

# Micro and Nano-Tomography of Biological Tissues

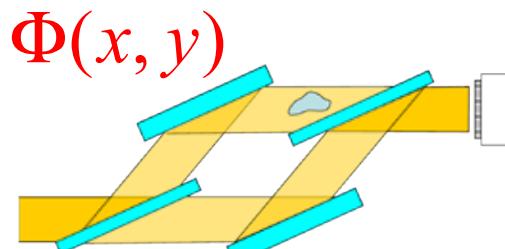
Marco Stampanoni and Kevin Mader

Swiss Light Source, Paul Scherrer Institut  
Institute for Biomedical Engineering, University and ETH Zürich

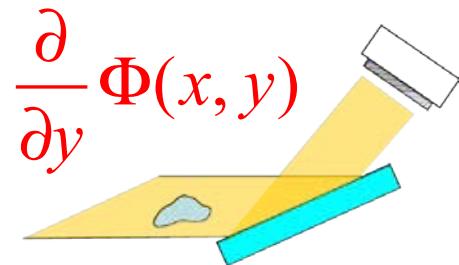
ETH-227-0965-00 L



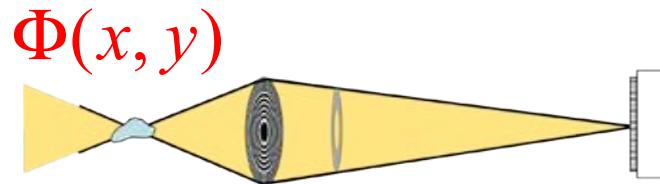
# X-ray phase contrast techniques



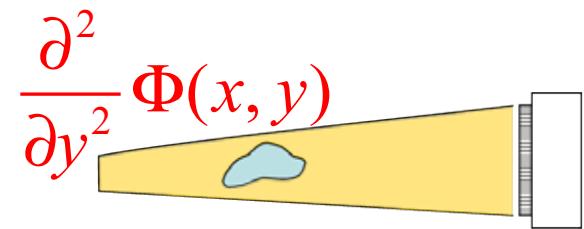
$\Phi(x, y)$   
Crystal interferometry  
Bonse et al. APL 6, 155 (1965)



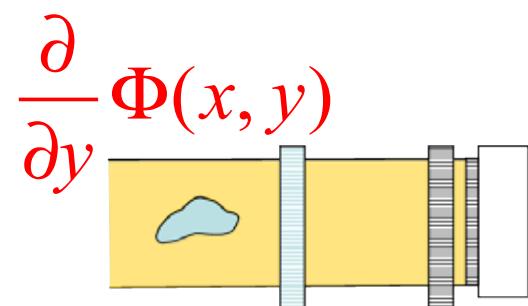
$\frac{\partial}{\partial y} \Phi(x, y)$   
Analyser-based (DEI)  
Chapman et al., PMB, 42, 2015 (1997)  
Davis et al., JOSAA 13, 1193 (1996)



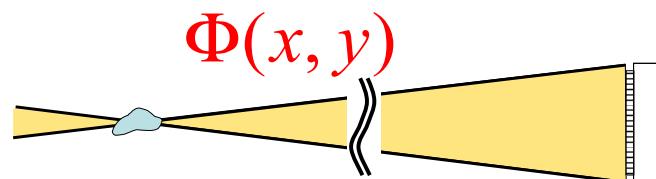
$\Phi(x, y)$   
Zernike Phase Contrast  
Weiss et al., UM 84, 185 (2000)  
Stampanoni et al., PRB 81, 140105R (2010)



$\frac{\partial^2}{\partial y^2} \Phi(x, y)$   
Free Space Propagation (TIE)  
Snigirev et al., RSI 66, 5486 (1995)  
Cloetens et al., APL 75, 2912 (1999)  
Groso et al., OptExp 14, 8103 (2006 )



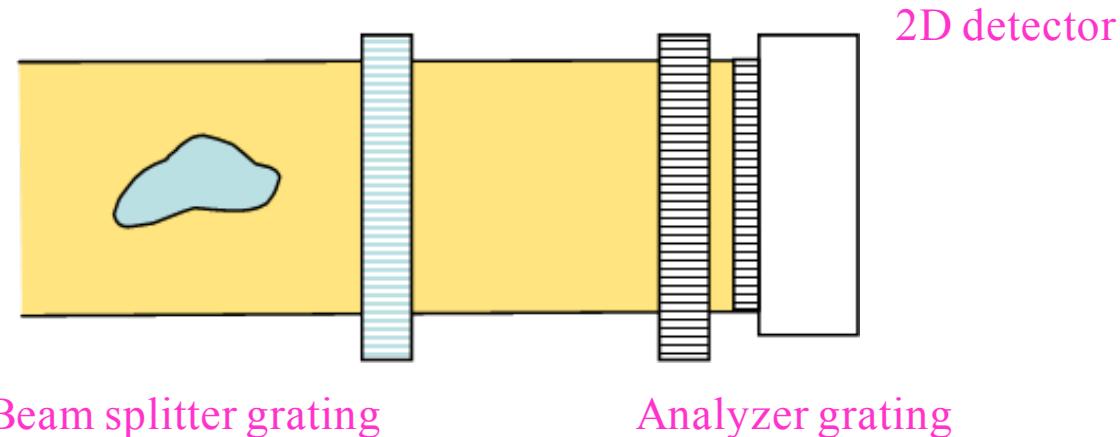
$\frac{\partial}{\partial y} \Phi(x, y)$   
Grating interferometry (DPC)  
Weitkamp et al., OptExp 13, 6296 (2005)  
Pfeiffer et al., Nature Phys 2, 258 (2006)



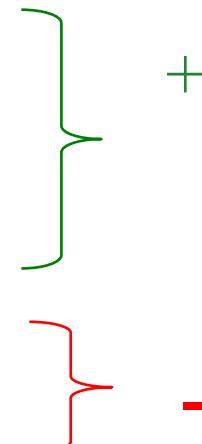
$\Phi(x, y)$   
Coherent Diffraction Imaging (CDI)  
Miao et al., Nature 400 (1999)  
Thibault et al., Science, 321, 379 (2008).

# Grating interferometry

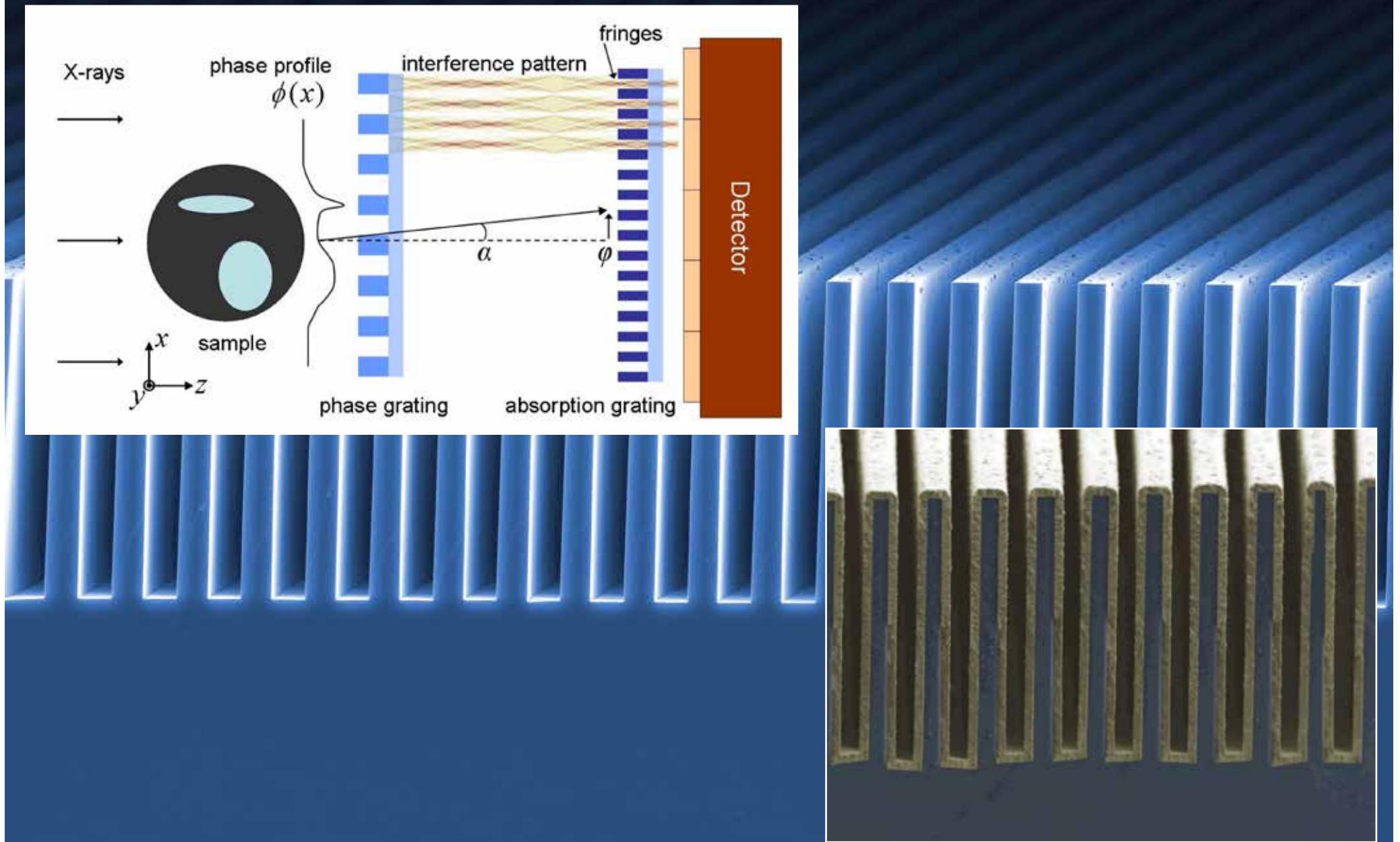
Weitkamp et al., Optics Express (13), 6296 (2005)  
Pfeiffer et al., Nature Physics 2 (4): 258-261 (2006)



- The measured quantity is  $(\partial\Phi/\partial y)$ , as in DEI.
- Phase stepping technique followed by integration
- **Simple setup, mechanically robust**
- **Large field of view**
- **Usable with divergent and polychromatic beams**
- **Usable with standard X-ray tubes, low coherence required**
- **Moderate spatial resolution, limited by grid period**

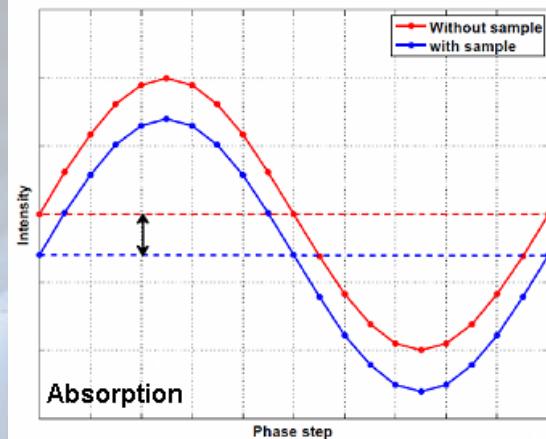


# Sensing the wavefront with grating interferometry



# Sensing the wavefront with grating interferometry

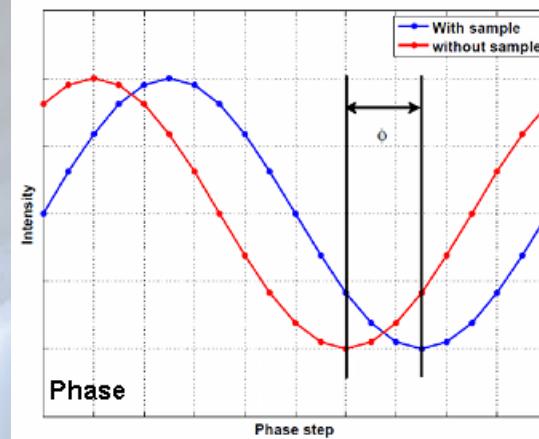
Absorption contrast



$$-\log\left(\frac{I_s}{I_b}\right)$$



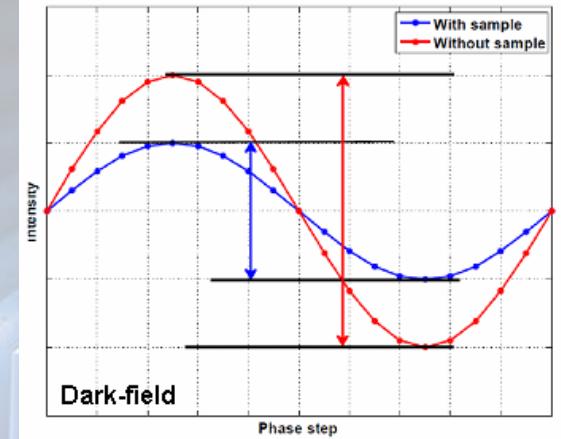
Differential phase contrast



$$\Phi_s - \Phi_b$$



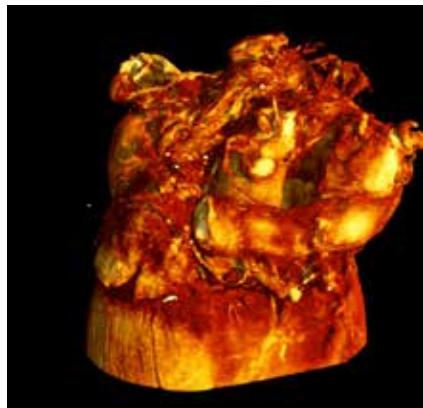
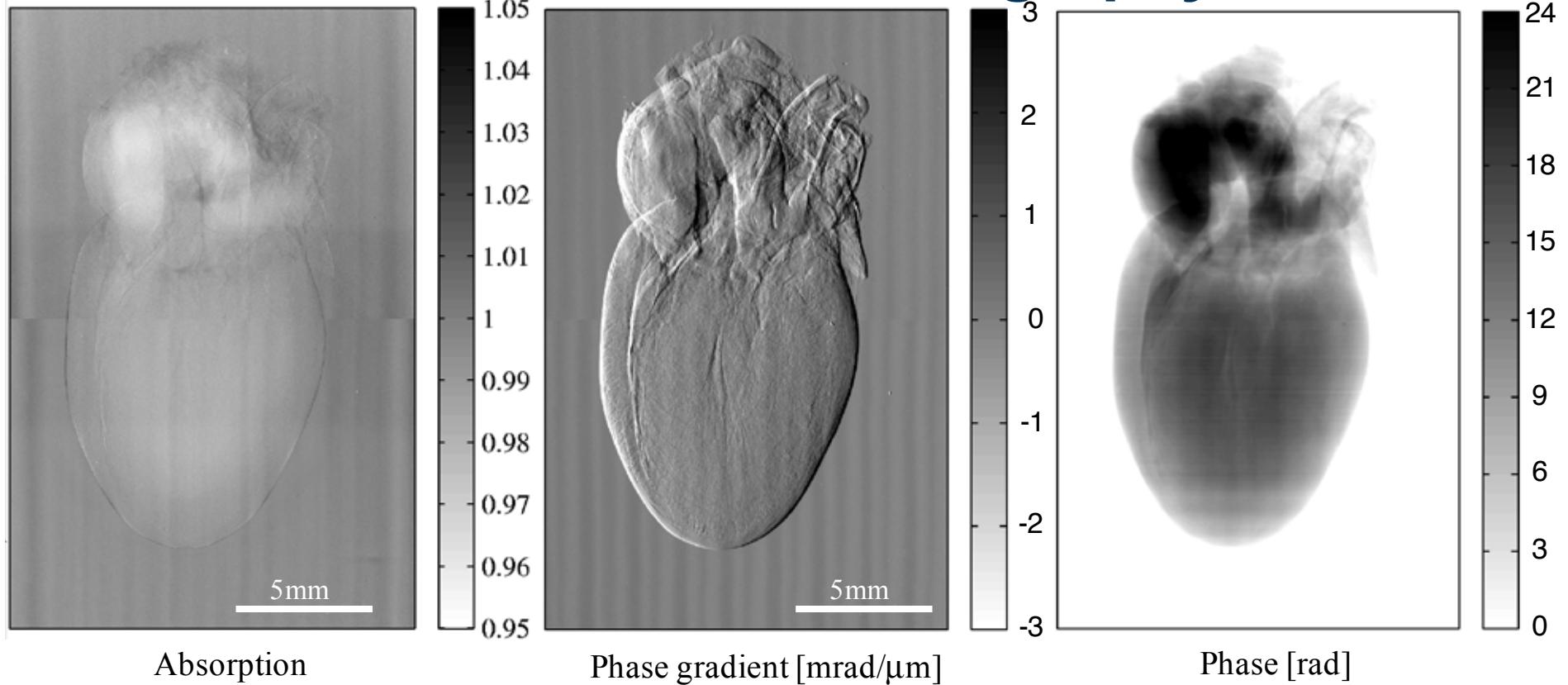
Dark-field contrast



$$-\log\left(\frac{V_s}{V_b}\right) \quad V = \frac{I_{\max} - I_{\min}}{I_{\max} + I_{\min}}$$

