Transducers & Instrumentation

Module 05 - 02

Measuring Pressure, Flow, and Volume

Flow rate

- Measured as volume flow rate → Volume of substances that crosses an area of cross-section in unit time. (Unit: m^3/s)

- Mass flow rate → Mass that crosses a surface in unit time. (Unit: Kg/s)

- Blood flow is an important physiological parameter of interest.

- Inspiration and expiration rates.
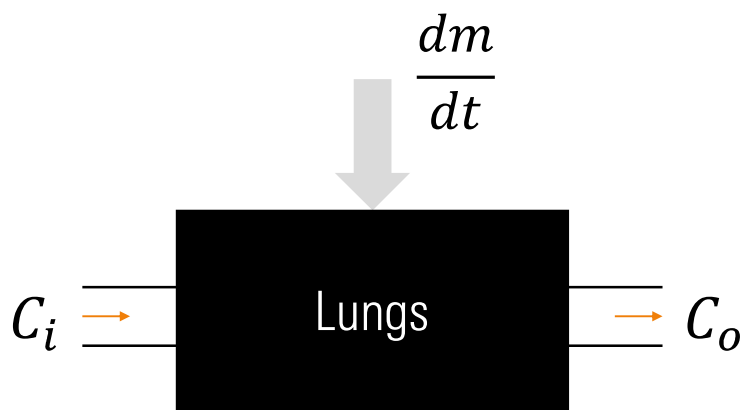
Cardiac Output (CO)

- Amount of blood pumped by the ventricles.

$$CO = SV \times HR$$

- SR: Stroke Volume – Volume of pumped out by the single contraction of the ventricles.
- HR: Heart Rate – Number of heart beats per minute.
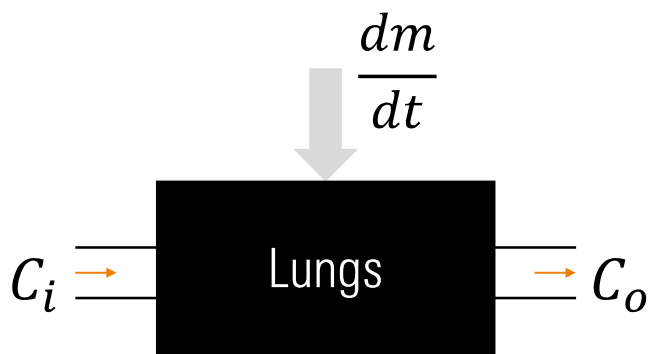- CO is an important parameter of ventricular function.

Fick's method

- Proposed by Adolf Fick in 1870.

$$\frac{dm}{dt}$$

$$CO = \frac{\frac{dm}{dt}}{C_o - C_i}$$

Fick's method

$$\frac{dm}{dt}$$

$$C_i \rightarrow \boxed{\text{Lungs}} \rightarrow C_o$$

$$CO = \frac{\dfrac{dm}{dt}}{C_o - C_i}$$

Inspired oxygen = 210 mL/L
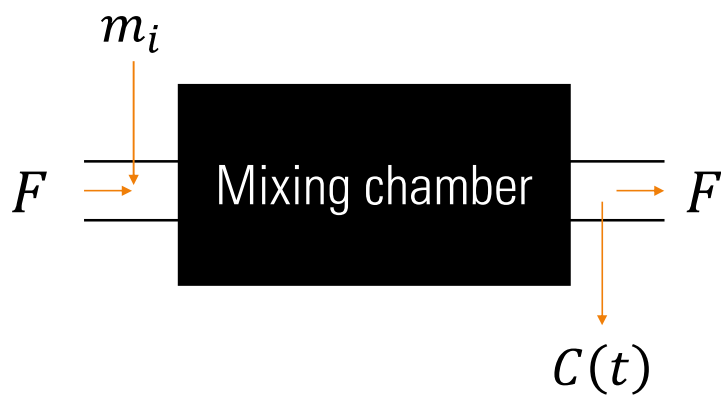Expired oxygen = 160 mL/L
Total volume = 26L
Duration = 3min
Arterial oxygen concentration = 195 mL/L
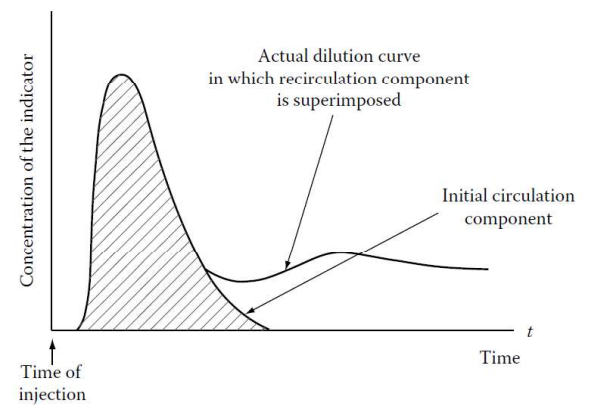Venous oxygen concentration = 132 mL/L

