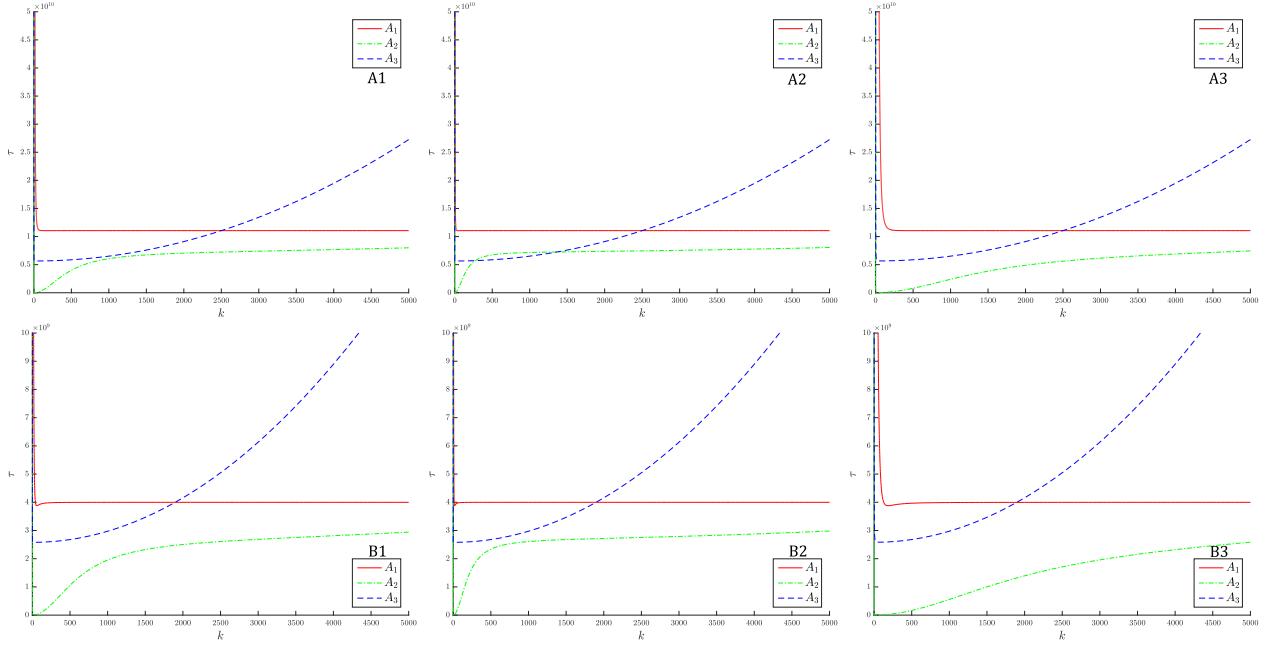


Figure 2.9: Null level set of the characteristic polynomial coefficients a_i with respect to τ defined in (2.1) for the general coupled system and for different coupling term θ . (A1) $\beta_1 = 170$ with $\theta^{(1)}$. (A2) $\beta_1 = 17$ with $\theta^{(1)}$. (A3) $\beta_1 = 1700$ with $\theta^{(1)}$. (B1-B3) Similar analysis for $\theta^{(2)}$. In all plots we use $\rho = 1$ and $\gamma = 10^{-4}$.

the red (a_0) and green (a_2) level sets that overlap with respect to the wave number k , but not with respect to β_2 . Consequently, and depending on the strength of the coupling between reaction-diffusion and poroelastic effects, we can discriminate different values of β_2 that will produce distinct patterns at desired specific scales. This is more clearly seen for the case with $\theta = \theta^{(2)}$, where the interval of β_2 that leads to instability increases rapidly with the augmentation of τ and γ , and tends to finally overlap with the region delimited by a_0 (see red level in Fig. 2.11(B3)).

3. Numerical method and implementation

In [17] we propose a discretisation in space using a mixed finite element method. In its lowest-order form, the method consists of piecewise bilinear elements enriched with bubbles for the displacements (cubic for triangles, and quartic for tetrahedra), piecewise linear and continuous approximations for the fluid pressure and for the chemical solutes; and piecewise constant approximation for total pressure. For sake of completeness we outline here the spatio-temporal method.

The time discretisation is achieved by a backward Euler scheme and an implicit centred difference method for the first and second order time derivatives, respectively. Denoting

$$\delta_t X^{n+1} := \frac{X^{n+1} - X^n}{\Delta t}, \quad \delta_{tt} X^{n+1} := \frac{X^{n+1} - 2X^n + X^{n-1}}{\Delta t^2},$$

the fully discrete method reads: From initial data $\mathbf{u}_h^{s,0}, p_h^{f,0}, \psi_h^0, w_{1,h}^0, w_{2,h}^0$ (which will be projections of the continuous initial conditions of each field) and for $n = 1, \dots$, find $\mathbf{u}_h^{s,n+1} \in \mathbf{V}_h, p_h^{f,n+1} \in Q_h, \psi_h^{n+1} \in Z_h, w_{1,h}^{n+1} \in W_h, w_{2,h}^{n+1} \in W_h$ such that

$$\tilde{a}_1(\mathbf{u}_h^{s,n+1}, \mathbf{v}_h^s) + a_1(\mathbf{u}_h^{s,n+1}, \mathbf{v}_h^s) + b_1(\mathbf{v}_h^s, \psi_h^{n+1}) = F_{r_h^{n+1}}(\mathbf{v}_h^s) \quad \forall \mathbf{v}_h^s \in \mathbf{V}_h, \quad (3.1)$$

