

A parcellation scheme based on von Mises-Fisher distributions and Markov random fields for segmenting brain regions using resting-state fMRI

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29 April, 2022

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- 3 Results and Inferences

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- Introducing a prior on the number of labels, which helps in **uncovering the number of clusters automatically from the data**
- Modeling **spatial correlations in rs-fMRI data** to produce a parcellation even for non-contiguous regions of human brain

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- The **Positron Emission Tomography** based **invasive Cytoarchitectonic Mappings** in postmortem brains is a solution

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- Anatomical parcellations in these atlases are based on postmortem brains of the elderly, and are **less useful** for examining individual differences in the functional organization of the normal healthy adult brain
- Parcellation of the cortex into subnetworks based on resting-state fMRI data opens up the possibility of developing **novel functional atlases based entirely on cortical function**

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- Currently used methods include **hierarchical clustering**, **Gaussian mixture modeling**, **graph theory based spectral clustering**, **computer vision based edge detection** and the commonly used **K-means based clustering methods**

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- With the exception of edge detection methods all of these methods **require the specification of number of clusters**
- This is a problem because the choice of number of clusters **can significantly influence functional modules uncovered by each method**
- A second major limitation of current methods used to parcellate the brain is that they **do not exploit spatial correlations** that are inherent in rs-fMRI data

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Von Mises-Fisher Distribution

Probability Density Function

The probability density function of the von Mises–Fisher distribution for the random p -dimensional unit vector \mathbf{x} is given by $f_p(\mathbf{x}; \mu, \kappa) = C_p(\kappa) e^{\kappa \mu^\top \mathbf{x}}$, where $\kappa \geq 0$, $\|\mu\| = 1$ and the normalization constant $C_p(\kappa) = \frac{\kappa^{\frac{p}{2}-1}}{(2\pi)^{\frac{p}{2}} I_{\frac{p}{2}-1}(\kappa)}$, where I_ν denotes the modified Bessel function of the first kind at order ν .

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Relation to Isotropic Covariance MVG

Starting from a normal distribution, with isotropic covariance, $\kappa^{-1}I$, and a mean μ of length $r > 0$ that has the density $G_p(\mathbf{x}; \mu, \kappa) = (\sqrt{\frac{\kappa}{2\pi}})^p e^{-\kappa \frac{(\mathbf{x}-\mu)^\top (\mathbf{x}-\mu)}{2}}$ the Von Mises-Fisher distribution $f_p(\mathbf{x}; r^{-1}\mu, r\kappa)$ is obtained by conditioning on $\|\mathbf{x}\| = 1$.

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- μ is the mean parameter and κ is the concentration parameter.

Algorithm

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- We will iterate over these steps until the energy function converges.

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- Let each T dimensional normalized voxel time series y_i given its cluster label $X_i = l$ follow T -variate VMF distribution given by
$$p(y_i | X_i = l, \mu_l, \kappa_l) = C(\kappa_l) e^{\kappa_l \mu_l^\top y_i}$$

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- We model the prior distribution of unknown cluster labels X as discrete MRF given by $P(X) = \frac{1}{Z} e^{-(U_s(X) + U_l(X))}$, where $U_s(X)$ is the energy function which imposes spatial regularization and $U_l(X)$ is the label cost

Notation for this problem

- $U_s(X) = \sum_{i=1}^M \sum_{j \in N_i} V(X_i, X_j)$ where the potts potential function is defined as $V(X_i, X_j) = \beta_s(1 - \delta(X_i - X_j))$, where $\delta(z) = 1$ if $z = 0$ and $\delta(z) = 0$ otherwise

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- The posterior distribution of X given the data Y and model parameters

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- Henceforth, we intend to maximise this posterior probability over the labels and parameters. This is same as minimising the total energy function $U = U_s(X) + U_l(X) + U_D(Y)$. Smell of a graph cut?

