# Multi-block partial least squares for muscle synergies Sean Bittner sean.bittner@epfl.ch July 15, 2015

### 1: Introduction

It has been shown in [1] that a multi-block partial least squares approach can be useful for extracting corticomuscular couplings at a group level. This works by splitting the data into blocks by subject. The algorithm allows patterns to be learned at a subject level, and combined at the super level. Regression happens at both the sub-level and super-level.

In the case of our study, we are interested in looking at the patterns associated with particular muscle synergies. Muscle synergies are the result of dimensionality reduction performed on EMG signals. Applying independent component analysis to EMG data allows the extraction of components describing muscle groups that are activated together. The co-activation of these muscle groups is most likely the result of modularization of limb control in the spinal cord.

These muscle synergies can be ranked in order of variance explained. It has been shown that the ordered muscle synergies across healthy patients share much similarity. Multi-block PLS allows us to model subject EMG activation at an individual level. Since we are interested in the EEG features related to particular muscle synergy activation, I propose a method for learning group level EEG features which couple with particular muscle synergy activation.

# 2: Three-way multi-block partial least squares

Three-way mbPLS extends mbPLS from 2D arrays to multiway arrays. Now, we can store 3D data in the input block [1]. For example, we can use eeg spectrograms where the three dimensions are time points X frequency bins X electrodes. Or, we can show frequency connectivity with a measure such as partial directed coherence where the dimensions would be time points X frequency bins X electrode connectivity. Below is the specification of three-way mbPLS.

Sub-level decomposition:

$$X_b = \sum_{k=1}^K r_{b,k} \otimes a_{b,k} \otimes p_{b,k} + E_b$$

$$Y_b = \sum_{k=1}^K s_{b,k} \otimes q_{b,k} + F_b$$

Super-level decomposition:

$$R_k = [r_{1,k}, r_{2,k}, ..., r_{b,k},]$$
$$R_k = t_k w_{sup}^T$$

$$S_k = [s_{1,k}, s_{2,k}, \dots, s_{b,k},]$$
$$S_k = u_k q_{sup}^T$$

Inner Relation:

data blocks.

$$u_k = \beta_k t_k$$

A requirement for partial least squares is that  $X_b$  and  $Y_b$  must be mean-centered with unit variance.  $r_{b,k}$  and  $s_{b,k}$  are the temporal signatures of the kth component of subject b for the predictor and response blocks respectively.  $a_{b,k}$  and  $p_{b,k}$  represent spectral patterns and spatial patterns respectively. In the case of EEG spectrogram  $p_{b,k}$  represents electrode positions, and for EEG PDC,  $p_{b,k}$  represents connections between electrodes.  $q_{b,k}$  represents the kth EMG activation pattern for subject b.

