# **Project Report**

## Information Retrieval (CS60092)

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Breast Cancer Image Retrieval

Group – 18

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#### Abstract:

2 In this project, our aim is to develop an image

3 retrieval system for the early detection and

4 diagnosis of breast cancer. Breast cancer is a

5 common and deadly form of cancer that affects

6 women worldwide, and early detection is crucial

7 in ensuring successful treatment outcomes. The

8 proposed system employs deep learning

9 techniques, specifically convolutional neural

10 networks (CNNs), for the accurate classification

11 of breast cancer images. A content-based image

12 retrieval (CBIR) technique is used to retrieve

13 similar images from the database. The system

14 was evaluated on a dataset of breast cancer

15 images, achieving high accuracy in both

16 classification and retrieval.

## 17 Introduction:

18 Breast cancer image retrieval is a technique used

19 in medical imaging to retrieve and analyze

20 images of breast tissue. It involves the use of

21 computer algorithms and machine learning

22 techniques to analyze and retrieve images of

23 breast cancer. The main purpose of breast cancer 24 image retrieval is to assist physicians in making

25 accurate diagnoses and treatment decisions by

26 providing them with access to large amounts of

27 medical imaging data.

28 Breast cancer image retrieval typically involves

29 several steps, including image acquisition, pre-

30 processing, feature extraction, and image

31 retrieval. During image acquisition, medical

32 imaging technologies such as mammography,

33 ultrasound, and magnetic resonance imaging

34 (MRI) are used to capture images of the breast

35 tissue. These images are then pre-processed to

36 remove any artifacts or noise that may interfere

37 with the analysis

38 Next, feature extraction techniques are used to

39 identify and extract relevant features from the

40 images. These features can include the shape,

41 texture, and intensity of the breast tissue.

42 Machine learning algorithms are then used to

43 analyze these features and generate a set of

44 relevant features that can be used to identify and

45 retrieve similar images.

46 Finally, image retrieval techniques are used to

47 search through a database of medical images and

48 retrieve images that are similar to the ones being

49 analysed. This can be done using a variety of

50 techniques, including similarity-based retrieval

51 and content-based retrieval.

52 Breast cancer image retrieval has the potential to

53 significantly improve the accuracy and speed of

54 breast cancer diagnosis and treatment. By

55 providing physicians with access to large

56 amounts of medical imaging data, they can make

57 more informed decisions about the best course of

58 treatment for each individual patient.

59 In earlier research, Elaheh Mahraban Nejad et al.

60 performed Content Based Medical Image

61 Retrieval on breast cancer images using the

62 BreakHis dataset, utilising the VGG-19 pre-63 trained deep CNN model for feature extraction 64 and Euclidean Distance to determine the 65 similarity distance of the captured images. The 66 highest trial results from the five studies carried 67 out produced a MAP value of 0.80 [5]. Similar 68 research on CBMIR on breast cancer images was 69 carried out by Yun Gu et al. using the BreakHis 70 dataset. The approach used in this study, CNN-71 based Densely-Connected Multi-Magnification 72 Hashing (DCMMH), applies different 73 magnification levels to the applied data, 74 including 40X, 100X, 200X, and 400X. The two 75 techniques, such as low-magnification and high-<sub>76</sub> magnification pictures, are further applied in this 77 work.

78 With an average MAP for each magnification 79 level of 0.95, the test results show that the 80 overall employed methodologies were capable of 81 producing an enhanced accuracy in the picture 82 retrieval task compared to the prior model. On 83 the main-class dataset, this study hardly manages 84 to retrieve any images. Moreover, Yun Gu, et al. 85 conducted a new study in 2019 using the same 86 dataset as the previous one. This study uses this 87 research as its primary source of information. In 88 this study, Yun Gu and colleagues carried out a 89 retrieval technique for the main-class and sub-90 class categories of class datasets. Multi-91 Magnification Correlation Hashing was the 92 technique employed (MMCH) Overall, the main-93 class dataset performance of the suggested 94 technique was satisfactory, with the highest 95 MAP value of 0.9416.