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- $\hat{X} = \arg \min_X U$

VMF Parameter Estimate

To get the optimal parameters, we maximise the likelihood. We get

$$\bar{r}_l = \frac{\sum_{\{i|X(i)=l\}} y_i}{N}, \hat{\mu}_l = \frac{\bar{r}_l}{\|\bar{r}\|} \text{ and } \hat{\kappa}_l = \frac{\bar{r}_l T - \bar{r}_l^3}{1 - \bar{r}_l^2}$$

Parameters and Labels Update

VMF Parameter Estimate

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α Expansion Algorithm

1. Start with an arbitrary labelling \mathbf{f}
2. Set **success** := 0
3. For each label $\alpha \in \mathcal{L}$
 - 3.1 Find $\hat{\mathbf{f}} = \arg \min \mathbf{E}(\mathbf{f}')$ among \mathbf{f}' within one α expansion of α
 - 3.2 If $\mathbf{E}(\hat{\mathbf{f}}) < \mathbf{E}(\mathbf{f})$, set $\mathbf{f} = \hat{\mathbf{f}}$ and **success**:=1
4. If **success** = 1 goto 2
5. Return \mathbf{f}

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 - 6 Low correlation within cluster ($\rho_{in} = 0.3$) and across the clusters ($\rho_{ac} = 0.2$)

Results on Simulated Data

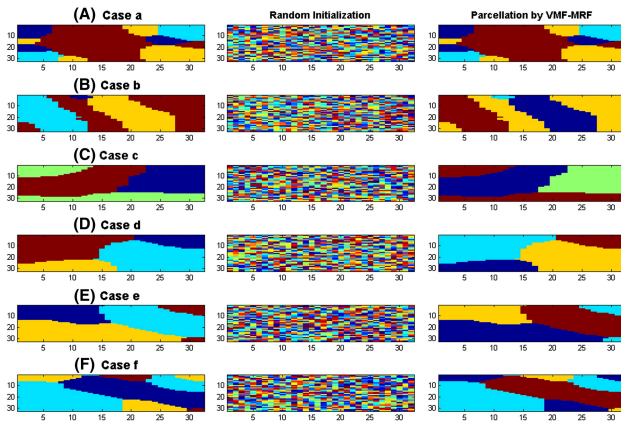


Figure: All 6 Simulated data samples

Iterations in case 4

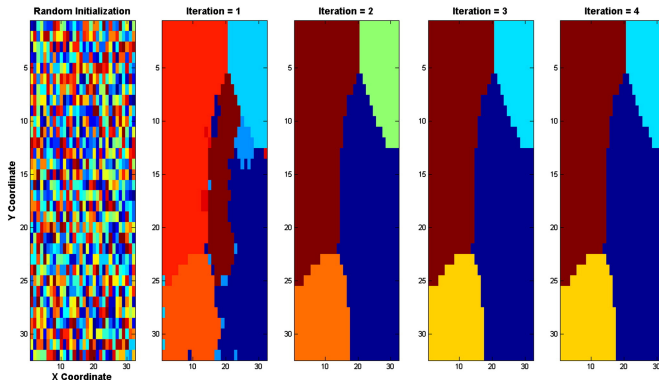


Figure: Clusters estimated by this algorithm in case 4

Clustering Human Brain RS-fMRI Data

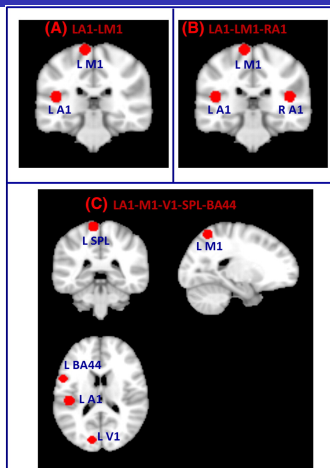


Figure: Clusters constructed from fMRI data(3 Input Data Sets)

