

# Sparse recovery in Inverse Problems

Silvio Fanzon

Department of Mathematics  
University of Hull, UK

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Sapienza, Roma



SAPIENZA  
UNIVERSITÀ DI ROMA



UNIVERSITY  
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# Sparse recovery in Inverse Problems

based on joint works with

Kristian Bredies, Marcello Carioni, Francisco Romero, Daniel Walter

## Outline

- ① Introduction: Inverse Problems & Sparsity
- ② Algorithm for sparse solutions recovery
- ③ Dynamic Inverse Problems
- ④ Application to Dynamic MRI



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Christian Doppler Research Society (CDG) Project PIR27  
“Mathematical methods for motion-aware medical imaging”



- 1 **Introduction to Inverse Problems & Sparsity**
- 2 Algorithm for sparse solution recovery
- 3 Dynamic Inverse Problems
- 4 Application to Dynamic MRI



# What is an Inverse Problem?

Mathematical models and data play a big role in modern science

- ▶ Inverse Problems: Link between model parameters and data

**Direct Problem:**      Model Parameters       $\leadsto$       Data      (easy)

**Inverse Problem:**      Data       $\leadsto$       Model Parameters      (hard)

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Bredies, Lorenz. *Mathematical Image Processing*. Springer (2018)

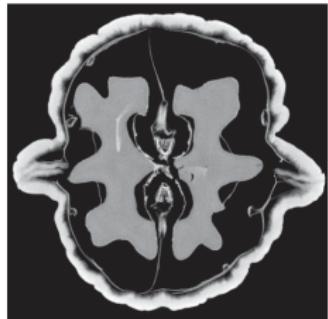
Mueller, Siltanen. *Linear and Nonlinear Inverse Problems with Practical Appl.* SIAM, 2012

van Leeuwen, Brune. *10 Lectures on Inverse Problems and Imaging*. [Online link](#)



# Example: X-ray Imaging

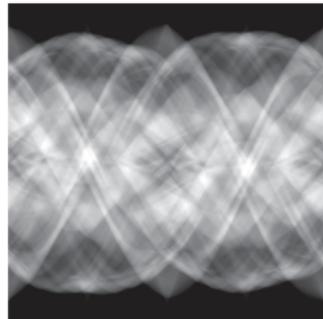
Walnut



X-ray data (sinogram form)

Direct problem →

← Inverse problem



Direct Problem: X-rays pass through walnut, detectors measure attenuation

Inverse problem: Given many X-ray measurements from different angles, reconstruct the walnut



# Example: Image Deblurring

Original Image



Blurred image



Direct problem

Inverse problem

Direct problem: Sharp image becomes blurred due to camera motion or focus issues

Inverse problem: Given the blurred image, recover the original sharp image

# Famous example: Hubble Space Telescope



- ▶ Hubble Space Telescope launched in 1990
- ▶ However images were blurred due to flawed lenses (Left)
- ▶ This issue was corrected through image processing (Right)

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Link to [article](#) on NASA's website



# Mathematical formulation

**Inverse Problem:** Given data  $f \in Y$ , find parameters  $u \in X$  such that

$$Ku = f$$

- ▶  $f$  is data  $\quad Y$  data space – Banach space or  $\mathbb{R}^n$
- ▶  $u$  are parameters  $\quad X$  the parameters space – Same as above
- ▶  $K: X \rightarrow Y$  is Forward Operator
- ▶  $K$  models the process to obtain the data from the parameters



# III-posed Inverse Problems

Consider the inverse problem

$$Ku = f \quad (\text{P})$$

Problem (P) is **well-posed** if all three conditions hold:

- ① **Existence:** There exists at least one solution
- ② **Uniqueness:** There exists at most one solution
- ③ **Stability:** The solution depends continuously on the data, i.e., there exists a constant  $C > 0$  such that

$$\|u - u'\|_X \leq C \|f - f'\|_Y \quad \text{where} \quad Ku = f, \quad Ku' = f'$$

Problem (P) is **ill-posed** if it is not well-posed



# Measurements are noisy

Consider the inverse problem

$$Ku = f \quad (\text{P})$$

- ▶ **Ideal world:** Measurement comes from operator  $\leadsto f = Ku$
- ▶ **Reality:** We can only observe noisy measurements

$$f^\varepsilon = Ku + \varepsilon, \quad \varepsilon \text{ random (unknown) noise}$$

**Goal:** To recover  $u$  from noisy measurement  $f^\varepsilon$

**Main difficulty:**  $K^{-1}$  does not exist or is not continuous  $\leadsto$  **ill-posedness**



# Variational Regularization

$$Ku = f \tag{P}$$

- ▶ (P) might not have solution. Find **approximate** solution by **least-squares**

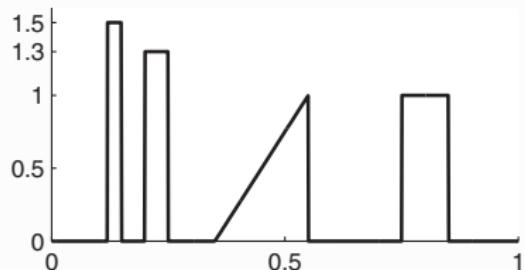
$$\min_{u \in X} \|Ku - f\|_Y^2 \tag{P'}$$

- ▶ **Problem:** Might still have **non-existence, non-uniqueness** and / or **instability**
- ▶ **Solution:** Replace (P) with the **regularized** least-squares problem

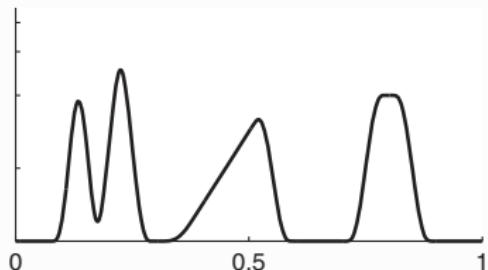
$$\min_{u \in X} \|Ku - f\|_X^2 + \alpha R(u), \quad R: X \rightarrow [0, +\infty], \quad \alpha > 0$$

- ①  $R$  makes the problem well-posed and stable – if chosen properly
- ②  $R$  favors certain solutions – the ones for which  $R(u)$  is small

# Example: 1D deconvolution



Original signal  $\tilde{u}: [0, 1] \rightarrow \mathbb{R}$



Blurred signal  $f = \psi \star \tilde{u}$

- ▶ Goal: Recover  $\tilde{u}$  from noisy data  $f^\varepsilon = f + \varepsilon$
- ▶ This means solving the 1D-deconvolution problem:

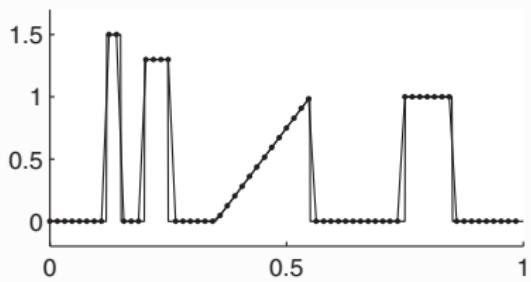
$$\text{Find } u \text{ such that } \psi \star u = f^\varepsilon$$

# Naive deconvolution

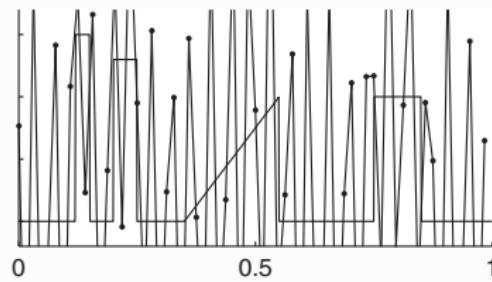
Solve the discrete 1D-deconvolution problem by least-squares:

$$u^\varepsilon \in \arg \min_{u \in L^2(0,1)} \|\psi * u - f^\varepsilon\|_{L^2(0,1)}^2$$

- ▶ Solution behaves well when noise  $\varepsilon = 0$  but is terrible when  $\varepsilon \neq 0$ 
  - ▶ Instability amplifies noise in the reconstruction
- ▶ Below the solid line represents the ground truth  $\tilde{u}$
- ▶ We need regularizer which penalizes oscillations



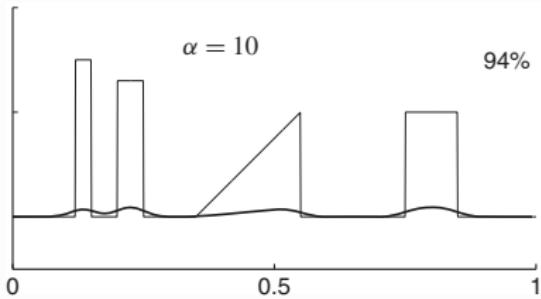
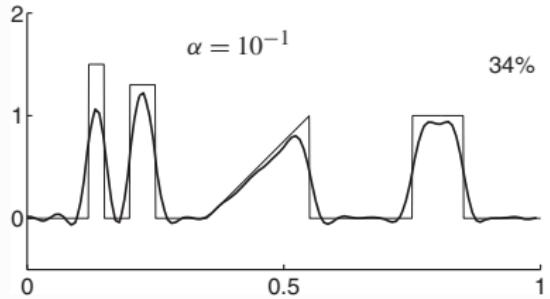
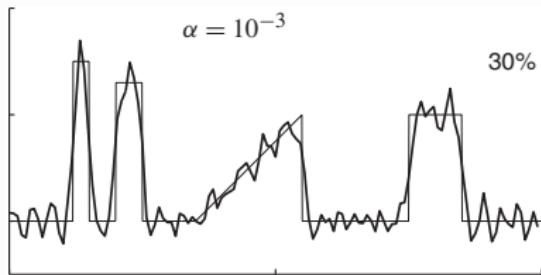
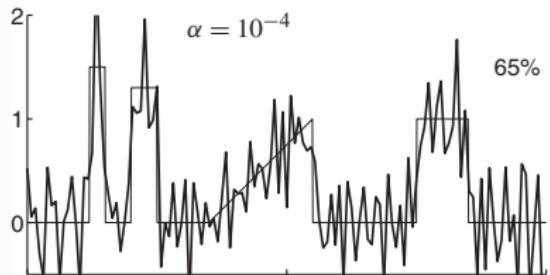
$u^0$



$u^\varepsilon$

Regularize with  $L^2$  norm:

$$\min_{u \in L^2(0,1)} \|\psi * u - f^\varepsilon\|_{L^2(0,1)}^2 + \alpha \|u\|_{L^2(0,1)}^2$$

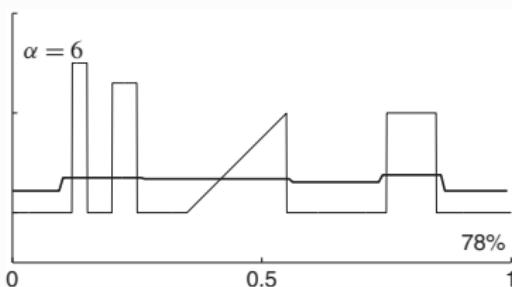
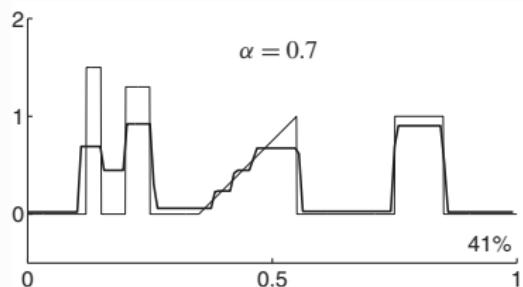
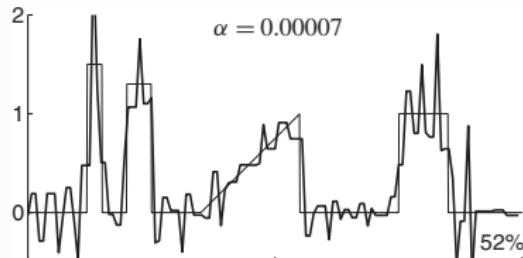


- Best is  $\alpha = 10^{-1}$ . Notice the smoothing effect of  $L^2$  regularization
- Smoothness not always desirable (e.g. if  $u$  is image with sharp edges – like here)

## Reg. with Total Variation (BV semi-norm):

$$\min_{u \in L^1(0,1)} \|\psi \star u - f^\varepsilon\|_{L^2(0,1)}^2 + \alpha \operatorname{TV}(u)$$

$$\operatorname{TV}(u) = \sup_{\text{partitions of } [0,1]} \sum_{i=1}^n |u(x_i) - u(x_{i-1})|$$



- ▶ Best is  $\alpha = 0.009$ . Notice the **sparsifying effect** of TV (the jumps)
- ▶ Sparsity assumes different forms, depending on the setting
- ▶ **Extremal points of regularizer describe features of sparse solutions**



# Summary

**Setting:**  $X, Y$  Banach spaces,  $K: X \rightarrow Y$  linear continuous operator

**Inverse Problem:** Given  $f \in Y$ , find  $u \in X$  such that

$$Ku = f$$

**Main difficulty:**  $K^{-1}$  does not exist or is not continuous

**Variational regularization:** Given  $f \in Y$ , find  $u \in X$  which solves

$$\min_{u \in X} \|Ku - f\|_Y^2 + \alpha R(u) \quad (\text{P})$$

## Goals of the Talk:

- ▶ Algorithm to recover sparse solutions to (P)
- ▶ Framework for regularizing dynamic inverse problems



# Outline

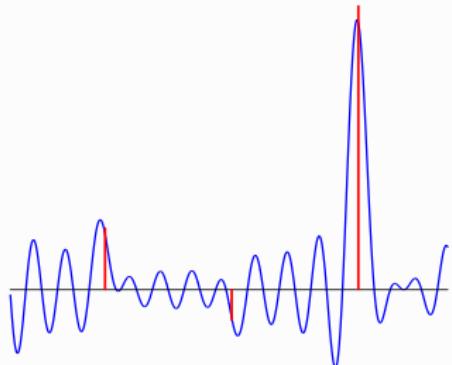
1 Introduction to Inverse Problems & Sparsity

2 Algorithm for sparse solution recovery

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# Motivation: Sparse peak recovery



**Well-studied problem: Superresolution**

- ▶ Solve  $\mathfrak{F}u = f$  on  $\Omega$
- ▶  $\mathfrak{F}$  Fourier transform,  $\Omega \subset \mathbb{R}^d$  finite set
- ▶ **Sparsity assumption:**  $\bar{u} = \sum_{i=1}^N \lambda_i \delta_{x_i}$

**Radon-norm regularization:**

- ▶ Solve variational problem in space of Radon measures (noisy data)

$$\min_{u \in \mathcal{M}(\Omega)} \|\mathfrak{F}u - f\|_{L^2(\Omega)}^2 + \alpha \|u\|_{\mathcal{M}(\Omega)}$$

- ▶ Want to recover sparse solution  $\bar{u} = \sum_{i=1}^N \lambda_i \delta_{x_i}$
- ▶ [Candès, Fernandez-Granda. **CPAM** (2013)] and many more

↷ **(Fast) algorithms for a general setting**



# Minimization Problem in General Setting

$$\min_{u \in X} F(Ku) + R(u)$$

- **Parameters:**  $X$  separable Banach space with predual  $X_*$
- **Data:**  $Y$  Hilbert space
- **Forward operator:**  $K: X \rightarrow Y$  linear and weak\*-to-strong continuous
- **F ~ Loss function:** Smooth + Strictly Convex

$$F: Y \rightarrow [0, \infty) \quad \left( F(y) = \|y - f\|_Y^2 \right)$$

- **R ~ Regulariser:** Convex + 1-homogeneous + Coercive

$$R: X \rightarrow [0, \infty] \quad (\text{Promotes Sparsity})$$

**Theorem [1]:** Direct method  $\implies$  Minimizer exists

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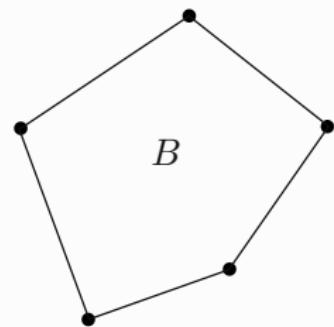
[1] Bredies, Carioni, **Fanzon**, Walter. Mathematical Programming (2024)



# Sparsity

**Unit Ball** of regularizer  $R$

$$B := \{u \in X : R(u) \leq 1\}$$



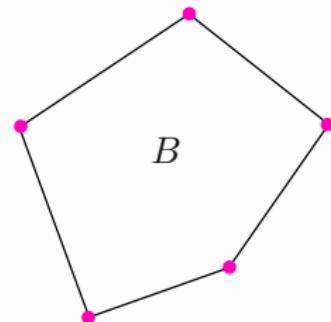
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**Extremal Points:**  $u \in B$  s.t.

$$\begin{cases} u = \alpha u_1 + (1 - \alpha) u_2 \\ \alpha \in (0, 1), \ u_1, u_2 \in B \end{cases} \implies u = u_1 = u_2$$



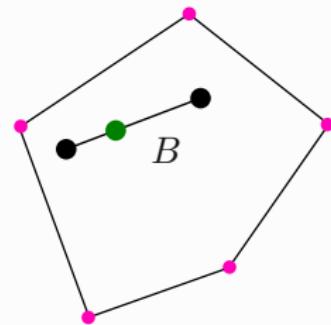
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[1] Bredies, Carioni, **Fanzon**, Walter. **Mathematical Programming** (2024)