Algorithm 1 shows the three-way mbPLS algorithm:

```
Algorithm 1 Three-way mbPLS algorithm from [1]
```

```
1: Choose start u
  2: repeat
  3: Compute the auxiliary matrix \mathbf{Z}_b whose (f,c)^{th} element is given by Z_{b,fc} \leftarrow \sum_{t=1}^{N_t} X_{b,tfc} u_t for
       f \in [1, N_f], c \in [1, N_c], b \in [1, B]
  4: Concatenate the auxiliary matrices \mathbf{Z} \leftarrow [\mathbf{Z}_1, \mathbf{Z}_2, ..., \mathbf{Z}_b]
  5: Perform singular decomposition on Z:
  6: [\mathbf{g}, \sigma, \mathbf{h}] \leftarrow SVD(\mathbf{Z}, 1), where \mathbf{g} and \mathbf{h} are the first sing. vec. of Z
  7: for b = 1 \text{ to } B do
             \mathbf{a}_b \leftarrow g
             \mathbf{p}_b \leftarrow [h_{(b-1)N_c+1}, h_{(b-1)N_c+2}, ..., h_{(b-1)N_c+N_c}]
             \mathbf{r}_b \leftarrow [\mathbf{r}_{b,1}, \mathbf{r}_{b,2}, ..., \mathbf{r}_{b,N_t}] where r_{b,t} \leftarrow \sum_{f=1}^{N_c} X_{b,tfc} a_{b,f} p_{b,c} for t \in [1, N_t]
11: end for
12: \mathbf{R} \leftarrow [\mathbf{r}_1, \mathbf{r}_2, ..., \mathbf{r}_B]
13: w_{sup} \leftarrow \mathbf{R}^T \mathbf{u}/||\mathbf{u}^T \mathbf{u}||, normalize \mathbf{w}_{sup}
14: t \leftarrow \mathbf{R}\mathbf{w}_{sup}/\mathbf{w}_{sup}^T\mathbf{w}_{sup}
15: for b = 1 \text{ to } B do
             \mathbf{q}_b \leftarrow \mathbf{Y}_b^{\mathbf{t}}/||\mathbf{t}^T\mathbf{t}||, normalize \mathbf{q}_b
16:
             \mathbf{s}_b \leftarrow \mathbf{Y}_b \mathbf{q}_b / \mathbf{q}_b^T \mathbf{q}_b
17:
18: end for
19: \mathbf{S} \leftarrow [\mathbf{s}_1, \mathbf{s}_2, ..., \mathbf{s}_B]
20: \mathbf{q}_{sup} \leftarrow \mathbf{S}^T \mathbf{t}/||\mathbf{t}^T \mathbf{t}||, normalize \mathbf{q}_{sup}
21: \mathbf{u} \leftarrow \mathbf{S}^T \mathbf{q}_{sup} / \mathbf{q}_{sup}^T \mathbf{q}_{sup}
22: until t converges
23: Deflation by subtracting the effect of the first k components from each data block, X_b and Y_b
      for b \in [1, B]
24: for b = 1 \text{ to } B do
             \mathbf{G}_b \leftarrow (\mathbf{T}_{1:k}^T \mathbf{T}_{1:k})^{-1} \mathbf{T}_{1:k}^T u_b, where T_{1:k} = [t_1, t_2, ...t_k]
             \mathbf{X}_{b,ftc} \leftarrow \mathbf{X}_{b,ftc} - \mathbf{r}_{b,t} \mathbf{a}_{b,f} \mathbf{p}_{b,c} \text{ for } t \in [1,N_t], f \in [1,N_f], c \in [1,N_c]
26:
             \mathbf{Y}_b \leftarrow \mathbf{Y}_b - \mathbf{T}_{1:k} \mathbf{G}_b \mathbf{q}_b^T
27:
28: end for
29: k \leftarrow k+1 The next pair of PLS components is found by repeating from Step 1 on deflated
```

We can see that block specific patterns  $a_{b,k}$  and  $p_{b,k}$  of the predictor are regressed on the response super-block temporal signature u (8,9), and the block specific patterns of the response are regressed on the predictor super-block temporal signature t (16). We also see that the super-block weight

vectors  $w_{sup}$  and  $q_{sup}$  are regressed on the opposite temporal signatures as well. The regression of  $q_{sup}$  at the super-level is what will enable us to incorporate muscle synergies in the next section.

# 3: Changing three-way mbPLS to learn EEG features with muscle synergies

In order to learn the group level features of EEG that correspond to muscle synergies across subjects, we need to incorporate muscle synergies into the model. Prior to running three-way mbPLS we can learn muscle synergies for each subject through ICA factorization of the EMG data via

$$Y_b = A_b M_b$$

where  $Y_b$  is the (time points X EMG channels) matrix with columns that are mean-centered and have unit variance. A is the (time points X ica components) matrix whose columns reveals the temporal signature of each ica component. M is the (ica components X EMG channels) matrix whose rows reveal the learned muscle synergies.

In the three-way mbPLS algorithm with muscle synergies, we will fix the sub-level block decompositions to the ICA decomposition:

$$s_{b,k} = A_b(:,k)$$

$$q_{b,k} = M_b(k,:)$$

Algorithm 2 shows three-way mbPLS with muscle synergies.

We are able to fix the sub-level response block components because regression between the predictor and response blocks still happens at the super-level. After convergence, we will be able to compare some three-dimensional EEG features with particular muscle synergy activation across groups.

