



An Unsupervised Approach for Artifact Severity Scoring in Multi-Contrast MR Images

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Introduction

- Motivation:**
 - There exists a need for robust, interpretable, and scalable **quality assurance** (QA) in MRI, especially for large, multi-site datasets
 - Challenges with existing methods:**
 - Manual QA is **subjective** and **slow**¹
 - MRIQC² takes **several minutes** to run and struggles with certain modalities
 - Supervised methods **require labels** and struggle to generalize

Our Contribution

- An unsupervised, interpretable framework that uses **contrastive learning** and **simulated artifacts** to assign artifact severity scores to MR images
- Works across **T1-w, T2-w, FLAIR, and PD images** without the need for preprocessing

Methods: Dataset, Model Training, and Model Testing

- Dataset:**
 - 297 **high-quality structural MR volumes** from the TRaditional vs. Early Aggressive Therapy for Multiple Sclerosis (TREAT-MS) pragmatic, clinical trial (NCT03500328)
 - Acquired from 7 different imaging sites and included **T1-w, T2-w, FLAIR, and proton density** images

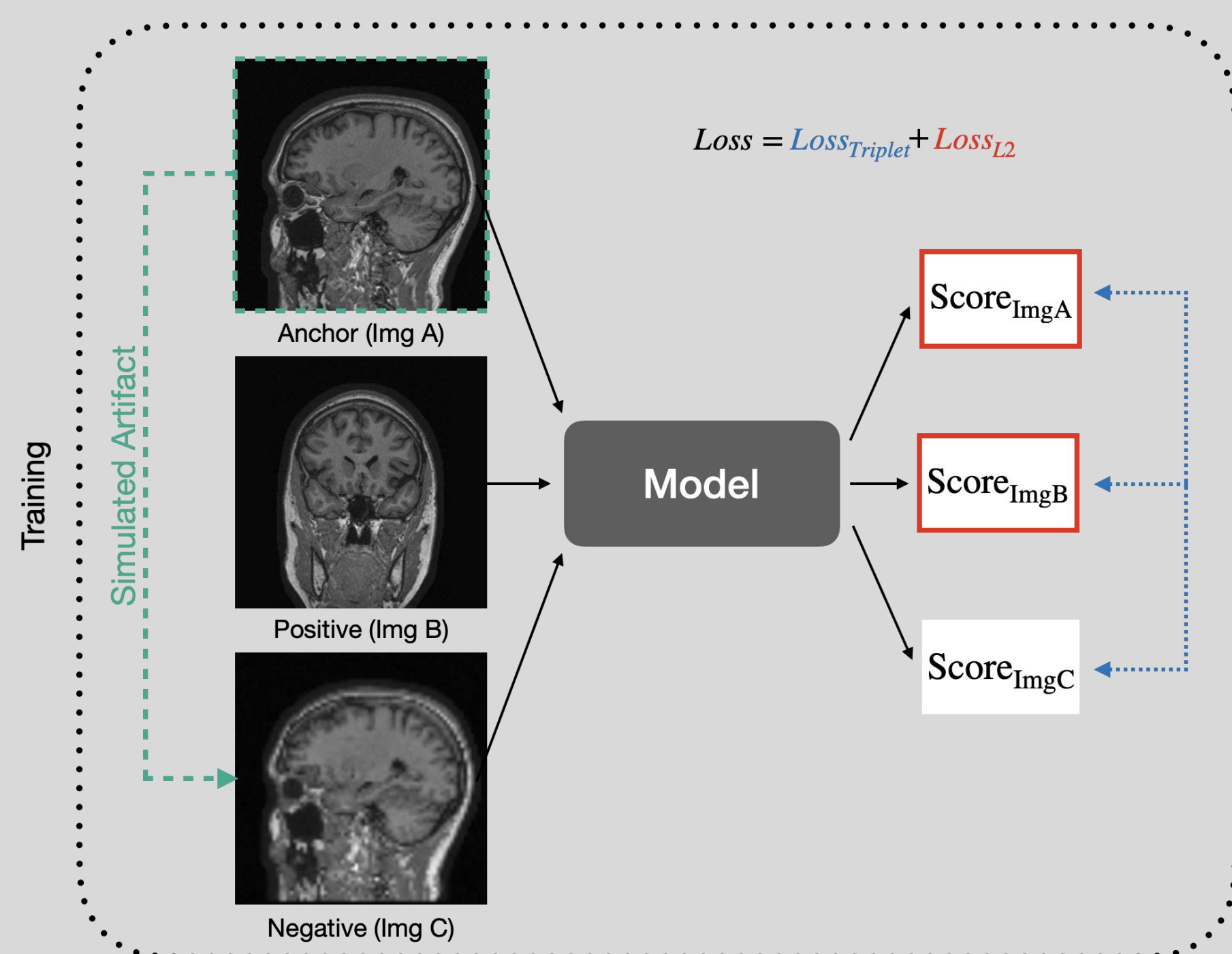


Figure 1: During training, three images are used to calculate the total loss. Img A and Img B are two different, clean image slices, while Img C is Img A with a randomly simulated artifact.

- Model Training:**
 - Input: **2D slices**, which are resized to 224x224
