

## Part I : Sampling & quantization

1. Discretization of continuous signals
2. Signal representation in the frequency domain
3. Effects of sampling and quantization

## Part II : Image enhancement

1. Noise suppression
2. De-blurring
3. Contrast enhancement

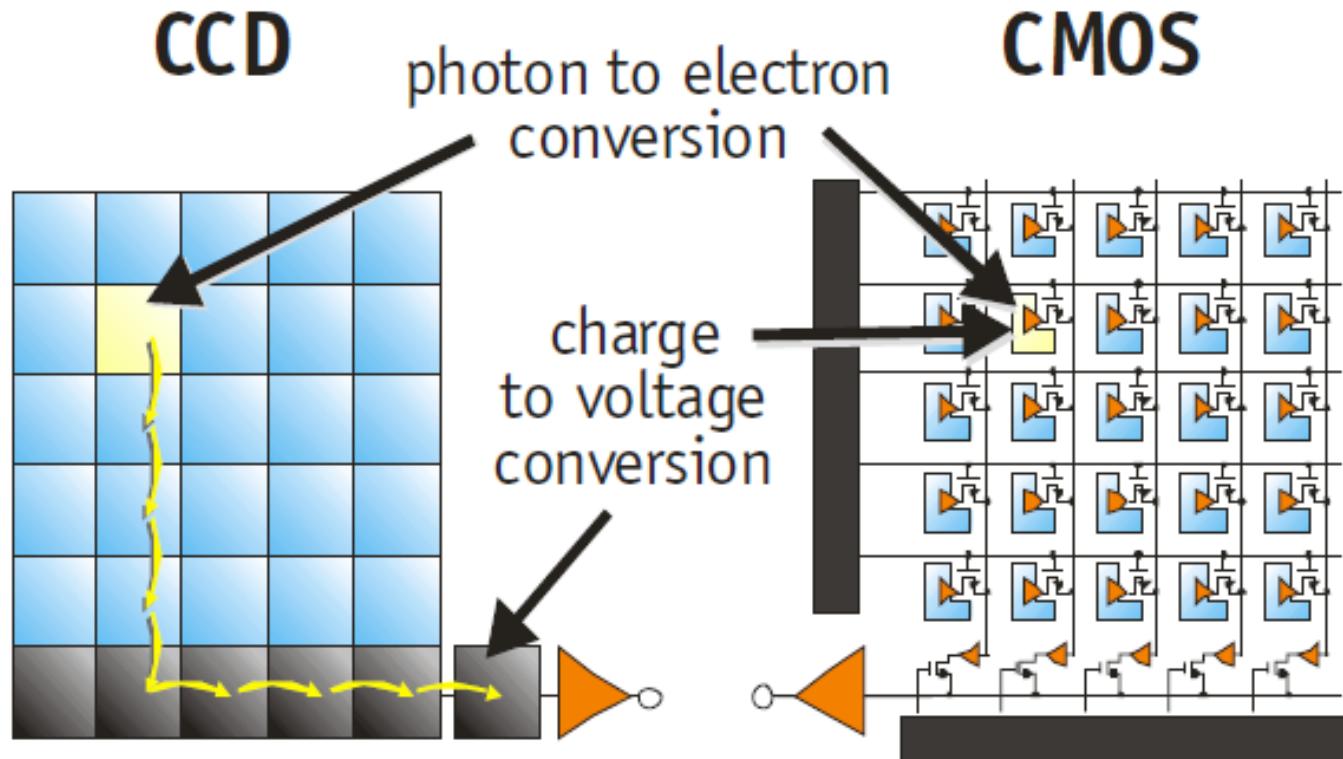


# Part I

# Sampling and

# Quantization

## Recall cameras



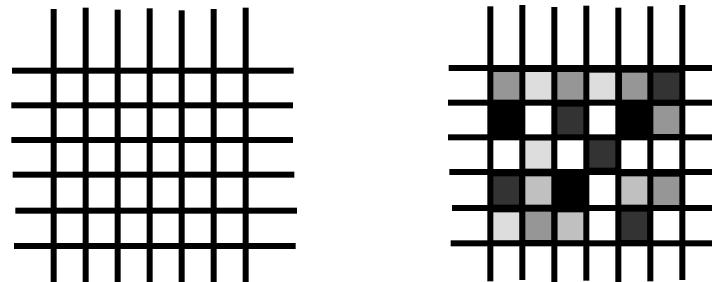
CCD = Charge-coupled device

CMOS = Complementary Metal Oxide Semiconductor

## Discretization

Computer to process an image :

1. sampling ▶ “pixels”
2. quantisation ▶ “grey levels”



# Sampling & quantization

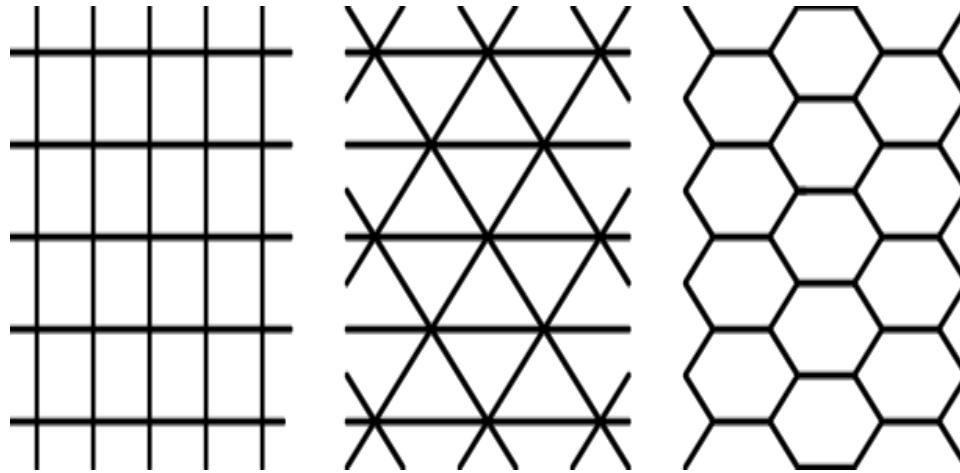


84 133 226 212 218 218 222 212 218 222 226 218  
75 156 177 218 212 218 218 218 218 218 222 218 218  
96 84 133 203 218 218 218 218 218 218 218 222 218  
123 75 111 156 212 218 212 212 218 218 218 226 218  
93 75 71 133 185 231 226 226 222 212 212 218 218  
51 75 75 75 156 206 218 218 218 218 222 212 218 218  
44 110 75 65 143 194 231 218 218 218 218 218 218 218  
52 123 69 84 60 156 199 231 231 231 222 226 226 226  
52 75 84 81 65 69 150 231 231 231 226 231 231 231  
36 36 84 93 84 71 156 160 240 240 240 231 231 231  
36 40 113 75 69 75 71 133 194 240 240 240 231 231  
52 52 105 85 69 75 75 123 111 222 231 231 231 231  
69 44 69 93 81 75 75 69 150 177 247 240 240 240  
73 44 40 96 101 75 75 75 84 133 231 240

## Sampling schemes

regular, image covering tessellation

11 with regular polygons ▶ 3 if equal



rectangular (square) most popular

hexagonal has advantages (more isotropic, no connectivity ambiguities, ...) + similar structure in retina



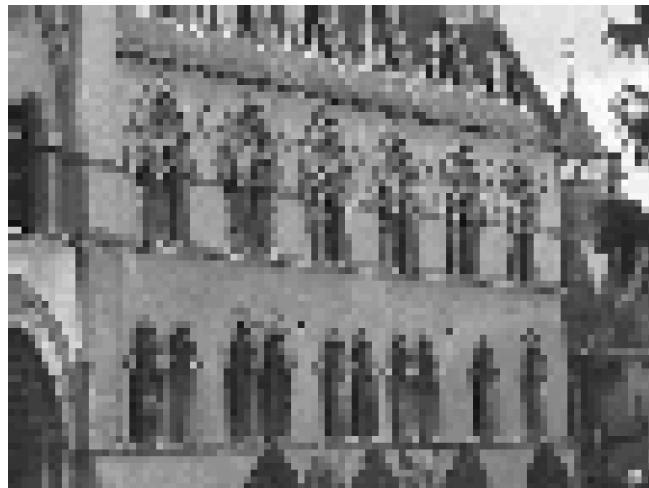
## Example of sampling :



384 x 288 pixels



192 x 144 pixels

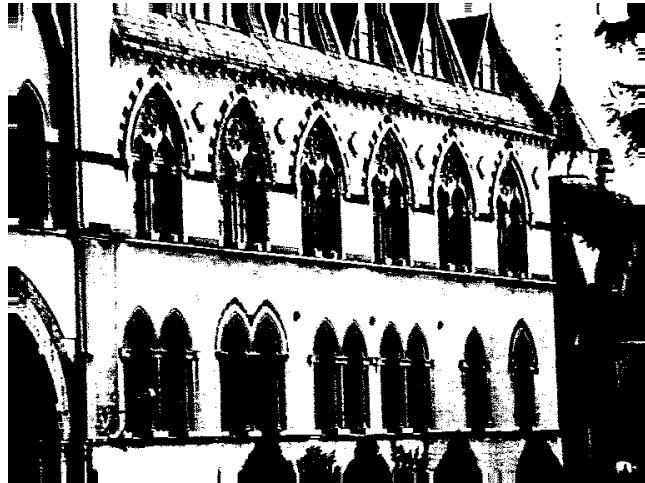


92 x 72 pixels



48 x 36 pixels

## Example of quantisation :



2 levels - binary



4 levels

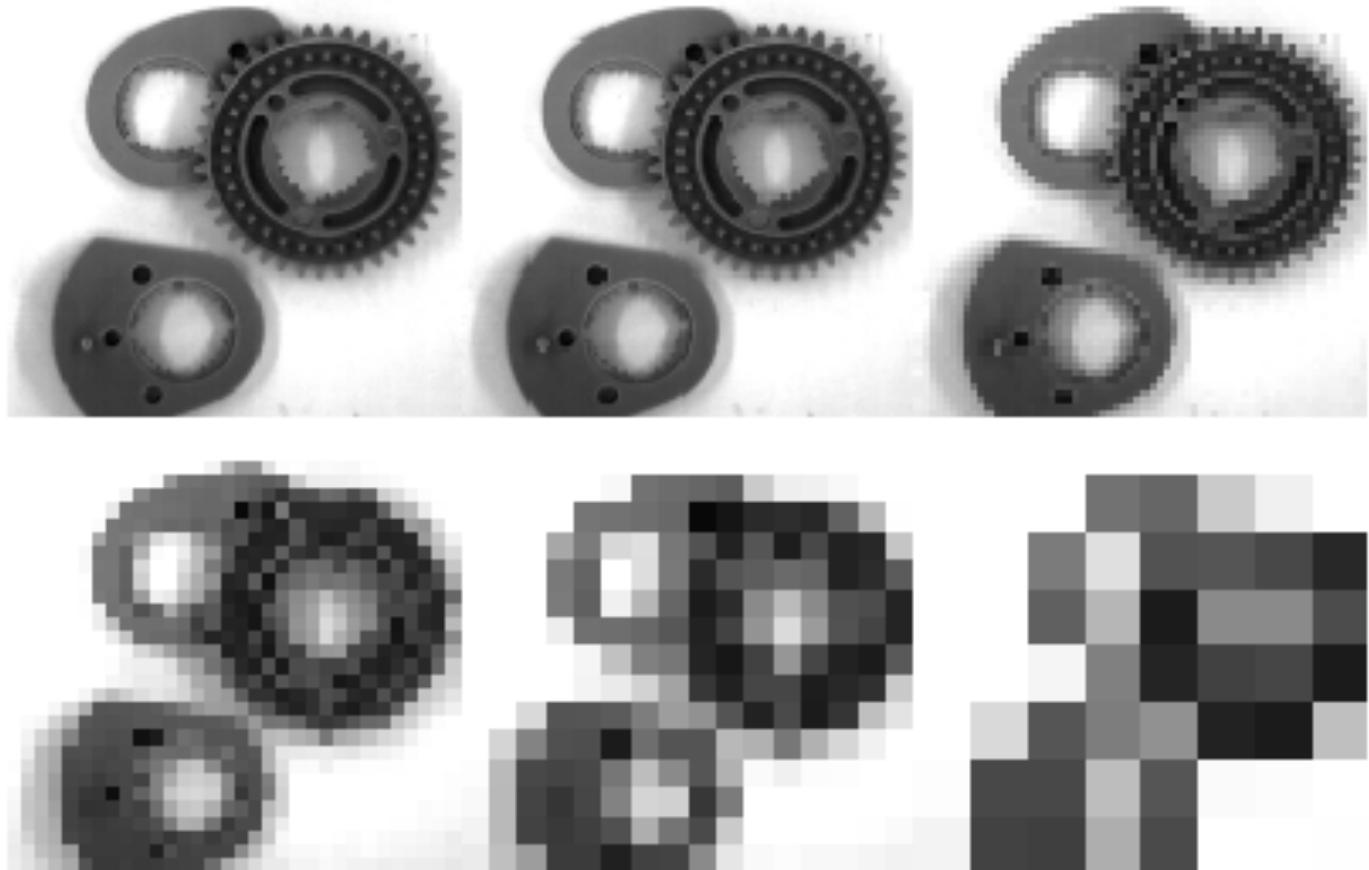


8 levels

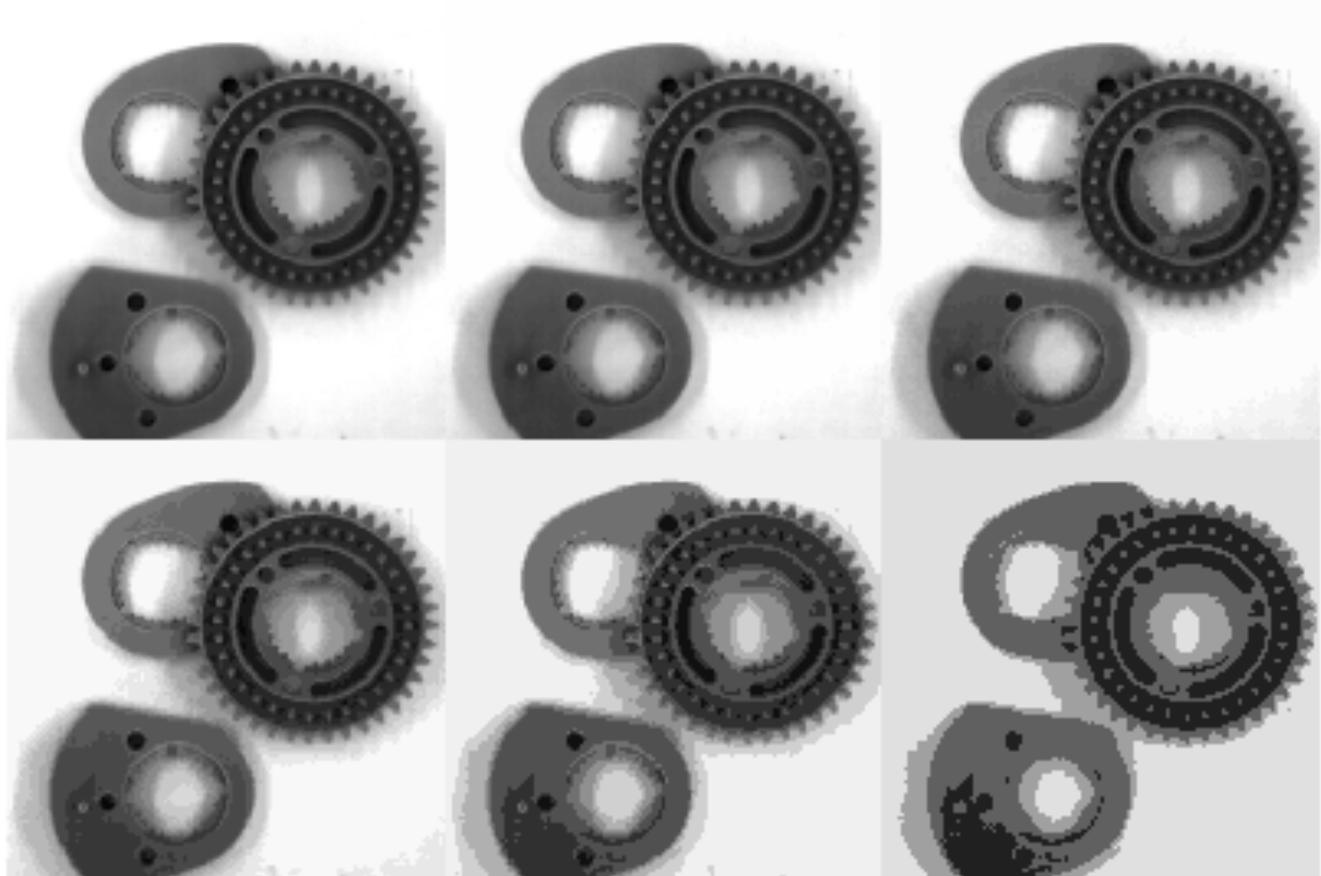


256 levels – 1 byte

## Image distortion through sampling



## Image distortion through quantisation



## Remarks

1. Binary images – 1-bit quantization – useful in industrial applications
2. Non-uniform sampling and/or quantization
  - a. fine sampling for details
  - b. fine quantization for homogeneous regions



## A model for sampling

1. Integrate brightness over cell window

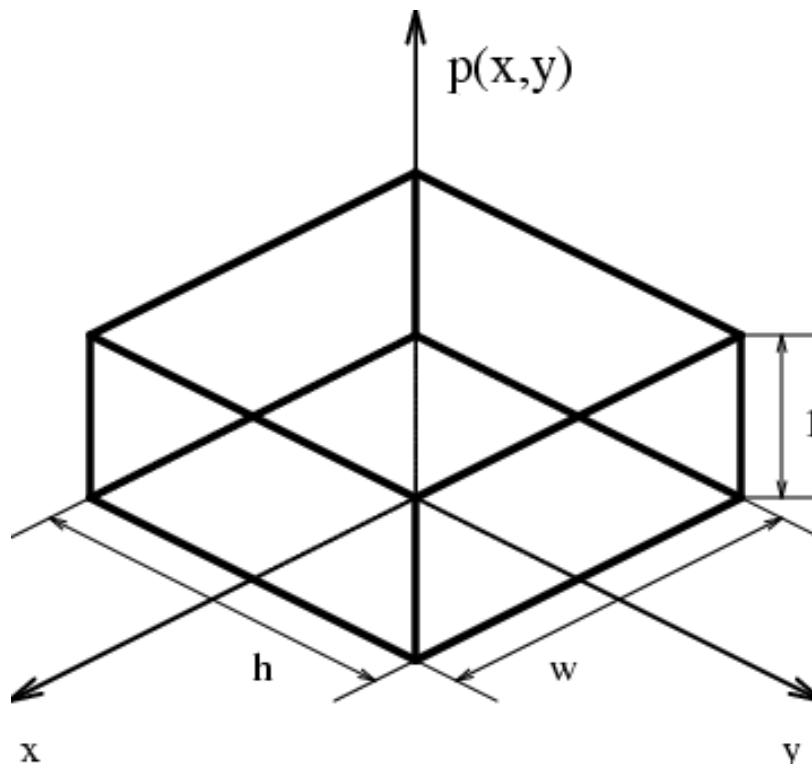
Image degradations

2. Read out values only at the pixel centers

Aliasing  
Leakage



## STEP 1 : integrating over a pixel cell

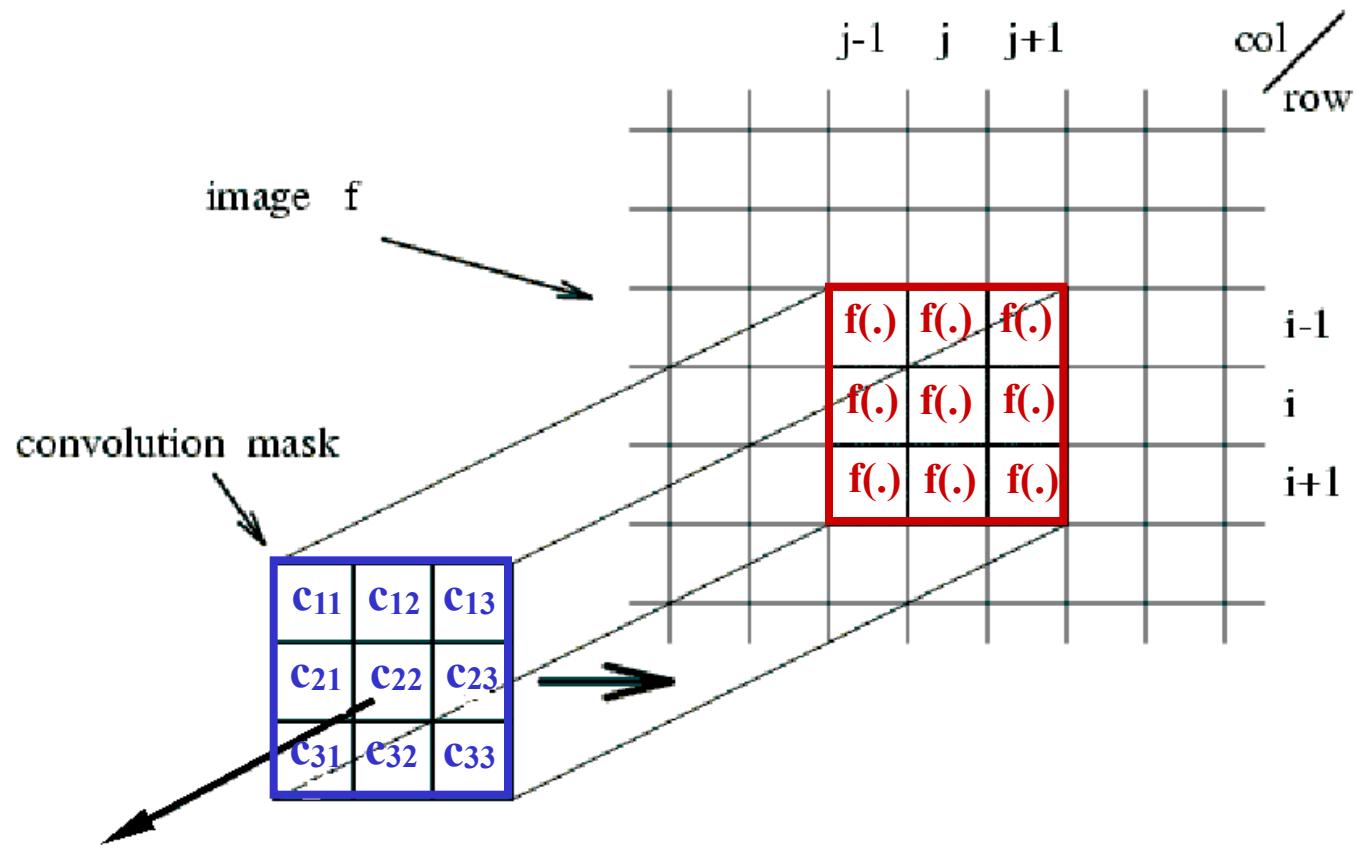


$$o(x', y') = \iint i(x, y) p(x - x', y - y') dx dy$$

This is a *convolution*:  $i(x, y) * p(-x, -y)$



# Convolution



$$o(i, j) = c_{11} f(i-1, j-1) + c_{12} f(i-1, j) + c_{13} f(i-1, j+1) + \\ c_{21} f(i, j-1) + c_{22} f(i, j) + c_{23} f(i, j+1) + \\ c_{31} f(i+1, j-1) + c_{32} f(i+1, j) + c_{33} f(i+1, j+1)$$



## Properties of convolution

$$f * g = g * f$$

$$\begin{aligned} k &= h * f \\ &= (h_1 * h_2) * f \\ &= h_1 * (h_2 * f) \end{aligned}$$



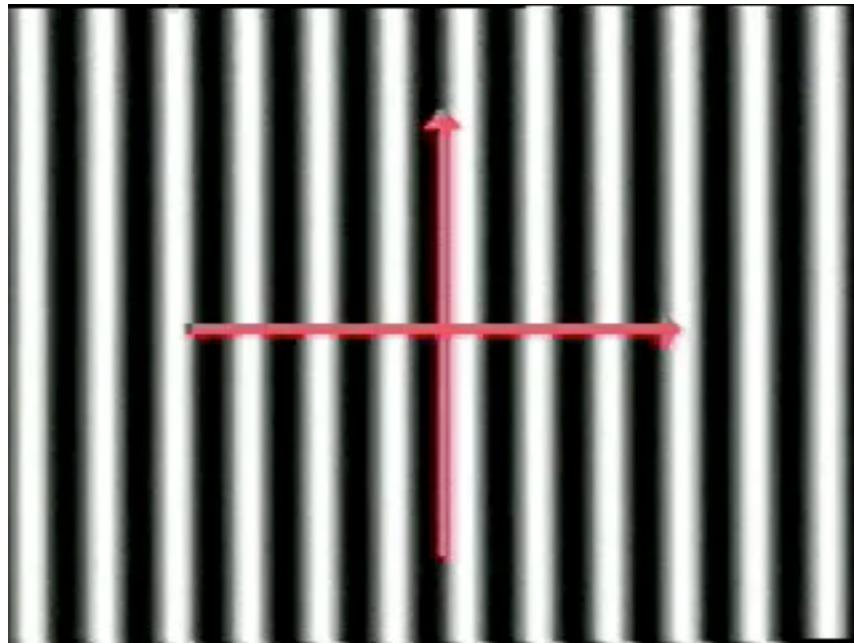
## Fourier transform

To understand the effect of the convolution in STEP 1 on the image



## Characterization of functions in the frequency domain

orthonormal basis functions  $e^{i2\pi(ux+vy)}$   
 $= \cos 2\pi(ux + vy) + i \sin 2\pi(ux + vy)$



$$\lambda = \frac{1}{\sqrt{u^2 + v^2}}$$

## The Fourier transform

Linear decomposition of functions in the new basis  
Scaling factor for basis function ( $u, v$ )

$$\mathcal{F}[f(x, y)] = F(u, v) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) e^{-i2\pi(ux+vy)} dx dy$$

