

# Single-molecule analysis of fluorescently labeled G-protein–coupled receptors reveals complexes with distinct dynamics and organization

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**G-protein–coupled receptors (GPCRs) constitute the largest family of receptors and major pharmacological targets. Whereas many GPCRs have been shown to form di-/oligomers, the size and stability of such complexes under physiological conditions are largely unknown. Here, we used direct receptor labeling with SNAP-tags and total internal reflection fluorescence microscopy to dynamically monitor single receptors on intact cells and thus compare the spatial arrangement, mobility, and supramolecular organization of three prototypical GPCRs: the  $\beta_1$ -adrenergic receptor ( $\beta_1$ AR), the  $\beta_2$ -adrenergic receptor ( $\beta_2$ AR), and the  $\gamma$ -aminobutyric acid ( $\text{GABA}_B$ ) receptor. These GPCRs showed very different degrees of di-/oligomerization, lowest for  $\beta_1$ ARs (monomers/dimers) and highest for  $\text{GABA}_B$  receptors (prevalently dimers/tetramers of heterodimers). The size of receptor complexes increased with receptor density as a result of transient receptor–receptor interactions. Whereas  $\beta_1$ -/ $\beta_2$ ARs were apparently freely diffusing on the cell surface,  $\text{GABA}_B$  receptors were prevalently organized into ordered arrays, via interaction with the actin cytoskeleton. Agonist stimulation did not alter receptor di-/oligomerization, but increased the mobility of  $\text{GABA}_B$  receptor complexes. These data provide a spatiotemporal characterization of  $\beta_1$ -/ $\beta_2$ ARs and  $\text{GABA}_B$  receptors at single-molecule resolution. The results suggest that GPCRs are present on the cell surface in a dynamic equilibrium, with constant formation and dissociation of new receptor complexes that can be targeted, in a ligand-regulated manner, to different cell-surface microdomains.**

live cell imaging | protein–protein interactions

**G**-protein–coupled receptors (GPCRs) constitute the largest family of cell-surface receptors and important pharmacological targets (1). Whereas research performed over the past 30 y has revealed in great detail the basic mechanisms and kinetics of GPCR signaling (1, 2), fundamental aspects, such as receptor di-/oligomerization or G-protein coupling and dissociation, remain controversial, mostly due to technical limitations to directly observe these phenomena (3–5).

Although GPCRs were initially thought to be monomeric, evidence accumulated over the past two decades suggests that they can form dimers or oligomers in intact cells (6–10). In a few cases, such as the  $\gamma$ -aminobutyric acid type B ( $\text{GABA}_B$ ) receptor and other family-C GPCRs, di-/oligomerization is essential for receptor function (10–12). It is now well established that functional  $\text{GABA}_B$  receptors consist of a  $\text{GABA}_{B1}$  subunit (which binds GABA but cannot activate G proteins) and a  $\text{GABA}_{B2}$  subunit (which is binding deficient but can signal to G proteins) (10–12). Interestingly, heterodimerization of  $\text{GABA}_{B1}$  with  $\text{GABA}_{B2}$  masks an endoplasmic reticulum retention signal on the C-terminal tail of  $\text{GABA}_{B1}$ , and this is required for  $\text{GABA}_{B1}$  to reach the cell surface (10–12). For family-A GPCRs, the situation is more controversial, even for well-studied members such as the  $\beta_1$ -adrenergic receptor ( $\beta_1$ AR) and the  $\beta_2$ -adrenergic receptor ( $\beta_2$ AR) (6–10). For instance,  $\beta_2$ ARs have been suggested to be

monomers (13), constitutive dimers (14, 15), or higher-order oligomers (16). Similarly,  $\beta_1$ ARs have been suggested to form either stable (15) or transient interactions (16). Moreover, whereas the di-/oligomerization of family-A GPCRs has been proposed to play roles in receptor trafficking (17) and/or signaling (18), it is apparently not required for receptor function (19–21). The current uncertainty on these topics calls for new methods capable of directly monitoring the size and stability of GPCR supramolecular complexes at physiological expression levels in living cells.

