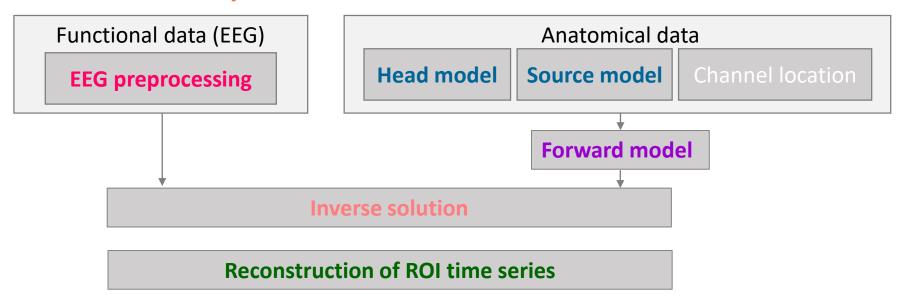
### **Outline**

EEG preprocessing MRI preprocessing Inverse solution ROI time courses

## **Tutorial 3 – from scalp to sources**



## **EEG** preprocessing

Data import, data filtering, bad channel identification, artefact removal and rejection

## **MRI** preprocessing

MRI segmentation for head model computation and grid definition for source model computation

## Solution of the inverse problem

Leadfield matrix extraction, spatial filter estimation

#### Reconstruction of ROI time series

Parcellation selection, dimensionality reduction from sources to ROIs

## EEG – first steps/ data import and filtering

## Import the data

ft\_preprocessing(cfg)

- BDF data are the voltages between each electrode and CMS (50 Hz, ADC noise)
  - → rereference the data to A1 (Cz) to remove CMS contribution

## Downsample

Outline

**EEG** preprocessing

MRI preprocessing

Inverse solution

ROI time courses

• To 250 Hz, reduce computational load

ft resampledata(cfg,data)

## High-pass filter

Above 1 Hz; eye-blinks are identified later by ICA

ft\_preprocessing(cfg)

## Segment the data

- Read event definition from sub-01\_task-faces\_events.tsv (onset + value)
- Identify trials corresponding to FACES (value=1) and SCRAMBLE (value=0)
  - → Define epoch length ([prestim poststim])
- Actually segment continuous data

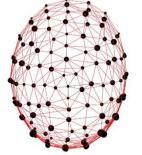
ft read event(filename)

ft\_trialfun\_gen(cfg)

ft redefinetrial(cfg,data)

## <u>Define neighbouring electrodes</u>

Needed for the bad channel interpolation



ft prepare neighbours(cfg,data)

## **EEG** – bad channels

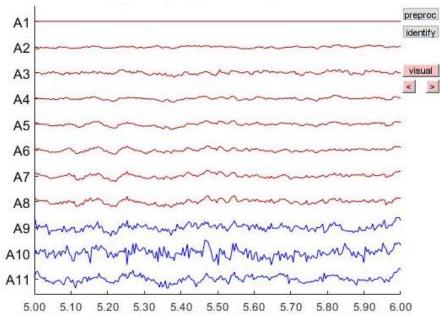
## What they are

Channels with low SNR in general (due for example to high impedance...)

## Outline **EEG preprocessing**MRI preprocessing Inverse solution ROI time courses

## How to identify them

- Channels with low correlation with their neighbours
- Channels with SD very different from that of the others
- Visually



## Read bad channels

Channels are labelled as 'bad' in sub-01\_task-faces\_channels.tsv

## Only keep the good channels

ft selectdata(cfg,data)

## **EEG – ICA for artefact removal**

### What is it

- Separates source signals from mixed signals (cocktail party problem)
- Several algorithm exists: FastICA, Infomax (used here)
- Needs to be done after bad channels removal!

```
cfg = [];
cfg.method = 'runica';
cfg.channel = {'all' '-A1'};
cfg.updatesens = 'no';
ICs = ft_componentanalysis(cfg, data);
```

