

Biomedical Imaging - Nuclear imaging (I)

①

Rem: X-Rays $10\text{pm} \leq \lambda \leq 10\text{nm}$

γ -Rays $\lambda < 10\text{pm}$

Photon energy: $E_{\text{ph}} = h \cdot \nu = h \cdot \frac{c}{\lambda}$

Radiotracer - unstable isotopes

e.g. ^{18}F - FDG

(fluorodeoxyglucose)

- sugar analog

- uptake in energy-hungry cells \rightarrow brain example

H_2^{15}O

(radioactive water)

- freely diffusible,

- metabolically inert \rightarrow cardiac example

Radioactive nuclei

A - mass

Z ~~X~~

Z - number

$A < 50$ if $\#n = \#p$

$A \geq 50$ if $\#n > \#p$ then stable

otherwise unstable

Historical notes

1896 Béquerel

- Uranium

1898 Curie

- Radium

1911 Rutherford

- P,N,C

• α -Decay -



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Half Value Layer (HVL) $\sim 1\text{ mm}$

• β^- -Decay -



(Negation)

antineutrino

HVL

$\sim 4\text{ mm}$

• β^+ -Decay -



(Position)

neutrino

HVL

$\sim 4\text{ mm}$

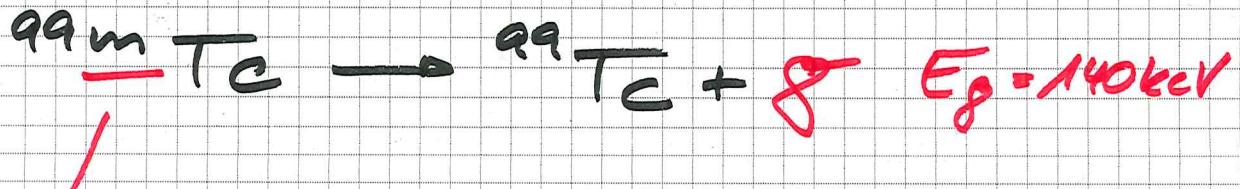
Biological half-life time

$$\cdot N(t_{1/2\text{eff}}) = \frac{N_0}{2} = N_0 e^{-(\lambda + \lambda_{\text{Bio}}) t_{1/2\text{eff}}}$$

$$\ln(2) = \left(\frac{\ln(2)}{t_{1/2}} + \frac{\ln(2)}{t_{1/2\text{Bio}}} \right) \cdot t_{1/2\text{eff}}$$

$$\boxed{t_{1/2\text{eff}} = \frac{t_{1/2\text{Bio}} \cdot t_{1/2}}{t_{1/2} + t_{1/2\text{Bio}}}}$$

