

Unsupervised Accelerated MRI Reconstruction via Ground-Truth-Free Flow Matching

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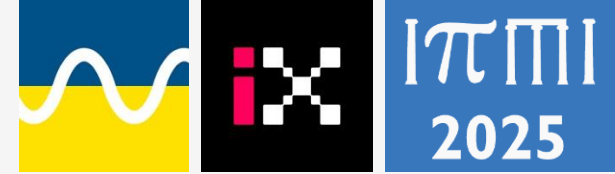


Motivation



Motivation

MRI reconstruction

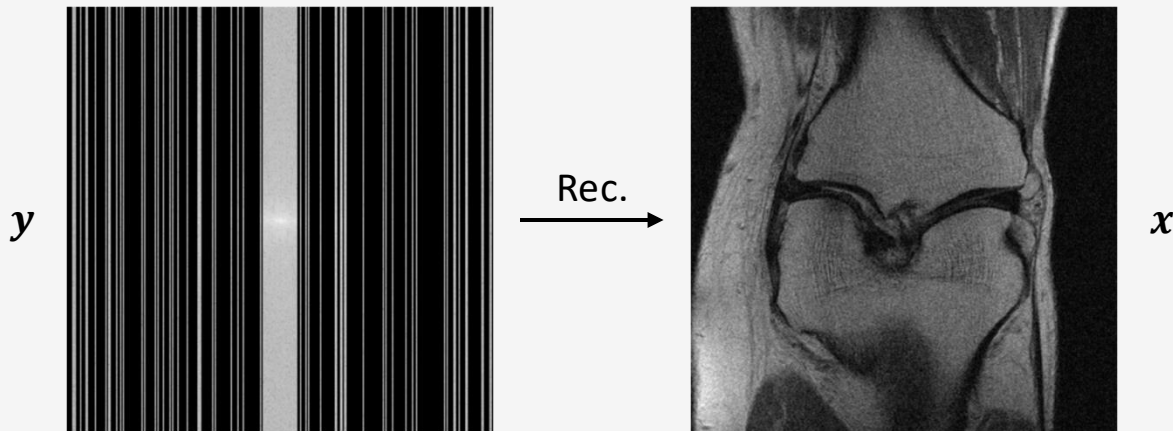


- I** Reconstruct the fully-sampled MR image $\mathbf{x} \in \mathbb{C}^D$ from under-sampled k-space measurements $\mathbf{y} \in \mathbb{C}^d$ through the forward model

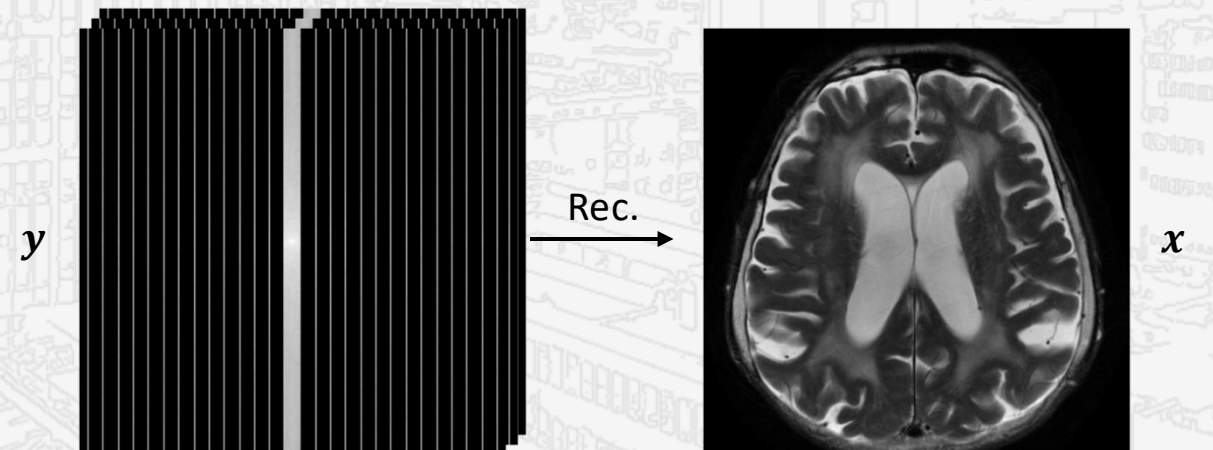
$$\begin{bmatrix} \mathbf{y}_1 \\ \mathbf{y}_2 \\ \vdots \\ \mathbf{y}_C \end{bmatrix} := \mathbf{y} = \mathbf{A}\mathbf{x} + \mathbf{e} := \begin{bmatrix} \mathbf{MFS}_1 \\ \mathbf{MFS}_2 \\ \vdots \\ \mathbf{MFS}_C \end{bmatrix} \mathbf{x} + \mathbf{e},$$

where $\mathbf{M} \in \{0,1\}^{d \times D}$ denotes the under-sampling mask, $\mathbf{F} \in \mathbb{C}^{D \times D}$ the discrete Fourier transform, $\mathbf{S}_i \in \mathbb{C}^{D \times D}$ the sensitivity map of the i -th coil, and $\mathbf{e} \sim \mathcal{CN}(\mathbf{0}, 2\sigma^2 \mathbf{I}_{cd})$ the complex Gaussian noise in k-space.

Emulated single coil

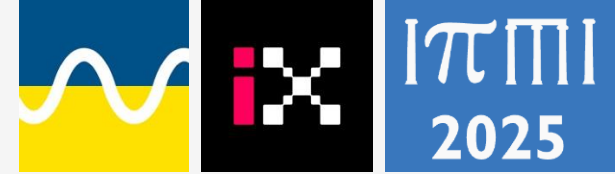


Multi-coil k-space



Motivation

Research gaps of MRI reconstruction



Previous work

I Optimisation-based:

$$\mathbf{x}^* \in \arg \min_{\mathbf{x}} \{-\log p(\mathbf{y} | \mathbf{x}) + \mathcal{R}(\mathbf{x})\},$$

where $\mathcal{R}(\cdot)$ is some regularization term.

I Supervised learning-based:

- given paired training data $\{(\mathbf{x}_i, \mathbf{y}_i)\}_{i=1}^N$, train a neural network $f_{\theta}: \mathbf{y} \mapsto \mathbf{x}$ via loss minimization^{1,2}

I Bayesian inference:

- Learn the prior distribution of fully-sampled images by generative models
- Reconstruct the observation through posterior sampling^{3,4,5,6}

¹Aggarwal et al., TMI 2018

²Hammernik et al., MRM 2018

³Song et al., ICLR 2022

⁴Wang et al., ICLR 2023

⁵Chung et al., ICLR 2023

⁶Song et al., ICLR 2023

Research gaps

- I Both supervised and prior learning approaches require large datasets of fully-sampled MR images, which can be inaccessible.
- I The high number of neural function evaluations (NFEs) of diffusion-model-based MRI reconstruction is computationally prohibitive in practice.

