Medical Image Processing for Diagnostic Applications

Fan Beam – Rebinning

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Topics

Parallel Beam to Fan Beam Conversion

Distance Dependent Projections

General Transform

Transform for Equally-spaced Flat Panel Detectors

Parallel Beam to Fan Beam Conversion – Summary

Summary

Take Home Messages
Further Readings







Example: Homogeneous Cylinder

- Source is at position $\boldsymbol{a} = (a_x, a_y)^T$.
- Detector detects rays:

$$g(\boldsymbol{a}, \gamma) = \int_{-\infty}^{\infty} f(a_x + t \cos \gamma, a_y + t \sin \gamma) dt.$$

• Object is bounded by $\{(x,y)|R^2 = (x^2 + y^2)\}.$

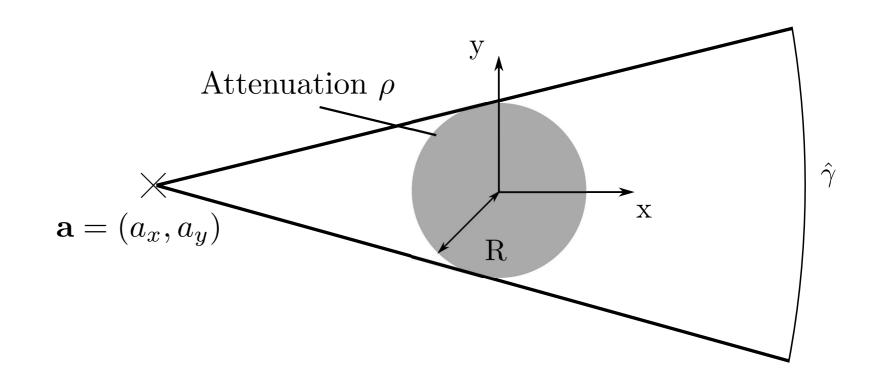


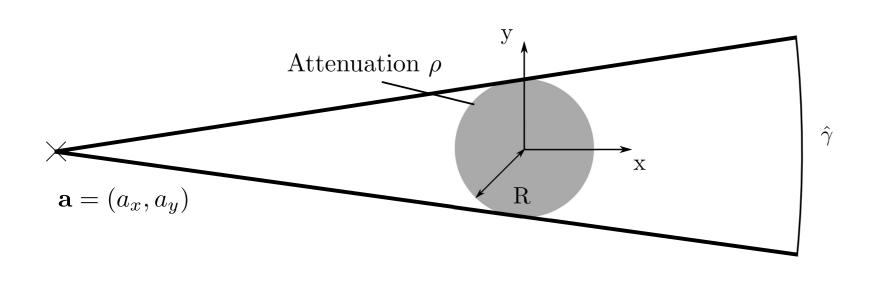
Figure 1: Cross section fan beam projection of a cylinder requires the opening angle $\hat{\gamma}$.