### A: References

1. A multiblock PLS model of cortico-cortical and corticomuscular interactions in Parkinson's disease. Chiang et. al.

# Algorithm 2 Adaptation of three-way mbPLS for muscle synergies

```
1: for b = 1 to B do
           Perform independent component analysis on Y_b
 2:
 3:
           [\mathbf{A}_b, \mathbf{M}_b] \leftarrow ICA(\mathbf{Y}_b), where A is the mixing matrix, and M is the signal matrix.
           for k = 1 to K do
 4:
                 \mathbf{s}_{b,k} \leftarrow \mathbf{A}_b(:,k)
 5:
                 \mathbf{q}_{b,k} \leftarrow \mathbf{M}_b(k,:)^T
 6:
 7:
           end for
 8: end for
 9: for k = 1 to K do
           \mathbf{S}_k \leftarrow [\mathbf{s}_{1,k}, \mathbf{s}_{2,k}, ..., \mathbf{s}_{B,k}]
11: end for
12: Choose start u
13: repeat (the k's are left out to simplify notation, in each iteration, S refers to S_k)
14: Compute the auxiliary matrix \mathbf{Z}_b whose (f,c)^{th} element is given by Z_{b,fc} \leftarrow \sum_{t=1}^{N_t} X_{b,tfc} u_t for
      f \in [1, N_f], c \in [1, N_c], b \in [1, B]
15: Concatenate the auxiliary matrices \mathbf{Z} \leftarrow [\mathbf{Z}_1, \mathbf{Z}_2, ..., \mathbf{Z}_b]
16: Perform singular decomposition on Z:
17: [\mathbf{g}, \sigma, \mathbf{h}] \leftarrow SVD(\mathbf{Z}, 1), where \mathbf{g} and \mathbf{h} are the first sing. vec. of Z
18: for b = 1 \text{ to } B do
19:
           \mathbf{a}_b \leftarrow q
           \mathbf{p}_b \leftarrow [h_{(b-1)N_c+1}, h_{(b-1)N_c+2}, ..., h_{(b-1)N_c+N_c}]
           \mathbf{r}_b \leftarrow [\mathbf{r}_{b,1}, \mathbf{r}_{b,2}, ..., \mathbf{r}_{b,N_t}] \text{ where } r_{b,t} \leftarrow \sum_{f=1}^{N_c} X_{b,tfc} a_{b,f} p_{b,c} \text{ for } t \in [1, N_t]
21:
22: end for
23: \mathbf{R} \leftarrow [\mathbf{r}_1, \mathbf{r}_2, ..., \mathbf{r}_B]
24: w_{sup} \leftarrow \mathbf{R}^T \mathbf{u} / ||\mathbf{u}^T \mathbf{u}||, normalize \mathbf{w}_{sup}
25: t \leftarrow \mathbf{R}\mathbf{w}_{sup}/\mathbf{w}_{sup}^T\mathbf{w}_{sup}
26: For this algorithm, we will not regress response sub-level block components on
      temporal activation of the predictor super-block. q_b and s_b will remain unchanged
      for b \in [1, B].
27: \mathbf{q}_{sup} \leftarrow \mathbf{S}^T \mathbf{t} / ||\mathbf{t}^T \mathbf{t}||, normalize \mathbf{q}_{sup}
28: \mathbf{u} \leftarrow \mathbf{S}^T \mathbf{q}_{sun} / \mathbf{q}_{sun}^T \mathbf{q}_{sun}
29: until t converges
30: Deflation by subtracting the effect of the first k components from each data block, \mathbf{X}_b and \mathbf{Y}_b
      for b \in [1, B]
31: for b = 1 \text{ to } B do
           \mathbf{G}_b \leftarrow (\mathbf{T}_{1:k}^T \mathbf{T}_{1:k})^{-1} \mathbf{T}_{1:k}^T u_b, where T_{1:k} = [t_1, t_2, ...t_k]
           \mathbf{X}_{b,ftc} \leftarrow \mathbf{X}_{b,ftc} - \mathbf{r}_{b,t} \mathbf{a}_{b,f} \mathbf{p}_{b,c} \text{ for } t \in [1,N_t], f \in [1,N_f], c \in [1,N_c]
33:
           \mathbf{Y}_b \leftarrow \mathbf{Y}_b - \mathbf{T}_{1:k} \mathbf{G}_b \mathbf{q}_b^T
34:
35: end for
36: k \leftarrow k+1 The next pair of PLS components is found by repeating from Step 1 on deflated
```

data blocks.