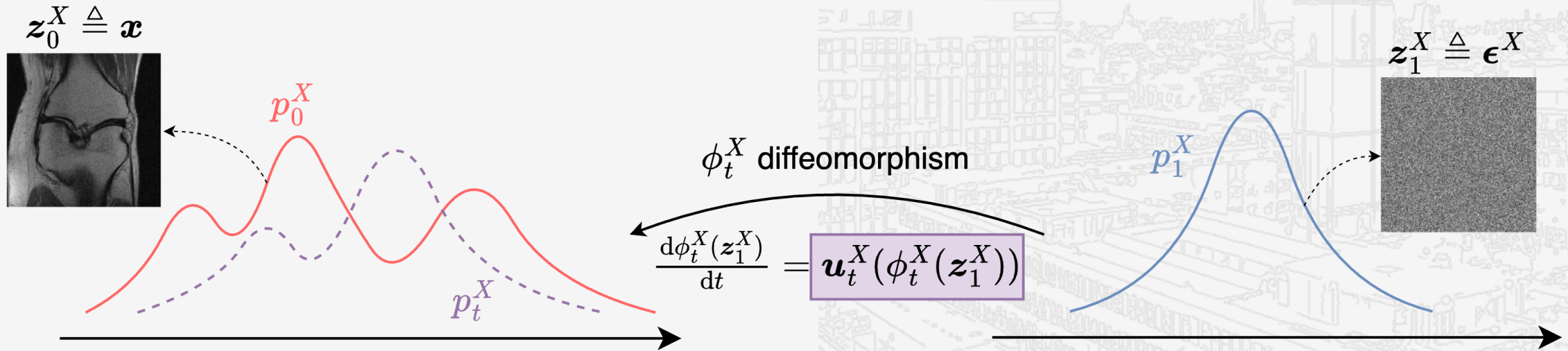
Methodology



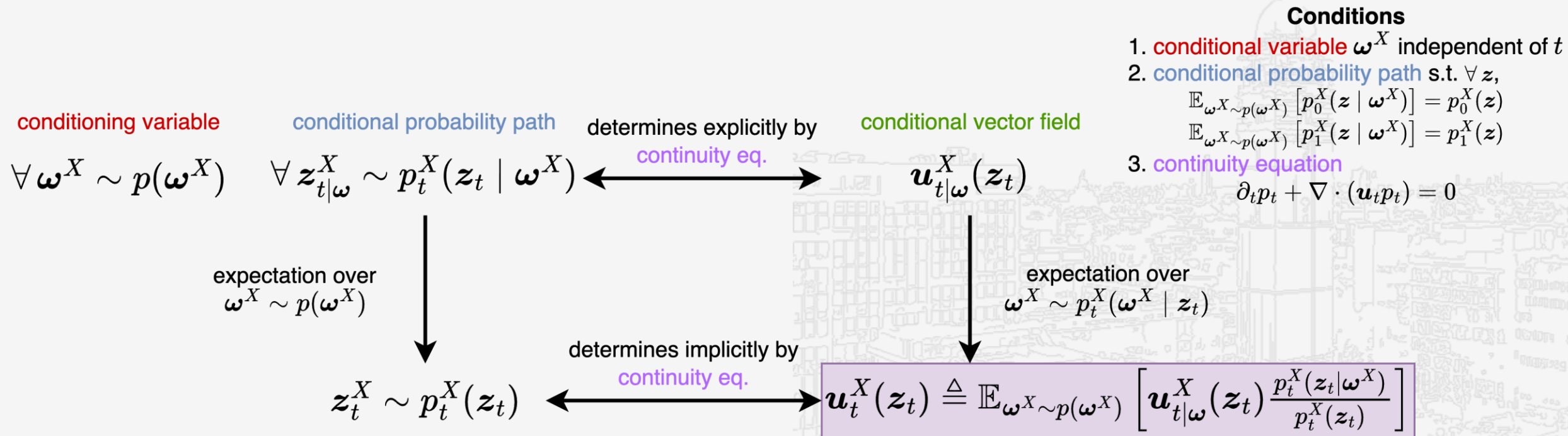
- I Goal:** learn a continuous normalising flow (CNF) from $p_1^X = \mathcal{N}(\mathbf{0}, \mathbf{I}_D)$ to p_0^X of the fully-sampled MR images.
- I** Flow matching offers a **simulation-free** approach to learning the CNF.

I Formulation: define the CNF in the image space (X) by a diffeomorphism $\phi_t^X: [0,1] \times \mathbb{R}^D \rightarrow \mathbb{R}^D$

- I** ϕ_t^X parameterised by a **time-dependent vector field** $\mathbf{u}_t^X: [0,1] \times \mathbb{R}^D \rightarrow \mathbb{R}^D$,
- $$\mathbf{z}_t^X \triangleq \phi_t^X(\mathbf{z}_1^X), \quad \forall \mathbf{z}_1^X \sim p_1^X, \quad d\mathbf{z}_t^X = \mathbf{u}_t^X(\mathbf{z}_t^X)dt, \quad \phi_1^X = \text{id}.$$



Question: How to construct the vector field \mathbf{u}_t^X such that $p_0^X = [\phi_{1 \rightarrow 0}^X]_{\#} p_1^X$ (**push-forward** of p_1^X by $\phi_{1 \rightarrow 0}^X$)?





I Specification of the flow:

- I Choose the **conditioning variable** $\omega^X \triangleq (\mathbf{x}, \epsilon^X) \sim p_0^X \times p_1^X$.
- I Choose the **conditional probability path** $p_t^X(\mathbf{z}_t | \omega^X) \triangleq \delta_{a_t \mathbf{x} + b_t \epsilon^X}(\mathbf{z}_t)$ (linear interpolation).
- I Then, the **conditional vector field** is $\mathbf{u}_{t|\omega}^X(\mathbf{z}_{t|\omega}^X) = a'_t \mathbf{x} + b'_t \epsilon^X$ satisfying the **continuity equation**.

