

# Fluorescence yield for plastic scintillators after irradiation

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## Abstract

The ratio of the fluorescence yield versus wavelength for plastic scintillators EJ-200 and EJ-260 before and after irradiation by a  $^{60}\text{Co}$  source for various doses and dose rates and for different concentrations of the primary and secondary dopant was measured. While the nominal dopant concentration gives the highest light output prior to irradiation, a higher concentration is found to be optimal for irradiated plastics.

*Keywords:* plastic scintillator, fluorescence, radiation hardness

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## 1. Introduction

Organic scintillators such as polystyrene (PS) or polyvinyltoluene (PVT) containing wave-length shifting additives in solution have long been popular elements in detectors used in particle physics, nuclear physics, radiation safety, and health physics applications due to their high light output, low cost, fast response, and versatility of physical construction. Prolonged exposure of plastic scintillator to ionizing radiation, however, can result in damage: light self-absorption (yellowing) increases and the transfer efficiency of the initial excitation of the polymer to the dopants combined with the dopant's probability of radiative decay ("initial light output") can lessen. In this paper, we present measurements

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of the ratio of the light output before and after irradiation for two different types of plastic scintillator manufactured by Eljen corporation, EJ-200 (similar to BC-408 from Bicron corporation) and EJ-260 (similar to BC-428), before and after irradiation by a  $^{60}\text{Co}$  source for various doses and dose rates and for  
15 different concentrations of the primary and secondary dopant. Dose rate effects are of interest because materials testing is typically done at much higher dose rates than the scintillator will experience in use, because of the cost of reactor time. Dose rate effects may be responsible for the factor of three larger light loss with integrated luminosity in the CMS endcap calorimeter [1, 2] than expected  
20 based on high dose rate exposures using  $^{60}\text{Co}$  sources [3, 4].

The effect of dose and dose rate on radiation-induced yellowing have been the subject of many investigations. The results are summarized in [5]. Dose rate effects during irradiation for the yellowing are well documented [5, 6, 7, 8, 9, 10, 11]. The presence of oxygen plays an important role. The studies show  
25 that the penetration depth of oxygen into the substrate depends on the dose rate: at lower dose rates, oxygen penetrates more deeply. As discussed in [12], the presence of oxygen increases the number of migration mechanisms for the radicals produced during irradiation. Because of the importance of the interaction of oxygen with radicals produced from the substrate during irradiation, this  
30 can lead to dose rate effects. Simulations based on oxygen diffusion have been shown to reproduce the time dependence of the induced attenuation length in scintillators based on PS and PMMA [7]. Thus, immediately after irradiation at a high dose rate (Mrads/hr), the probability of absorption for visible light increases for wavelengths shorter than around 600 nm (yellow) due to color  
35 centers that form in the substrate [13]. At low dose rate, because the oxygen penetrates deeper, the initial damage is less. At very low dose rates, sufficient migration can occur even without oxygen, reducing the initial damage. After irradiation, oxygen continues to play a role. Oxygen diffuses into the plastic, reduces the color center density, and the plastic “bleaches”. On time scales of  
40 the order of months, the bleaching stops, and some permanent damage (color centers) remains [5]. The amount of permanent damage seems to be indepen-

dant of the dose rate [5]. Oxygen is essential for this curing process, although samples irradiated in inert atmospheres have smaller permanent damage, even if the initial damage for high dose rate exposures maybe larger [14].

45 Studies on the effect of radiation on the light yield are fewer than those on self-absorption. Several studies indicate that the damage is to the substrate and/or the transfer of its excitation to the dopants and not to the dopants themselves. In an early study, Rosman and Zimmer [15] found that the light output for organic scintillators based on PS versus dose is described, approx-  
 50 imately and for relatively large dose rates, by a double exponential, with a small-dose component whose constant is approximately 100 Mrad. For a PS scintillator doped with 1.5% TPB, they also used UV light to illuminate the samples and found that this showed less reduction of light than excitation via charged particles. Since PS is transparent to UV, this indicates that the TPB  
 55 was not damaged, and instead the damage was either to the PS or the migration of excitation from the PS to the dopant. Subsequent studies ([16, 10]) came to a similar conclusions for liquid scintillators and for various plastic scintillators respectively.

If the damage is related to oxygen diffusion, a dose rate effect is expected.  
 60 An interesting result, from 1996, is described in [17]. They look at light output reduction for two PS-based scintillators (SCSN-38 and SCSN-81, from Kuraray) and a PVT-based scintillator (Bicron-499-35). Measurements were done as a function of time subsequent to irradiation, until the light output stabilized, using a  $^{241}\text{AM}$  alpha source. They find a reduction in post-recovery light output that  
 65 depends linearly on the log of the dose rate for dose rates ranging from 0.01 to 2 Mrad/hr. Note that the effect is not small: for a dose of 2 Mrad, the light loss is negligible for a dose rate of 2 Mrad/hr but 20% for a dose rate of 0.01 Mrad/hr for SCSN-81.