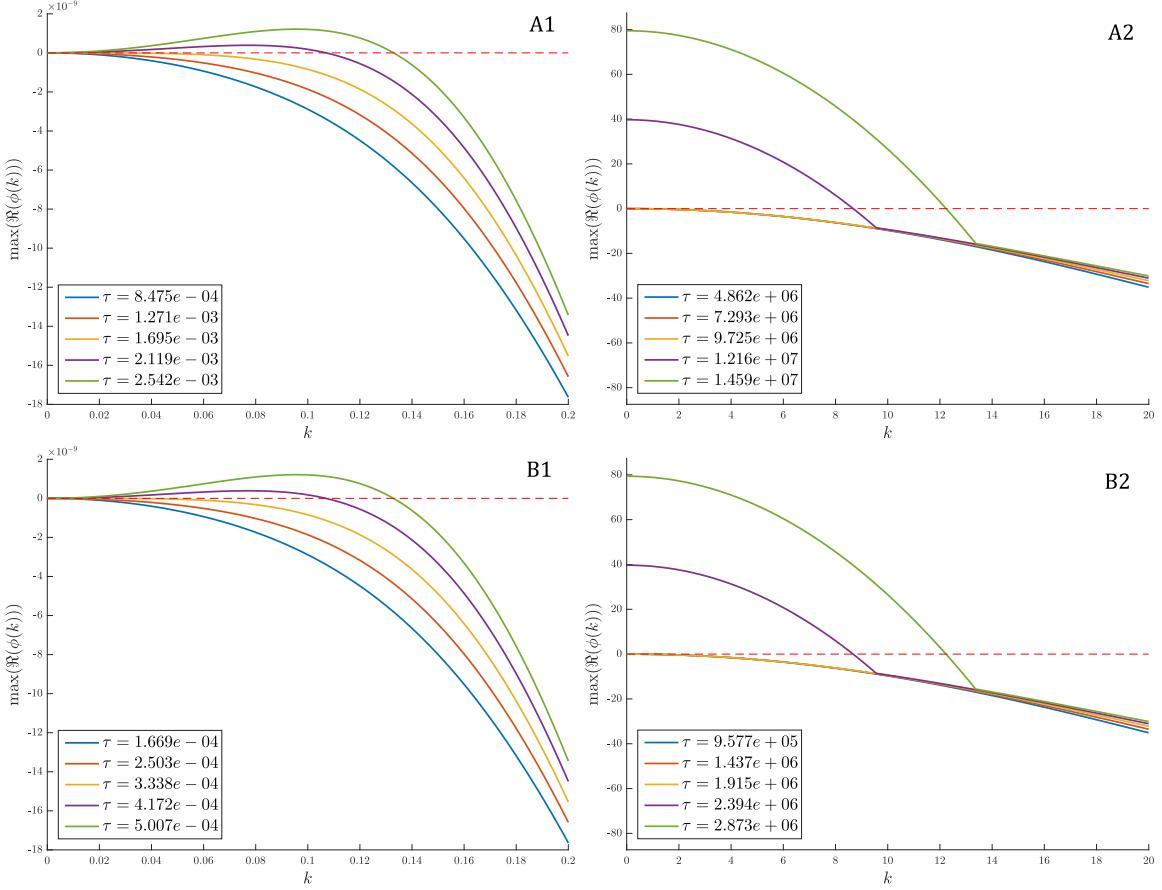


Figure 2.10: Dispersion relations for the general coupled poromechanical-chemical model for different coupling terms $\boldsymbol{\theta}$. (A1) Dispersion relation associated to $\rho = 1$ with $\boldsymbol{\theta}^{(1)}$. (A2) Dispersion relation associated to $\rho = 0$ with $\boldsymbol{\theta}^{(1)}$. (B1-B2) Similar analysis with $\boldsymbol{\theta}^{(2)}$. In all plots, curves are drawn from the critical value τ_c (yellow) and for 25% and 50% increase/decrease of the parameter values, additionally we use $\beta_2 = 0.6319$ and $\gamma = 10^{-4}$.

$$\tilde{a}_2(p_h^{f,n+1}, q_h^f) + a_2(p_h^{f,n+1}, q_h^f) - b_2(q_h^f, \delta_t \psi_h^{n+1}) = G_{\ell^{n+1}}(q_h^f) \quad \forall q_h^f \in Q_h, \quad (3.2)$$

$$b_1(\mathbf{u}_h^{s,n+1}, \phi_h) + b_2(p_h^{f,n+1}, \phi_h) - a_3(\psi_h^{n+1}, \phi_h) = 0 \quad \forall \phi_h \in Z_h, \quad (3.3)$$

$$\tilde{a}_4(w_{1,h}^{n+1}, s_{1,h}) + a_4(w_{1,h}^{n+1}, s_{1,h}) = J_{f_h^{n+1}}(s_{1,h}) \quad \forall s_{1,h} \in W_h, \quad (3.4)$$

$$\tilde{a}_5(w_{2,h}^{n+1}, s_{2,h}) + a_5(w_{2,h}^{n+1}, s_{2,h}) = J_{g_h^{n+1}}(s_{2,h}) \quad \forall s_{2,h} \in W_h, \quad (3.5)$$

with the bilinear forms and linear functionals defined as

$$\begin{aligned} \tilde{a}_1(\mathbf{u}_h^{s,n+1}, \mathbf{v}_h^s) &:= \int_{\Omega} \delta_{tt} \mathbf{u}_h^{s,n+1} \cdot \mathbf{v}_h, \quad a_1(\mathbf{u}^{s,n+1}, \mathbf{v}^s) := 2\mu \int_{\Omega} \boldsymbol{\varepsilon}(\mathbf{u}_h^{s,n+1}) : \boldsymbol{\varepsilon}(\mathbf{v}_h^s), \\ b_1(\mathbf{v}_h^s, \phi_h) &:= - \int_{\Omega} \phi_h \operatorname{div} \mathbf{v}_h^s, \quad b_2(p_h^{f,n+1}, \phi_h) := \frac{\alpha}{\lambda} \int_{\Omega} p_h^{f,n+1} \phi_h, \quad a_3(\psi_h^{n+1}, \phi_h) := \frac{1}{\lambda} \int_{\Omega} \psi_h^{n+1} \phi_h, \\ \tilde{a}_2(p_h^{f,n+1}, q_h^f) &:= \left(c_0 + \frac{\alpha^2}{\lambda} \right) \int_{\Omega} \delta_t p_h^{f,n+1} q_h^f, \quad a_2(p_h^{f,n+1}, q_h^f) := \frac{1}{\eta} \int_{\Omega} \kappa \nabla p_h^{f,n+1} \cdot \nabla q_h^f, \\ \tilde{a}_4(w_{1,h}^{n+1}, s_1) &:= \delta_t \int_{\Omega} w_{1,h}^{n+1} s_1, \quad a_4(w_{1,h}^{n+1}, s_1) := \int_{\Omega} D_1(\mathbf{x}) \nabla w_{1,h}^{n+1} \cdot \nabla s_1, \end{aligned} \quad (3.6)$$

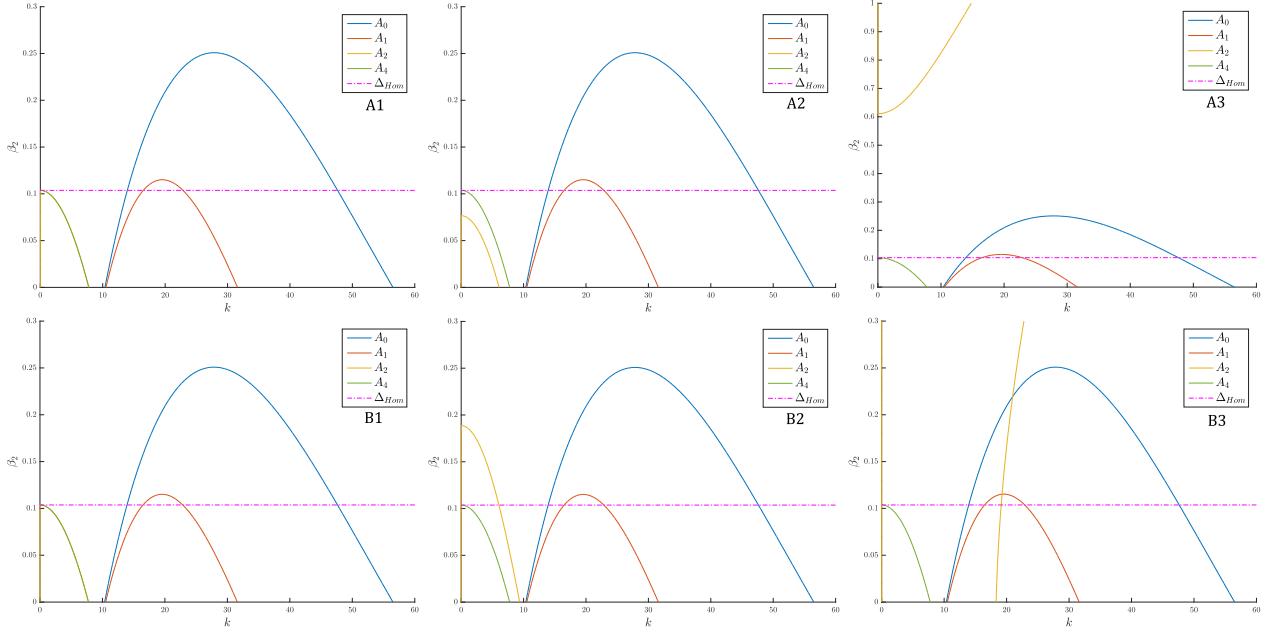


Figure 2.11: Null level set of the characteristic polynomial coefficients a_i with respect to β_2 defined in (2.1) for the general coupled system and for different coupling term $\boldsymbol{\theta}$. (A1) $\tau = 100, \gamma = 10^{-4}$, with $\boldsymbol{\theta}^{(1)}$. (A2) $\tau = 10^4, \gamma = 10^{-2}$ with $\boldsymbol{\theta}^{(1)}$. (A3) $\tau = 10^5, \gamma = 10^{-2}$ with $\boldsymbol{\theta}^{(1)}$. (B1-B3) Similar analysis with $\boldsymbol{\theta}^{(2)}$. In all plots we use $\rho = 1$.