Homogeneous Cylinder: Far Source



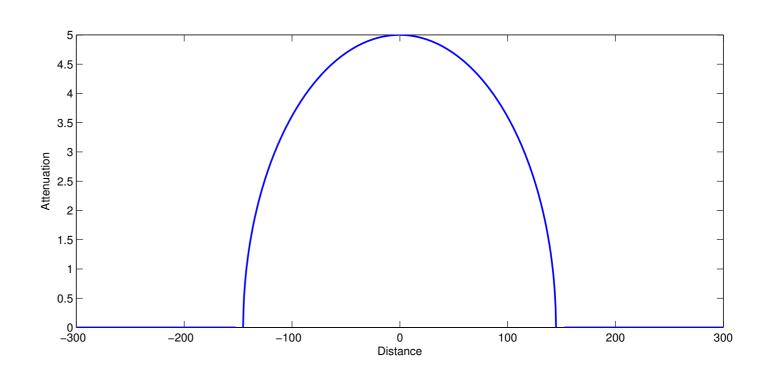


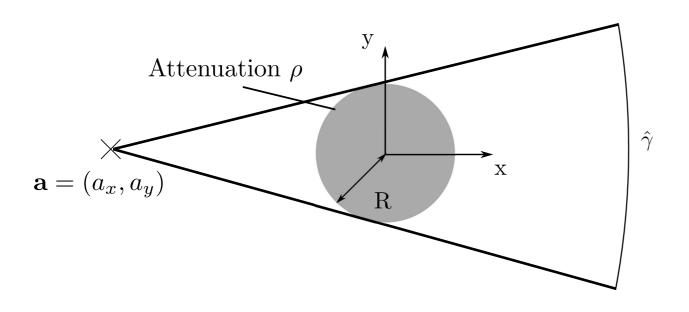
Figure 2: When the object is far from the source (left) its fan beam projection $g(\boldsymbol{a},\gamma), \gamma \in [-\frac{\hat{\gamma}}{2},\frac{\hat{\gamma}}{2}],$ is condensed in a smaller part of the detector (right).







Homogeneous Cylinder: Close Source



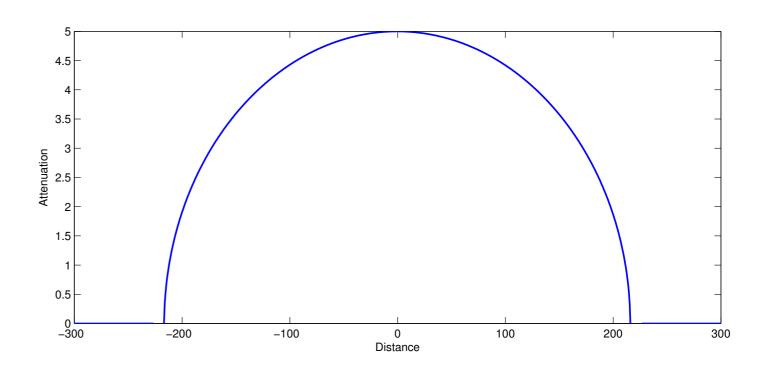
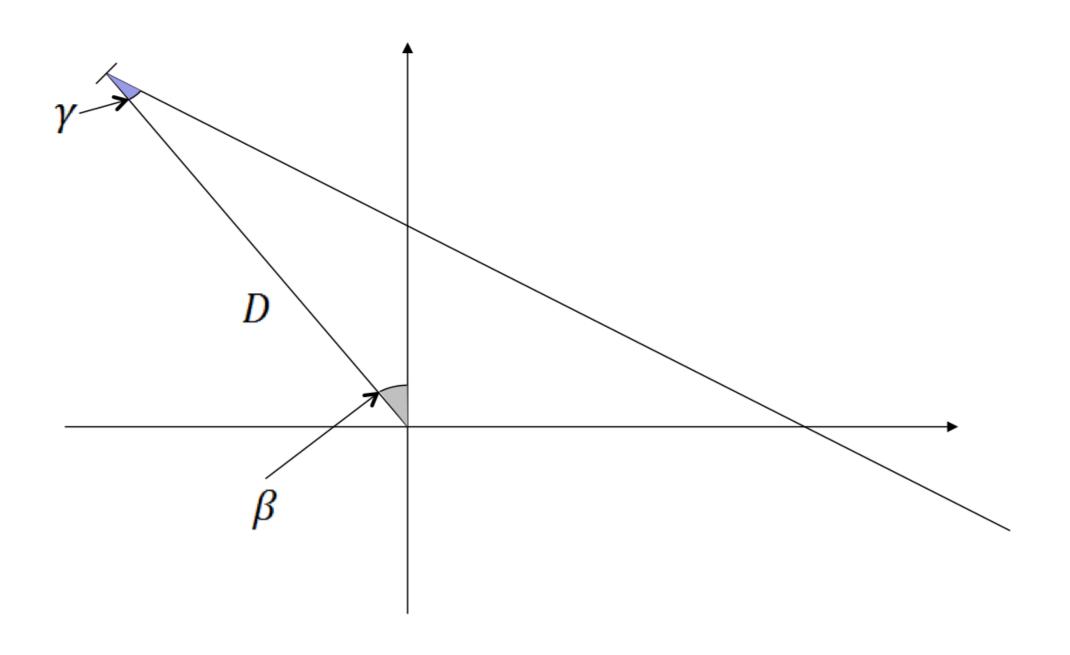