I Training of the flow:

I Flow matching (FM) objective:

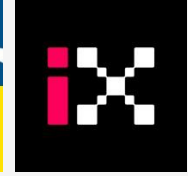
$$\mathcal{L}_{\text{FM}}(\boldsymbol{\theta}) := \mathbb{E}_{t \sim p_T, \mathbf{z}_t^X \sim p_t^X(\mathbf{z}_t)} \|\mathbf{v}_{\boldsymbol{\theta}}^X(\mathbf{z}_t^X, t) - \mathbf{u}_t^X(\mathbf{z}_t^X)\|_2^2$$

- **Problem**: no closed-form expression for the marginal vector field $\mathbf{u}_t^X(\mathbf{z}_t^X)$

I Conditional flow matching (CFM) objective:

$$\mathcal{L}_{\text{CFM}}(\boldsymbol{\theta}) := \mathbb{E}_{t \sim p_T, \omega^X \sim p(\omega^X), \mathbf{z}_{t|\omega}^X \sim p_t^X(\mathbf{z}_t | \omega^X)} \|\mathbf{v}_{\boldsymbol{\theta}}^X(\mathbf{z}_{t|\omega}^X, t) - \mathbf{u}_{t|\omega}^X(\mathbf{z}_{t|\omega}^X)\|_2^2$$

- The gradient of the CFM is equivalent to that of the FM objective.
- **Problem**: training requires large number of fully-sampled images.



I Dual-space conditional vector fields

I Measurement (Y)-space **conditioning variable**: $\omega^Y \triangleq (\mathbf{y}, \epsilon^Y)$, $\epsilon^Y \triangleq \mathbf{A}\epsilon^X$.

I Y -space **conditional probability path**: $p_t^Y(\mathbf{z}_t \mid \omega^Y) \triangleq \delta_{a_t\mathbf{y}+b_t\epsilon^Y}(\mathbf{z}_t)$.

I Y -space **conditional vector field**: $\mathbf{u}_{t|\omega}^Y(\mathbf{z}_{t|\omega}^Y) = a'_t\mathbf{y} + b'_t\epsilon^Y$.

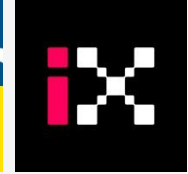
I Forward model of the dual-space conditional paths and vector fields

I Using the conditions $\mathbf{y} = \mathbf{A}\mathbf{x} + \mathbf{e}$ and $\epsilon^Y \triangleq \mathbf{A}\epsilon^X$, we can derive

$$\mathbf{z}_{t|\omega}^Y = \mathbf{A}\mathbf{z}_{t|\omega}^X + a_t\mathbf{e},$$

where $\mathbf{z}_{t|\omega}^X \triangleq a_t\mathbf{x} + b_t\epsilon^X$, $\mathbf{z}_{t|\omega}^Y \triangleq a_t\mathbf{y} + b_t\epsilon^Y$ and

$$\mathbf{u}_{t|\omega}^Y(\mathbf{z}_{t|\omega}^Y) = \mathbf{A}\mathbf{u}_{t|\omega}^X(\mathbf{z}_{t|\omega}^X) + a'_t\mathbf{e}.$$



I **Goal:** to learn the X -space marginal vector field $\mathbf{u}_t^X(\mathbf{z}_t^X)$ in a ground-truth-free manner.

I Denote $\mathbf{h}_\theta^X(\cdot)$: the **predictor network** for $\mathbf{u}_t^X(\mathbf{z}_t^X)$.

I **GTF²M objective:**

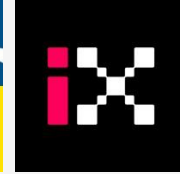
$$\mathcal{L}_{\text{GTF}^2\text{M}}(\boldsymbol{\theta}) \triangleq \mathbb{E}_{t \sim p_T, \boldsymbol{\omega}^X \sim p(\boldsymbol{\omega}^X), \mathbf{z}_{t|\boldsymbol{\omega}}^X \sim p_t^X(\mathbf{z}_t | \boldsymbol{\omega}^X), \mathbf{z}_{t|\boldsymbol{\omega}}^Y \sim p_t^Z(\mathbf{z}_t^Y | \mathbf{z}_{t|\boldsymbol{\omega}}^X)} \|\mathbf{h}_\theta^X(\mathbf{z}_{t|\boldsymbol{\omega}}^Y, t) - \mathbf{u}_{t|\boldsymbol{\omega}}^X(\mathbf{z}_{t|\boldsymbol{\omega}}^X)\|_2^2$$

where $p_t^Z(\mathbf{z}_{t|\boldsymbol{\omega}}^Y | \mathbf{z}_{t|\boldsymbol{\omega}}^X)$ is induced from $\mathbf{z}_{t|\boldsymbol{\omega}}^Y = \mathbf{A}\mathbf{z}_{t|\boldsymbol{\omega}}^X + a_t\mathbf{e}$.

I It turns out that $\mathcal{L}_{\text{GTF}^2\text{M}}(\boldsymbol{\theta})$ can be written as

$$\mathcal{L}_{\text{GTF}^2\text{M}}(\boldsymbol{\theta}) = \mathbb{E}_{t \sim p_T, \mathbf{z}_t^X \sim p_t^X(\mathbf{z}_t), \mathbf{z}_t^Y \sim p_t^Z(\mathbf{z}_t^Y | \mathbf{z}_t^X)} \|\mathbf{h}_\theta^X(\mathbf{z}_t^Y, t) - \mathbf{u}_t^X(\mathbf{z}_t^X)\|_2^2 + \text{const.}$$

- \Rightarrow The GTF²M objective drives $\mathbf{h}_\theta^X(\cdot)$ to predict $\mathbf{u}_t^X(\mathbf{z}_t^X)$.



I **Goal:** to learn the X -space marginal vector field $\mathbf{u}_t^X(\mathbf{z}_t^X)$ in a ground-truth-free manner.

I **ENsemble Stein's Unbiased Risk Estimator (ENSURE)** (Aggarwal et al., TMI 2022)

I Assume the forward operator \mathbf{A}_s is random and parameterised by a random variable s ;

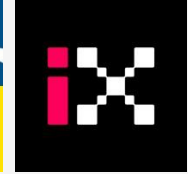
I Assume the forward model $\mathbf{y}_s = \mathbf{A}_s \mathbf{x} + \mathbf{e}$, $\mathbf{e} \sim \mathcal{N}(\mathbf{0}, \mathbf{C})$;

I Denote $\boldsymbol{\rho}_s \triangleq \mathbf{A}_s^* \mathbf{C}^{-1} \mathbf{y}_s$ the sufficient statistic, and $\hat{\mathbf{x}} \triangleq f_{\boldsymbol{\theta}}(\boldsymbol{\rho}_s)$ the reconstruction network.