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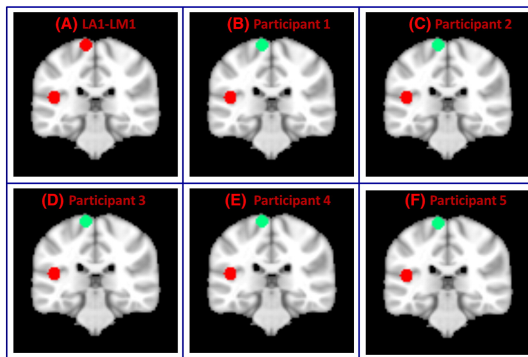


Figure: Left auditory and motor cortices (LA1-LM1)

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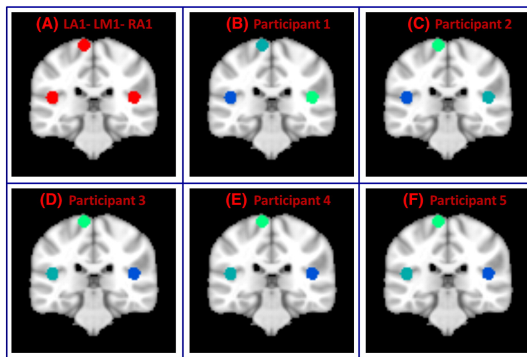


Figure: Left auditory, motor and right auditory cortices(LA1-LM1-RA1)

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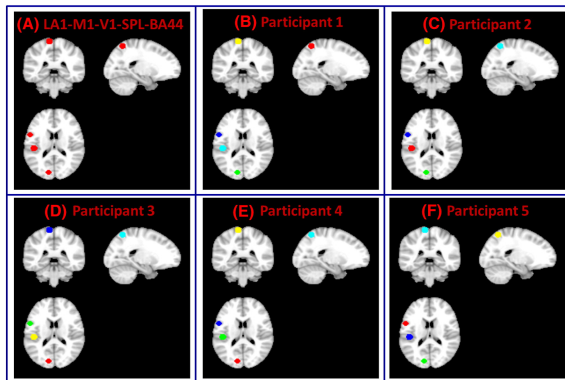


Figure: Left auditory, motor, and visual cortices, the superior parietal lobule (SPL) and inferior frontal gyrus (Brodmann Area BA 44) (LA1-M1-V1-SPL-BA44)

- Cases 1, 3 and 5 involve high spatial contrast ($\rho_{in} > \rho_{ac}$) whereas cases 2, 4 and 6 involve low spatial contrast ($\rho_{in} \approx \rho_{ac}$) and should be more difficult to parcellate. We evaluated the robustness of our method using these test cases and as visible the algorithm correctly parcellated the data sets.

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- It predicted the number of cluster labels and also parcellated spatially contiguous as well as non-contiguous regions appropriately (even in case 6)
- The usage of α expansion significantly improved the running time over ICM or simulated annealing based approaches. It does so by allowing updates on several voxels simultaneously instead of just one as in other cases.

- Cases 1, 3 and 5 involve high spatial contrast ($\rho_{in} > \rho_{ac}$) whereas cases 2, 4 and 6 involve low spatial contrast ($\rho_{in} \approx \rho_{ac}$) and should be more difficult to parcellate. We evaluated the robustness of our method using these test cases and as visible the algorithm correctly parcellated the data sets.
- It predicted the number of cluster labels and also parcellated spatially contiguous as well as non-contiguous regions appropriately (even in case 6)
- The usage of α expansion significantly improved the running time over ICM or simulated annealing based approaches. It does so by allowing updates on several voxels simultaneously instead of just one as in other cases.
- Now, since this approach worked for cases where the ground truth was already known (as depicted in the above results), we can run this algorithm to develop finer insights into functional brain segmentation

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- We expect the consensus matrix to average out the opinions of all the initializations for all voxel pairs and hence be a bimodal distribution with modes at 0 and 1.
- We could also generate updates for β_s and β_l , which may be done by several methods such as EM optimization with priors on β_s and β_l having latent variables.



- For the research paper click [here](#)
- For α expansion click [here](#)
- For Von Mises-Fisher Distribution click [here](#)

Thanks for your attention! Any questions?

Hope you slept comfortably!