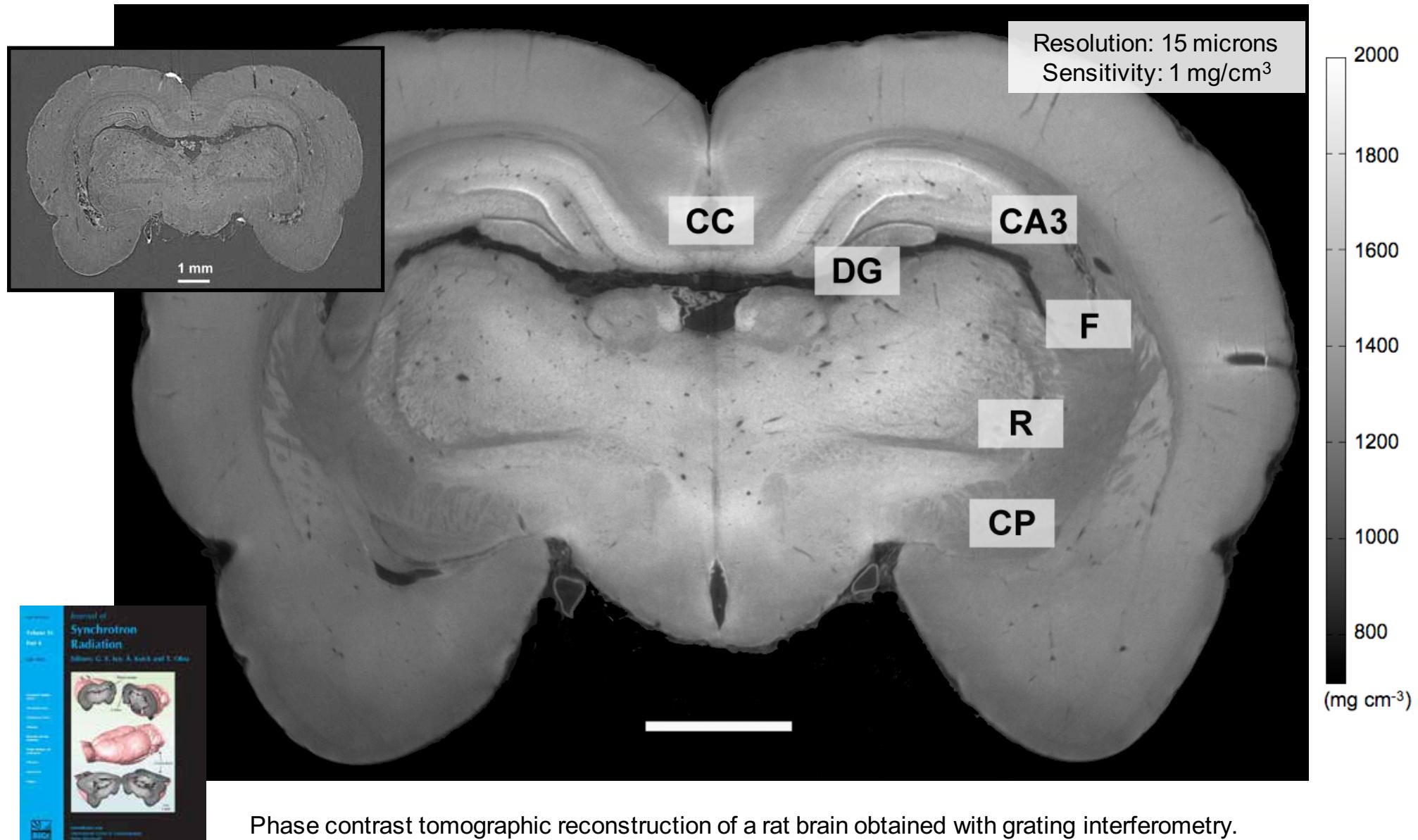


# Phase contrast radiography



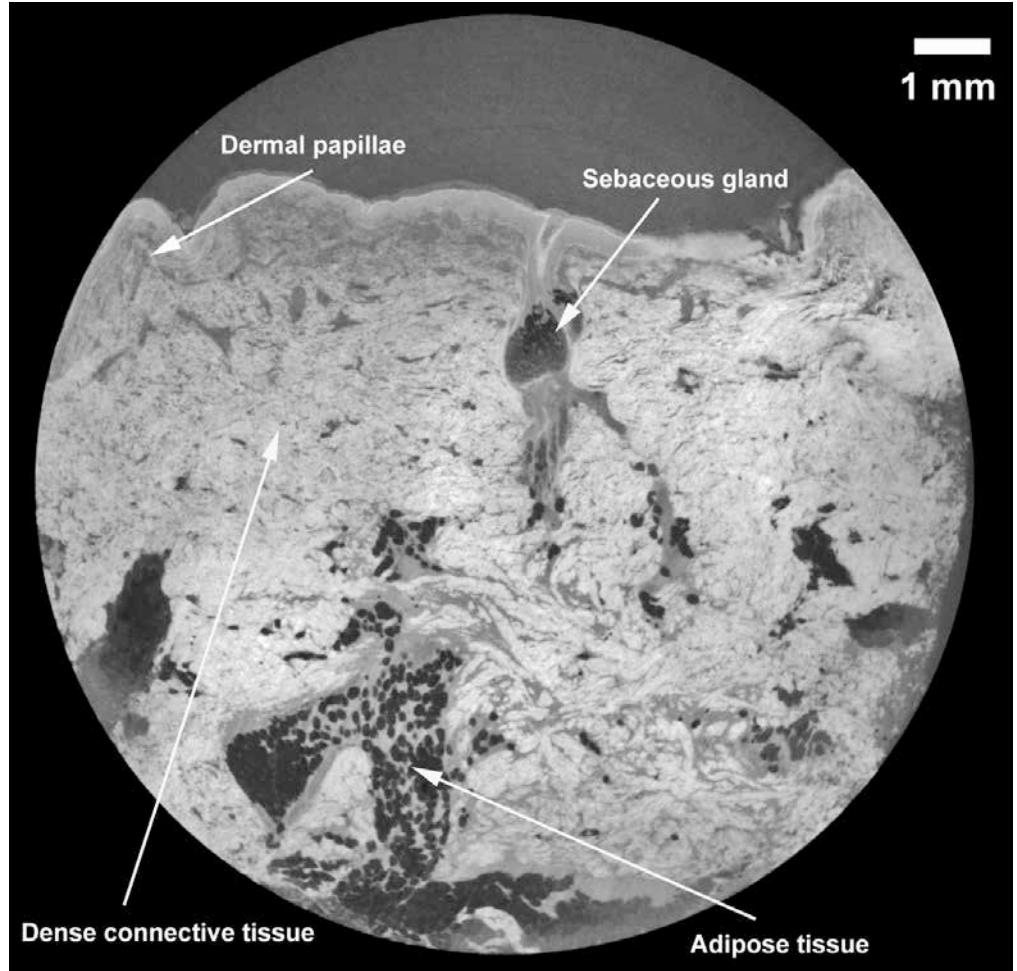
Rat heart in formalin solution, ESRF, ID19, 17.8 keV.  
Images courtesy of T. Weitkamp

# High sensitivity at isotropic, high resolution



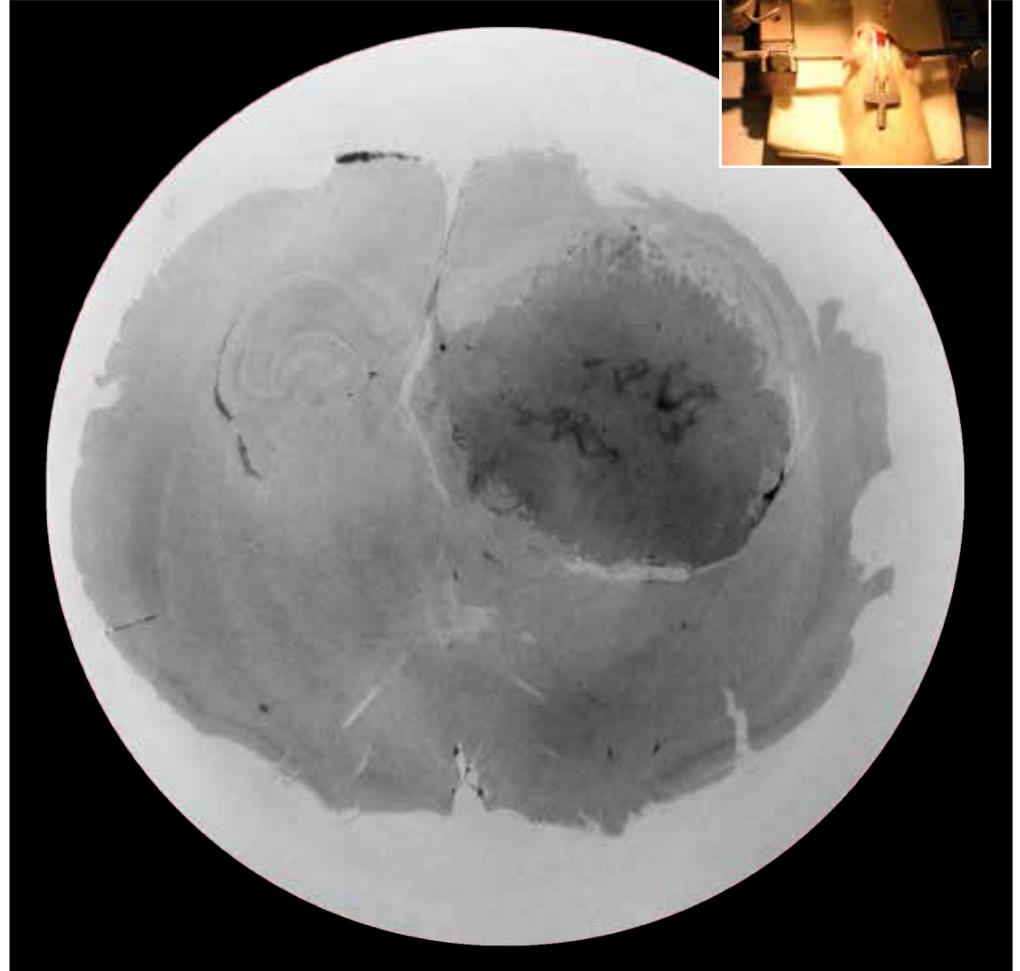
# Soft-tissue sensitivity

M. Stampanoni et al., MASR 2010



Human skin tissue biopsy

E. Schültke, unpublished data

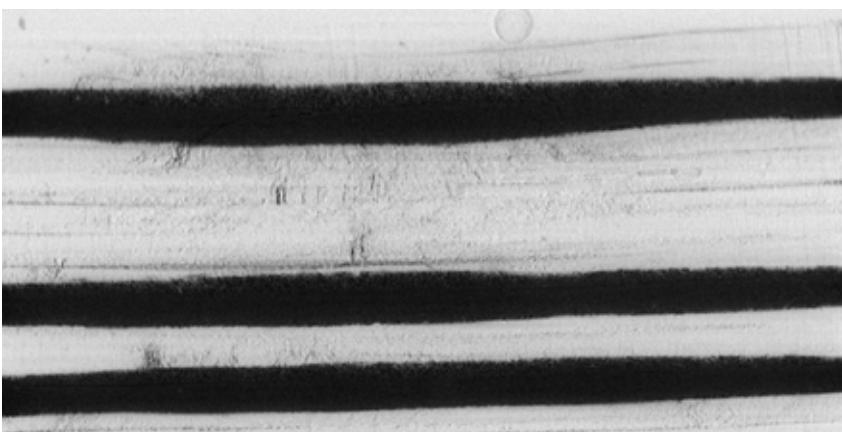
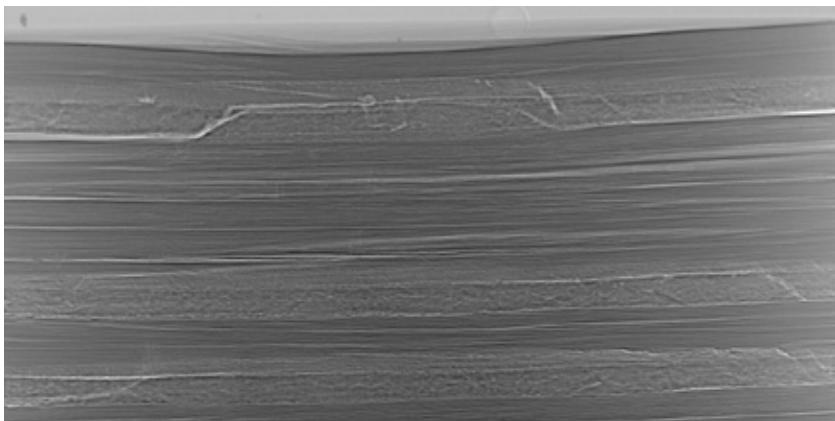


Inoculated GNP-F98 glioma

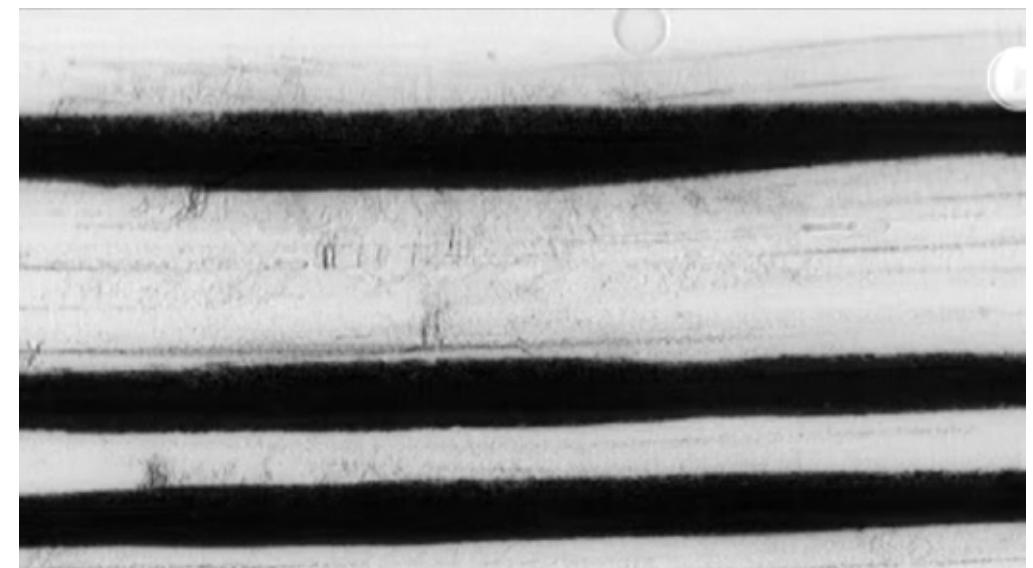
TOMCAT Interferometer: 25 keV, 3<sup>rd</sup> Talbot Distance

