# Uncertainty Quantification of Thermal Damage in Hyperthermia as a Cancer Therapy

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#### Overview



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- 2. Matematical Model
- 3. Numerical Scheme

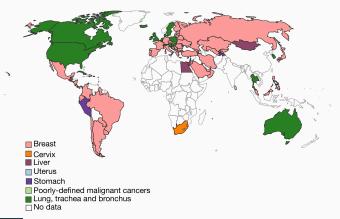
- 4. Thermal Damage
- 5. Uncertainty Quantification
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## Introduction

#### Cancer



Cancer remains a major global health concern, with breast cancer being the leading cause of cancer-related death among women in many countries.



## Hyperthermia



- Promising non-invasive cancer treatment;
- Heats the tumor region to induce necrosis;
- Hyperthermia is a complementary treatment to chemotherapy and radiotherapy;
- One strategy involves the use of a ferrofluid containing magnetic nanoparticles.

## Matematical Model

### Mathematical Model: Pennes' Equation



The Pennes equation was considered to simulate bioheat transfer<sup>1</sup>.

$$\begin{cases} \rho c \frac{\partial T}{\partial t} = \nabla \cdot k \nabla T + \omega_b \rho_b c_b (T_a - T) + Q_m + Q_r & \text{em } \Omega \times I \\ k \nabla T \cdot \vec{n} = 0 & \text{em } \partial \Omega \times I \\ T(\cdot, 0) = 37, 0 & \text{em } \Omega \end{cases}$$

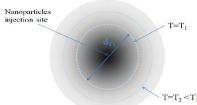
<sup>&</sup>lt;sup>1</sup>Fatigate, G. R., Lobosco, M., and Reis, R. F. (2023). A 3D Approach Using a Control Algorithm to Minimize the Effects on the Healthy Tissue in the Hyperthermia for Cancer Treatment. *Entropy*, 25(4), 684.

## Pennes' Model: Magnetic Nanoparticles



- Possibility of using high energy potential;
- Water-based, biocompatible ferrofluid solution;
- Injection of ferromagnetic fluid, e.g., 0.1, 0.2, or 0.3 cc;
- SAR<sup>2</sup> is responsible for modeling the overheating caused by the injections.

$$Q_r = \sum_{i=1}^{N_p} A e^{-r_i^2/r_{0,i}^2},$$



<sup>&</sup>lt;sup>2</sup>Salloum, M., Ma, R., and Zhu, L. (2009). Enhancement in treatment planning for magnetic nanoparticle hyperthermia: optimization of the heat absorption pattern. *International Journal of Hyperthermia*, 25(4), 309–321.

#### Pennes' Model: Limitations



#### Simplifications adopted in the Pennes' model:

- Heat transfer is assumed to occur only through capillaries;
- Blood flow is considered isotropic;
- Vascular geometry is not taken into account;
- Capillary temperature is assumed to be equal to body temperature;

## Numerical Scheme

#### Finite Difference Method



The solution was approximated using the Finite Difference Method (FDM) in a heterogeneous medium, applying the FTCS scheme.

$$T_{i,j,k}^{n+1} = \frac{h_t}{\rho c} \left[ \frac{k_{i+1/2,j,k} (T_{i+1,j,k}^n - T_{i,j,k}^n) - k_{i-1/2,j,k} (T_{i,j,k}^n - T_{i-1,j,k}^n)}{h^2} + \frac{k_{i,j+1/2,k} (T_{i,j+1,k}^n - T_{i,j,k}^n) - k_{i,j-1/2,k} (T_{i,j,k}^n - T_{i,j-1,k}^n)}{h^2} + \frac{k_{i,j+1/2} (T_{i,j,k+1}^n - T_{i,j,k}^n) - k_{i,j,k-1/2} (T_{i,j,k}^n - T_{i,j,k-1}^n)}{h^2} + \rho_b c_b \omega_b (T_a - T_{i,j,k}^n) + Q_m + Q_r \right] + T_{i,j,k}^n$$

$$(2)$$

## Thermal Damage

## **Thermal Damage: Arrhenius**



Thermal damage was evaluated using the Arrhenius model in both tumor and healthy tissue regions.

$$\Omega(x, y, z, t) = \ln\left(\frac{C(0)}{C(t)}\right) = \int_0^t Ae^{\frac{-E_a}{R_u T(x, y, z, \tau)}} d\tau, \tag{3}$$

- If the computed damage parameter  $\Omega(x, y, z, t)$  reaches 1.0, approximately 63.2% of the cells are considered to be dead;
- An Arrhenius damage parameter of 4 indicates nearly 98.2% cellular death;
- Omega values in the range  $4 \le \Omega \le 10$  are considered indicative of complete tumor ablation.

**Uncertainty Quantification** 

## **Uncertainty Quantification**



Monte Carlo simulations with 1,000 samples were performed to quantify the uncertainties associated with two correlated parameters in the Arrhenius model: the frequency factor A and the activation energy  $E_a$ .

$$E_a \approx 2.63 \times 10^3 \, \text{ln(A)} + 2.46 \times 10^4 \left\{ \begin{smallmatrix} E_{a_u} & = W \sim \textit{U(E}_{a_{min}}, E_{a_{max}}), \\ A & = e^{3.832 \times 10^{-4} E_{a} - 10.042}, \end{smallmatrix} \right.$$

$$\ln(A) = 3.832 \times 10^{-4} E_a - 10.042 \begin{cases} A_u = W \sim U(A_{\min}, A_{\max}), \\ E_a = 2.63 \times 10^3 \ln(A_u) + 2.46 \times 10^4 \end{cases}$$

## **Results**

#### **Execution Environment**



- Implemented in C;
- AMD(R) EPYC<sup>TM</sup> 7713 CPU;
- NVIDIA A100 GPU (for CUDA parallelization);
- Single-core execution;
- Results visualized using ParaView;
- Execution parameters and domain taken from the literature.

