

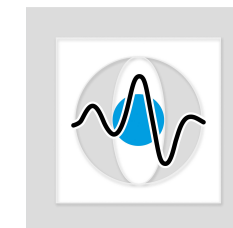
# Medical Image Processing for Diagnostic Applications

## Fan Beam – Truncation Correction

Online Course – Unit 42

Andreas Maier, Joachim Hornegger, Markus Kowarschik, Frank Schebesch

Pattern Recognition Lab (CS 5)



# Topics

## Truncation Correction Algorithms

Defect Pixel Extrapolation

Heuristic Extrapolation

Water Cylinder Assumption

Use of Prior Knowledge

Use of a Semi-transparent Filter

ATTRACT Filtering

## Summary

Take Home Messages

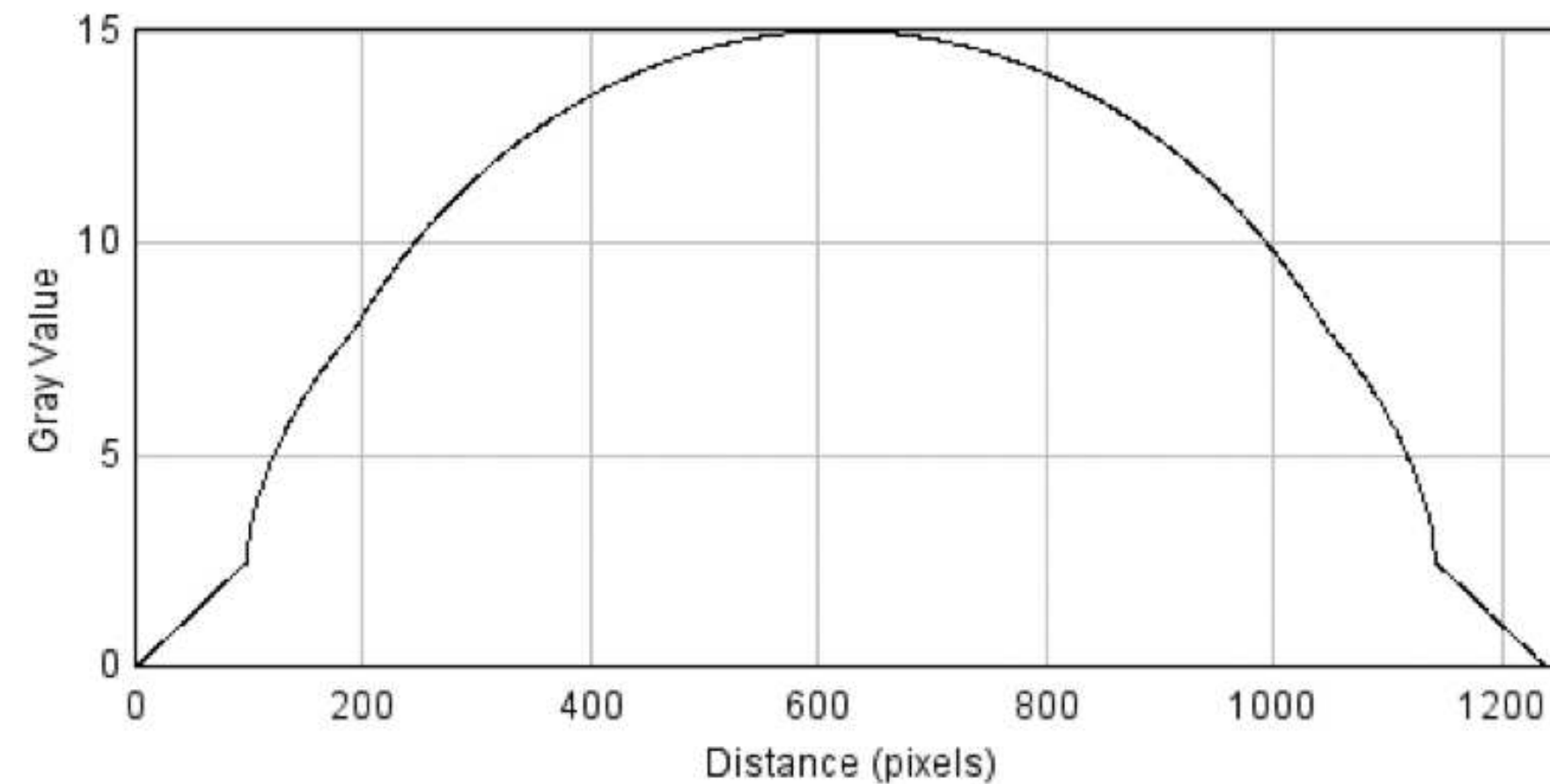
Further Readings

# Truncation Correction via Extrapolation

- Solution 1: Defect pixel extrapolation
- Solution 2: Heuristic extrapolation
- Solution 3: Water cylinder assumption
- Solution 4: Use of prior knowledge
- Solution 5: Use of a semi-transparent filter
- Solution 6: ATRACT filtering

# Defect Pixel Extrapolation

- Model extrapolation as deconvolution.
- Use a defect pixel interpolation algorithm.