Evidence for GPCR di-/oligomerization has been mostly obtained with biochemical methods or with biophysical techniques, such as resonance energy transfer (RET) (6–10). Compared with biochemical methods, fluorescence resonance energy transfer (FRET) and bioluminescence resonance energy transfer (BRET) have the advantage of analyzing GPCR di-/oligomerization in intact cells. However, even though these methods have provided important insights on GPCR di-/oligomerization, they are based on average proximity measurements and usually require high receptor expression levels. Moreover, an intense debate arose a few years ago on the possible occurrence of RET due to random collisions (13, 22, 23).

Besides BRET and FRET, other optical methods have been proposed to study protein–protein interactions in living cells (4, 16, 24, 25). Of these, single-molecule microscopy has the great potential of directly observing the state and behavior of individual proteins. Interestingly, two recent single-molecule microscopy studies using fluorescent ligands showed dynamic dimerization of M1 muscarinic and *N*-formyl peptide receptors (26, 27).

Here, we used the SNAP-tag technology (28) to directly label cell-surface GPCRs with small organic fluorophores and visualize individual receptors on the surface of living cells by total internal reflection fluorescence microscopy (TIRF-M). Three prototypical GPCRs, i.e., the  $\beta_1$ AR, the  $\beta_2$ AR (both family-A GPCRs), and the  $\text{GABA}_B$  receptor (family C), which are implicated in fundamental physiological processes such as heart contraction and neurotransmission and represent major pharmacological targets, were analyzed. This allowed us to precisely monitor over time and thus accurately compare the spatial arrangement, mobility, and supramolecular organization of these GPCRs, both under basal conditions and after agonist stimulation.

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## Results

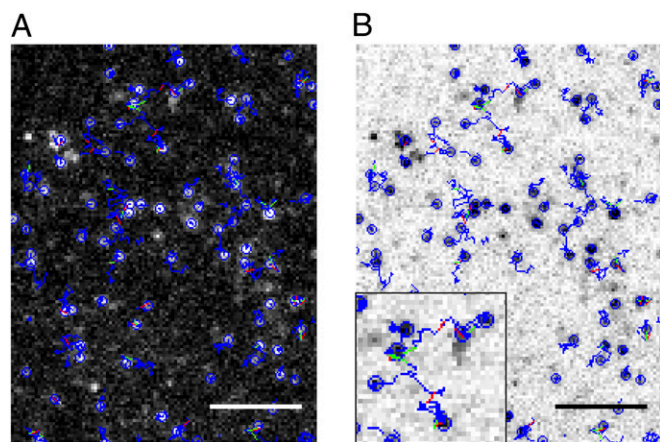
**Validation of Single-Molecule Analysis.** To directly and efficiently label cell-surface GPCRs with a bright fluorophore, we used the SNAP-tag (28). The SNAP-tag is a 20-kDa protein derived from the enzyme *O*<sup>6</sup>-alkylguanine-DNA alkyltransferase (AGT), which can be fused to a protein of interest and covalently labeled with fluorescent benzylguanine (BG) derivatives. We initially calibrated the method, using single molecules of the cell-impermeant Alexafluor 647 BG derivative (Alexa647-BG) spotted on glass coverslips that were imaged by TIRF-M (*SI Results* and Fig. S1).