What is the cardiac output?

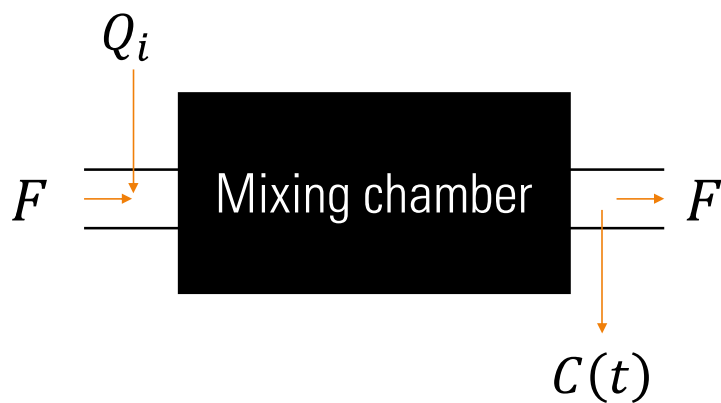# Indicator dilution method (Stewart-Hamilton Method)

m_i

Mixing chamber

F → → F

$C(t)$

$$CO = \frac{m_i}{\int C(t)dt}$$

- Sudden injection of indicator compound.

Concentration of the indicator

Actual dilution curve
in which recirculation component
is superimposed

Initial circulation
component

t

Time

Time of
injection

Thermodilution method

$$\rho_i C_i V_i [T_b(0) - T_i] = \rho_b C_b \int_0^\infty [T_b(t) - T_b(0)] \, F dt$$
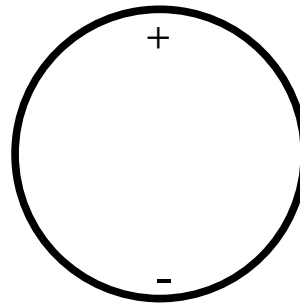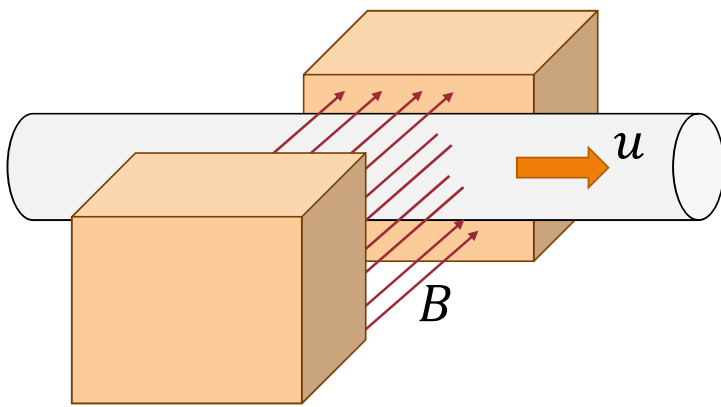
Q_i

F → Mixing chamber → F

$C(t)$

$$F = \frac{\rho_i C_i V_i [T_b(0) - T_i]}{\rho_b C_b \int_0^\infty [T_b(t) - T_b(0)] \, dt}$$