Figure 3: When the same object is closer to the source (left) its fan beam projection $g(\boldsymbol{a}, \gamma), \gamma \in [-\frac{\hat{\gamma}}{2}, \frac{\hat{\gamma}}{2}]$, fills a larger part on the detector (right).









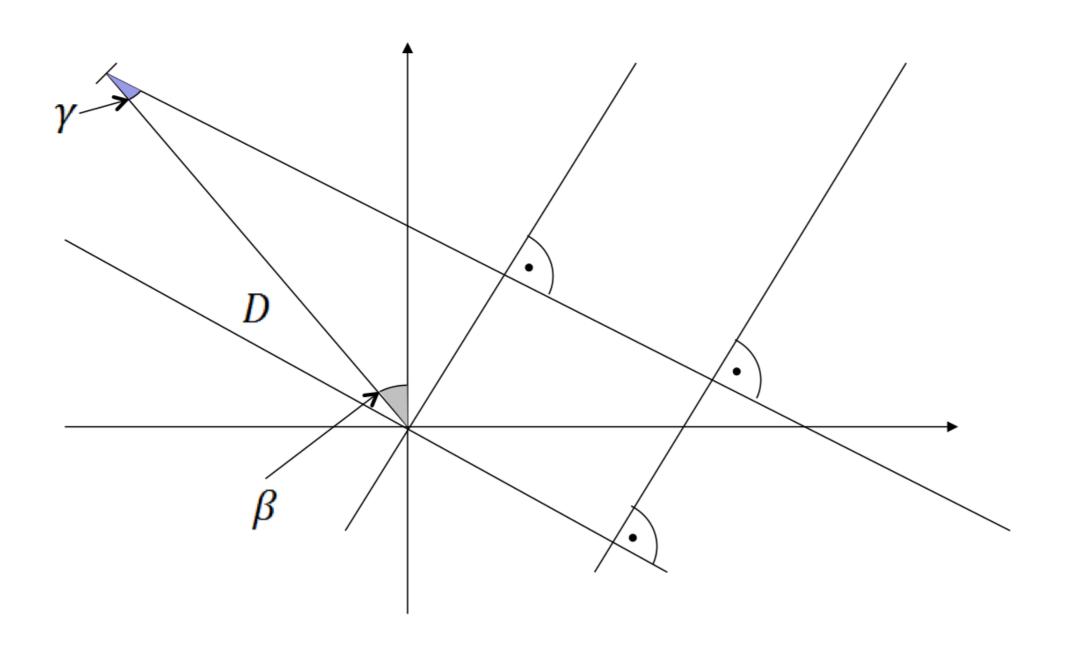
$$\theta = \gamma + \beta$$