→ **The Fourier transform**

Reconstruction of the original function in the spatial domain: weighted sum of the basis functions

$$\mathcal{F}^{-1}[F(u, v)] = f(x, y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} F(u, v) e^{i2\pi(ux+vy)} dx dy$$

→ **The inverse Fourier transform**

$$f(x, y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(\alpha, \beta) \delta(x - \alpha, y - \beta) d\alpha d\beta$$



## Fourier coefficients

$F(u, v)$  is complex :  $F_R(u, v) + iF_I(u, v)$

The magnitude

$$|F(u, v)| = \sqrt{F_R(u, v)^2 + F_I(u, v)^2}$$

The phase angle

$$\arctan(F_I(u, v) / F_R(u, v))$$

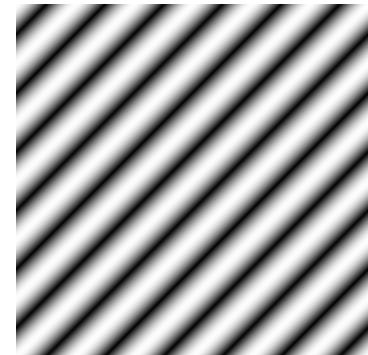
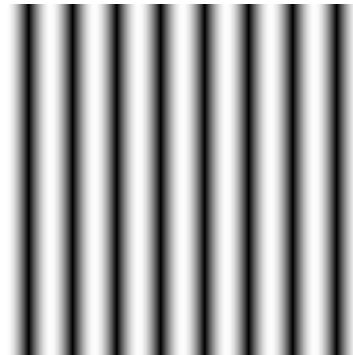
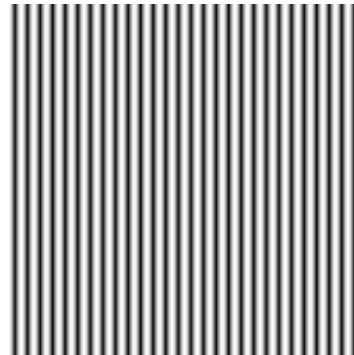


# Fourier decomposition of images

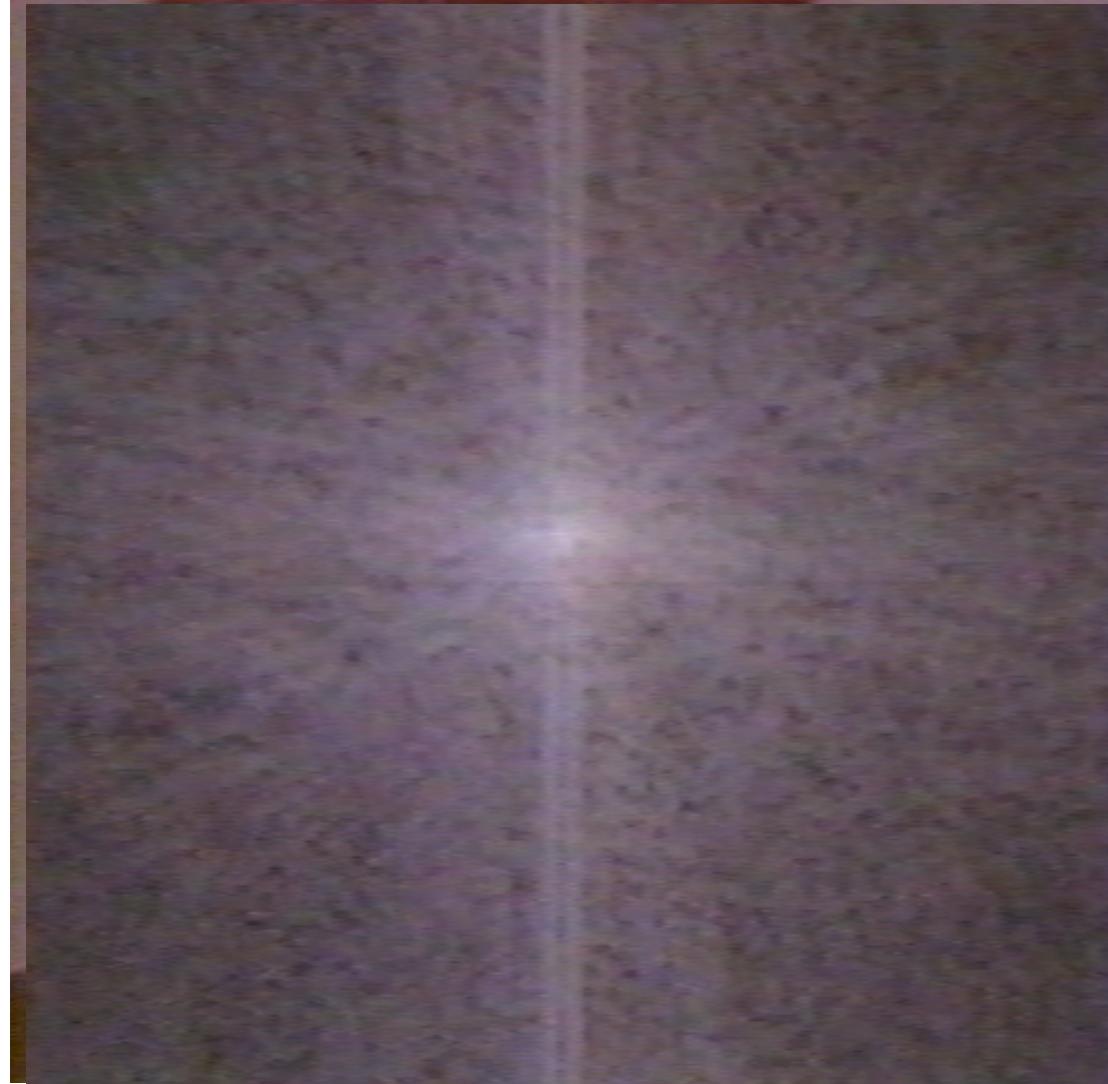
$$f(x,y) =$$



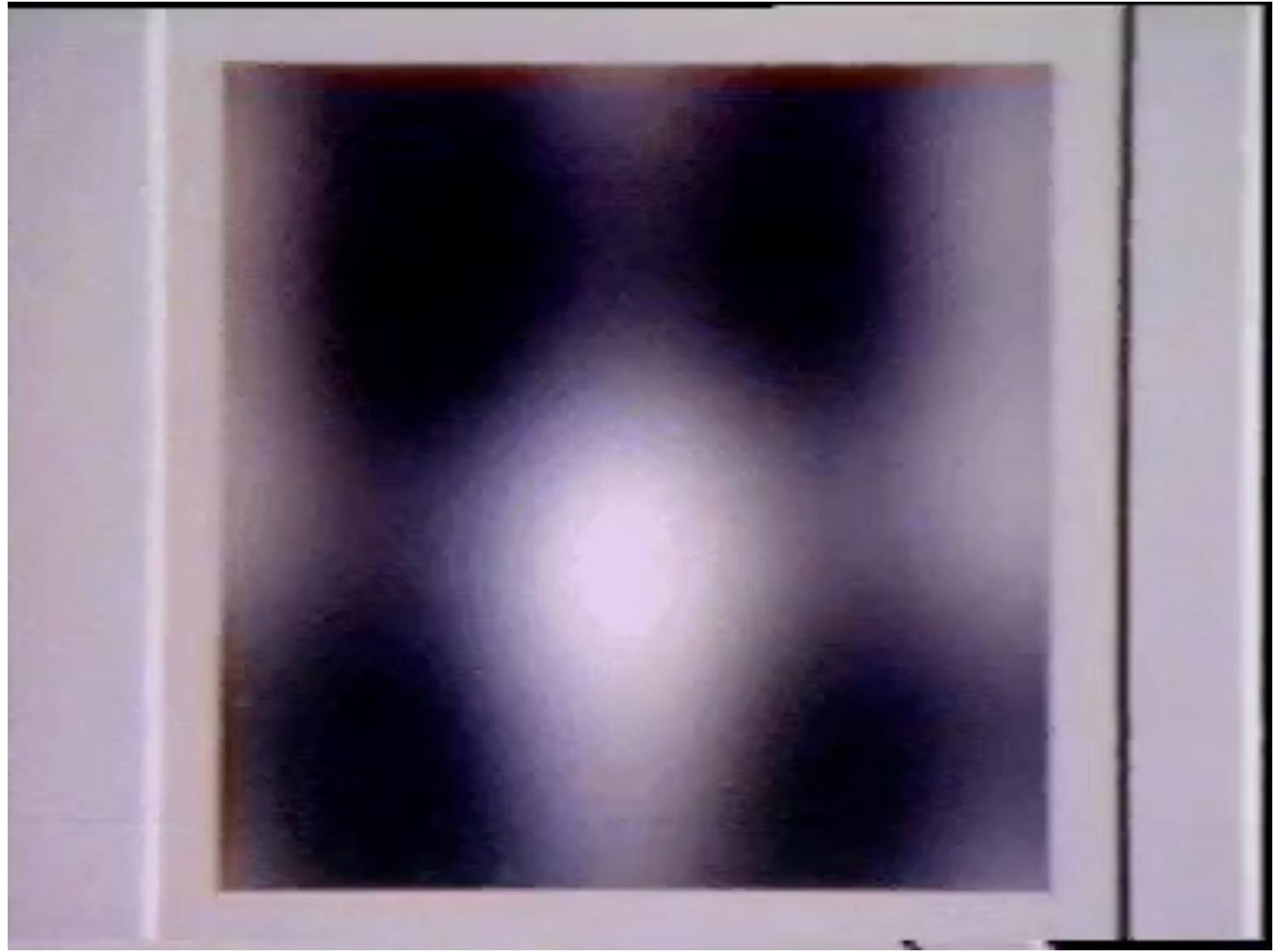
$$= \frac{F(u,v)}{\mathbf{X}} + \frac{F(u',v')}{\mathbf{X}} + \frac{F(u'',v'')}{\mathbf{X}} + \dots$$



# Fourier decomposition of images

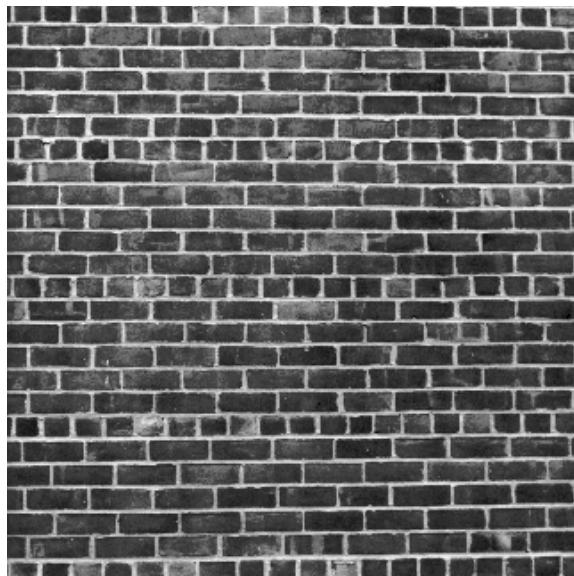


## Fourier decomposition of images

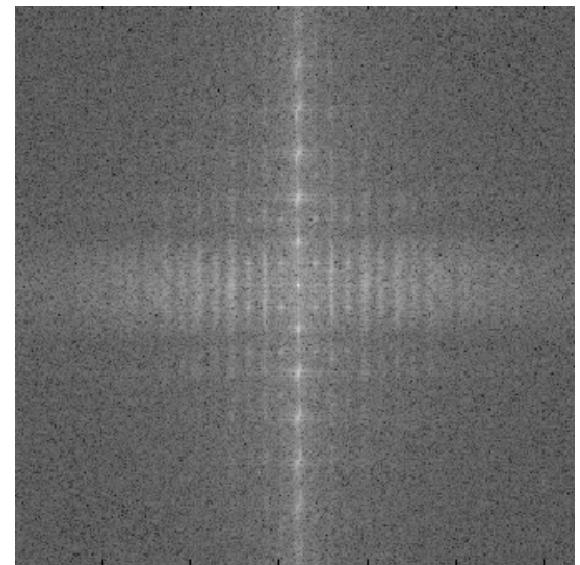


## Example importance of magnitude

- Image with periodic structure



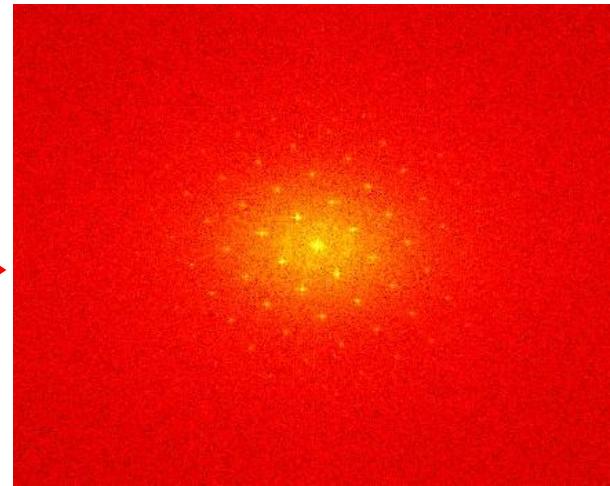
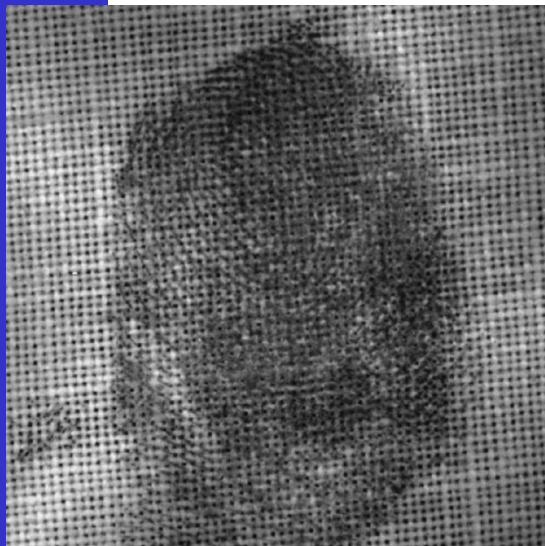
$$f(x,y)$$



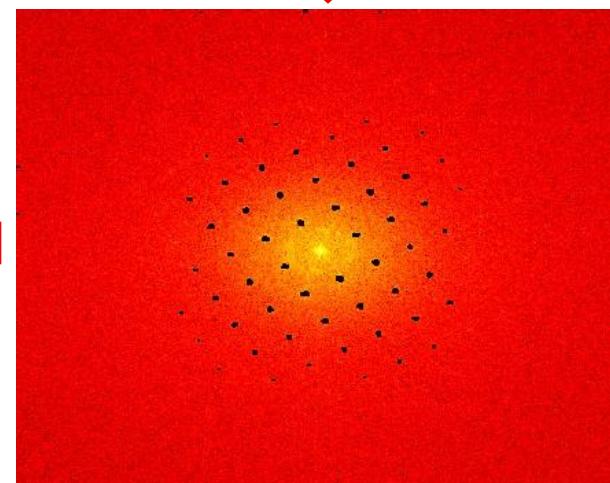
$$|F(u,v)|$$

FT has peaks at spatial frequencies of repeated texture

## Example importance of magnitude



$|F(u,v)|$



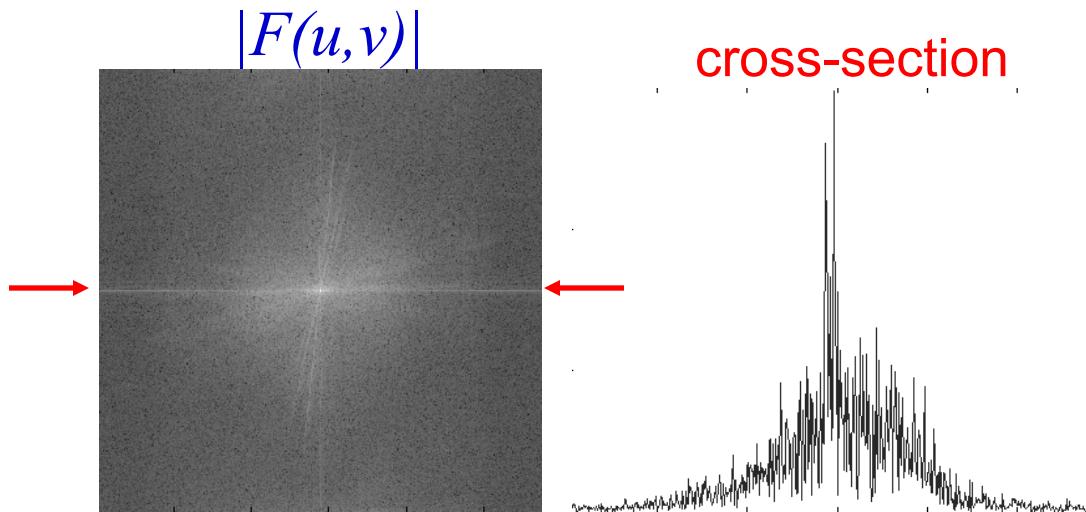
remove  
peaks

Periodic background removed

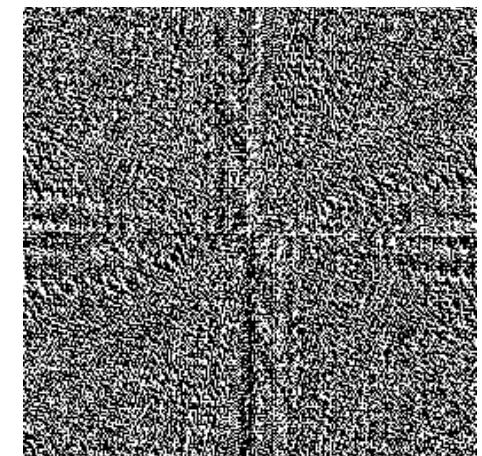
## Example importance of magnitude



$f(x,y)$



$|F(u,v)|$



- $|F(u,v)|$  generally decreases with higher spatial frequencies
- phase appears less informative

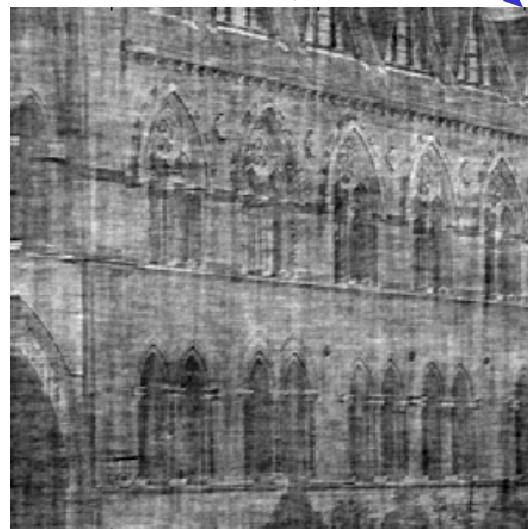
# The importance of the phase



phase

magnitude

phase



## The convolution theorem

$$c(x, y) = a(x, y) * b(x, y)$$

↓ Fourier

$$C(u, v) =$$

$$\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} [a(x, y) * b(x, y)] e^{-i2\pi(ux+vy)} dx dy$$

$$\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \left[ \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} a(x-\alpha, y-\beta) b(\alpha, \beta) d\alpha d\beta \right] e^{-i2\pi(ux+vy)} dx dy$$

$$\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \left[ \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} a(x-\alpha, y-\beta) e^{-i2\pi(ux+vy)} dx dy \right] b(\alpha, \beta) d\alpha d\beta$$



## The convolution theorem

$$\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \left[ \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} a(x-\alpha, y-\beta) e^{-i2\pi(ux+vy)} dx dy \right] b(\alpha, \beta) d\alpha d\beta$$

$$\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \left[ \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} a(x^*, y^*) e^{-i2\pi(u(x^*+a)+v(y^*+b))} dx^* dy^* \right] b(\alpha, \beta) d\alpha d\beta$$

$$\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \left[ \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} a(x^*, y^*) e^{-i2\pi(ux^*+vy^*)} dx^* dy^* \right] e^{-i2\pi(ua+vb)} b(\alpha, \beta) d\alpha d\beta$$

That is,

$$\begin{aligned} & \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} A(u, v) e^{-i2\pi(u\alpha+v\beta)} b(\alpha, \beta) d\alpha d\beta \\ &= A(u, v) B(u, v) \end{aligned}$$

Space convolution = frequency multiplication



## Point spread function and Modulation transfer function

$$\begin{aligned} O(u, v) &= \mathcal{F}\{o(x, y)\} \\ &= \mathcal{F}\{i(x, y) * r(x, y)\} \\ &= I(u, v)R(u, v) \end{aligned}$$

$$\begin{aligned} R(u, v) &= \mathcal{F}\{r(x, y)\} \\ &= \mathcal{F}\{\text{point spread function}\} \end{aligned}$$

**= modulation transfer function**



## The convolution theorem: reciprocity

$$\begin{aligned} C(u, v) &= A(u, v)B(u, v) \\ c(x, y) &= a(x, y) * b(x, y) \end{aligned}$$

$$\begin{aligned} C(u, v) &= A(u, v) * B(u, v) \\ c(x, y) &= a(x, y)b(x, y) \end{aligned}$$

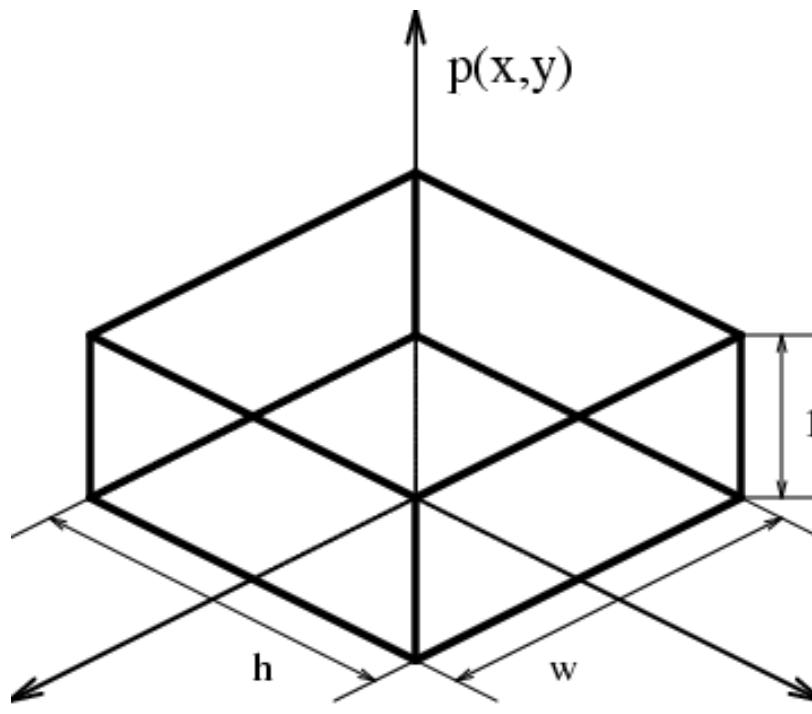
Space multiplication = frequency convolution



Back to STEP 1



## STEP 1 : integrating over a pixel cell



$$o(x', y') = \iint i(x, y) p(x - x', y - y') dx dy$$

This is *convolution*:  $i(x, y) * p(-x, -y)$

$$O(u, v) = I(u, v)P(u, v)$$



# Modulation Transfer Function of the window function

Fourier transform of window :