# Darkfield radiology

CFRP laminated structure consisting of alternate layers of plastic matrix and fiber reinforcement



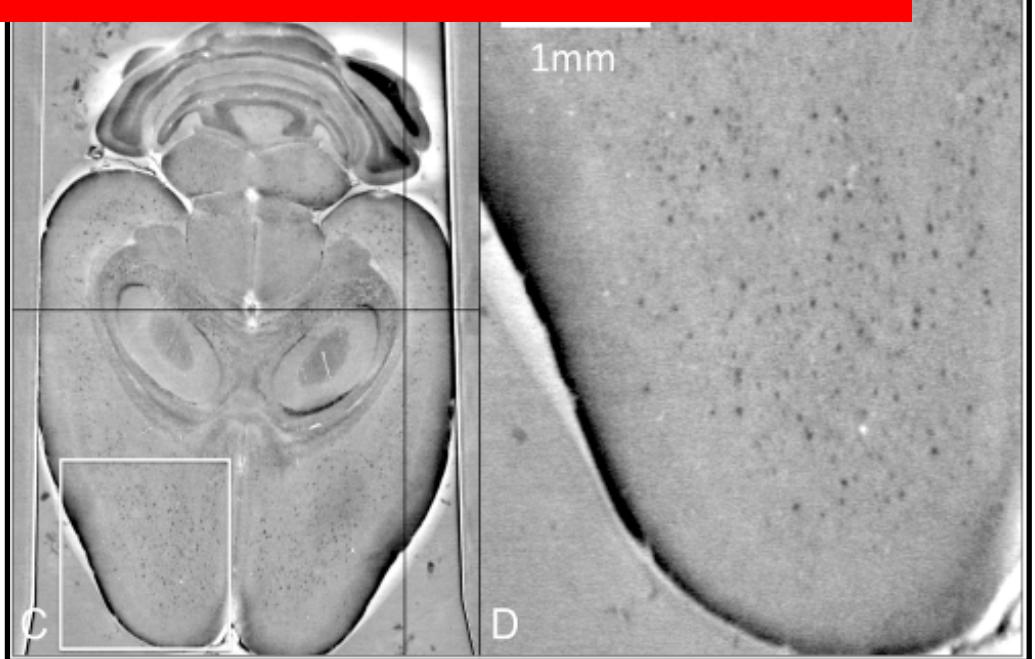
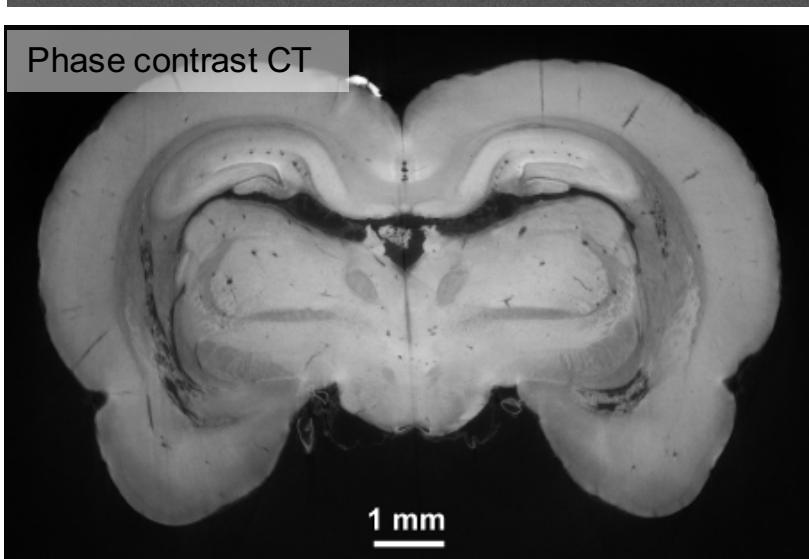
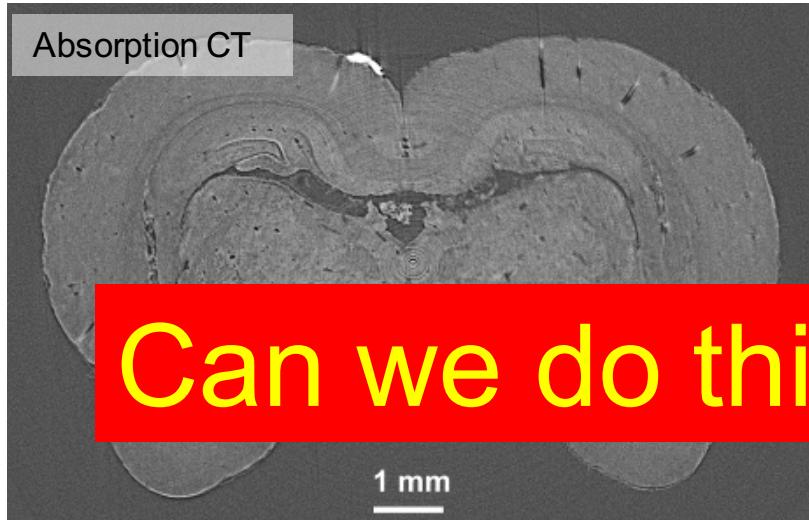
← 10 mm →



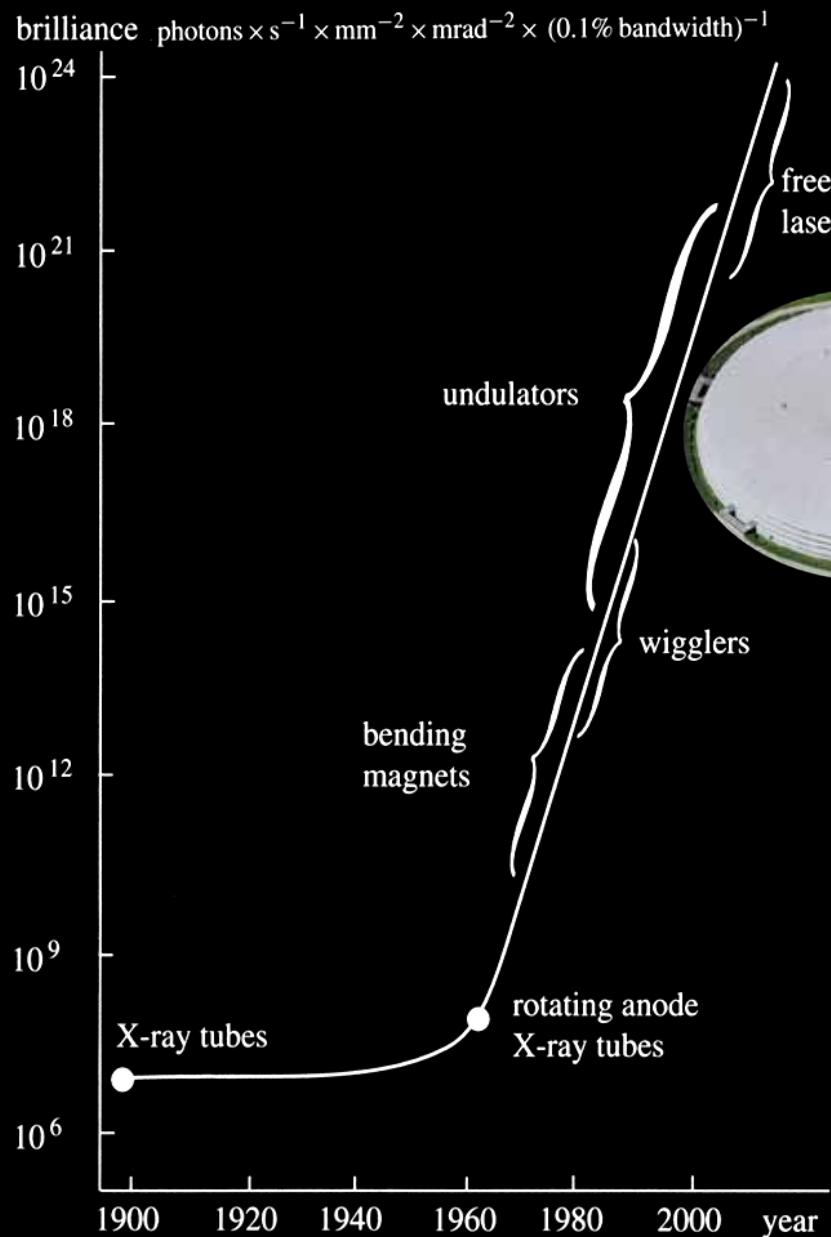
Directional dependency of the darkfield signal.  
Issues with the tomographic reconstruction...

S. McDonald, M. Stampanoni et al. , Journal of Synchrotron Radiation 16, 562-572,(2009)

# Phase contrast imaging (CT) at synchrotron (10 microns isotropic resolution)

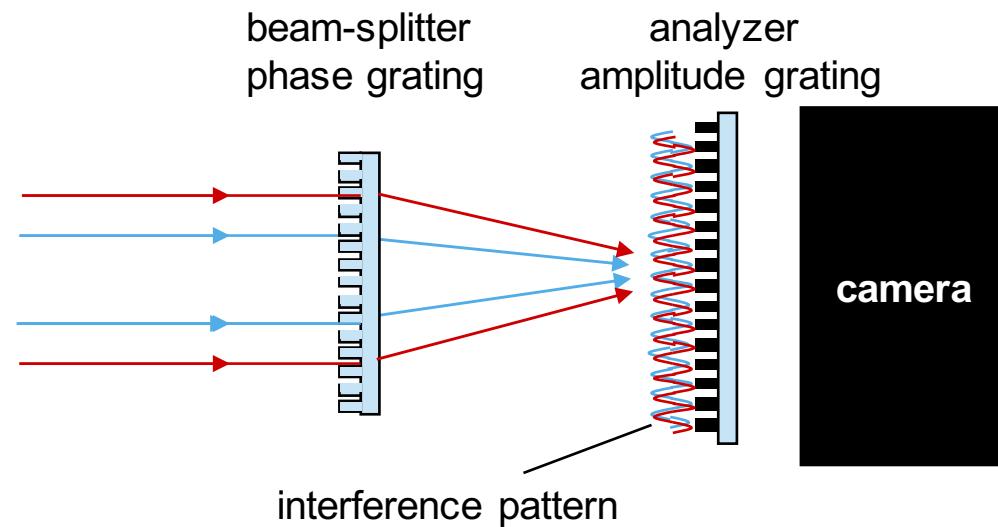


# Moving back to the “origins”...



Low spatial and temporal coherence!!

# Temporal (longitudinal) coherence requirements

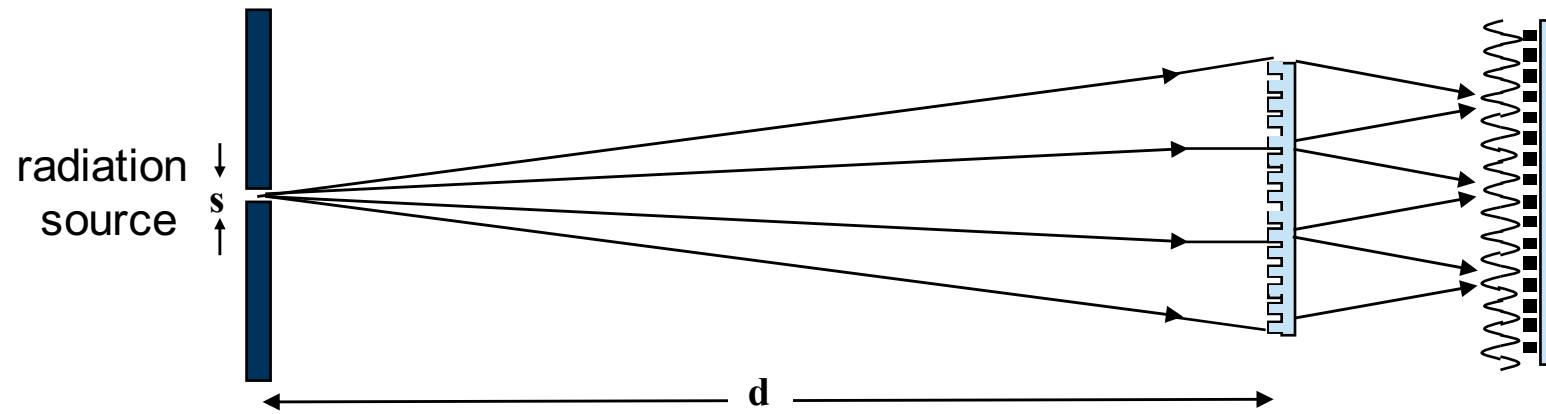


The position and pitch of the interference pattern does not depend on the wavelength!