Two studies may be in contradiction to those described above. Two indicated  
 70 very little damage to light output, and one indicated damage to the dopant.

In [11], from 1993, SCSN-81, SCSN-23, and 3HF (based on PS) were studied at doses between 10 krad to 1 Mrad and three dose rates, 1.2 Mrad/hr, 0.01

Mrad/h, using a long piece of plastic and a  $^{90}\text{Sr}$  beta source. They also looked at 0.0003 Mrad/hr with doses of 1.3 and 0.57 Mrad. They saw a small decrease  
75 in light output after recovery, indicating very little effect on the light yield. In another study, by Bross, Pla-Dalmau, *et al.* from 1991 [13], the authors looked at light output for various primary (DAT, MOPOM, OLIGO408, OLIGO415A) and secondary (BBQ, K27, DMPOPOP, 3HF) dopants in PS for a dose of 10 Mrad accumulated with a relatively high dose rate (0.4 Mrad/h). They looked  
80 at this for 2 different concentrations of the secondary dopant. They optimized the concentration of the first dopant using the light output before irradiation. They found no change to the intrinsic light output, indicating at high dose rates the dopants were not damaged by this large dose. Perhaps the damage was not seen in the first due to the relatively low doses and in the second due to the  
85 high dose rate.

In [7], decreased light output for a plastic scintillator from Kuraray, SCSN-38, which is based on PS with b-PBD primary and BDB secondary dopants, was seen. The main absorption wavelengths for PS typically range between between 230 to 260 nm, for the primary dopant b-PBD between 270 to 330 nm, and for  
90 the wavelength shifting dopant BDB between 310 to 400 nm. They found that light loss was much stronger in the presence of oxygen. Note that while oxygen plays a beneficial role in regards to annealing of induced absorption length at the end of radiation, it plays a detrimental role in regards to light output. They also found the light output loss was independent of the wavelength of the light  
95 that was used to excite the scintillator when it was varied between 230 and 400 nm. From this they conclude that the damage is due to destruction of the second floor. This is different than what was found in the other studies, which indicated that damage to the dopants was small and that damage was mostly to the substrate, although different dopants were used in the studies. By looking  
100 at the damage as a function of the thickness of the scintillator, they concluded that the BDB molecules are mainly destroyed near the surface, which lends support to a mechanism involving oxygen diffusion.

If there is damage, and the damage is to the transfer mechanism, increasing

the dopant concentration could help. In [18] (perhaps better documented in  
105 [5]), the authors show that for a PS fiber with primary dopant of PTP and  
secondary dopant of 3HF, increasing the dopant concentration from nominal to  
20 times nominal continuously increases the light output after 100 Mrad (dose  
rate unknown).

In [19], the radiation resistance of BC-408 (from Bicon Corporation) was  
110 studied for different concentrations of the dopant from half to 3/2 the nominal  
concentration. The study was done at very high dose rate (36 Mrad/hr) and a  
total dose of 3 Mrad. They saw that varying the concentration of the secondary  
fluor did not affect the output as studied with a  $^{207}\text{Bi}$  electron source. They  
found decreasing the secondary dopant made it less rad hard, but increasing did  
115 not help.

In order to understand the relative role of destruction of the dopants ver-  
sus damage to the substrate for modern scintillating plastics, we have studied  
the light output for two plastic scintillators, EJ-200 and EJ-260, varying the  
concentration of the dopants, for different total doses and dose rates.

## 120 2. Measurements

Both EJ-200 and EJ-260 use PVT as a substrate. EJ-200 has a light output  
that is 60% of anthracene and a wavelength of maximum emission of 435 nm  
(blue). EJ-260 also has a light output that is 60% of anthracene but a wave-  
length of maximum emission of 490 nm (green). Eljen prepared scintillator bars  
125 with dimensions of 1x1x5cm. For the EJ-200, bars were made with concen-  
tration of the primary scintillation dopant at 0.5, 1.0, 1.5, and 2.0 that of the  
standard concentration. For the EJ-260, bars with made with concentrations of  
the primary (x) and secondary (p) dopant of 1x1p, 1x2p, 1x4p, 2x1p, 4x1p, 2x2p,  
and 4x4p. The fluorescence output was measured using a fluoromax-4 fluo-  
130 rometer by Horiba Scientific using a right-angle configuration and an excitation  
wavelength of xx nm. For the absorption measurements, a xx by xx was used.  
Air was used as the reference. In [13], the integration of the fluorescence spectra

was shown to reproduce the results using a  $^{207}\text{Bi}$  source to within a few percent for most dopants.