Electromagnetic flow meter

- Blood is a conducting fluid.
- Applying a magnetic field perpendicular to the flow will induce an EMG.
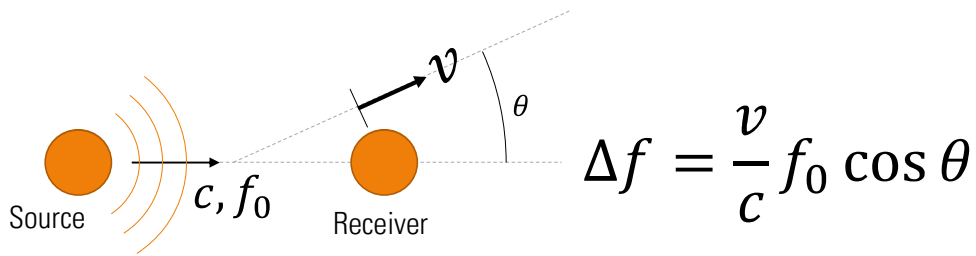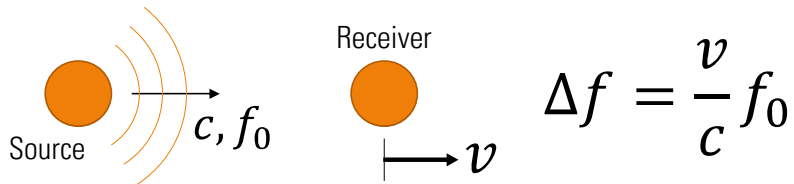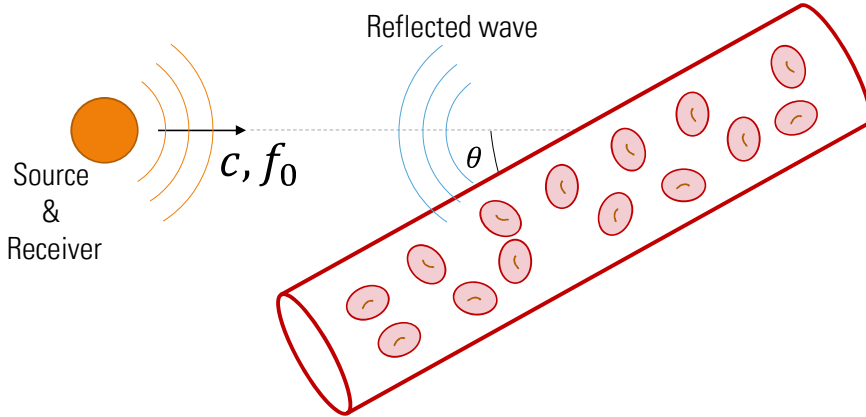
$$e = \int_0^L u(l) \times B\, dl$$
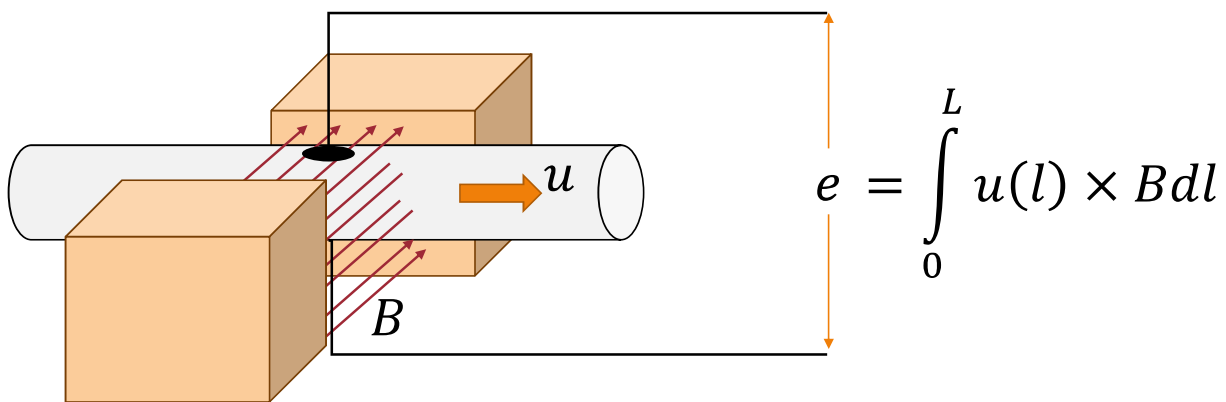
Electromagnetic flow meter

Ultrasound continuous Doppler flow sensing

- Use the Doppler effect to determine flow rate.