I Then, the MSE has an unbiased estimator as

$$\begin{aligned} \mathcal{L}_{\text{MSE}}(\boldsymbol{\theta}) &= \mathbb{E}_{\boldsymbol{\rho}} \|\mathbf{f}_{\boldsymbol{\theta}}(\boldsymbol{\rho}) - \mathbf{x}\|_2^2 \\ &= \mathbb{E}_s \mathbb{E}_{\boldsymbol{\rho}_s} \|\mathbf{R}_s(\mathbf{f}_{\boldsymbol{\theta}}(\boldsymbol{\rho}_s) - \mathbf{x})\|_2^2 \\ &= \mathbb{E}_s \mathbb{E}_{\boldsymbol{\rho}_s} \left[\|\mathbf{R}_s(\mathbf{f}_{\boldsymbol{\theta}}(\boldsymbol{\rho}_s) - \boldsymbol{\rho}_{s,\text{ML}})\|_2^2 + 2\nabla_{\boldsymbol{\rho}_s} \cdot \mathbf{R}_s^* \mathbf{R}_s \mathbf{f}_{\boldsymbol{\theta}}(\boldsymbol{\rho}_s) \right] + \text{const.} \end{aligned}$$

where $\mathbf{R}_s \triangleq \mathbf{W} \mathbf{P}_s$ with $\mathbf{P}_s \triangleq \mathbf{A}_s^{\dagger} \mathbf{A}_s$ and $\mathbf{W} \triangleq \mathbb{E}_s[\mathbf{P}_s]^{-1/2}$, and $\boldsymbol{\rho}_{s,\text{ML}} \triangleq (\mathbf{A}_s^* \mathbf{C}^{-1} \mathbf{A}_s)^{\dagger} \mathbf{A}_s^* \mathbf{C}^{-1} \mathbf{y}_s$ is the MLE solution for $\mathbf{y}_s = \mathbf{A}_s \mathbf{x} + \mathbf{e}$.



Goal: to learn the X -space marginal vector field $\mathbf{u}_t^X(\mathbf{z}_t^X)$ in a ground-truth-free manner.

Recall the following facts:

I Induced forward model over dual-space conditional vector fields:

$$\mathbf{u}_{t|\omega}^Y(\mathbf{z}_{t|\omega}^Y) = \mathbf{A}\mathbf{u}_{t|\omega}^X(\mathbf{z}_{t|\omega}^X) + a'_t\mathbf{e}.$$

I Relationship between the measurement-space conditional path and vector field:

$$\mathbf{z}_{t|\omega}^Y = a_t\mathbf{y} + b_t\boldsymbol{\epsilon}^Y = \frac{a_t}{a'_t}\mathbf{u}_{t|\omega}^Y(\mathbf{z}_{t|\omega}^Y) - b'_t\left(\frac{a_t}{a'_t} - \frac{b_t}{b'_t}\right)\boldsymbol{\epsilon}^Y,$$

which implies that we can make prediction based on $\mathbf{u}_{t|\omega}^Y(\mathbf{z}_{t|\omega}^Y)$ instead of $\mathbf{z}_{t|\omega}^Y$:

$$\mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{z}_{t|\omega}^Y, t) = \mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{u}_{t|\omega}^Y(\mathbf{z}_{t|\omega}^Y), t).$$

I The GTF²M objective takes the form as an MSE:

$$\mathcal{L}_{\text{GTF}^2\text{M}}(\boldsymbol{\theta}) = \mathbb{E}_{t \sim p_T, \omega^X \sim p(\omega^X), \mathbf{z}_{t|\omega}^X \sim p_t^X(\mathbf{z}_t|\omega^X), \mathbf{z}_{t|\omega}^Y \sim p_t^Y(\mathbf{z}_{t|\omega}^Y|\mathbf{z}_{t|\omega}^X)} \|\mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{u}_{t|\omega}^Y(\mathbf{z}_{t|\omega}^Y), t) - \mathbf{u}_{t|\omega}^X(\mathbf{z}_{t|\omega}^X)\|_2^2.$$



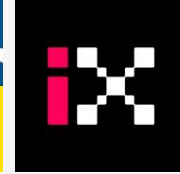
Goal: to learn the X -space marginal vector field $\mathbf{u}_t^X(\mathbf{z}_t^X)$ in a ground-truth-free manner.

ENSURE for GTF²M:

$$\begin{aligned}\mathcal{L}_{\text{GTF}^2\text{M}}(\boldsymbol{\theta}) &= \mathbb{E}_{t, \omega^X, \mathbf{z}_{t|\omega}^X, \mathbf{z}_{t|\omega}^Y | \mathbf{z}_{t|\omega}^X} \left\| \mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{u}_{t|\omega}^Y(\mathbf{z}_{t|\omega}^Y), t) - \mathbf{u}_{t|\omega}^X(\mathbf{z}_{t|\omega}^X) \right\|_2^2 \\ &= \mathbb{E}_{s, t, \omega^X, \mathbf{z}_{t|\omega, s}^X, \mathbf{z}_{t|\omega, s}^Y | \mathbf{z}_{t|\omega, s}^X} \left\| \mathbf{R}_s [\mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{u}_{t|\omega, s}^Y(\mathbf{z}_{t|\omega, s}^Y), t) - \mathbf{u}_{t|\omega, s}^X(\mathbf{z}_{t|\omega, s}^X)] \right\|_2^2 \\ &= \mathbb{E}_{s, t, \omega^Y, \mathbf{z}_{t|\omega, s}^Y} \left[\left\| \mathbf{R}_s [\mathbf{h}_{\boldsymbol{\theta}}^X(\boldsymbol{\mu}_{t|\omega, s}^X, t) - \hat{\mathbf{u}}_{t|\omega, s, \text{ML}}^X] \right\|_2^2 + 2 \nabla_{\boldsymbol{\mu}_{t|\omega, s}^X} \cdot \mathbf{R}_s^* \mathbf{R}_s \mathbf{h}_{\boldsymbol{\theta}}^X(\boldsymbol{\mu}_{t|\omega, s}^X, t) \right] + \text{const.}\end{aligned}$$

where $\boldsymbol{\mu}_{t|\omega, s}^X \triangleq \mathbf{A}_s^* \mathbf{C}_t^{-1} \mathbf{u}_{t|\omega, s}^Y(\mathbf{z}_{t|\omega, s}^Y)$ is a sufficient statistic for $\mathbf{u}_{t|\omega, s}^X(\mathbf{z}_{t|\omega, s}^X)$ with $\mathbf{C}_t = (a'_t \sigma)^2 \mathbf{I}_d$, and $\hat{\mathbf{u}}_{t|\omega, s, \text{ML}}^X \triangleq (\mathbf{A}_s^* \mathbf{C}_t^{-1} \mathbf{A}_s)^{\dagger} \mathbf{A}_s^* \mathbf{C}_t^{-1} \mathbf{u}_{t|\omega, s}^Y(\mathbf{z}_{t|\omega, s}^Y)$ the MLE solution for $\mathbf{u}_{t|\omega, s}^Y(\mathbf{z}_{t|\omega, s}^Y) = \mathbf{A} \mathbf{u}_{t|\omega, s}^X(\mathbf{z}_{t|\omega, s}^X) + a'_t \mathbf{e}$.