$$s = D \sin \gamma$$









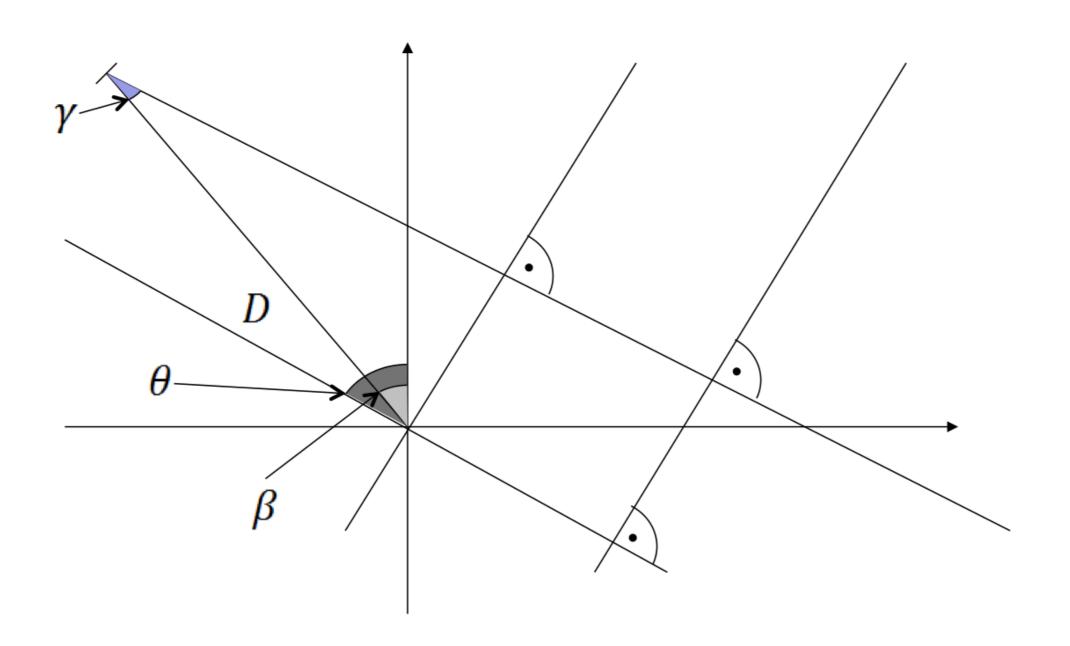
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$$s = D\sin \gamma$$









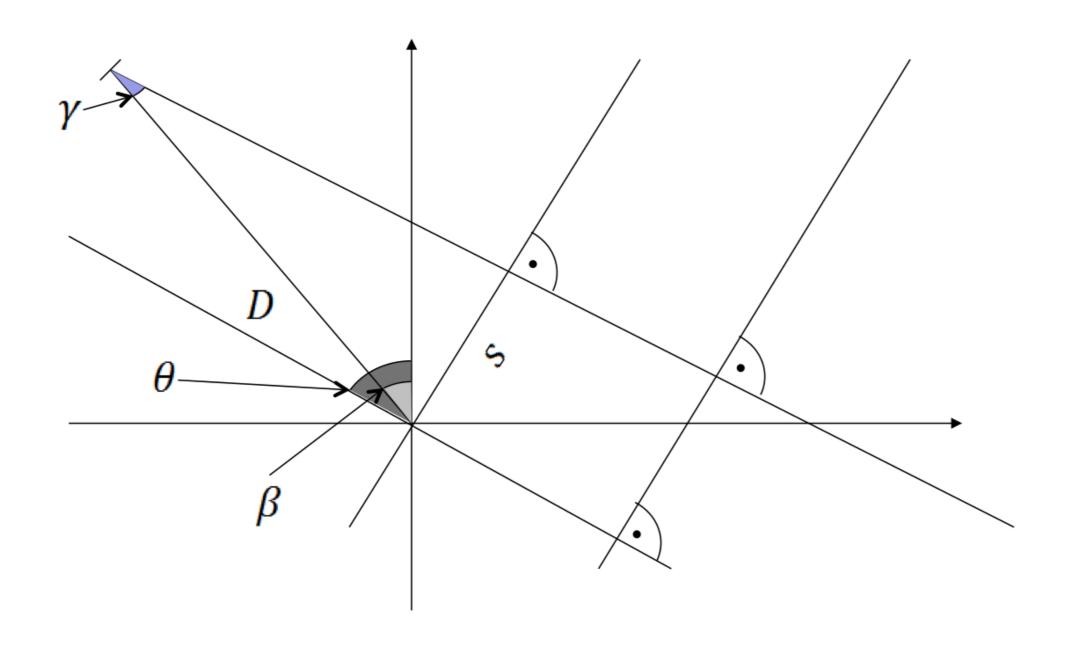
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$$s = D\sin \gamma$$