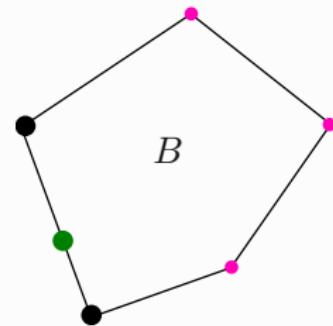
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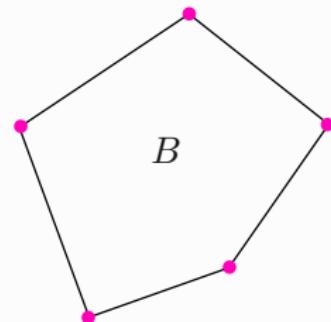
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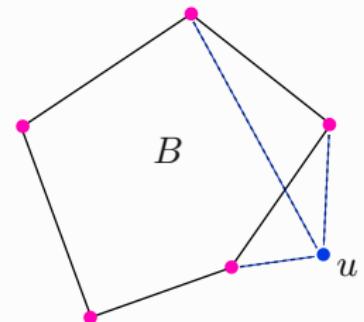
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**Definition:**  $u \in X$  **sparse**

$$u = \sum_{i=1}^N \lambda_i u_i, \quad \lambda_i \geq 0, \quad u_i \in \text{Ext}(B)$$

Conic combination

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[1] Bredies, Carioni, **Fanzon**, Walter. **Mathematical Programming** (2024)



# Main Task

Numerical **Algorithm** to compute

$$\bar{u} \in \arg \min_{u \in X} F(Ku) + R(u)$$

which is **sparse**

$$\bar{u} = \sum_{i=1}^N \lambda_i u_i, \quad \lambda_i \geq 0, \quad u_i \in \text{Ext}(B)$$

**Existence of sparse solutions:** Proven for  $K: X \rightarrow \mathbb{R}^n$  [1,2]

**Very general setting**  $\rightsquigarrow$  **Important Examples:**

- ▶ Training of Machine Learning models  $\rightsquigarrow X = \mathbb{R}^d$
- ▶ Microstructures in Materials  $\rightsquigarrow X = \text{BV}(\mathbb{R}^d)$  Bounded Variation
- ▶ Recovery of sparse sources  $\rightsquigarrow X = \mathcal{M}(\mathbb{R}^d)$  Radon Measures

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[1] Bredies, Carioni. **Calc. Var. PDE** (2020)

[2] Boyer, Chambolle, De Castro, Duval, De Gournay, Weiss. **SIAM Optimization** (2019)

# Example: Training of Machine Learning models

**Parameters:** vector  $\Theta = (\theta_1, \dots, \theta_d) \in \mathbb{R}^d$

**ML Model:** Fit model to given data

$$\min_{\Theta \in \mathbb{R}^d} F(\theta) + \|\Theta\|_1$$

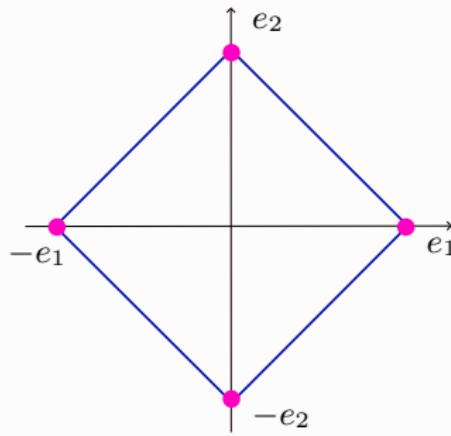
- ▶ Fidelity term  $F$  promotes data fit
- ▶ 1-norm promotes sparsity – e.g. solutions will have lots of zeros

$$\hat{\Theta} = (0, 0, \theta_i, 0, 0, \dots, 0, 0, \theta_d)$$

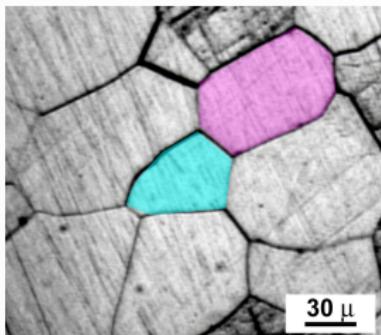
Banach space:  $X = \mathbb{R}^d$

Regularizer:  $\|x\|_1 := \sum_{i=1}^d |x_i|$

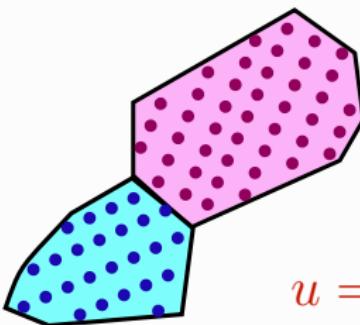
$$\text{Ext}(B) = \{\pm e_i\}_{i=1}^d$$



# Example: Microstructures in Materials



Polycrystalline Metal



$$E_i \subset \mathbb{R}^2$$

$$A_i \in \mathbb{R}^{2 \times 2}$$

$$u = \sum_{i=1}^N A_i \chi_{E_i}$$

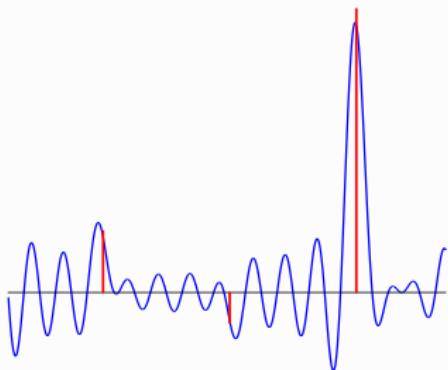
Banach space:  $X = \text{BV}(\mathbb{R}^2)$  functions of bounded variation

Regularizer:  $R(u) := \|Du\|_{\mathcal{M}}$ ,  $\text{Ext}(B) = \{\chi_E : E \subset \mathbb{R}^2 \text{ simply connected}\}$

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[2] **Fanzon**, Palombaro, Ponsiglione. **SIAM Journal on Mathematical Analysis** (2019)

# Example: Recovery of sparse sources



## Well-studied problem: Superresolution

- ▶ Solve  $\mathfrak{F}u = f$  on  $\Omega$
- ▶  $\mathfrak{F}$  Fourier transform,  $\Omega \subset \mathbb{R}^d$  finite set
- ▶ **Sparsity assumption:**  $\bar{u} = \sum_{i=1}^N \lambda_i \delta_{x_i}$

Banach space:  $X = \mathcal{M}(\mathbb{R}^d)$  Radon measures

Regularizer:  $R(u) := \|u\|_{\mathcal{M}}$   $\text{Ext}(B) = \{\pm \delta_x : x \in \mathbb{R}^d\}$

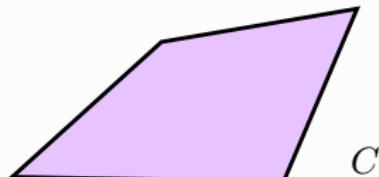
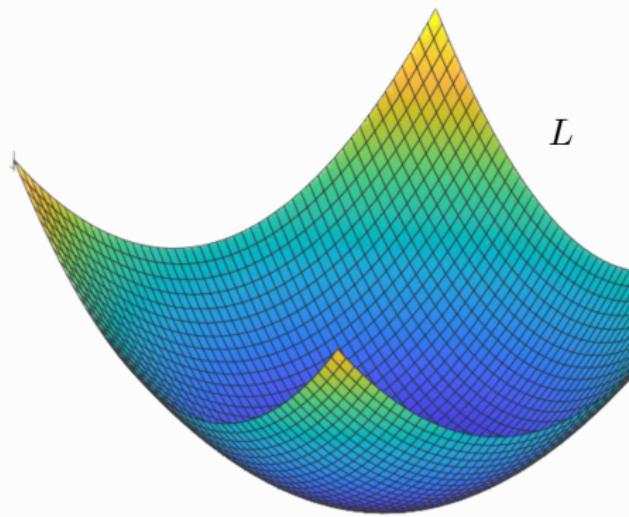
# Starting Point: Classic Frank-Wolfe



**Problem:** Constrained minimization

$$\min_{x \in C} L(x)$$

- $L: \mathbb{R}^N \rightarrow \mathbb{R}$  regular convex
- $C \subset \mathbb{R}^N$  convex compact set



M. Jaggi. Proceedings of Machine Learning Research (2013)

# Starting Point: Classic Frank-Wolfe



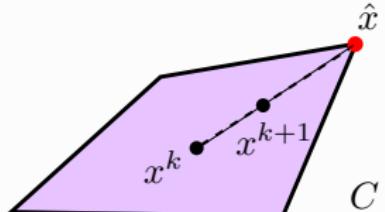
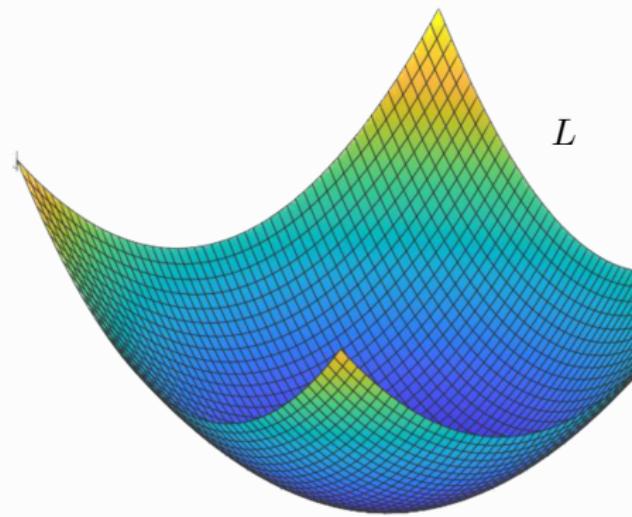
**Frank-Wolfe Algorithm:** Given  $x^k \in C$

- ① **Insertion:** Solve linearized problem

$$\min_{x \in C} \langle \nabla L(x^k), x \rangle \quad \mapsto \quad \hat{x}$$

- ② **Convex update:** Set

$$x^{k+1} := x^k + \alpha(\hat{x} - x^k), \quad \alpha := \frac{2}{k+2}$$

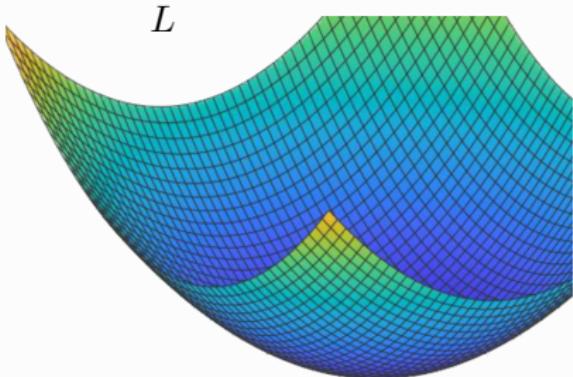


M. Jaggi. Proceedings of Machine Learning Research (2013)

# Proposed Algorithm: Generalized Frank-Wolfe

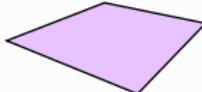


$$\min_{u \in X} L(u) + R(u), \quad L(u) = F(Ku)$$



**Idea:** Set  $B = \{R \leq 1\}$ . Consider

$$\min_{u \in X} L(u) + \chi_B(u) \iff \min_{u \in B} L(u)$$



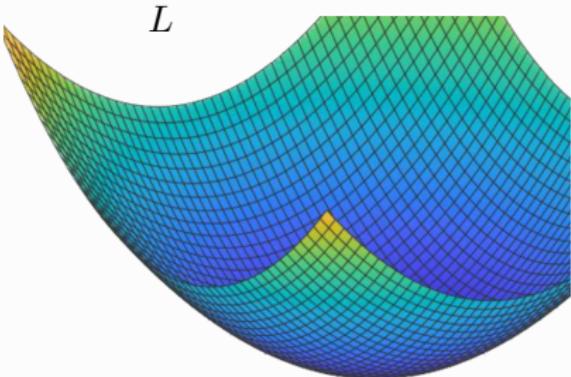
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[1] Bredies, Carioni, **Fanzon**, Walter. **Mathematical Programming** (2024)

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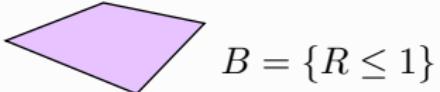


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**Descent Direction:** Solve

$$\min_{v \in B} \langle \nabla L(u), v \rangle \mapsto \hat{v}$$




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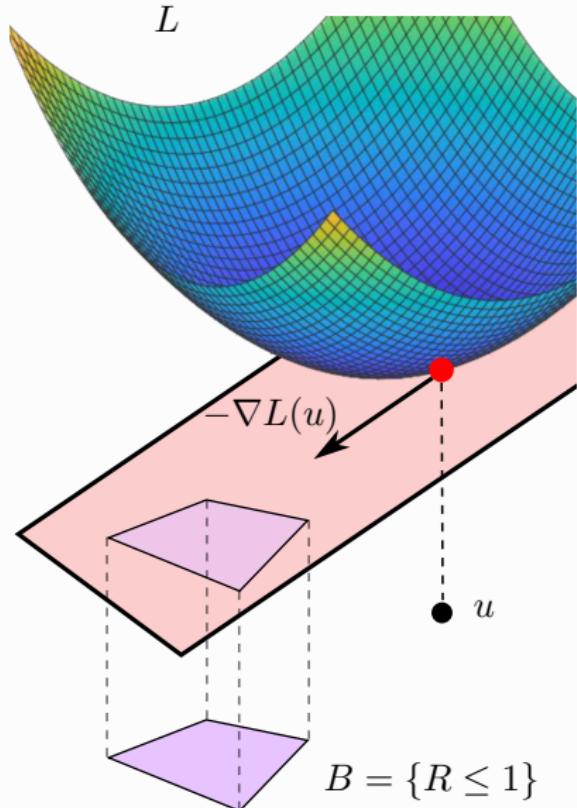
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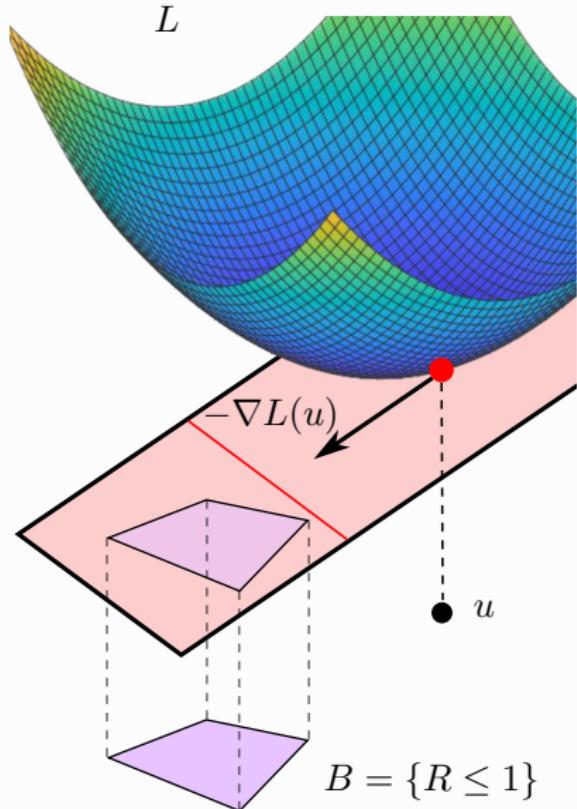
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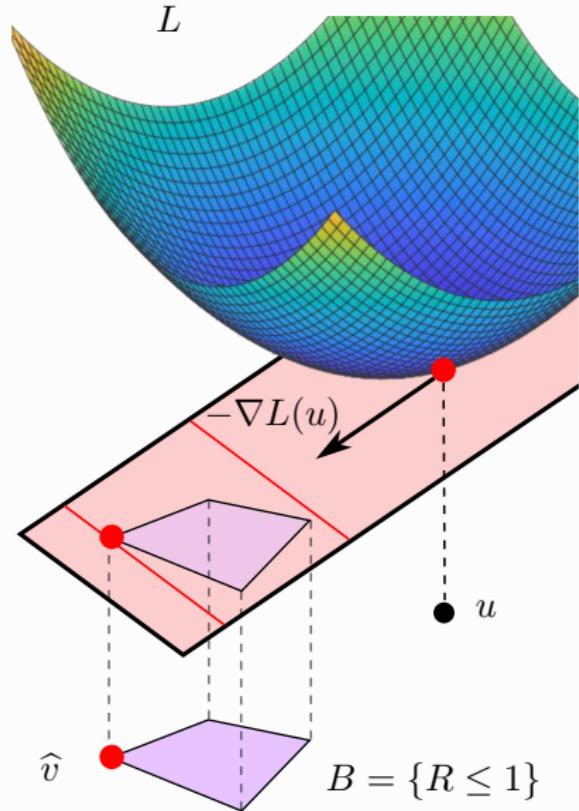
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[1] Bredies, Carioni, **Fanzon**, Walter. **Mathematical Programming** (2024)