I For single-coil MRI $\mathbf{A}_s = \mathbf{M}_s \mathbf{F}$, $\mathbf{M}_s = [\mathbf{I}_d \mid \mathbf{0}] \mathbf{T}_s$ for some permutation matrix $\mathbf{T}_s \in \{0, 1\}^{D \times D}$, the projection operator $\mathbf{R}_s \triangleq \mathbf{W} \mathbf{P}_s = \mathbf{F}^* \mathbf{T}_s^{\text{T}} \text{diag}(p_1^{-1/2}, \dots, p_d^{-1/2}, 0, \dots, 0) \mathbf{T}_s \mathbf{F}$, where p_i is the probability that the i th k-space measurement is acquired.



Goal: to learn the X -space marginal vector field $\mathbf{u}_t^X(\mathbf{z}_t^X)$ in a ground-truth-free manner.

Computation of the GTF²M objective

I Note that $\boldsymbol{\mu}_{t|\omega,s}^X = \mathbf{A}_s^* \mathbf{C}_t^{-1} \mathbf{u}_{t|\omega,s}^Y(\mathbf{z}_{t|\omega,s}^Y) = \frac{1}{a'_t a_t \sigma^2} [\mathbf{A}_s^* \mathbf{z}_{t|\omega,s}^Y + c \boldsymbol{\epsilon}^Y]$; we can write

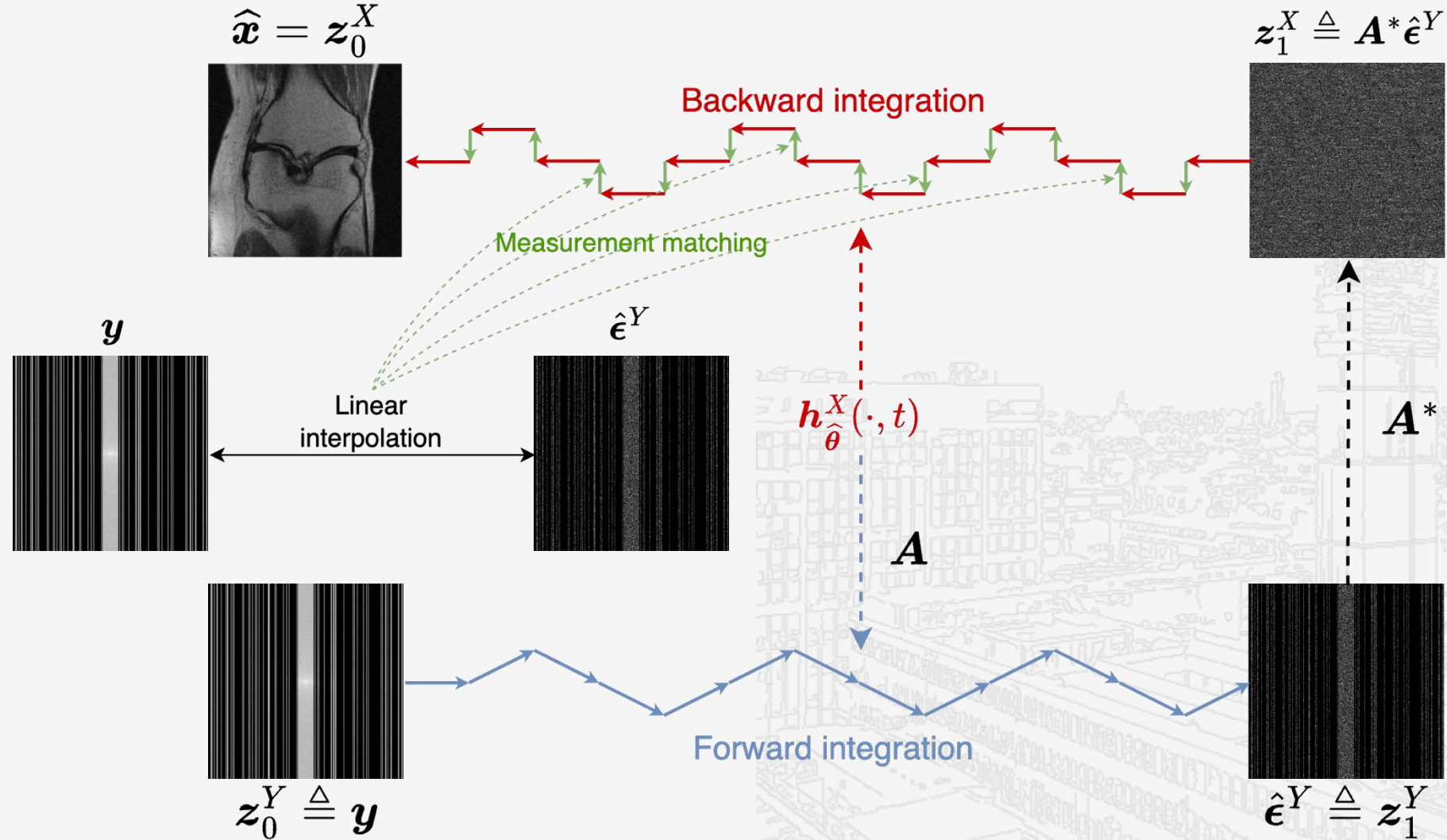
$$\mathbf{h}_{\boldsymbol{\theta}}^X(\boldsymbol{\mu}_{t|\omega,s}^X, t) = \mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{A}_s^* \mathbf{z}_{t|\omega,s}^Y, t).$$

I By change of variables, the GTF²M objective can be written as

$$\mathcal{L}_{\text{GTF}^2\text{M}}(\boldsymbol{\theta}) = \mathbb{E}_{s, t, \omega^Y, \mathbf{z}_{t|\omega,s}^Y} \left[\left\| \mathbf{R}_s [\mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{A}_s^* \mathbf{z}_{t|\omega,s}^Y, t) - \hat{\mathbf{u}}_{t|\omega,s,\text{ML}}^X] \right\|_2^2 + 2a'_t a_t \sigma^2 \nabla_{\mathbf{A}_s^* \mathbf{z}_{t|\omega,s}^Y} \cdot \mathbf{R}_s^* \mathbf{R}_s \mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{A}_s^* \mathbf{z}_{t|\omega,s}^Y, t) \right] + \text{const.}$$

I Using the Hutchinson trace estimator, the divergence term can be estimated as

$$\nabla_{\mathbf{A}_s^* \mathbf{z}_{t|\omega,s}^Y} \cdot \mathbf{R}_s^* \mathbf{R}_s \mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{A}_s^* \mathbf{z}_{t|\omega,s}^Y, t) = \mathbb{E}_{\mathbf{b} \sim \mathcal{N}(\mathbf{0}, \mathbf{R}_s^* \mathbf{R}_s)} \left[\mathbf{b}^T \nabla_{\mathbf{A}_s^* \mathbf{z}_{t|\omega,s}^Y} \mathbf{h}_{\boldsymbol{\theta}}^X(\mathbf{A}_s^* \mathbf{z}_{t|\omega,s}^Y, t) \mathbf{b} \right].$$