→ Unfortunately, the algorithm works not as well as expected.

# Heuristic Extrapolation

- Use mirroring for extrapolation.
- In order to enforce a limited size of the object, a cosine-like weighting is added.

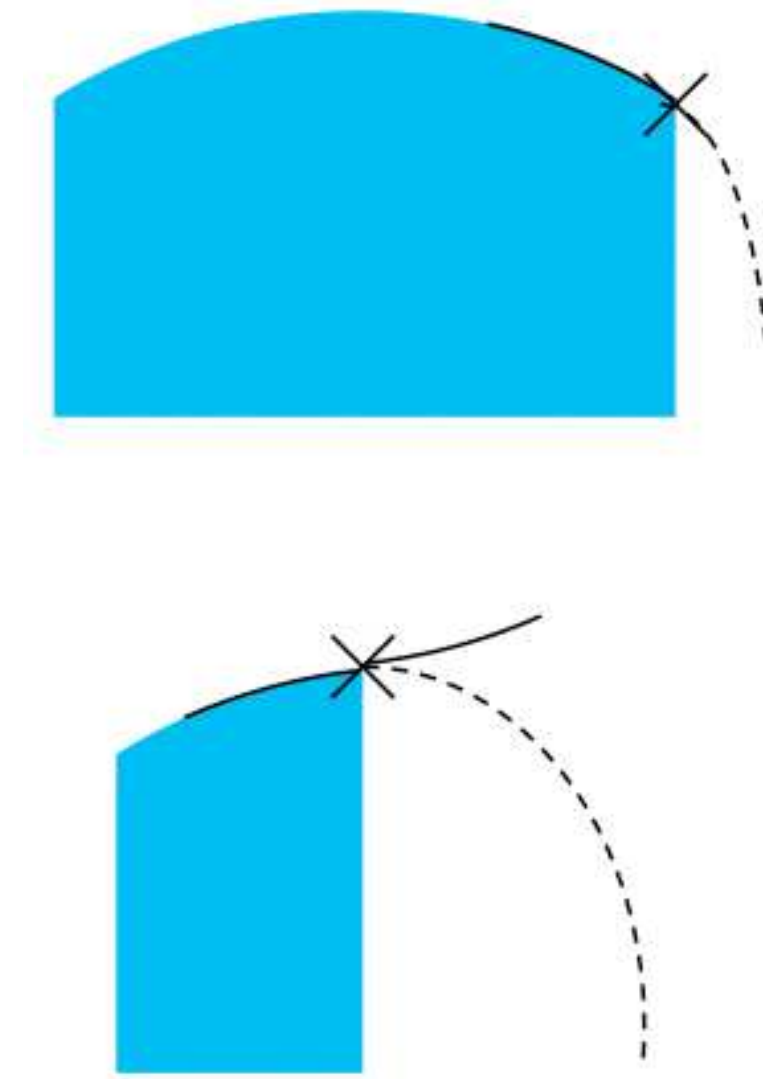


Figure 1: Heuristic extrapolation scheme



# Heuristic Extrapolation

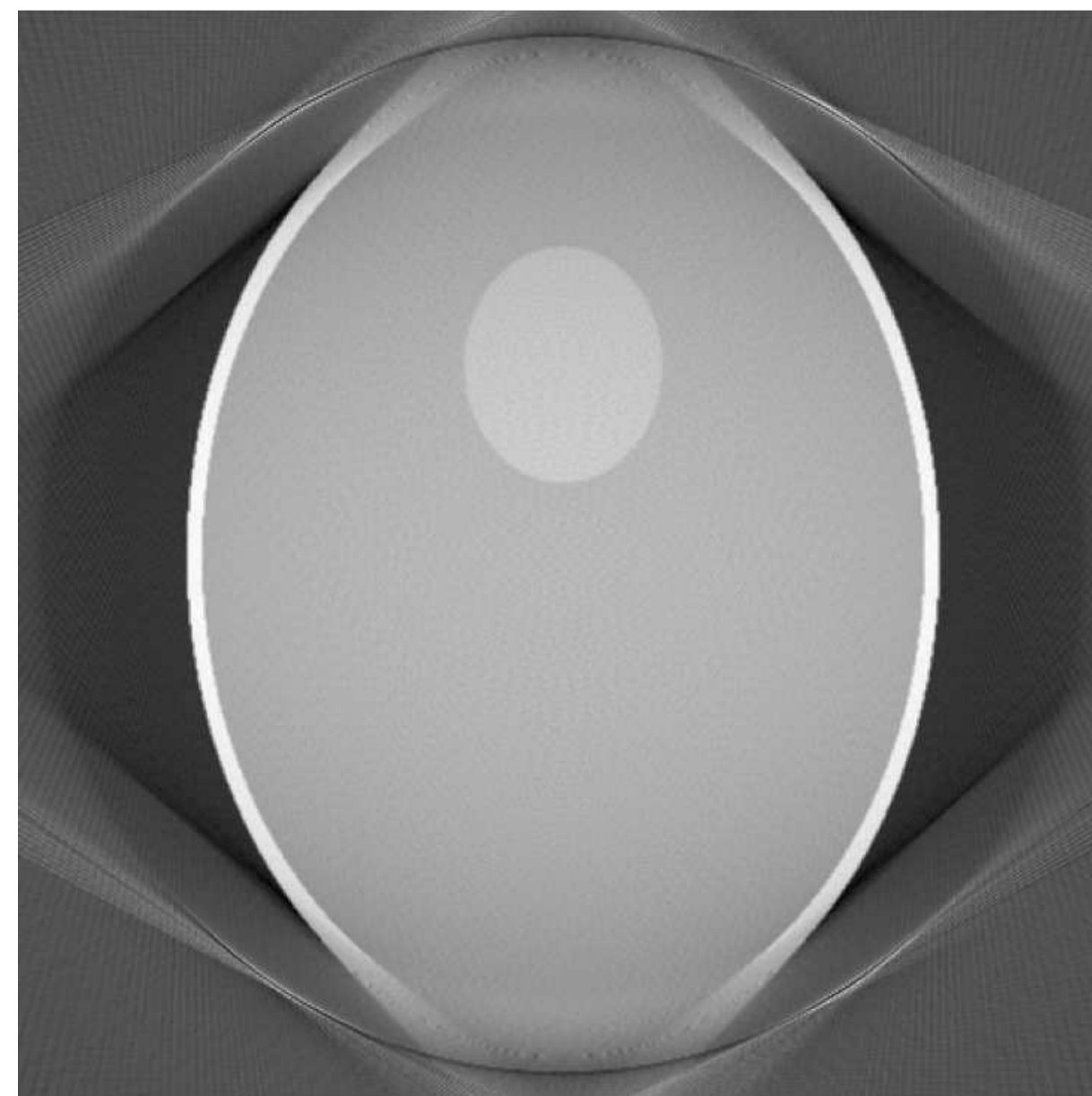
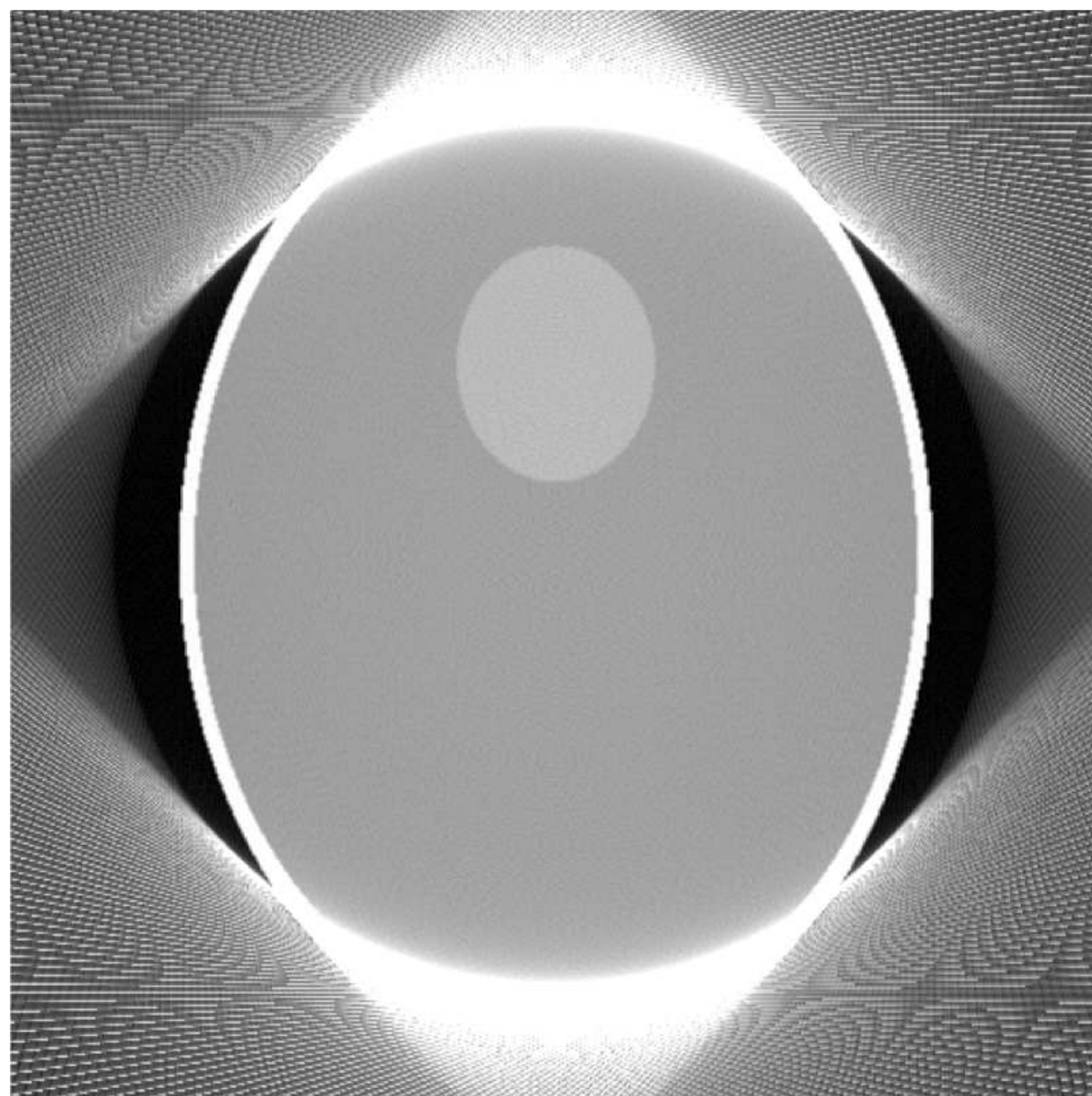