# Proposed Algorithm: Generalized Frank-Wolfe



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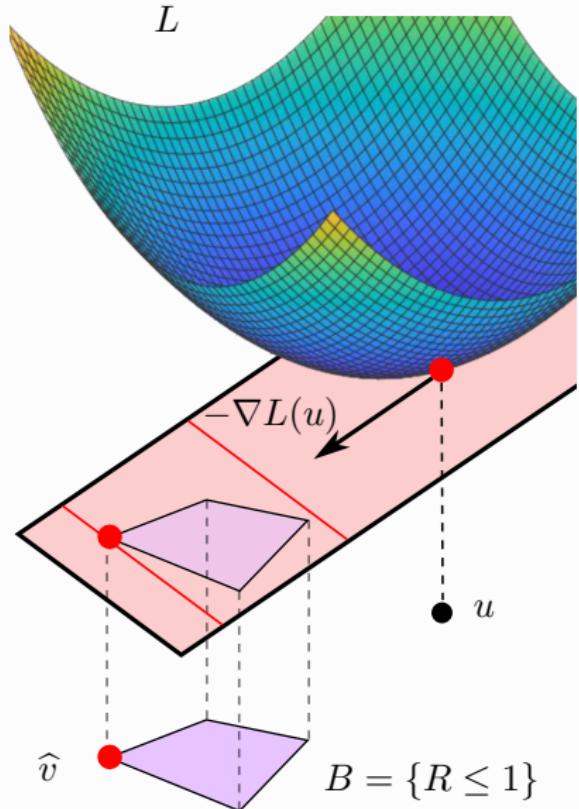
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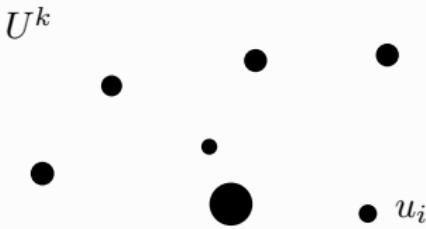
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Sparse  $k$ -th iterate

$$U^k = \sum_{i=1}^n \lambda_i u_i$$

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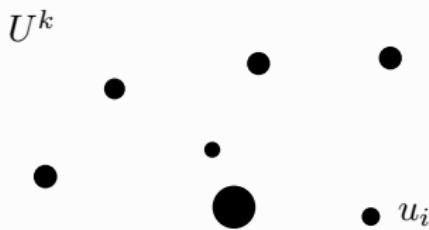


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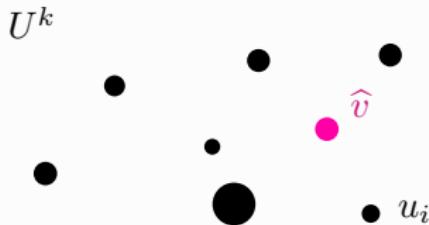
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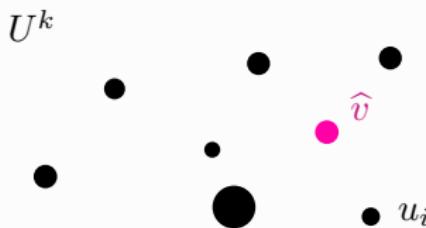
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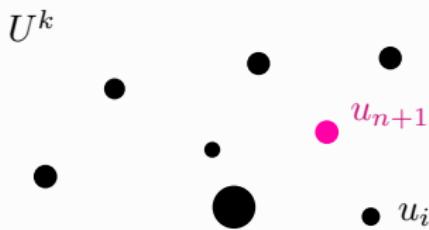
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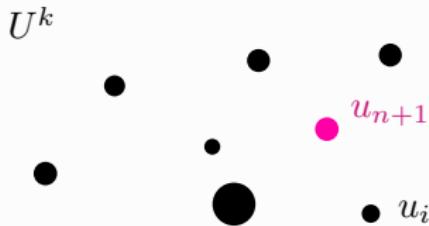


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$$(\lambda_1^*, \dots, \lambda_{n+1}^*) \in \arg \min_{\lambda_i \geq 0} (L + R) \left( \sum_{i=1}^{n+1} \lambda_i u_i \right) \rightsquigarrow U^{k+1} := \sum_{i=1}^{n+1} \lambda_i^* u_i$$

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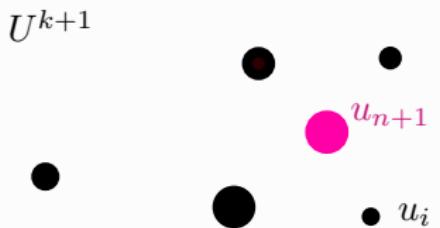
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- ① Non-linear problem (usually)
  - ▶ Non-linearity due to  $\text{Ext}(B)$
  - ▶ Expensive and / or hard to solve
- ② Quadratic program – Easy to solve

① **Insertion Step:** Solve

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# Convergence Analysis

## Theorem [1]

$U^k$  sparse iterate from the Generalized Frank-Wolfe Algorithm. Then

$$U^k \xrightarrow{*} \bar{u}, \quad \bar{u} \in \arg \min G, \quad G := L + R$$

General convergence rate is **sublinear**

(expected for gradient methods)

$$G(U^k) - \min G \lesssim \frac{1}{k}$$

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**Highlight:**  $\bar{u}$  **sparse** + **“Source Condition”** + **“Quadratic Growth”**

$$\implies \text{linear convergence:} \quad G(U^k) - \min G \lesssim \frac{1}{2^k}$$

---

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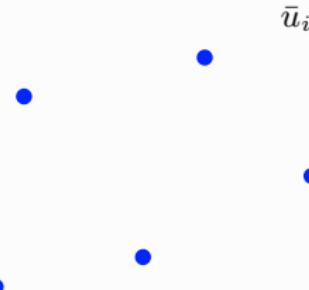
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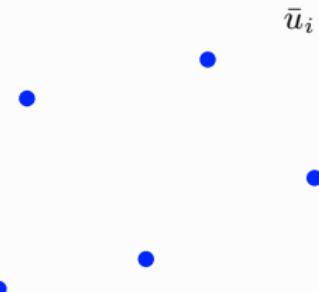
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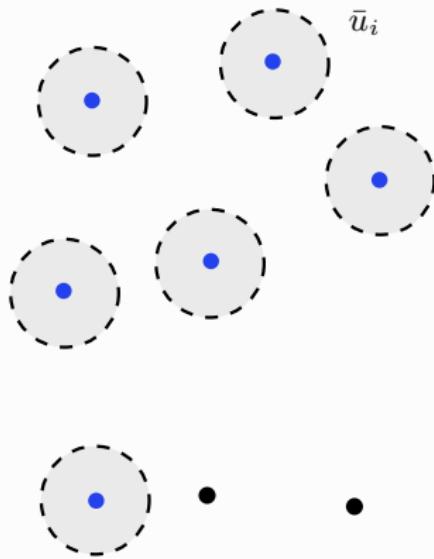
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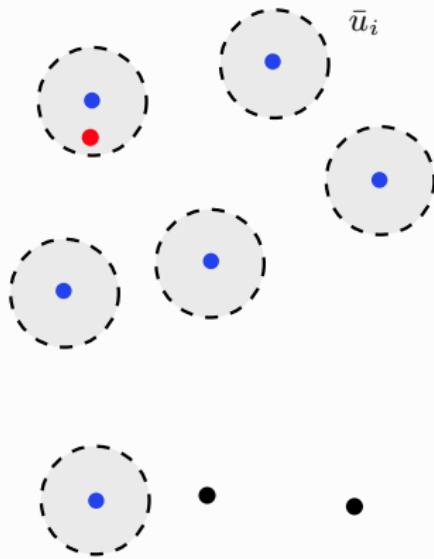
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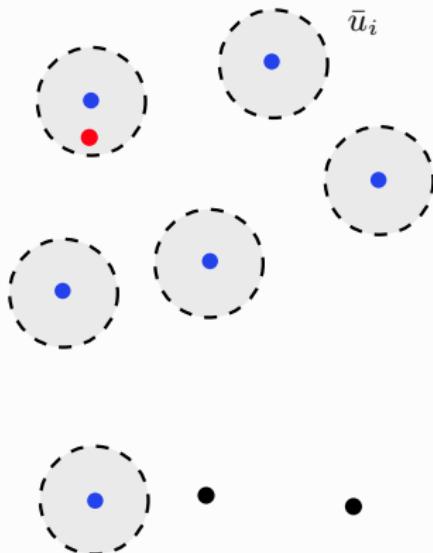
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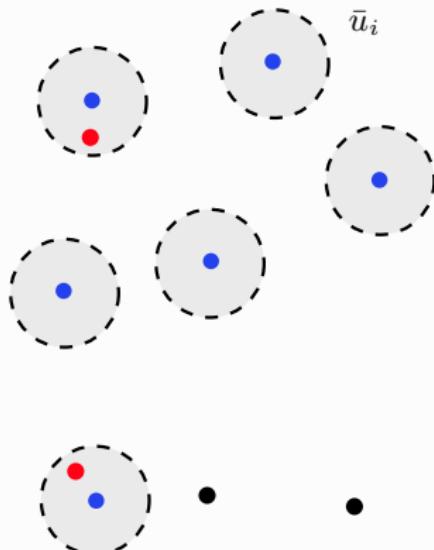
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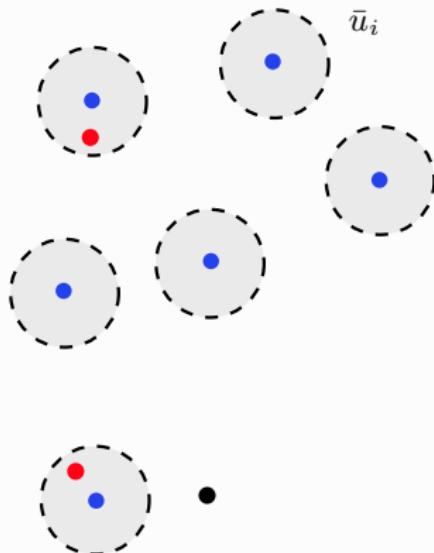
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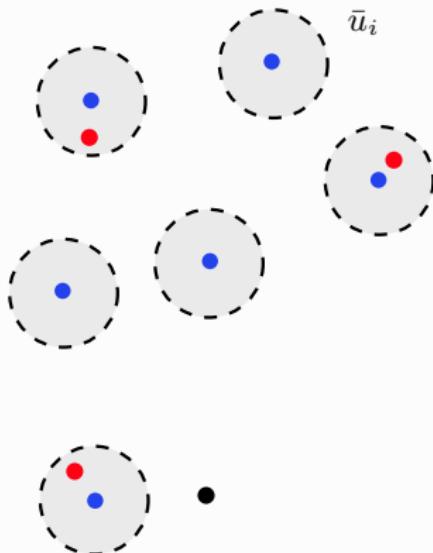
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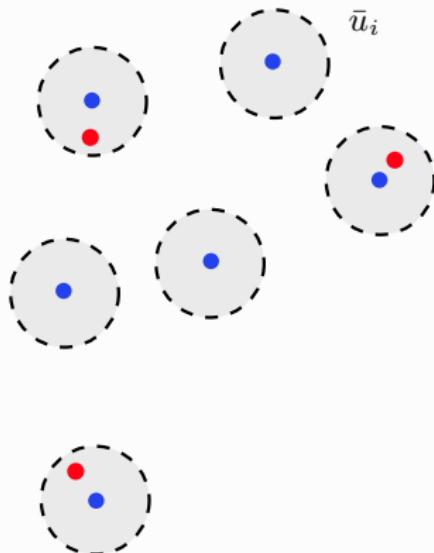
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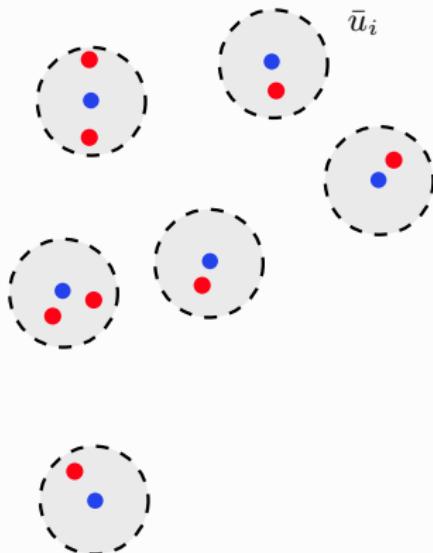
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# Comments on Linear Convergence Assumptions

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- ▶ (S) + (SC) widely accepted

- ▶ only proven in few cases [2]
- ▶ can be verified numerically

- ▶ (QG) is novelty

- ▶ In applications we need to:

- ▶ Characterize  $\text{Ext}(B)$
- ▶ Define suitable distance  $g$
- ▶ Show (QG) under reasonable assumptions

- ▶ Applications: [1] Prove fast convergence of Gen. Frank-Wolfe

- ▶ Minimum effort prob.
- ▶ Trace-norm regularized prob.
- ▶ Sparse source identification (heat eqn)

[1] Bredies, Carioni, F., Walter. **Math. Prog.** ('24) [2] Candès, Fernandez-Granda. **CPAM** ('13)

# Application: Sparse peak recovery [1, 2]

$$\min_{u \in \mathcal{M}(\Omega)} \frac{1}{2} \|Ku - f^\varepsilon\|_{L^2(\Omega)}^2 + \|u\|_{\mathcal{M}(\Omega)}$$

- Given:  $\Omega \subset \mathbb{R}^d$  and  $f^\varepsilon \in L^2(\Omega)$  noisy data
- Forw. operator:  $K: \mathcal{M}(\Omega) \rightarrow L^2(\Omega)$

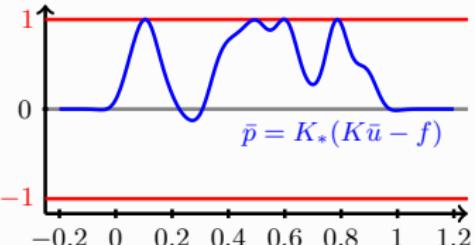
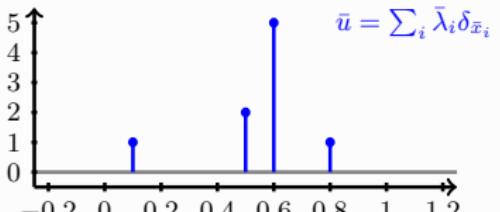
$$Ku = \psi \star u, \quad \psi = \text{Gauss. Kern.}$$

- Ext. points:  $B = \{\|u\|_{\mathcal{M}(\Omega)} \leq 1\}$

$$\text{Ext}(B) = \{\pm \delta_x : x \in \Omega\}$$

- (S)  $\exists$  sparse solution:

$$\bar{u} = \sum_{i=1}^M \bar{\lambda}_i \delta_{\bar{x}_i}, \quad \bar{\lambda}_i > 0, \quad \bar{x}_i \in \Omega$$



- (SC)  $\bar{p} = K_*(K\bar{u} - f^\varepsilon) \in C(\Omega)$

$$\arg \max_{v \in \text{Ext}(B)} \langle \bar{p}, v \rangle = \{\delta_{\bar{x}_1}, \dots, \delta_{\bar{x}_M}\}$$

$$\max_{v \in \text{Ext}(B)} \langle \bar{p}, v \rangle = \max_{x \in \Omega} \bar{p}(x) = 1$$

[1] Bredies, Carioni, F., Walter. **Math. Prog.** (2024)    [2] Pieper, Walter. **ESAIM: COCV** (2021)

# Application: Sparse peak recovery [1, 2]

$$\min_{u \in \mathcal{M}(\Omega)} \frac{1}{2} \|Ku - f^\varepsilon\|_{L^2(\Omega)}^2 + \|u\|_{\mathcal{M}(\Omega)}$$

- **(HP)**  $\bar{p}$  strictly concave at  $x_i$

$$\text{sign}(\bar{p}(x_i)) \langle \xi, \nabla^2 \bar{p}(x_i) \xi \rangle \gtrsim |\xi|^2$$

- **Metric:**  $g: \text{Ext}(B) \times \text{Ext}(B) \rightarrow [0, \infty)$

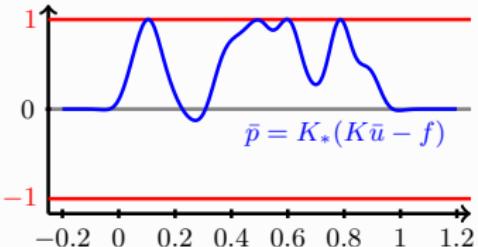
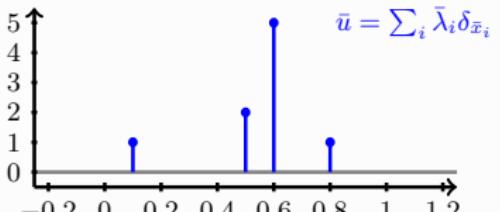
$$g(s_1 \delta_{x_1}, s_2 \delta_{x_2}) := |s_1 - s_2| + |x_1 - x_2|$$

- **(QG)** Quadratic growth of  $\bar{p}$  around  $\bar{u}_i$

$$1 - \langle \bar{p}, u \rangle \gtrsim g(u, u_i)^2, \quad u \sim u_i$$

**Theorem [1,2]: (HP)  $\implies$  (QG)**

Gen. Frank-Wolfe converges linearly



- **(SC)**  $\bar{p} = K_*(K\bar{u} - f^\varepsilon) \in C(\Omega)$

$$\arg \max_{v \in \text{Ext}(B)} \langle \bar{p}, v \rangle = \{\delta_{\bar{x}_1}, \dots, \delta_{\bar{x}_M}\}$$

$$\max_{v \in \text{Ext}(B)} \langle \bar{p}, v \rangle = \max_{x \in \Omega} \bar{p}(x) = 1$$

[1] Bredies, Carioni, F., Walter. **Math. Prog.** (2024)

[2] Pieper, Walter. **ESAIM: COCV** (2021)

# Application: Sparse peak recovery [1, 2]

$$\min_{u \in \mathcal{M}(\Omega)} \frac{1}{2} \|Ku - f^\varepsilon\|_{L^2(\Omega)}^2 + \|u\|_{\mathcal{M}(\Omega)}$$

**Gen. Frank-Wolfe:**  $\text{Ext}(B) = \{\pm \delta_x : x \in \Omega\}$

**Initialize:**  $u^0 = 0$

**Iterate:** Given  $u^k = \sum_{i=1}^n \lambda_i \delta_{x_i}$

**① Insertion Step:**  $p^k = K_*(Ku^k - f^\varepsilon)$

$$\max_{v \in \text{Ext}(B)} \langle p^k, v \rangle = \max_{x \in \Omega} p^k(x) \rightsquigarrow \hat{x}$$