Algorithm 1: Decoupled continuous de-aliasing via cyclic integration

- I Input:** k-space measurement $\mathbf{y} = (\mathbf{y}_c)_{c=1}^C$, pretrained flow predictor $\mathbf{h}_{\hat{\theta}}^X(\cdot, t)$, forward steps L , backward steps K , regularisation parameter ζ
- I Output:** reconstructed MR image $\hat{\mathbf{x}}$ of \mathbf{y}
- I Steps:**
1. Set $\mathbf{z}_0^Y := \mathbf{y}$;
 2. For $t = 0, \dots, (L-1)/L$ do
 - $\mathbf{z}_{t+1/L}^Y \leftarrow \mathbf{z}_t^Y + \frac{1}{L} \mathbf{A} \mathbf{h}_{\hat{\theta}}^X(\mathbf{A}^* \mathbf{z}_t^Y, t)$; // forward integration
 3. Set $\hat{\mathbf{e}}^Y := \mathbf{z}_1^Y, \mathbf{z}_1^X := \mathbf{A}^* \hat{\mathbf{e}}^Y$;
 4. For $t \in \{1, \dots, 1/K\}$ do
 - $\mathbf{z}_{t|\hat{\omega}}^Y = a_t \mathbf{y} + b_t \hat{\mathbf{e}}^Y$;
 - $\mathbf{z}_{t-1/K}^X \leftarrow \mathbf{z}_t^X - \frac{1}{K} \mathbf{h}_{\hat{\theta}}^X(\mathbf{A}^* \mathbf{z}_{t|\hat{\omega}}^Y, t)$; // backward integration
 - $\mathbf{z}_t^X \leftarrow \mathbf{z}_t^X - \lambda_t \mathbf{A}^* (\mathbf{A} \mathbf{z}_t^X - \mathbf{z}_{t|\hat{\omega}}^Y)$; // measurement consistency update
 5. Set $\hat{\mathbf{x}} := \mathbf{z}_0^X$ for single-coil or $\hat{\mathbf{x}} := (\sum_{c=1}^C \mathbf{S}_c^* \mathbf{S}_c)^{-1} \sum_{c=1}^C \mathbf{S}_c^* \mathbf{z}_{0,c}^X$ for multi-coil reconstruction;
- I Return** $\hat{\mathbf{x}}$

Experiments & Results



Experiments

Datasets and preprocessing

NYU fastMRI Initiative database:

- Single-coil proton density (PD) weighted knee MRI without fat suppression.
- Multi-coil T2 weighted brain MRI.

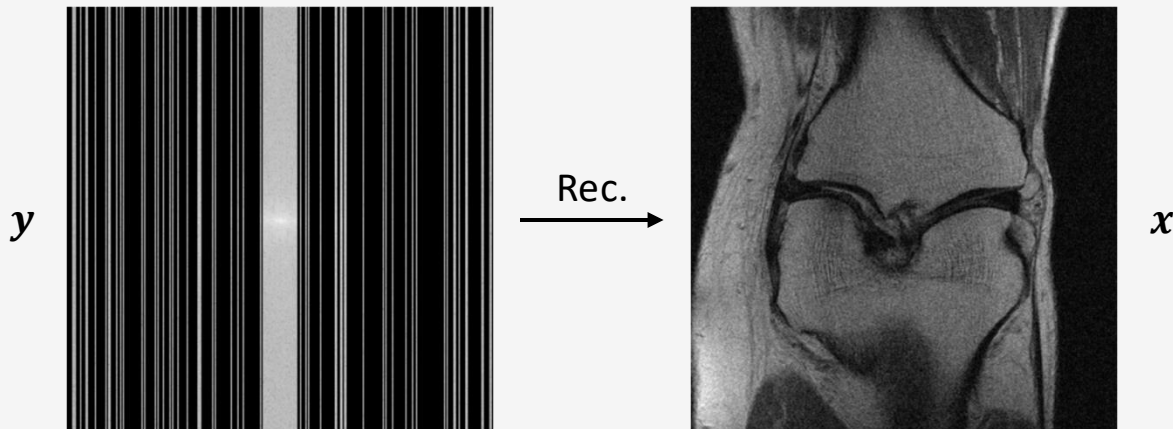
Cartesian sampling masks:

- 8% and 4% fully-sampled low-frequency k-space lines for 4x and 8x, respectively.
- The other lines are sampled random-uniformly and equidistantly for knee and brain MRI, respectively.

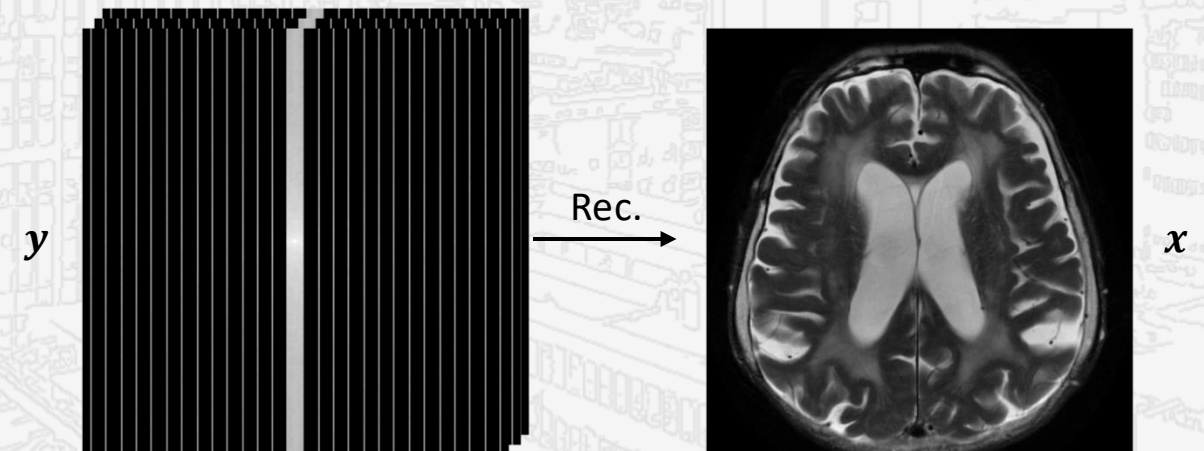
Ground truth:

- Knee: emulated single-coil image; Brain: SENSE reconstruction.

Emulated single coil



Multi-coil k-space



Experiments

Implementation details



Hyperparameters:

- I Linear interpolation: $a_t = 1 - t$ and $b_t = t$;
- I Noise level: $\sigma = 0.01$.