Figure 2: Heuristic extrapolation applied on a phantom

# Water Cylinder Assumption

- Assume that the imaged object consists of water ( $\rho = \rho_{H_2O}$ ).
- Fit water cylinder model to observed data

$$g(\gamma) = 2\rho_{H_2O}\sqrt{R^2 - D^2\sin^2\gamma}.$$

- Use model to extrapolate.

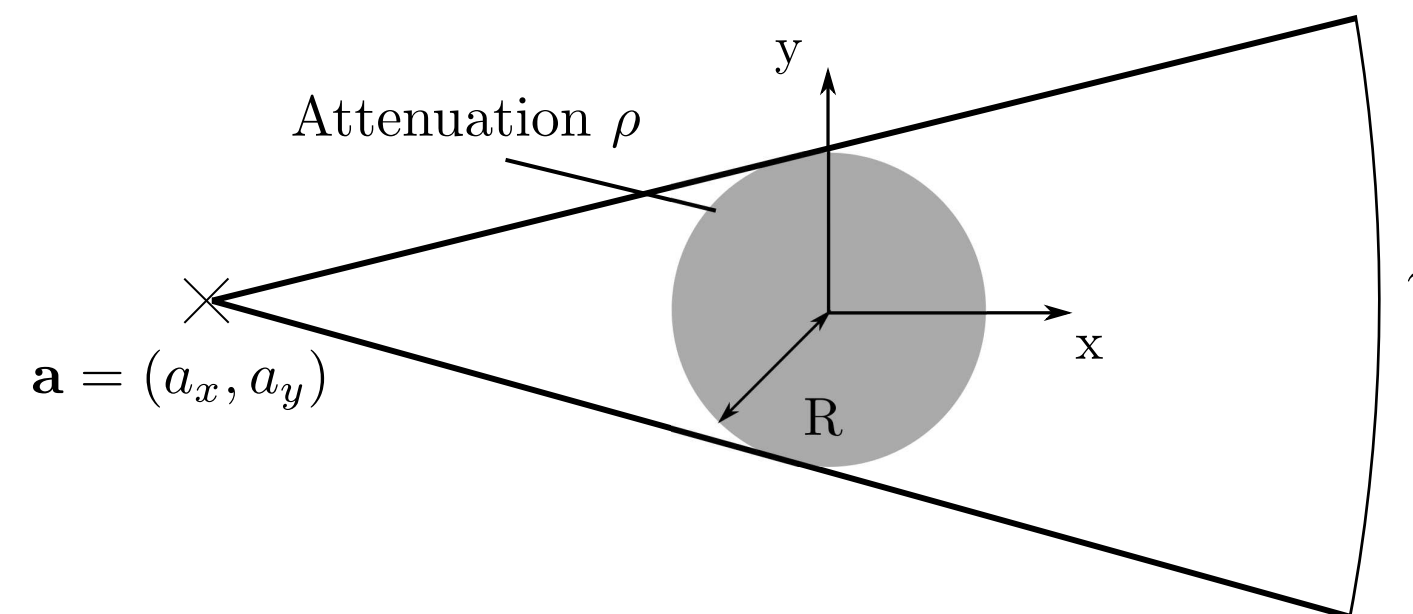


Figure 3: Assume the object to have a shape very similar to a water cylinder.