**② Fully-corrective Step:** Solve

$$(\lambda_1^*, \dots, \lambda_{n+1}^*) \in \arg \min_{\lambda_i \geq 0} G(u^k + \lambda_{n+1} \delta_{\hat{x}}) \rightsquigarrow u^{k+1} := \left( \sum_{i=1}^n \lambda_i^* \delta_{x_i} \right) + \lambda_{n+1}^* \delta_{\hat{x}}$$

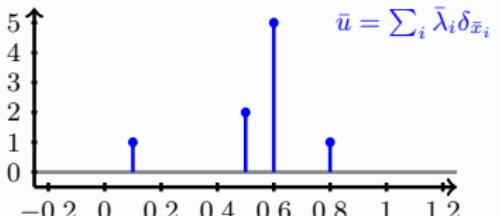
**Stop:** Based on Primal-Dual gap

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[1] Bredies, Carioni, F., Walter. **Math. Prog.** (2024)    [2] Pieper, Walter. **ESAIM: COCV** (2021)

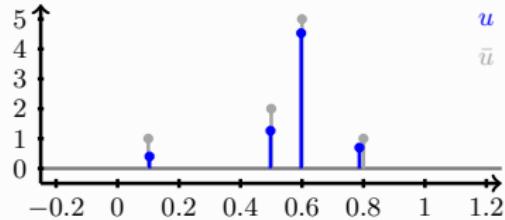
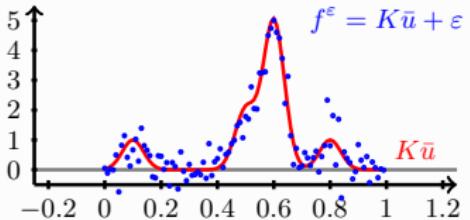
# Application: Sparse peak recovery [1, 2]

$$\min_{u \in \mathcal{M}(\Omega)} \frac{1}{2} \|Ku - f^\varepsilon\|_{L^2(\Omega)}^2 + \|u\|_{\mathcal{M}(\Omega)}$$



## Numerical experiment:

- ▶ Ground truth  $\bar{u}$  with 4 peaks
- ▶ Noiseless data  $f = K\bar{u}$
- ▶ Noisy data  $f^\varepsilon = K\bar{u} + \varepsilon$
- ▶ Run Gen. Frank-Wolfe  $\rightsquigarrow u$ 
  - ▶  $u$  is minimizer (by Thm)
  - ▶  $u$  correctly has 4 peaks
  - ▶ Weights of peaks are shrunk (effect of regularization)
  - ▶ Empirical **linear convergence**



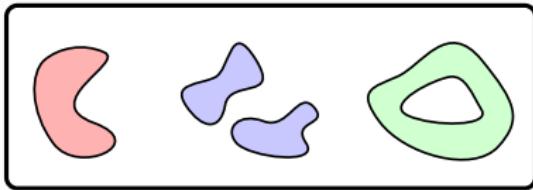
[1] Bredies, Carioni, F., Walter. **Math. Prog.** (2024)

[2] Pieper, Walter. **ESAIM: COCV** (2021)

# An open problem

**Total variation:**  $X = \text{BV}(\Omega)$ ,  $\Omega \subset \mathbb{R}^d$

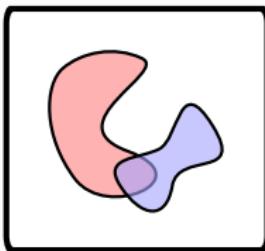
$$G(u) := F(Ku) + \|\nabla u\|_{\mathcal{M}} , \quad \text{Ext}(B) = \left\{ \frac{\chi_E}{\text{Per}(E)} : E \subset \Omega \text{ simple} \right\}$$



**Assume:** sparse solution  $\hat{u} = \sum_{i=1}^M \lambda_i \chi_{E_i}$

**Fast convergence:** Which “metric”???

$$g(E_i, E_j) := |E_i \triangle E_j|^{-1} \text{ ???}$$



- **Connected problems:** Exact recovery, Noise Robustness



# Outline

1 Introduction to Inverse Problems & Sparsity

2 Algorithm for sparse solution recovery

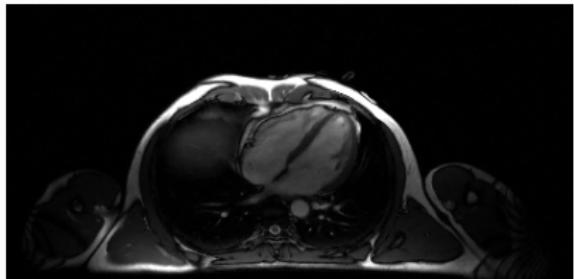
3 Dynamic Inverse Problems

4 Application to Dynamic MRI

# Motivation: Magnetic Resonance Imaging (MRI)



MRI Scanner



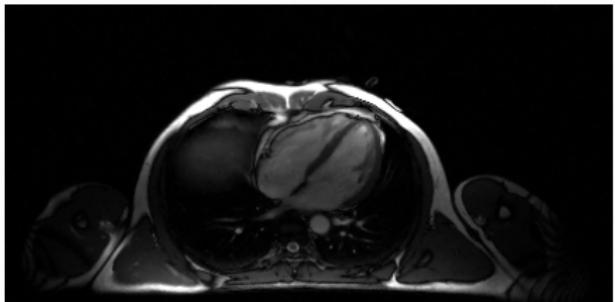
Human Heart

**MRI:** Medical imaging device, producing gray-scale images

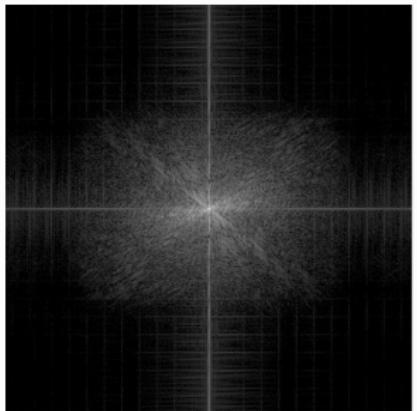
$$u : \Omega \subset \mathbb{R}^2 \rightarrow \mathbb{R}$$

# Mathematical model for MRI

Image  $u: \Omega \rightarrow \mathbb{R}$



$$\xrightarrow{\mathfrak{F}}$$



$$(\mathfrak{F}u) [\xi] = \frac{1}{2\pi} \int_{\mathbb{R}^2} u(x) e^{i\xi \cdot x} dx, \quad \xi \in \mathbb{R}^2$$

**MRI machine measures Fourier coefficients**



# MRI Inverse Problem

## Inverse Problem:

- ▶ Given MRI data  $y$
- ▶ Find image  $u: \Omega \rightarrow \mathbb{R}$  s.t.

$$\mathfrak{F}u = y$$

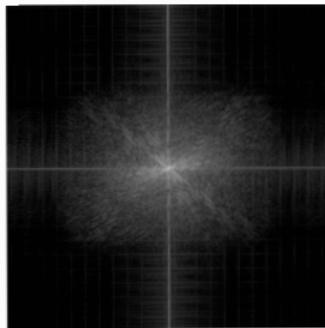
# MRI Inverse Problem

## Inverse Problem:

- ▶ Given MRI data  $y$
- ▶ Find image  $u: \Omega \rightarrow \mathbb{R}$  s.t.

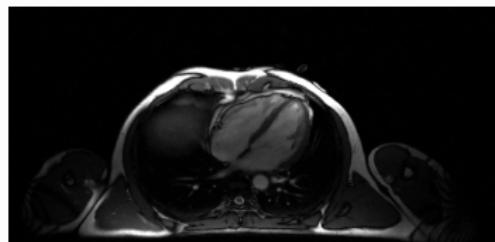
$$\mathfrak{F}u = y$$

**Ideal World:** Fourier transform is invertible. Unique solution is  $u = \mathfrak{F}^{-1}y$



Data  $y$

$$\xrightarrow{\mathfrak{F}^{-1}}$$



Reconstruction  $u$



# MRI Inverse Problem

**Reality:** Things are not straightforward

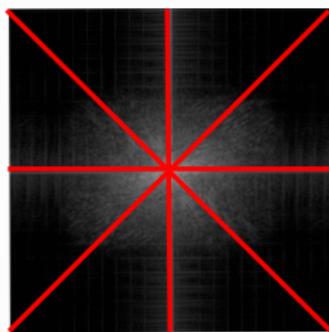
- ▶ Machine is slow in acquiring data  $\implies$  can only sample **limited data**
- ▶ Measurement process is inherently **noisy**

# MRI Inverse Problem

**Reality:** Things are not straightforward

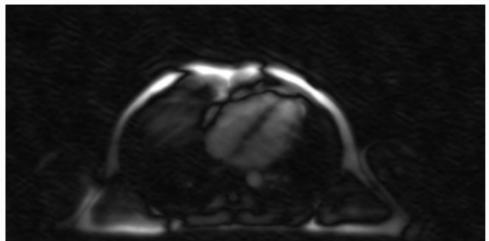
- ▶ Machine is slow in acquiring data  $\implies$  can only sample **limited data**
- ▶ Measurement process is inherently **noisy**

**Issue:** Plain inversion  $\leadsto$  poor reconstructions



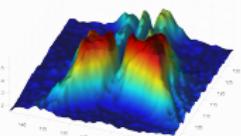
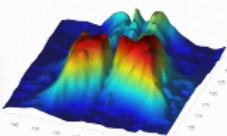
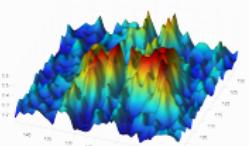
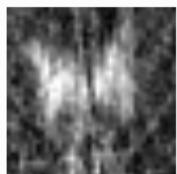
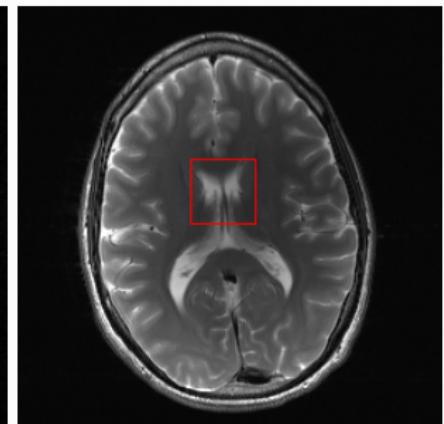
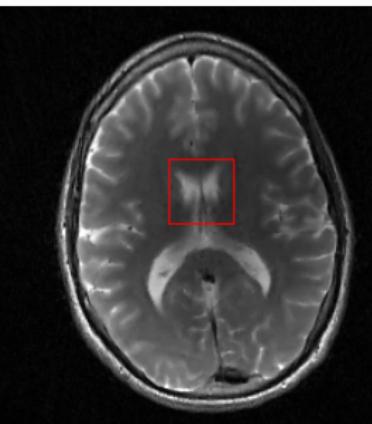
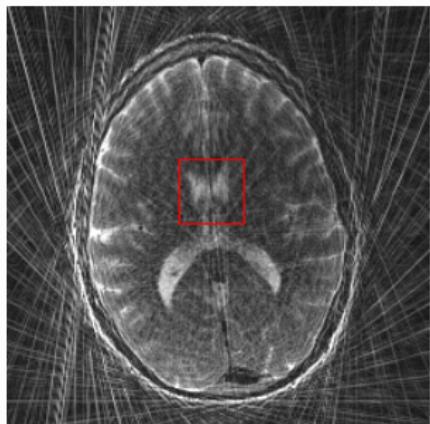
Undersampled noisy data  $y$

$$\xrightarrow{\mathcal{F}^{-1}}$$



Reconstruction  $u$

# Benchmark Regularizer: TGV



Unders. Noisy Data  
Least Squares

Unders. Noisy Data  
Regularized (TGV)

Full Data  
Least Squares

Bredies, Kunisch, Pock. **Total Generalized Variation. SIAM Imaging** (2010)



# Motivation: Undersampled Dynamic MRI

**Goal:** Dynamic MRI  $\rightsquigarrow$  **Motion** is big challenge to accurate reconstructions

- ▶ High resolution imaging
- ▶ Imaging moving organs

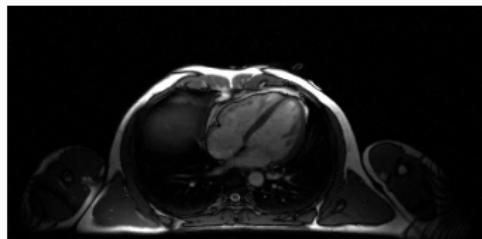
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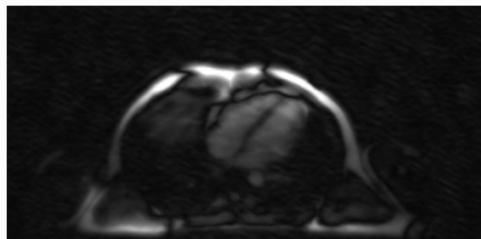
- ▶ High resolution imaging
- ▶ Imaging moving organs

**Dynamic IP:** Reconstruct movie  $u_t$  from undersampled data series  $y_t$

$$\mathfrak{F}(u_t) = y_t \quad \text{for all } t \in [0, 1]$$



Fully sampled data



Undersampled data

**Solution:** We need regularization for **dynamic inverse problems**



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Fully sampled data

Undersampled data

**Solution:** We need regularization for **dynamic inverse problems**



# Dynamic Inverse Problem

- ▶ **Images:** Radon Measures  $\mu \in \mathcal{M}(\Omega)$       ( $\Omega \subset \mathbb{R}^N$  bounded closed domain)
- ▶ **Data spaces:** Hilbert spaces  $H_t$  for  $t \in [0, 1]$
- ▶ **Measurement Operators:** linear continuous maps

$$K_t: \mathcal{M}(\Omega) \rightarrow H_t$$

- ▶ **Data points:** Curve  $t \mapsto y_t$  with  $y_t \in H_t$

---

[2] Bredies, Fanzon. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)



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**Dynamic Inverse Problem:** Find **curve** of measures  $t \mapsto \mu_t \in \mathcal{M}(\Omega)$  s.t.

$$K_t \mu_t = y_t \quad \text{for all } t \in [0, 1] \tag{P}$$

**Assumptions:** weak time-regularity for  $\{H_t\}_t$  and  $K_t^*$       (wk\*-measurability)

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[2] Bredies, Fanzon. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)



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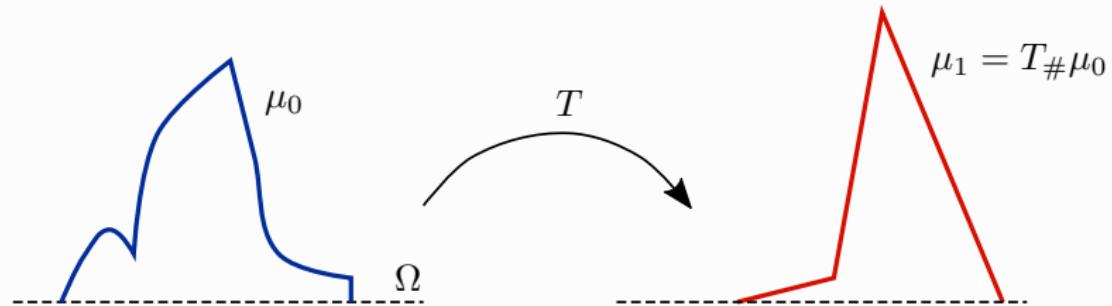
**Assumptions:** weak time-regularity for  $\{H_t\}_t$  and  $K_t^*$       (wk\*-measurability)

**Proposal:** Regularize (P) with an **Optimal Transport Energy**

[2] Bredies, **Fanzon**. *ESAIM: Mathematical Modelling and Numerical Analysis* (2020)

# Optimal Transport - Static Formulation

$\Omega \subset \mathbb{R}^d$  bounded domain,  $\mu_0, \mu_1 \in \mathcal{P}(\Omega)$ ,  $T: \Omega \rightarrow \Omega$  measurable displacement



**Goal:** move  $\mu_0$  to  $\mu_1$  in the cheapest way, with cost of moving mass from  $x$  to  $y$

$$c(x, y) := |x - y|^2$$

**Optimal Transport:** a transport plan  $\hat{T}$  solving

$$\hat{T} \in \arg \min \left\{ \int_{\Omega} |T(x) - x|^2 d\mu_0(x) : T: \Omega \rightarrow \Omega, T_{\#}\mu_0 = \mu_1 \right\}$$

# Optimal Transport - Dynamic Formulation

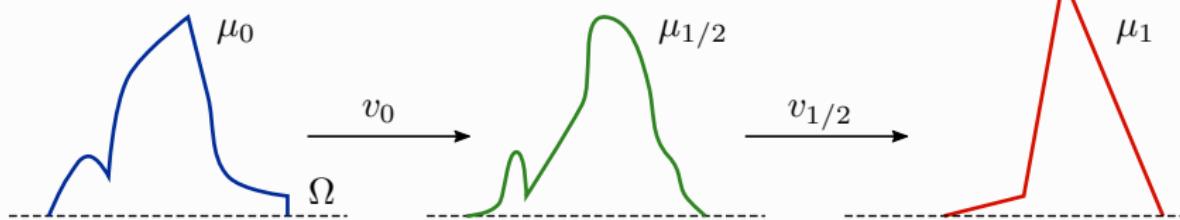
**Idea:** introduce a time variable  $t \in [0, 1]$  and consider the density **evolution**