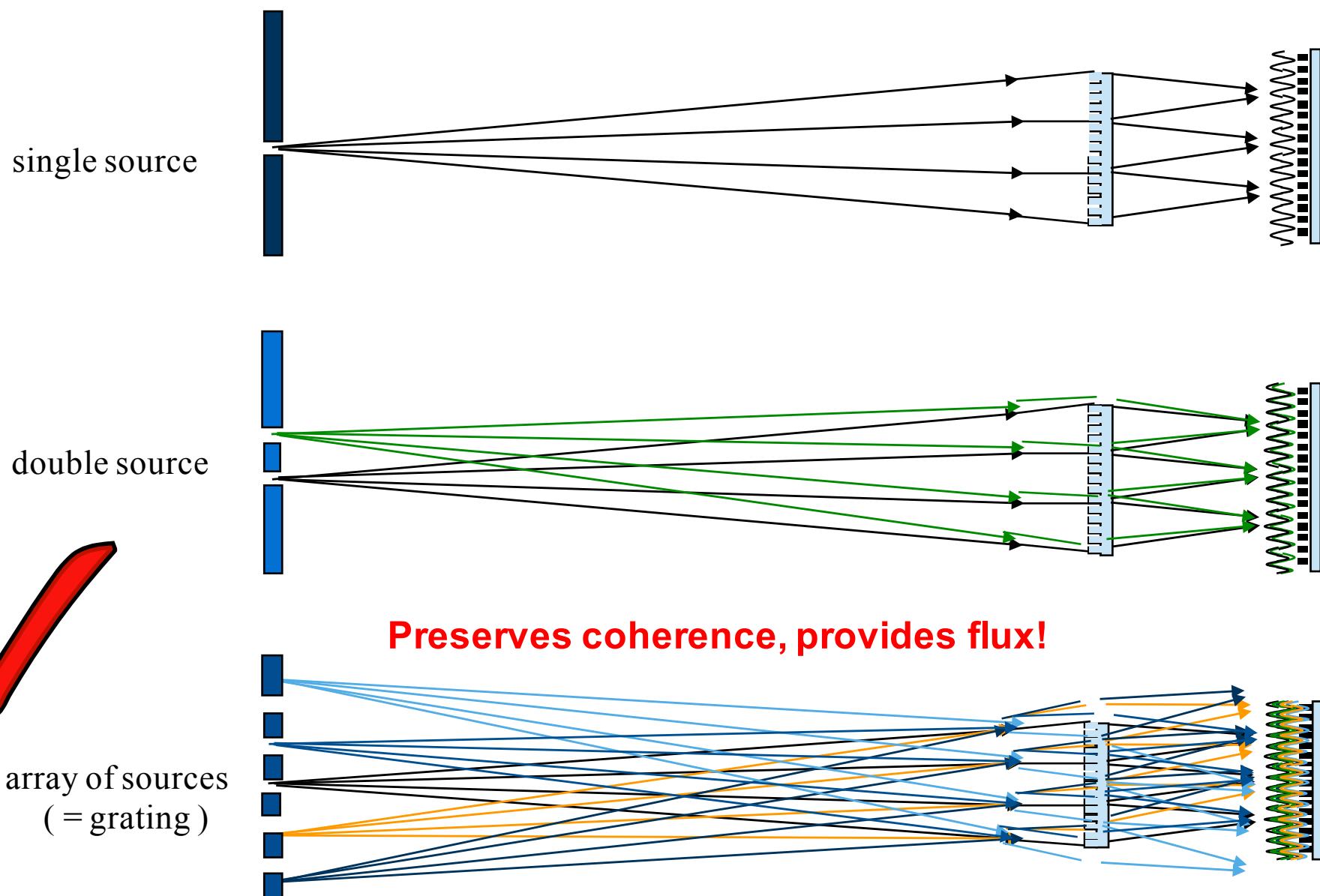
10-20% bandwidth is OK

# Spatial (transverse) coherence requirements



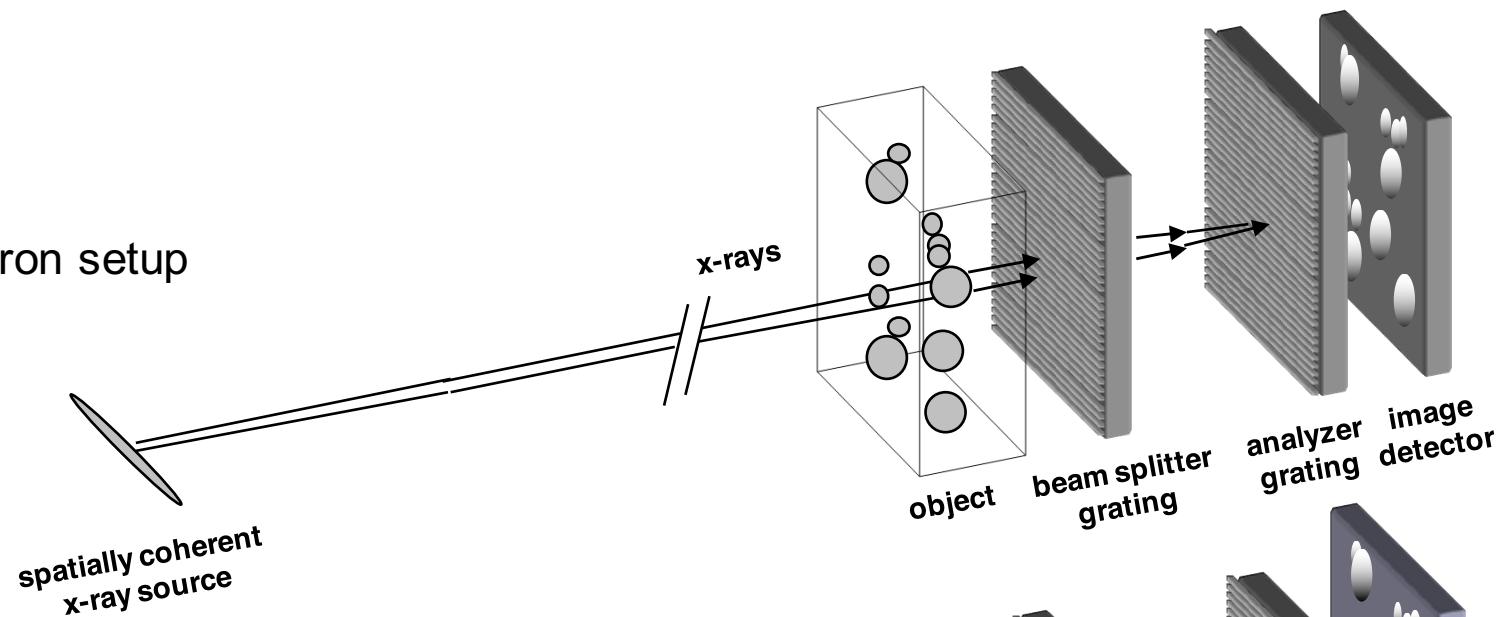
- Required in one direction
  - Depends on wavelength, geometry, ....
  - For Energy = 20 keV, d=1m, → **s < 10-20 μm**
- LOW FLUX !!

# The Talbot-Lau interferometer

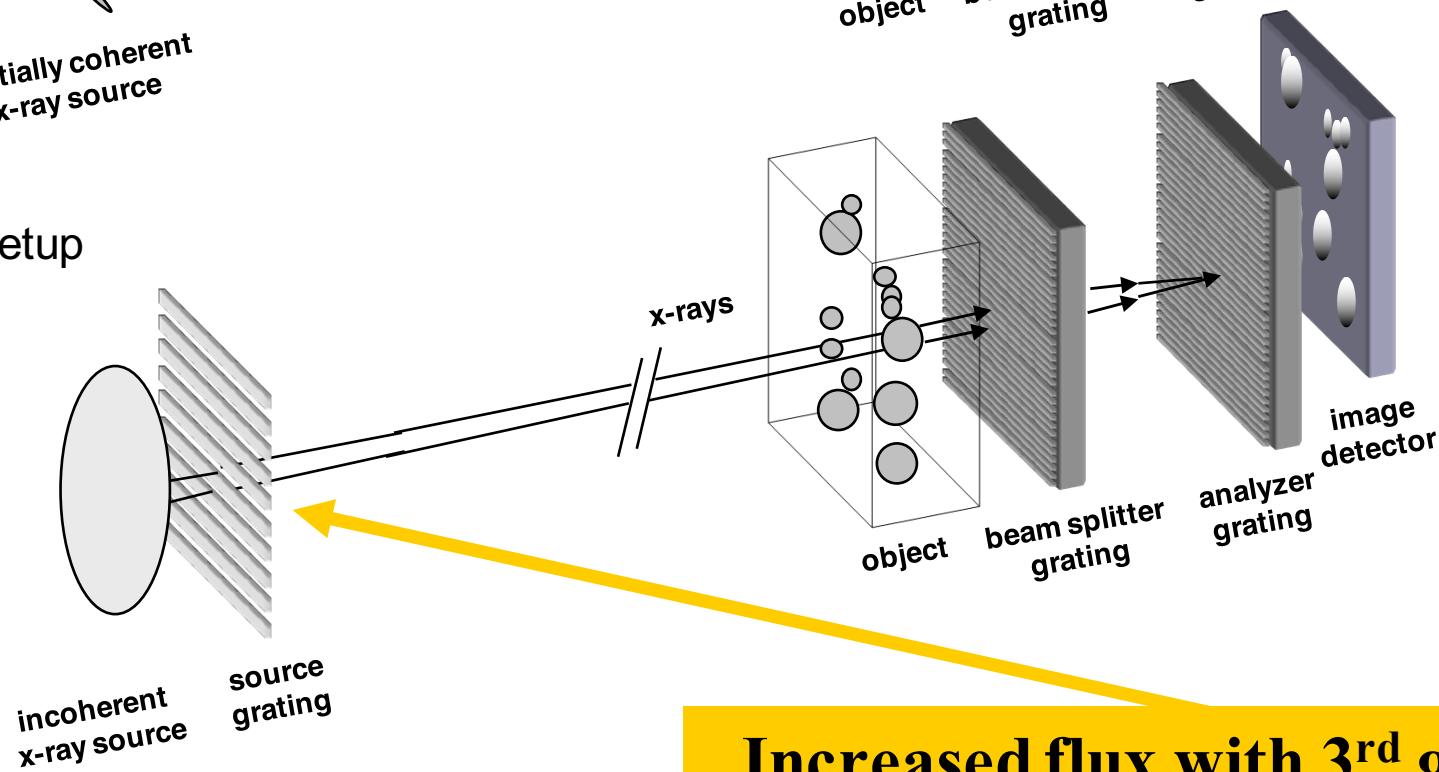


# The Talbot-Lau interferometer

Synchrotron setup



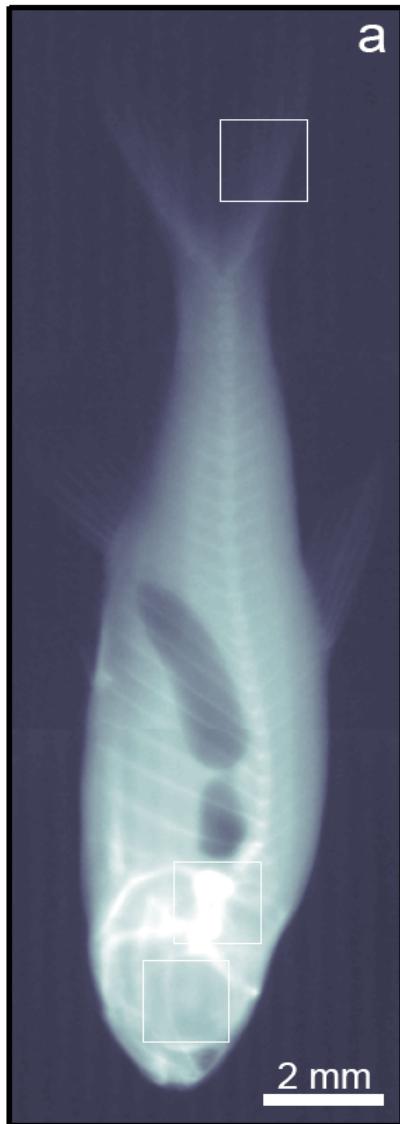
X-ray tube setup



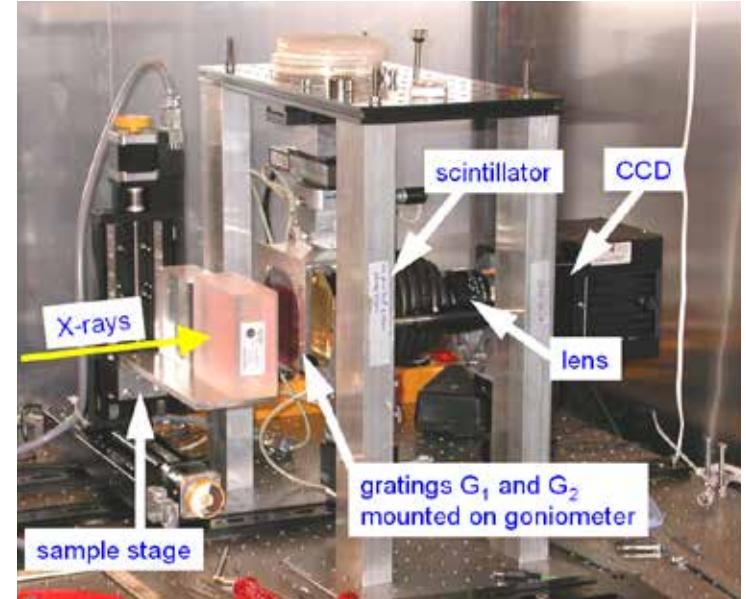
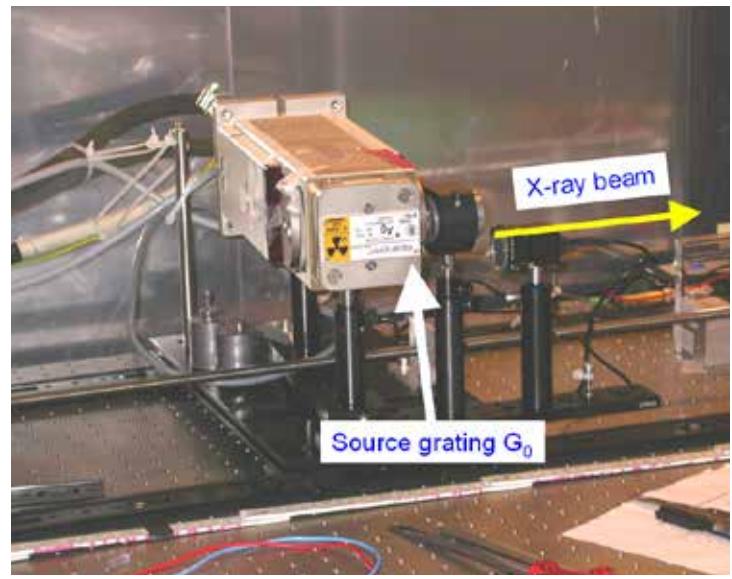
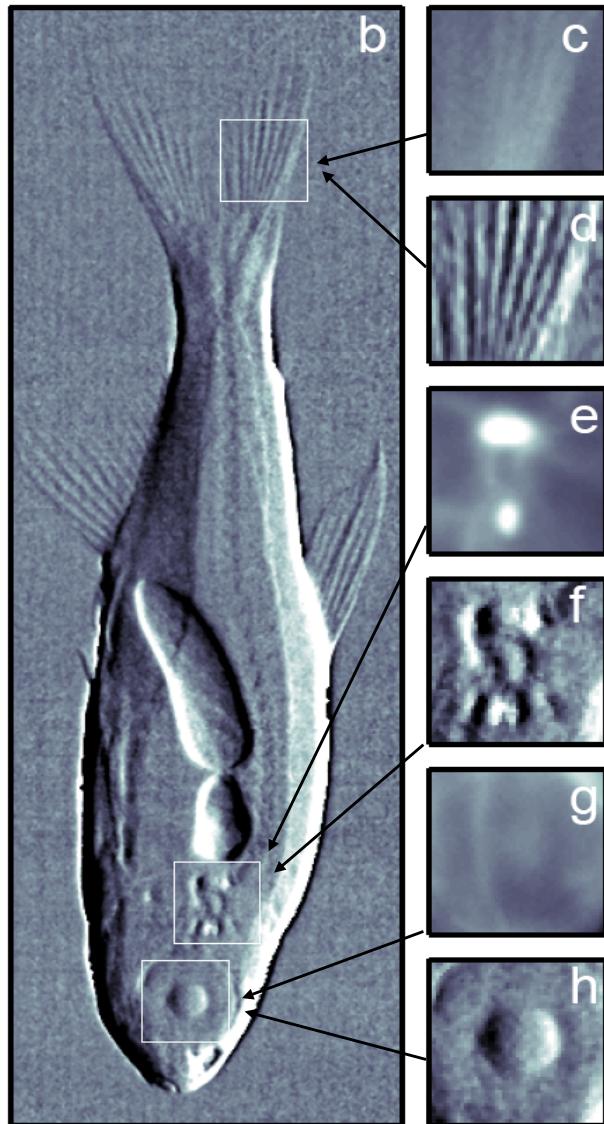
Increased flux with 3<sup>rd</sup> grating

# DPC on a X-ray tube

Amplitude



Phase (gradient)