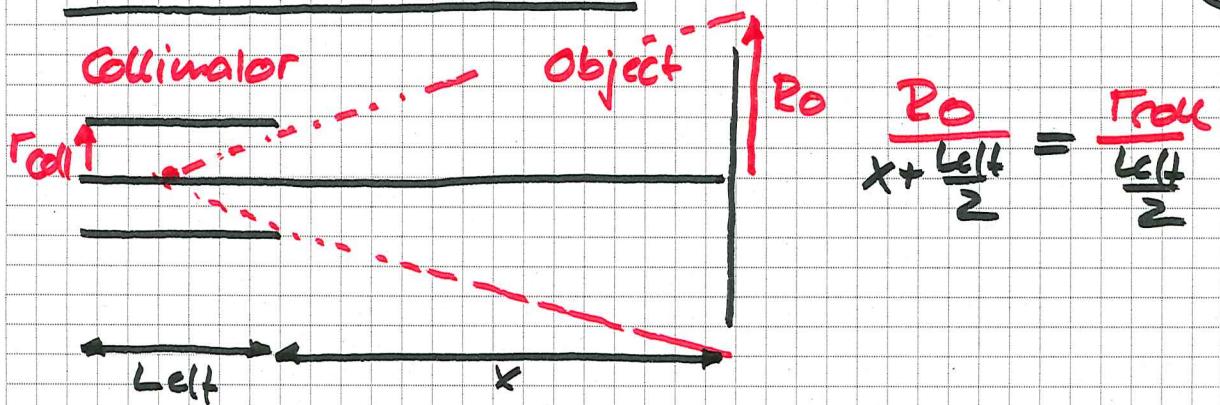
Radioisotopes



metastable = γ emission + internal conversion

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Collimation and PSF

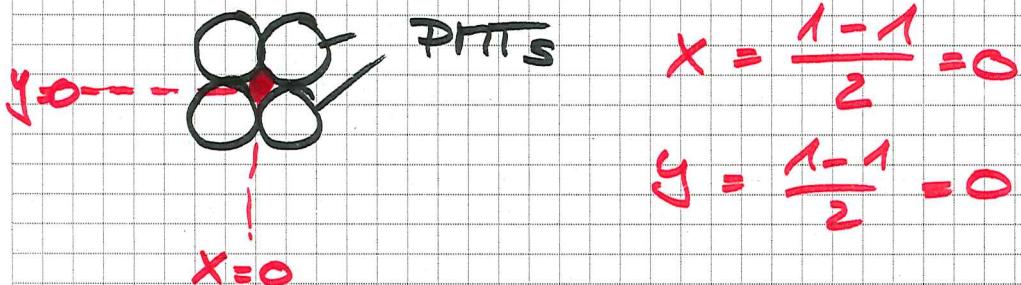


PSF

Full-width-at-half-maximum (FWHM)

$$\begin{aligned}
 \text{PSF}(x) &= \Delta r_{\text{col}}(x) = \left(\frac{R_o - r_{\text{col}} + r_{\text{col}}}{2} \right) \cdot 2 \\
 &= R_o + r_{\text{col}} = \frac{2r_{\text{col}}(x + \frac{Left}{2}) + Left}{Left} \\
 &= \frac{2r_{\text{col}}}{Left} x + 2r_{\text{col}} \boxed{= \frac{2r_{\text{col}}}{Left} (x + Left)}
 \end{aligned}$$

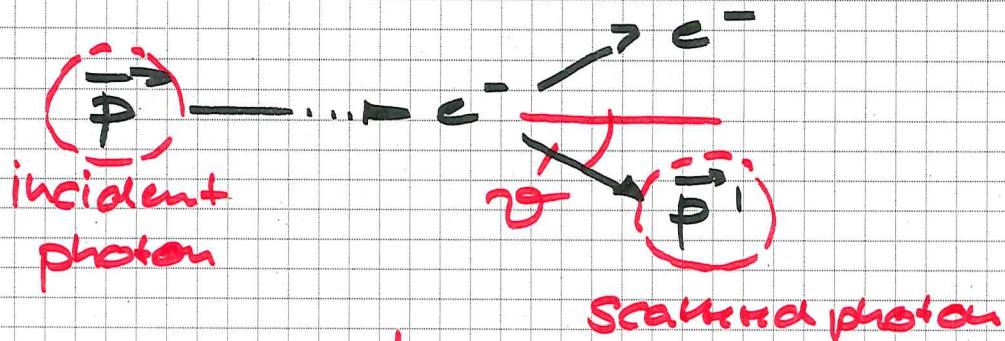
Positioning network



→ 4 PMTs determine location of event
- improved sensitivity + accuracy

Scatter detection

(K)