Receiver

Source c, f_0

$\longmapsto v$

$$\Delta f = \frac{v}{c} f_0$$

Source c, f_0 Receiver

v

θ

$$\Delta f = \frac{v}{c} f_0 \cos \theta$$

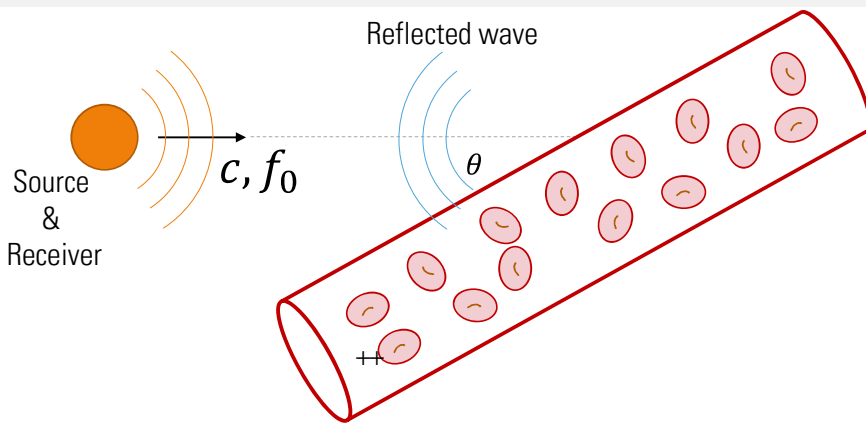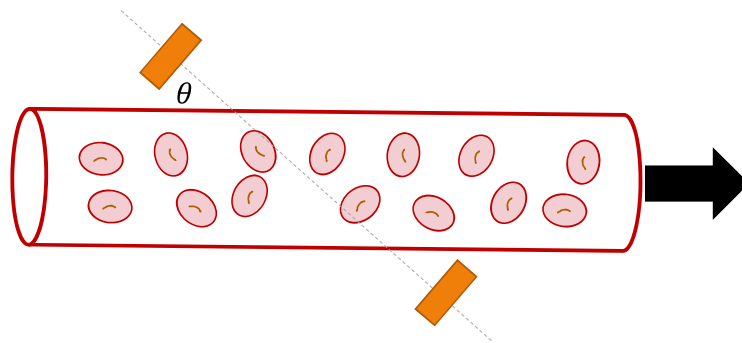# Ultrasound continuous Doppler flow sensing

$$\Delta f = \frac{2v}{c} f_0 \cos \theta$$

Ultrasound continuous Doppler flow sensing

Reflected wave

c, f_0

Source
&
Receiver

θ

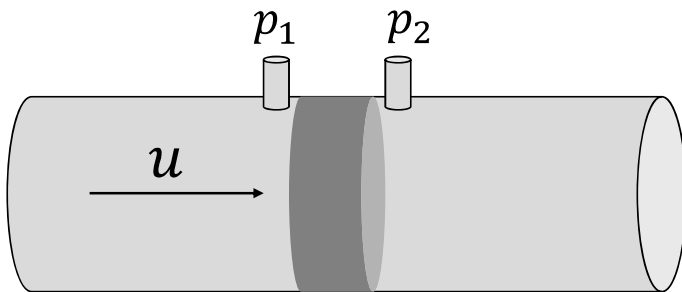$$\Delta f = \frac{2v}{c} f_0 \cos \theta$$