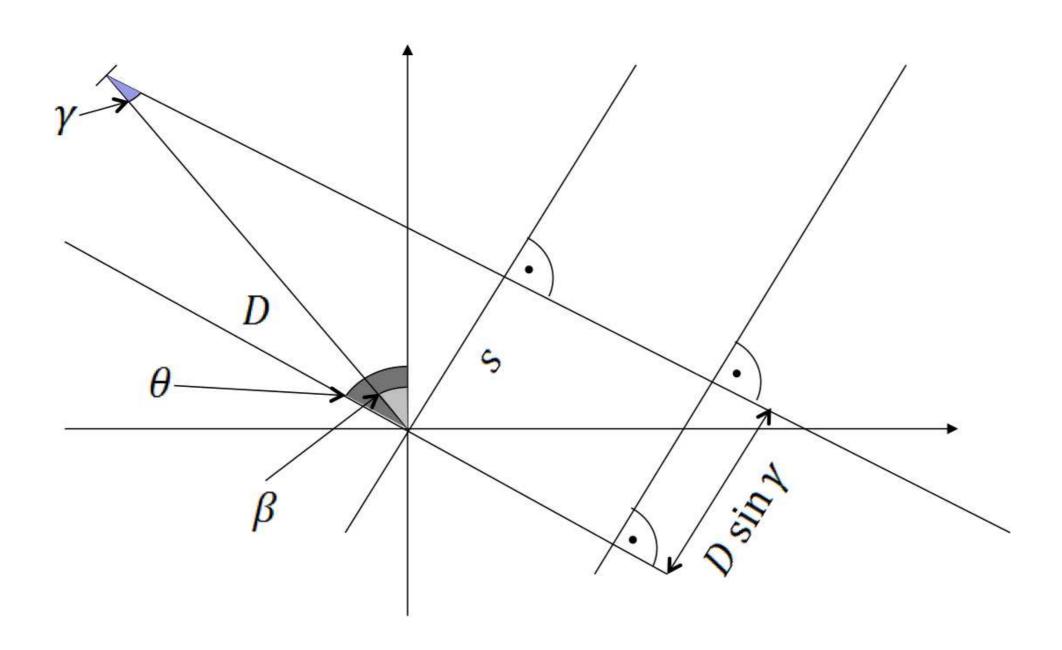
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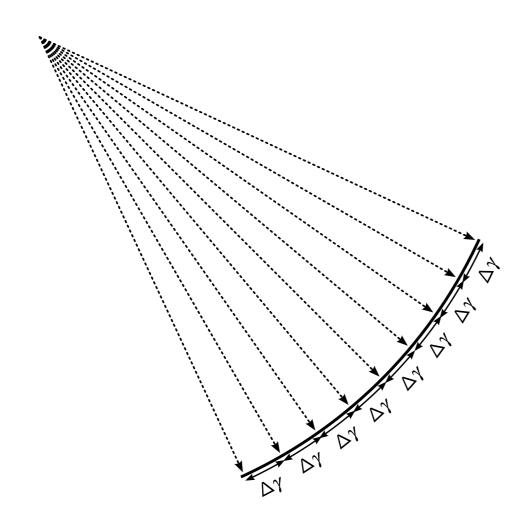






Equally-spaced and Equiangular Detectors

Sampling is different in both detector geometries:



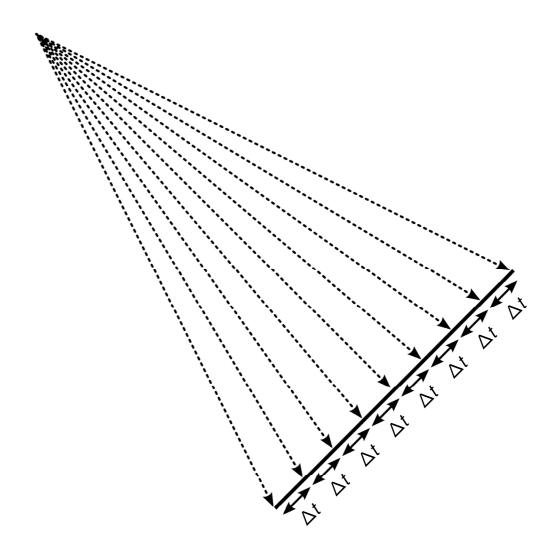


Figure 5: Flat detector with equiangular spacing $\Delta \gamma$ (left), curved detector fan beam with equal spacing Δt (right) (Magdalena Herbst)







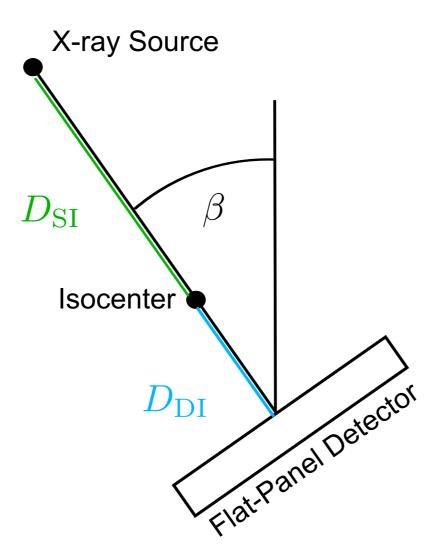


Figure 6: Graphical derivation of the conversion from fan beam to parallel beam geometry for a flat panel detector not centered in the origin. DDI denotes the detector-isocenter distance and D_{SI} is the source-isocenter distance.







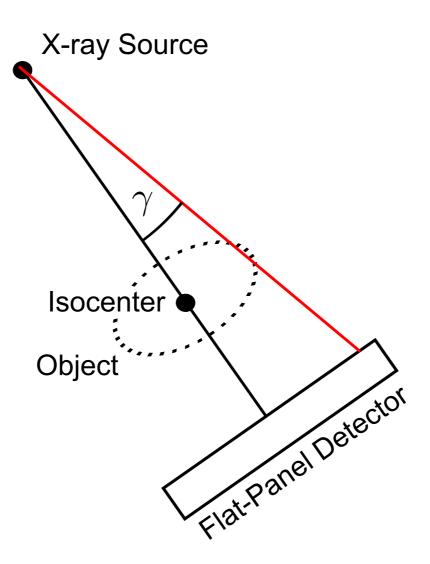


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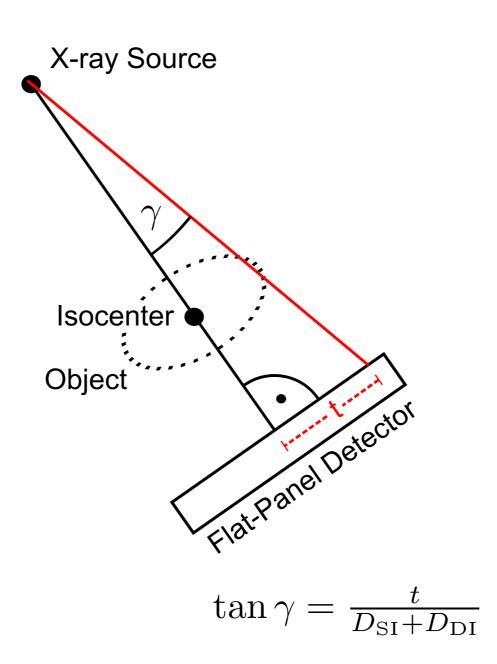