Network architecture: ADM (ablated diffusion model), *Dhariwal and Nichol, NeurIPS 2021*

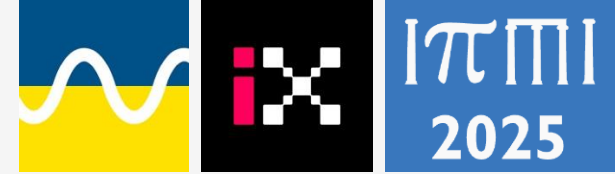
- I U-Net;
- I Adaptive group normalisation (conditioned on linear projection of the positional embeddings of t);
- I Self attention and dropout at the lowest three resolutions of the U-Net.

Training details:

- I AdamW optimiser with learning rate 1×10^{-4} , weight decay coefficient 0.1;
- I Exponential moving average of the network parameters.

Experiments

Compared baselines



Supervised end-to-end learning:

- I** MoDL: Model-based Deep Learning, *Aggarwal et al., TMI 2018;*

Diffusion model-based posterior sampling methods with prior learning:

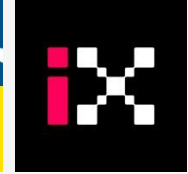
- I** DDNM⁺: Denoising Diffusion Null-space Models, *Wang et al., ICLR 2023;*
- I** IIGDM: Pseudoinverse Guided Diffusion Models, *Song et al., ICLR 2023;*
- I** FlowPS: Flow-based Posterior Sampling, *Pokle et al., TMLR 2024;*

Unsupervised methods without prior learning:

- I** REI: Robust Equivariant Imaging, *Chen et al., CVPR 2022;*
- I** ENSURE: Ensemble Stein's Unbiased Risk Estimator + MoDL, *Aggarwal et al., TMI 2022.*

Results

Comparison study



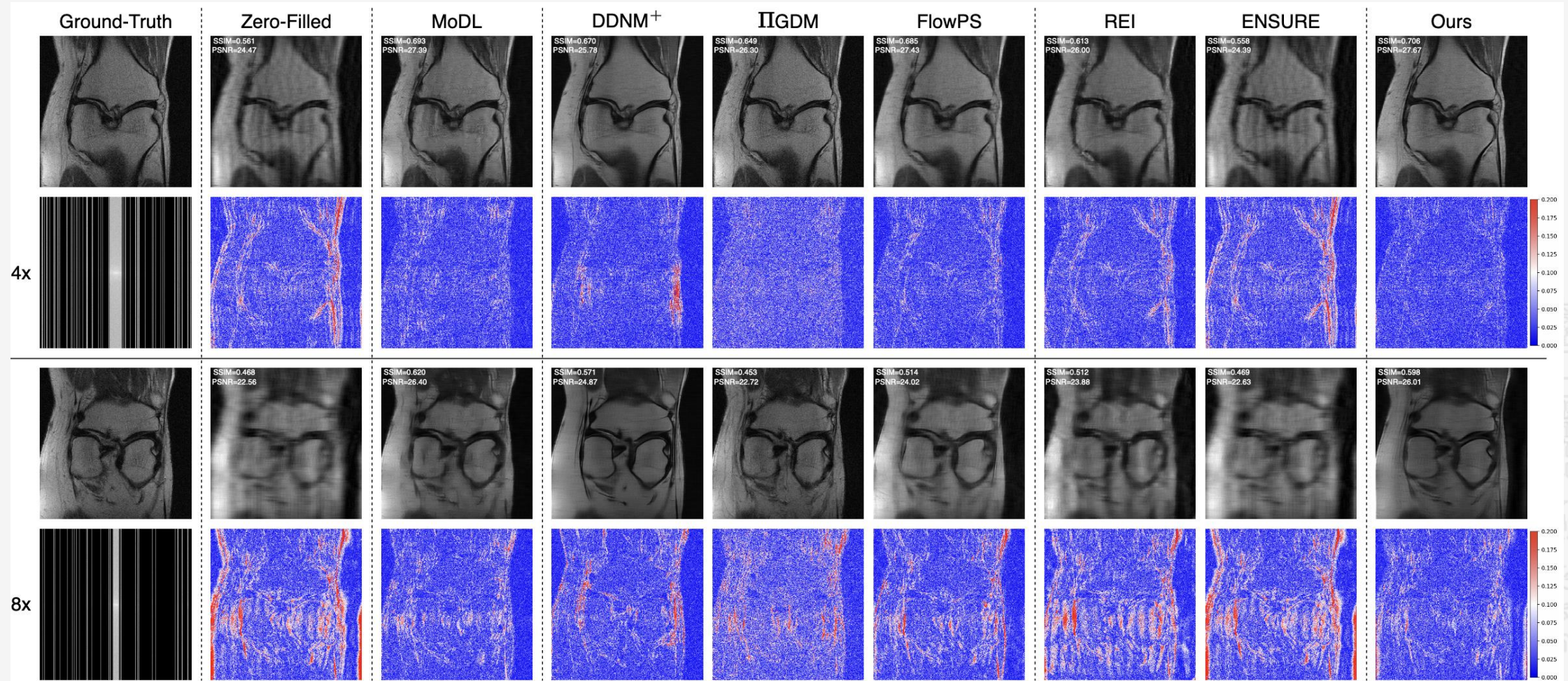
Single-coil knee MRI

Method	SSIM \uparrow		PSNR \uparrow		NFEs \downarrow
	4 \times	8 \times	4 \times	8 \times	
Zero-filled	$0.684 \pm 0.086^*$	$0.556 \pm 0.106^*$	$27.60 \pm 2.78^*$	$23.92 \pm 2.75^*$	N/A
(a) Supervised methods using fully sampled images					
MoDL [1]	$0.786 \pm 0.069^*$	$0.692 \pm 0.107^*$	$30.72 \pm 3.07^*$	$28.58 \pm 2.96^*$	1
(b) Prior learning methods using fully sampled images					
DDNM ⁺ [30]	$0.791 \pm 0.076^*$	$0.681 \pm 0.108^*$	$31.73 \pm 3.29^*$	28.00 ± 3.20	100
ITGDM [24]	$0.728 \pm 0.098^*$	$0.581 \pm 0.114^*$	$30.27 \pm 3.34^*$	$25.83 \pm 3.13^*$	100
FlowPS [20]	$0.763 \pm 0.077^*$	$0.631 \pm 0.101^*$	$30.66 \pm 2.73^*$	$26.30 \pm 2.55^*$	100
(c) Unsupervised methods w/o prior learning					
REI [4]	$0.740 \pm 0.087^*$	$0.591 \pm 0.110^*$	$29.96 \pm 2.87^*$	$25.04 \pm 2.97^*$	1
ENSURE [2]	$0.684 \pm 0.086^*$	$0.556 \pm 0.106^*$	$27.65 \pm 2.79^*$	$23.91 \pm 2.75^*$	1
(d) Unsupervised methods w/ prior learning					
Ours	0.801 ± 0.073	0.688 ± 0.095	31.64 ± 2.95	27.95 ± 2.64	20

