March 25, 2020 18:21

Homework #10, EECS 598-006, W20. Due **Thu. Apr. 03**, by 4:00PM

1. [41] Image super-resolution using wavelet sparsity regularizer

In a **image super-resolution** problem, we are given a low-resolution image y = vec(Y) and the goal is to create a higher resolution image x = vec(X) from it. Usually there is noise in the given image too, so an appropriate measurement model is $y = Ax + \varepsilon$, where A is a matrix (linear map) representing the down sampling operation. If we believe that the higher resolution image has sparse wavelet transform coefficients, then a reasonable optimization problem is:

$$\hat{\boldsymbol{x}} = \operatorname*{arg\,min}_{\boldsymbol{x}} \Psi(\boldsymbol{x}), \quad \Psi(\boldsymbol{x}) = \frac{1}{2} \left\| \boldsymbol{A} \boldsymbol{x} - \boldsymbol{y} \right\|_{2}^{2} + \beta \left\| \boldsymbol{D} \boldsymbol{W} \boldsymbol{x} \right\|_{1},$$

where W denotes an orthogonal discrete wavelet transform, and D is a diagonal matrix of 0 and 1 values to select the wavelet detail coefficients.

(a) [10] To solve the above optimization problem, we need code for A, which means we first need a mathematical model for how the low-resolution image y relates to the high-resolution image x in the absence of noise. If x[m, n] is a $M \times N$ digital image for $m = 0, \ldots, M-1$ and $n = 0, \ldots, N-1$, where M and N are even, then a typical model for a factor of two down-sampling is

$$y[m,n] = \frac{1}{4}(x[2m,2n] + x[2m+1,2n] + x[2m,2n+1] + x[2m+1,2n+1]), \quad \begin{array}{l} m = 0, \dots, M/2 - 1 \\ n = 0, \dots, N/2 - 1. \end{array}$$

Study the following code that implements A as a LinearMapAA object.

```
using LinearMapsAA  (n1,n2) = (64,128) \text{ # test size (M,N) just for illustration} \\ down1 = (x) -> (x[1:2:end,:] + x[2:2:end,:])/2 \text{ # 1D down-sampling by } 2x \\ down2 = (x) -> down1 (down1(x)')' \text{ # 2D down-sampling by factor of } 2x \\ A = LinearMapAA(x -> down2 (reshape(x,n1,n2))[:], (Int((n1/2)*(n2/2)), n1*n2))
```

The size of \mathbf{A} is $(MN/4) \times (MN)$ which would be too large to store for realistic image sizes, so we use LinearMapAA. To use this \mathbf{A} for optimization, you will also need a method for implementing the **adjoint** operation corresponding to multiplying by the transpose \mathbf{A}' . Think about the linear operation above and examine Matrix (A) ' for small image sizes. Then write a subroutine that performs the adjoint operation efficiently. Do not use any sparse functions.

Hint. The general ideas here are similar to the earlier HW involving diff2d_adj.

Your file should be named down2 adj.jl and should contain the following function:

```
"""
    x = down2_adj(y)

Let `down2` denote the linear downsampling operation where each 2×2 block
of image pixels is averaged to form one output pixel.
This routine returns the *adjoint* of that linear operation.

in
    - `y` `[n1 n2]` where `n1` and `n2` are even.

out
    - `x` `[2*n1 2*n2]`
"""
function down2_adj(array::AbstractArray{<:Number,2})</pre>
```

Submit your solution to mailto:eecs556@autograder.eecs.umich.edu.

(b) [0] Use your subroutine as part of the second argument of the LinearMapAA call, i.e., y -> down2_adj ???

Then test it for a small image size by the command: Matrix(A)' == Matrix(A')

Hint: think about reshape and [:] here.

March 25, 2020 18:21 2

(c) [3] Determine the Lipschitz constant of the gradient of the data term above. The answer is a number and you do not need opnorm to find it. Hint. First consider the case where the input image size is just 2×2 .

(d) [10] Write a script that applies 10 iterations of POGM to minimize the cost function above for data generated as follows and produces the plots and images in the subsequent parts.

```
using Random: seed!
using LinearMapsAA, Plots
using MIRT: Aodwt, pogm_restart, jim, ellipse_im
nx,ny = 192,256
Xtrue = ellipse_im(ny, oversample=2)[Int((ny-nx)/2+1):Int(ny-(ny-nx)/2),:]
down1 = (x) -> (x[1:2:end,:] + x[2:2:end,:])/2 # 1D down-sampling by 2x
down2 = (x) -> down1(down1(x)')' # 2D down-sampling by factor of 2x
Ytrue = down2(Xtrue); seed!(0); sig=0.1; Y = Ytrue + sig * randn(size(Ytrue))
W, scales, mfun = Aodwt((nx,ny)) # orth. discrete wavelet transform (LinearMap)
plot(jim(Xtrue, "true"), jim(Ytrue, "lo-res"), jim(Y, "noisy"))
```

Use $\beta = 0.05$ here. Also, for the 1-norm above, only regularize the wavelet detail coefficients, not the wavelet approximation coefficients, just as you did in a previous HW problem.

Submit a screenshot of your code to gradescope.