 - Simulated artifacts using the TorchIO library for **random bias, random noise, random anisotropy, and random ghosting**
 - Triplet loss uses the assigned severity score (SS) as the **margin** to adapt based on severity level
 - L2 loss anchors **clean images to low** scores

Table 1: Each artifact and its parameters used in the severity score (SS). The parameters were uniformly sampled in the corresponding range to ensure continuity of the artifact space.

| Artifact | Input | Parameters | Severity Score (SS) |
|------------|-------------------------|--|--|
| Noise | std | $\mathcal{U}[0.005, 0.2]$ | $\frac{\text{std} - 0.005}{0.2 - 0.005}$ |
| Ghosting | num_ghosts intensity | $\mathcal{U}\{2, \dots, 10\}$ $\mathcal{U}\{0.2, 1.5\}$ | $\frac{(\text{intensity} - 0.2) + \frac{\text{num_ghosts}}{10}}{(1.5 - 0.2) + 1}$ |
| Bias Field | coefficients | $\mathcal{U}[0.01, 0.3]$ | $\frac{\text{coefficients} - 0.01}{0.3 - 0.01}$ |
| Anisotropy | scale | $\mathcal{U}[1, 4]$ | $\frac{\text{scale} - 1}{4 - 1}$ |

- Model Testing:**
 - During inference, a **3D volume** can be input as 2D slices
 - Volumetric score is computed from the **average of the middle 60%** of slices

Methods: Simulated Artifacts

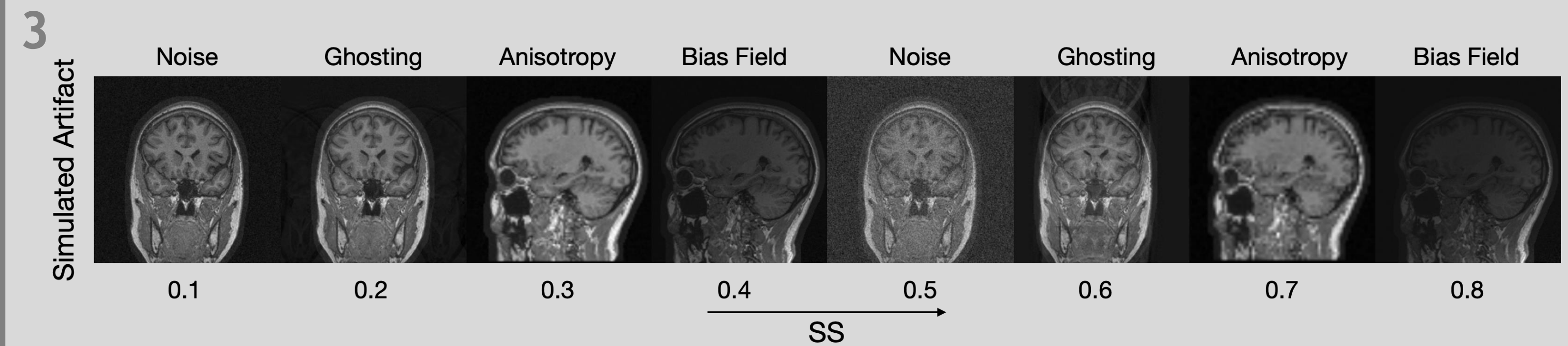


Figure 2: Increasing SS in the range [0, 1] (left to right) of selected simulated artifacts seen during training. During training, each artifact type is simulated on a continuous [0,1] scale.