135 Radiations were done using a  $^{60}\text{Co}$  source at the University of Maryland with an activity of xxx. The dose was measured using i don't know

Figure 4 shows the spectra for EJ-200 with nominal doping before irradiation and after 30 Mrad at 1 Mrad/hr and after 50 Mrad at 1 Mrad/hr.



Figure 1: Emission spectrum for EJ-200 at nominal doping before irradiation, after 30 Mrad at 1 Mrad/hr and after 50 Mrad at 1 Mrad/hr.

Table 1 shows the ratio of the light output at xxx nm for the EJ-200 to that  
 140 before irradiation for different doses, dose rates, and dopant concentrations.  
 Figure 2 shows the ratio of the light output at xxx nm for the EJ-200 to that  
 before irradiation as a function of dose rate for several total doses.

Tabl 2 shows the ratio of the light output at xxx nm for EJ-260 to that  
 before irradiation for different doses, dose rates, and dopant concentrations.  
 145 Figure 3 shows the ratio of the light output at xxx nm for EJ-260 to that before  
 irradiation as a function of dose rate for several total doses.

Table 1: Ratio of average light output at **xxx nm** to that before irradiation for EJ-200 scintillator. For the concentrations of the dopants, NpMs refers to N times the default concentration of primary and M times the default concentration of the secondary dopant the commercial version of the product.

Dose (Mrad)	Dose rate (Mrad/hr)	light output ratio for dopings			
		1p1s	0.5p1s	1.5p1s	2.0p1s
0	—	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>
2	0.1	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
2	0.3	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
2	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
4	0.1	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
4	0.3	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
4	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
10	0.3	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
10	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
30	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
50	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>

### 3. Interpretation

If this dose rate effect is due to oxygen diffusion, then we expect it to be governed by the diffusion equation. Since the oxygen diffusion depth is greater at lower dose rates, we expect the damage for the same dose at different dose rates to increase up to the point where the dose rate is low enough that oxygen permeates the entire sample. The dose rate effect should plateau at this point. Specifically, we predict (following [7]) that the light output reduction should depend on both the dose and the dose rate as:

$$L(R, D) = 1 - [f(D)Z(R) + a(D)(1 - Z(R))]$$

where L is the % light yield, D is the dose, R is the dose rate, Z(R) is the fraction of the scintillator containing oxygen and is given by

$$Z(R) = \min(\frac{2z_0(R)}{d}, 1)$$



Figure 2: Ratio average light output for EJ-260 at **xxx nm** to that before irradiation versus dose rate for several total doses.

where  $d$  is the thickness of the scintillator and  $z_0$  gives the depth of scintillator penetrated by oxygen,  $a(D)$  is related to the fraction of quenching in the part of the scintillator containing oxygen and is given by  $1 - e^{-a_0 D}$ , and  $f(D)$  is related to the fraction of quenching in the part of the scintillator not containing oxygen and is given by  $1 - e^{-f_0 D}$ . The diffusion depth  $z_0(R)$  is given by diffusion theory as

$$z_0(R) = \sqrt{\gamma/R}$$

where  $\gamma$  is a property of the substrate and the radicals that are dissolved in that substrate during the diffusion process. The value for  $\gamma$  depends on the material, oxygen pressure, radical concentration (which is proportional to the dose) and temperature. The minimization in  $Z(R)$  occurs because the fraction of scintillator containing oxygen can not exceed one. Note that this equation assumes the temperature and the surrounding atmosphere is held constant, as this can affect diffusion.



Table 2: Ratio of light output at **xxx nm** to that before irradiation for EJ-260 scintillator. For the concentrations of the dopants, NpMs refers to N times the default concentration of primary and M times the default concentration of the secondary dopant the commercial version of the product.

Dose (Mrad)	Dose rate (Mrad/hr)	light output ratio for dopings						
		1p1s	2p1s	4p1s	1p2s	1p4s	2p2s	4p4s
0	—	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
2	0.1	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
2	0.3	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
2	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
4	0.1	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
4	0.3	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
4	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
10	0.3	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
10	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
30	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>
50	1.0	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>	<b>xx</b>

#### 155 4. Conclusions

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Figure 3: Ratio average light output for EJ-260 at **xxx nm** to that before irradiation versus dose rate for several total doses.

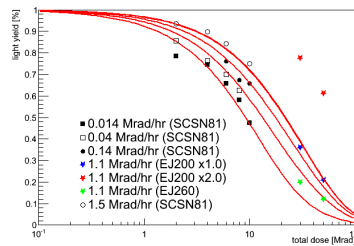


Figure 4: Comparison of results with data from Biagtan *et al.* [17]

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