$$\begin{aligned} \tilde{a}_5(w_{2,h}^{n+1}, s_{2,h}) &:= \delta_t \int_{\Omega} w_{2,h}^{n+1} s_{2,h}, \quad a_5(w_{2,h}^{n+1}, s_{2,h}) := \int_{\Omega} D_2(\mathbf{x}) \nabla w_{2,h}^{n+1} \cdot \nabla s_{2,h}, \\ F_{r_h^{n+1}}(\mathbf{v}_h^s) &:= \rho \int_{\Omega} \mathbf{b}^{n+1} \cdot \mathbf{v}_h^s + \tau \int_{\Omega} r_h^{n+1} \mathbf{k} \otimes \mathbf{k} : \boldsymbol{\varepsilon}(\mathbf{v}_h^s), \\ G_{\ell^{n+1}}(q_h^f) &:= \int_{\Omega} \ell^{n+1} q_h^f, \quad J_{f^{n+1}}(s_{1,h}) := \int_{\Omega} f^{n+1} s_{1,h}, \quad J_{g^{n+1}}(s_{2,h}) := \int_{\Omega} g^{n+1} s_{2,h}, \end{aligned}$$

and where for the treatment of the convection-diffusion-reaction problem, we have proceeded as in [23]. The only nonlinearities reside in the terms $F_{r_h^{n+1}}(\mathbf{v}_h^s)$, $J_{f^{n+1}}(s_{1,h})$, and $J_{g^{n+1}}(s_{2,h})$.

With the aim to rewrite the Galerkin scheme (3.1)-(3.5) as a matrix equation, we write the unknowns $\mathbf{u}_h^s, \psi_h, p_h, w_{1,h}$ and $w_{2,h}$ in terms of their basis functions:

$$\mathbf{u}_h^s = \sum_{j=1}^{N_1} U_j \varphi_j, \quad \psi_h = \sum_{j=1}^{N_2} \Phi_j \widehat{\varphi}_j, \quad p_h = \sum_{j=1}^{N_3} P_j \widetilde{\varphi}_j, \quad w_{1,h} = \sum_{j=1}^{N_4} W_{1,j} \overline{\varphi}_j, \quad w_{2,h} = \sum_{j=1}^{N_4} W_{2,j} \overline{\varphi}_j,$$

and substituting back into (3.1)-(3.5) we obtain

$$\begin{aligned} \sum_{j=1}^{N_1} (\varphi_j, \varphi_i) U_j^{n+1} + \Delta t^2 \sum_{j=1}^{N_1} a_1(\varphi_j, \varphi_i) U_j^{n+1} + \Delta t^2 \sum_{j=1}^{N_2} b_1(\varphi_i, \widehat{\varphi}_j) \Phi_j^{n+1} &= \Delta t^2 \sum_{j=1}^{N_1} F_{r_h^{n+1}}(\varphi_i) \\ + \sum_{j=1}^{N_1} (\varphi_j, \varphi_i) U_j^n - \sum_{j=1}^{N_1} (\varphi_j, \varphi_i) U_j^{n-1} &\quad i = 1, \dots, N_1, \\ \left(c_0 + \frac{\alpha^2}{\lambda} \right) \sum_{j=1}^{N_3} (\widetilde{\varphi}_j, \widetilde{\varphi}_i) P_j^{n+1} + \Delta t \sum_{j=1}^{N_3} a_2(\widetilde{\varphi}_j, \widetilde{\varphi}_i) P_j^{n+1} - \sum_{j=1}^{N_2} b_2(\widetilde{\varphi}_i, \widehat{\varphi}_j) \Phi_j^{n+1} &= \Delta t \sum_{j=1}^{N_3} G(\widetilde{\varphi}_i) \end{aligned}$$

$$\begin{aligned}
& + \left(c_0 + \frac{\alpha^2}{\lambda} \right) \sum_{j=1}^{N_3} (\tilde{\varphi}_j, \tilde{\varphi}_i) P_j^n - \sum_{j=1}^{N_2} b_2(\tilde{\varphi}_i, \hat{\varphi}_j) \Phi_j^n \quad i = 1, \dots, N_3, \\
\sum_{j=1}^{N_1} b_1(\varphi_j, \hat{\varphi}_i) U_j^{n+1} + \sum_{j=1}^{N_3} b_2(\tilde{\varphi}_j, \hat{\varphi}_i) P_j^{n+1} - \sum_{j=1}^{N_2} a_3(\hat{\varphi}_j, \hat{\varphi}_i) \Phi_j^{n+1} & = 0 \quad i = 1, \dots, N_2, \\
\sum_{j=1}^{N_4} (\bar{\varphi}_j, \bar{\varphi}_i) W_j^{n+1} - \Delta t \sum_{j=1}^{N_4} a_4(\bar{\varphi}_j, \bar{\varphi}_i) W_j^{n+1} & = \Delta t \sum_{j=1}^{N_4} J_{f_h^{n+1}}(\bar{\varphi}_i) + \sum_{j=1}^{N_4} (\bar{\varphi}_j, \bar{\varphi}_i) W_j^n \quad i = 1, \dots, N_4, \\
\sum_{j=1}^{N_4} (\bar{\varphi}_j, \bar{\varphi}_i) W_j^{n+1} - \Delta t \sum_{j=1}^{N_4} a_5(\bar{\varphi}_j, \bar{\varphi}_i) W_j^{n+1} & = \Delta t \sum_{j=1}^{N_4} J_{g_h^{n+1}}(\bar{\varphi}_i) + \sum_{j=1}^{N_4} (\bar{\varphi}_j, \bar{\varphi}_i) W_j^n \quad i = 1, \dots, N_4.
\end{aligned}$$

Then, we can organise the above system in terms of matrices and vectors:

$$\begin{aligned}
\tilde{A}_1 & \in \mathbf{R}^{N_1 \times N_1}, \quad A_1 \in \mathbf{R}^{N_1 \times N_1}, \quad B_1 \in \mathbf{R}^{N_2 \times N_1}, \quad B_2 \in \mathbf{R}^{N_3 \times N_2}, \quad \tilde{A}_2 \in \mathbf{R}^{N_3 \times N_3}, \quad A_2 \in \mathbf{R}^{N_3 \times N_3}, \\
A_3 & \in \mathbf{R}^{N_2 \times N_2}, \quad \tilde{A}_4 \in \mathbf{R}^{N_4 \times N_4}, \quad A_4 \in \mathbf{R}^{N_4 \times N_4}, \quad \tilde{A}_5 \in \mathbf{R}^{N_4 \times N_4}, \quad A_5 \in \mathbf{R}^{N_4 \times N_4}, \\
F & \in \mathbf{R}^{N_1}, \quad G \in \mathbf{R}^{N_3}, \quad J_1 \in \mathbf{R}^{N_4}, \quad J_2 \in \mathbf{R}^{N_4},
\end{aligned}$$