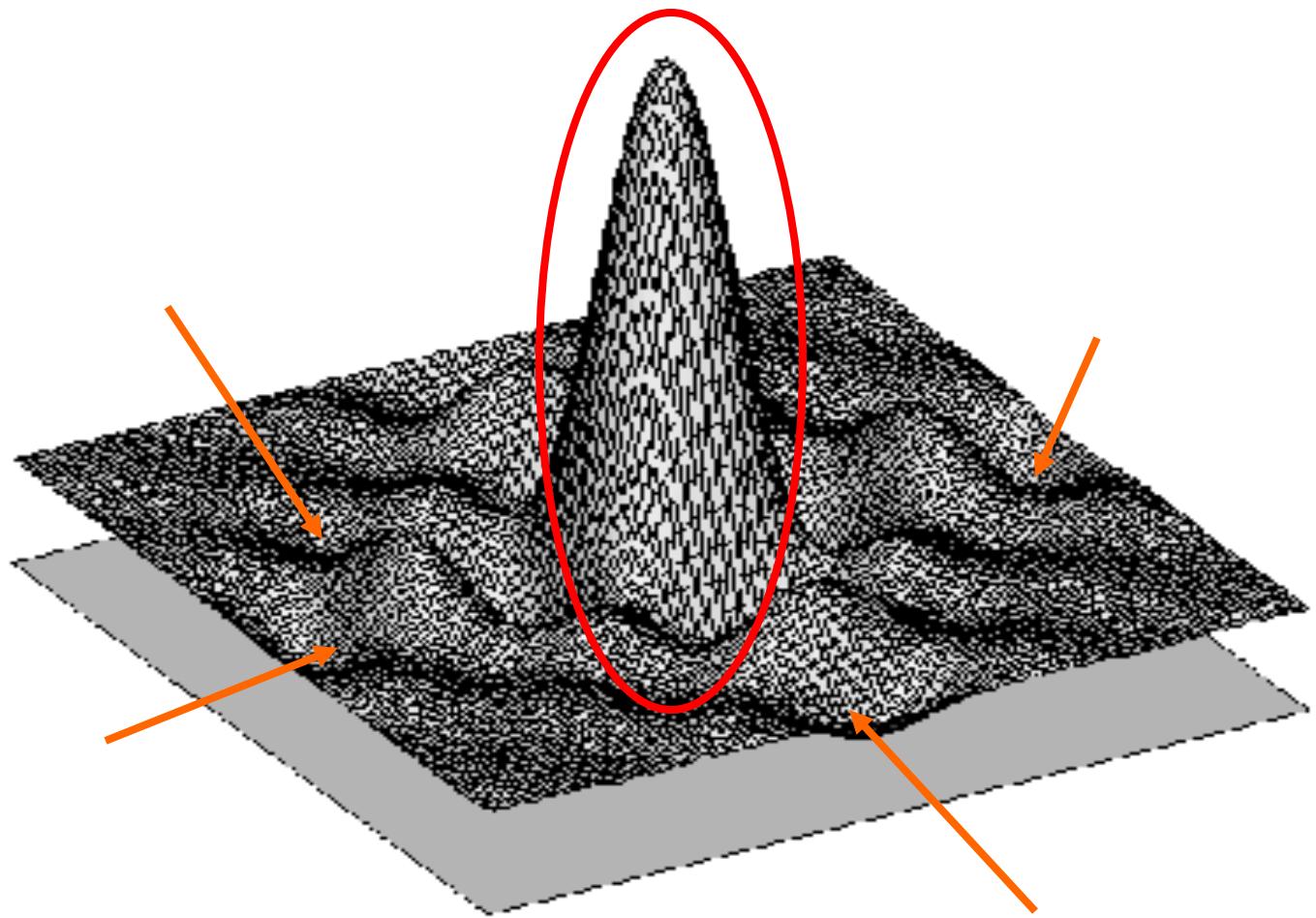
$$\begin{aligned} P(u, v) &= \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} e^{-i2\pi(ux+vy)} p(x, y) dx dy \\ &= \int_{-w/2}^{w/2} e^{-i2\pi ux} dx \int_{-h/2}^{h/2} e^{-i2\pi vy} dy \\ &= \left[ \frac{e^{-i2\pi ux}}{-i2\pi u} \right]_{-w/2}^{w/2} \left[ \frac{e^{-i2\pi vy}}{-i2\pi v} \right]_{-h/2}^{h/2} \\ &= -\frac{1}{4\pi^2 uv} \left( -2i \sin\left(2\pi u \frac{w}{2}\right) \right) \left( -2i \sin\left(2\pi v \frac{h}{2}\right) \right) \\ &= wh \left( \frac{\sin \pi w u}{\pi w u} \right) \left( \frac{\sin \pi h v}{\pi h v} \right) \end{aligned}$$



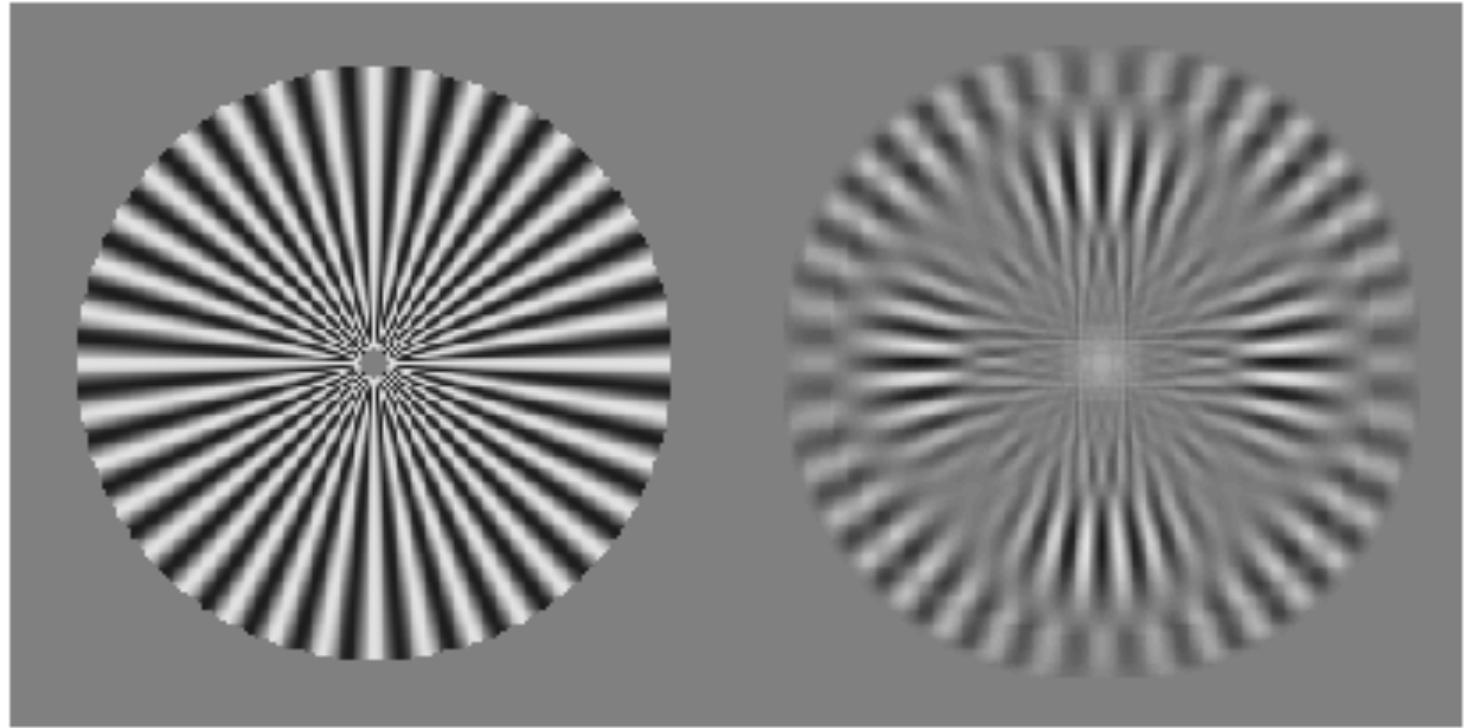
## Fourier transform of the window function

2D sinc :

real  $\rightarrow$  no phase shifts !  
however, periodic repetitions !



## Illustration of the sinc



$$P(u, v) = wh \left( \frac{\sin \pi w u}{\pi w u} \right) \left( \frac{\sin \pi h v}{\pi h v} \right)$$



## A model for sampling

1. Integrate brightness over cell window

Image degradations

2. Read out values only at the pixel centers

Aliasing  
Leakage

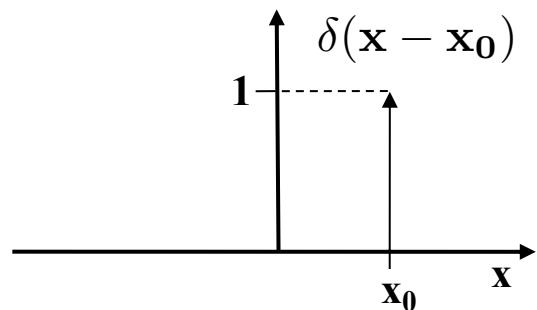


## STEP 2: local probing of functions

Distributions as extension of functions: the Dirac pulse

$$\delta(\mathbf{x} - \mathbf{x}_0) = 0 \quad \mathbf{x} \neq \mathbf{x}_0$$

$$\int_{-\infty}^{\infty} \dots \int_{-\infty}^{\infty} \delta(\mathbf{x} - \mathbf{x}_0) d\mathbf{x} = 1$$



Function probing (in 1D)

$$\int_{-\infty}^{\infty} \delta(x) f(x) dx = f(0)$$

$$\int_{-\infty}^{\infty} \delta(x - x_0) f(x) dx = f(x_0)$$



Discretization in the spatial domain  
is multiplication with a Dirac train

multiplication with 2D pulse train

$$\sum_{k=-\infty}^{\infty} \sum_{l=-\infty}^{\infty} \delta(x - kw, y - lh)$$

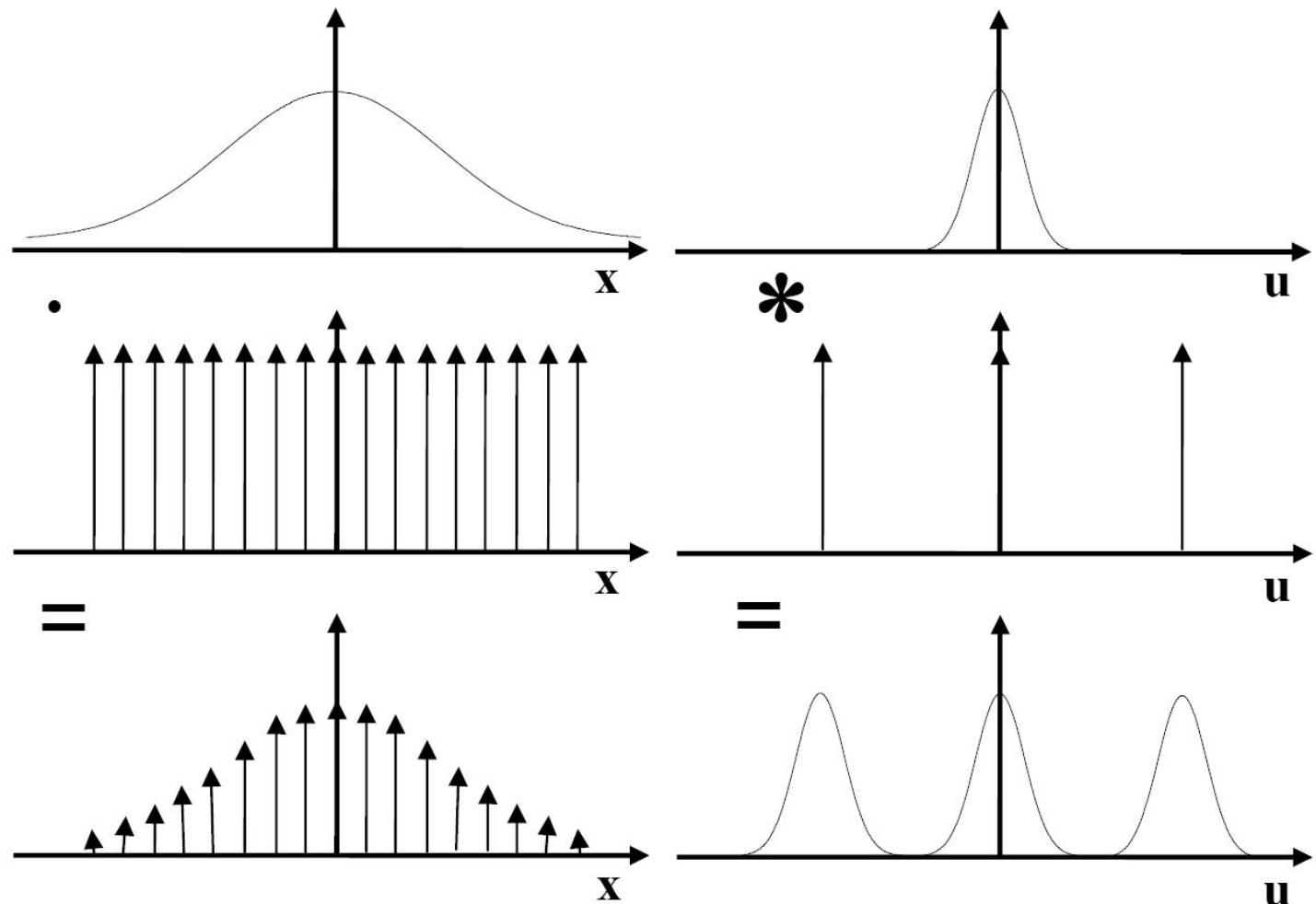
Fourier transform :

$$\frac{1}{wh} \sum_{k=-\infty}^{\infty} \sum_{l=-\infty}^{\infty} \delta(x - k \frac{1}{w}, y - l \frac{1}{h})$$

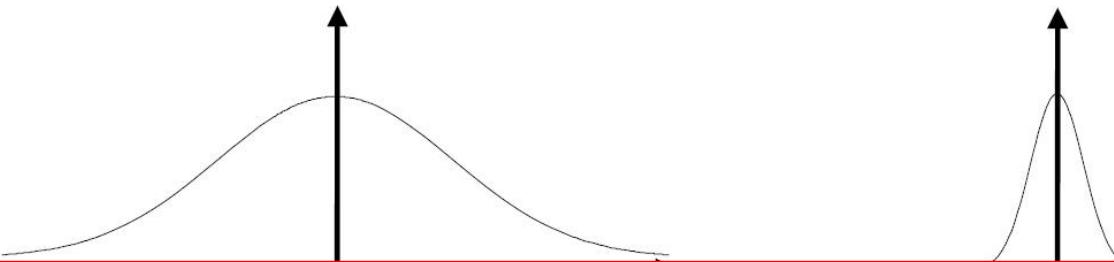
Convolution with a Dirac train: periodic repetition  
Yet another duality: discrete vs. periodic



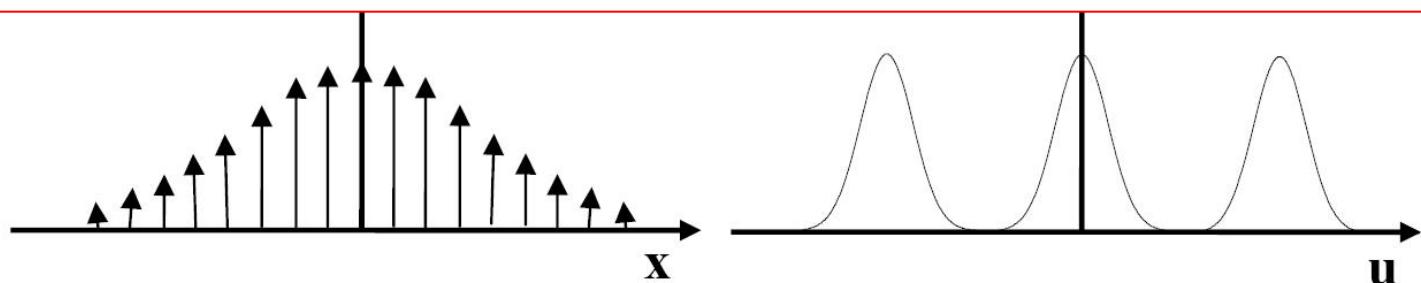
## Effect on the frequency domain



## Effect on the frequency domain



1. After sampling you may not get back the original signal
2. It depends on the frequency domain representation, only band limited signals can be sampled and retrieved back
3. Even then you need to sample at a certain rate



## The sampling theorem

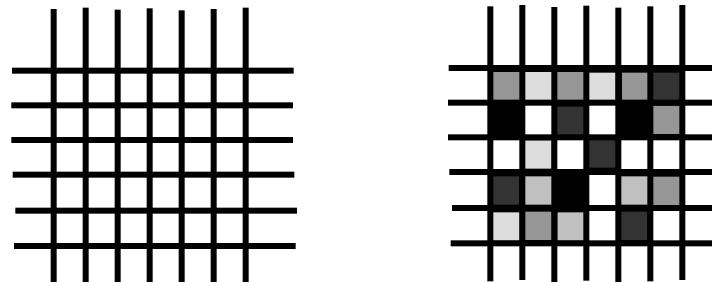
If the Fourier transform of a function  $f(x,y)$  is zero for all frequencies beyond  $u_b$  and  $v_b$ , i.e. if the Fourier transform is *band-limited*, then the continuous periodic function  $f(x,y)$  can be completely reconstructed from its samples as long as the sampling distances  $w$  and  $h$  along the  $x$  and  $y$  directions are such that  $w \leq \frac{1}{2u_b}$  and  $h \leq \frac{1}{2v_b}$



## Discretization

Computer to process an image :

1. sampling ▶ “pixels”
2. quantisation ▶ “grey levels”



## Quantisation

Create K intervals in the range of possible intensities measured in bits:  $\log_2(K)$

Design choices

- Decision levels

$$z_1, z_2, \dots, z_{K+1}$$

- Representative value

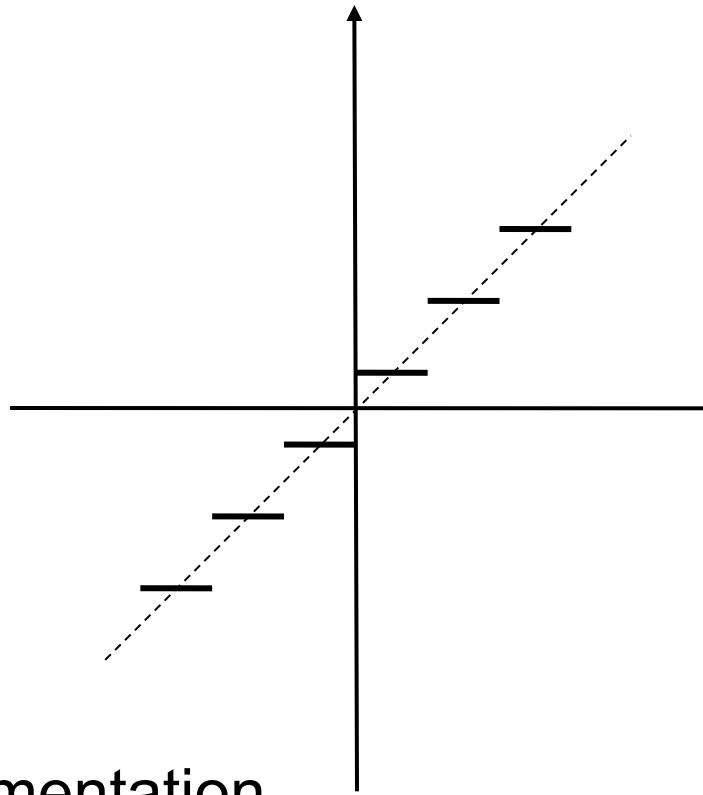
$$\text{interval } [z_k, z_{k+1}] \rightarrow q_k$$

- Simplest selection

- equal intervals
  - value is the mean
  - $\Delta$  uniform quantizer



# The uniform quantizer



- simple implementation
- fine quantization needed perceptually (7-8 bits)
- can be reduced by optimal design, e.g.

$$\text{minimize } \delta = \sum_{k=1}^K \int_{z_k}^{z_{k+1}} (z - q_k)^2 p(z) dz := \sum_{k=1}^K \delta_k$$

( $p(z)$ =prob. density function, for constant  $\Delta$  uniform)



## Underquantization example

256 gray level (8 bit)



11 gray level



## Remarks

- Quantization:
  - Often 8 bits per pixel (monochrome),  
24 bits per pixel (RGB)
  - Medical images 12 bits (4096 levels) or 16 bits  
(65536 levels)

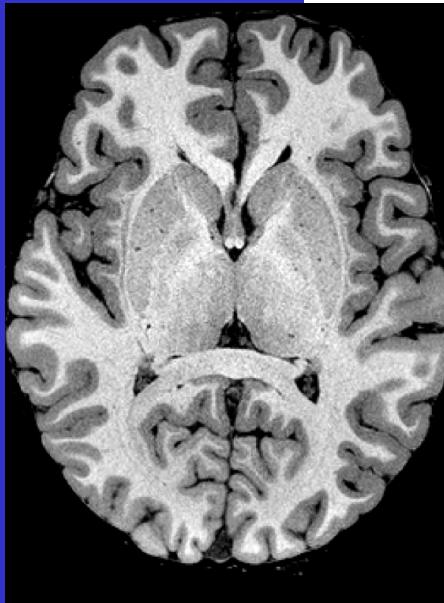


# Part II

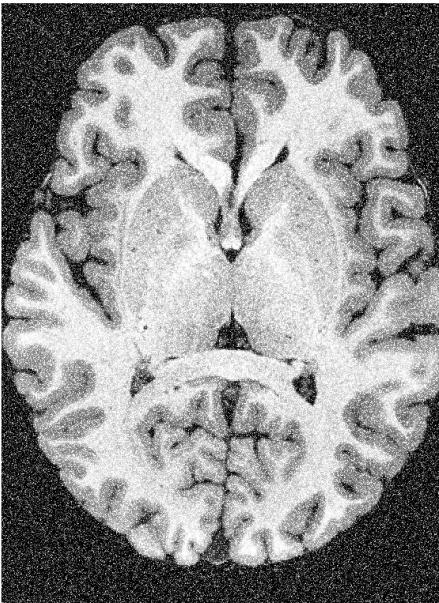
# Image Enhancement

## Three types of image enhancement

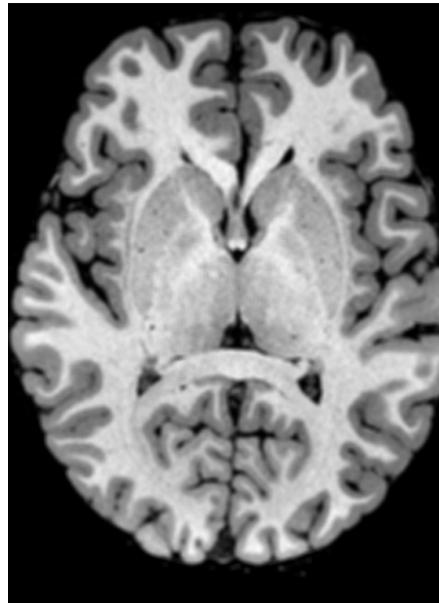
1. Noise suppression
2. Image de-blurring
3. Contrast enhancement



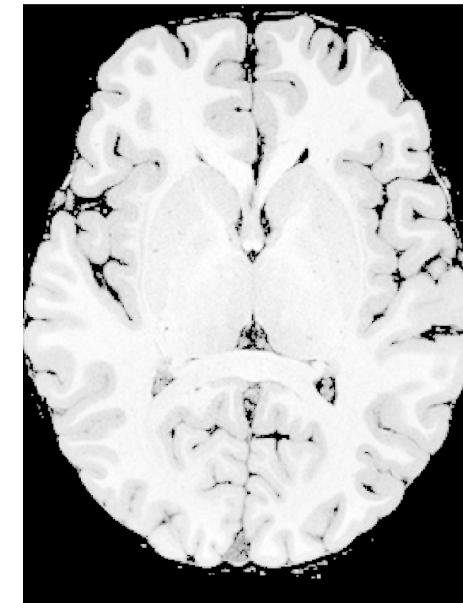
Original Image



Noise



Blur



Bad  
Contrast

## Fourier transform

Signal and noise



## Reminders from previous lecture: Fourier Transform

Linear decomposition of functions in the new basis  
Scaling factor for basis function ( $u, v$ )

$$\mathcal{F}[f(x, y)] = F(u, v) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) e^{-i2\pi(ux+vy)} dx dy$$

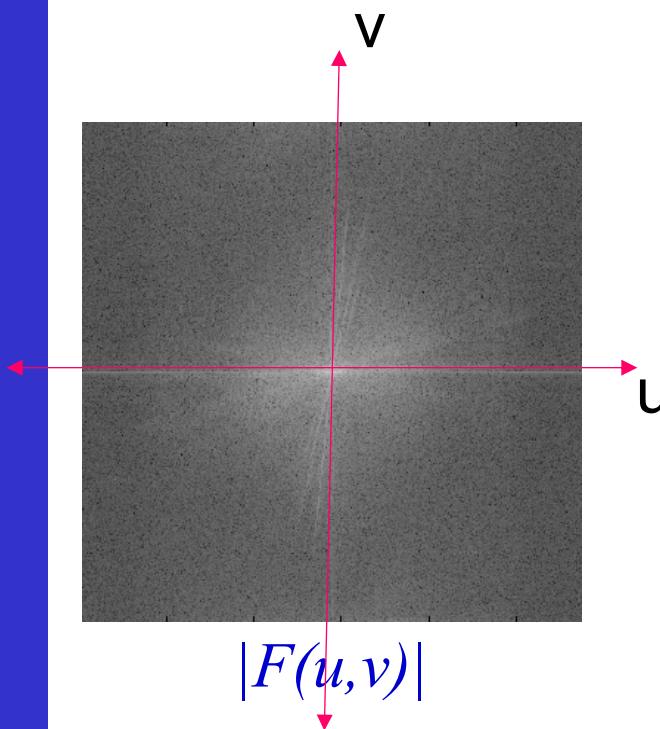
→ The Fourier transform

Reconstruction of the original function in the spatial domain: weighted sum of the basis functions

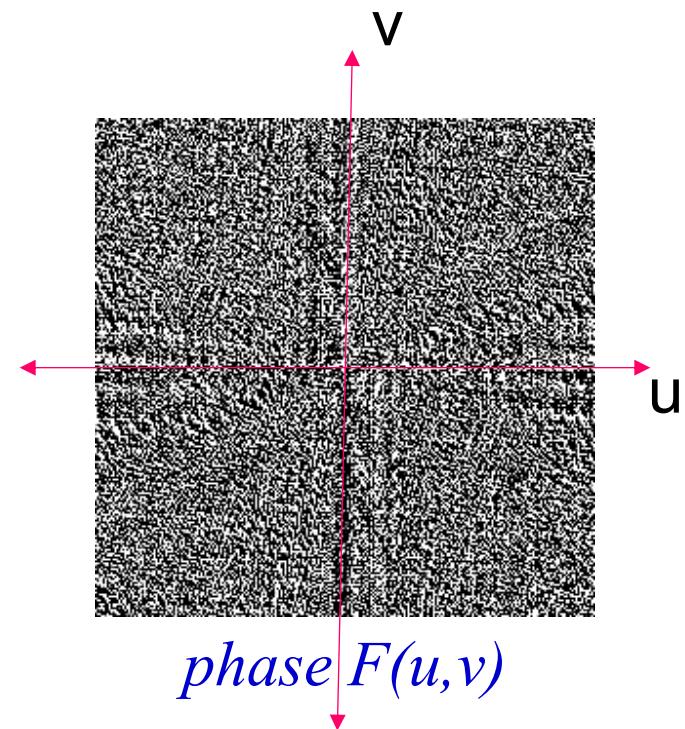
$$\mathcal{F}^{-1}[F(u, v)] = f(x, y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} F(u, v) e^{i2\pi(ux+vy)} dx dy$$