- ▶ time dependent probability measures

$$t \mapsto \mu_t \in \mathcal{P}(\Omega) \text{ for } t \in [0, 1]$$

- ▶  $\mu_t$  is advected by the velocity field

$$v_t(x): [0, 1] \times \Omega \rightarrow \mathbb{R}^d$$



**Dynamic model:**  $(\mu_t, v_t)$  solves the **continuity equation** with initial conditions

$$\begin{cases} \partial_t \mu_t + \operatorname{div}(\mu_t v_t) = 0 \\ \text{Initial data } \mu_0, \text{ final data } \mu_1 \end{cases} \quad (\text{CE-IC})$$



# Benamou-Brenier Formula

## Theorem: Benamou-Brenier [1]

$$\min_{\substack{(\mu_t, v_t) \\ \text{solving (CE-IC)}}} \int_0^1 \int_{\Omega} |v_t(x)|^2 \mu_t(x) dx dt = \min_{\substack{T: \Omega \rightarrow \Omega \\ T_{\#} \mu_0 = \mu_1}} \int_{\Omega} |T(x) - x|^2 \mu_0(x) dx$$

## Advantages of Dynamic Formulation:

- ① By introducing the momentum  $m_t := \rho_t v_t$  we have

$$\int_0^1 \int_{\Omega} |v_t(x)|^2 \mu_t(x) dx dt = \int_0^1 \int_{\Omega} \frac{|m_t(x)|^2}{\mu_t(x)} dx dt$$

which is **convex** in  $(\mu_t, m_t)$

- ② The continuity equation becomes **linear**

$$\partial_t \mu_t + \operatorname{div} m_t = 0$$

- ③ We know the full trajectory  $\mu_t$  and can recover the velocity field  $v_t$  from  $m_t$

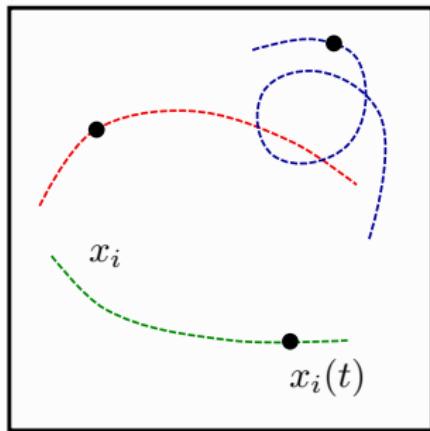
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[1] Benamou, Brenier. **Numerische Mathematik** (2000)

# Optimal Transport Regularization

**Trajectories:** Curve of measures

$$t \mapsto \mu_t \in \mathcal{M}(\Omega), \quad t \in [0, 1]$$



$$\mu_t = \sum_i \delta_{x_i(t)}$$

---

[2] Bredies, **Fanzon**. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)

# Optimal Transport Regularization

**Trajectories:** Curve of measures

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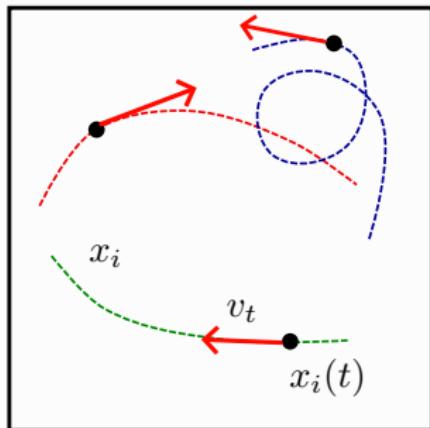
**Assumptions:**

- $\mu_t$  satisfies **Continuity Equation**

$$\partial_t \mu_t + \operatorname{div}(v_t \mu_t) = 0$$

for some velocity field (to find)

$$v_t : \mathbb{R}^2 \rightarrow \mathbb{R}^2$$



$$\mu_t = \sum_i \delta_{x_i(t)}$$

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[2] Bredies, **Fanzon**. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)

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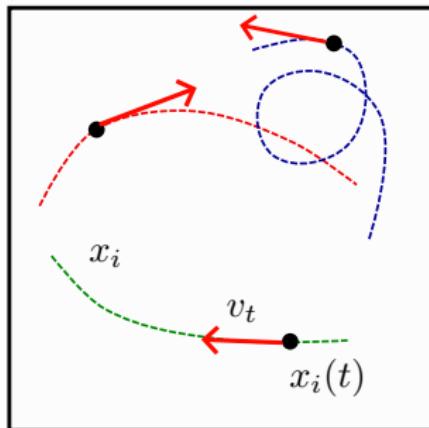
$$\partial_t \mu_t + \operatorname{div}(v_t \mu_t) = 0$$

for some velocity field (to find)

$$v_t : \mathbb{R}^2 \rightarrow \mathbb{R}^2$$

- Finite **Kinetic Energy**

$$\int_0^1 \int_{\mathbb{R}^2} |v_t(x)|^2 d\mu_t(x) dt < \infty$$



$$\mu_t = \sum_i \delta_{x_i(t)}$$

---

[2] Bredies, **Fanzon**. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)

# Optimal Transport Regularization



**Minimization Problem:** Given data  $t \mapsto y_t \in H_t$

$$K_t \mu_t = y_t \quad \leadsto \quad \min_{\mu, v} L(\mu) + R(\mu, v)$$

---

[2] Bredies, Fanzon. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)



# Optimal Transport Regularization

**Minimization Problem:** Given data  $t \mapsto y_t \in H_t$

$$K_t \mu_t = y_t \quad \leadsto \quad \min_{\mu, v} L(\mu) + R(\mu, v)$$

- $L \leadsto$  **Loss Function:** Fits  $t \mapsto \mu_t$  to data  $t \mapsto y_t$  (Generalized Bochner spaces [2])

$$L(\mu) := \int_0^1 \|K_t \mu_t - y_t\|_{H_t}^2 dt$$

---

[2] Bredies, Fanzon. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)



# Optimal Transport Regularization

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$$L(\mu) := \int_0^1 \|K_t \mu_t - y_t\|_{H_t}^2 dt$$

- **$R \sim$  Regularizer:** Connected to **Optimal Transport** (Benamou-Brenier formula)

$$R(\mu, v) := \underbrace{\int_0^1 \int_{\Omega} |v_t(x)|^2 d\mu_t(x) dt}_{\text{Kinetic Energy}} + \underbrace{\int_0^1 \|\mu_t\|_{\mathcal{M}(\Omega)} dt}_{\text{Radon Norm}}$$

s.t.  $\underbrace{\partial_t \mu_t + \operatorname{div}(v_t \mu_t)}_{\text{Continuity Equation}} = 0$

- **Theorem [2]:**  $R$  provides stable regularization for the dynamic inverse problem

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[2] Bredies, Fanzon. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)

# Extremal Points

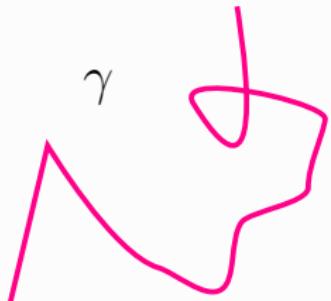
$$R(\mu, v) := \int_0^1 \int_{\Omega} |v_t(x)|^2 d\mu_t(x) dt + \int_0^1 \|\mu_t\|_{\mathcal{M}(\Omega)} dt$$

s.t.  $\partial_t \mu_t + \operatorname{div}(v_t \mu_t) = 0$  (CE)

## Theorem [1]

Let  $B = \{R \leq 1\}$ . Then  $\operatorname{Ext}(B)$  are measures  $t \mapsto \mu_t$  supported on **Sobolev Curves**

$$t \mapsto \mu_t = \delta_{\gamma(t)}, \quad \gamma \in H^1([0, 1]; \Omega)$$



**Superposition Principle [2]:**  $\mu_t$  solves (CE)  $\iff \exists \sigma \in P(H^1)$  concentrated on sol. to

$$\dot{\gamma}(t) = v(t, \gamma(t)) \text{ and s.t. } \int_{\Omega} \varphi d\mu_t = \int_{H^1} \varphi(\gamma(t)) d\sigma(\gamma), \forall \varphi \in C(\Omega)$$

**Proof Idea:**  $\mu_t$  extr. for  $R \iff \sigma$  extr. for  $\|\cdot\|_{\mathcal{M}(H^1)}$   $\stackrel{\text{Known}}{\iff} \sigma = \delta_{\gamma} \stackrel{\text{SP}}{\iff} \mu_t = \delta_{\gamma(t)}$

[1] Bredies, Carioni, **Fanzon**, Romero. **Bulletin London Mathematical Society** (2021)

[2] Ambrosio. **Inv. Math.** (2004)



# Non-homogeneous case

- Homogeneous continuity equation implies mass preservation

$$\mu_t(\Omega) \text{ is constant for all } t$$

- Restrictive in applications – e.g. contrast agent in MRI
- Modify the regularizer to allow change of mass
- Based on **Unbalanced OT** – a.k.a. Hellinger-Kantorovich distance [2,3]

$$R(\mu, v) := \int_0^1 \int_{\Omega} |v_t(x)|^2 + |g_t(x)|^2 d\mu_t(x) dt + \int_0^1 \|\mu_t\|_{\mathcal{M}(\Omega)} dt$$
$$\text{s.t. } \partial_t \mu_t + \operatorname{div}(v_t \mu_t) = g_t \mu_t \quad (\text{CE})$$

**Theorem [1]:**  $R$  is stable regularizer for the dynamic inverse problem

- 
- [1] Bredies, **Fanzon**. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)
  - [2] Chizat, Peyré, Schmitzer, Vialard. **Found. of Comp. Math.** (2018)
  - [3] Liero, Mielke, Savaré. **Inv. Math.** (2018)



# Extremal Points – Non-homogeneous case

$$R(\mu, v) := \int_0^1 \int_{\Omega} |v_t(x)|^2 + |g_t(x)|^2 d\mu_t(x) dt + \int_0^1 \|\mu_t\|_{\mathcal{M}(\Omega)} dt$$
$$\text{s.t. } \partial_t \mu_t + \operatorname{div}(v_t \mu_t) = g_t \mu_t \quad (\text{CE})$$

## Theorem [1]

Let  $B = \{R \leq 1\}$ . Then  $\operatorname{Ext}(B)$  are curves of measures of the form

$$t \mapsto \mu_t = h(t) \delta_{\gamma(t)}$$

- ▶  $h, \sqrt{h} \in \operatorname{AC}^2(0, 1)$ ,  $\gamma \in C(\{h > 0\}; \Omega)$ ,  $\sqrt{h}\gamma \in \operatorname{AC}^2([0, 1]; \mathbb{R}^d)$
- ▶  $\{h > 0\}$  is connected

**Proof Idea:** Novel Probabilistic Superposition Principle to (CE)

---

[1] Bredies, Carioni, **Fanzon**. Communications in PDEs (2022)



# Numerical optimization

**Dynamic IP:** Given  $t \mapsto y_t \in H_t$  find  $t \mapsto \mu_t \in \mathcal{M}(\Omega)$  s.t.

$$K_t \mu_t = y_t \quad \text{for all } t \in [0, 1]$$

**Optimal Transport Regularization:**  $\min_{\mu, v} L(\mu) + R(\mu, v)$

$$L = \int_0^1 \|K_t \mu_t - y_t\|_{H_t}^2 , \quad R = \int_0^1 \int_{\Omega} |v_t(x)|^2 dt + \int_0^1 \|\mu_t\|_{\mathcal{M}(\Omega)} dt$$

s.t.  $\partial_t \mu_t + \operatorname{div}(v_t \mu_t) = 0$

- ▶ **Given:**  $\Omega \subset \mathbb{R}^d$  and  $t \mapsto y_t \in H_t$  data
- ▶ **Forw. operator:**  $K: \mathcal{M}(\Omega) \rightarrow H_t$
- ▶ **Ext. points:**  $B = \{R \leq 1\}$

$$\operatorname{Ext}(B) = \left\{ t \mapsto \delta_{\gamma(t)} : \gamma \in H^1([0, 1]; \Omega) \right\}$$



# Generalized Frank-Wolfe [1]

$$\min_{\mu, v} \int_0^1 \|K_t \mu_t - y_t\|_{H_t}^2 + \int_0^1 \int_{\Omega} |v_t(x)|^2 dt + \int_0^1 \|\mu_t\|_{\mathcal{M}(\Omega)} dt$$

s.t.  $\partial_t \mu_t + \operatorname{div}(v_t \mu_t) = 0$

**Algorithm:**    **Initialize:**  $\mu^0 = 0$     **Iterate:** Given  $\mu^k = \sum_{i=1}^n \lambda_i \delta_{\gamma_i}$

**① Insertion Step:**  $p_t^k = K_*(K \mu_t^k - y_t)$      $p_t^k \in L^\infty([0, 1]; C(\Omega))$

$$\max_{w \in \operatorname{Ext}(B)} \langle p^k, w \rangle = \max_{\gamma \in H^1([0, 1]; \Omega)} \left( \int_0^1 |\dot{\gamma}(t)|^2 dt + 1 \right)^{-1} \int_0^1 p_t^k(\gamma(t)) dt \quad \leadsto \quad \hat{\gamma}$$

**② Fully-corrective Step:** Solve

$$\lambda_i^* \in \arg \min_{\lambda_i \geq 0} G \left( \mu^k + \lambda_{n+1} \delta_{\hat{\gamma}} \right) \quad \leadsto \quad \mu^{k+1} := \left( \sum_{i=1}^n \lambda_i^* \delta_{\gamma_i} \right) + \lambda_{n+1}^* \delta_{\hat{\gamma}}$$

---

[1] Bredies, Carioni, **Fanzon**, Romero. **Found. of Computational Mathematics** (2023)



# Convergence Analysis

## Theorem [1]

$\mu^k$  sparse iterate from the Generalized Frank-Wolfe Algorithm. Then

$$\mu^k \xrightarrow{*} \bar{\mu}, \quad \bar{\mu} \in \arg \min G, \quad G := L + R$$

General convergence rate is **sublinear**

(expected for gradient methods)

$$G(\mu^k) - \min G \lesssim \frac{1}{k}$$

**Work in Progress:**  $\bar{\mu}$  **sparse** + “**Source Condition**” + “**Quadratic Growth**”

$$\implies \text{linear convergence:} \quad G(\mu^k) - \min G \lesssim \frac{1}{2^k}$$

---

[1] Bredies, Carioni, **Fanzon**, Romero. **Found. of Computational Mathematics** (2023)



# Details and additional tweaks

- ▶ Solve the curve insertion problem

$$\hat{\gamma} \in \arg \max_{\gamma \in H^1([0,1];\Omega)} \left( \int_0^1 |\dot{\gamma}(t)|^2 dt + 1 \right)^{-1} \int_0^1 p_t^k(\gamma(t)) dt$$

via gradient descent with suitable stepsize rule

## Theorem [1]

Under suitable regularity assumptions, the gradient descent procedure converges subsequentially to stationary points and strongly in  $\text{AC}^2([0, 1]; \Omega)$ .

- ▶ Multiple starts with suitable initial guess (crossovers, random curves, etc.) to increase chance to obtain global minimizer
- ▶ Multiple insertion  $\leadsto$  insert all obtained stationary points

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[1] Bredies, Carioni, **Fanzon**, Romero. **Found. of Computational Mathematics** (2023)



# Outline

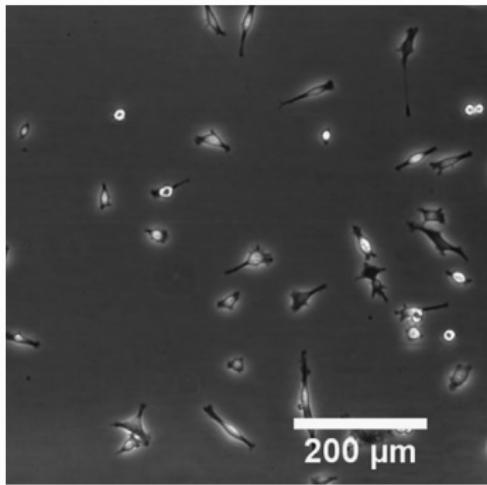
- 1 Introduction to Inverse Problems & Sparsity
- 2 Algorithm for sparse solution recovery
- 3 Dynamic Inverse Problems
- 4 Application to Dynamic MRI

# Motivation: Particle Tracking



**Imaging Method**  $\implies$

- ▶ Stars from ground-based telescope
- ▶ Microbubbles in blood vessels
- ▶ Cell migration



Microscopy image of cells

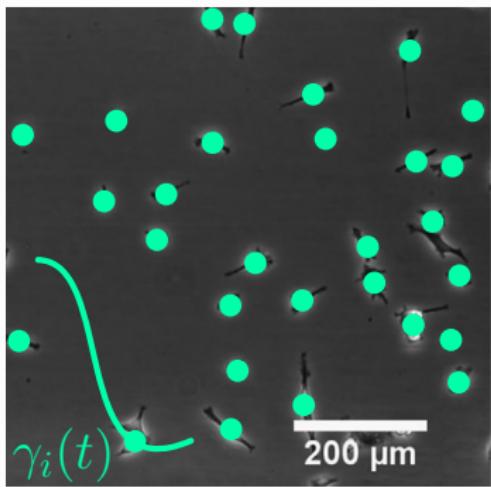
---

**Image from:** Yang, Venkataraman, Styles, et al. **Journal of Biomechanics** (2016)

# Motivation: Particle Tracking

Imaging Method  $\implies$

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Microscopy image of cells

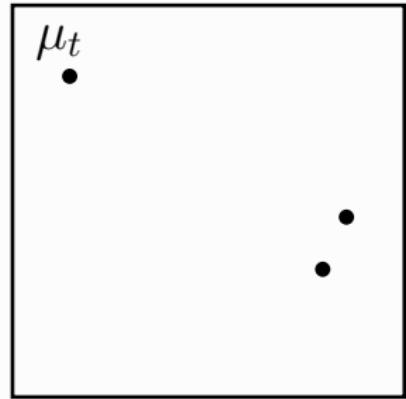
$$\mu_t = \sum_{i=1}^M \delta_{\gamma_i(t)}$$