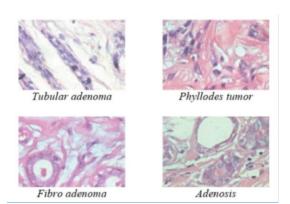
## 96 Datasets

The utilized dataset in this study is BreakHis
dataset retrieved from
https://web.inf.ufpr.br/vri/databases/breastcancerhistopathological-database-breakhis/.
The Breast Cancer Histopathological Database
(BreakHis) is a publicly available dataset of
histopathological images of breast tumor tissues.
The dataset contains 7,909 digitized histological
images of breast tumor tissues, which are
categorized into two main classes: benign and
malignant. The images were obtained from 82
malignants, with each patient having 50 images of
both benign and malignant tumors. The images
were captured at different magnification sizes
were captured at different magnification sizes

112 samples were stained with Hematoxylin and Eosin (H&E).

## 114 Training:

115 In this study, the training process will first start with an image separation method where 80% of the images are used for training, 10% are used 118 for validation, and the remaining 10% are used to measure the retrieval value (test). The CNNbased Autoencoder method will be used in this 121 study to transform the original image into a reconstructed image through the 2 phases of 123 encoder and decoder. The encoder network will take in the input image and progressively reduce 125 its dimensions by applying convolutional layers 126 followed by pooling layers. The number of 127 convolutional and pooling layers, as well as their parameters, will depend on the specific dataset and problem at hand. The encoder network will 130 end with a bottleneck layer that will represent the 131 compressed representation of the input image. 132 The decoder network will take the compressed 133 representation from the encoder network and 134 reconstruct the original image by applying deconvolutional layers followed by upsampling 136 layers. The number of deconvolutional and upsampling layers, as well as their parameters, will depend on the specific dataset and problem at hand. The decoder network will end with a 140 reconstruction layer that will output the 141 reconstructed image. The two networks will be 142 connected such that the output of the encoder 143 network will serve as the input to the decoder 144 network. The loss function for the autoencoder will be the difference between the original and reconstructed images, and the model will be trained using backpropagation to minimize this loss. The hyperparameters of the model, such as the learning rate, batch size, and number of 150 epochs, will need to be optimized through experimentation to achieve the best performance.



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Figure 1: Example of Benign Tumor Image

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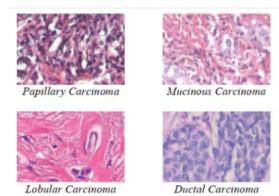


Figure 2: Example of Malignant Tumor Image

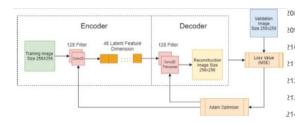


Figure 3: Flow of Training Stages

164 At the encoder stage, the input data will be 165 converted into smaller dimensions or also entitled as compression, which in this study will be converted into a latent dimension with a size of 48 nodes by using Conv2D(2D Convolution 169 Layer). Conv2D layer generates a tensor of 170 outputs by convolving a convolution kernel with the layer input, in this study two modified default parameter were used. The first one is strides, 173 stride is set to 2 for striding of the convolution along the height and width, another one is using "same" padding value which mean padding convolution with zero values is evenly distributed to the left/right or up/down of the input, resulting in output with the same height or width dimension as the input. The number of 180 filters used is 128 with a size of 3 X 3 pixels. LeakyReLU is a popular activation function used in many deep learning models, including CNNbased autoencoder applications for breast cancer image retrieval. The LeakyReLU activation function, which adds a slight slope to the negative part of the function, is a variation on the 187 ReLU (Rectified Linear Unit) activation 188 function. By doing this, it is possible to prevent the "dying ReLU" problem, which can happen

190 when the ReLU function becomes frozen at zero

for negative inputs, resulting in the disappearance of the gradient and slowing down the training process. The LeakyReLU function is defined as: f(x) = x for x > 0 f(x) = ax for x <= 0 where a is a small positive constant, typically set to 0.01 remove back ground color.

In a CNN-based autoencoder application for breast cancer image retrieval, the LeakyReLU activation function is commonly used in the convolutional layers of the encoder and decoder. This helps to introduce non-linearity into the model, allowing it to capture more complex patterns in the data. The LeakyReLU function is also computationally efficient, making it suitable for use in large-scale models with many layers.