Results

- Public Dataset (OASIS3, N=20)**
 - MRIQC often **failed**, especially on T2w images
 - Our model: **~1 second per volume** (MRIQC: 7-9 minutes per volume)

Table 2: Simulated artifact type and SS with MRIQC and our model results. We report the Pearson coefficient between the SS and result.

| Artifact Type | SS | MRIQC | | | | Ours↓ |
|----------------|-----|-------------|--------------|-------------|-------------|-------------|
| | | CJ↓ | CNR↑ | EFC↓ | FBER↑ | |
| None | 0.0 | 0.77 ± 0.13 | 1.14 ± 0.25 | 0.49 ± 0.05 | 6962 ± 2097 | 0.17 ± 0.47 |
| Bias | 0.1 | 0.80 ± 0.19 | 1.08 ± 0.27 | 0.51 ± 0.60 | 2367 ± 1572 | 0.01 ± 0.03 |
| Motion | 0.3 | 0.87 ± 0.19 | 1.05 ± 0.27 | 0.51 ± 0.05 | 5501 ± 2010 | 1.74 ± 0.49 |
| Anisotropy | 0.6 | 0.78 ± 0.05 | 1.32 ± 0.23 | 0.52 ± 0.05 | 9876 ± 3326 | 2.32 ± 0.48 |
| Ghosting | 0.8 | 1.03 ± 0.18 | 0.82 ± 0.12 | 0.53 ± 0.06 | 4161 ± 1852 | 2.34 ± 0.60 |
| Noise | 0.9 | — | — | — | — | 3.54 ± 0.06 |
| Pearson | | 0.36 | -0.16 | 0.13 | 0.35 | 0.92 |

Clinical Dataset (TREAT-MS, N=124)

- High-quality images score **near 0**, poor-quality images score **> 1**
- 83% of clinical scans flagged as low quality** (expected due to 2D acquisitions)