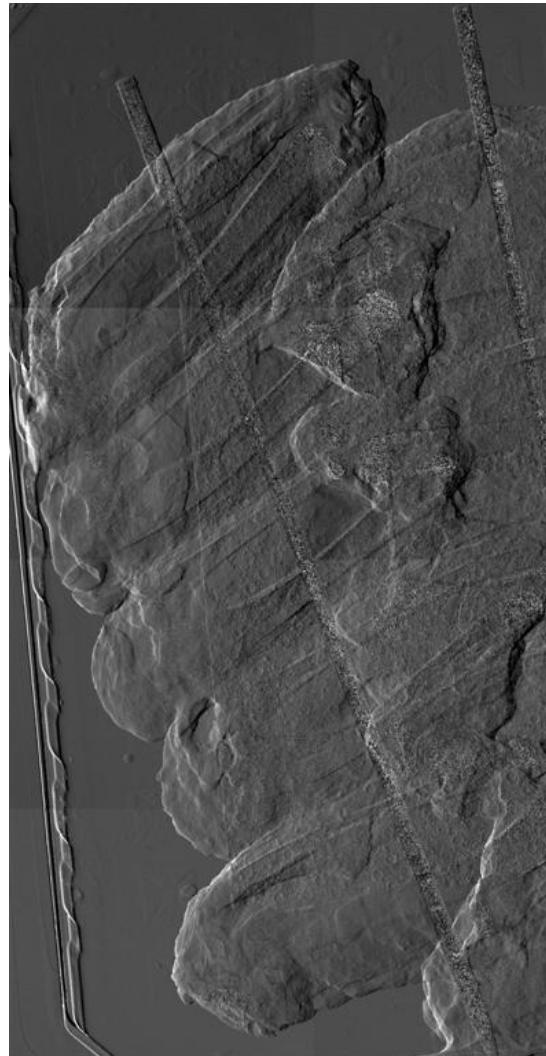


F. Pfeiffer et al., NATURE PHYSICS 2, (2006)

# Advanced imaging of large samples



Absorption



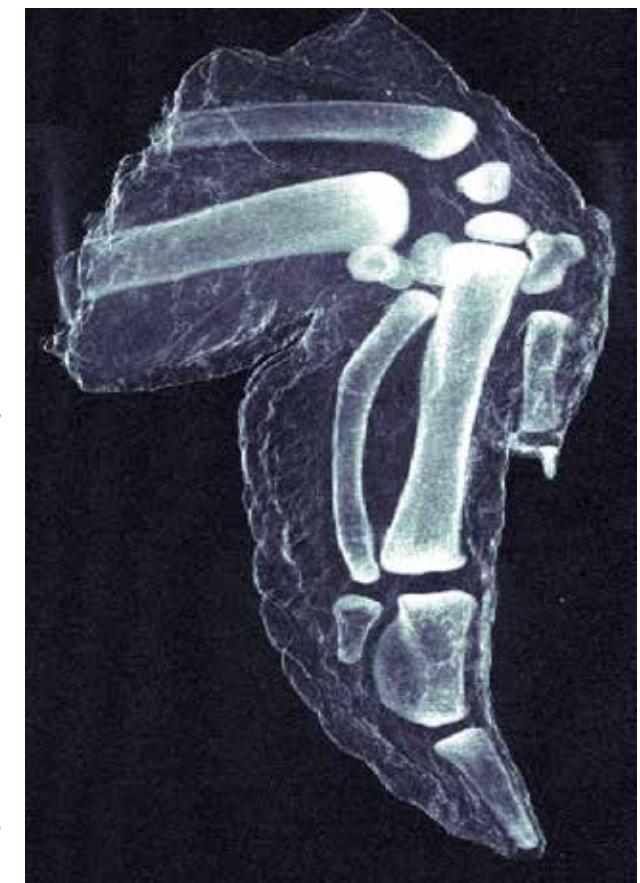
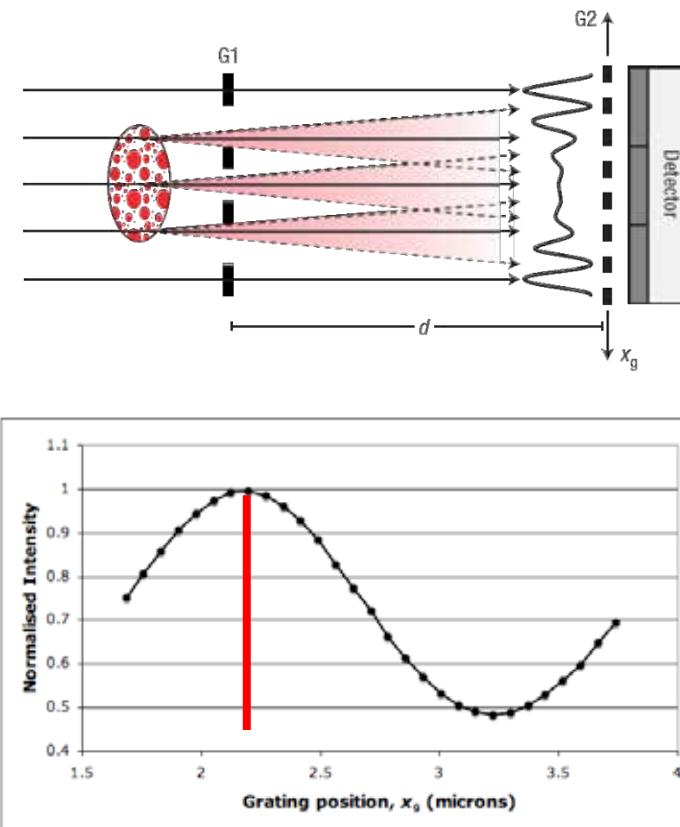
Differential Phase contrast



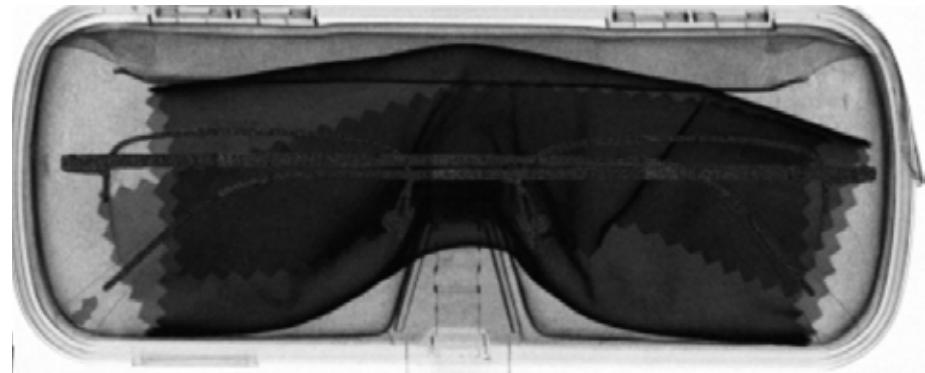
Dark Field

Data courtesy of Z. Wang, TOMCAT Group

# Absorption vs. dark-field imaging



Transmission image

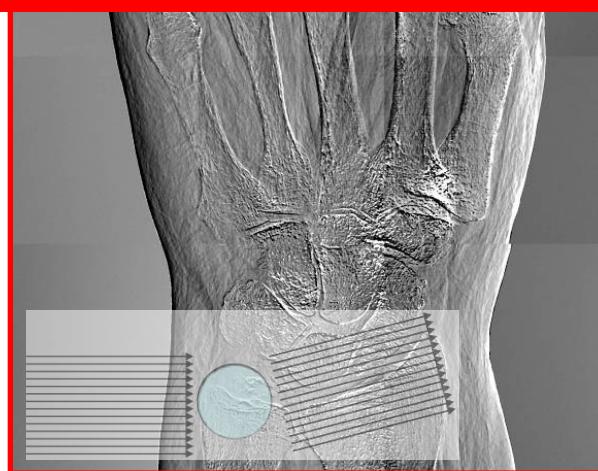
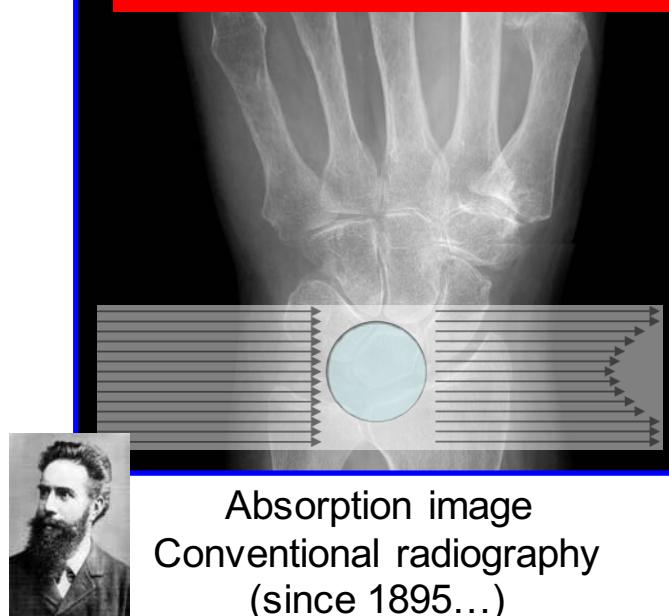


Darkfield image

# New radiological capabilities



Exploit these additional physical signals  
to improve (early) breast cancer detection

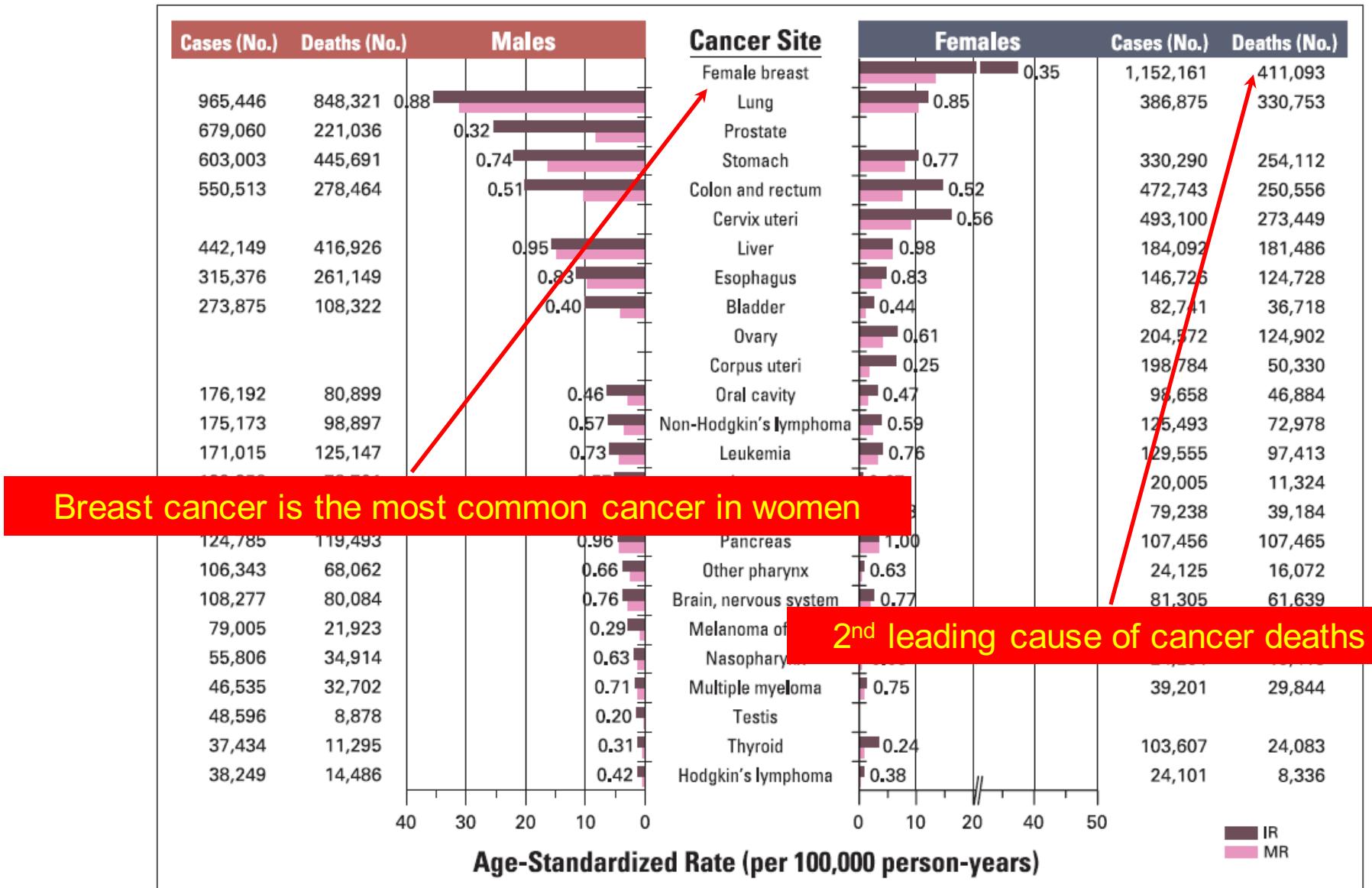


$$\text{Index of refraction: } n = 1 - \delta + i\beta$$

Phase      Absorption

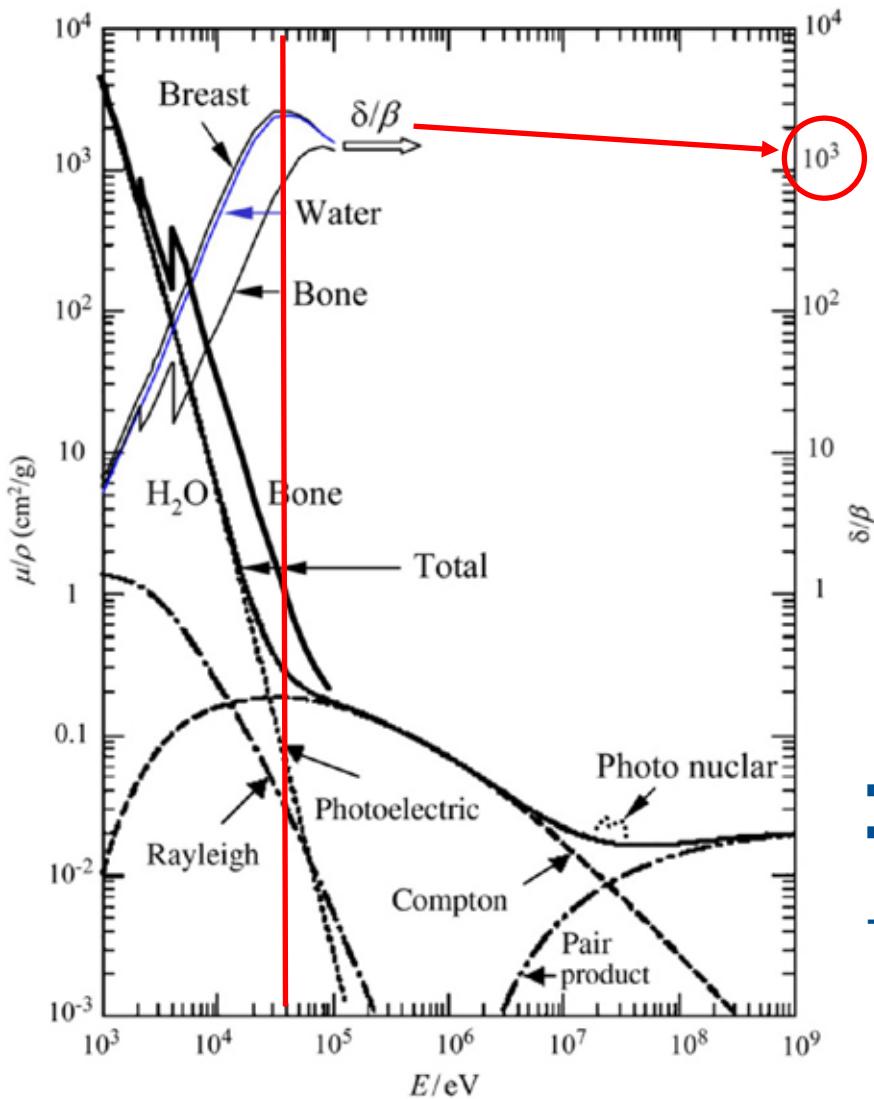
# Phase contrast mammography: why?

