T₂ Shuffling - Dynamic MRI Dimensionality Reduction

Siddharth Iyer, Jonathan I. Tamir, Michael Lustig

Department of Electrical Engineering and Computer Sciences, University of California at Berkeley, Berkeley, CA

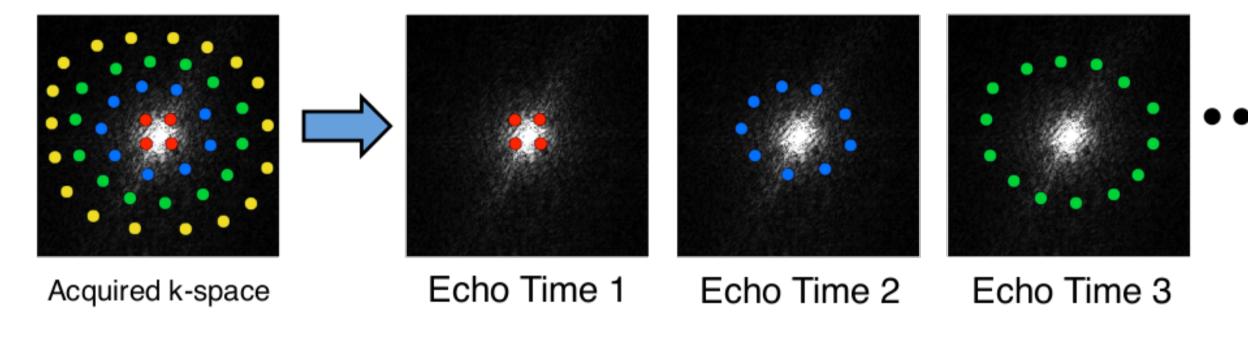


Introduction

- MRI is a safe and powerful tool that can be used to image both anatomy and function.
- Acquiring 3D MRI over time has several clinical applications:
- Reduce image blur from conventional 3D acquisition.
- Visualize signal behavior over time.
- Quantify tissue parameters in anatomy.
- We aim to find a robust and low-dimensional representation of the dynamic images.

Motivation

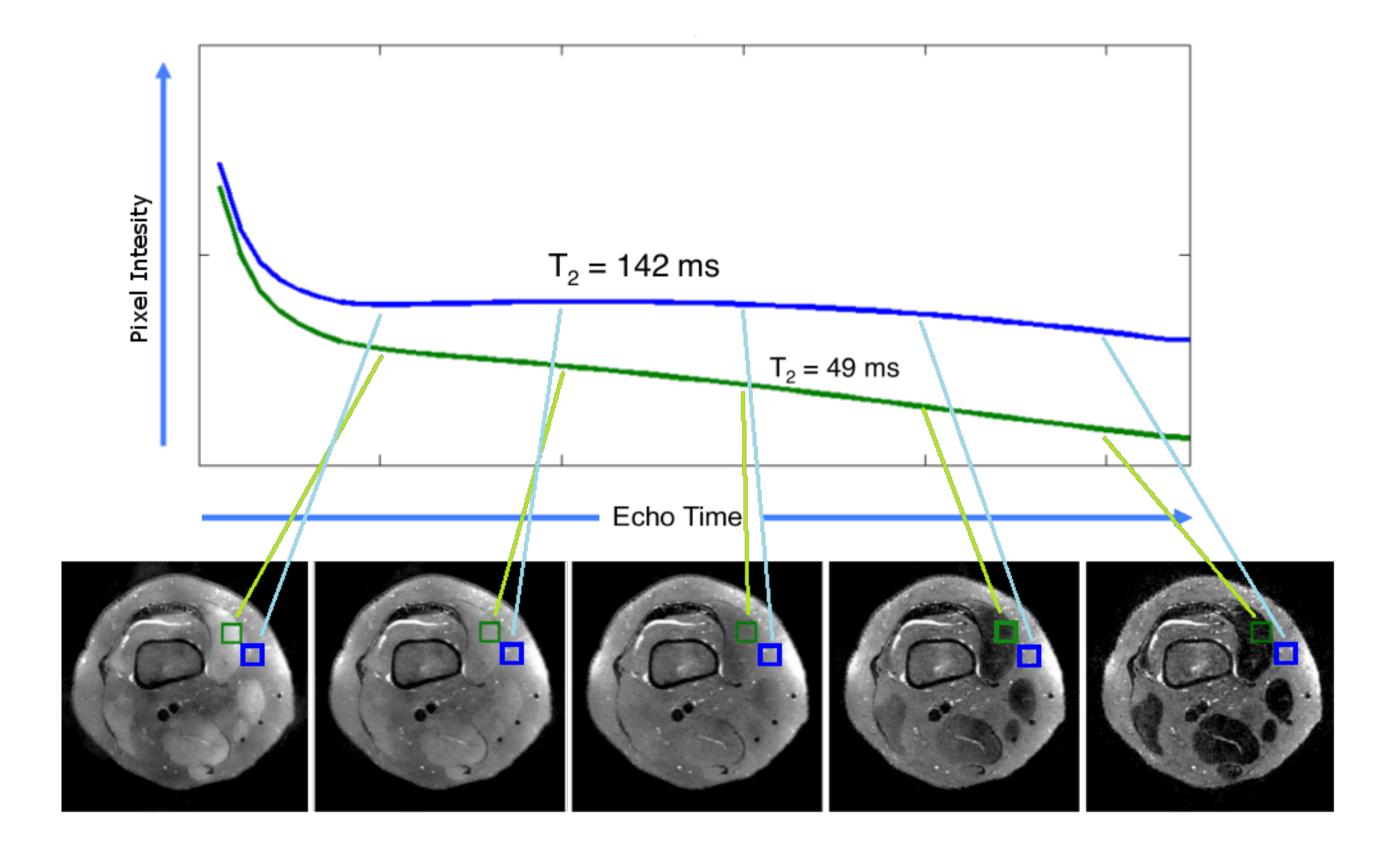
- The image's Fourier transform (called k-space) is sampled over time.
- The samples are grouped into time-consistent k-space bins.