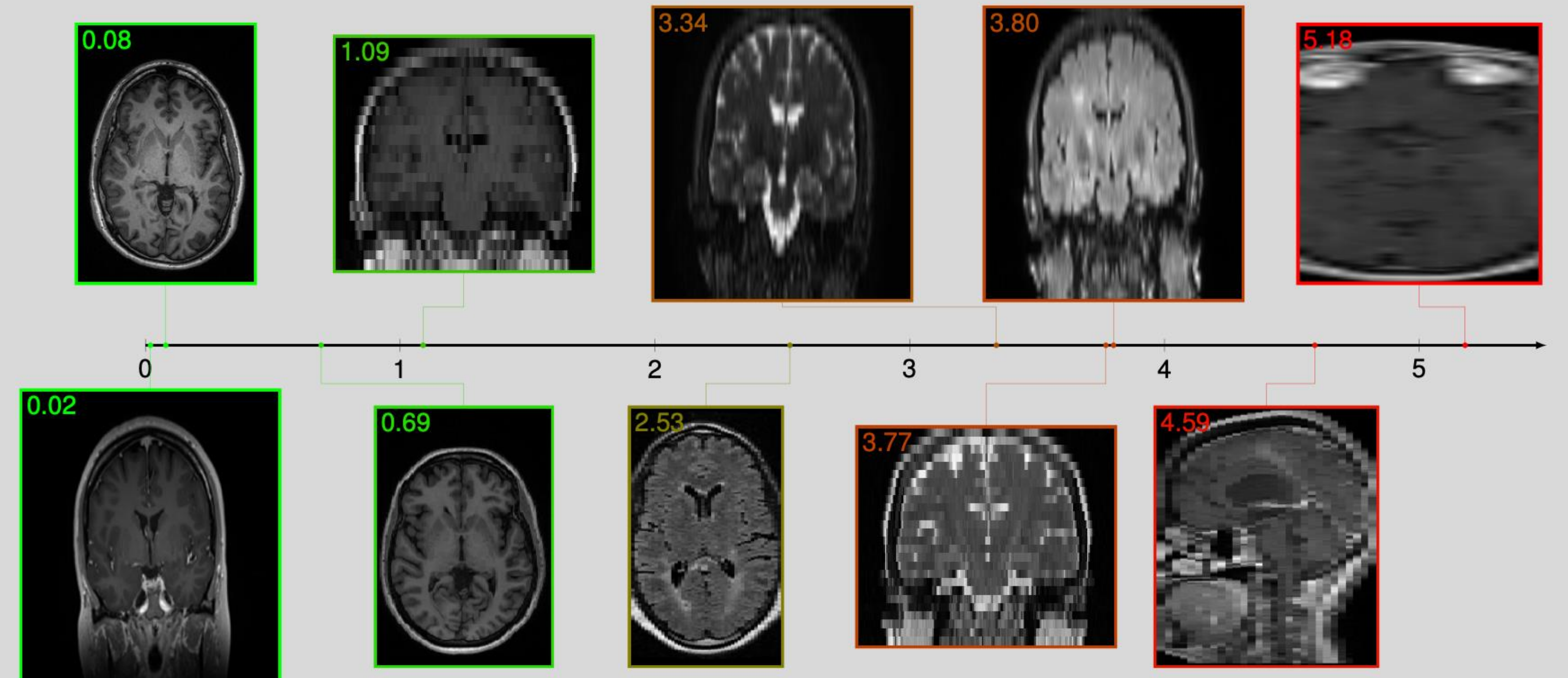


Figure 3: Clinically acquired images from the TREAT-MS dataset with our model scores. Although images are acquired at various sites following a standardized protocol, several low resolution 2D acquisitions are observed.

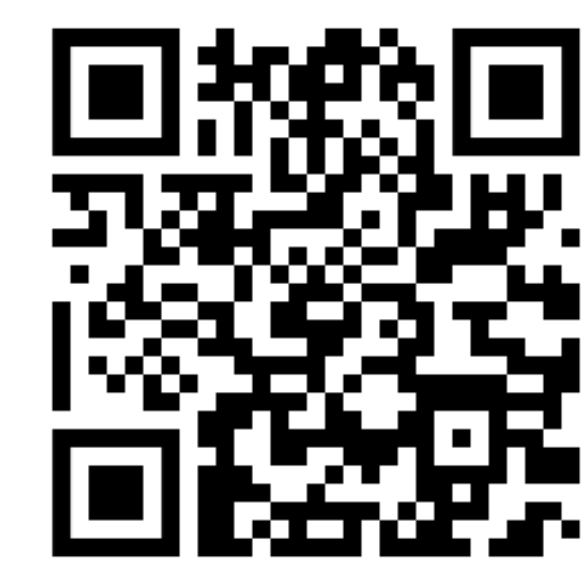
Discussion and Conclusion

- Key Takeaways:**
 - Scalable and **unsupervised** QA model for MR images.
 - Higher **Pearson coefficient** and **faster** runtime than MRIQC
 - Handles diverse contrasts and artifacts **without preprocessing**
 - Threshold of 1 can be **used to separate** acceptable from poor-quality images.
- Future Work:**
 - Simulate **combinations** of artifacts
 - Multi-dimensional score representing the **level of each artifact** type

References

- Alfaro-Almagro, et al. Image processing and quality control for the first 10,000 brain imaging datasets from UK biobank. *NeuroImage*, 166:400-424, 2018.
- Esteban et al. MRIQC: Advancing the automatic prediction of image quality in MRI from unseen sites. *PLOS ONE*, 12(9):1-21, 09 2017.

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