Image from: Yang, Venkataraman, Styles, et al. **Journal of Biomechanics** (2016)

# Application: Peak tracking for Dynamic MRI



$y_t$



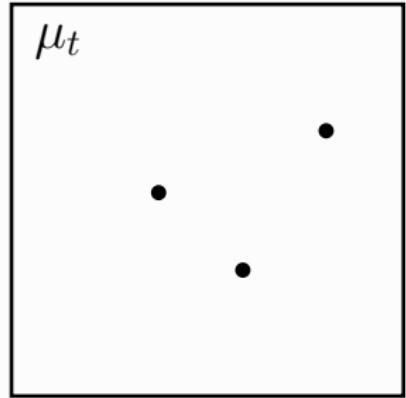
$$\mu_t = \sum_{i=1}^3 \delta_{\gamma_i(t)}$$

**Frame-by-Frame:** MRI Data  $y_t \rightsquigarrow$  Image  $\mu_t$

# Application: Peak tracking for Dynamic MRI



$y_t$



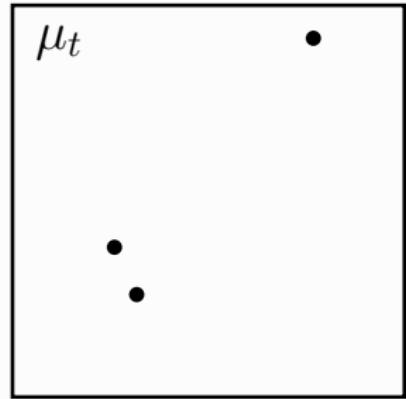
$$\mu_t = \sum_{i=1}^3 \delta_{\gamma_i(t)}$$

**Frame-by-Frame:** MRI Data  $y_t \rightsquigarrow$  Image  $\mu_t$

# Application: Peak tracking for Dynamic MRI



$y_t$



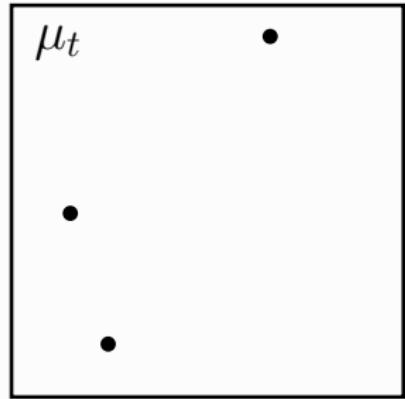
$$\mu_t = \sum_{i=1}^3 \delta_{\gamma_i(t)}$$

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# Application: Peak tracking for Dynamic MRI



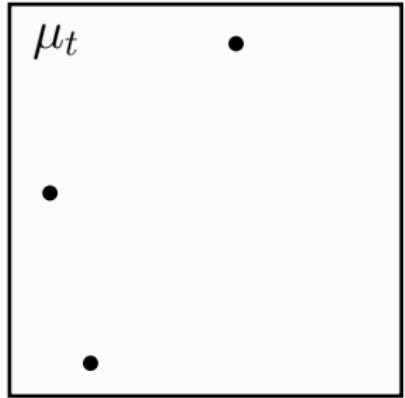
$y_t$



$$\mu_t = \sum_{i=1}^3 \delta_{\gamma_i(t)}$$

**Frame-by-Frame:** MRI Data  $y_t \rightsquigarrow$  Image  $\mu_t$

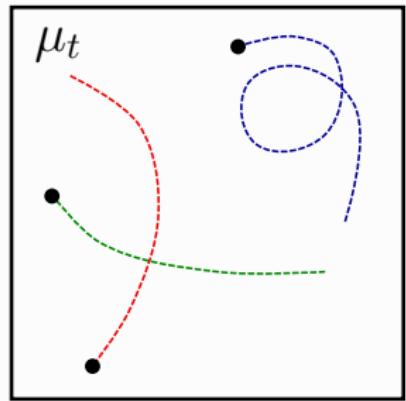
# Application: Peak tracking for Dynamic MRI



$$\mu_t = \sum_{i=1}^3 \delta_{\gamma_i(t)}$$

**Frame-by-Frame:** MRI Data  $y_t \rightsquigarrow$  Image  $\mu_t$

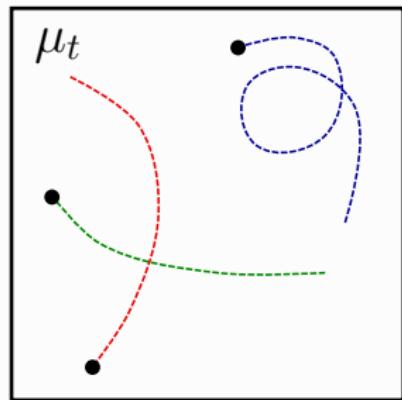
# Application: Peak tracking for Dynamic MRI



$$\mu_t = \sum_{i=1}^3 \delta_{\gamma_i(t)}$$

**Frame-by-Frame:** MRI Data  $y_t \rightsquigarrow$  Image  $\mu_t \implies$  Interpolate Trajectories

# Application: Peak tracking for Dynamic MRI

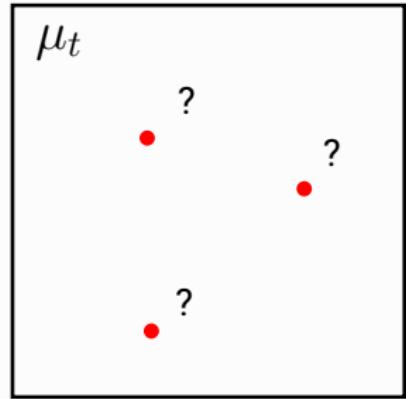


$$\mu_t = \sum_{i=1}^3 \delta_{\gamma_i(t)}$$

**Frame-by-Frame:** MRI Data  $y_t \sim$  Image  $\mu_t \implies$  Interpolate Trajectories

**Issue:** Motion  $\implies$  Low Scan Time  $\implies$  **Low Data**  $y_t$

# Application: Peak tracking for Dynamic MRI

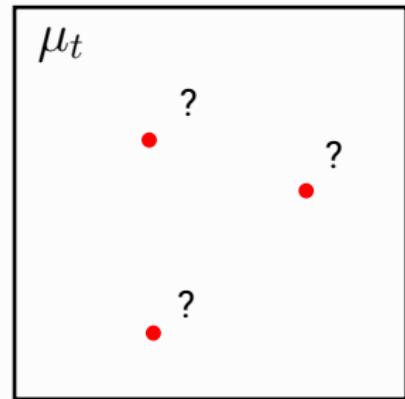
 $y_t$ 

$$\mu_t = \sum_{i=1}^3 \delta_{\gamma_i(t)}$$

**Frame-by-Frame:** MRI Data  $y_t \sim$  Image  $\mu_t \implies$  Interpolate Trajectories

**Issue:** Motion  $\implies$  Low Scan Time  $\implies$  **Low Data**  $y_t \sim$  **Particles?**

# Application: Peak tracking for Dynamic MRI



$$\mu_t = \sum_{i=1}^3 \delta_{\gamma_i(t)}$$

**Frame-by-Frame:** MRI Data  $y_t \sim$  Image  $\mu_t \implies$  Interpolate Trajectories

**Issue:** Motion  $\implies$  Low Scan Time  $\implies$  **Low Data**  $y_t \sim$  **Particles?**

**Global-in-Time:** Full Time-Series  $t \mapsto y_t \sim$  Trajectories  $t \mapsto \mu_t$

# The Dynamic Undersampled MRI problem



**Dynamic IP MRI:** Given  $t \mapsto y_t \in \mathbb{C}^{M_t}$  find  $t \mapsto \mu_t \in \mathcal{M}(\Omega)$  s.t.

$$K_t \mu_t = y_t \quad \text{for all } t \in [0, 1]$$

**Fourier Transform:** For  $\mu \in \mathcal{M}(\Omega)$

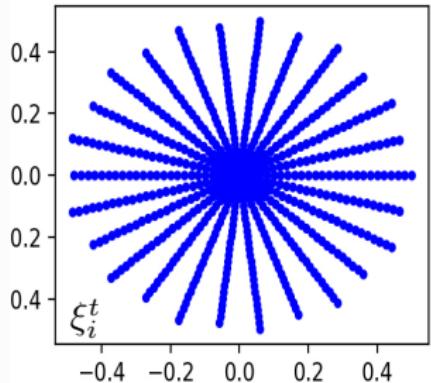
$$\hat{\mu}: \mathbb{C} \rightarrow \mathbb{C}, \quad \hat{\mu}[\xi] := \frac{1}{2\pi} \int_{\mathbb{R}^2} e^{i\xi \cdot x} d\mu(x)$$

**Sampling Frequencies:**  $M_t$  points

$$\xi_1^t, \dots, \xi_{M_t}^t \in \mathbb{C}$$

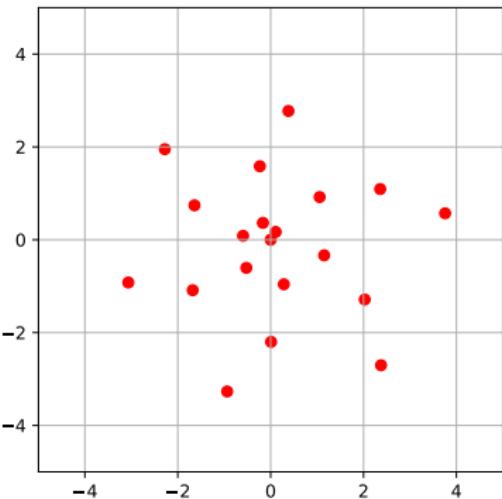
**Forward operators:** linear cont.  $K_t: \mathcal{M}(\Omega) \rightarrow \mathbb{C}^{M_t}$

$$K_t \mu := (\hat{\mu}[\xi_1^t], \dots, \hat{\mu}[\xi_{M_t}^t])$$



Example: Radial Sampling

# Experiment 1: Spiral sampling (static)



**Ground truth:** Curve of measures

$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

**Sampling Freq:**  $\xi_1, \dots, \xi_{20}$

**Data:** Defined by

$$y_t := K\bar{\mu}_t + 20\% \text{ Noise}$$



# Experiment 1: Spiral sampling (static)

**Algorithm: Generalized Frank-Wolfe**  $\leadsto t \mapsto \mu_t^k = \sum_{i=1}^M \lambda_i \delta_{\gamma_i(t)}$

**Ground truth:** Curve of measures

$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

**Reconstruction:** from data

$$y_t = K\bar{\mu}_t + 20\% \text{ Noise}$$

(Thresholded at 0.05)



# Experiment 1: Spiral sampling (static)

**Algorithm: Generalized Frank-Wolfe**  $\leadsto t \mapsto \mu_t^k = \sum_{i=1}^M \lambda_i \delta_{\gamma_i(t)}$

**Ground truth:** Curve of measures

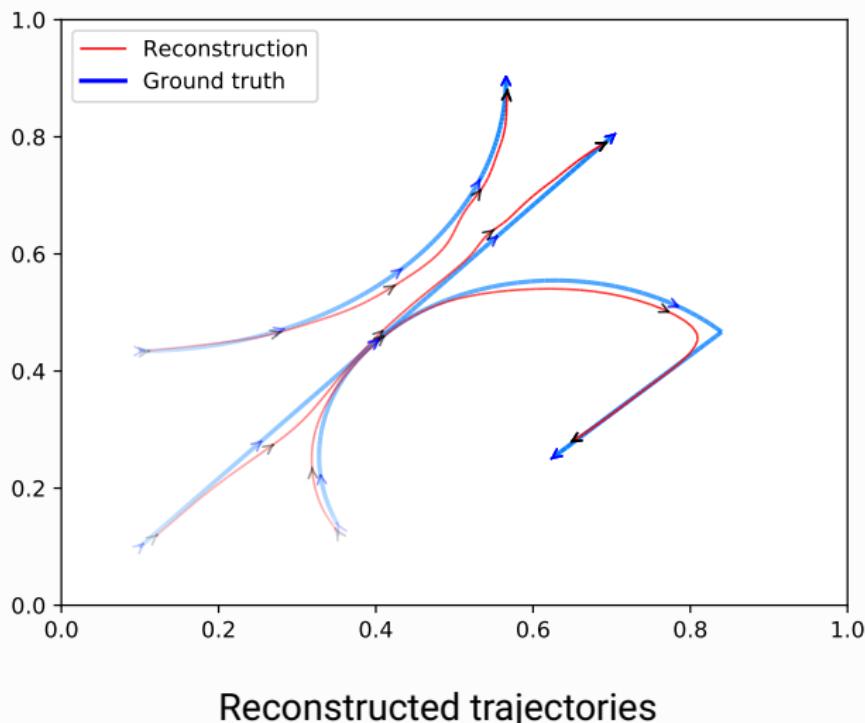
$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

**Reconstruction:** from data

$$y_t = K\bar{\mu}_t + 20\% \text{ Noise}$$

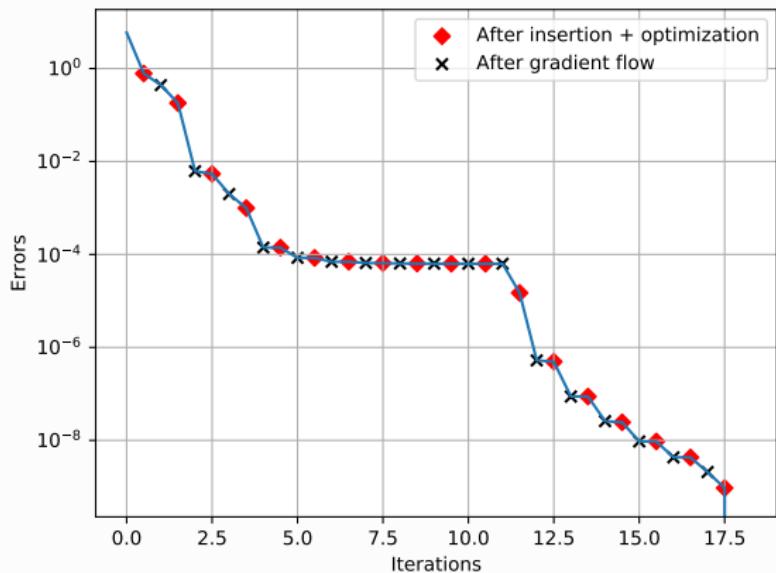
**(No Thresholding)**

# Experiment 1: Spiral sampling (static)



Reconstructed trajectories

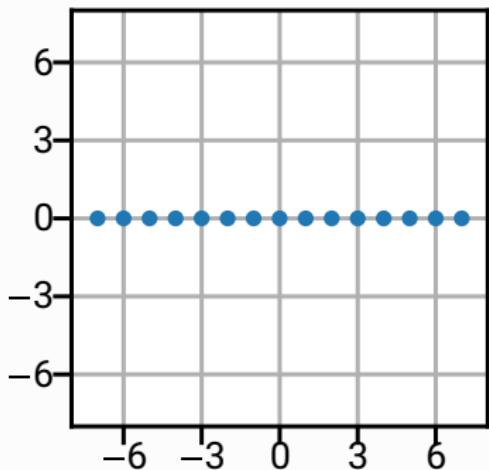
# Experiment 1: Spiral sampling (static)



Convergence plot: exhibits linear rate

$$\text{Error} = G(\mu^k) - G(\mu^{k+1})$$

## Experiment 2: Dynamic sampling on lines



$$t = 0$$

**Ground truth:** Curve of measures

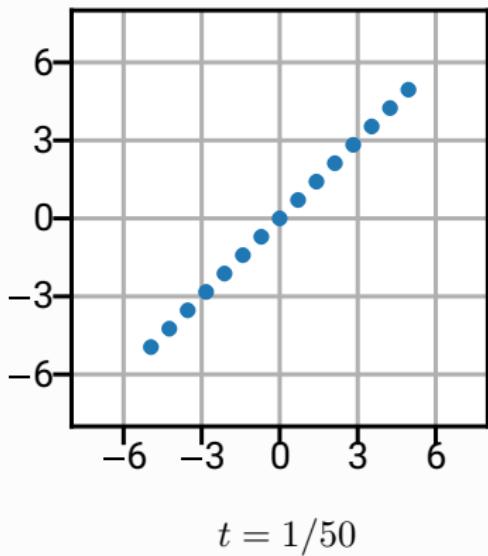
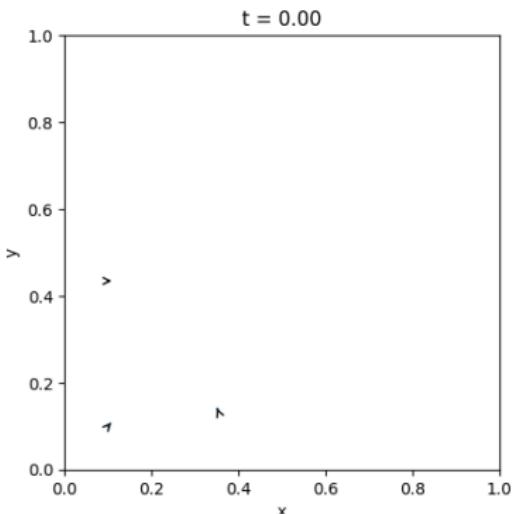
$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