■ Goal: Clinically feasible scan times by reducing dimensionality with low model error.

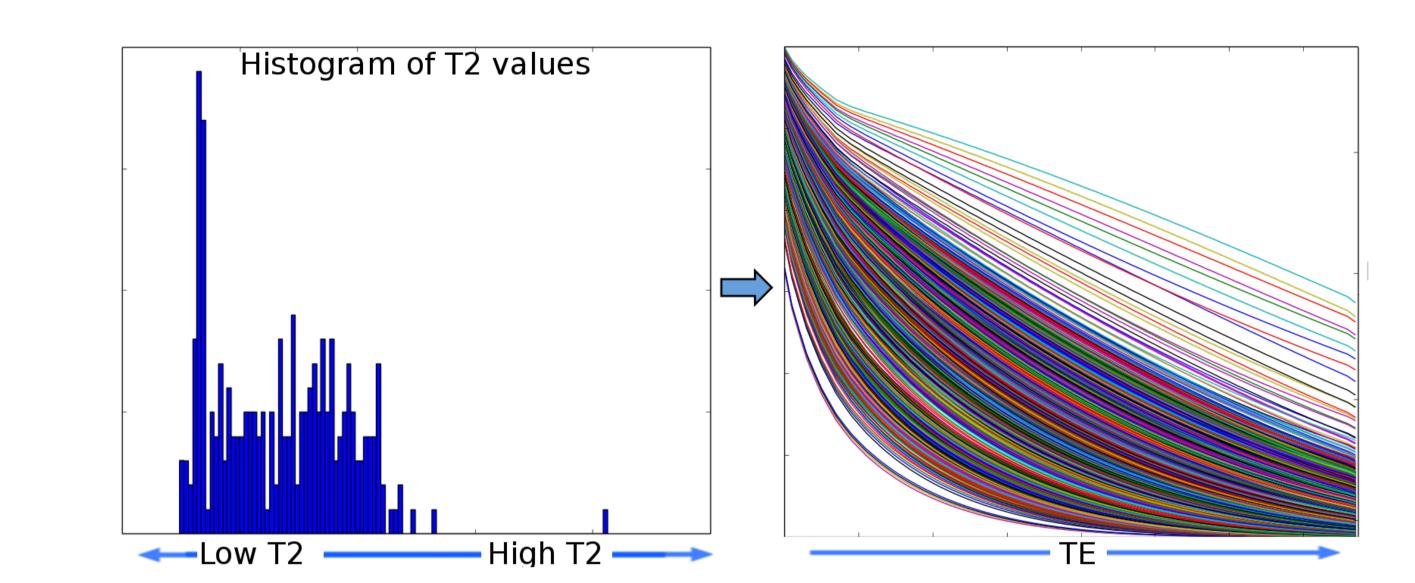
Background

Signal evolution of pixel intensity over time parametrized by tissue T_2 relaxation.



Signals evolutions are correlated \implies data captured by a low-dimensional subspace.

- In Estimate T_2 distribution from tissue in anatomy of interest.
- Form matrix X with signals as columns arranged in increasing order of ℓ_2 norm.