Ultrasound transit time flow sensing

$$\Delta T = \frac{D}{c \pm u \cos \theta}$$

Pressure drop method – Pneumotachometer

- There is a pressure drop when air flows through a path offering resistance to air flow.

p_1 p_2

u

Laminar Flow (through a set of capillaries)

$$\Delta p = p_1 - p_2 = \frac{128\mu L}{N\pi D^4} u$$
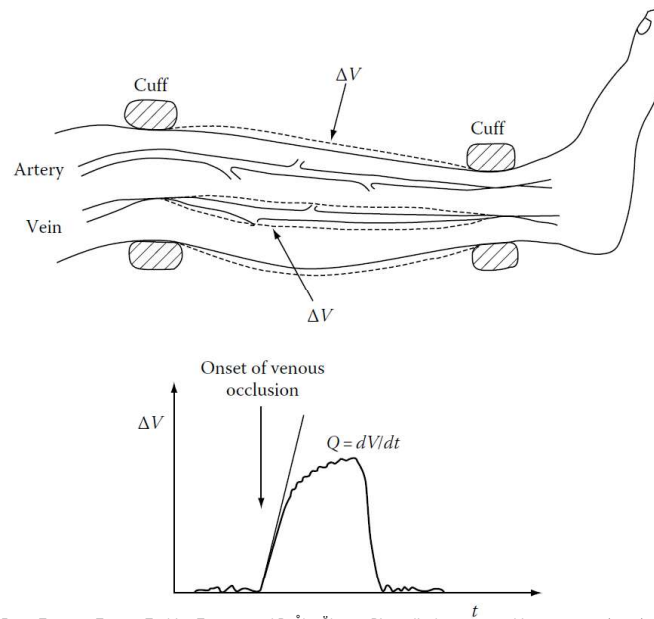
Turbulent Flow (with square edge orifice)

$$\Delta p = \frac{\rho}{2C_D A^4} |u|u$$

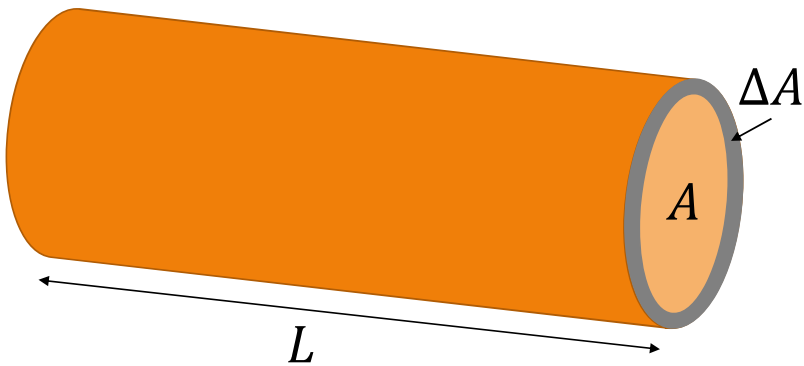$$\Delta p = Ru + k|u|u$$

Venous occlusion plethysmography

- Plethysmography is a technique of measuring volume change in a tissue.

From: Togawa, Tatsuo, Toshiyo Tamura, and P. Åke Öberg. "Biomedical sensors and instruments." (2011).
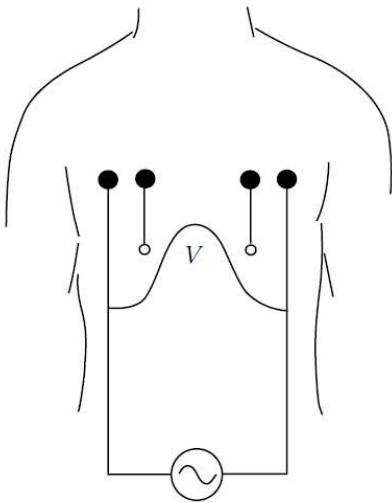
Impedance plethysmograph

- Change in impedance due to a change in volume of a body segment.

Two vs. Four electrodes plethysmograph

Thoracic pneumography

$$\frac{\Delta Z}{\Delta V} = 453.23 W^{-1.084}$$