Results

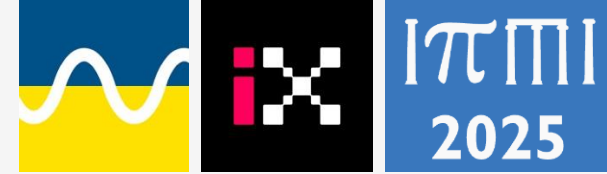
Comparison study

Single-coil knee MRI



Results

Comparison study

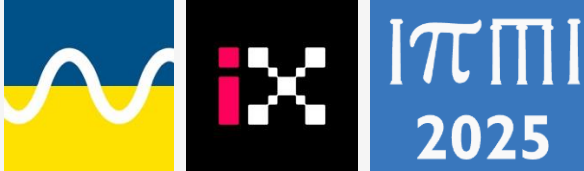


Multi-coil brain MRI

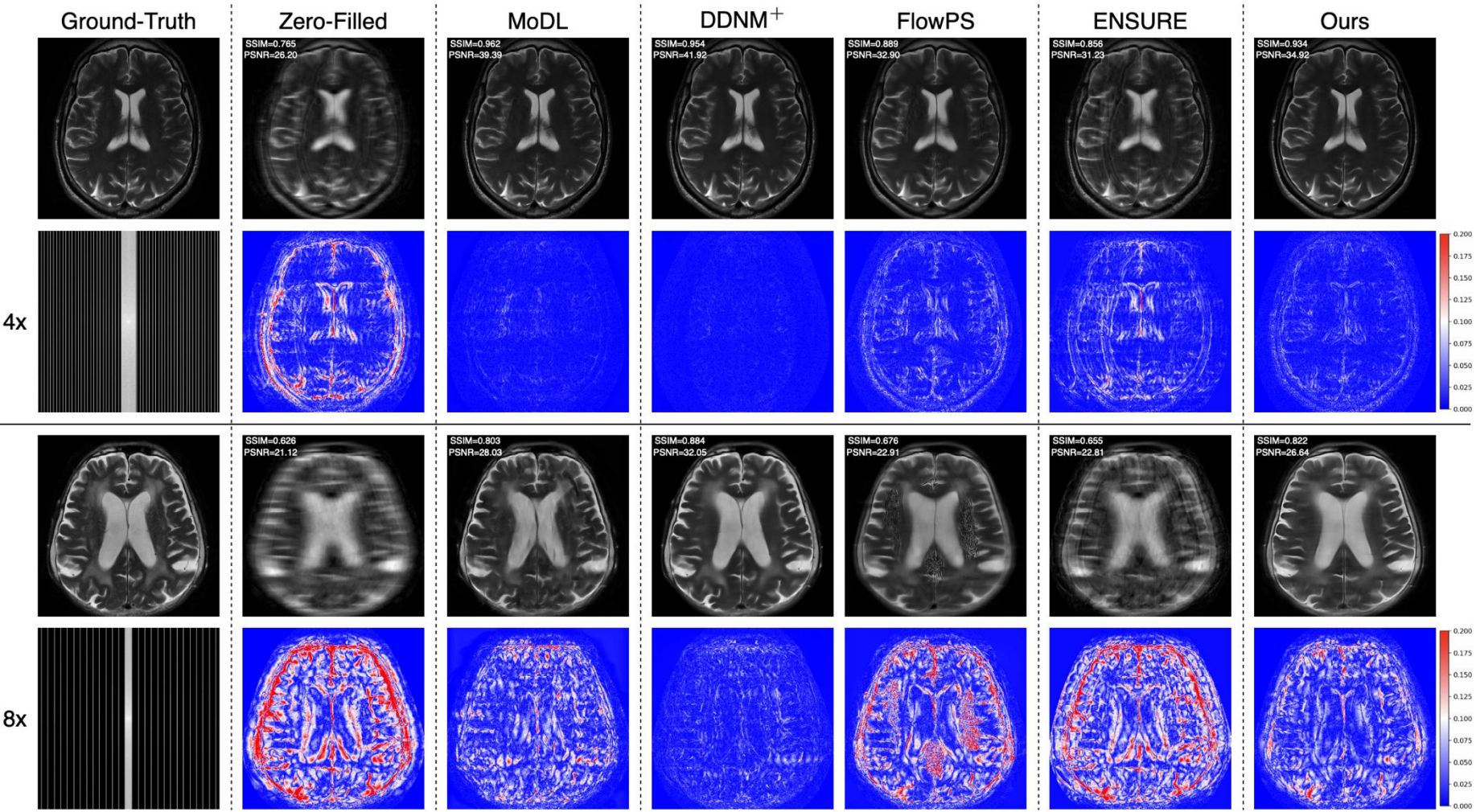
Method	SSIM \uparrow		PSNR \uparrow		NFEs \downarrow
	4 \times	8 \times	4 \times	8 \times	
Zero-filled	$0.800 \pm 0.089^*$	$0.716 \pm 0.117^*$	$27.66 \pm 3.78^*$	$24.10 \pm 3.97^*$	N/A
(a) Supervised methods using fully sampled images					
MoDL [1]	$0.948 \pm 0.044^*$	$0.820 \pm 0.051^*$	$38.28 \pm 3.37^*$	$30.18 \pm 3.04^*$	1
(b) Prior learning methods using fully sampled images					
DDNM ⁺ [30]	$0.929 \pm 0.045^*$	$0.887 \pm 0.048^*$	$40.61 \pm 3.43^*$	$34.13 \pm 2.92^*$	100
FlowPS [20]	$0.855 \pm 0.060^*$	$0.748 \pm 0.069^*$	$33.10 \pm 2.73^*$	$26.56 \pm 3.50^*$	100
(c) Unsupervised methods w/o prior learning					
ENSURE [2]	$0.825 \pm 0.053^*$	$0.739 \pm 0.108^*$	$31.75 \pm 3.99^*$	$25.56 \pm 3.50^*$	1
(d) Unsupervised methods w/ prior learning					
Ours	0.920 ± 0.060	0.859 ± 0.054	34.65 ± 2.32	28.72 ± 2.92	20

Results

Comparison study



Multi-coil brain MRI



Conclusion



Contributions

- An unsupervised prior learning framework for MRI reconstruction
 - No need for fully-sampled MRI during training;
 - An efficient cyclic integration algorithm as a decoupled continuous de-aliasing process.

Limitations and future work

- No closed-form expression of the GTF²M objective for the combined multi-coil MR forward operator;
- Extension of the reconstruction algorithm to noisy data;
- Extension of the framework in the semi-supervised setup.

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Physical Sciences
Research Council

Thank you! Q&A



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