

- Mobile EEG artifact correction on limited hardware
- using artifact subspace reconstruction
- Paul Maanen 1,2¶, Sarah Blum 3, and Stefan Debener 1,2
- 1 Department of Psychology, Carl von Ossietzky Universität Oldenburg, 26129 Oldenburg, Germany 2
- Cluster of Excellence "Hearing4All", Carl von Ossietzky Universität Oldenburg, Germany 3 Hörzentrum
- Oldenburg gGmbH, Oldenburg, Germany ¶ Corresponding author

DOI: 10.xxxxx/draft

Software

- Review 🗗
- Repository 🗗
- Archive 2

Editor: Marcel Stimberg 2 0

Submitted: 28 February 2024 Published: unpublished

License

Authors of papers retain copyrigh™ and release the work under a Creative Commons Attribution 4.0 International License (CC BY 4.0)

Summary

Biological data like electroencephalography (EEG) are typically contaminated by unwanted signals, called artifacts. Therefore, many applications dealing with biological data with low signal-to-noise ratio require robust artifact correction. For some applications like braincomputer-interfaces (BCI), the artifact correction needs to be real-time capable. Artifact subspace reconstruction (ASR) is a statistical method for artifact reduction in EEG. However, in its current implementation, ASR cannot be used in mobile data recordings using limited hardware easily. In this report, we add to the growing field of portable, online signal processing methods by describing an implementation of ASR for limited hardware like single-board computers. We describe the architecture, the process of translating and compiling a Matlab codebase for a research platform, and a set of validation tests using publicly available data sets. The implementation of ASR on limited, portable hardware facilitates the online interpretation of EEG signals acquired outside of the laboratory environment.

Statement of need

Electroencephalography (EEG) is a non-invasive method for the recording of brain-electrical activity. EEG signals can be recorded from several scalp sites concurrently with small, portable 22 devices. Therefore it is a strong contender for the interface part of BCIs (Blankertz et al., 2016; Botte-Lecocq et al., 2014; Liyanage & Bhatt, 2020; Lotte, 2014; Zander & Kothe, 2011). BCIs are systems that allow a direct link between a human and a computer by interpreting brain signals in near real-time and translating these signals to commands for the machine. There is demand for BCIs in the future to be mobile in order to reach their target audience and be useful in everyday situations outside of research contexts (Dauwels et al., 2016; Na et al., 2021; Ogino & Mitsukura, 2020). As BCIs have to react to changes in the user's brain state near instantaneously, EEG signal processing for BCIs has to be capable of low-latency, real-time operation, ideally on artifact-free data to avoid the influence of artifacts on the system.

Another field where mobile artifact handling is needed is neuropsychology research using recordings of human behavior during motion or natural environments rather than in the laboratory (De Vos et al., 2014; Debener et al., 2012; Jacobsen et al., 2020; Vos et al., 2014). This implicates a need for mobile research platforms capable of recording and processing EEG

signals, including before applying specific analyses steps.

However, both BCI and mobile EEG signals are prone to be contaminated by artifacts, in movement even more than stationary data (Jacobsen et al., 2020). Artifact correction therefore is indispensable for mobile EEG signal processing due to the fact that many abnormal data occur irregularly and with high amplitudes and can thus hinder correct interpretation of the data (Alchalabi et al., 2021; Blum et al., 2019; Chandola et al., 2009; Chaudhary et al., 2021;



Mane et al., 2020). Artifacts can have a large influence on the performance of signal processing methods, they may especially break the assumption of some methods that certain statistical properties remain stable in the data. Artifact correction for BCIs of the future and for mobile EEG experiments needs to be capable of online operation on mobile hardware and needs be able to handle artifacts that occur in mobile EEG.

One candidate method is artifact subspace reconstruction (ASR) (Mullen et al., 2015), a statistical method for artifact reduction in EEG. It has been shown to perform well with movement artifacts and eye blinks (Blum et al., 2019; Dehais et al., 2021; Jacobsen et al., 2020; Ladouce et al., 2021; Nathan & Contreras-Vidal, 2016; Nordin et al., 2018; Plechawska-Wojcik et al., 2019), artifact classes which are especially important for mobile EEG.

ASR is a statistical artifact correction method (Blum et al., 2019; Chang et al., 2018; Mullen et al., 2015; Pion-Tonachini et al., 2018). It detects artifacts based on their abnormal statistical properties when compared to artifact-free data. After detection, a correction is applied and the result of the method are data with the same amount of samples and channels as the (possibly corrupted) input data.