→ The inverse Fourier transform

# Computer Vision



$f(x,y)$



## Reminders from previous lecture: Convolution Theorem

$$C(u, v) = A(u, v)B(u, v)$$

$$c(x, y) = a(x, y) * b(x, y)$$

Space convolution = frequency multiplication

$$C(u, v) = A(u, v) * B(u, v)$$

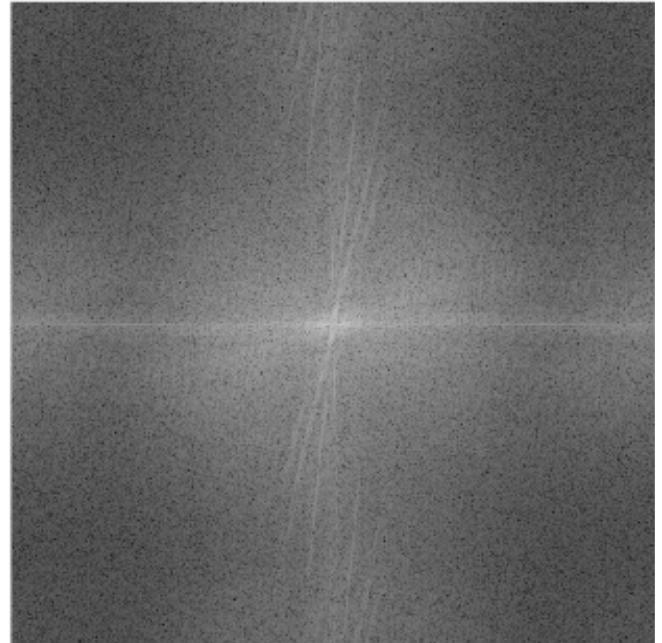
$$c(x, y) = a(x, y)b(x, y)$$

Space multiplication = frequency convolution

## Fourier power spectra of images



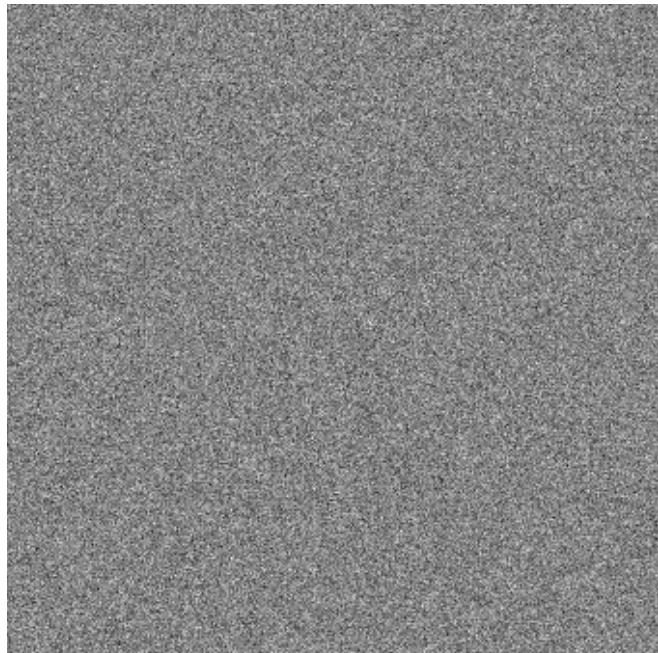
$i(x,y)$



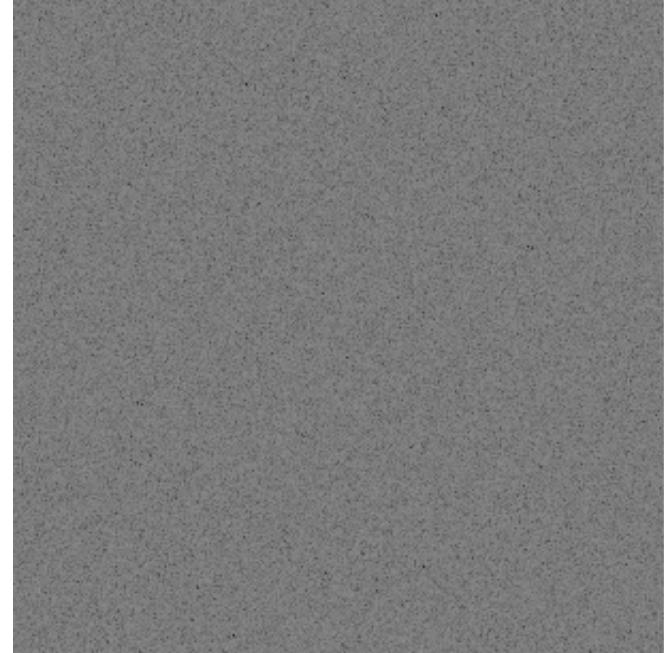
$\phi_{ii} = |I(u,v)|^2$

- Amount of signal at each frequency pair
- Images are mostly composed of homogeneous areas
- Most nearby object pixels have similar intensity
- Most of the signal lies in low frequencies!
- High frequency contains the edge information!

## Fourier power spectra of noise



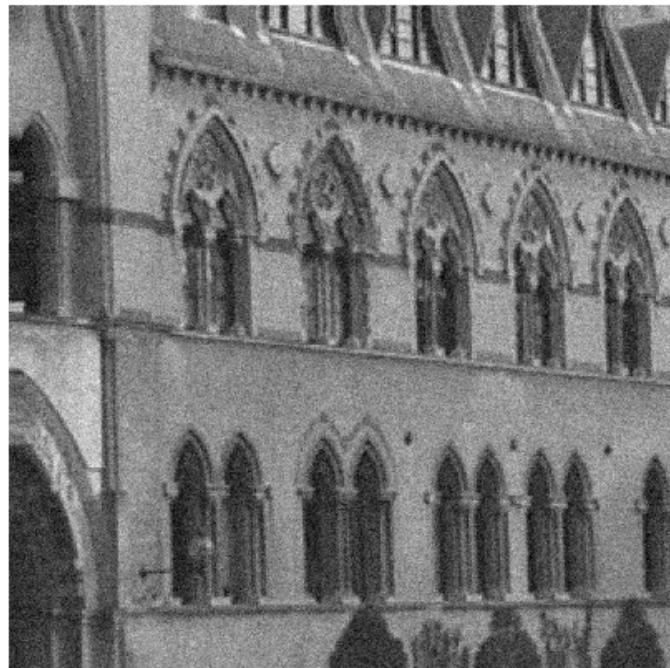
$n(x,y)$



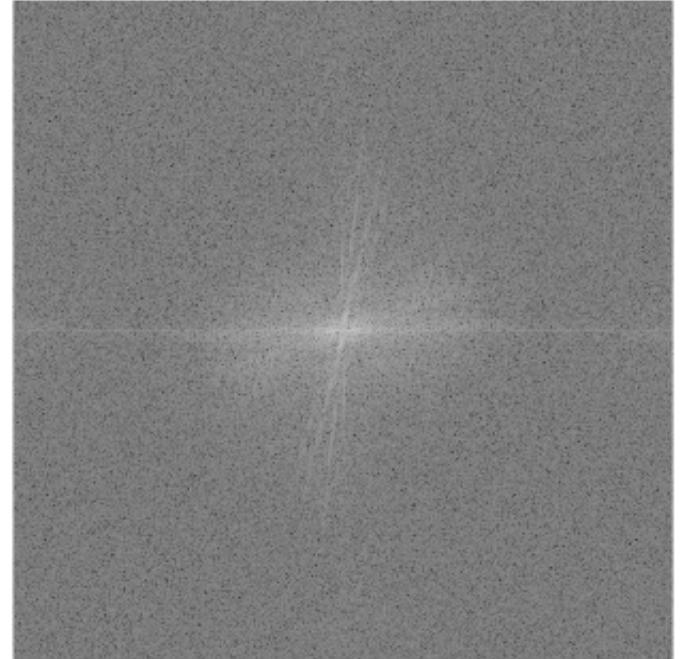
$\phi_{nn} = |N(u,v)|^2$

- Pure noise has a uniform power spectra
- Similar components in high and low frequencies.

## Fourier power spectra of noisy image



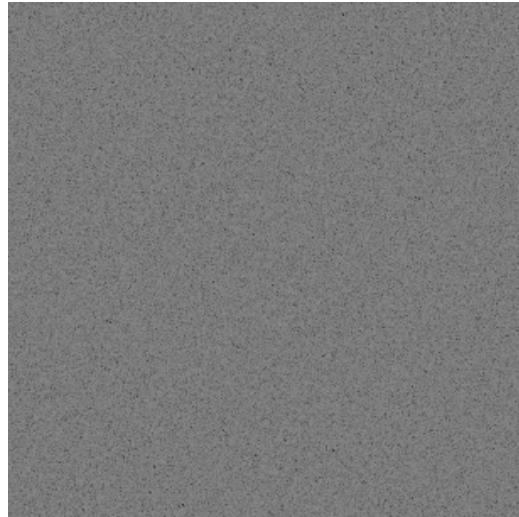
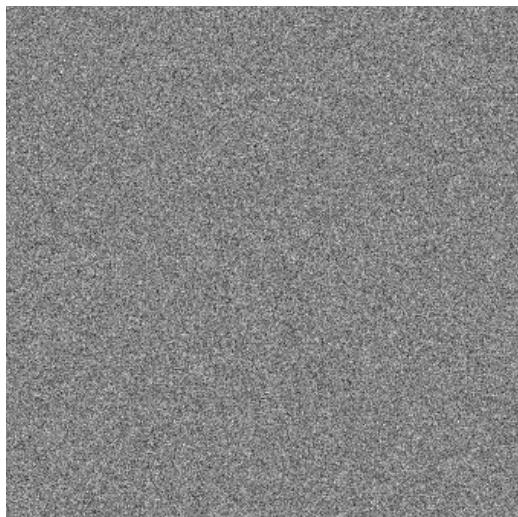
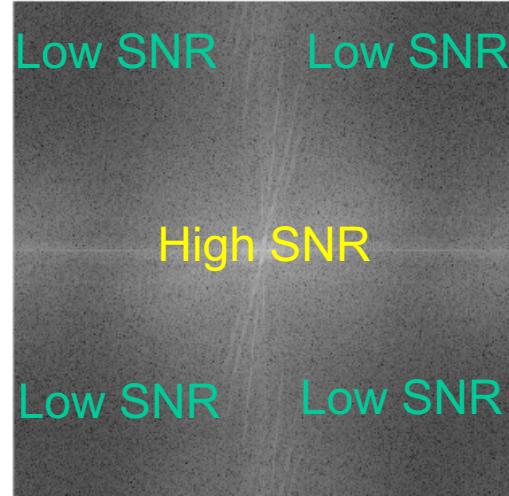
$f(x,y)$



$$\phi_{ff} = |F(u,v)|^2$$

Power spectra is a combination of image and noise

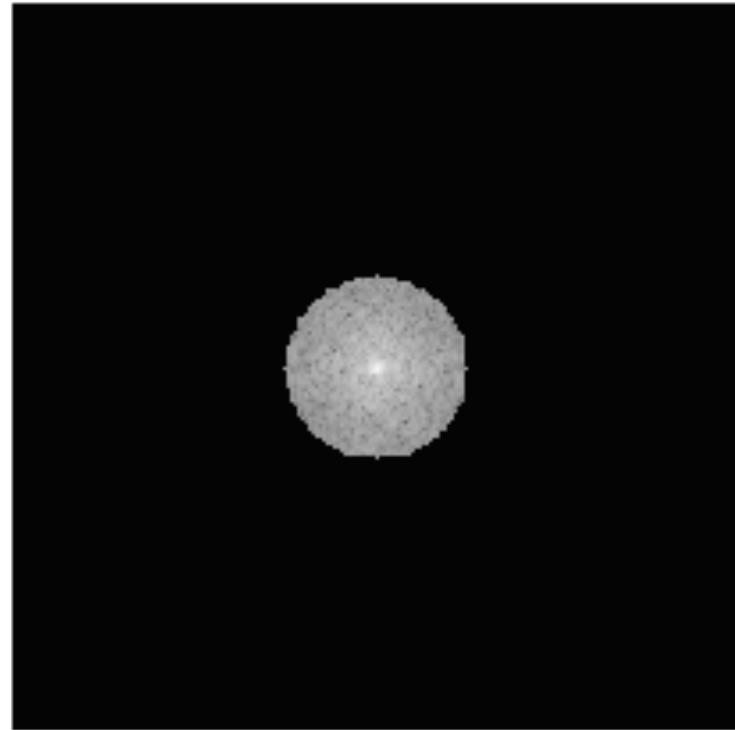
# Signal to Noise Ratio



$$\phi_{ii}(u,v) / \phi_{nn}(u,v)$$

## Only retaining the low frequencies

Low signal/noise ratio at high frequencies  $\Rightarrow$   
eliminate these



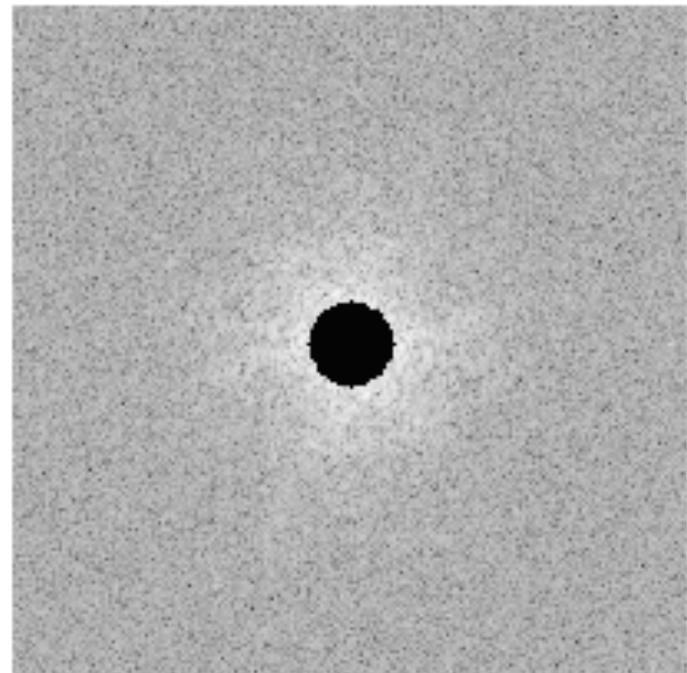
Smoother image but we lost details!



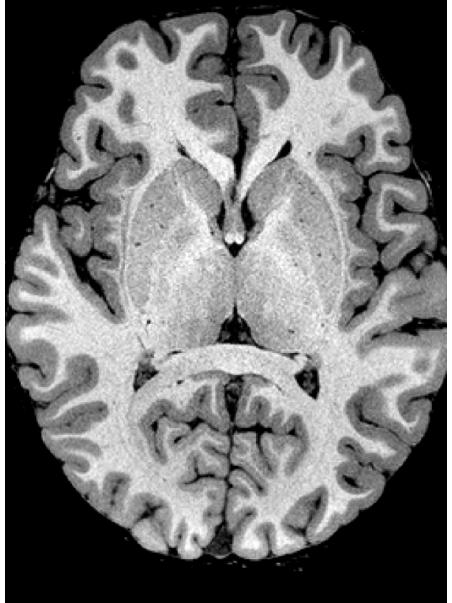
## High frequencies contain noise but also Edges!

We cannot simply discard the higher frequencies

They are also introduced by edges ; example :



# Computer Vision



Original Image

Noise  
Suppression



Noisy  
Observation

## Noise suppression

specific methods for specific types of noise

we only consider 2 general options :

1. Convolutional linear filters
  - low-pass convolution filters
2. Non-linear filters
  - edge-preserving filters
    - a. Median
    - b. Anisotropic diffusion

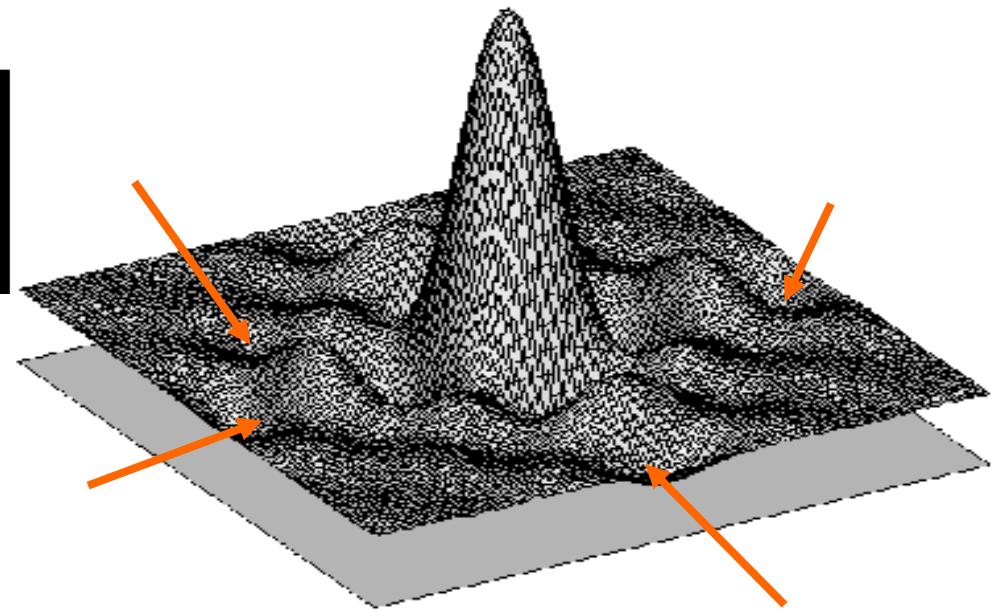
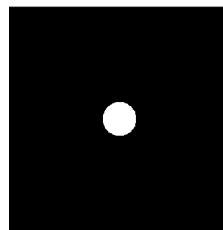
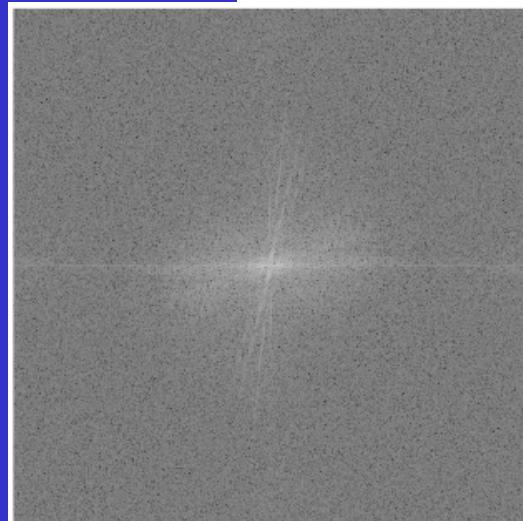


## Low-pass filters: principle

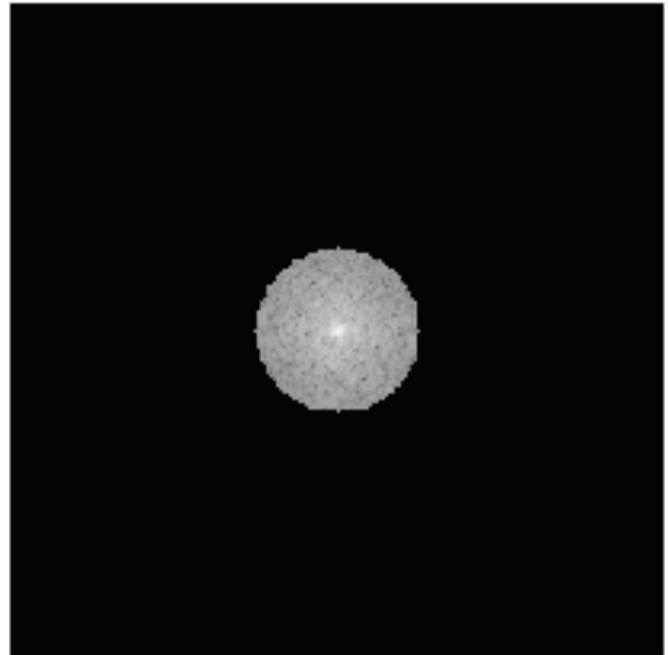
Goal: remove low-signal/noise part of the spectrum

Approach 1: Multiply the Fourier domain by a mask

Such spectrum filters yield “rippling”  
due to ripples of the spatial filter and convolution



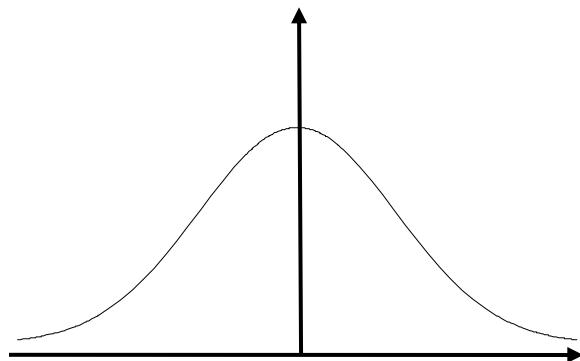
## Illustration of rippling



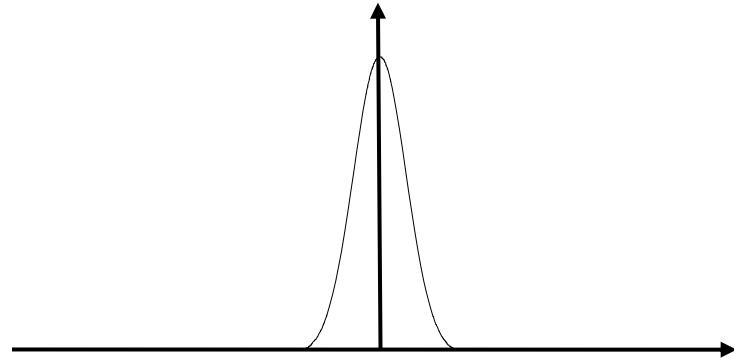
## Approach 2: Low-pass convolution filters

generate low-pass filters that do not cause rippling

Idea: Model convolutional filters in the spatial domain to approximate low-pass filtering in the frequency domain



Convolutional  
filter



Frequency  
mask



## Averaging

One of the most straight forward convolution filters: averaging filters

1/9

1	1	1
1	1	1
1	1	1

1/25

1	1	1	1	1
1	1	1	1	1
1	1	1	1	1
1	1	1	1	1
1	1	1	1	1

Separable:

$$1/9 \begin{array}{|c|c|c|} \hline 1 & 1 & 1 \\ \hline 1 & 1 & 1 \\ \hline 1 & 1 & 1 \\ \hline \end{array} = 1/3 \begin{array}{|c|} \hline 1 \\ \hline 1 \\ \hline 1 \\ \hline \end{array} * 1/3 \begin{array}{|c|c|c|} \hline 1 & 1 & 1 \\ \hline \end{array}$$

$\rightarrow o(x, y) = f(x, y) * i(x, y) = f_1(x, y) * (f_2(x, y) * i(x, y))$

## Example for box averaging



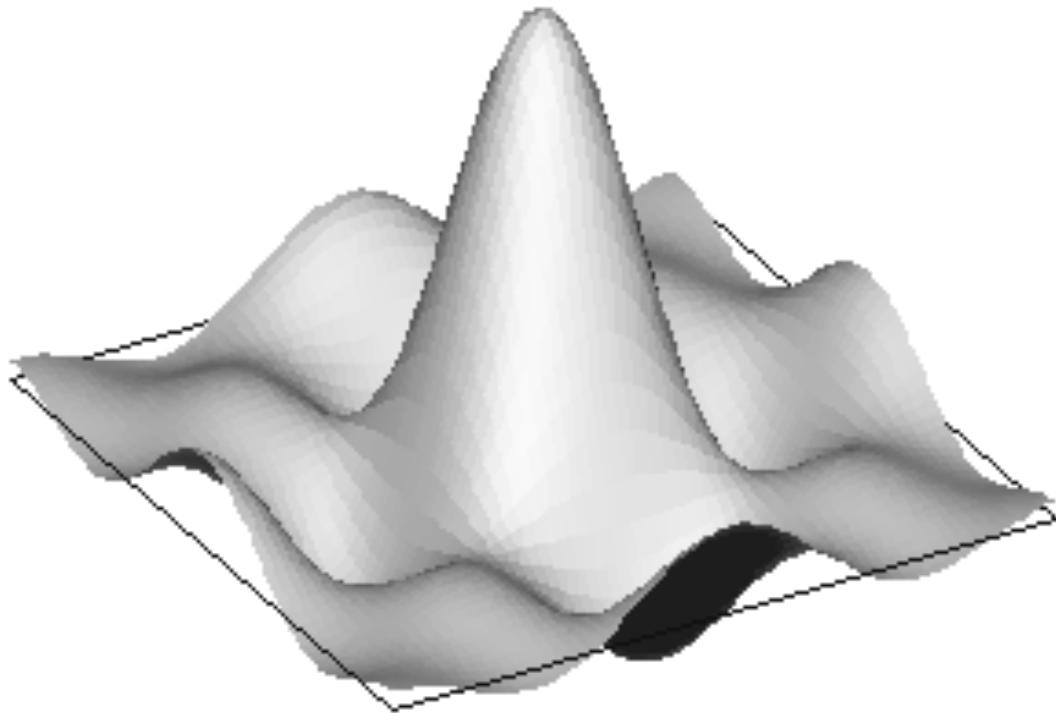
Noise is gone.  
Result is blurred!