such that

$$\begin{aligned}
\tilde{a}_{1,ij} & = (\varphi_j, \varphi_i), \quad a_{1,ij} = \Delta t^2 a_1(\varphi_j, \varphi_i) \quad i, j = 1, \dots, N_1, \quad a_{3,ij} = a_3(\hat{\varphi}_j, \hat{\varphi}_i), \quad i, j = 1, \dots, N_2, \\
\tilde{a}_{2,ij} & = \left(c_0 + \frac{\alpha}{\lambda} \right) (\tilde{\varphi}_j, \tilde{\varphi}_i), \quad a_{2,ij} = \Delta t a_2(\tilde{\varphi}_j, \tilde{\varphi}_i) \quad i, j = 1, \dots, N_3, \\
b_{1,ij} & = b_1(\varphi_j, \hat{\varphi}_i) \quad i = 1, \dots, N_2, \quad j = 1, \dots, N_1, \quad b_{2,ij} = b_2(\tilde{\varphi}_i, \hat{\varphi}_i) \quad i = 1, \dots, N_2, \quad j = 1, \dots, N_3, \\
\tilde{a}_{4,ij} & = (\bar{\varphi}_j, \bar{\varphi}_i), \quad a_{4,ij} = \Delta t a_4(\bar{\varphi}_j, \bar{\varphi}_i) \quad i, j = 1, \dots, N_4, \\
\tilde{a}_{5,ij} & = (\bar{\varphi}_j, \bar{\varphi}_i), \quad a_{5,ij} = \Delta t a_5(\bar{\varphi}_j, \bar{\varphi}_i) \quad i, j = 1, \dots, N_4, \quad F_i = \Delta t^2 F_{r^{n+1}}(\varphi_i) \quad i = 1, \dots, N_1, \\
G_i & = \Delta t G(\tilde{\varphi}_i) \quad i = 1, \dots, N_3, \quad J_{1,i} = \Delta t J_{f_h^{n+1}}(\bar{\varphi}_i), \quad J_{2,i} = \Delta t J_{g_h^{n+1}}(\bar{\varphi}_i) \quad i = 1, \dots, N_4,
\end{aligned}$$

and then, denoting

$$\begin{aligned}
\mathbf{A} & := \begin{bmatrix} \tilde{A}_1 + A_1 & \Delta t^2 B_1^\top & \mathbf{O} & F \\ \mathbf{O} & \tilde{A}_2 + A_2 & -B_2^\top & \mathbf{O} \\ B_1 & B_2 & -A_3 & \mathbf{O} \\ \mathbf{O} & \mathbf{O} & \mathbf{O} & \tilde{A}_4 + A_4 + \tilde{A}_5 + A_5 \end{bmatrix}, \quad \mathbf{X} := \begin{bmatrix} U_j \\ P_j \\ \Phi_j \\ (W_{1,j}, W_{2,j}) \end{bmatrix} \\
\mathbf{H} & := \begin{bmatrix} 2\tilde{A}_1 U_j^n - \tilde{A}_1 U_j^{n-1} \\ G + A_2 P_j^n - B_2 \Phi_j^n \\ \mathbf{O} \\ J_1 + \tilde{A}_4 W_{1,j}^n + J_2 + \tilde{A}_5 W_{1,j}^n \end{bmatrix},
\end{aligned}$$

the fully-discrete matrix problem for (3.6) reads

$$\mathbf{A} \mathbf{X}^{n+1} = \mathbf{H}^n,$$

which will be used for the development of the numerical tests.

In addition, a Newton method with exact Jacobian is derived for the solution of (3.1)-(3.5) at each time step. Then, regarding both chemical species in a single vector \mathbf{W} , the tangent algebraic systems to be solved at each Newton step (for a given time step) adopt the following form

$$\hat{A}_{11} \delta \mathbf{U}_{k+1}^s + \hat{B}_{13} \delta \Psi_{k+1} + \hat{F}_1 \delta \mathbf{W}_{k+1} = \mathbf{R}_{1,k},$$

$$\begin{aligned}
& \widehat{A}_{22} \delta \mathbf{P}_{k+1}^f - \widehat{B}_{23} \delta \boldsymbol{\Psi}_{k+1} & = \mathbf{R}_{2,k}, \\
& \widehat{B}_{13}^\top \delta \mathbf{U}_{k+1}^s + \widehat{B}_{32} \delta \mathbf{P}_{k+1}^f - \widehat{A}_{33} \delta \boldsymbol{\Psi}_{k+1} & = \mathbf{R}_{3,k}, \\
& \widehat{C}_{42}^k \delta \mathbf{U}_{k+1}^s & + (\widehat{J}_4 + \widehat{C}_{41}^k + \widehat{A}_{41}) \delta \mathbf{W}_{k+1} = \mathbf{R}_{4,k},
\end{aligned}$$

where $\delta(\cdot)_{k+1}$ represent the vector of nodal values for the incremental unknowns that are premultiplied by the respective elementary matrices constructed with the bilinear forms in (3.6) or their linearisation; that is, the matrix \widehat{F}_1 is induced by the linearisation of $F_{r_h^{n+1}}(\cdot)$, \widehat{A}_{11} by $a_1(\cdot, \cdot) + \tilde{a}_1(\cdot, \cdot)$, \widehat{B}_{13} and \widehat{B}_{13}^\top by $b_1(\cdot, \cdot)$, \widehat{A}_{22} by $a_2(\cdot, \cdot) + \tilde{a}_2(\cdot, \cdot)$, \widehat{B}_{23} by $b_2(\cdot, \delta_t(\cdot))$, \widehat{B}_{32} by $b_2(\cdot, \cdot)$, \widehat{A}_{33} by $a_3(\cdot, \cdot)$, \widehat{J}_4 by the linearisation of $J_{f_h^{n+1}}(\cdot)$ and $J_{g_h^{n+1}}(\cdot)$, \widehat{C}_{41}^k and \widehat{C}_{42}^k by the linearisation of $c(\cdot, \cdot, \cdot)$ (see its definition in [17, eq. (2.7)]), and \widehat{A}_{41} by $\tilde{a}_4(\cdot, \cdot) + a_4(\cdot, \cdot)$ and $\tilde{a}_5(\cdot, \cdot) + a_5(\cdot, \cdot)$. The right-hand side vectors $\mathbf{R}_{i,k}$ account for body forces, mass sources, terms associated with the previous time step, and residuals from the previous Newton iteration k . The system is solved by the GMRES Krylov solver with incomplete LU factorisation (ILUT) preconditioning. The stopping criterion on the nonlinear iterations is based on a weighted residual norm dropping below the fixed tolerance of $1 \cdot 10^{-6}$.

4. Numerical tests

4.1. Test 1: Periodic traction preventing stable patterning

In order to investigate the impact that the structural deformation has on the emerging spatial patterns of solutes, we first consider the spatial domain $\Omega = (0, 1) \times (0, 0.6)$, where the clamped boundary is $\Gamma = \{\mathbf{x} : x_1 = 0, x_1 = 1, x_2 = 0\}$ and the top face constitutes Σ where we apply a periodic traction defined by

$$\mathbf{t} = \begin{cases} (0, -s_0 \sin(\pi t))^\top & \text{if } 0.4 \leq x_1 \leq 0.6, \\ \mathbf{0} & \text{otherwise,} \end{cases}$$

with $s_0 = 25000$ (similarly as in the footing problem from, e.g., [18]). A schematic description of the domain can be seen in Figure 4.1 (top). According to (1.10)-(1.11), on Γ we also impose zero fluid pressure fluxes, whereas on Σ we set a uniform fluid pressure $p^f = 0$. The parameters that are modified with respect to Test 2 are only the coupling constants of active stress modulation $\tau = 100$ (using again $r = w_1 + w_2$), the direction $\mathbf{k} = (1, 0)^\top$, the density $\rho = 1$, and the volume-dependent source $\gamma = 0.05$. The resulting patterns (exemplified by transients of the activator chemical w_1 and final states of poromechanical variables) are depicted in Figure 4.1. One can readily observe that, apart from altering substantially the distribution of chemical concentrations from the beginning of the simulation, the periodic traction applied on part of the top edge (and which only produces less than a 10% of vertical stretch) prevents the system from reaching a state with stable spatial patterns. For this test we have used a uniform mesh (top panel of Figure 4.1).