However, because ASR is implemented in Matlab, in its current implementation, ASR cannot be used in mobile EEG recordings easily. Matlab needs a decently powerful PC (Mathworks, 2022) and is only available for operating systems running on an Intel-architecture processor. Mobile recording hardware is typically not fast enough to run Matlab and usually sports some variation of ARM architecture. There have been efforts to modify ASR for mobile devices Van et al. (2021), but they aim mainly at field programmable gate arrays (FPGAs), which are more specialised and harder to use for the average scientist, and there is no open source implementation of mobile ASR as of yet.

Therefore we propose mobile ASR (mASR), an implementation of ASR for limited hardware, in our case a research platform to evaluate audio/time domain/hearing aid signal processing.

In this report, we describe the architecture, the process of translating and compiling a Matlab codebase for this research platform, and a set of validation tests using publicly available data sets. With the implementation of ASR on portable hardware, the interpretation of neural data in different contexts is possible. Furthermore, we hope that this report provides a guideline for others looking to translate Matlab code into compiled languages for usage on limited hardware.

Acknowledgements

⁷⁴ We like to thank the original authors and current maintainers of the Matlab ASR implementation.

Funding statement

76 This work was supported by the DFG Cluster of Excellence EXC 1077/1 "Hearing4all".

References

Alchalabi, B., Faubert, J., & Labbé, D. R. (2021). A multi-modal modified feedback self-paced
BCI to control the gait of an avatar. *Journal of Neural Engineering*, 18(5), 056005.
https://doi.org/10.1088/1741-2552/abee51

Blankertz, B., Acqualagna, L., Dähne, S., Haufe, S., Schultze-Kraft, M., Sturm, I., Ušćumlic, M., Wenzel, M. A., Curio, G., & Müller, K.-R. (2016). The Berlin Brain-Computer Interface: Progress Beyond Communication and Control [Journal Article]. Frontiers in Neuroscience, 10(530). https://doi.org/10.3389/fnins.2016.00530



- Blum, S., Jacobsen, N. S. J., Bleichner, M. G., & Debener, S. (2019). A riemannian modification of artifact subspace reconstruction for EEG artifact handling. Frontiers in Human Neuroscience, 13. https://doi.org/10.3389/fnhum.2019.00141
- Botte-Lecocq, C., Bekaert, M.-H., Vannobel, J.-M., Leclercq, S., & Cabestaing, F. (2014).
 Considering human factors in BCI experiments: a global approach. *Journal Européen Des Systèmes Automatisés (JESA)*, 48(4-6), 283–301. https://doi.org/10.3166/jesa.48.283-301
- ⁹¹ Chandola, V., Banerjee, A., & Kumar, V. (2009). Anomaly detection: A survey. *ACM Comput. Surv.*, *41*(3). https://doi.org/10.1145/1541880.1541882
- Chang, C.-Y., Hsua, S.-H., Pion-Tonachini, L., & Jung, T.-P. (2018). Evaluation of artifact subspace reconstruction for automatic EEG artifact removal. Annual International Conference of the IEEE Engineering in Medicine; Biology. https://doi.org/10.1109/embc.2018.8512547
- Chaudhary, U., Mrachacz-Kersting, N., & Birbaumer, N. (2021). Neuropsychological and
 neurophysiological aspects of brain-computer-interface (BCI) control in paralysis. The
 Journal of Physiology, 599(9), 2351–2359. https://doi.org/10.1113/jp278775
- Dauwels, J., Stawicki, P., Gembler, F., & Volosyak, I. (2016). Driving a semiautonomous mobile robotic car controlled by an SSVEP-based BCI. *Computational Intelligence and Neuroscience*, 2016, 4909685. https://doi.org/10.1155/2016/4909685
- De Vos, M., Gandras, K., & Debener, S. (2014). Towards a truly mobile auditory brain–computer interface: Exploring the P300 to take away. *International Journal of Psychophysiology*, 91(1), 46–53. https://doi.org/10.1016/j.ijpsycho.2013.08.010
- Debener, S., Minow, F., Emkes, R., Gandras, K., & Vos, M. de. (2012). How about taking a low-cost, small, and wireless EEG for a walk? Psychophysiology, 49(11), 1617-1621. https://doi.org/10.1111/j.1469-8986.2012.01471.x
- Dehais, F., Somon, B., Mullen, T., & Callan, D. E. (2021). A neuroergonomics approach to measure pilot's cognitive incapacitation in the real world with EEG. In H. Ayaz & U.

 Asgher (Eds.), Advances in neuroergonomics and cognitive engineering (pp. 111–117).