Worldwide annual number of cancer cases and cancer deaths, incidence rates and mortality rates



F. Kamangar et al., Journal of Clinical Oncology, 24(14), 2137-2150 (2006)

# Towards clinical phase contrast mammography



Zhou et al., Physica Medica (2008) 24, 129-148

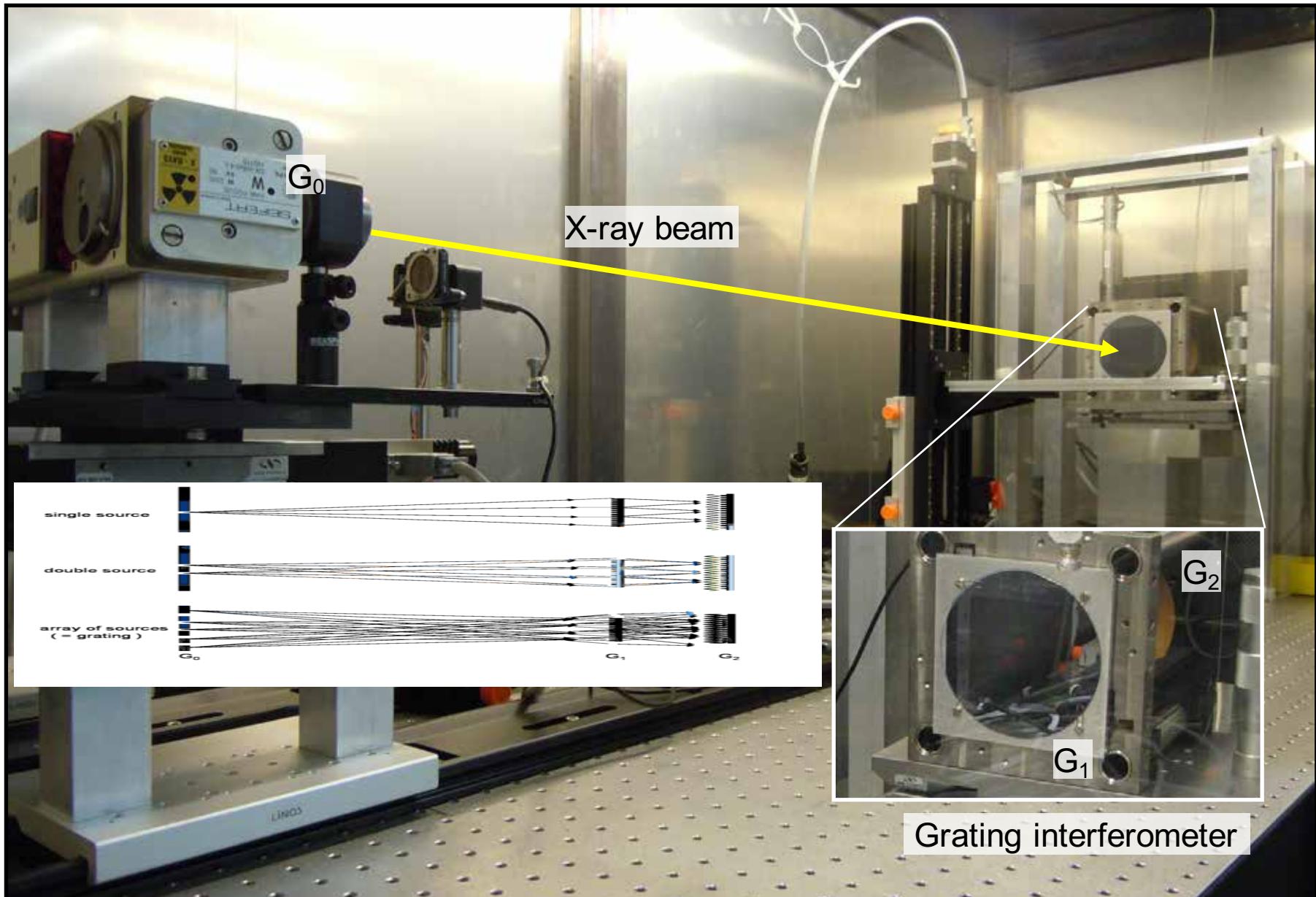
Index of refraction:  $n = 1 - \delta + i\beta$

Phase Absorption



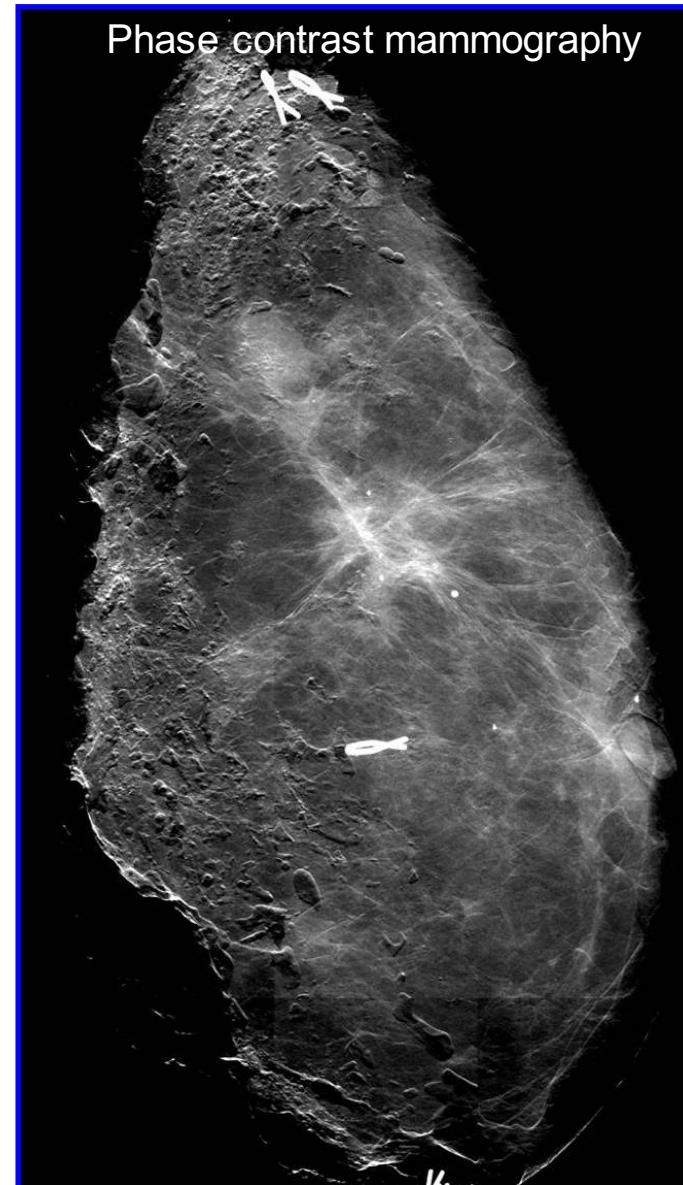
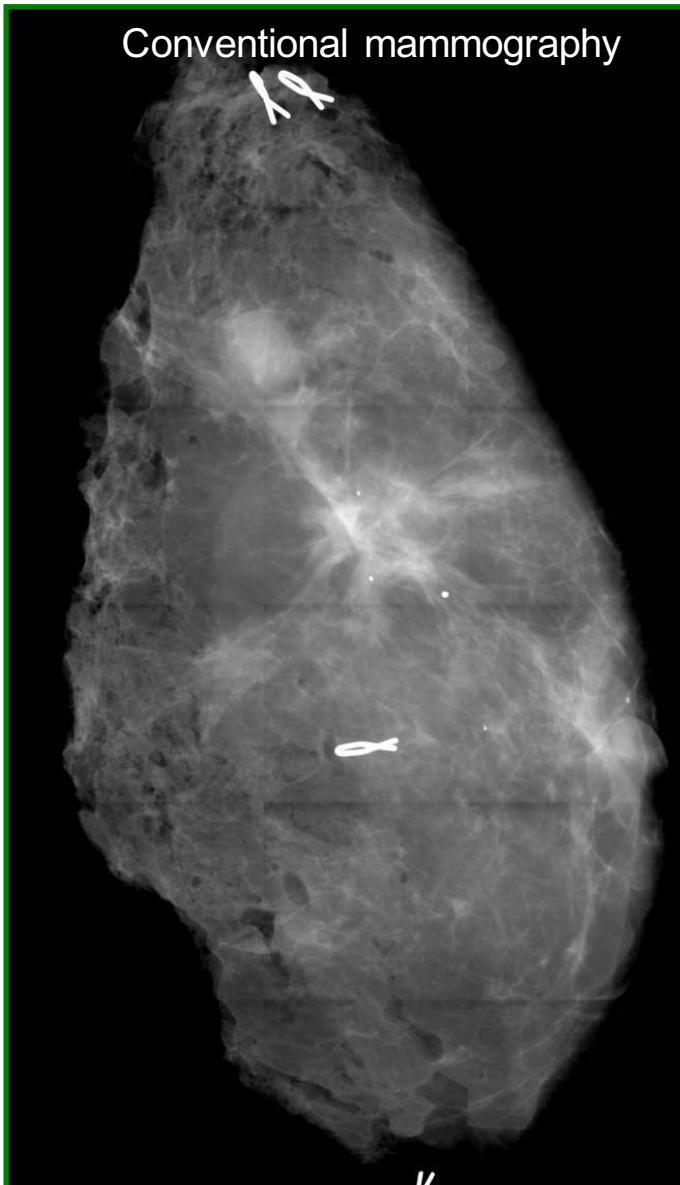
- Working energy for mammography: 20-30 keV
- For 20-30 keV,  $\delta/\beta > 1000$
- When comparing various tissue samples, relative differences in angular deviations are larger than the corresponding relative changes in attenuation
- We expect improved diagnostic capabilities when compared to conventional methods

# Phase contrast mammography demonstrator



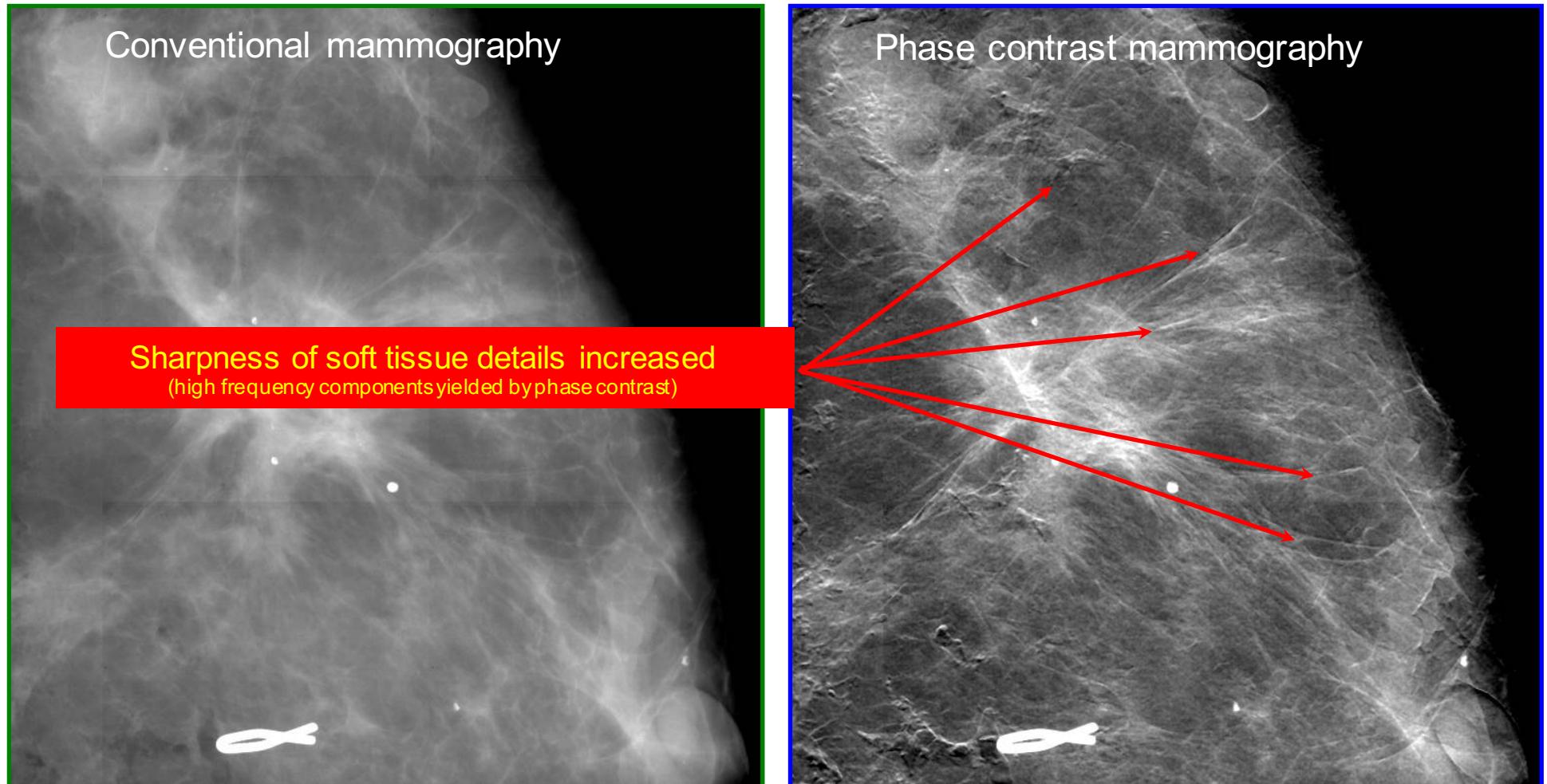
M. Stampanoni et al., Investigative Radiology, 46,801, (2011)

# Differential phase signal enhances *spiculations* visibility



M. Stampanoni et al., Investigative Radiology, 46,801, (2011)

# Differential phase signal enhances *spiculations* visibility



Same dose!

M. Stampanoni et al., Investigative Radiology, 46,801, (2011)

# Phase contrast enhanced mammography

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ORIGINAL ARTICLE

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## A Study on Mastectomy Samples to Evaluate Breast Imaging Quality and Potential Clinical Relevance of Differential Phase Contrast Mammography

**TABLE 2.** Statistical Outcome Showing the Criteria Under Which mammoDPC Is Superior to Absorption-Based Mammography

Evaluated Criteria (mammoDPC Is Superior)	P*	IQR
General quality of image	<0.001	2–3†
Sharpness and lesion delineation	<0.001	2–3
Delineation of surface structures	<0.001	2–3
Sharpness of microcalcifications	<0.001	2–2
General visibility of microcalcifications	<0.001	2–3
Potentially clinically relevant information	<0.001	4–5‡
Identification of spiculations	<0.015§	

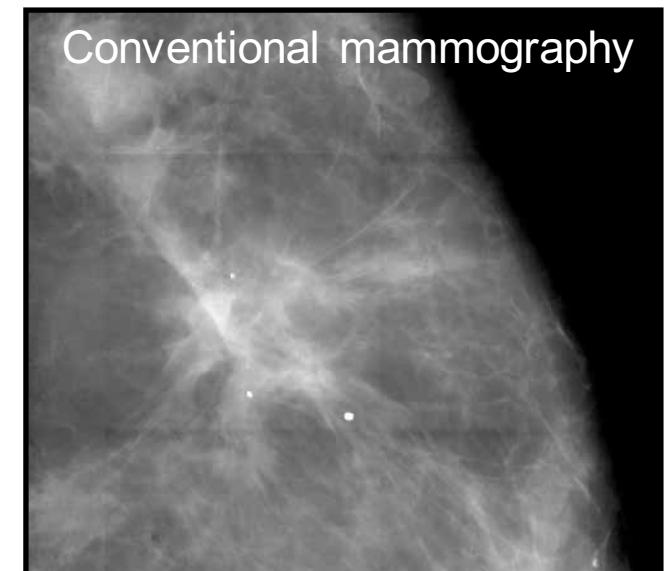
\*P < 0.005 is considered to be significant with Bonferroni correction.