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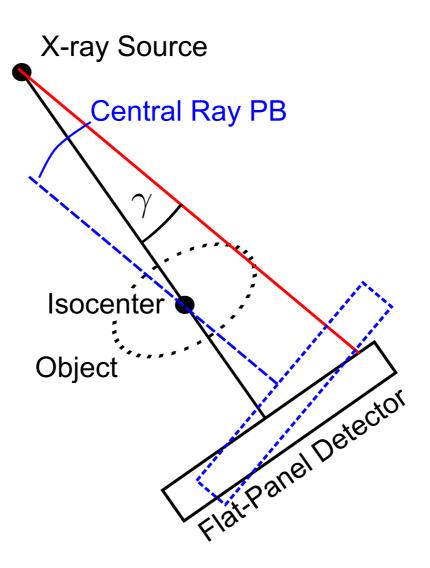


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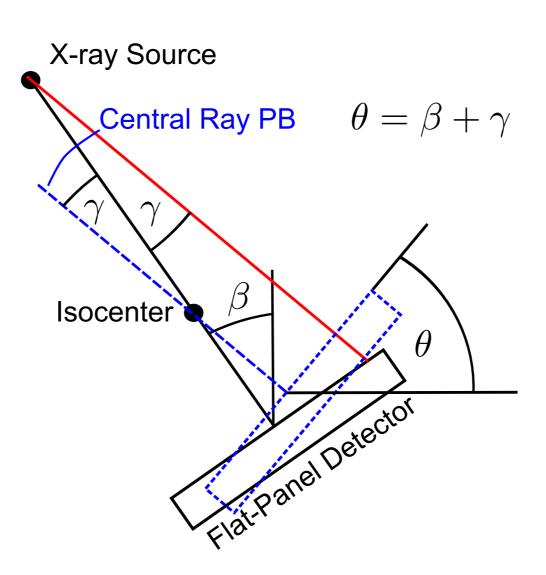


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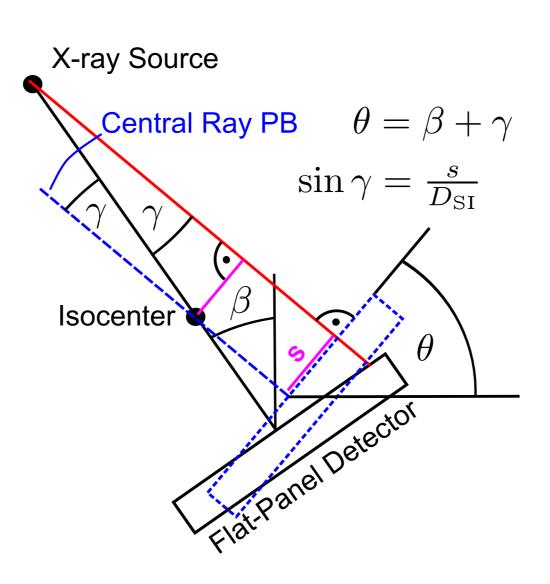


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Parallel Beam to Fan Beam Conversion

• Idea: Find equal rays in both geometries:

$$\theta = \gamma + \beta$$
, $s = D \sin \gamma$.

• Then set:

$$p(s, \theta) = g(\gamma, \beta).$$

• For flat panels these equations hold:

$$heta=eta+rctanrac{t}{D_{ extsf{SI}}+D_{ extsf{DI}}}, \ s=rac{D_{ extsf{SI}}t}{\sqrt{(D_{ extsf{SI}}+D_{ extsf{DI}})^2+t^2}}, \ p(s, heta)=g(t,eta).$$

This process is called *rebinning*.