 Springer International Publishing. https://doi.org/10.1007/978-3-030-51041-1_16
- Jacobsen, N. S. J., Blum, S., Witt, K., & Debener, S. (2020). A walk in the park? Characterizing gait-related artifacts in mobile EEG recordings. *European Journal of Neuroscience*.
- Ladouce, S., Mustile, M., & Dehais, F. (2021). Capturing cognitive events embedded in the real-world using mobile EEG and eye-tracking. *bioRxiv*. https://doi.org/10.1101/2021.11. 30.470560
- Liyanage, S. R., & Bhatt, C. (2020). Wearable electroencephalography technologies for brain-computer interfacing. In *Wearable and implantable medical devices* (pp. 55–78). Elsevier. https://doi.org/10.1016/B978-0-12-815369-7.00003-3
- Lotte, F. (2014). A tutorial on EEG signal-processing techniques for mental-state recognition in brain–computer interfaces. In E. R. Miranda & J. Castet (Eds.), *Guide to brain-computer music interfacing* (pp. 133–161). Springer London. https://doi.org/10.1007/978-1-4471-6584-2_7
- Mane, R., Chouhan, T., & Guan, C. (2020). BCI for stroke rehabilitation: Motor and beyond.

 Journal of Neural Engineering, 17(4), 041001. https://doi.org/10.1088/1741-2552/aba162
- Mathworks. (2022). System requirements for MATLAB R2021b. https://de.mathworks.com/support/requirements/matlab-system-requirements.html
- Mullen, T. R., Kothe, C. A. E., Chi, Y. M., Ojeda, A., Kerth, T., Makeig, S., Jung, T.-P., & Cauwenberghs, G. (2015). Real-time neuroimaging and cognitive monitoring using wearable dry EEG. *IEEE Transactions on Biomedical Engineering*, 62(11), 2553–2567. https://doi.org/10.1109/TBME.2015.2481482



- Na, R., Hu, C., Sun, Y., Wang, S., Zhang, S., Han, M., Yin, W., Zhang, J., Chen, X., & Zheng, D. (2021). An embedded lightweight SSVEP-BCI electric wheelchair with hybrid stimulator. Digital Signal Processing, 116, 103101. https://doi.org/10.1016/j.dsp.2021.103101
- Nathan, K., & Contreras-Vidal, J. L. (2016). Negligible motion artifacts in scalp electroencephalography (EEG) during treadmill walking. Frontiers in Human Neuroscience, 9. https://doi.org/10.3389/fnhum.2015.00708
- Nordin, A. D., Hairston, W. D., & Ferris, D. P. (2018). Dual-electrode motion artifact cancellation for mobile electroencephalography. *Journal of Neural Engineering*, 15(5), 056024. https://doi.org/10.1088/1741-2552/aad7d7
- Ogino, M., & Mitsukura, Y. (2020). A mobile auditory brain-computer interface system with sequential auditory feedback. 2020 IEEE 9th Global Conference on Consumer Electronics (GCCE), 590–593. https://doi.org/10.1109/GCCE50665.2020.9291762
- Pion-Tonachini, L., Hsu, S.-H., Chang, C.-Y., Jung, T.-P., & Makeig, S. (2018). Online automatic artifact rejection using the real-time EEG source-mapping toolbox (REST). 2018
 40th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC), 106–109. https://doi.org/10.1109/embc.2018.8512191
- Plechawska-Wojcik, M., Kaczorowska, M., & Zapala, D. (2019). The artifact subspace reconstruction (ASR) for EEG signal correction. A comparative study. In J. Świątek, L. Borzemski, & Z. Wilimowska (Eds.), Information systems architecture and technology: Proceedings of 39th international conference on information systems architecture and technology ISAT 2018 (pp. 125–135). Springer International Publishing. https://doi.org/10.1007/978-3-319-99996-8_12
- Van, L.-D., Tu, Y.-C., Chang, C.-Y., Wang, H.-J., & Jung, T.-P. (2021). Hardware-oriented
 memory-limited online artifact subspace reconstruction (HMO-ASR) algorithm. *IEEE Transactions on Circuits and Systems II: Express Briefs*, 68(12), 3493–3497. https://doi.org/10.1109/TCSII.2021.3124253
- Vos, M. D., Kroesen, M., Emkes, R., & Debener, S. (2014). P300 speller BCI with a mobile EEG system: Comparison to a traditional amplifier. *Journal of Neural Engineering*, 11(3), 036008. https://doi.org/10.1088/1741-2560/11/3/036008
- Zander, T. O., & Kothe, C. (2011). Towards passive brain–computer interfaces: applying brain–computer interface technology to human–machine systems in general. *Journal of Neural Engineering*, 8(2), 025005. https://doi.org/10.1088/1741-2560/8/2/025005