#### Simulated Scenario



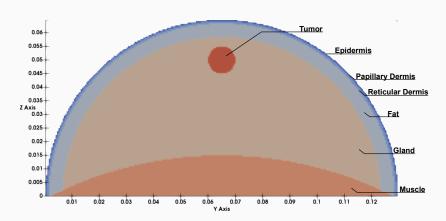
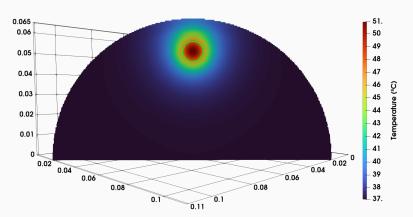


Figure 1: Simulated breast tumor

## **Heat Spread**

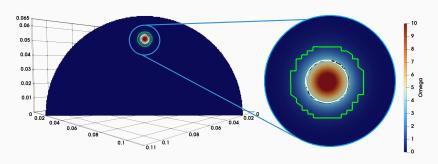




**Figure 2:** Temperature distribution computed from the bioheat equation at t = 50 min.

## Frequency Factor A Scenario

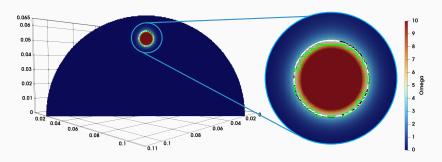




**Figure 3:** Simulation results for the scenario with uncertainty in the frequency factor A at t=5 min.

## Frequency Factor A Scenario

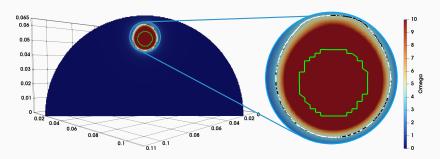




**Figure 4:** Simulation results for the scenario with uncertainty in the frequency factor A at  $t=10\,\mathrm{min}$ .

## Frequency Factor A Scenario

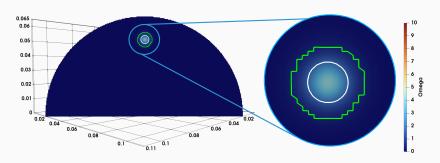




**Figure 5:** Simulation results for the scenario with uncertainty in the frequency factor A at t=50 min.

## Activation Energy $E_a$ Scenario

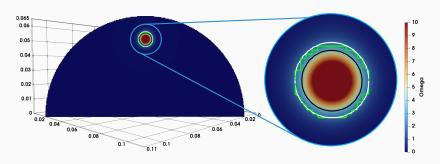




**Figure 6:** Simulation results for the scenario with uncertainty in the activation energy  $E_a$  at  $t=5\,\mathrm{min}$ .

## **Activation Energy** *E*<sub>a</sub> **Scenario**

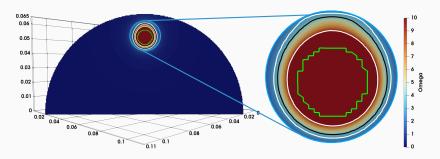




**Figure 7:** Simulation results for the scenario with uncertainty in the activation energy  $E_a$  at  $t=10\,\mathrm{min}$ .

## **Activation Energy** *E*<sub>a</sub> **Scenario**

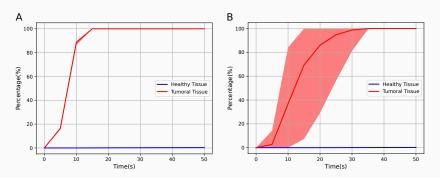




**Figure 8:** Simulation results for the scenario with uncertainty in the activation energy  $E_a$  at  $t=50\,\mathrm{min}$ .

## **Uncertainty Quantification Results**





**Figure 9:** Results of the uncertainty quantification due to variations in A and  $E_a$  for assessing tumor damage during hyperthermia treatment.

**Conclusion and Future Works** 

#### **Conclusion and Future Works**



- Variations in the frequency factor A have a minor influence on tissue damage predictions, even when A spans from  $A_{\min} = 7.39 \times 10^{39}$  to  $A_{\max} = 3.10 \times 10^{98}$ .
- In contrast, variations in the activation energy  $E_a$  significantly affect the outcomes, with  $E_a$  ranging from  $E_{a_{\min}} = 2.577 \times 10^5 \, \text{J/mol}$  to  $E_{a_{\max}} = 6.030 \times 10^5 \, \text{J/mol}$ .
- The confidence intervals observed in the thermal damage suggest that uncertainty in  $E_a$  leads to a critical damage threshold ( $\Omega \geq 4$ ) being reached between 15 and 35 minutes.

#### **Conclusion and Future Works**



- In future work, we plan to study different tissue layers in the human body using realistic tumor and tissue geometries;
- Incorporate Multilevel Monte Carlo (MLMC) methods to accelerate simulations and improve computational efficiency;
- Finally, we intend to validate the model results using clinical or experimental data.

## **Acknowledgements**



Obrigado! Thanks!













<sup>&</sup>lt;sup>3</sup>423278/2021-5

<sup>&</sup>lt;sup>4</sup>APQ-01226-21