The decoder uses the same convolution method 209 configuration as the encoder, which uses 128 210 filters with a 3 X 3-pixel filter size and the same activation function processed differently. Data 212 from the latent dimension is transposed by the decoder into the reconstructed image. The stage moves on to the error calculation and optimization phase when the encoder and decoder stages are finished. At this point, each iteration of the process involves calculating the loss for each function to see which has the lowest 219 loss value. Mean Square Error serves as the 220 study's loss function (MSE). The MSE measures 221 the average squared difference between the 222 predicted output and the actual target output, and 223 is defined as:

 $_{224}$  MSE =  $(1/N) * \sum (y - \hat{y}) ^2$ 

226 Where N= number of samples of dataset y= actual target output  $\hat{y}=$  predicated output

The goal of the model is to minimize the MSE loss by adjusting the model parameters through backpropagation and gradient descent. By minimizing the MSE loss, the model is able to generate high-quality reconstructed images that closely resemble the original input images. This is important in breast cancer image retrieval, where accurate and detailed images are necessary for accurate diagnosis and treatment.

#### **Feature Extraction**

The encoder part of the autoencoder handles feature extraction. Convolutional layers in the encoder component apply filters to the input image to extract features at different levels of 246 set of feature maps that indicate whether or not 247 specific visual patterns are present in the image. 249 a pooling layer that decreases their spatial 250 dimensions and a non-linear activation function, such as ReLU, that incorporates non-linearity into 252 the feature representation. The final step is to flatten the resulting feature vectors and feed them into a fully connected layer, which converts them into a representation of a lower-dimensional latent

## **Replacing AE with VAE:**

VAEs model the latent space as a probabilistic 260 distribution, typically a Gaussian distribution, as opposed to a deterministic latent space in AEs 262 providing a more robust and flexible <sup>263</sup> representation of the data, allowing for better 264 handling of uncertainty and generating more diverse samples. VAEs are capable of generating new samples by sampling from the latent space. This allows for creative exploration of the data distribution and generation of novel data points that may not be present in the original dataset. VAEs employ a regularization term in their loss function, known as the Kullback-Leibler (KL) 272 divergence, which encourages the learned latent 273 space to follow a specific distribution (e.g., Gaussian). This helps in preventing overfitting and encourages the model to learn meaningful 276 representations of the data.

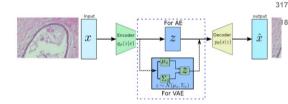


Figure 4: Overview of AE and VAE

#### **Using ImageNet model head as Encoder:**

Current SOTA model uses only one layered CNN model as an encoder. This limits the learning capability of the encoder considering the images size used is 256x256. To increase the complexity of encoder we use SOTA ImageNet models such as Swin Transformer, DenseNet, EfficientNet, 288 ResNet as encoders by removing the classification 289 layer. To match the complexity of encoder and 290 decoder we increase the number of layers/stages of 323 <sup>291</sup> Conv + Upsample Layers in decoder till we reach <sup>324</sup> Figure 7: Precision Comparison for all experiments

245 abstraction. Each layer of convolution generates a 292 the comparable model complexity. For our task we 293 have replaced 1 stage Conv + Upsample network <sup>294</sup> with 4 stage Conv + Upsample layers. Considering <sup>248</sup> Following this, these feature maps are subjected to <sup>295</sup> our dataset is entirely different from ImageNet we 296 didn't use any pretrained weights before training.

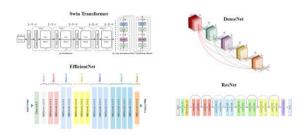


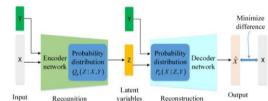
Figure 5: Various ImageNet models

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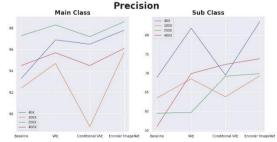
# **Conditioning Encoder and Decoder with**

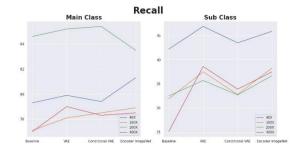
303 Conditional Variational Autoencoders (CVAEs) are 304 a variant of Variational Autoencoders (VAEs) that 305 incorporate additional conditional information 306 during training. CVAEs learn a probabilistic latent 307 space that is conditioned on the input conditions, which allows for a more meaningful and structured 309 representation of the data. This can result in better 310 disentanglement of the factors of variation in the 311 data, making CVAEs suitable for tasks such as 312 disentangled representation learning, style transfer, and data manipulation. We have used embedding 314 layer followed by flattening it's output to convert a 315 label to 48D embedding. Later this embedding is 316 concatenated with encoder output. Finally a FC Layer is added on top of match the original AE's encoder's feature vector dimension.