4.2. Test 2: Small poromechanical effects

Next we take the domain as the disk centred at $(0.5, 0.5)$ with radius 0.5, and assume that the boundary coincides with Γ . Then the displacements are set to zero on the whole boundary and we take relatively small values for the coupling constants on the chemical source and on the active stress $\gamma = 0.0001$, $\tau = 100$, implying in particular that the patterns produced by the coupled poroelastic-convection-diffusion-reaction system are expected to be qualitatively similar to those observed on a fixed domain. In (1.8) we assume a dependence of the form $r = w_1 + w_2$, and the remaining model constants are taken as $D_1 = 0.05$, $D_2 = 1$, $\beta_1 = 170$, $\beta_2 = 0.1305$, $\beta_3 = 0.7695$, $E = 3 \cdot 10^4$, $\nu = 0.495$, $\rho = 1$, $c_0 = 1 \cdot 10^{-3}$, $\kappa = 1 \cdot 10^{-4}$, $\alpha = 0.1$, $\eta = 1$, $\mathbf{k} = (x_1 - 0.5, x_2 - 0.5)^\top$. The initial condition for the chemicals is a perturbation of the homogeneous steady state $w_1^0 = \beta_2 + \beta_3$, $w_2^0 = \beta_3(\beta_2 + \beta_3)^{-2}$ and for the displacements and fluid pressure we use zero initial conditions. The domain is discretised into an unstructured mesh of 64926 triangles and we employ a fixed time-step $\Delta t = 0.0025$. The system is advanced until $t_{\text{final}} = 1.5$ and plots with patterns of w_2 , small

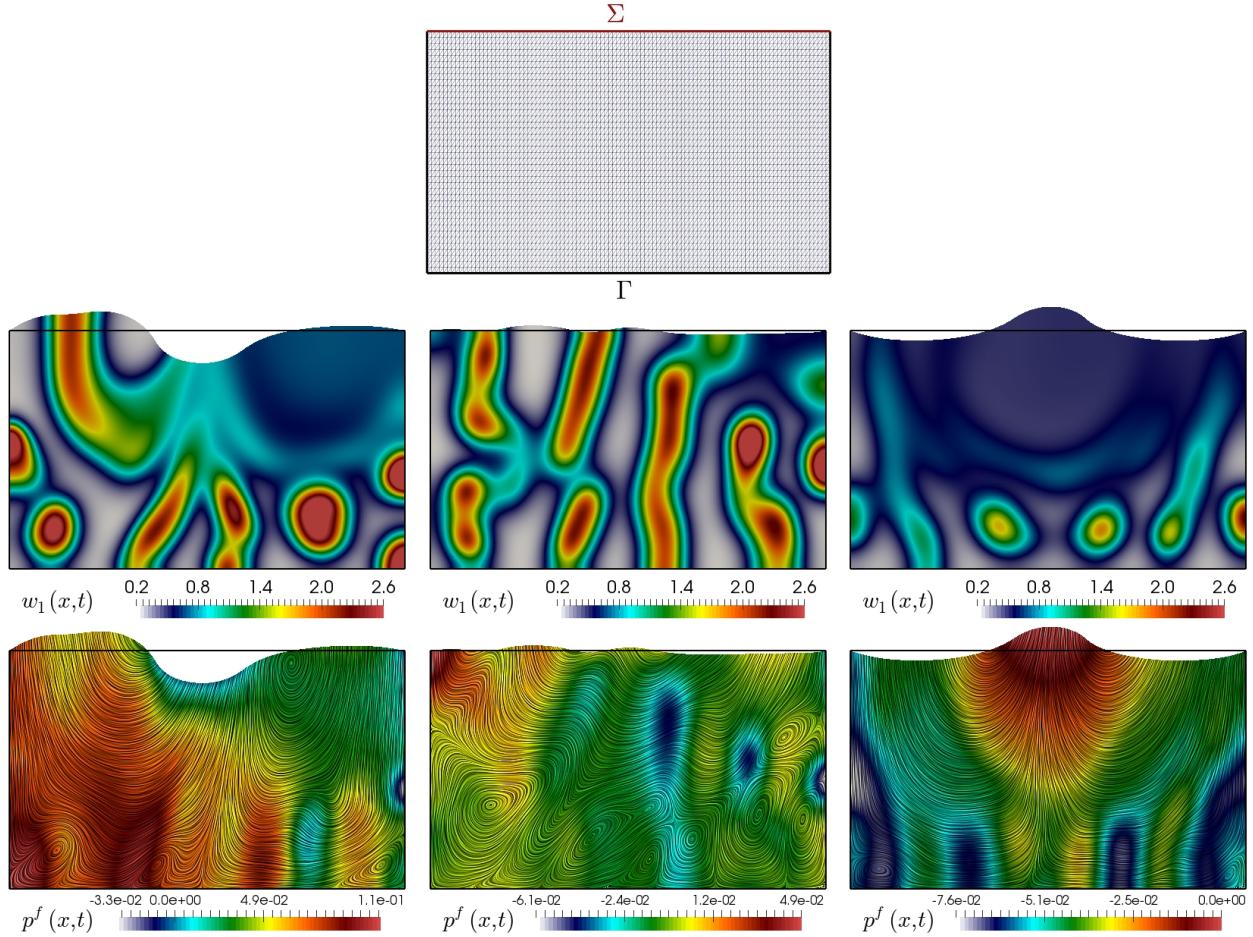


Figure 4.1: Test 1. Sketched mesh and domain before deformation (top) and sample of concentrations of w_1 (middle) and fluid pressure (bottom) at times $t = 0.5, 1, 1.75$ and plotted on the deformed domain according to the solid displacements.

deformations, as well as fluid and total pressures are shown in Figure 4.2. In the bottom row we can see how the initial perturbation of the steady state evolves into organised dot-shaped spatial structures, seen clearly for the inhibitor chemical w_2 and also captured by the total pressure. No deformation occurs along the domain boundary, but the local deformation patterns show also tissue contraction near the zones of high concentration of the activator species w_1 .

4.3. Test 3: Linear growth and active stress

Maintaining the same domain and discretisation parameters as in Test 2 above, we now fix the mechanochemical coupling constant $\gamma = 0.01$ and study the competing effect between linear growth with radial traction, and the active stress depending on the concentration of the activator species w_1 . This is done with an activation of the type $r = \tau_2 t + w_1^2$, and for this 2D case we consider Robin boundary conditions for the solid motion (1.9) with $\zeta = t\tau_2$, on the circular boundary (whereas for the 3D case below we impose zero normal displacement on the bottom of the cylinder and a traction $\mathbf{t} = \tau_2 t \mathbf{n}$ on the remainder of the boundary). We set \mathbf{k} to be the radial vector, and vary τ, τ_2 . The results are shown in Figure 4.3. From left to right we display snapshots of the chemical patterns produced with the parameter choices $(\tau = 2 \cdot 10^5, \tau_2 = 0.2)$, $(\tau = 10^5, \tau_2 = 2)$, $(\tau = 10^4, \tau_2 = 10)$, and $(\tau = 100, \tau_2 = 20)$.