# Water Cylinder Assumption

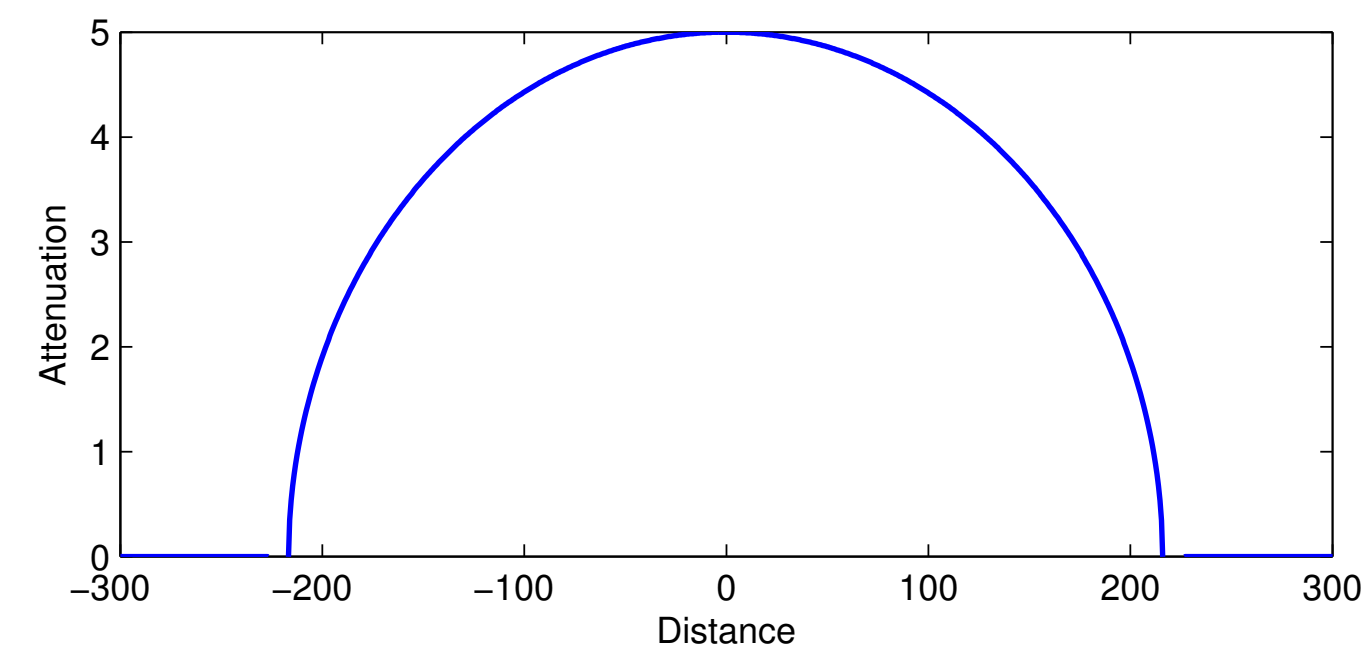
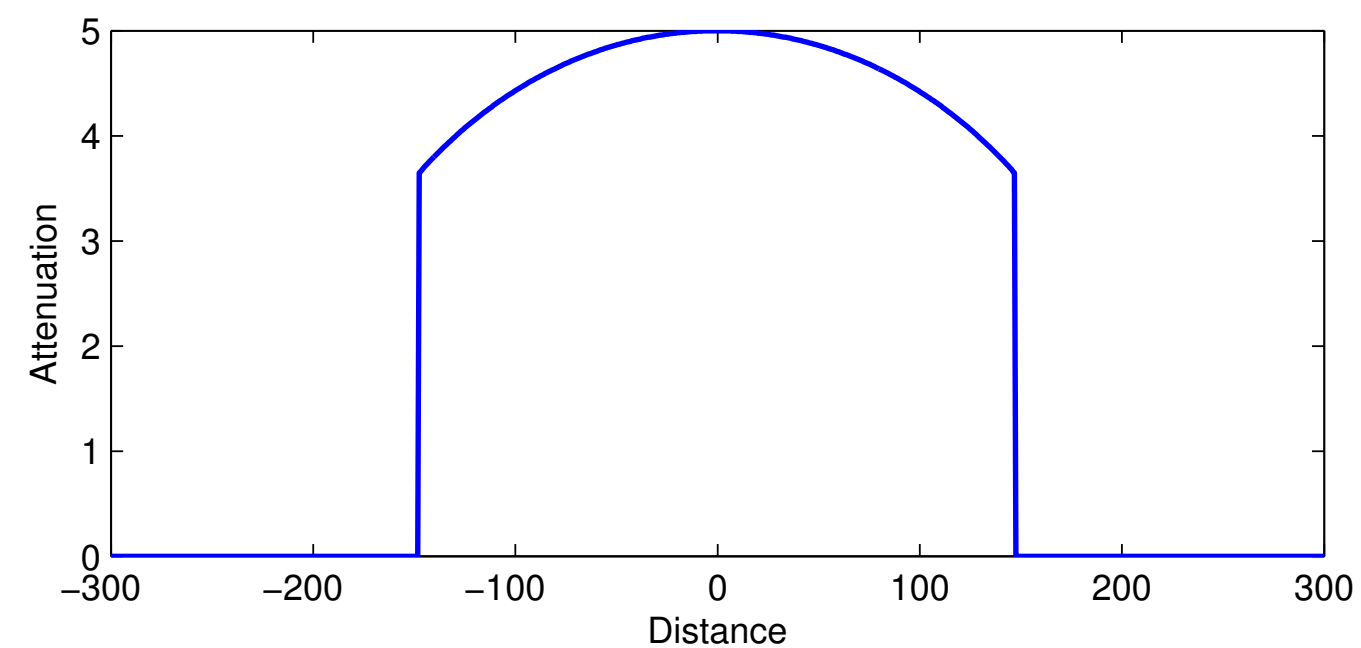


Figure 4: Extrapolate by assuming cylindric shape.