†2 being “superior” and 3 being “equivalent” quality.

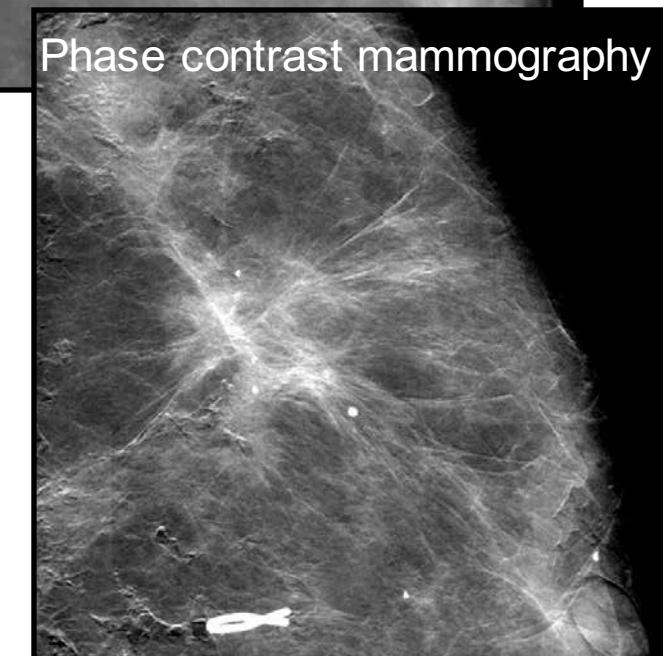
‡4 being “11% to 20% superior” and 5 being “1% to 10% superior.”

§This criterion was evaluated in study 2. P < 0.025 is significant with the Bonferroni correction.

IQR indicates interquartile range; mammoDPC, phase contrast-enhanced mammography.



Conventional mammography

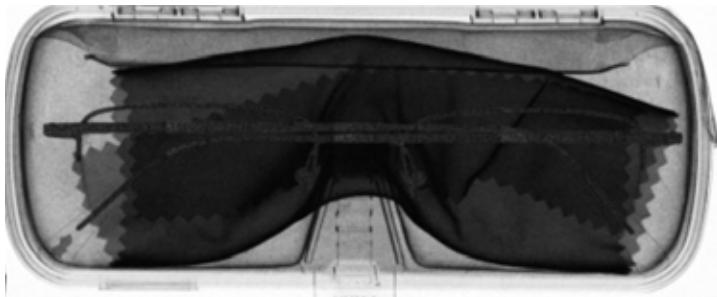
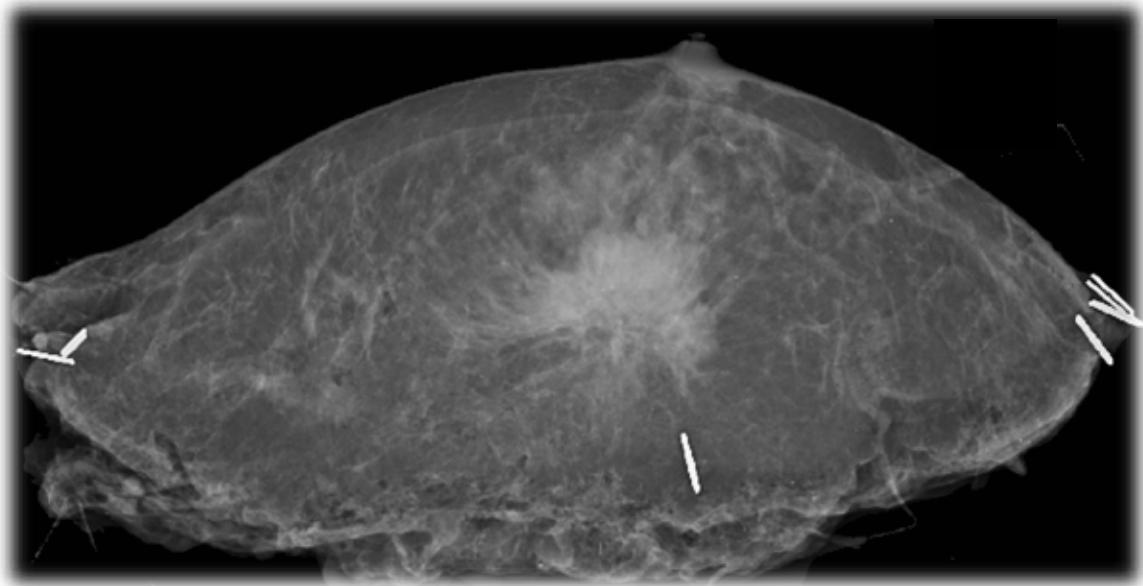


Phase contrast mammography

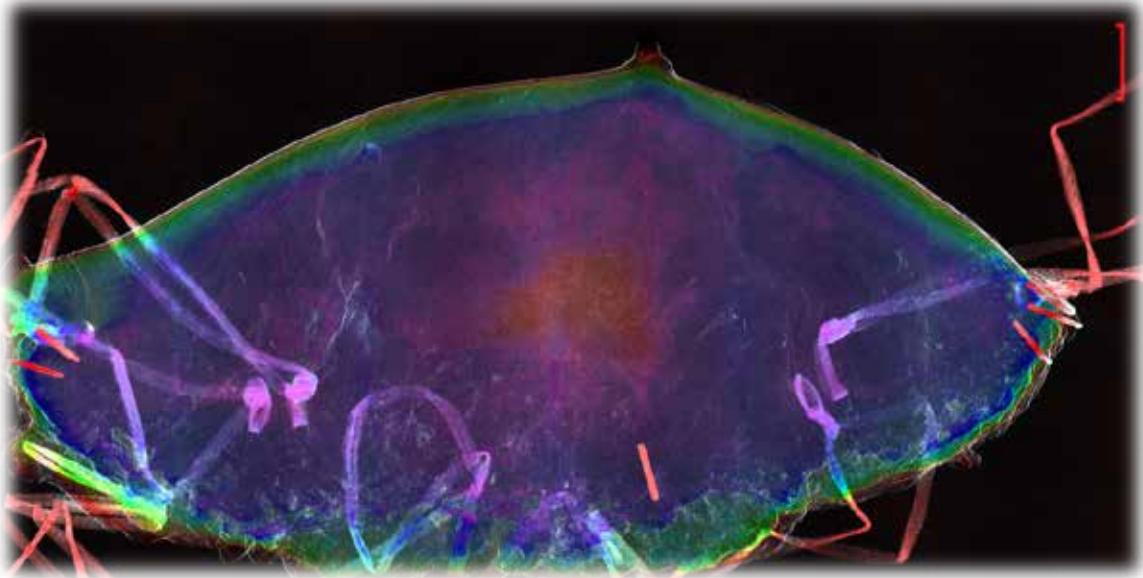
# Dark field signals...



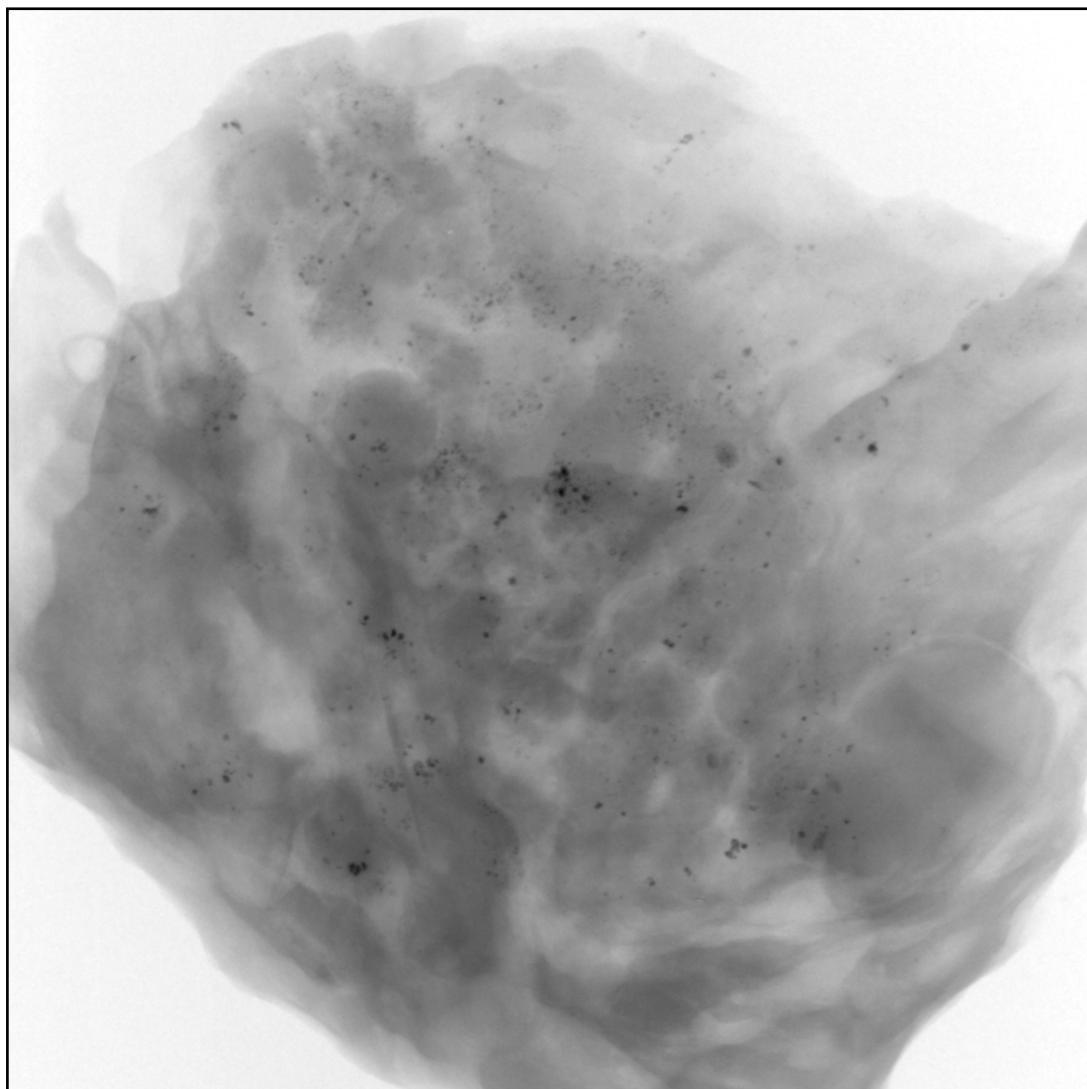
Absorption



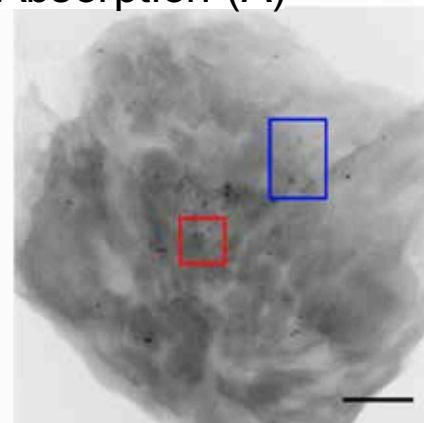
Scattering



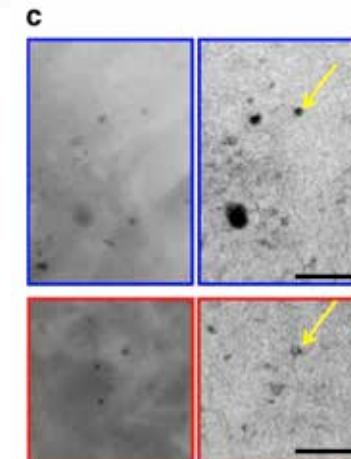
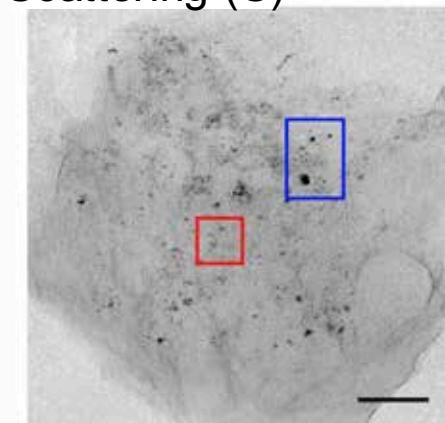
# Dark-field: the key for microcalcs discrimination?



Absorption (A)



Scattering (S)



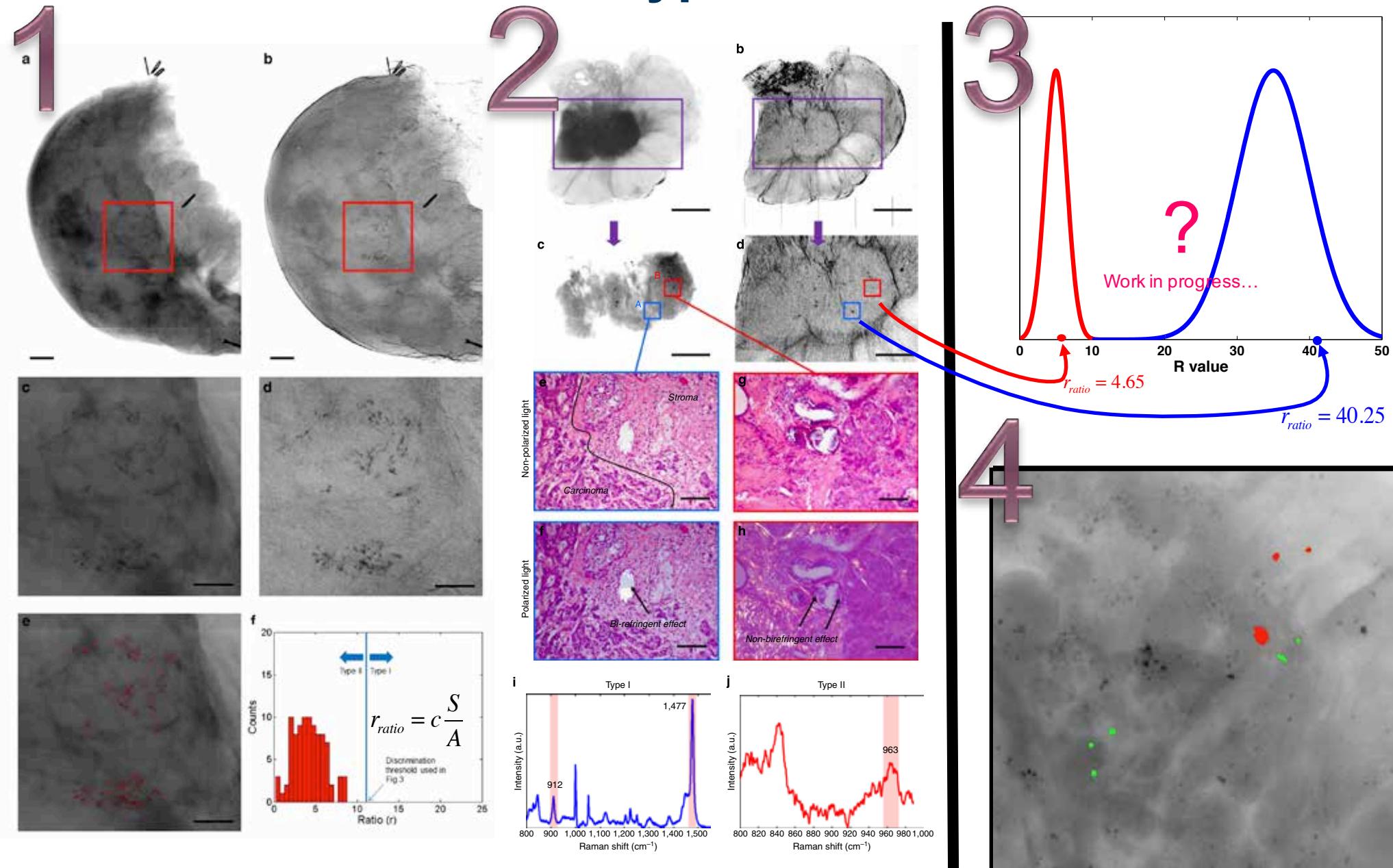
Observation: Opposite behaviors of A and S