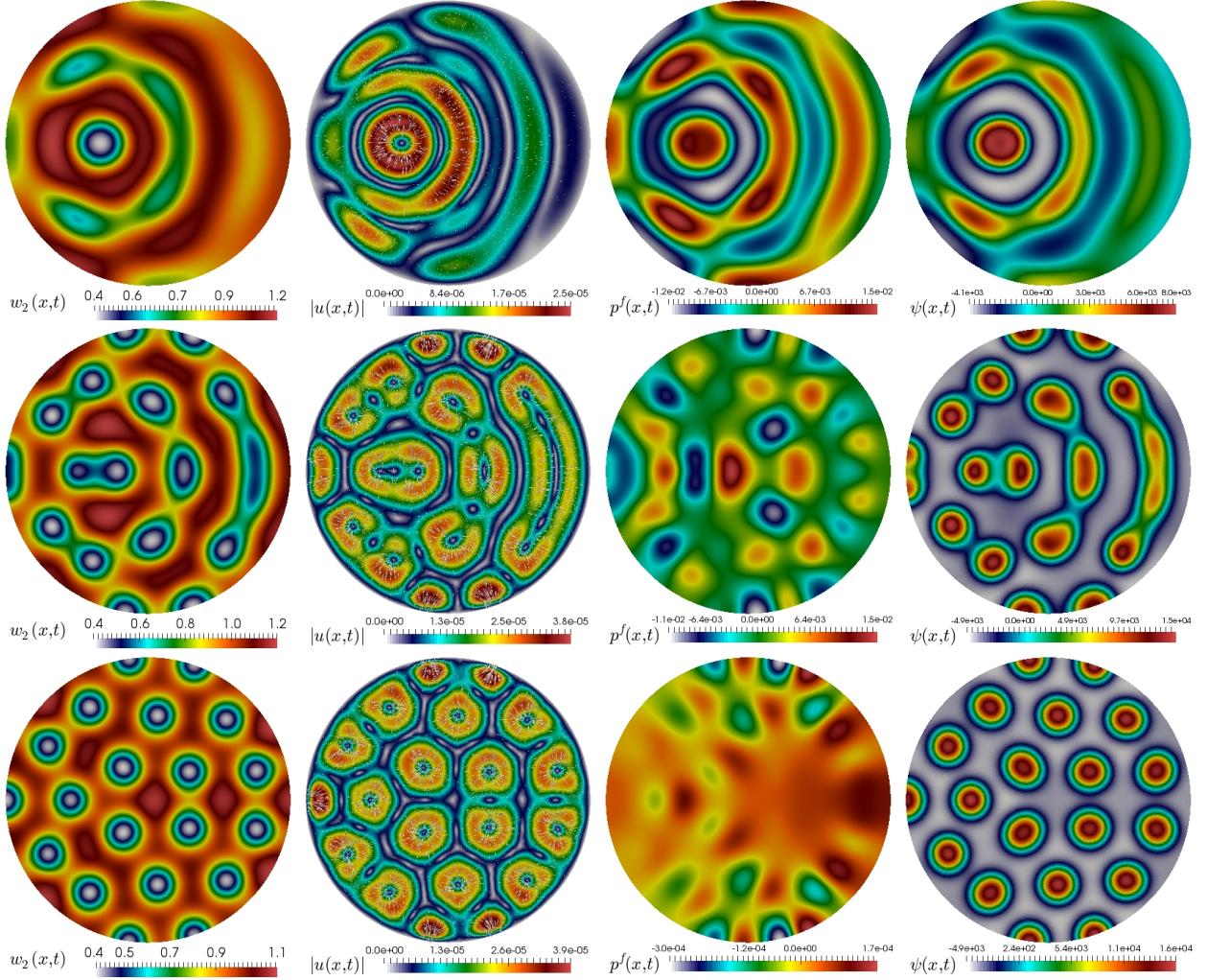


Figure 4.2: Test 2. Patterns generated with relatively small chemo-mechanical feedback $\gamma = 0.0001$ and clamped boundary conditions, plotted on the undeformed domain at times $t = 0.25$ (top), $t = 0.375$ (middle row), and $t = 1.5$ (bottom panels). From left to right: w_2 concentration, solid displacement magnitude, fluid pressure, and total pressure.

4.4. Test 4: Linear growth in 3D

We extend the previous test to assess the behaviour of the model and the finite element scheme in a 3D setting. We modify (1.8) to include axial symmetry on another preferential direction for active deformation. The domain is a cylinder of height 0.05 and radius 0.5 (see top panel of Figure 4.4 showing the different boundaries of the geometry and the generated volumetric mesh), and we set

$$\boldsymbol{\sigma}_{\text{act}} = -\tau [\tau_2 t \mathbf{k}_{12} \otimes \mathbf{k}_{12} + w_1^2 \mathbf{k}_3 \otimes \mathbf{k}_3],$$

where \mathbf{k}_{12} is the radial vector in the plane $x_1 x_2$ and $\mathbf{k}_3 = (0, 0, 1)^T$. This implies that the active deformation due to linear growth will occur in the radial direction whereas the stress due to the chemical concentration will act on the x_3 -direction. On the bottom surface (denoted Σ) we set zero normal displacements $\mathbf{u} \cdot \mathbf{n} = 0$, while on the remainder of the boundary, which is denoted by Γ , we impose zero traction. In Figure 4.4 we show the resulting patterns of w_1 concentration for two sets of Lamé and poromechanical-chemical coupling parameters. For the first case we use $E = 1 \cdot 10^4$, $\nu = 0.499$, and $\tau = 10$, $\tau_2 = 20$, $\gamma = 0.05$ and show the

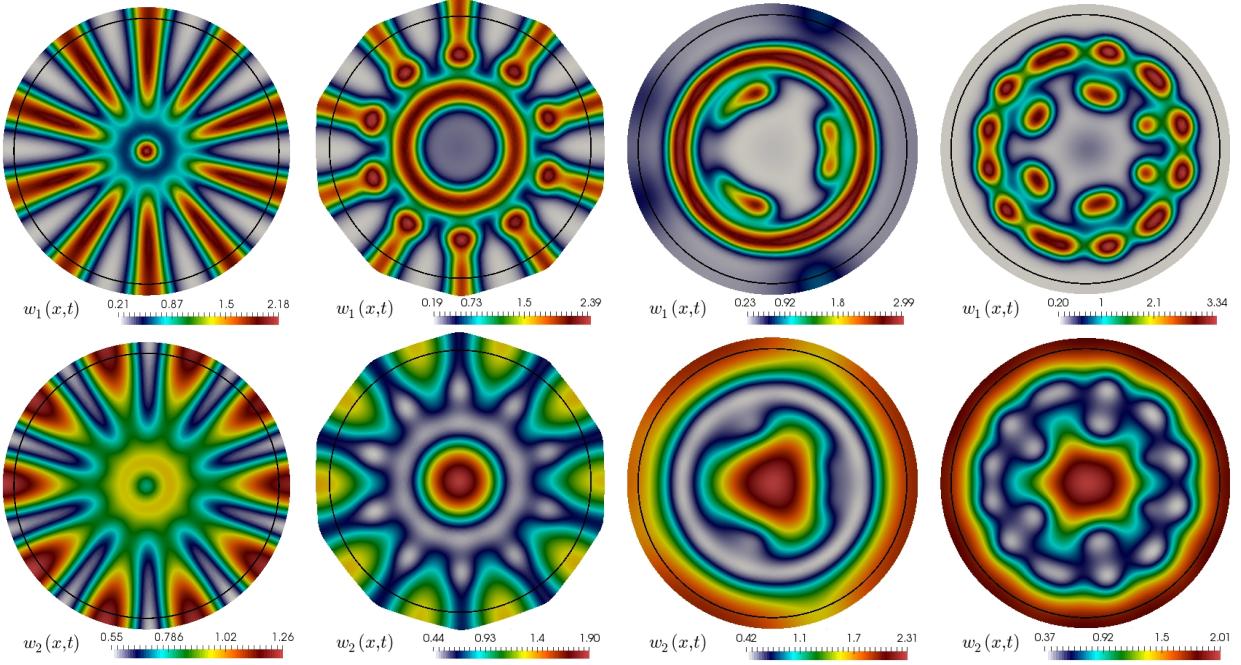


Figure 4.3: Test 3. Interplay between linear growth and active stress. Concentrations of w_1 and w_2 (top and bottom) on the deformed domain, at time $t = 1.25$, for different mild values of the coupling constants τ, τ_2 . The black circle in all plots represents the boundary of the initial domain.

patterns on the deformed domain in the left panels; while the plots on the right panels were produced with $E = 1 \cdot 10^3$, $\nu = 0.3$, and $\tau = 50$, $\tau_2 = 60$, $\gamma = 0.1$. We observe stable pattern generation with the first set of model parameters, similar to the expected patterning in the case of pure reaction-diffusion effects, whereas the patterns on the right exhibit large qualitative differences in w_1 (also in the other species) as well as in the deformation behaviour.