## Outline **EEG preprocessing**MRI preprocessing Inverse solution ROI time courses

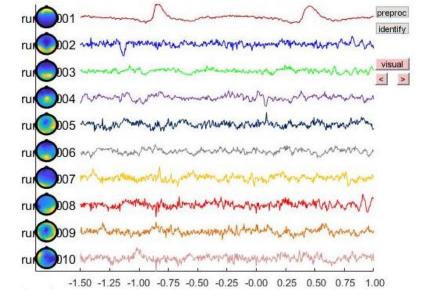
### What it yields

Components that are non-Gaussian and statistically independent from each other

## Select the ICs that capture artefacts

- Eye-blinks
- Muscle twitches

```
cfg = [];
cfg.layout = layout;
cfg.viewmode = 'component';
cfg.continuous='no';
cfg.component = 1:10;
cfg.allowoverlap='yes';
ft_databrowser(cfg, ICs)
```



ft\_rejectcomponent(cfg, ICs, data)

## Finally remove the components

Backprojects the components and substracts them from the data

## **EEG** – final steps

## **Interpolate bad channels**

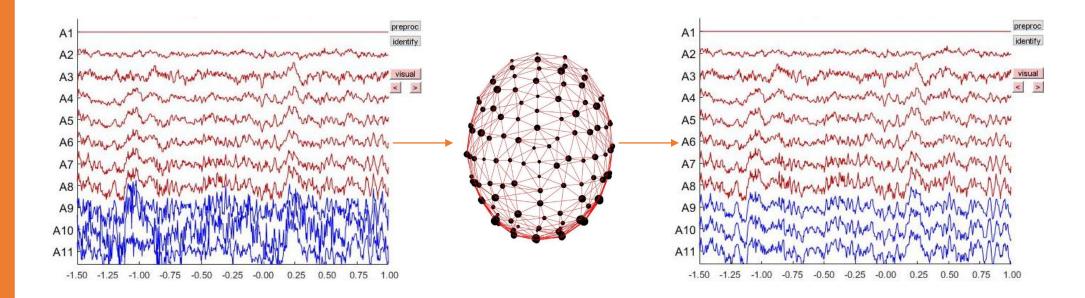
ft\_channelrepair(cfg,data)

Replace the bad channels with the spherical interpolation of the neighbours

Outline **EEG preprocessing**MRI preprocessing

Inverse solution

ROI time courses



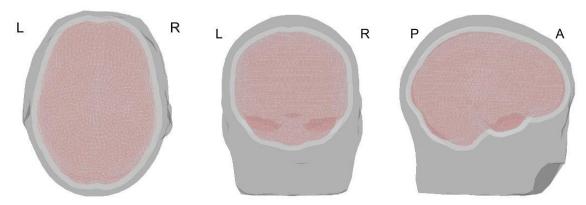
## Average re-reference

Needed for the source localization

## MRI - head model

## What is it

- Model that describes the electrical properties of the head
- Necessary to solve the forward model



Outline
EEG preprocessing
MRI preprocessing
Inverse solution
ROI time courses

## How to estimate it

MRI import

ft\_read\_mri(mri\_filename)

 MRI segmentation to extract surfaces of skin, skull and brain (nested and closed layers that correspond to the boundaries separating these tissues)

ft volumesegment(cfg, mri)

Create these surfaces using a triangular mesh (required for BEM method)

ft\_prepare\_mesh(cfg, segmentedmri)

 Boundary element method (BEM): assign a conductivity to each layer/surface ft\_prepare\_headmodel(cfg, mesh)

## Outline EEG preprocessing MRI preprocessing Inverse solution ROI time courses

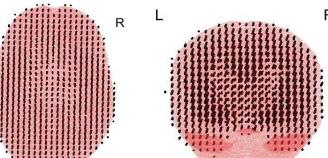
## MRI - source model

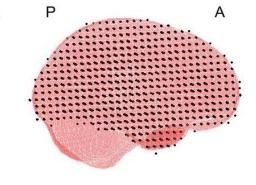
### What is it

- Model that describes the position of the current dipoles
- Dipoles are placed in the grey matter (not in the basal ganglia)

Dipoles have not a fix orientation (1 point source = 3 dipoles, one for each axis)

Necessary to solve the forward model





ft\_read\_mri(mri\_filename)