## MTFs for averaging

5 x 5 (separable)

$$(1+2\cos(2\pi u)+2\cos(4 \pi u))(1+2\cos(2\pi v)+2\cos(4 \pi v))$$



→ not even low-pass!

## So far

1. Masking frequency domain with window type low-pass filter yields sinc-type of spatial filter and ripples -> disturbing effect
2. box filters are not exactly low-pass, ripples in the frequency domain at higher freq. remember phase reversals?

no ripples in either domain required!



## Solution: Binomial filters

iterative convolutions of (1,1)

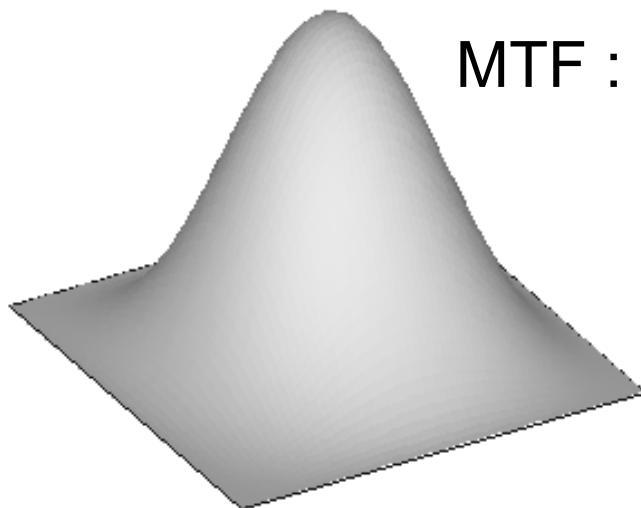
only odd filters : (1,2,1), (1,4,6,4,1)

2D :

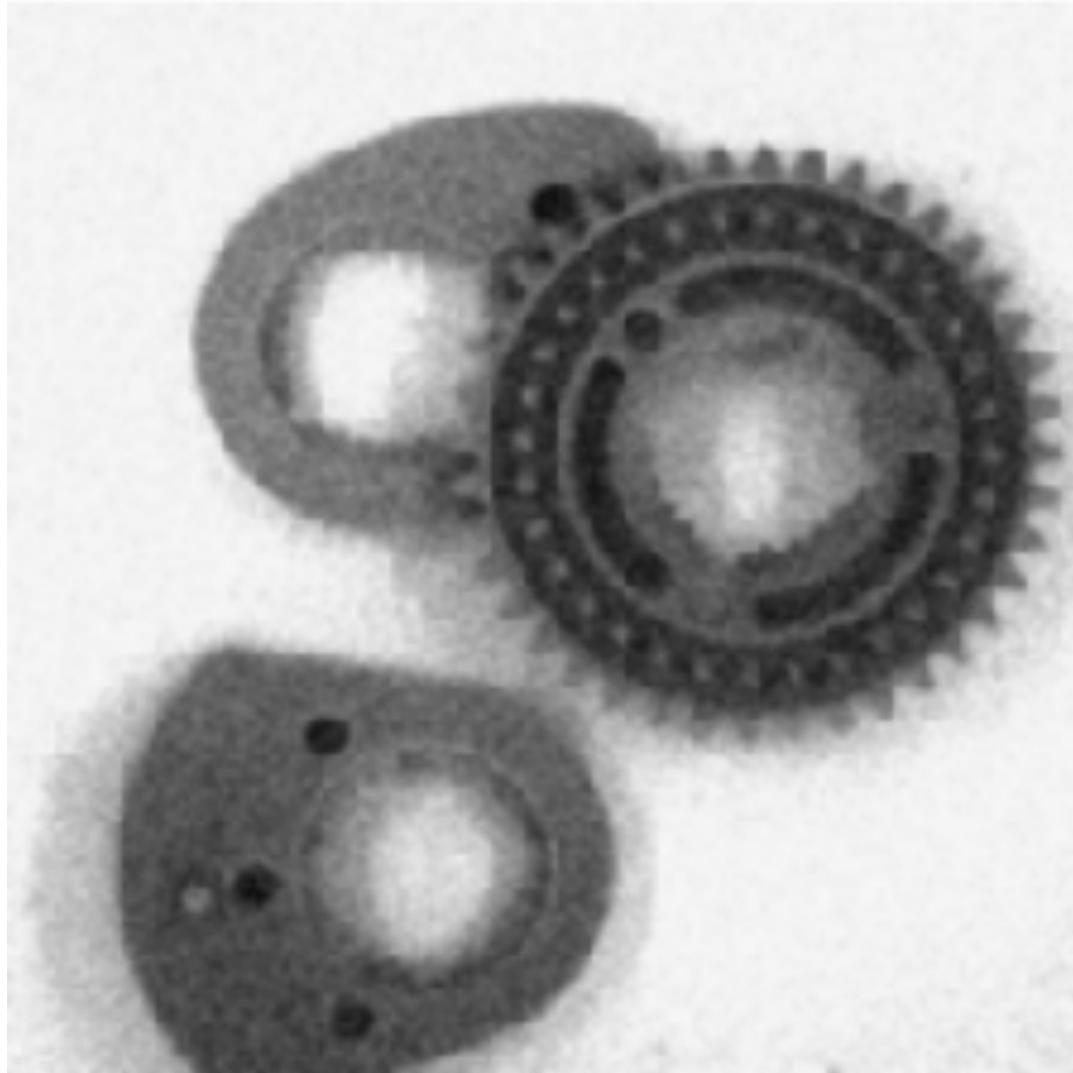
1	2	1
2	4	2
1	2	1

Also separable

MTF :  $(2+2\cos(2 \pi u))(2+2\cos(2 \pi v))$



## Result of binomial filter



## Limit of iterative binomial filtering

f :

1	2	1
2	4	2
1	2	1

$$f(x, y) * f(x, y) * \dots * f(x, y) = f^n(x, y)$$

$$f^n(x, y) \rightarrow a \exp\left(\frac{\|(x, y)\|^2}{b}\right), \text{ as } n \rightarrow \infty$$

Gaussian

## Gaussian smoothing

Gaussian is limit case of binomial filters



noise gone, no ripples, but still blurred...

Actually linear filters cannot solve this problem



## Some implementation issues

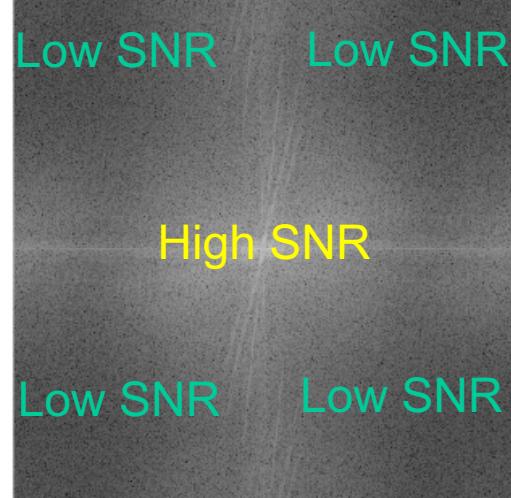
separable filters can be implemented efficiently

large filters through multiplication in the frequency domain

integer mask coefficients increase efficiency  
powers of 2 can be generated using shift operations



## Question



Can a linear-shift-invariant systems do a perfect job?

Can they separate edge information from noise in the higher frequency components?

Why?

## Noise suppression

specific methods for specific types of noise

we only consider 2 general options :

1. Convolutional linear filters
  - low-pass convolution filters
2. Non-linear filters
  - edge-preserving filters
    - a. Median
    - b. Anisotropic diffusion



## Median filters : principle

non-linear filter

method :

- 1. rank-order neighbourhood intensities
- 2. take middle value

no new grey levels emerge...



## Median filters : odd-man-out

advantage of this type of filter is its “odd-man-out” effect

e.g.

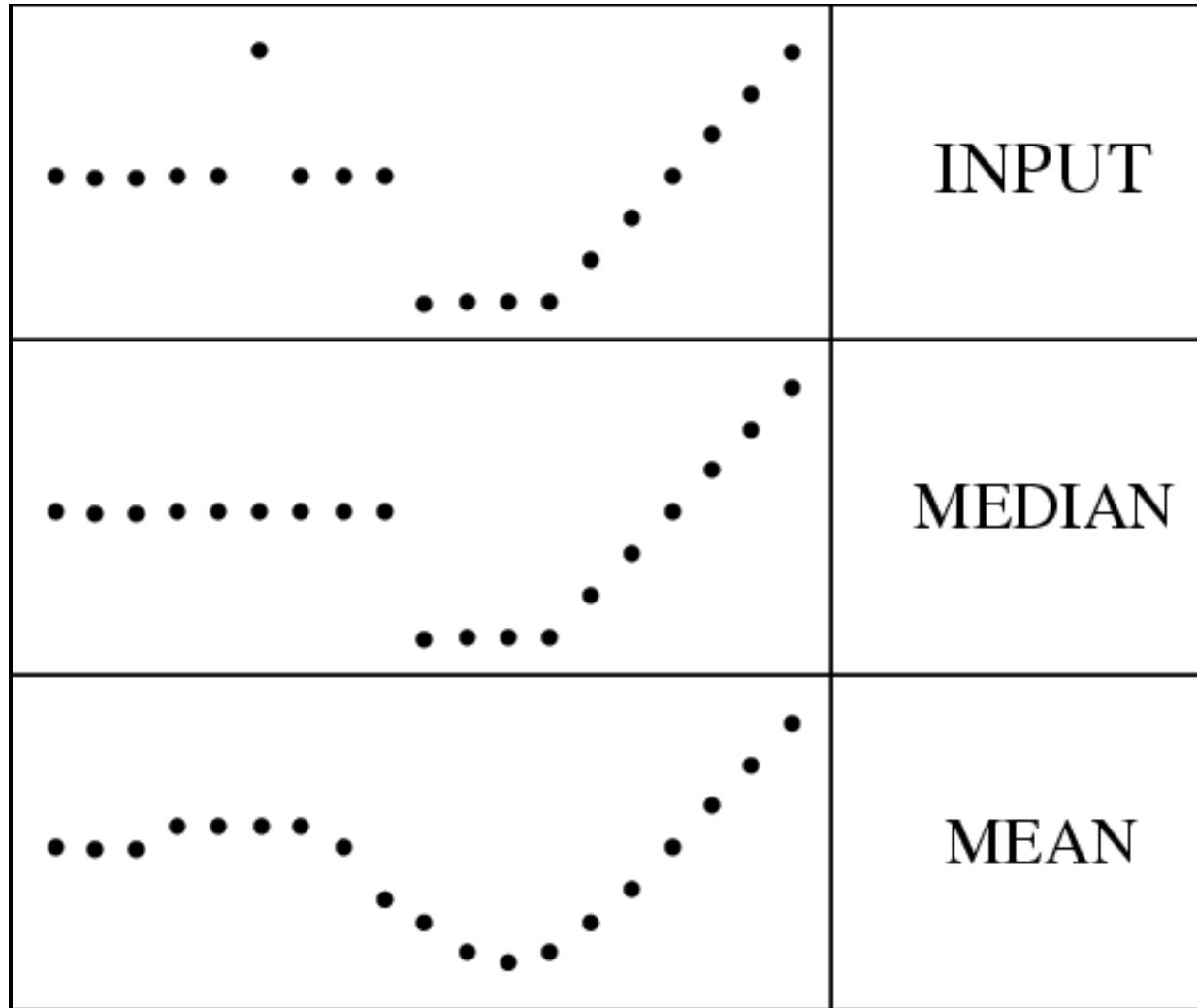
1,1,1,7,1,1,1,1



? , 1,1,1.1,1,1,?

## Median filters : example

filters have width 5 :



## Median filters : analysis

median completely discards the spike,  
linear filter always responds to all aspects

median filter preserves discontinuities,  
linear filter produces rounding-off effects

DON'T become all too optimistic



## Median filter : results

3 x 3 median filter :



sharpens edges, destroys edge cusps  
and protrusions



## Median filters : results

Comparison with Gaussian :



e.g. upper lip smoother, eye better preserved



## Example of median

10 times 3 X 3 median



patchy effect  
important details lost (e.g. ear-ring)



## Question

For what types of noise would you clearly prefer median filtering over Gaussian filtering?

- a) Gaussian noise, i.e. noise distributed by independent normal distribution
- b) Salt and pepper noise
- c) Uniform noise, i.e. distributed by uniform distribution
- d) Exponential noise model
- e) Rayleigh noise

## Anisotropic diffusion : principle

non-linear filter

method :



- 1. Gaussian smoothing across homogeneous intensity areas
- 2. No smoothing across edges

# The Gaussian filter revisited



The diffusion equation

$$\frac{\partial f(\vec{x}, t)}{\partial t} = \nabla \cdot (c(\vec{x}, t) \nabla f(\vec{x}, t))$$

Initial/Boundary conditions

$$f(\vec{x}, 0) = i(x, y), \text{ for } \vec{x} \in \Omega$$

$$f(\vec{x}, t) = 0, \text{ for } \vec{x} \in \delta(\Omega)$$

If  $c(\vec{x}, t) = c$

$$\frac{\partial f(\vec{x}, t)}{\partial t} = c \Delta f(\vec{x}, t) \quad \text{in 1D:} \quad \frac{\partial f(x, t)}{\partial t} = c \frac{\partial^2 f(x, t)}{\partial x^2}$$

Solution is a convolution!

$$f(\vec{x}, t) = f(\vec{x}, 0) * g(\vec{x}, t) = i(\vec{x}) * g(\vec{x}, t)$$

## Diffusion as Gaussian lowpass filter



$$f(\vec{x}, t) = i(\vec{x}) * \frac{1}{(2\pi)^{d/2} \sqrt{ct}} \exp \left\{ -\frac{\vec{x} \cdot \vec{x}}{4ct} \right\}$$

Gaussian filter with time dependent standard deviation:  $\sigma = \sqrt{2ct}$

Nonlinear version can change the width of the filter locally

$$c(\vec{x}, t) = c(f(\vec{x}, t))$$

Specifically dependening on the edge information through gradients

$$c(\vec{x}, t) = c(|\nabla f(\vec{x}, t)|)$$

## Selection of diffusion coefficient

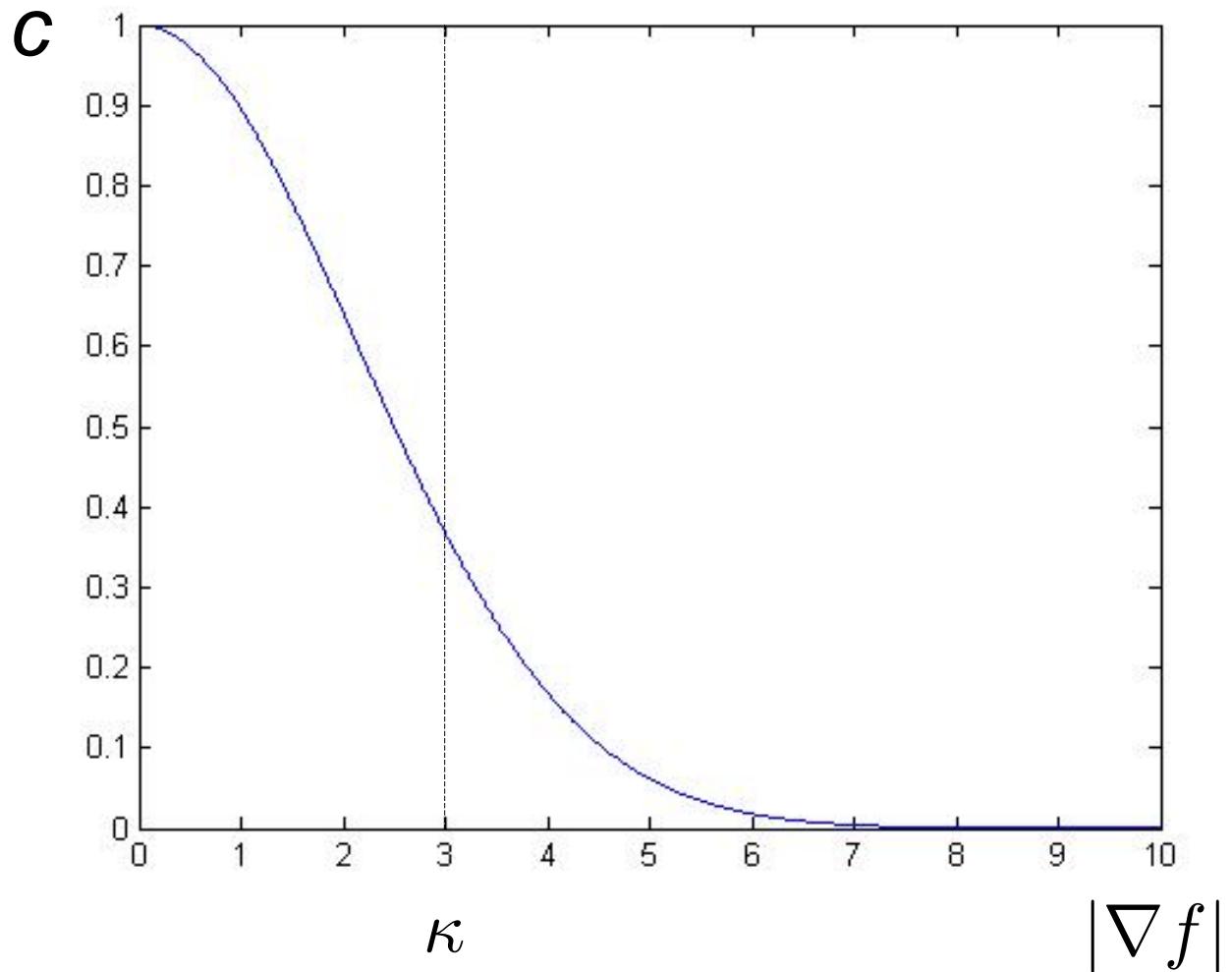
$$c(|\nabla f(\vec{x}, t)|) = \exp \left\{ -\frac{|\nabla f|^2}{2\kappa^2} \right\}$$

or

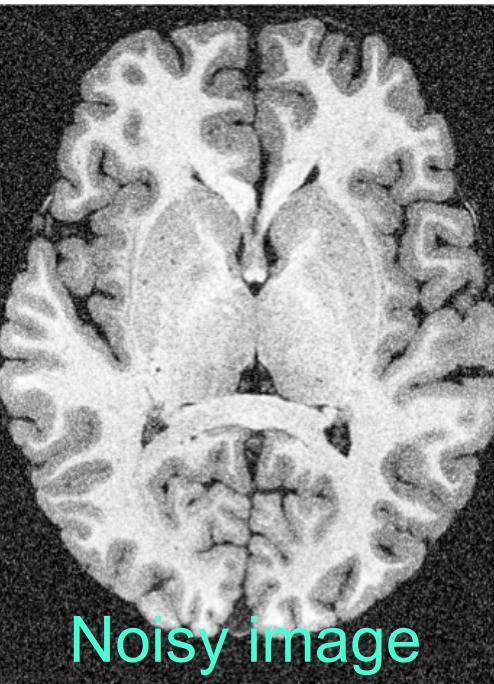
$$c(|\nabla f(\vec{x}, t)|) = \frac{1}{1 + \left( \frac{|\nabla f|}{\kappa} \right)^2}$$

$\kappa$  controls the contrast to be preserved by smoothing  
actually edge sharpening happens

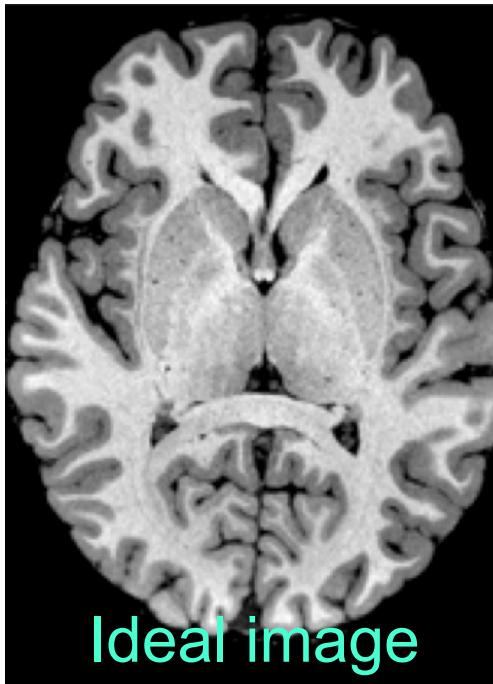
## Dependence on contrast



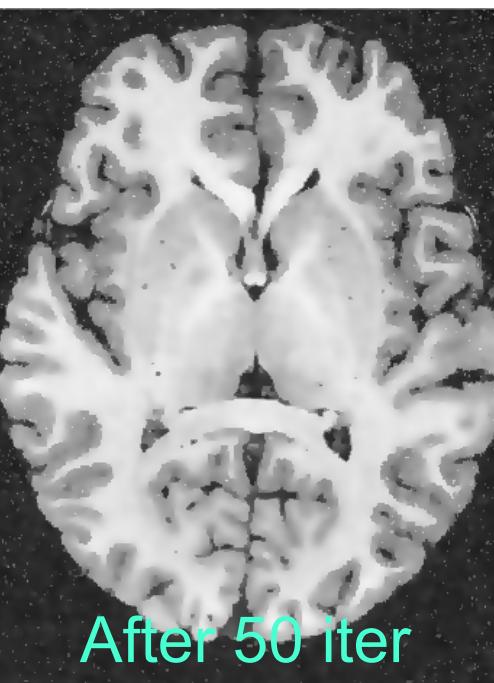
# Computer Vision



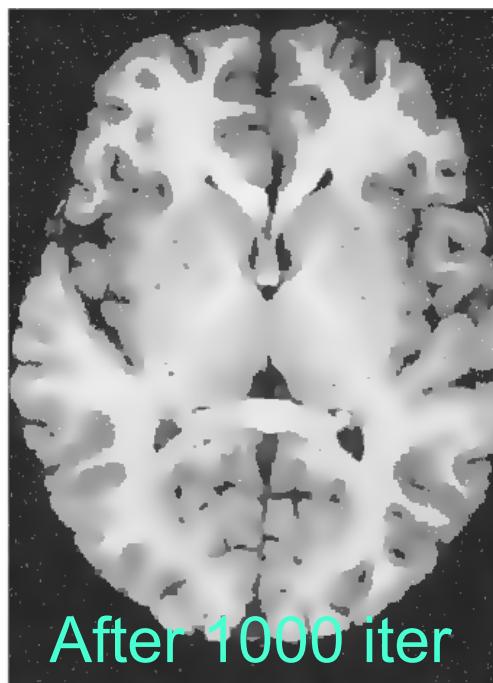
Noisy image



Ideal image

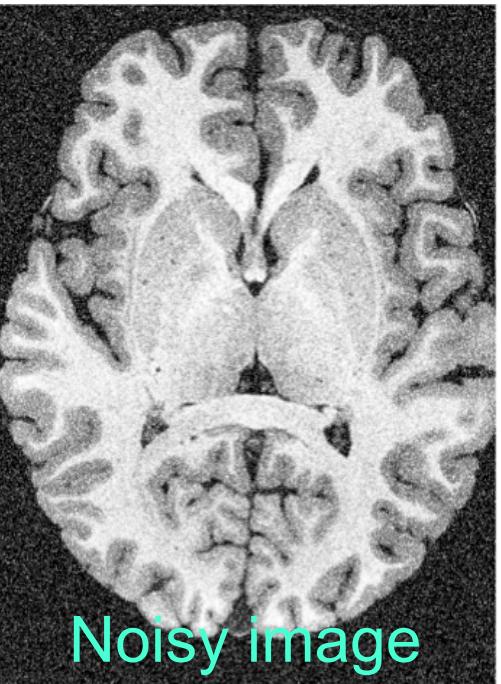


After 50 iter

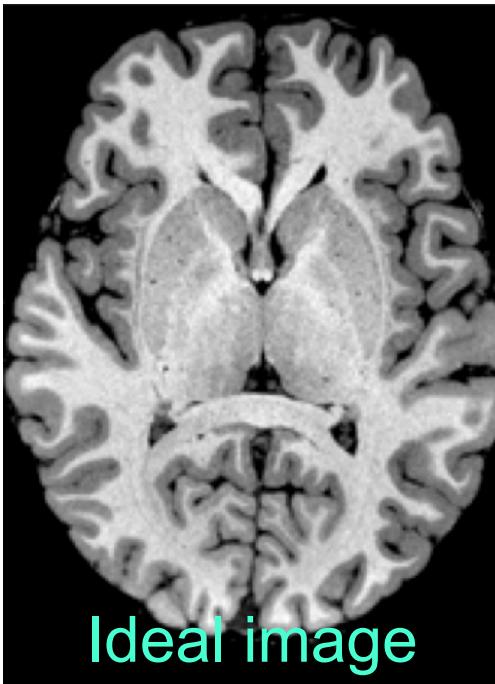


After 1000 iter

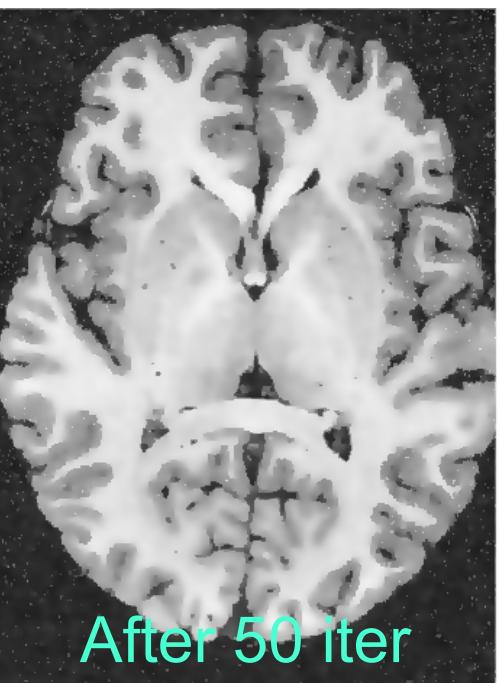
# Computer Vision



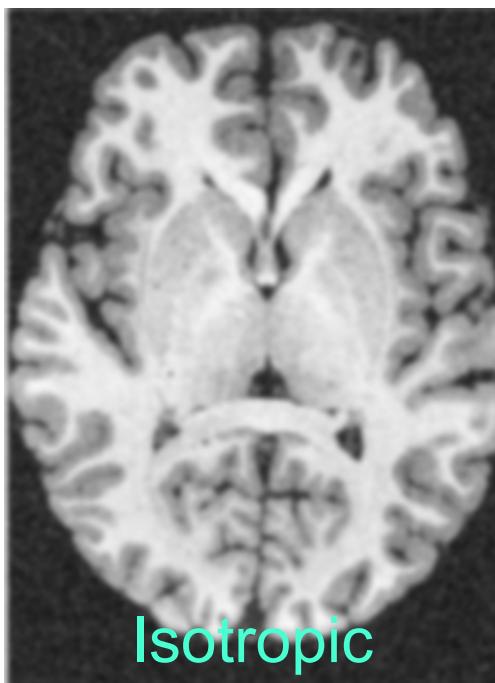
Noisy image



Ideal image



After 50 iter



Isotropic

## Anisotropic diffusion: Output



End state is  
homogeneous

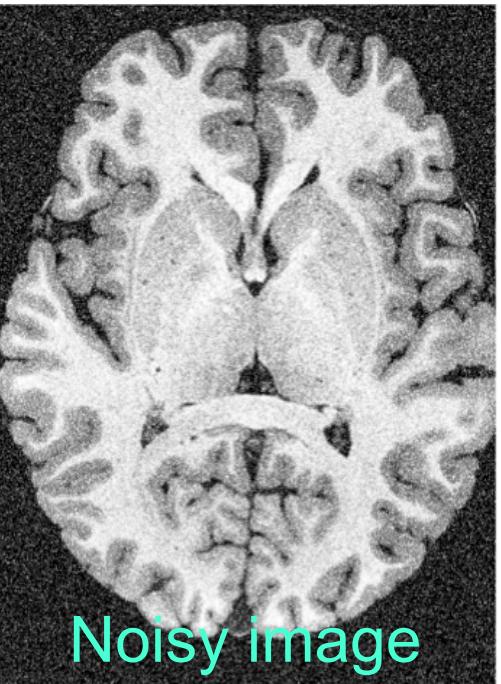
## Restraining the diffusion



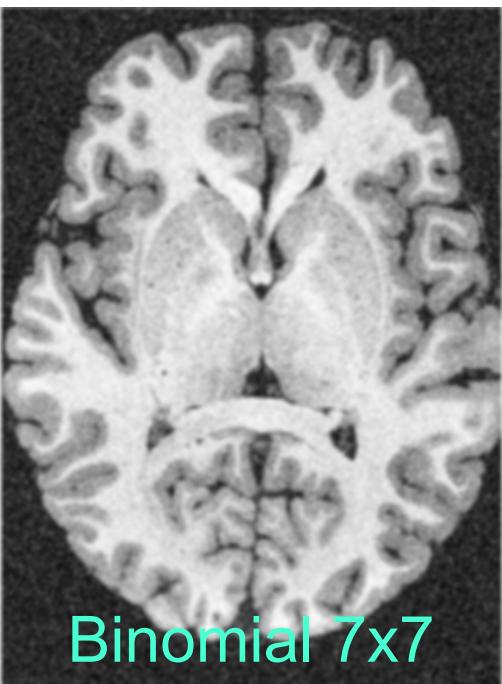
adding restraining force :