Type I: calcium oxalate dehydrate,  $\text{CaC}_2\text{O}_4(2\text{H}_2\text{O})$

Type II: calcium hydroxyapatite,  $\text{Ca}_5(\text{PO}_4)_3(\text{OH})$

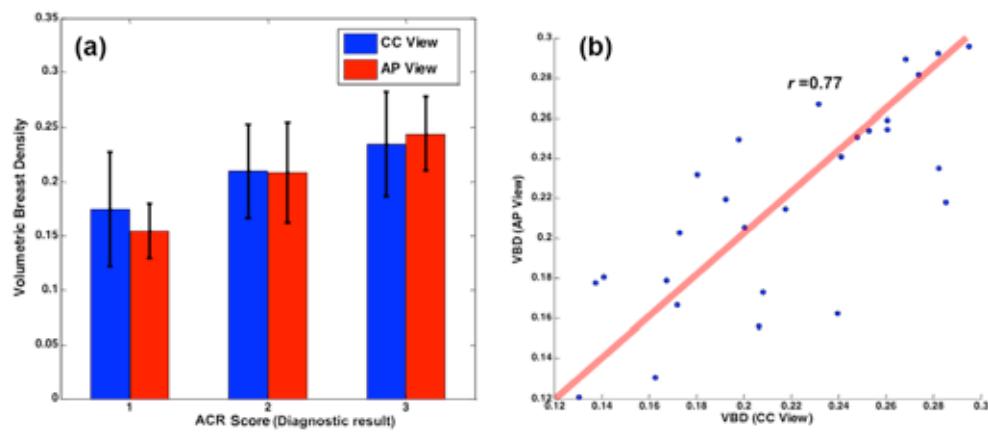
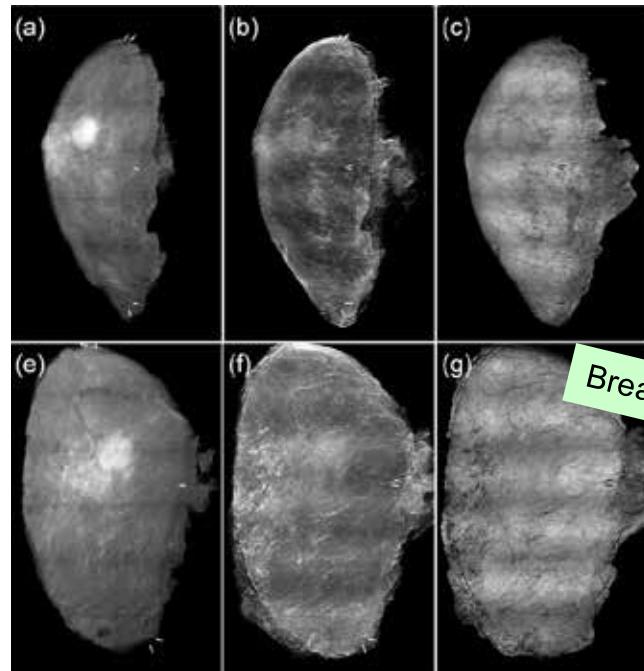
Can we discriminate between Type I (benign) and Type II (malignant) micro-calcifications *non-invasively* ?

# Our hypothesis

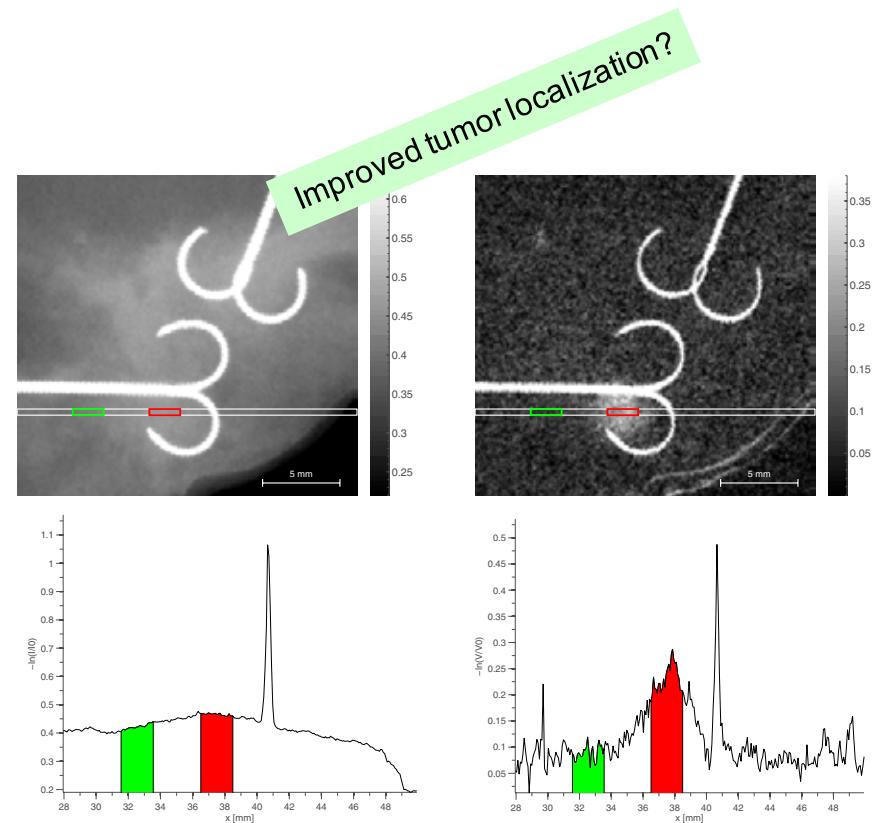


Z. Wang et al., Nat. Communications 5:3797 (2014)

# Dark-field signal: the key for improved diagnostic?

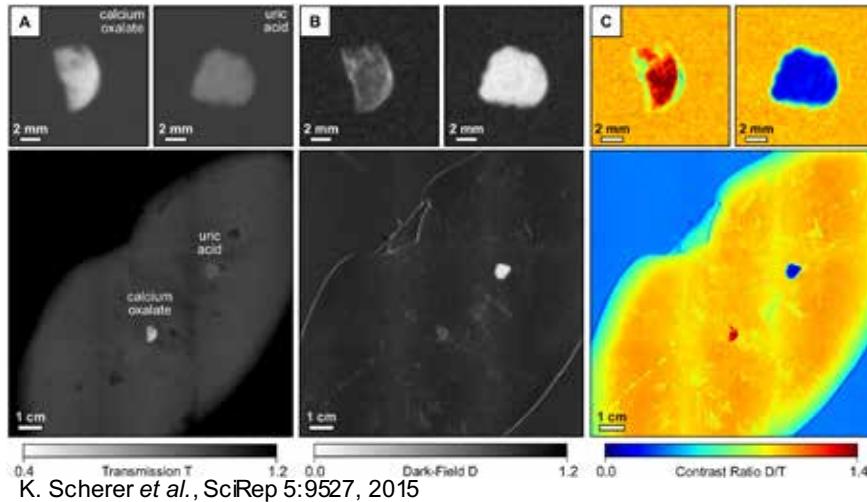


Wang et al, PMB 2015

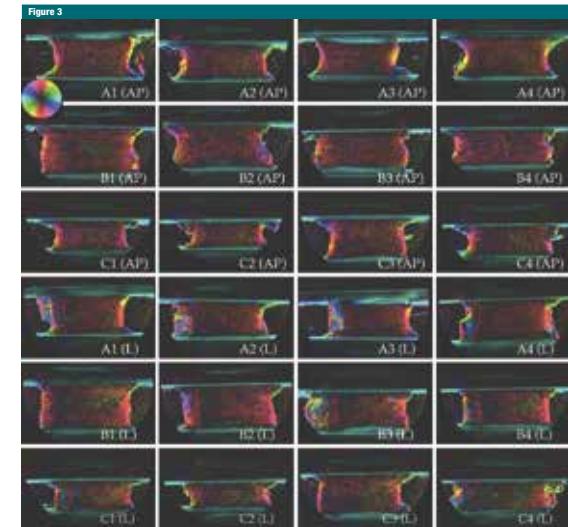


# Clinical applications of dark-field imaging

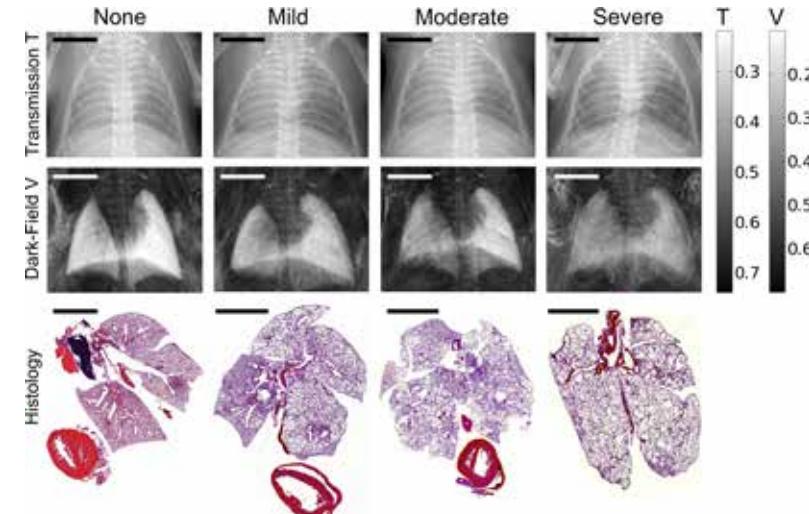
## Non-invasive kidney stone differentiation



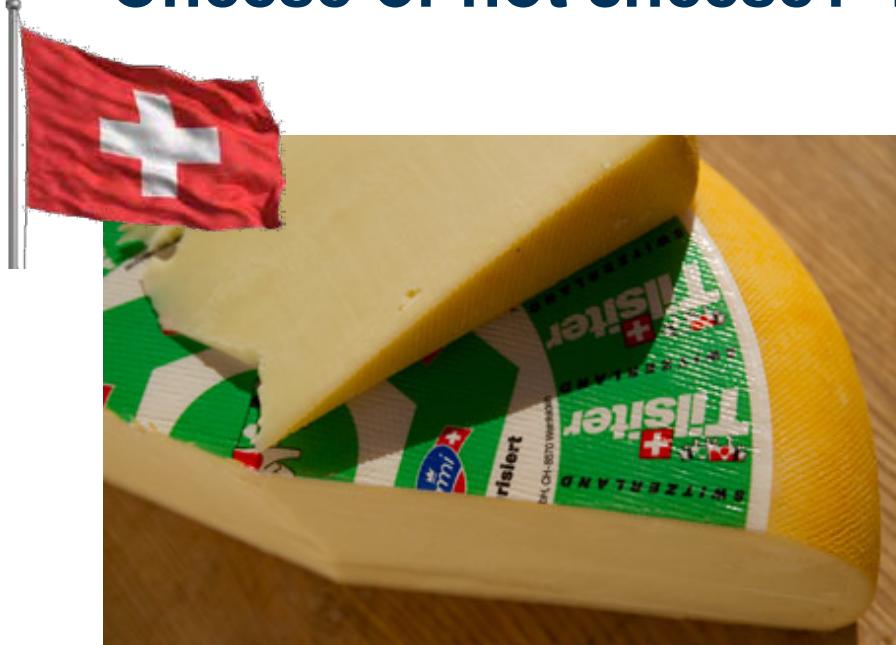
## Prediction of bone failure load with XVR



## Diagnosis and staging of pulmonary emphysema

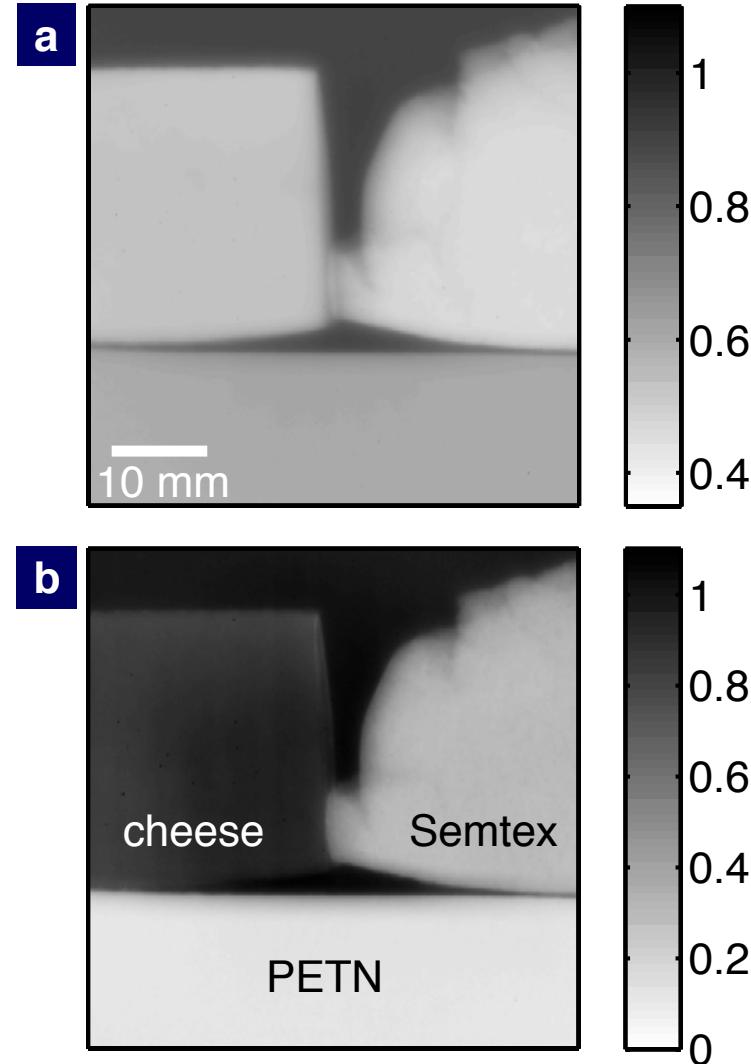


# Cheese or not cheese? That's the (homeland) problem



250g of SEMTEX are sufficient to fully destroy an airliner

F. Pfeiffer et al., Nature Methods, 7, 134 - 137 (2008)



Different granular microstructures distinguish high-performance explosives from good cheese...