**Sampling Freq:**  $\xi_1^t, \dots, \xi_{15}^t$

**Data:** Defined by

$$y_t := K_t \bar{\mu}_t + 20\% \text{ Noise}$$

# Experiment 2: Dynamic sampling on lines



**Ground truth:** Curve of measures

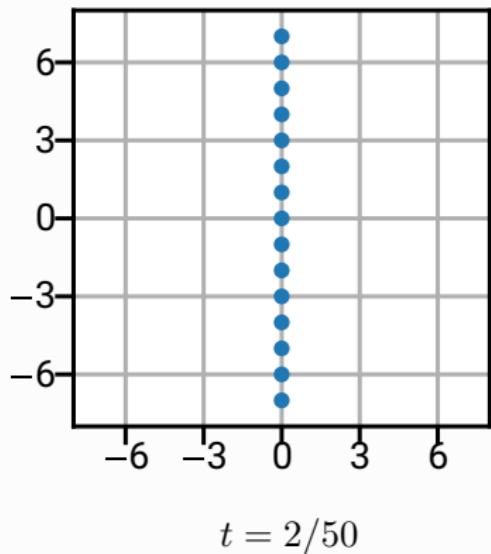
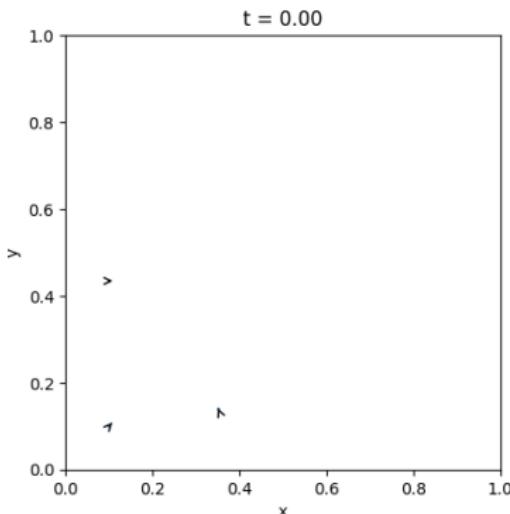
$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

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**Data:** Defined by

$$y_t := K_t \bar{\mu}_t + 20\% \text{ Noise}$$

# Experiment 2: Dynamic sampling on lines



**Ground truth:** Curve of measures

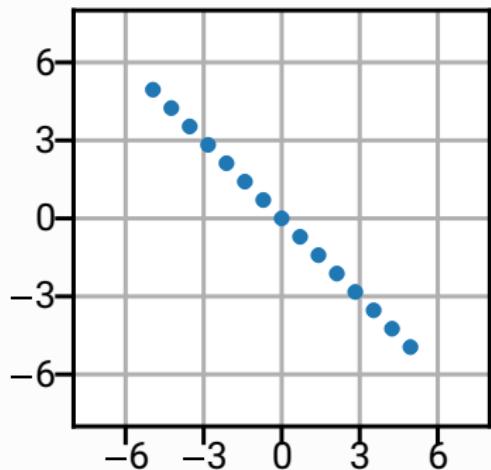
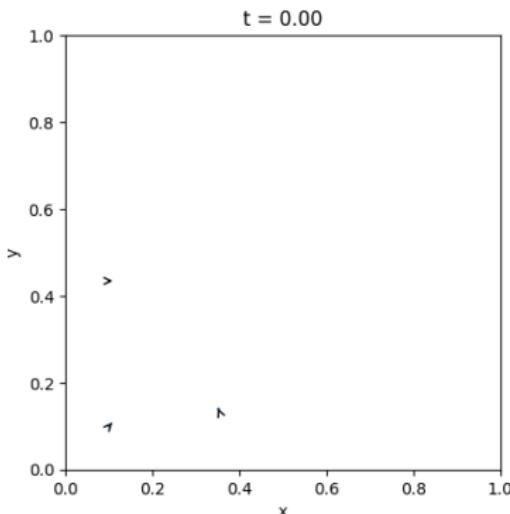
$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

**Sampling Freq:**  $\xi_1^t, \dots, \xi_{15}^t$

**Data:** Defined by

$$y_t := K_t \bar{\mu}_t + 20\% \text{ Noise}$$

# Experiment 2: Dynamic sampling on lines



$t = 3/50$

**Ground truth:** Curve of measures

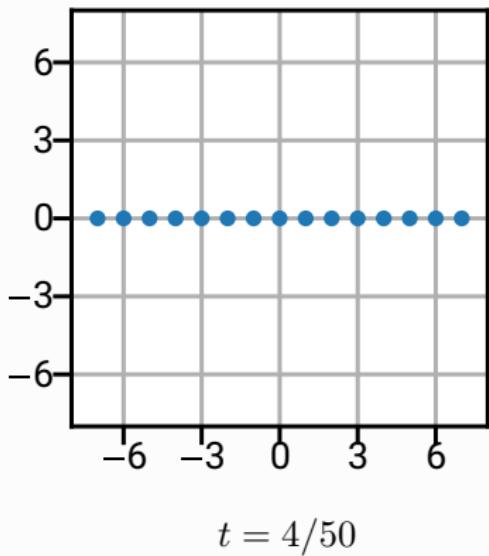
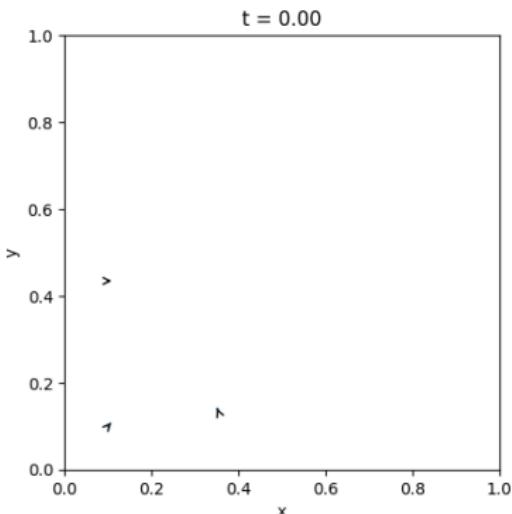
$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

**Sampling Freq:**  $\xi_1^t, \dots, \xi_{15}^t$

**Data:** Defined by

$$y_t := K_t \bar{\mu}_t + 20\% \text{ Noise}$$

# Experiment 2: Dynamic sampling on lines



**Ground truth:** Curve of measures

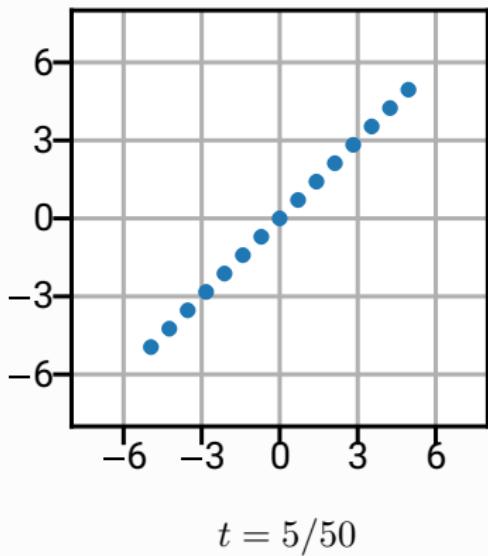
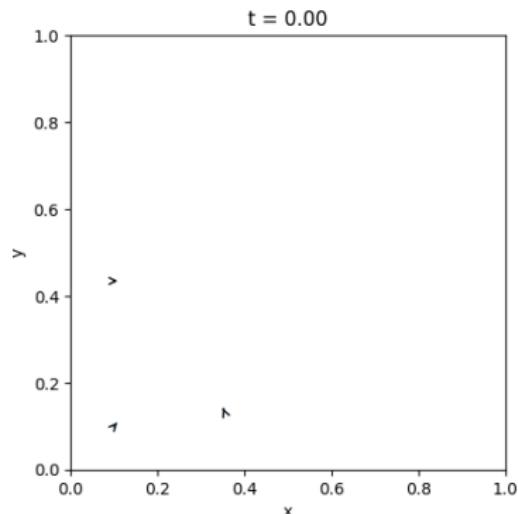
$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

**Sampling Freq:**  $\xi_1^t, \dots, \xi_{15}^t$

**Data:** Defined by

$$y_t := K_t \bar{\mu}_t + 20\% \text{ Noise}$$

# Experiment 2: Dynamic sampling on lines



**Ground truth:** Curve of measures

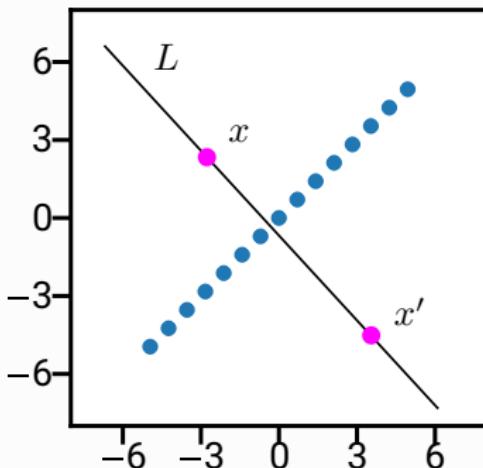
$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

**Sampling Freq:**  $\xi_1^t, \dots, \xi_{15}^t$

**Data:** Defined by

$$y_t := K_t \bar{\mu}_t + 20\% \text{ Noise}$$

## Experiment 2: Dynamic sampling on lines



- $L$  line orthogonal to the line of sampling frequencies at time  $t$

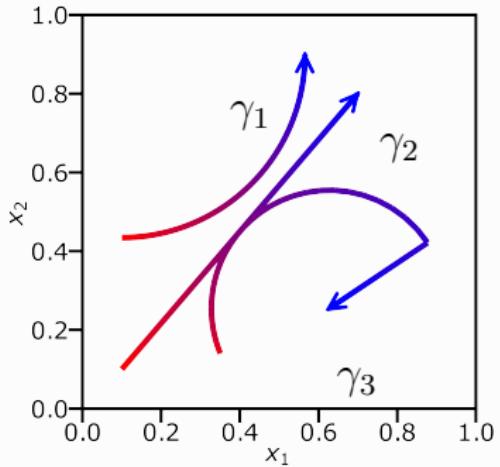
$$x, x' \in L \quad \Rightarrow \quad K_t \delta_x = K_t \delta_{x'}$$

- Impossible to locate source along  $L$  at time  $t$
- Only way to locate source is to enforce time regularity
- Example showcases need for time regularization

# Experiment 2: Dynamic sampling on lines

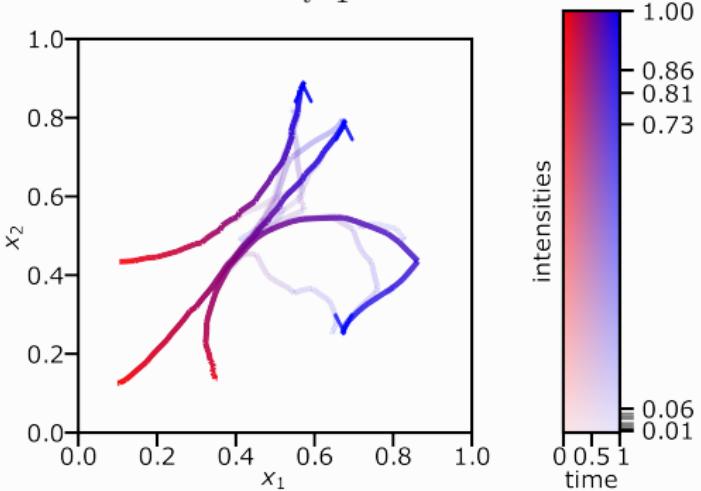
**Algorithm: Generalized Frank-Wolfe**

$$\sim t \mapsto \bar{\mu}_t^k = \sum_{i=1}^M \lambda_i \delta_{\gamma_i(t)}$$



**Ground truth:** Curve of measures

$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)} + \delta_{\gamma_3(t)}$$

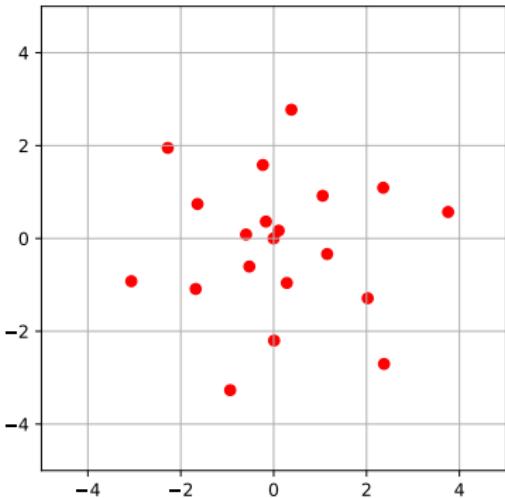


**Reconstruction:** from data

$$y_t = K_t \bar{\mu}_t + 20\% \text{ Noise}$$

**Remarkable reconstructions – considering unfavorable sampling pattern**

# Experiment 3: Crossing



**Ground truth:** Curve of measures

$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)}$$

**Sampling Freq:**  $\xi_1, \dots, \xi_{20}$

**Data:** Defined by

$$y_t := K\bar{\mu}_t + 20\% \text{ Noise}$$



# Experiment 3: Crossing

**Algorithm: Generalized Frank-Wolfe**  $\leadsto t \mapsto \mu_t^k = \sum_{i=1}^M \lambda_i \delta_{\gamma_i(t)}$

**Ground truth:** Curve of measures

$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)}$$

**Reconstruction:** from data

$$y_t = K\bar{\mu}_t + 20\% \text{ Noise}$$

(Thresholded at 0.01)



# Experiment 3: Crossing

**Algorithm: Generalized Frank-Wolfe**  $\leadsto t \mapsto \mu_t^k = \sum_{i=1}^M \lambda_i \delta_{\gamma_i(t)}$

**Ground truth:** Curve of measures

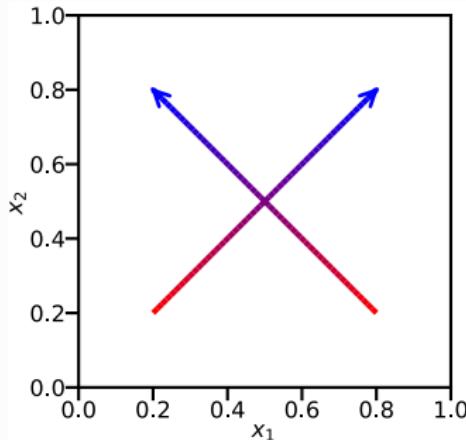
$$\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)}$$

**Reconstruction:** from data

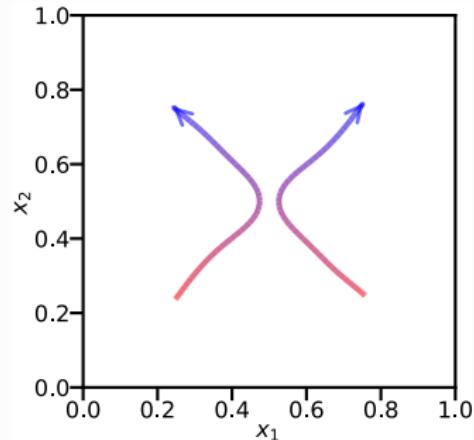
$$y_t = K\bar{\mu}_t + 20\% \text{ Noise}$$

**(No Thresholding)**

# Experiment 3: Crossing



**Ground truth:**  $\bar{\mu}_t := \delta_{\gamma_1(t)} + \delta_{\gamma_2(t)}$



**Reconstruction:**  $\tilde{\mu}_t := \delta_{\tilde{\gamma}_1(t)} + \delta_{\tilde{\gamma}_2(t)}$

**Question:** Why do reconstructed trajectories differ from ground truth ones?

**Answer:** They don't! When regarded as measures they are basically the same

$$dt \otimes \bar{\mu}_t \approx dt \otimes \tilde{\mu}_t$$

Regularizer is Dynamic OT  $\implies$  Particles chose shortest path

**What to do?** Maybe could include curvature penalization



# Conclusion

- ① Algorithm for computing **sparse** solutions to

$$\min_{u \in X} F(Ku) + R(u)$$

in **Banach** space



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- ① Algorithm for computing **sparse** solutions to

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- ② Linear convergence if solution is **Sparse** + “**Source Condition**” + “**Quadratic Growth**”
- ③ General framework for **dynamic** inverse problems



# Conclusion

- ① Algorithm for computing **sparse** solutions to

$$\min_{u \in X} F(Ku) + R(u)$$

in **Banach** space

- ② Linear convergence if solution is **Sparse** + “**Source Condition**” + “**Quadratic Growth**”
- ③ General framework for **dynamic** inverse problems
- ④ Application to **Dynamic MRI**

Thank You!