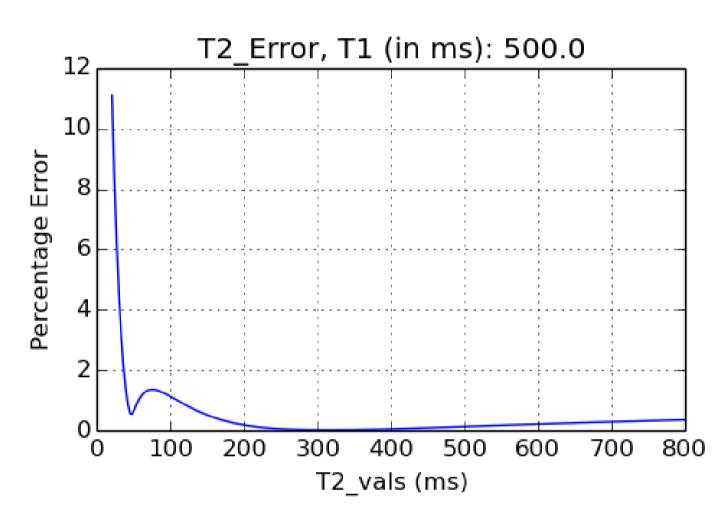


Methods and Results

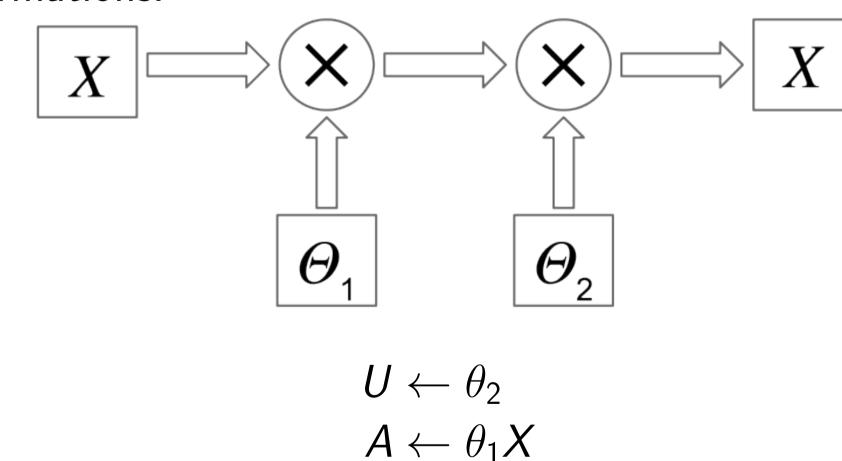
Principal Component Analysis: Project X onto first 3 principal components, U. This solves:

$$\min_{U,A} ||X - UA||_F^2$$

Estimated matrix X' = UA. Normalized model error of X'_i :