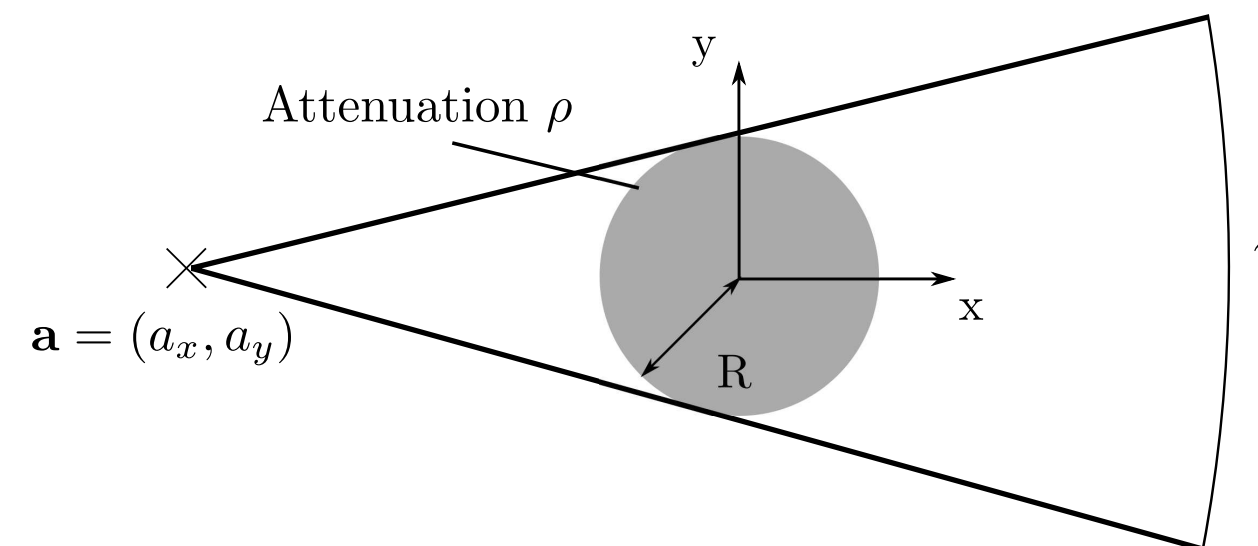
# Water Cylinder Assumption

This approach ...

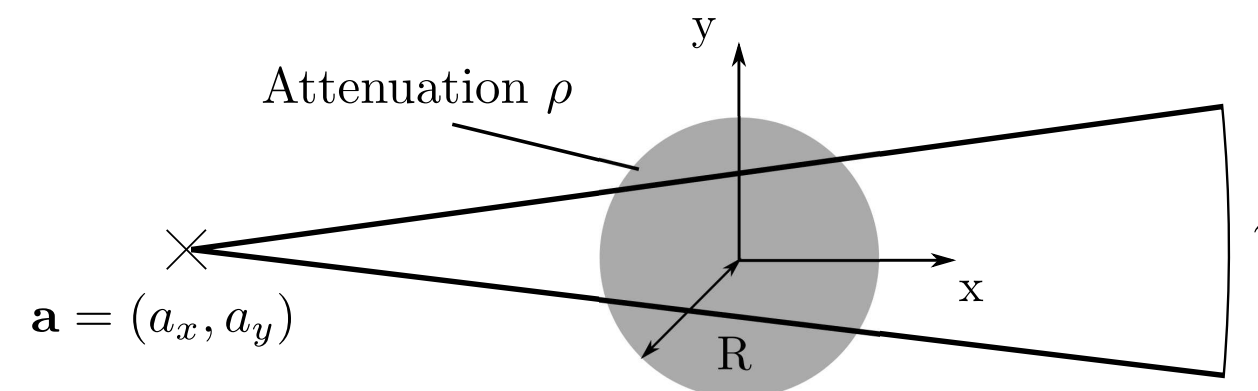
- ... will work perfectly if a water cylinder is imaged.
- ... yields good results for most objects (head, abdomen, etc...).
- ... will yield suboptimal results if the water cylinder assumption is violated (e. g., two cylinders).
- Different versions exist:
  - water ellipsoid assumption,
  - combination with cosine-like roll-off.

# Use of Prior Knowledge

Prior scan (low dose)



Volume-of-interest scan (higher dose)



# Use of Prior Knowledge

- Use data from a first scan to complete the data from a second scan.
- Correction will be perfect if the object did not change.
- One might also use a lower resolution prior scan.
- Movement and deformation of the object have to be compensated.
- This approach is only applicable if a prior scan exists.