$$\frac{\partial f}{\partial t} = \Delta \cdot (c(|\nabla f|) \nabla f) - \frac{1}{\sigma^2} (f - i)$$

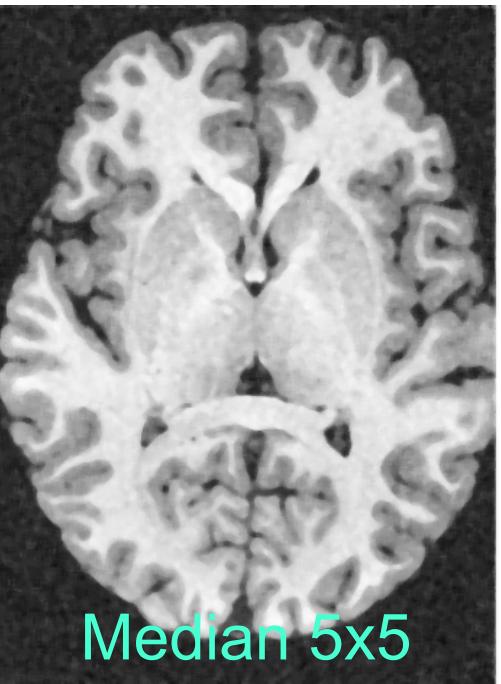
# Computer Vision



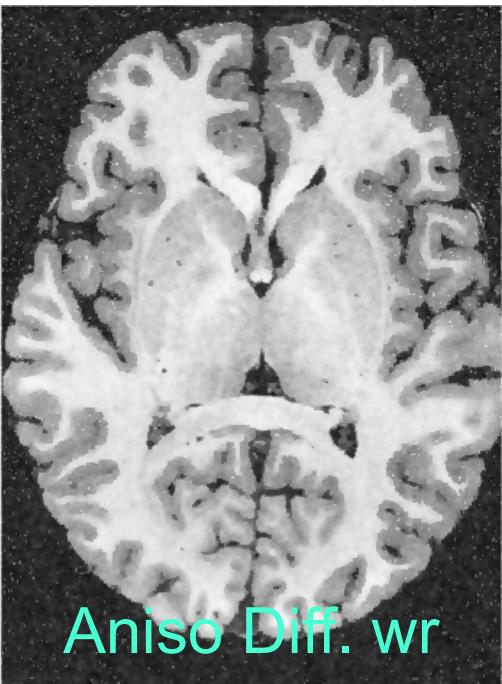
Noisy image



Binomial 7x7



Median 5x5



Aniso Diff. wr

## Anisotropic diffusion: Numerical solutions

When  $c$  is not a constant solution is found through solving the equation

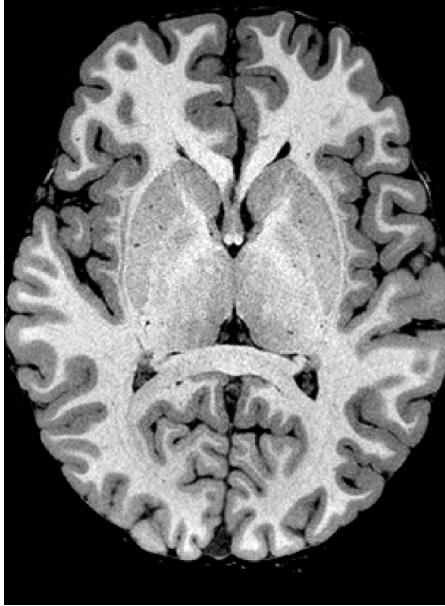
$$\frac{\partial f(\vec{x}, t)}{\partial t} = \nabla \cdot (c(\vec{x}, t) \nabla f(\vec{x}, t))$$

Partial differential equation

Numerical solutions through discretizing the differential operators and integrating

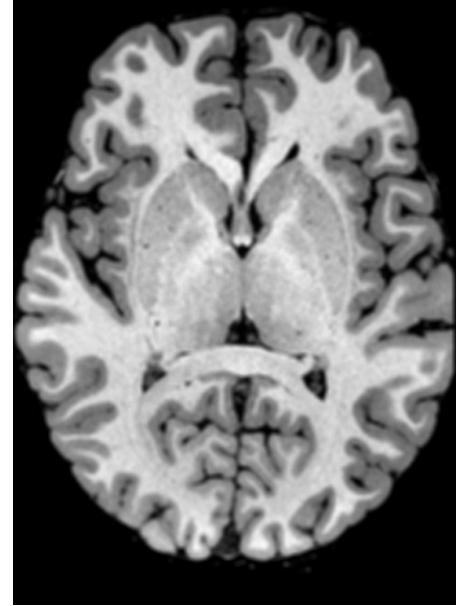
Finite differences in space and integration in time

# Computer Vision



Original Image  
What we want

Deblurring



Blurred image  
What we observe

## Unsharp masking

simple but effective method

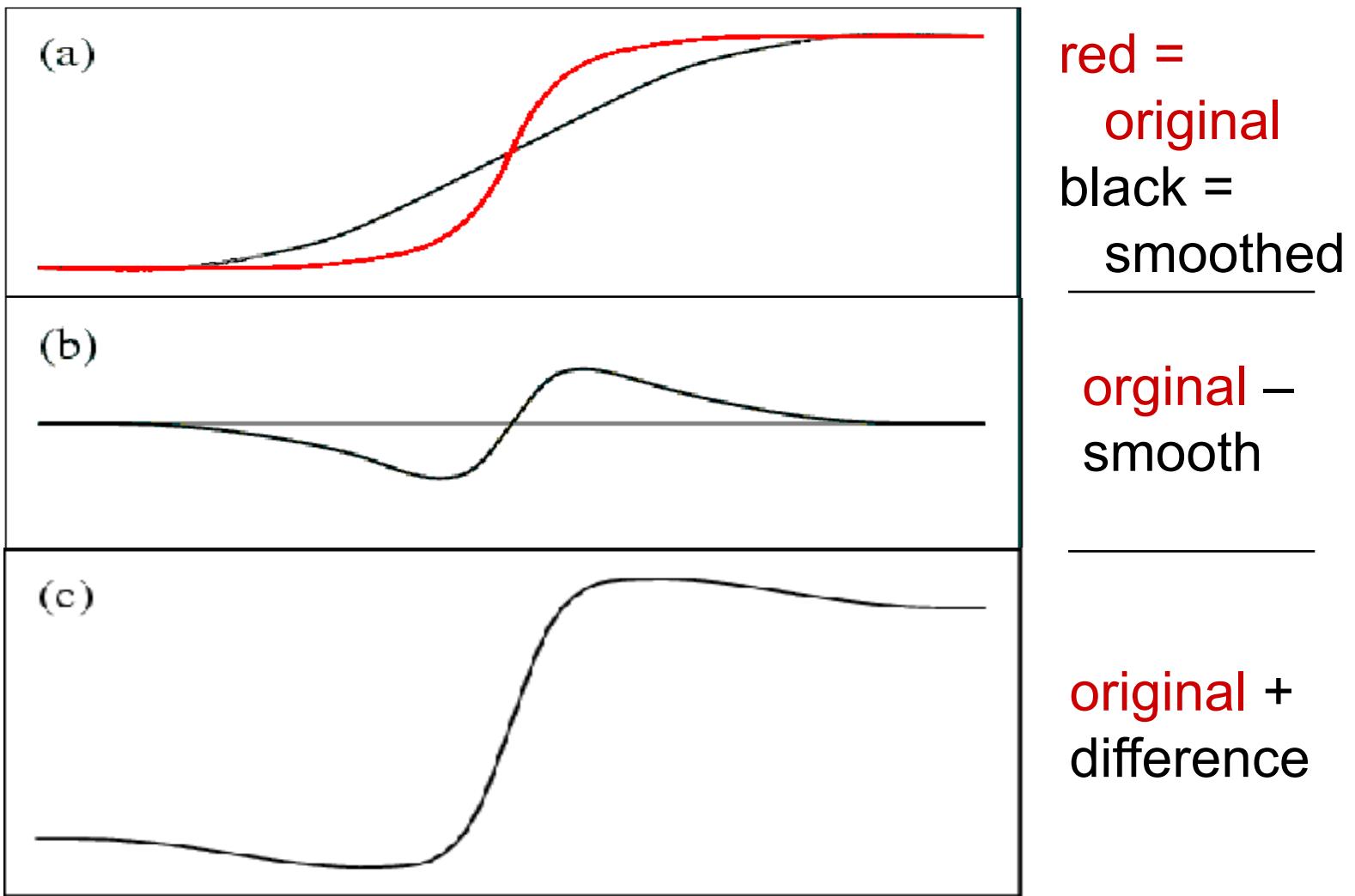
image independent

linear

used e.g. in photocopiers and scanners



## Unsharp masking : sketch



## Unsharp masking : principle

Interpret blurred image as snapshot of diffusion process

$$\frac{\partial f}{\partial t} = c(\nabla^2 f)$$

In a first order approximation, we can write

$$f(x, y, t) \approx f(x, y, 0) + \frac{\partial f}{\partial t} t$$

Hence,

$$f(x, y, 0) \approx f(x, y, t) - \frac{\partial f}{\partial t} t = f(x, y, t) - ct\nabla^2 f$$

Unsharp masking produces  $o$  from  $i$

$$o = i - k\nabla^2 i$$

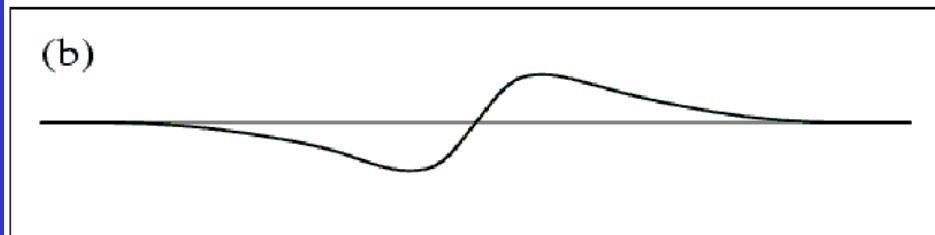
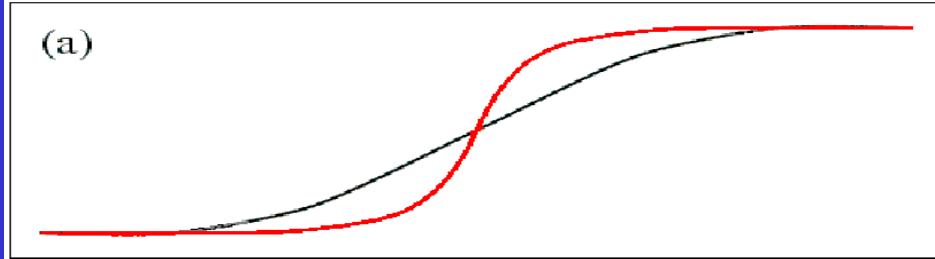
with  $k$  a well-chosen constant



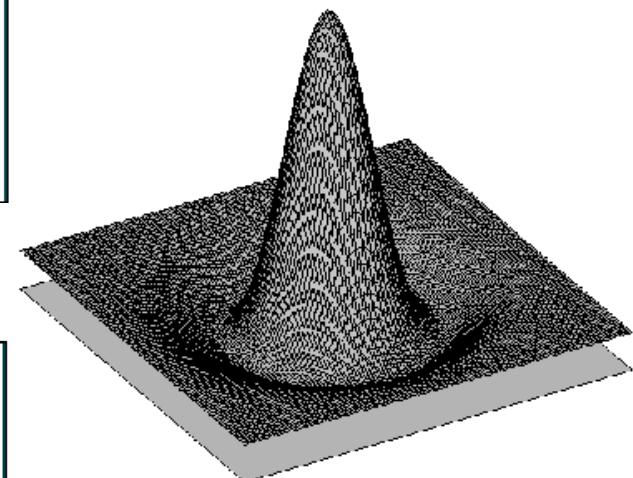
Need to estimate  $\nabla^2 i(x, y)$

DOG (Difference-of-Gaussians) approximation  
for Laplacian :

*Our 1D example:*



*Convolution  
mask in 2D:*



## Unsharp masking: Analysis

(b)



$$o = i - k\nabla^2 i$$

(c)



The edge profile becomes steeper, giving a sharper impression

Under-and overshoots flanking the edge further increase the impression of image sharpness



## Unsharp masking : images



## Inverse filtering

Relies on system view of image processing

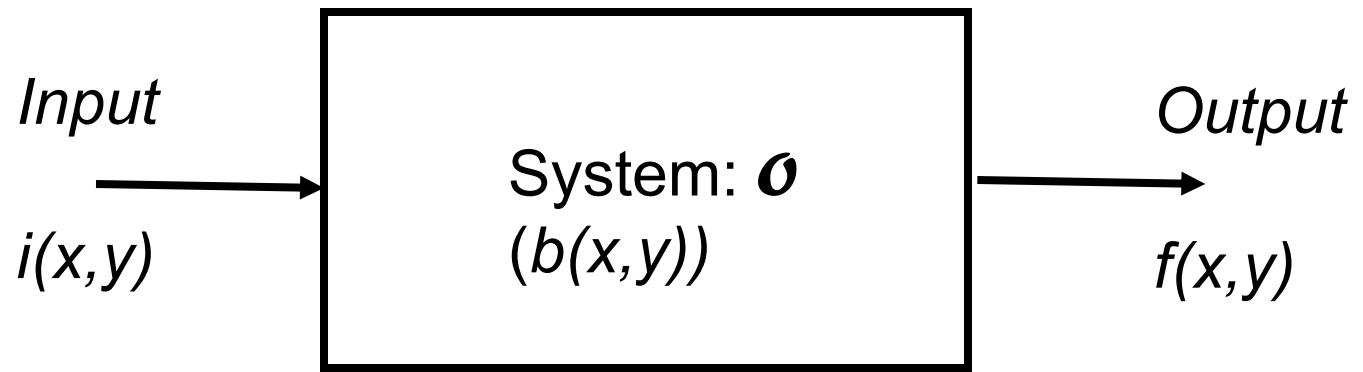
Frequency domain technique

Defined through Modulation Transfer Function

Links to theoretically optimal approaches



## A system view on image restoration



$i, b$  known  $f=?$ : simulation, smoothing

$i, f$  known  $b=?$ : system identification

$b, f$  known  $i=?$ : image restoration

for de-blurring:  $b$  is the blurring filter

## Inverse filtering : principle

Frequency domain technique

suppose you know the MTF  $B(u, v)$  of the blurring filter

$$f(x, y) = b(x, y) * i(x, y)$$

$$F(u, v) = B(u, v)I(u, v)$$

to undo its effect new filter with MTF  $B'(u, v)$  such that

$$B'(u, v)B(u, v) = 1$$

$$I(u, v) = B'(u, v)F(u, v)$$



## Inverse filtering : formal derivation

$$B'(u, v) = 1/B(u, v)$$

For additive noise after filtering

$$F(u, v) = B(u, v)I(u, v) + N(u, v)$$

Result of inverse filter

$$F(u, v)B'(u, v) = I(u, v) + N(u, v)/B(u, v)$$



## Problems of inverse filtering

$$F(u, v) = B(u, v)I(u, v) + N(u, v)$$

- Frequencies with  $B(u, v) = 0$   
Information fully lost during filtering  
Cannot be recovered  
Inverse filter is ill-defined

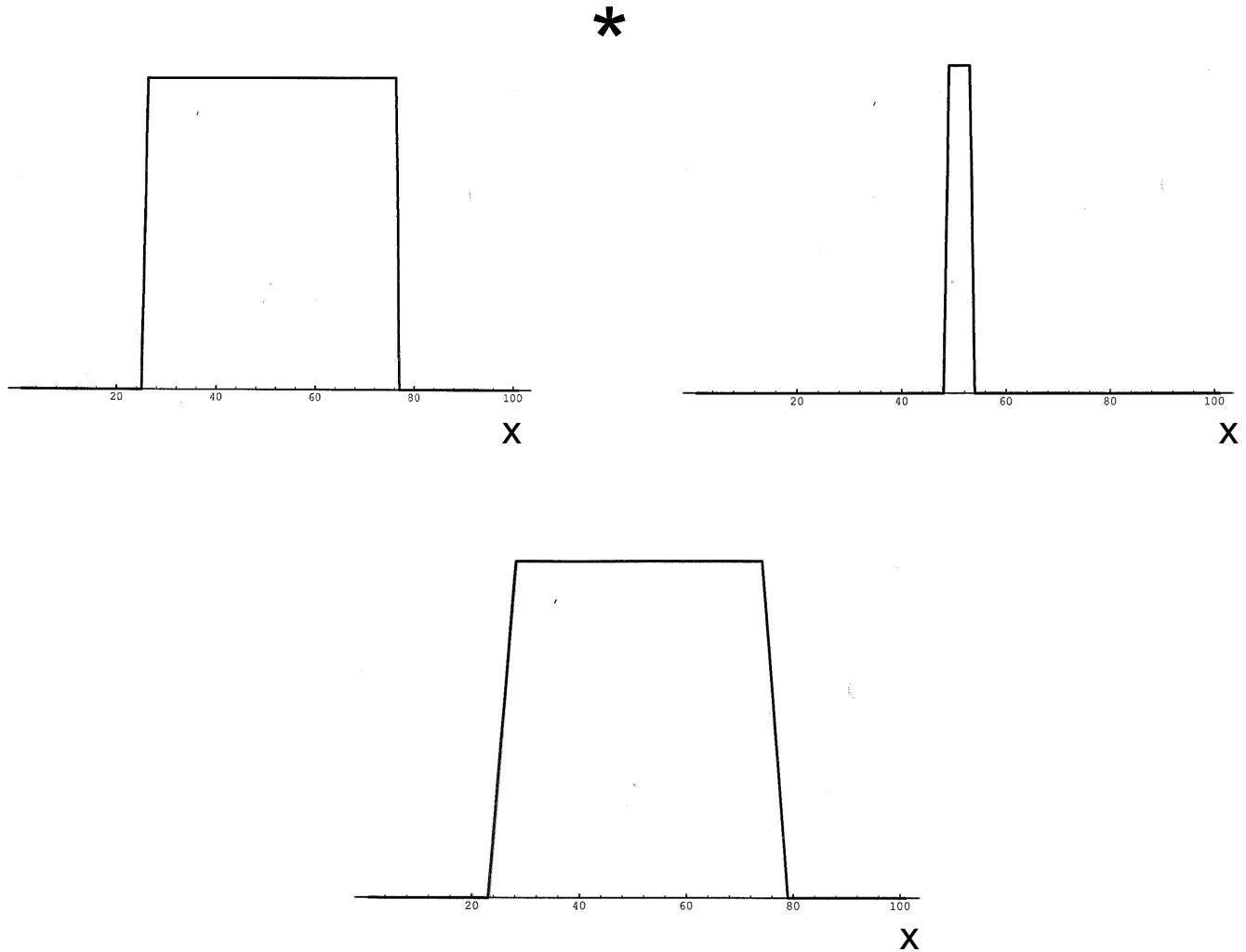
$$F(u, v)B'(u, v) = I(u, v) + N(u, v)/B(u, v)$$

- Also problem with noise added after filtering  
 $B(u, v)$  is low  $\rightarrow 1/B(u, v)$  is high,  
VERY strong noise amplification

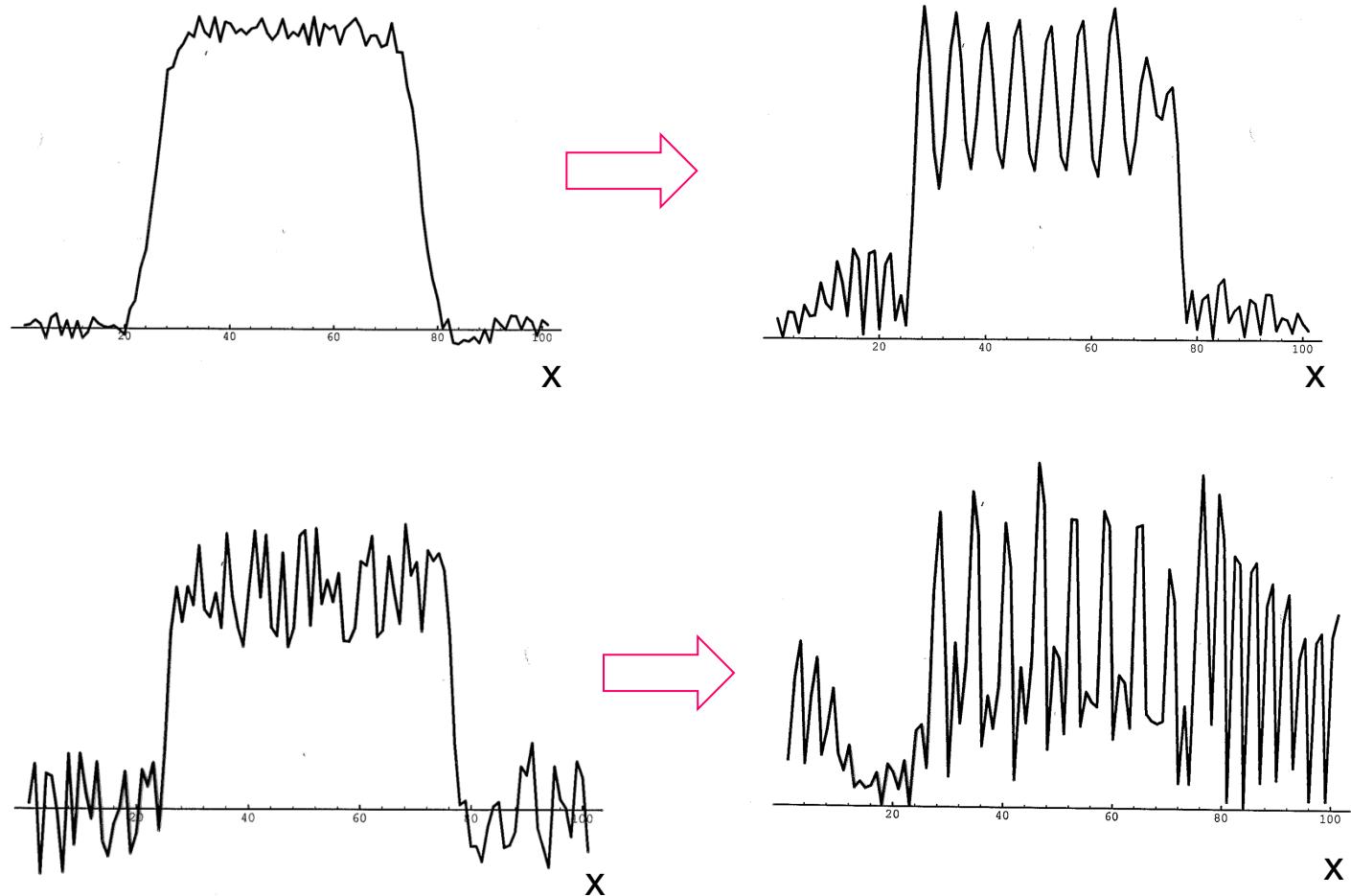


# Computer Vision

## 1D Example



# Restoration of noisy signals



## Inverse filtering : 2D example

we will apply the method to a Gaussian smoothed example ( $\sigma = 16$  pixels)