(e) [5] To apply any iterative algorithm to that cost function, we need an initial image $x_0 = \text{vec}(X_0)$. For this application, the initial image x_0 should be computed from y by replicating each pixel in y twice in each direction.

For example, if
$$\mathbf{Y} = \begin{bmatrix} 1 & 2 \\ 3 & 4 \end{bmatrix}$$
 then $\mathbf{X}_0 = \begin{bmatrix} 1 & 1 & 2 & 2 \\ 1 & 1 & 2 & 2 \\ 3 & 3 & 4 & 4 \\ 3 & 3 & 4 & 4 \end{bmatrix}$, for which $\mathbf{y} = \text{vec}(\mathbf{Y}) = \mathbf{A}\mathbf{x}_0 = \mathbf{A} \text{vec}(\mathbf{X}_0)$.

Submit a screen shot of your initial image to gradescope. It should look pretty similar to the true image.

- (f) [5] Plot the cost function versus iteration k for the POGM approach. You should see that POGM converges quite quickly, probably because W is unitary and A'A is block diagonal.
- (g) [5] Show images of the true x, the noisy low-resolution image y, the initial image x_0 , and the final image \hat{x} .
- (h) [3] Report the NRMSE values of x_0 and \hat{x} .
- (i) [0] You will find that the NRMSE improves only a little. Speculate why.
- (j) [0] Optional. Explore other wavelet types https://github.com/JuliaDSP/Wavelets.jl using the optional argument of Aodwt to try to improve the results.

March 25, 2020 18:21

2. [26] Compressed sensing MRI

This problem focuses on a relatively simple version of image reconstruction for magnetic resonance imaging (MRI). A simple model for 2D MRI is that the data consists of samples of the 2D **DFT** of a 2D slice of the object being scanned.

If X denotes a $M \times N$ (discretized) slice of the patient, then the data model for "fully sampled" 2D MRI is

$$oldsymbol{y} = ext{ fft (X) [:] } + oldsymbol{arepsilon} \in \mathbb{C}^{MN}$$

where the JULIA fft function computes the 2D FFT of a 2D input argument, and ε denotes a complex additive Gaussian noise vector of length MN. If we collect such fully sampled measurements, then image reconstruction is a trivial inverse 2D FFT:

$$\hat{X} = \text{ifft (reshape (y, M, N))}.$$

One way to reduce scan time in MRI is to collect fewer than MN samples for a $M \times N$ image and then used **compressed sensing** methods to estimate X from y. Let samp denote a boolean $M \times N$ array that is true for DFT coefficients that we sample, and false otherwise and let $K = \text{sum}(\text{samp}) \le MN$ denote then number of samples. Then for such "under-sampled" scans the measurement model becomes:

$$y = ext{fft}(X) ext{[samp]} + arepsilon \in \mathbb{C}^K.$$

Mathematically we can write this as

$$y = Fx + \varepsilon$$

where x = vec(X) and F denotes the $K \times MN$ matrix consisting of the K rows of the DFT corresponding to the elements of samp. Two equivalent ways to make F in JULIA for a 1D signal are:

```
F = \exp.(-2im*pi*(findall(samp).-1)*(0:N-1)'/N)

F = \exp.(-2im*pi*(0:N-1)*(0:N-1)'/N)[samp,:]
```

Such code is incomplete for the 2D DFT, and uses too much memory for large problems anyway.

We must use something like a LinearMapAA to represent F, e.g., as follows:

```
F = LinearMapAA(x \rightarrow fft(reshape(x, M, N))[samp], (sum(samp), M*N); T=ComplexF32)
```

You should think carefully about all of the arguments used in the above LinearMapAA call!

A typical compressed sensing model is to assume that Tx is sparse for some transform T, such as a wavelet transform. Under that model, a reasonable estimator is

```
\hat{\boldsymbol{x}} = \mathop{\arg\min}_{\boldsymbol{x} \in \mathbb{C}^{MN}} \frac{1}{2} \left\| \boldsymbol{F} \boldsymbol{x} - \boldsymbol{y} \right\|_2^2 + \beta \left\| \boldsymbol{D} \boldsymbol{T} \boldsymbol{x} \right\|_1,
```

where D is a diagonal weighting matrix. For now, we focus on the case where T is a unitary matrix, specifically an **orthogonal discrete wavelet transform**. As seen previously, the **proximal optimized gradient method** (**POGM**) is well-suited to such problems.