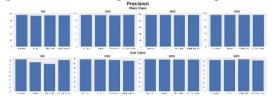
320 Figure 6: Conditional VAE

#### 322 Results:

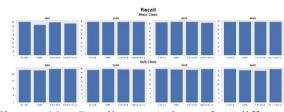




327 Figure 8: Recall Comparison for all experiments



330 Figure 9: Precision comparison for different ImageNet encoders



comparison for different Figure 10: Recall 335 ImageNet encoders

#### 337 Observations:

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338 From Figure 7 and 8 we can clearly see that for 339 both main class and sub class level ImageNet encoder approach gave best results vol. 357, pp. 1–10, 2019. 342 in-terms of both Precision and Recall. Figure 393 344 different **ImageNet** encoders ResNet, 345 Transformer, 347 almost the same with slight difference in 398 Technology (ICCCT), 2012, pp. 1010–1015. 348 performance. By considering the average 399 349 Precision and Recall for all the experiments 400 350 varying class level and magnifications, 351 DenseNet outperformed other ImageNet 402

#### 354 References:

352 encoders.

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355 [1] Z. Liu et al., 'Swin Transformer: Hierarchical 406 Vision Transformer using Shifted Windows', 407 357 CoRR, vol. abs/2103.14030, 2021.

[2] G. Huang, Z. Liu, and K. O. Weinberger, 'Densely Connected Convolutional Networks', CoRR, vol. abs/1608.06993, 2016.

[3] K. He, X. Zhang, S. Ren, and J. Sun, 'Deep Residual Learning for Image Recognition', CoRR, vol. abs/1512.03385, 2015.

367 [4] D. P. Kingma and M. Welling, 'Auto-Encoding Variational Bayes', arXiv [stat.ML]. 2022.

370 [5] A. E. Minarno, K. M. Ghufron, T. S. Sabrila, L. 371 Husniah, and F. D. S. Sumadi, 'CNN Based 372 Autoencoder Application in Breast Cancer Image 373 Retrieval', in 2021 International Seminar on 374 Intelligent Technology and Its Applications 375 (ISITIA), 2021, pp. 29-34.

377 [6] L. Wei, Y. Yang, and R. M. Nishikawa, 378 'Microcalcification classification assisted by 379 content-based image retrieval for breast cancer 380 diagnosis', Pattern Recognition, vol. 42, no. 6, pp. 381 1126–1132, 2009.

383 [7] Y.-L. Huang, D.-R. Chen, and Y.-K. Liu, 'Breast 384 cancer diagnosis using image retrieval for different 385 ultrasonic systems', in 2004 386 Conference on Image Processing, 2004. ICIP '04., 387 2004, vol. 5, pp. 2957-2960 Vol. 5.

[8] R. S. Bressan, P. H. Bugatti, and P. T. M. Saito, 390 'Breast cancer diagnosis through active learning in classifications irrespective of magnifications, 391 content-based image retrieval, Neurocomputing,

9, 10 shows precision and recall scores of 394 [9] J. Zhou, C. Feng, X. Liu, and J. Tang, 'A texture (Swin 395 features based medical image retrieval system for DenseNet, 396 breast cancer', in 2012 7th 346 EfficientNet). All the encoders performed 397 Conference on Computing and Convergence

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## **Work Distribution:**

Name	Work
D G Pranathi (19CS10025)	
	<ul> <li>Wrote the necessary code and scripts to carry out the experiments.</li> <li>Tested and validated the code to ensure accuracy and reliability of results.</li> <li>Analyzed the data obtained from the experiments to draw meaningful conclusions.</li> </ul>
Sonu Kumar Yadav (20CS10061)	Conducted thorough research on the assigned topic.
	<ul> <li>Helped Bhagoti in Report making.</li> </ul>
	<ul> <li>Ensured that the report adhered to the guidelines of the ARR format.</li> </ul>
Bhagoti (20CS30010)	<ul> <li>Conducted thorough research on the assigned topic.</li> <li>Gathered information from reliable sources.</li> <li>Compiled the findings into a well-structured</li> </ul>
	report.