4.5. Test 5: Application to the simulation of brain injuries and calcium propagation

We close this section with an example related to the one-way coupling between poroelastic deformations in the brain (induced by a localised high stress) and the subsequent propagation and reaction of two types of calcium concentration, intracellular and extracellular, throughout the tissue. This illustrative test is based on the kinetic and 1D models recently advanced in [24]. In there, the authors propose that hydrostatic stress build up due to the brain trauma affect (in an exponentially decreasing manner) the reacting fluxes between the calcium concentrations. We do not include acceleration but we propose to incorporate this in the coupled model using a modification of (1.5)-(1.6) to include a dependence of the reaction terms on the total pressure

$$f(w_1, w_2, \psi) = -D_1(w_1 - w_2) + \frac{1}{\chi_1} \left[-\chi_1 + (1 + \chi_1) \exp(-k|\psi|) \right] \frac{w_2^2}{w_2^2 + k_1^2},$$

$$g(w_1, w_2, \psi) = -f(w_1, w_2, \psi) + D_2(w_0 - w_2) - \frac{1}{\chi_2} \left[-\chi_2 + (1 + \chi_2) \exp(-k|\psi|) \right] \frac{w_2}{w_2 + k_2},$$

where w_1, w_2 represent respectively, the extracellular and intracellular calcium concentrations (in [mM] units) and the model parameters are as in [24]

$$D_1 = 2.94 \cdot 10^{-6} \text{ [1/s]}, \quad D_2 = 3.17 \cdot 10^{-5} \text{ [1/s]}, \quad k_1 = 2 \cdot 10^{-4} \text{ [mM]}, \quad k_2 = 5 \cdot 10^{-4} \text{ [mM]},$$

$$\chi_1 = 2 \cdot 10^3, \quad \chi_2 = 4 \cdot 10^3, \quad k = 4.5 \cdot 10^{-5} \text{ [Pa}^{-1}\text{]}, \quad w_0 = 0.1 \text{ [mM]}.$$

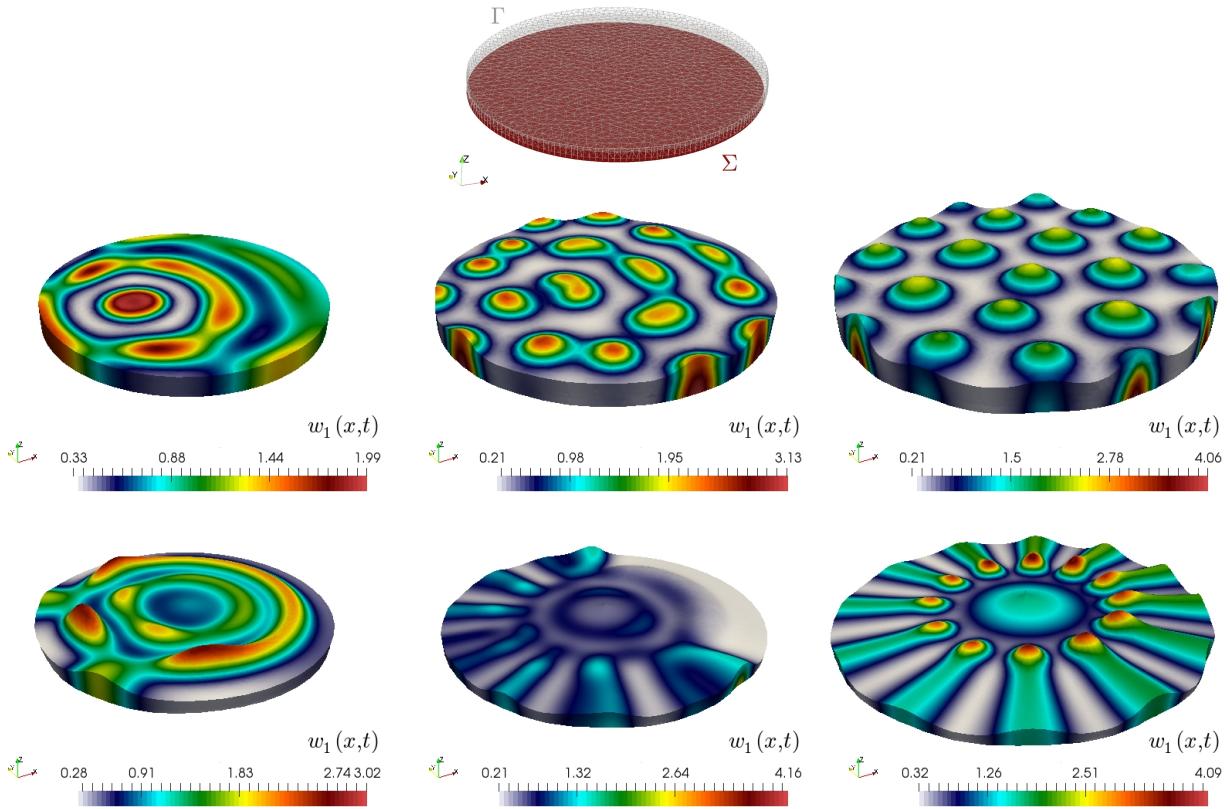


Figure 4.4: Test 4. Sample coarse mesh and domain/boundary configuration (top), and interplay between linear growth and active stress for two sets of elasticity and coupling parameters (middle and bottom). Concentrations of w_1 on the deformed domain, at times $t = 0.25, 0.5, 1.25$ (left, centre, and right panels, respectively).

On the other hand, the fact that calcium activity effects are negligible in producing deformations of the poroelastic structure (at least, when compared to high stress impacts on the skull or with important kinematic forces building up because of rapid shocks) implies that in the proposed model the total stress (1.7) does not contain an active component modulated by w_1, w_2 . Also, the present model is different than the one in [24] in that we do not consider viscoelastic effects but do include poroelasticity of the brain, and we also include diffusion of the calcium concentrations. The remaining constants in the model and the initial conditions adopt the values

$$E = 3.15 \cdot 10^4 \text{ [Pa]}, \quad \nu = 0.45, \quad \rho = 1130 \text{ [Kg/m}^3\text{]}, \quad \frac{\kappa}{\eta} = 10^{-5} \text{ [mm}^2\text{Pa}^{-1}\text{s}^{-1}\text{]}, \quad \alpha = 0.1, \\ c_0 = 3.9 \cdot 10^{-4} \text{ [Pa}^{-1}\text{]}, \quad \mathbf{u}^s(0) = \mathbf{0}, \quad p^f = 0, \quad \psi(0) = 0, \quad w_{1,0} = 1 \text{ [mM]}, \quad w_{2,0} = 10^{-4} \text{ [mM]}.$$

The spatial domain consists of a 3D structure of the human brain and the boundaries are split between ventricles and the outer meningeal region of the brain, in contact with the skull. The interstitial flow in this case is by cerebrospinal fluid. The domain consists of an adult human brain atlas [25] and we use a tetrahedral mesh with 29037 vertices. An initial traction of magnitude $1.7 \cdot 10^4$ [Pa] is applied for 5.5 [ms] on a location near the ventricles and on the skull we impose zero normal displacements and zero fluid pressure, whereas on the ventricles we assume zero fluid pressure flux. We employ a timestep of $\Delta t = 0.1$ [ms] and run the simulation until $t = 180$ [s]. Transients of the intracellular calcium concentration as well as the total pressure are recorded on two points (one near the ventricles, point A, and another near the meninges, point B), and are displayed in Figure 4.5. One can observe an initial peak of several folds the initial homeostatic value of the intracellular calcium followed by a slowly decaying profile (which however does not go back to the homeostatic value).