## How to estimate it

- Import atlas.nii and GM.nii (cmp output)
- Remove basal ganglia ROI from GM
- Coregister (linearly) with template to have a correct grid orientation
- Create the source model using a 6 mm-resolution grid of unfixed dipoles

```
mask=ismember(atlas.anatomy, ROI2remove);
GM.anatomy(mask)=0;
```

```
cfg=[];
cfg.resolution=6;
cfg.unit='mm';
cfg.tight='yes';
cfg.mri=realign_reslice_GM;
ft_prepare_sourcemodel(cfg)
```

## Outline EEG preprocessing MRI preprocessing Inverse solution ROI time courses

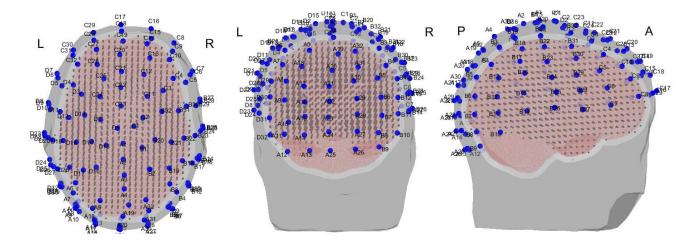
## Solution of the inverse problem-leadfield matrix extraction

## What is it

• Matrix (A) that describes the contribution of the source activity s(t) to each scalp electrode, so that the ECDM model describing the EEG scalp signals x(t) holds true:

$$x(t) = A * s(t) + n(t)$$

- For each source, the leadfield matrix (X\*3) represents the field distribution (the potential) across all X sensors due to a unitary current dipole in its x,y,z-orientations
- Requires (head model) + (source model) + (sensors location)



## How to estimate it

```
cfg = [];
cfg.elec = data.elec;
cfg.sourcemodel = sourcemodel;
cfg.headmodel = headmodel;
Leadfield = ft_prepare_leadfield(cfg);
```

# Outline EEG preprocessing MRI preprocessing Inverse solution ROI time courses

## Solution of the inverse problem – spatial filters estimation

### What is it

• The spatial filers W are spatial maps —one per source dipole component and one per source position—so that the following holds true

$$s(t) = W * x(t)$$

- Obtained with 'imaging' approach (i.e. by inversion of the Equivalent Current Dipole model (ECDM): MNE, wMNE) or with a 'scanning' approach (beamformer)
- The ECDM is ill-posed (S>>X)

## How to estimate it

weighted-minimum norm estimate

 $W = RA^{T}(ARA^{T} + lambdaC)^{-1}$ 

• Estimate covariance of the data C from baseline (prestim)

```
cfg = [];
cfg.covariance = 'yes';
cfg.covariancewindow = [-.1 0];
data = ft_timelockanalysis(cfg, data);
```

Estimate the spatial filters W

```
spatial_filters = ft_inverse_mne(leadfield, [], [], [], ...
    'noisecov', data.cov, 'keepfilter', 'yes', 'prewhiten',...
    'yes','scalesourcecov', 'yes','lambda', .05);
```

## Outline EEG preprocessing MRI preprocessing Inverse solution

**ROI time courses** 

## **ROI** time courses

### What is it

- For each ROI, 'summarise' the 3d-time series of the sources belonging to that ROI in a single time course
- Need (atlas from cmp) + (spatial filters) + (clean EEG data)

## How to estimate it

- Import atlas.nii and set the basal ganglia ROI to zero
- Assign ROI label to each source point (for each source point, find the 26 closest voxels around each it and assign the label of the most present tissue around the source point)
- Concatenate time courses
- For each ROI, use Singular Value Decomposition (SVD) to go from many sources → to one time-course
  - Concatenate the spatial filters of the given ROI
  - Apply the inverse transformation
  - Get the first left singular vector
- Segment the ROI time courses in the original epochs

```
ft_read_mri(mri_filename)

mask=ismember(atlas.anatomy,ROI2remove);
atlas.anatomy(mask) = 0;

assigned_label2source_points(sourcemodel, nifti_atlas, tbl_idx2label)
```

time courses = cat(2, data.trial(:));

```
for ROI_id = 1:n_ROIs
    curr_ROI_bln = strcmp(src_label, ROIs_lbl{ROI_id});
    curr_filters = filters(curr_ROI_bln);
    curr_filters = cat(1,curr_filters{:});

[ROI_traces(ROI_id,:),S,V] = svds(ESI_tmp,1);
end
```