## Inverse filtering : 2D example



→ noise leads to spurious high frequencies

## The Wiener Filter

Looking for the optimal filter to do the deblurring

Take into account the noise to avoid amplification

Optimization formulation

Filter is given analytically in the Fourier Domain



## Wiener filter and its behavior

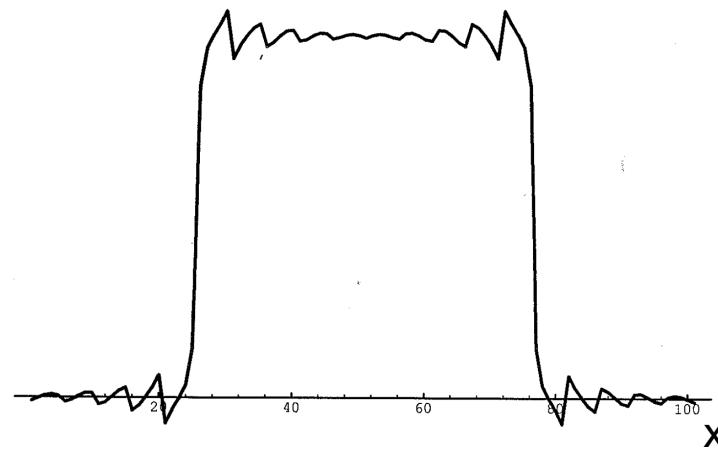
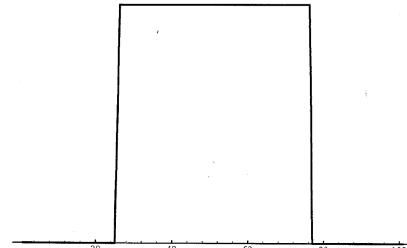
$$Wf(H) = H'(u, v) = \frac{H(u, v)}{H^*(u, v)H(u, v) + 1/\text{SNR}}$$

$$\text{SNR} = \frac{\Phi_{ii}}{\Phi_{nn}}$$

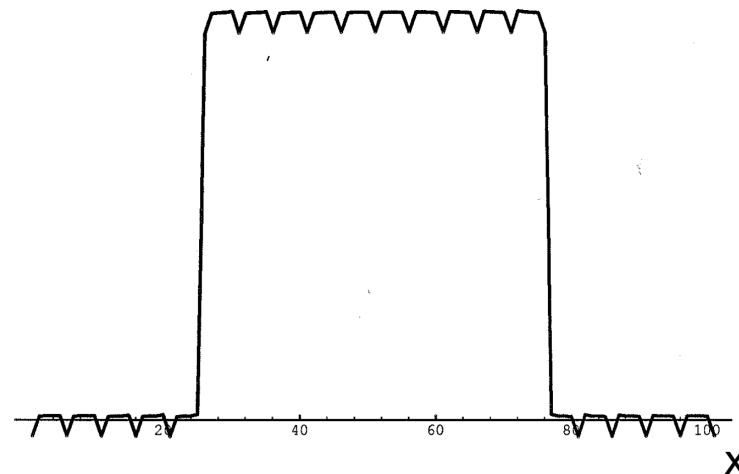
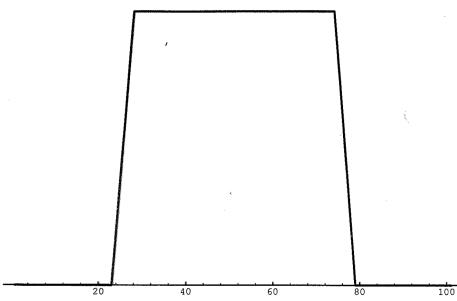
- $H(u, v) = 0 \implies Wf(H) = 0$  ✓
- $\text{SNR} \rightarrow \infty \implies 1/\text{SNR} \rightarrow 0$  ✓
- $Wf(H) \rightarrow \frac{1}{H}$
- $\text{SNR} \rightarrow 0 \implies 1/\text{SNR} \rightarrow \infty$  ✓
- $Wf(H) \rightarrow 0$



# Wiener filter: Noiseless reconstruction



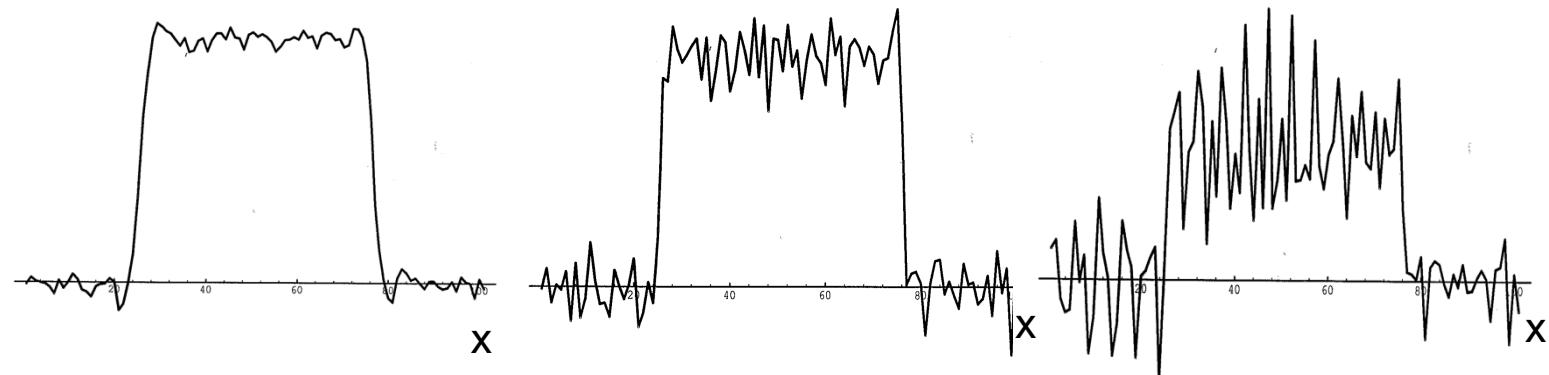
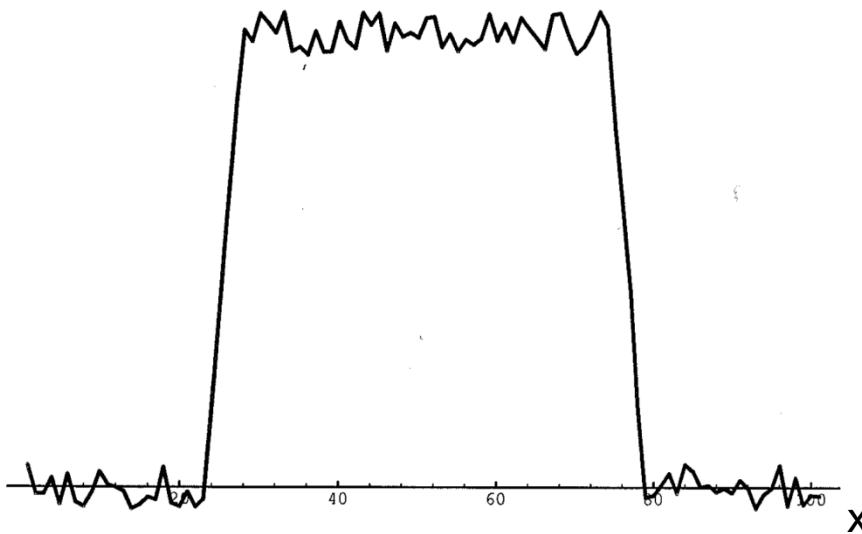
Medium confidence



High confidence



## Wiener filter: Noisy reconstruction



Low confidence

Medium confidence  
Correct SNR

High confidence



## Wiener filtering : example



spurious high freq. eliminated, conservative



## Wiener filter: problems of application

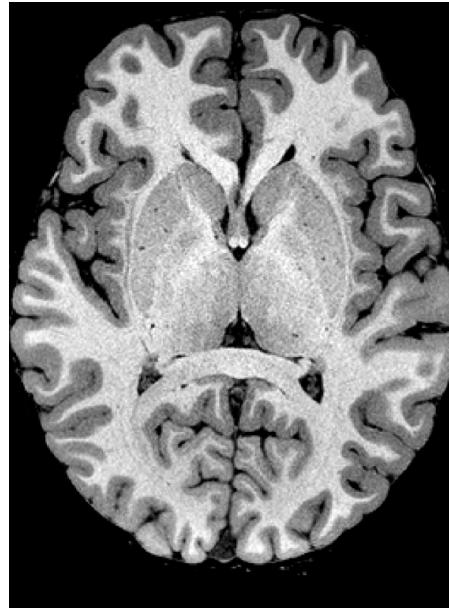
$$\begin{aligned} O(u, v) &= Wf(H)(H(u, v)I(u, v)) \\ &= (Wf(H)H(u, v))I(u, v) \end{aligned}$$

$Ef = Wf(H)H$  is the effective filter (should be 1)

- Conservative
  - if  $SNR$  is low tends to become low-pass blurring instead of sharpening
- $SNR = \Phi_{ii}(u, v)/\Phi_{nn}(u, v)$  depends on  $I(u, v)$ 
  - strictly speaking is unknown
  - power spectrum is not very characteristic
- $H(u, v)$  must be known very precisely

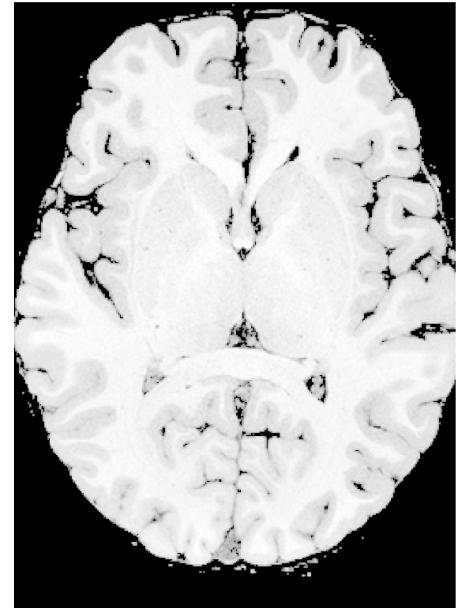


# Computer Vision



Original Image

Contrast  
Enhancement



Observation  
with  
Bad Contrast

## Contrast enhancement

Use 1 : compensating under-, overexposure

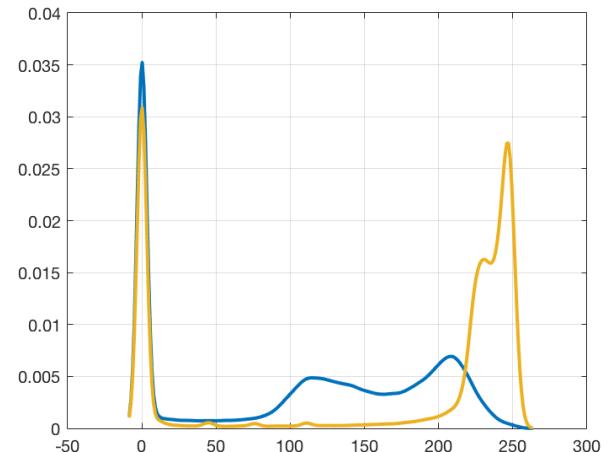
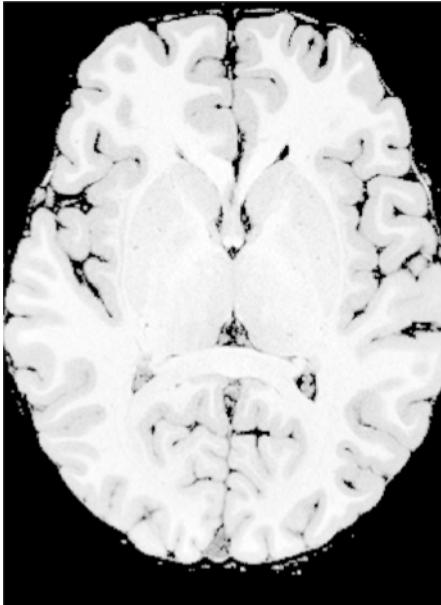
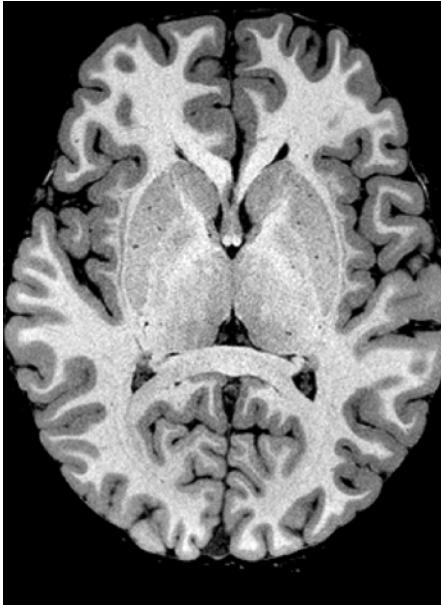
Use 2 : spending intensity range on interesting part of the image

We'll study *histogram equalisation*

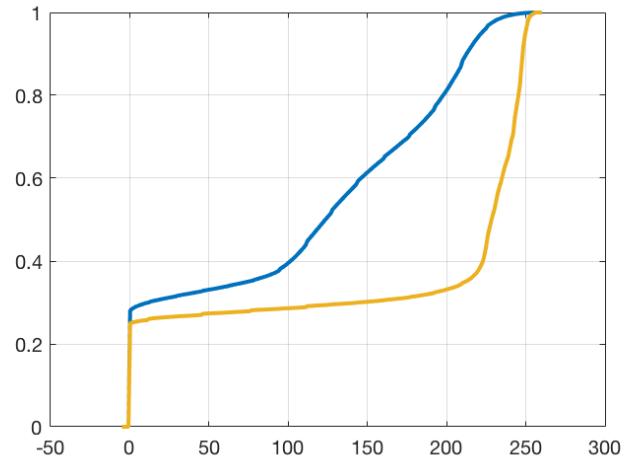


# Computer Vision

## Intensity distribution



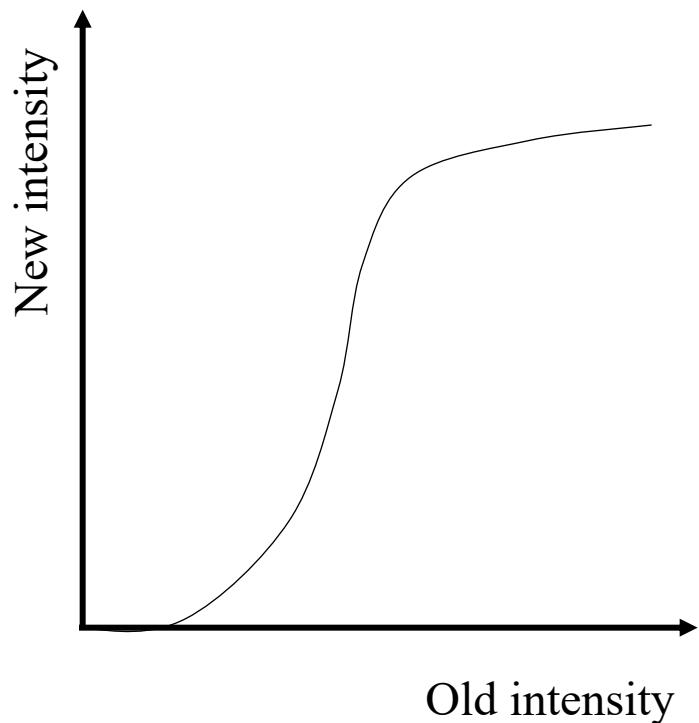
Histogram



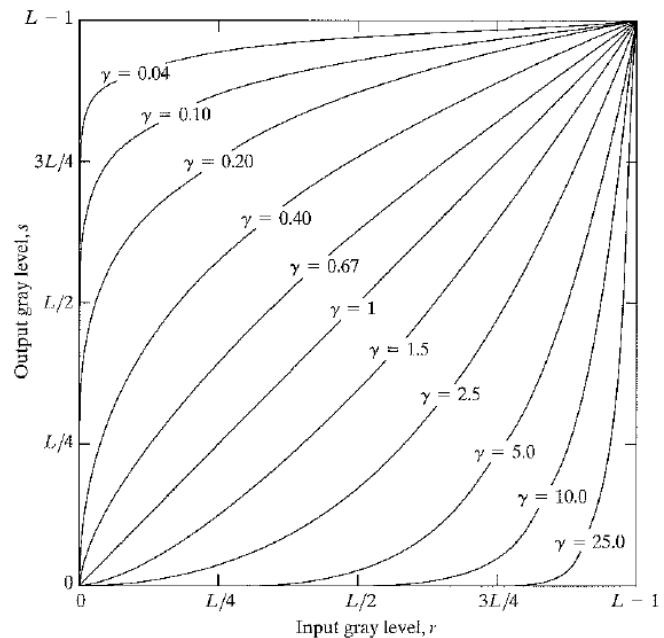
Cumulative histogram

# Intensity mappings

Usually monotonic mappings required



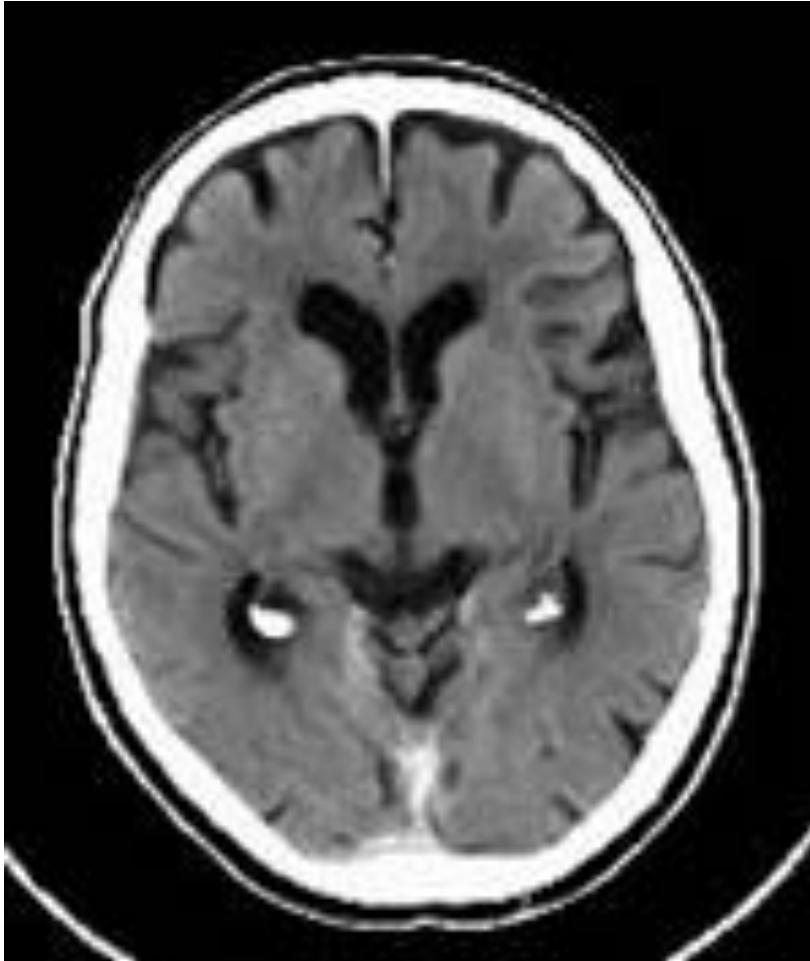
Generic transformation function



Power law transformation

$$I_{\text{new}} = I_{\text{old}}^{\gamma}$$

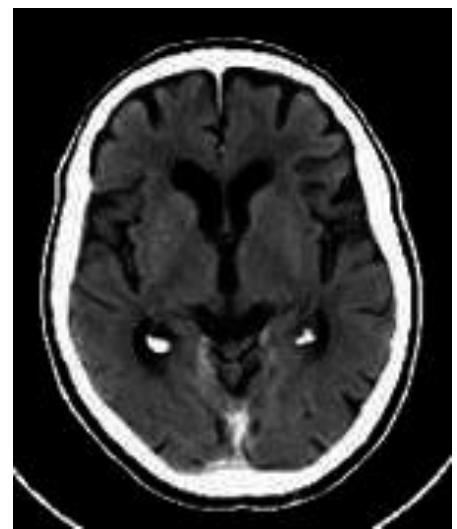
## Gamma correction



Original



$$\gamma = 2$$



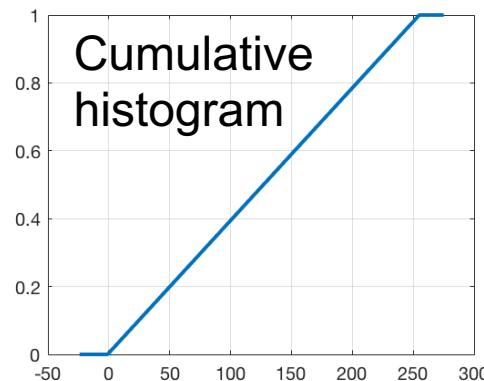
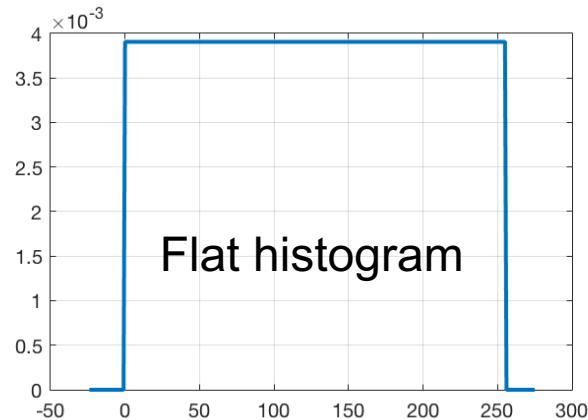
$$\gamma = 0.5$$

Slide 120

# HISTOGRAM EQUALISATION

WHAT :

create a flat histogram



HOW :

apply an appropriate intensity map  
depending on the image content

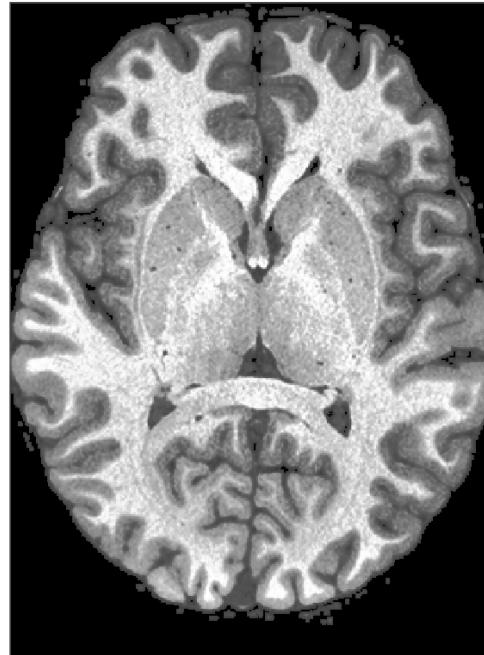
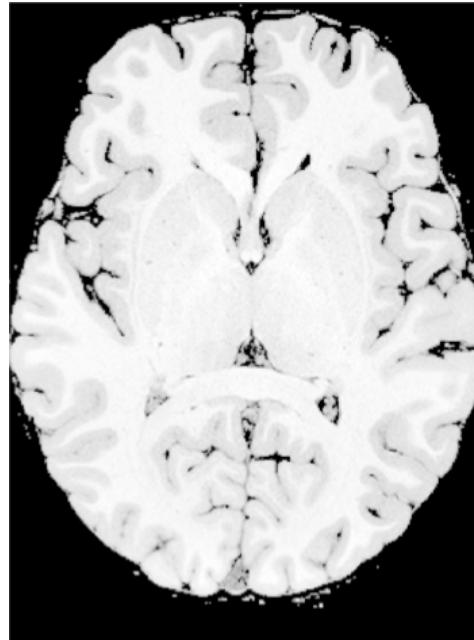
method will be generally applicable