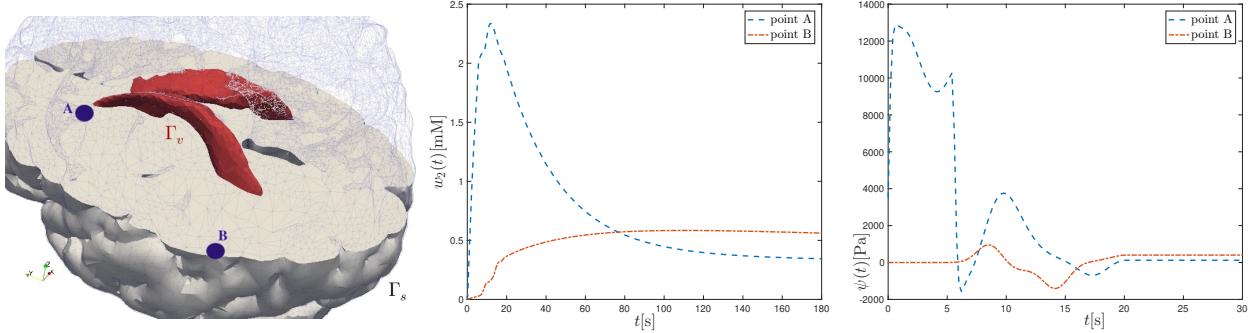


Figure 4.5: Test 5. Cut of the human brain geometry and tetrahedral mesh, showing boundaries on the ventricles Γ_v and near the skull Γ_s , also indicating points A and B where we record quantities of interest (left panel). Time evolution of intracellular calcium concentration and of total pressure (centre and right plots).

We also see that the oscillations in total pressure due to the application of high stresses decrease over time. All this is qualitatively consistent with the model predictions from [24].

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References

- [1] A. E. Ehret, K. Bircher, A. Stracuzzi, V. Marina, M. Zündel, and E. Mazza. Inverse poroelasticity as a fundamental mechanism in biomechanics and mechanobiology. *Nature Comm.*, 10:e1002, 2017.
- [2] R. F. Reis, R. Weber Dos Santos, B. M. Rocha, and M. Lobosco. On the mathematical modeling of inflammatory edema formation. *Comput. Math. Appl.*, 78(9):2994–3006, 2019.
- [3] K. H. Støverud, M. Alnæs, H. P. Langtangen, V. Haughton, and K.-A. Mardal. Poro-elastic modeling of syringomyelia – a systematic study of the effects of pia mater, central canal, median fissure, white and gray matter on pressure wave propagation and fluid movement within the cervical spinal cord. *Comput. Methods Biomed. Engrg.*, 19(6):686–698, 2016.
- [4] R. T. Mauck, C. T. Hung, and G. A. Ateshian. Modelling of neutral solute transport in a dynamically loaded porous permeable gel: implications for articular cartilage biosynthesis and tissue engineering. *J. Biomech. Engrg.*, 125:602–614, 2003.
- [5] V. M. Calo, N. F. Brasher, Y. Bazilevs, and T. J. R. Hughes. Multiphysics model for blood flow and drug transport with application to patient-specific coronary artery flow. *Comp. Mech.*, 43(1):161–177, 2008.
- [6] R. Sacco, P. Causin, C. Lelli, and M. T. Raimondi. A poroelastic mixture model of mechanobiological processes in biomass growth: theory and application to tissue engineering. *Meccanica*, 52(14):3273–3297, 2017.
- [7] E. Moeendarbary, L. Valon, M. Fritzsche, A. R. Harris, D. A. Mouling, A. J. Thrasher, E. Stride, L. Mahadevan, and G. T. Charras. The cytoplasm of living cells behaves as a poroelastic material. *Nature Materials*, 12:3517, 2013.
- [8] P. Royer and F. Cherblanc. Homogenisation of advective-diffusive transport in poroelastic media. *Mech. Res. Commun.*, 37(2):133–136, 2010.

- [9] M. Radszuweit, H. Engel, and M. Bär. An active poroelastic model for mechanochemical patterns in protoplasmic droplets of *physarum polycephalum*. *PLOS ONE*, 9(6):e99220, 2014.
- [10] J. Collis, D. L. Brown, M. E. Hubbard, and R. D. O'Dea. Effective equations governing an active poroelastic medium. *Proc. R. Soc. A*, 473(2198):20160755, 2017.
- [11] P. Moreo, E. A. Gaffney, J. M. García-Aznar, and M. Doblaré. On the modelling of biological patterns with mechanochemical models: Insights from analysis and computation. *Bull. Math. Biol.*, 72(2):400–431, 2010.
- [12] A. J. Catllá, A. McNamara, and C. M. Topaz. Instabilities and patterns in coupled reaction-diffusion layers. *Phys. Rev. E.*, 85(2):026215, 2012.
- [13] A. Goriely and R. Vandiver. On the mechanical stability of growing arteries. *IMA J. App. Math.*, 75(4):549–570, 2010.
- [14] A. A. Neville, P. C. Matthews, and H. M. Byrne. Interactions between pattern formation and domain growth. *Bull. Math. Biol.*, 68(8):1975–2003, 2006.
- [15] M. Pourjafar and K. Sadeghy. Pressure-driven flows of Quemada fluids in a channel lined with a poroelastic layer: A linear stability analysis. *J. Non-Newt. F. Mech.*, 242:23–47, 2017.
- [16] P. Recho, A. Hallou, and E. Hannezo. Theory of mechano-chemical patterning in biphasic biological tissues. *PNAS.*, 116(12):5344–5349, 2019.
- [17] N. Verma, B. Gómez-Vargas, L. M. De Oliveira Vilaca, S. Kumar, and R. Ruiz-Baier. Well-posedness and discrete analysis for advection-diffusion-reaction in poroelastic media. Submitted preprint (2019). Available from <https://arxiv.org/abs/1908.09778>.
- [18] R. Oyarzúa and R. Ruiz-Baier. Locking-free finite element methods for poroelasticity. *SIAM J. Numer. Anal.*, 54(5):2951–2973, 2016.
- [19] J. J. Lee, K.-A. Mardal, and R. Winther. Parameter-robust discretization and preconditioning of Biot's consolidation model. *SIAM J. Sci. Comput.*, 39(1):A1–A24, 2017.
- [20] G. W. Jones and S. J. Chapman. Modeling growth in biological materials. *SIAM Rev.*, 54(1):52–118, 2012.
- [21] S. Zak. *Modern automatic control*. Lecture notes, University of Purdue, 2015.
- [22] P. Liu, J. Shi, Y. Wang, and X. Feng. Bifurcation analysis of reaction-diffusion Schnakenberg model. *J. Math. Chem.*, 51(8):2001–2019, 2013.
- [23] L. Murphy and A. Madzvamuse. A moving grid finite element method applied to a mechanobiochemical model for 3D cell migration. Submitted preprint (2019). Available from <https://arxiv.org/abs/1903.09535>.
- [24] A. Kant, T. K. Bhandakkar, and N. V. Medhekar. Stress enhanced calcium kinetics in a neuron. *Biomech. Model. Mechanobiol.*, 17(1):169–180, 2018.
- [25] Q. Fang and D. A. Boas. Monte Carlo simulation of photon migration in 3D turbid media accelerated by graphics processing units. *Opt. Express*, 22(17):20178–20190, 2009.