(a) [3] You are going to apply POGM to data generated as follows:

```
using Random: seed!
using FFTW: fft
using MIRT: Aodwt, jim
M,N = 192,256; Xtrue = zeros(M,N);
Xtrue[30:50,20:90] .= 1; Xtrue[90:100,100:110] .= 1; Xtrue[130:150,20:90] .= 1;
Xtrue[20:170,150:200] .= 1; Xtrue[150:151,160:161] .= 0
seed!(0); sampfrac = 0.3; samp = rand(M,N) .< sampfrac; sig = 1
mod2 = (N) -> mod.((0:N-1) .+ Int(N/2), N) .- Int(N/2)
samp .|= (abs.(mod2(M)) .< Int(M/8)) * (abs.(mod2(N)) .< Int(N/8))' # center
ytrue = fft(Xtrue)[samp]; y = ytrue + sig * randn(size(ytrue)) +
    lim * sig * randn(size(ytrue)); # complex noise!
T, scales, mfun = Aodwt((M,N)) # Orthogonal disc. wavelet transform (LinearMapAA)</pre>
```

As an easy warm-up, generate the data and then display the true image X_{true} and the sampling pattern as follows: plot(jim(Xtrue), jim(samp))

March 25, 2020 18:21

Make an initial $M \times N$ image X_0 by taking the inverse FFT of "zero-filled" k-space data, defined as follows:

```
zfill = zeros(eltype(y), M,N); zfill[samp] = y
```

Let X0 denote the inverse FFT of that data.

Make a nice display of these initial ingredients:

plot(jim(Xtrue, "Xtrue"), jim(samp, "sampling", fft0=true), jim(X0, "X0"))

If your code is correct, X_0 should look like a blurry version of X_{true} because it is missing many high spatial frequency components that correspond to fine details. (The fft0=true option displays the DFT coefficients with 0 in the middle, akin to MATLAB's fftshift command, which is usually more intuitive.)

Optional: also show the wavelet detail coefficients of $X_{\rm true}$.

Submit a screenshot of your figure to gradescope.

- (b) [0] Can you explain the sampling pattern? If not, ask someone in class who knows about MRI.
- (c) [3] To apply a gradient-based method, we need the (best) Lipschitz constant L for the data term above. Determine L. Hint. $F = P\sqrt{MN}(Q_N \otimes Q_M)$, where Q_N having elements $Q_{kn} = \frac{1}{\sqrt{N}} \exp(-i2\pi kn/N)$ denotes the $N \times N$ unitary DFT matrix, and P denotes the $K \times MN$ matrix that is all zeros except for a single 1 in each row that selects the DFT coefficients that we sample. Specifically: $Px = x \lceil \text{samp} \rceil$. Now think about P'P.
- (d) [5] The gradient of the data term above is F'(Fx y), so to apply any gradient-based method to this optimization problem, we need the adjoint operation F'. Modify the initial LinearMapAA definition given above to provide that capability.

Hint. If $A \operatorname{vec}(X) = \operatorname{fft}(X)$ [:], then A is not unitary, but $A^{-1} = \frac{1}{MN}A'$. See inverse DFT.

Hint. MIRT.jl includes a function embed that may be useful.

Write a JULIA script that runs POGM and produces the figures below.

Submit a screenshot of your script, including the modified LinearMapAA call, to gradescope.

Choose the diagonal weighting matrix D to regularize only the detail wavelet coefficients.

Use $\beta = 0.004MN$ and 100 iterations.

- (e) [5] Plot the cost function $\Psi(x_k)$ (no logarithm) versus iteration k. Optional: compare to ISTA and FISTA.
- (f) [5] Plot the peak signal-to-noise ratio (PSNR) of x_k versus iteration k, where PSNR is defined by

$$20\log_{10}\left(\frac{\left\|\operatorname{vec}(\boldsymbol{X}_{\operatorname{true}})\right\|_{\infty}}{\left\|\operatorname{vec}(\boldsymbol{X}_{k}-\boldsymbol{X}_{\operatorname{true}})\right\|_{2}/\sqrt{MN}}\right)$$

You should see a dramatic rise in the PSNR, from about 25dB to over 50dB.

(g) [5] Make figure showing X_{true} , X_0 , \hat{X} and the corresponding error images $X_0 - X_{\text{true}}$, $\hat{X} - X_{\text{true}}$. You should see that the error is reduced dramatically.

Optional problem(s) _

3. [0] **Sparsity regularizers**

Challenge. Consider the following two optimization formulations for transform sparsity:

$$\begin{split} \hat{\boldsymbol{x}}_0 &= \operatorname*{arg\,min}_{\boldsymbol{x}} \Phi_0(\boldsymbol{x}), \quad \Phi_0(\boldsymbol{x}) \triangleq f(\boldsymbol{x}) + \beta \, \|\boldsymbol{T}\boldsymbol{x}\|_1 \\ \hat{\boldsymbol{x}}_\alpha &= \operatorname*{arg\,min}_{\boldsymbol{x}} \Phi(\boldsymbol{x}; \alpha), \quad \Phi(\boldsymbol{x}; \alpha) \triangleq f(\boldsymbol{x}) + \beta R_\alpha(\boldsymbol{x}), \quad R_\alpha(\boldsymbol{x}) = \frac{1}{\alpha} \left(\min_{\boldsymbol{z}} \frac{1}{2} \|\boldsymbol{T}\boldsymbol{x} - \boldsymbol{z}\|_2^2 + \alpha \|\boldsymbol{z}\|_1 \right), \end{split}$$

where $\beta > 0$ and $\alpha > 0$. Assume f(x) is convex. You may also assume that \hat{x}_0 and \hat{x}_{α} are unique minimizers.

Prove, or disprove this conjecture: $\lim_{\alpha\to 0} \hat{x}_{\alpha} = \hat{x}_{0}$.