# References

## Generalized Frank-Wolfe Algorithm

- [1] Bredies, Carioni, **Fanzon**, Walter. **Mathematical Programming** (2024)

## Particles Tracking + Dynamic Inverse Problems

- [2] **Fanzon**, Bredies. **ESAIM: Mathematical Modelling and Numerical Analysis** (2020)
- [3] Bredies, Carioni, **Fanzon**, Romero. **Bulletin London Mathematical Society** (2021)
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“Mathematical methods for motion-aware medical imaging”

# Infinite dimensional Example: Deblurring



Direct problem



Inverse problem

Original Image  $u: \Omega \rightarrow \mathbb{R}$

Blurred image  $f: \Omega \rightarrow \mathbb{R}$

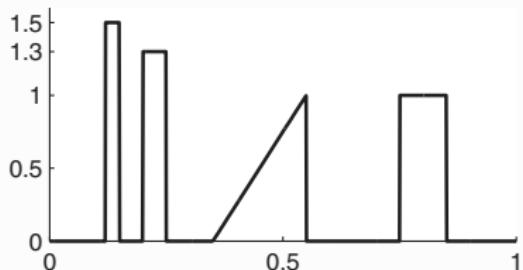
- Deblurring can be achieved by **deconvolution**

$$\text{Solve } Ku = f, \quad (Ku)(x) = \int_{\mathbb{R}^2} \psi(y)u(x-y) dy = (\psi \star u)(x)$$

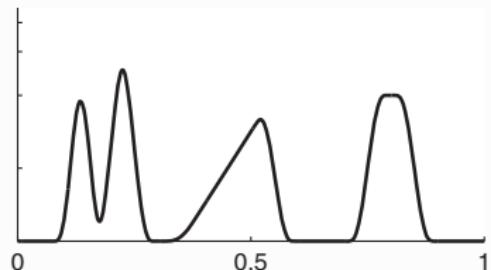
with  $\psi$  suitable kernel (e.g. point-spread function)

- $K: L^2(\Omega) \rightarrow L^2(\Omega)$  compact operator  $\implies K^{-1}$  unbounded (ill-posed)

# Simpler case: 1D deconvolution



Original signal  $\tilde{u}: [0, 1] \rightarrow \mathbb{R}$

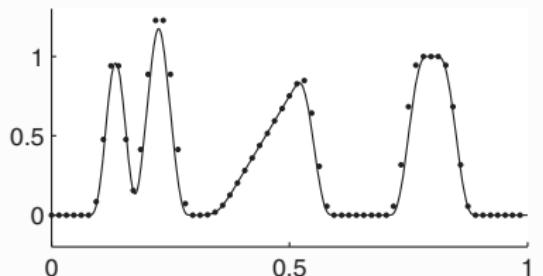


Blurred signal  $f = \psi \star \tilde{u}$

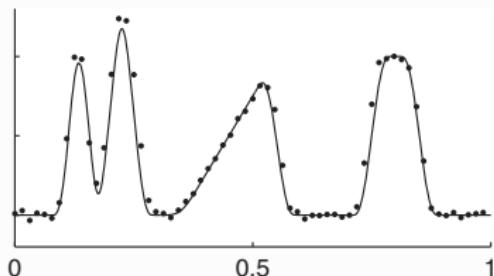
- ▶ Goal: Recover  $\tilde{u}$  from noisy data  $f^\varepsilon = f + \varepsilon$
- ▶ This means solving the 1D-deconvolution problem: Find  $u$  such that

$$\psi \star u = f^\varepsilon$$

# Discretize interval $[0, 1]$ with $n = 64$ points



Discrete  $f$  with  $n = 64$  grid points



Add 1% noise to obtain  $f^\varepsilon \in \mathbb{R}^{64}$

- ▶ The convolution  $\psi \star u$  can be discretized using Riemann sums
- ▶ The discrete inverse problem is therefore: Find  $u \in \mathbb{R}^{64}$  such that

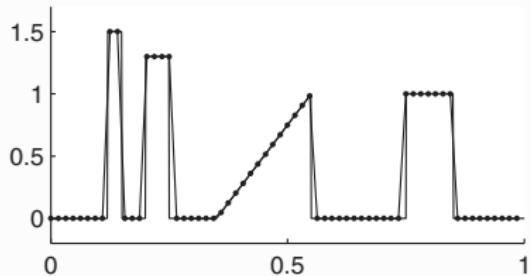
$$Ku = f^\varepsilon, \quad K \in \mathbb{R}^{64 \times 64}$$

# Naive deconvolution

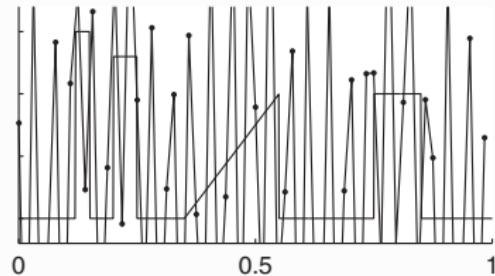
Solve the discrete 1D-deconvolution problem: Find  $u \in \mathbb{R}^{64}$  such that

$$Ku = f^\varepsilon, \quad K \in \mathbb{R}^{64 \times 64}$$

- ▶ The naive solution is  $u = K^{-1}f^\varepsilon$
- ▶ This behaves well when  $\varepsilon = 0$  but is terrible when  $\varepsilon \neq 0$
- ▶ Below the solid line represents the ground truth  $\tilde{u}$
- ▶ We need regularizer which penalizes oscillations



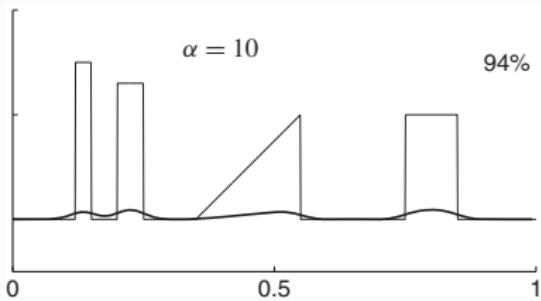
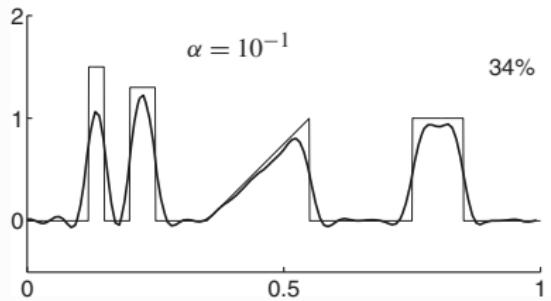
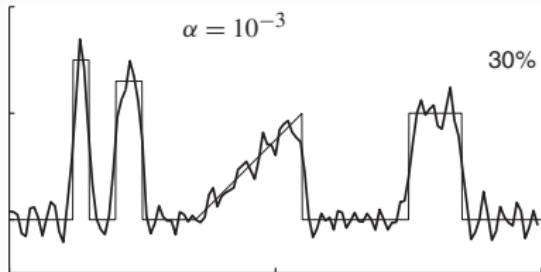
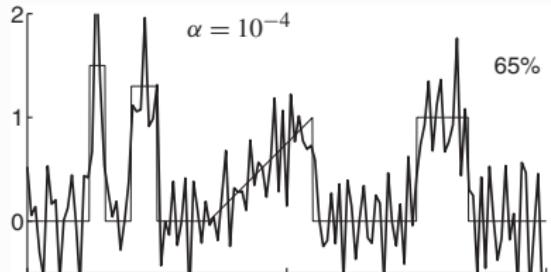
$$u = K^{-1}f$$



$$u = K^{-1}f^\varepsilon$$

Regularize the discrete inverse problem with the  $\ell_2$  norm:

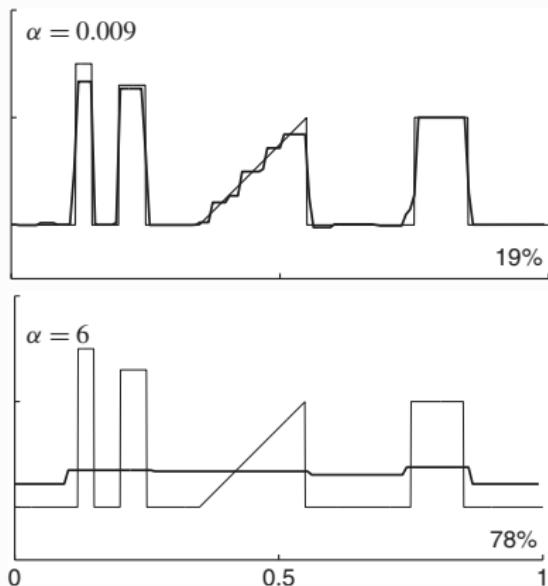
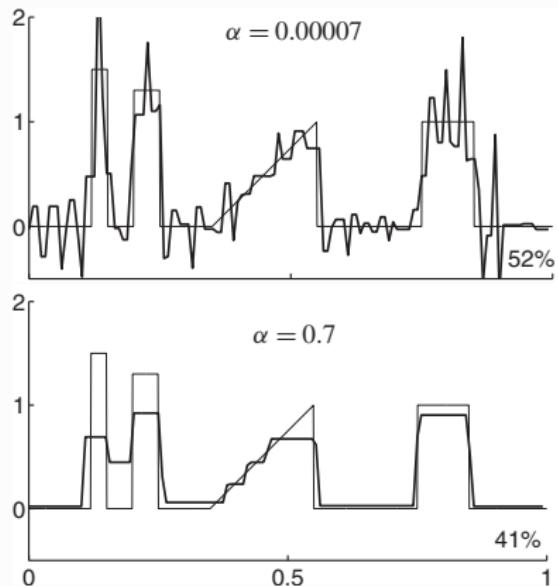
$$\min_{u \in L^2(0,1)} \|Ku - f^\varepsilon\|_{L^2(0,1)}^2 + \alpha \|u'\|_{L^2(0,1)}^2$$



Best is  $\alpha = 10^{-1}$ . Notice the smoothing effect of  $\ell_2$  Smoothness is not always desirable (e.g. if  $u$  is image with sharp edges)

Regularize inverse problem with the Total Variation (BV) semi-norm:

$$\min_{u \in L^1(0,1)} \|Ku - f^\varepsilon\|_{L^2(0,1)}^2 + \alpha \operatorname{TV}(u)$$



$\alpha = 0.7$

41%

0.5

1

78%

0.5

1

Best is  $\alpha = 0.009$ . Notice the sparsifying effect of TV (the jumps)



# Elementary example: Matrix inversion

Given  $f \in \mathbb{R}^m$  and a matrix  $K \in \mathbb{R}^{m \times n}$  we want to find  $u \in \mathbb{R}^n$  such that

$$Ku = f + \varepsilon \quad (\text{P})$$

What could go wrong:

- ①  $m > n \implies \text{Range}(K) \neq \mathbb{R}^m \implies \text{No solution when } f + \varepsilon \notin \text{Range}(K)$
- ②  $m < n \implies \ker(K) \neq \{0\} \implies \text{There are several solutions}$
- ③  $m = n$  and  $K^{-1}$  exists: However condition number  $\kappa = \lambda_1/\lambda_n$  could be large. Then  $K$  is almost singular and

$$\|K^{-1}\varepsilon\| \approx \frac{\|\varepsilon\|}{\lambda_n} \implies \text{Naive reconstruction is dominated by noise}$$

$$\tilde{u} = u + K^{-1}\varepsilon \implies \text{instability}$$

Therefore (P) is in general **ill-posed**



# Least-squares solution

Given  $f \in \mathbb{R}^m$  and a matrix  $K \in \mathbb{R}^{m \times n}$  we want to find  $u \in \mathbb{R}^n$  such that

$$Ku = f \tag{P}$$

- (P) might not have solution. Find approximate solution by **least-squares**

$$\min_{u \in \mathbb{R}^n} \|Ku - f\|_2^2 \tag{P'}$$

with  $\|\cdot\|_2$  the Euclidean norm

- (P') always has the explicit solution (seen by differentiation)

$$\tilde{u} = (K^T K)^{-1} K^T f$$

- **Problem 1:** Solution to (P') **not unique** (if  $K$  is not injective)
- **Problem 2:** Solution might be **instable** (depends on eigenvalues of  $K^T K$ )



# Variational Regularization

Given  $f \in \mathbb{R}^m$  and a matrix  $K \in \mathbb{R}^{m \times n}$  we want to find  $u \in \mathbb{R}^n$  such that

$$Ku = f \tag{P}$$

- ▶ **Question:** Non uniqueness and / or instability. What to do?
- ▶ **Answer:** Replace (P) with the **regularized** least-squares problem

$$\min_{u \in \mathbb{R}^n} \|Ku - f\|_2^2 + \alpha R(u)$$

with  $R: \mathbb{R}^n \rightarrow [0, +\infty]$  **regularizer** and  $\alpha > 0$  to be chosen

- ①  $R$  promotes stability (if chosen properly)
- ②  $R$  selects only some solutions (the ones for which  $R(u)$  is small)



# First Example: $\ell_2$ regularization

Regularize using the  $\ell^2$  norm:

$$\min_{u \in \mathbb{R}^n} \|Ku - f\|_2^2 + \alpha \|u\|_2^2 \quad (\text{P})$$

- ▶ (P) is known as Ridge-regression in Statistics
- ▶ (P) always has the explicit solution (seen by differentiation)

$$\tilde{u} = (K^T K + \alpha I)^{-1} K^T f$$

- ▶ (P) more stable because eigenvalues of  $K^T K + \alpha I$  are away from zero
- ▶  $\ell_2$  norm **shrinks components**  $\implies$  mitigates effects of noise



## Second Example: $\ell_1$ regularization

Regularize using the  $\ell^1$  norm

$$\min_{u \in \mathbb{R}^n} \|Ku - f\|_2^2 + \alpha \|u\|_1 \quad (\text{P})$$

- ▶ (P) is known as LASSO-regression in statistics
- ▶ (P) always admits a solution (no explicit formula available)
- ▶  $\ell_1$  norm automatically **sets some components to zero**  $\leadsto$  **sparsity**

$$\tilde{u} = (0, 0, 0, *, 0, 0, \dots, 0, *, 0, 0, 0, 0, 0)$$

- ▶ Desirable when  $n$  is large (many parameters), as it simplifies the model

---

Models like GPT-5 have 10s of trillions of parameters

# Why does $\ell_1$ set components to zero?

$$\min_{u \in \mathbb{R}^n} \|Ku - f\|_2^2 + \alpha \|u\|_1$$

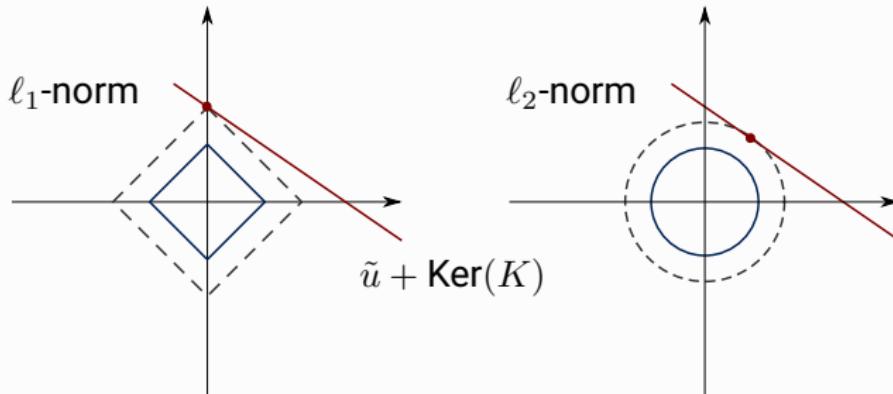
$\Updownarrow$

$$\min_{\|u\|_1 \leq s} \|Ku - f\|_2^2$$

$$\min_{u \in \mathbb{R}^n} \|Ku - f\|_2^2 + \alpha \|u\|_2^2$$

$\Updownarrow$

$$\min_{\|u\|_2 \leq s} \|Ku - f\|_2^2$$



**Extremal points** are different  $\implies \ell_1$  and  $\ell_2$  select different solutions

**Extremal points of regularizer describe features of sparse solutions**

# Example: Portfolio Optimization

**Portfolio:** Vector

$$P = (w_1, \dots, w_d) \quad w_i = \text{capital to invest in asset } i$$

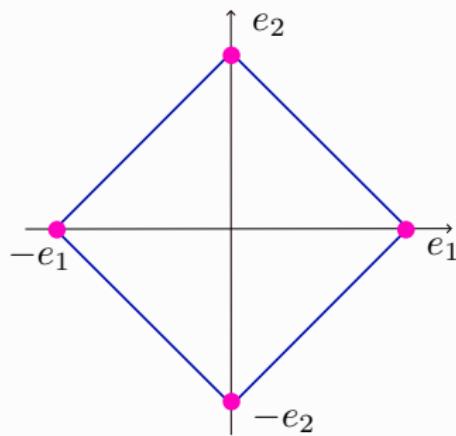
**Sparsity:** Invest in few assets

$$P = (0, 0, \mathbf{w}_i, 0, 0, \dots, 0, 0, \mathbf{w}_d) \implies \text{lower managing fees}$$

**Banach space:**  $X = \mathbb{R}^d$

**Regularizer:**  $\|x\|_1 := \sum_{i=1}^d |x_i|$

$$\text{Ext}(B) = \{\pm e_i\}_{i=1}^d$$





# Extremal Points

$$R(\mu, v) := \int_0^1 \int_{\Omega} |v_t(x)|^2 d\mu_t(x) dt + \int_0^1 \|\mu_t\|_{\mathcal{M}(\Omega)} dt$$

s.t.  $\partial_t \mu_t + \operatorname{div}(v_t \mu_t) = 0$  (CE)

[3] Bredies, Carioni, **Fanzon**, Romero. **Bulletin London Mathematical Society** (2021)

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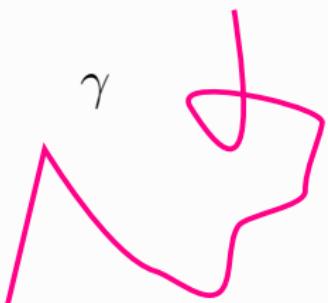
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## Theorem [3]

Let  $B = \{R \leq 1\}$ . Then  $\operatorname{Ext}(B)$  are measures

$t \mapsto \mu_t$  supported on **Sobolev Curves**

$$t \mapsto \mu_t = \delta_{\gamma(t)}, \quad \gamma \in H^1([0, 1]; \mathbb{R}^2)$$



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**Proof Idea:** Probabilistic Superposition Principle

for measure solutions to

$$\partial_t \mu_t + \operatorname{div}(v_t \mu_t) = 0 \quad (= g_t \mu_t )$$

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[3] Bredies, Carioni, **Fanzon**, Romero. **Bulletin London Mathematical Society** (2021)