# Semi-transparent Filter

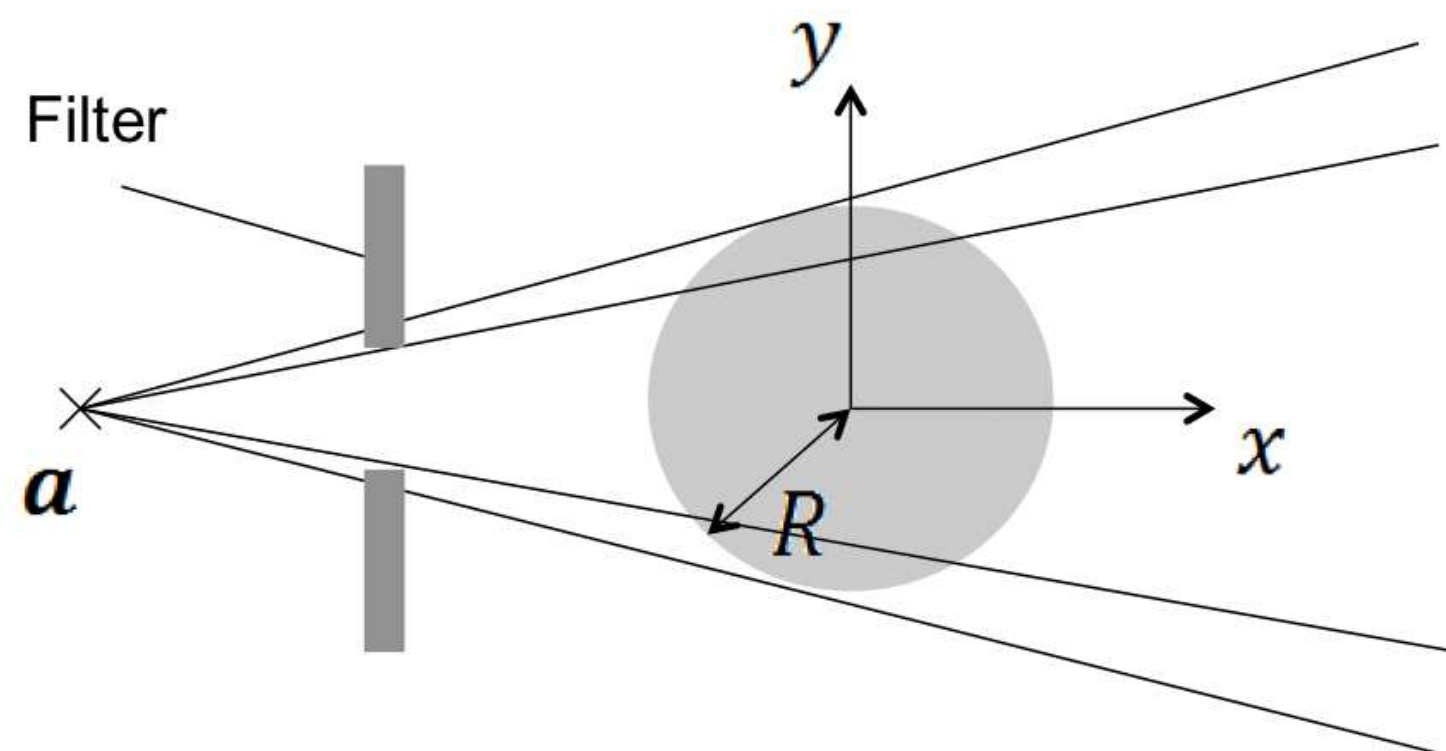
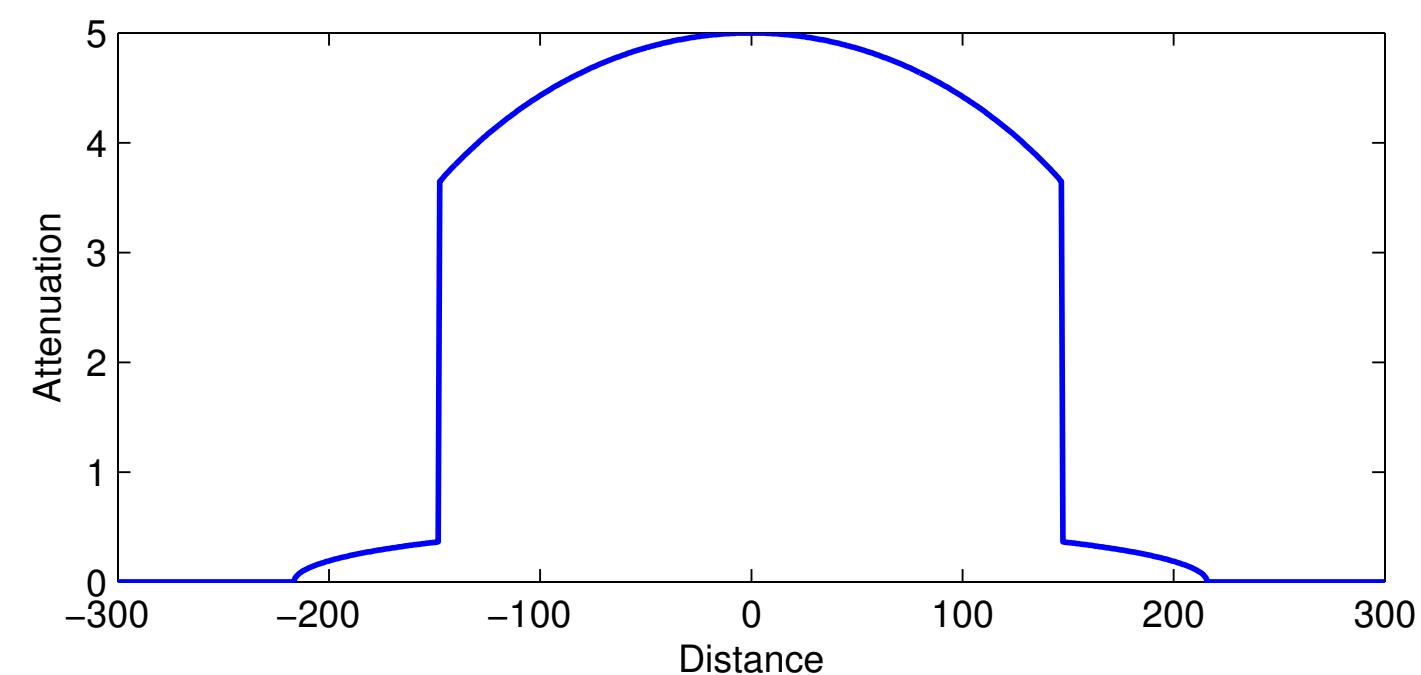
 $\hat{\gamma}$ 