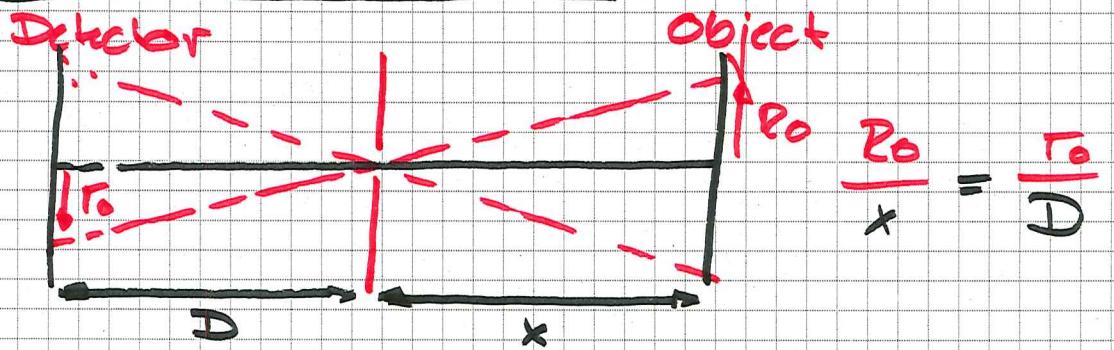


$$\lambda - \lambda' = \frac{h}{mc} (1 - \cos \theta)$$

$$\rightarrow |E - E' = h \cdot c \left(\frac{1}{\lambda} - \frac{1}{\lambda'} \right)|$$

→ Scattered photon have larger wavelength λ'
 A filter out

Pinhole collimation



Position emitters

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position

Half-life/min



annihilation

2 γ -photons (511 keV)

Coincidence detection

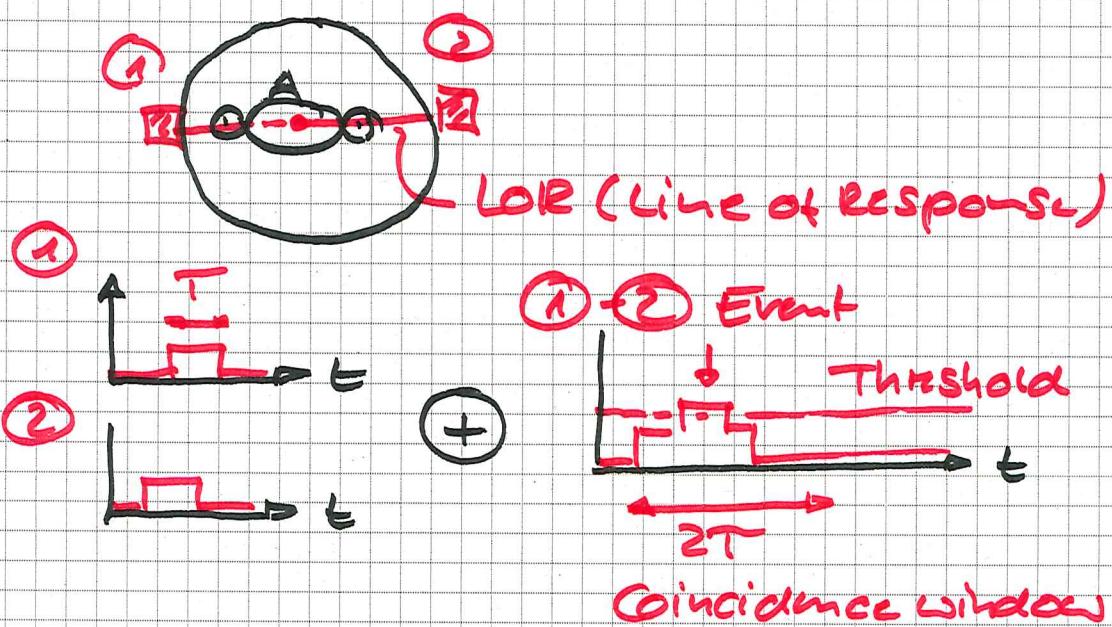


Image reconstruction

• Activity $S_0 = \int \text{act}(s) dS$

→ CT recon approach

⑥

Point - Spread function

- Activity in iso-centre

$$\text{FWHM} = \frac{\omega}{2}$$

ω ... detector width

- Activity off centre

$$\text{FWHM} = \omega \frac{r+x}{2r}$$

r ... radius detector ring

x ... off centre

Attenuation correction

- Activity + attenuation

$$S_p = \int \text{act}(s) \alpha s \cdot e^{-\int \mu(s) \alpha s}$$

Attenuation

due to Compton scatter

- Attenuation correction

- measure $\int \mu(s) \alpha s$ using e.g. CT

- convert $\mu_{CT} \rightarrow \mu_{Siemens}$

- multiply $S_p \cdot e^{\int \mu_{Siemens}(s) \alpha s}$

Attenuation correction