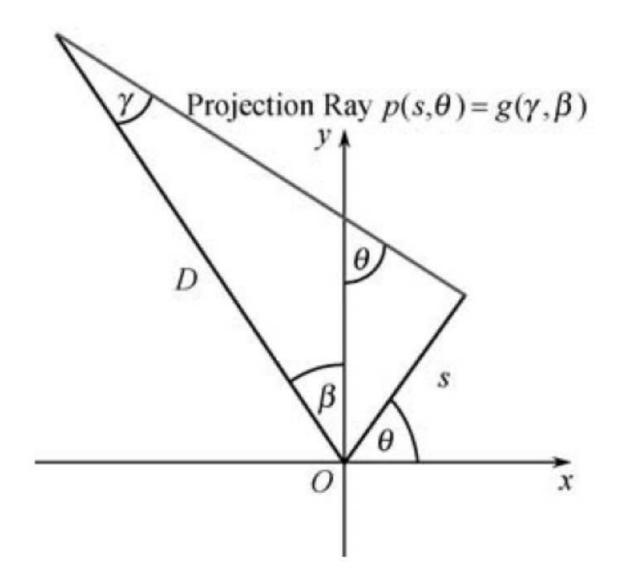


Figure 7: Corresponding rays yield the same projection value (Zeng, 2009).







Parallel Beam to Fan Beam Conversion

- Rebinning is a feasible solution.
- Change of coordinate systems requires interpolation which can introduce inaccuracies.
- Hence, rebinning might not be the method of choice.
- ⇒ Derive a reconstruction method for fan beam data by analytical conversion of the reconstruction algorithm.







Concept for finding a reconstruction algorithm

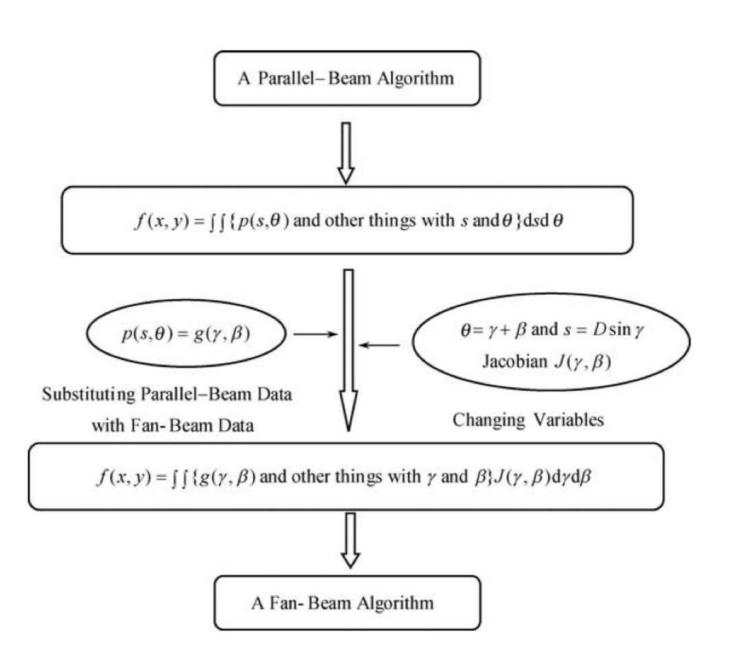


Figure 8: Flow chart showing the steps needed to develop a fan beam reconstruction algorithm (Zeng, 2009).







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- Since the PSFs of fan beam and parallel beam geometry are equal, there is a process called rebinning which transforms one into the other.
- The rebinning concept mainly servers analytical purposes, because interpolation errors make reconstructions inaccurate.
- Fan beam reconstruction is dependent on the distances between source, isocenter and detector, in contrast to parallel beam.
- One has to distinguish flat panel detectors from curved detectors which both are in use.







Further Readings

Helpful reads for the current unit:

Gengsheng Lawrence Zeng. *Medical Image Reconstruction – A Conceptual Tutorial*. Springer-Verlag Berlin Heidelberg, 2010. DOI: 10.1007/978-3-642-05368-9

Ronald N. Bracewell. The Fourier Transform and Its Applications. 3rd ed. Electrical Engineering Series.

Boston: McGraw-Hill, 2000