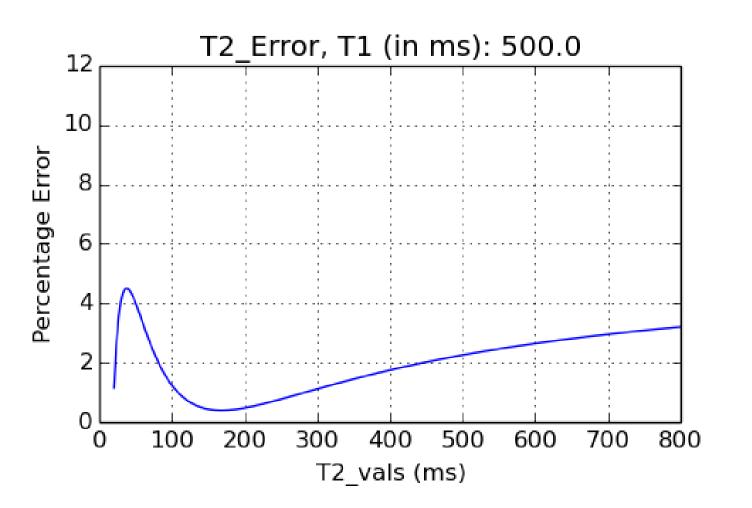


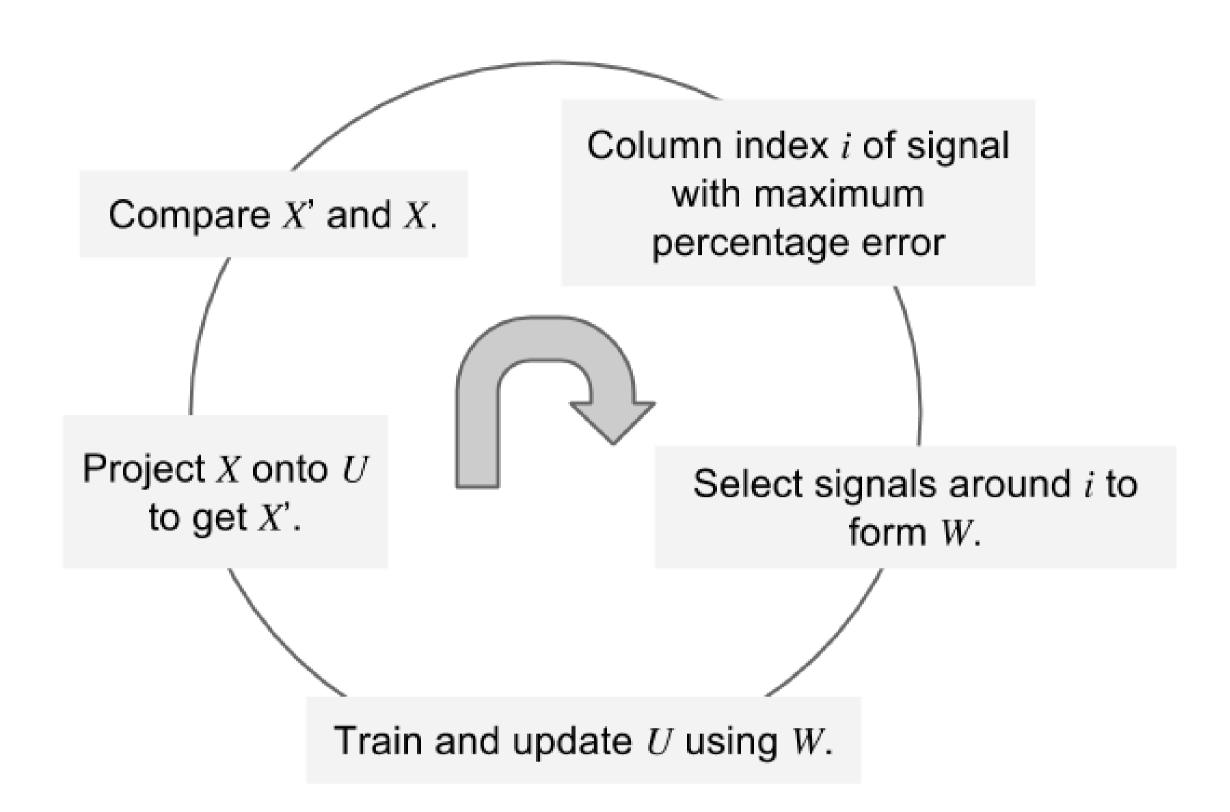
■ Multilayer Linear Regressor: Inspired by Neural Networks, this only uses linear transformations.



This framework is used to solve:

$$\min_{U,A} \max_{i} ||X_i - Ua_i||_2^2$$





Results

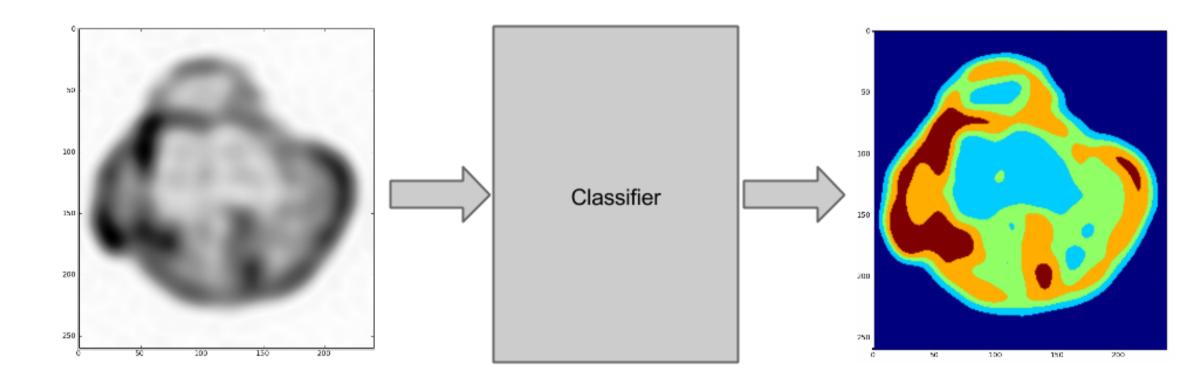
	PCA	MLR
Global Error	0.33%	2.46%
Maximal Error	11.1%	4.50%

Discussion and Conclusion

- Our flexible framework enables the evaluation of different cost functions.
- We produce a low-dimensional representation with lower maximal error at a small cost of global error.

Future Work

 $\blacksquare T_2$ mapping and classification: Classifying T_2 values from signal evolutions.



References

- [1] Tamir JI, Lai P, Uecker M, Lustig M. Reduced blurring in 3D fast spin echo through joint temporal espirit reconstruction. Proc. Intl. Soc. Mag. Reson. Med. 22 2014; p. 0616.
- [2] Busse RF, Hariharan H, Vu A, Brittain JH. Fast spin echo sequences with very long echo trains: design of variable refocusing flip angle schedules and generation of clinical t2 contrast. Magn Reson Med 2006; 55:10307.

Acknowledgements

I would like to thank Jonathan Tamir for allowing me to work with him on his project, Prof. Michael Lustig for letting me be a part of his research group and all the MikGroup members for making me feel welcome.