Figure 5: Scheme of a semi-transparent filter: setup (left) and example of a projection result (right)

# Semi-transparent Filter

- Locate filter boundary.
  - Amplify filtered signal to original amplitude.
  - Reduce noise in the amplified signal.
- This yields perfect truncation correction.



# Semi-transparent Filter

## Challenges:

- Filter boundary must be located correctly (which may be influenced by the object).
- Correct amplification factor has to be estimated.
- Method has to be applied carefully in order not to introduce artificial high frequencies.
- Requires additional hardware in the scanner.

# ATTRACT

## Idea:

$$|\omega| = 2\pi i \omega \cdot \left( -\frac{1}{2\pi} i \operatorname{sgn}(\omega) \right) = (2\pi i \omega)^2 \cdot \left( -\frac{1}{4\pi^2} i \frac{\operatorname{sgn}(\omega)}{\omega} \right)$$

The first term is the 2nd order derivative (local), and the right is called residual filter (global).

At the truncation boundaries the 2nd derivative produces a sparse signal. The resulting peaks are filled with zero and then the global filter is applied.

**Remark:** Without further considerations this does not preserve the mean value.

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## Take Home Messages

- Truncation artifacts can be dealt with by extrapolating the projection data at the truncation boundaries.
- We have learned about six methods, which basically divide into
  - estimation of the truncated part,
  - incorporating prior knowledge from earlier scans, or
  - a special hardware setup.
  - filtering during reconstruction.

## Further Readings

Helpful reads for the current unit:

B. Ohnesorge et al. “Efficient Correction for CT Image Artifacts Caused by Objects Extending Outside the Scan Field of View”. In: *Medical Physics* 27.1 (Oct. 2000), pp. 39–46. DOI: [10.1118/1.598855](https://doi.org/10.1118/1.598855)

Frank Dennerlein and Andreas Maier. “Approximate Truncation Robust Computed Tomography–ATTRACT”. In: *Physics in Medicine and Biology* 58.17 (Aug. 2013), pp. 6133–6148. DOI: [10.1088/0031-9155/58/17/6133](https://doi.org/10.1088/0031-9155/58/17/6133)

Yan Xia et al. “Scaling Calibration in Region of Interest Reconstruction with the 1D and 2D ATTRACT Algorithm”. In: *International Journal for Computer Assisted Radiology and Surgery* 9.3 (May 2014), pp. 345–356. DOI: [10.1007/s11548-014-0978-z](https://doi.org/10.1007/s11548-014-0978-z)

L. A. Shepp and Logan B. F. “The Fourier Reconstruction of a Head Section”. In: *IEEE Transactions on Nuclear Science* 21.3 (June 1974), pp. 21–43. DOI: [10.1109/TNS.1974.6499235](https://doi.org/10.1109/TNS.1974.6499235)

W. P. Segars et al. “Realistic CT Simulation Using the 4D XCAT Phantom”. In: *Medical Physics* 35.8 (Aug. 2008), pp. 3800–3808. DOI: [10.1118/1.2955743](https://doi.org/10.1118/1.2955743)