## Histogram equalisation : example



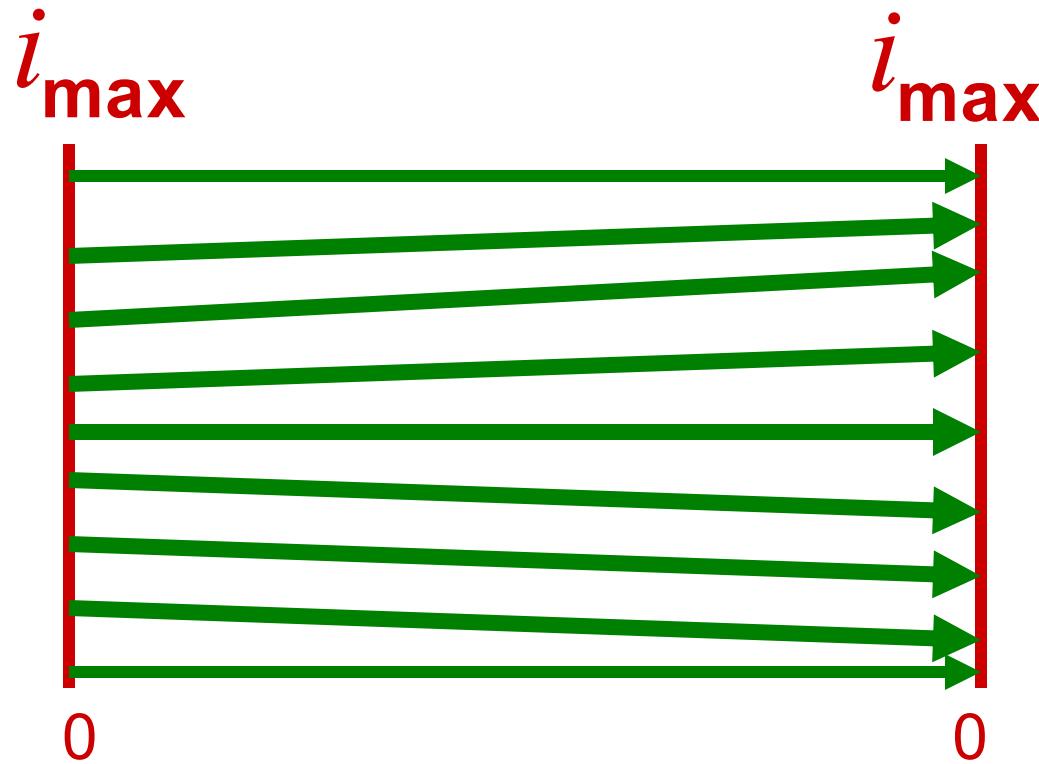
## Histogram equalisation : example



## Histogram equalisation : principle

Redistribute the intensities, 1-to-several (1-to-1 in the continuous case) and keeping their relative order, as to use them more evenly

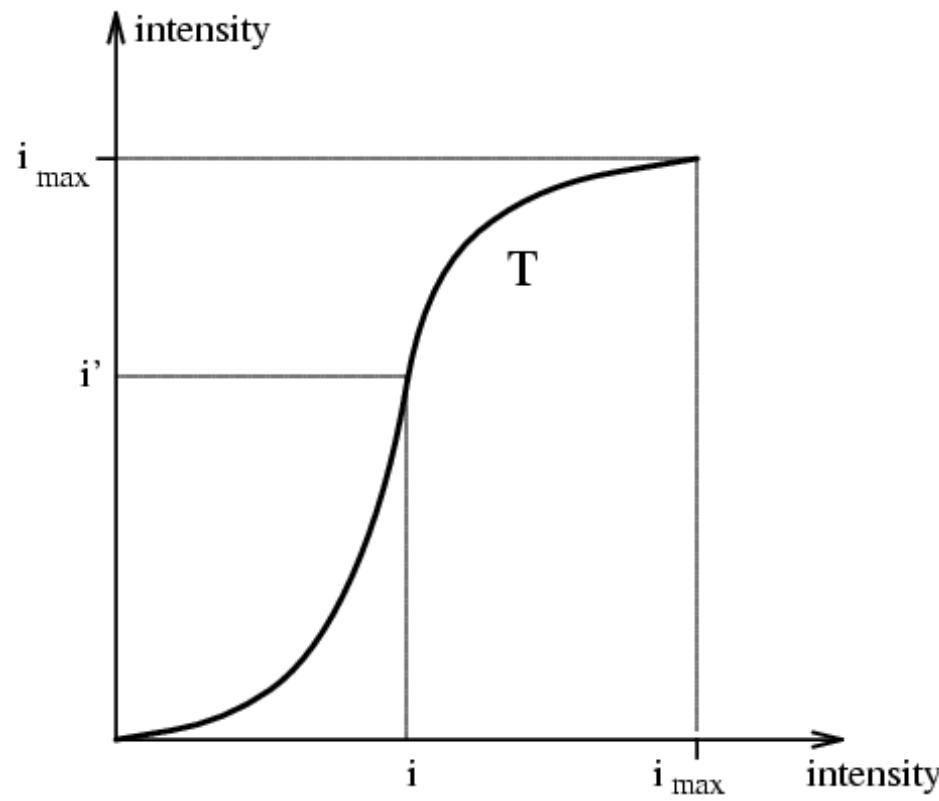
Ideally, obtain a constant, **flat histogram**



## Histogram equalisation : algorithm

This mapping is easy to find:

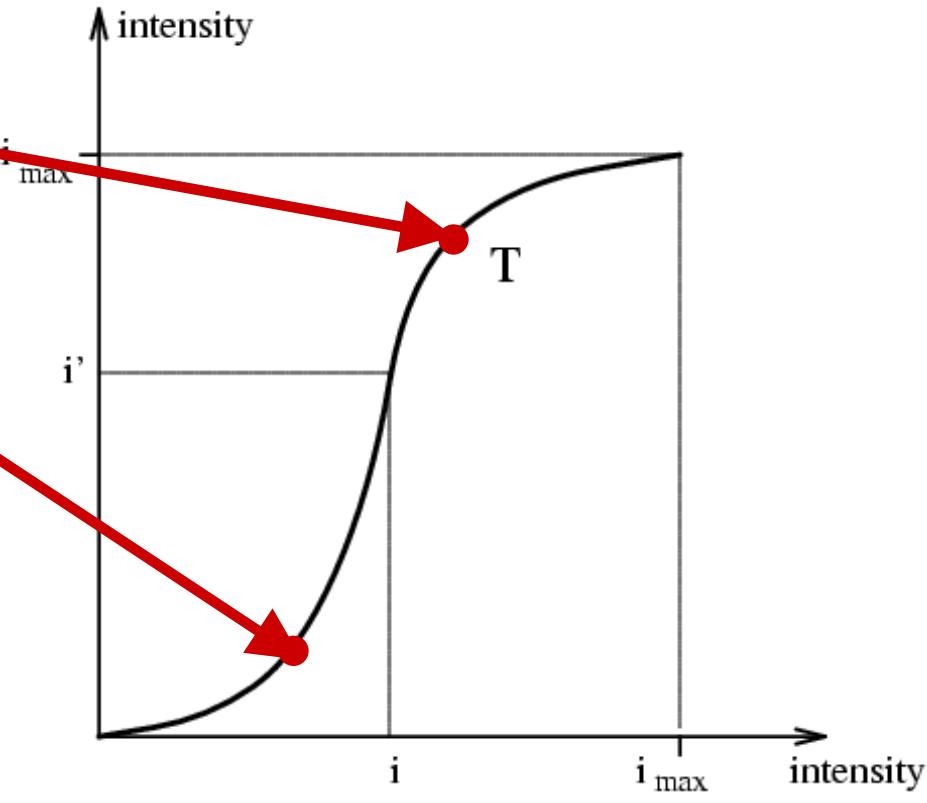
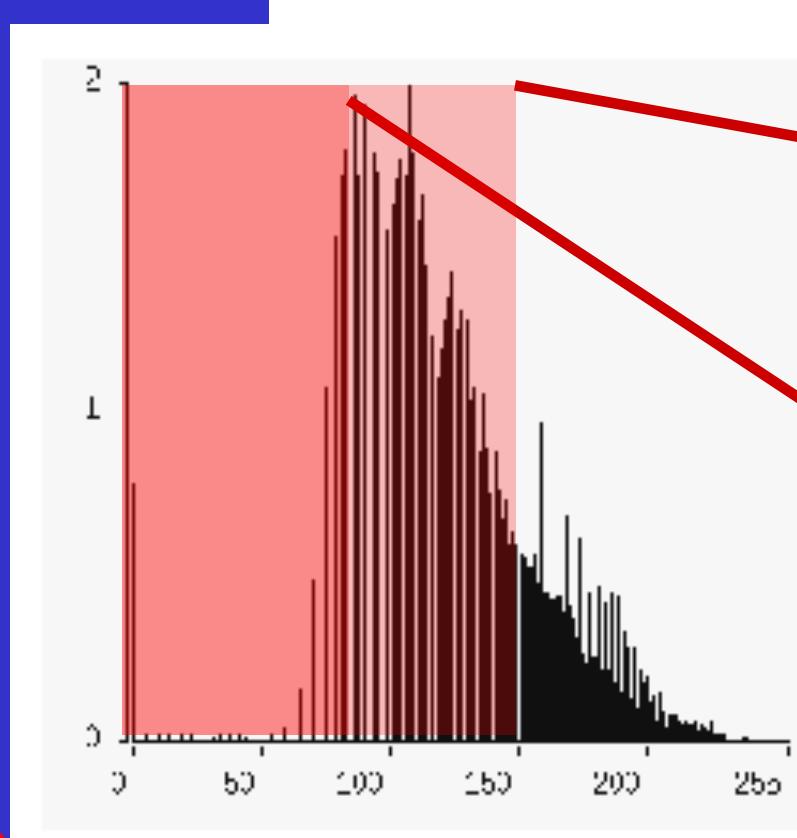
It corresponds to the **cumulative intensity probability**,  
i.e. by integrating the histogram from the left



## Histogram equalisation : algorithm

This mapping is easy to find:

It corresponds to the **cumulative intensity probability**,  
i.e. by integrating the histogram from the left



## Histogram equalisation : algorithm

suppose continuous probability density  $p(i)$

cumulative probability distribution :

$$P(i) = \int_0^i p(i^*) di^*$$

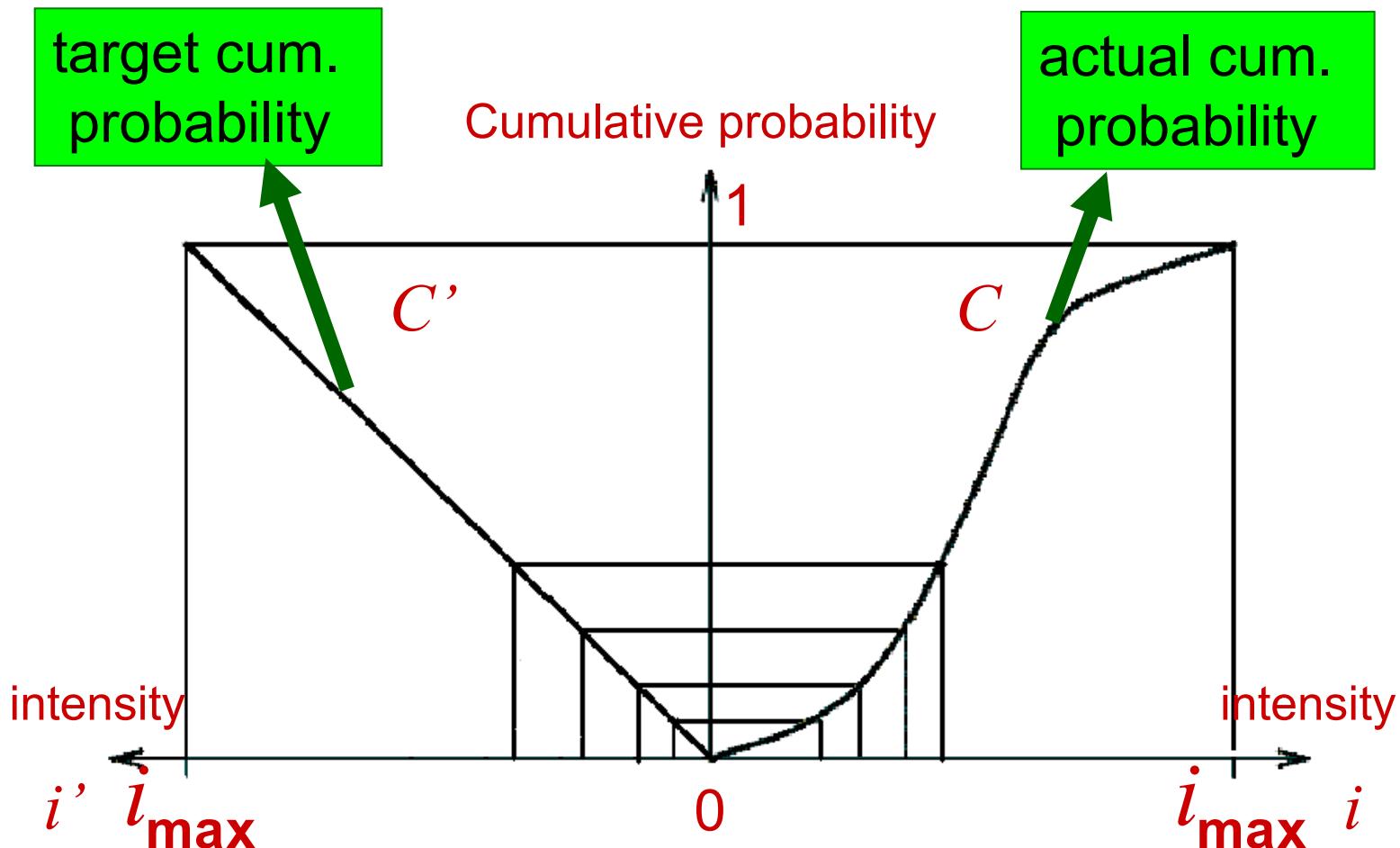
distribution as our map  $T(i)$ :

$$i' = T(i) = i_{\max} \int_0^i p(i^*) di^*$$

$$p' = p \frac{di}{di'} = p \left( \frac{1}{p} \right) \left( \frac{1}{i_{\max}} \right) = \frac{1}{i_{\max}} !!!$$



## Histogram equalisation : sketch

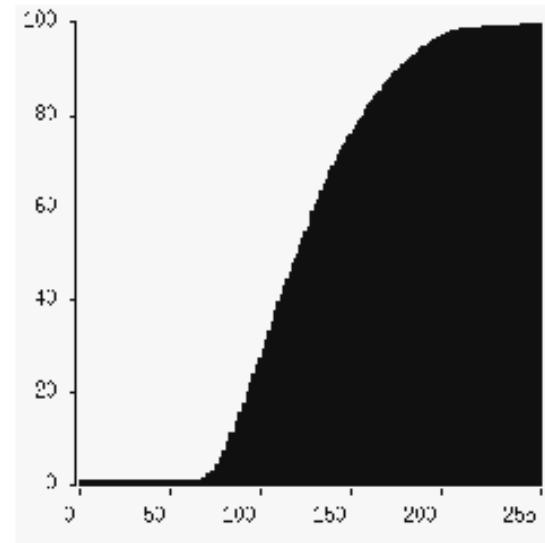


$$i' = T(i) = i_{\max} C(i) = i_{\max} \int_0^i p(i^*) di^*$$

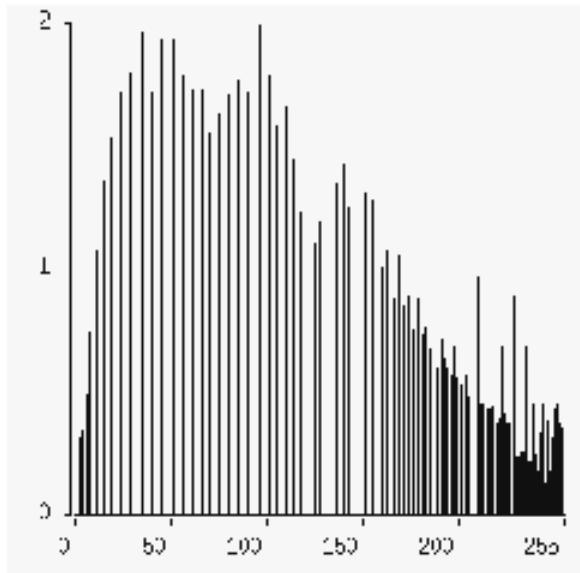
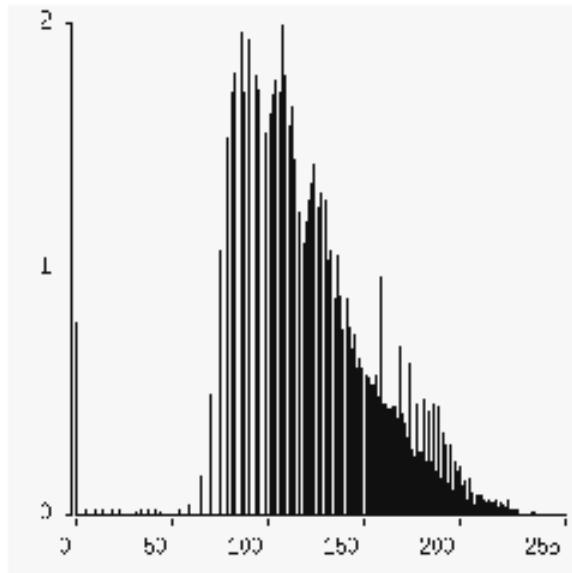


## Histogram equalisation : result

intensity map :

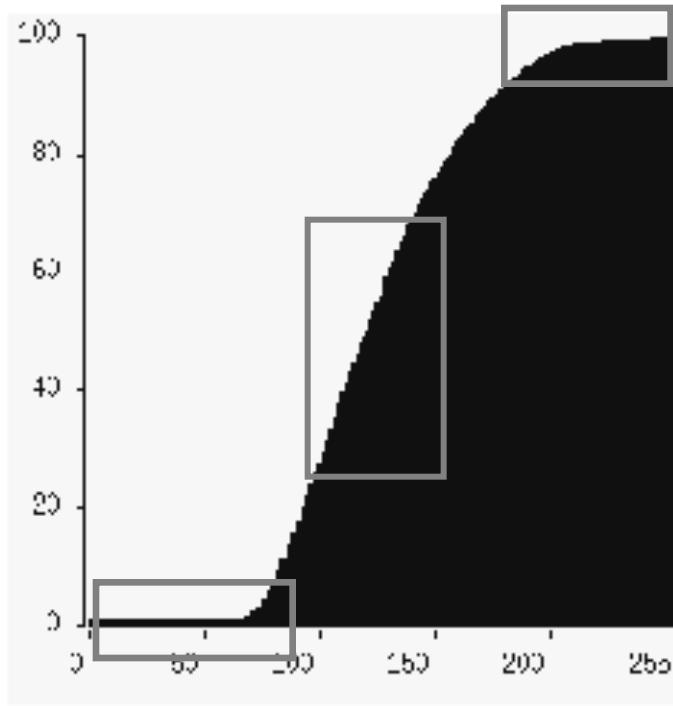


original and flattened histograms :



## Histogram equalisation : analysis

Intervals where many pixels are packed together are expanded

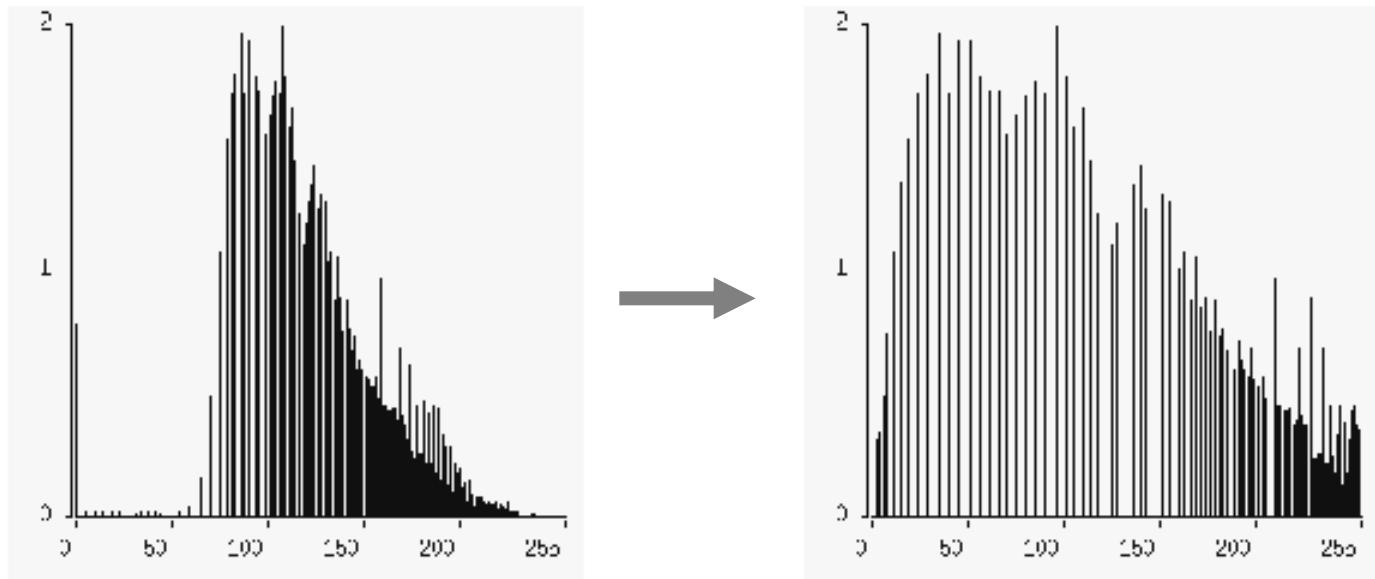


Intervals with only few corresponding pixels are compressed



## Histogram equalisation : analysis

... BUT we don't obtain a flat histogram



This is due to the discrete nature of the input histogram and the equalisation procedure

Jumps in the discretised cumulative probability distribution lead to gaps in the histogram



## Histogram equalisation : example revisited



## Histogram equalisation : generalisation

Find a map  $i' = T(i)$  that yields probability density  $p'$

$$C'(i') = \int_0^{i'} p'(w) dw = \int_0^i p(v) dv = C(i).$$

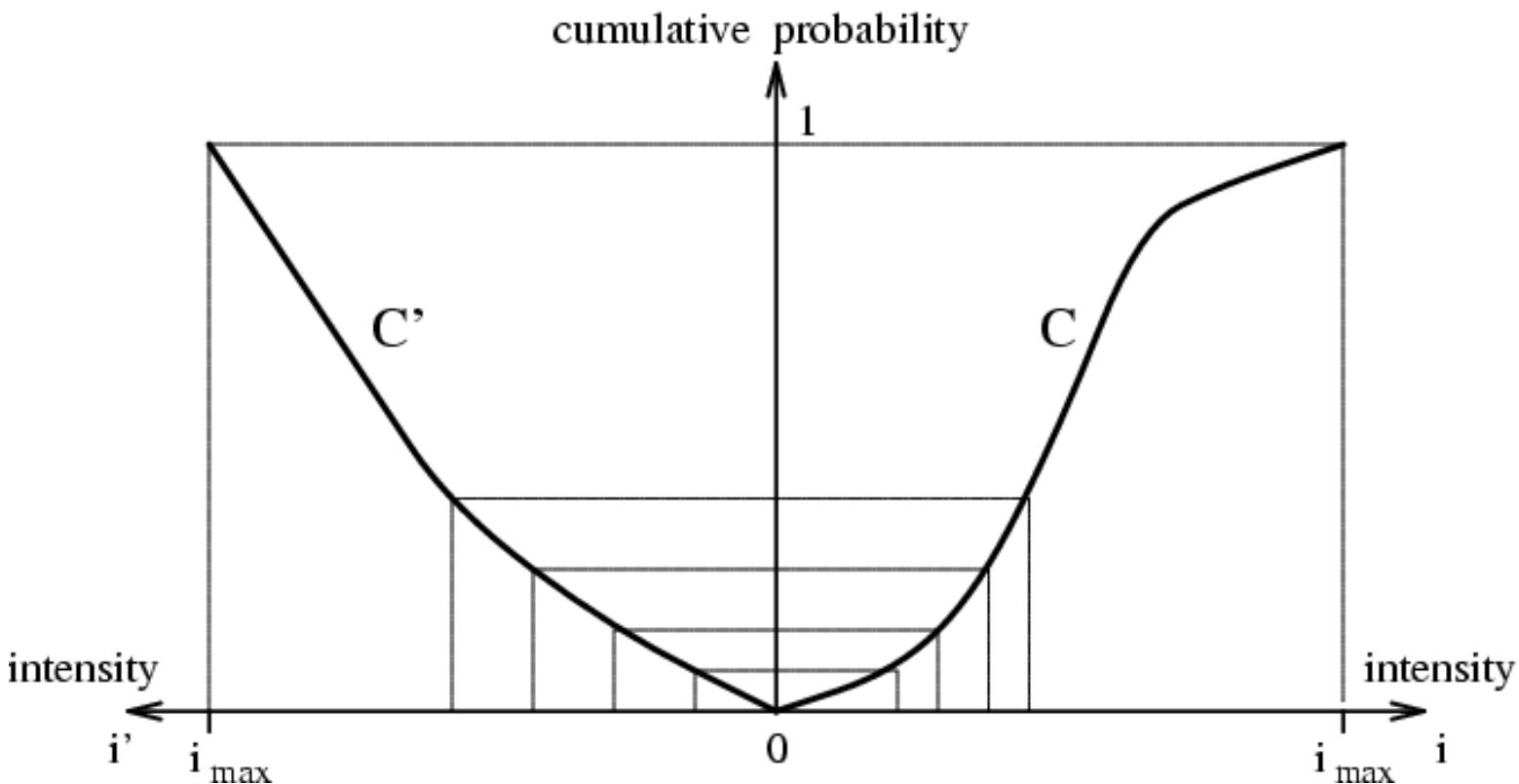
with  $C'(i')$  and  $C(i)$  the prescribed and original cumulative probability distributions

Thus

$$i' = C'^{-1}(C(i))$$



## Histogram equalisation : sketch



$$i' = C'^{-1}(C(i))$$