Then, we evaluated the possibility of using the SNAP method to visualize single cell-surface proteins in living cells. A construct coding for a monomeric cell-surface receptor, CD86 (16), with an N-terminal SNAP-tag (SNAP-CD86) was used. After transfection of CHO cells with this construct, labeling with saturating concentrations of Alexa647-BG produced a highly specific staining (Fig. S2). When low-expressing cells were visualized by TIRF-M, individual fluorescent particles were visible in SNAP-CD86-transfected (Fig. S2 and Movie S1) but not in mock-transfected cells. Particles were automatically detected and tracked with algorithms developed by Jaqaman et al. (29). This analysis was able to correctly recognize (Fig. 1 *A* and *B*, blue circles) and track (Fig. 1 *A* and *B*, blue splines) a large majority of particles (typically >90%) present in SNAP-CD86 image sequences (Fig. 1 *A* and *B* and Movie S2).

Next, we exploited the single-molecule data to analyze the size of receptor complexes. In the case of a monomeric protein, particle intensities are expected to be normally distributed with a mean ( $\mu$ ) corresponding to that of single fluorophores. In the case of a mixture of complexes with different size (e.g., monomers, dimers, and oligomers), the distribution of particle intensities is expected to be the sum of  $n$  components, each having mean  $\mu \cdot n$ . Thus, a mixed Gaussian fitting was performed on the distribution of particle intensities to retrieve the weight of each underlying component. This analysis was validated on monomeric receptors containing either one (SNAP-CD86) or two (SNAP2x-CD86) SNAP-tags fused to their N termini. The latter represents a valuable control, because virtually all of the receptors are expected to be labeled with two fluorophores and should therefore be detected as “dimers”. In cells transfected with the SNAP-CD86 construct (Fig. S2), a predominant peak with an average intensity of  $0.0205 \pm 0.0057$  (mean  $\pm$  SD) was observed. These values were almost superimposable to those of Alexa647-BG molecules

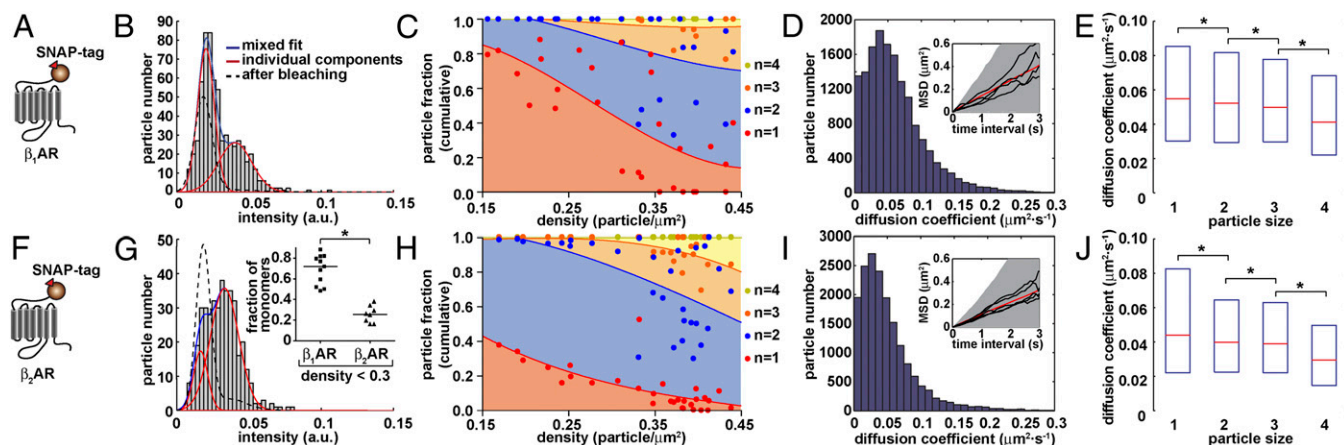
on glass (compare with Fig. S1) and were correctly detected by the mixed Gaussian fitting analysis as monomers ( $n = 1$ ). In addition, particles bleached in one step, further confirming that they were single molecules (Fig. S3). An analysis of particle intensities at different expression levels (Fig. S2) revealed that, at all particle densities measured (0.15–0.45 particle/ $\mu\text{m}^2$ ), the monomeric fraction ( $n = 1$ ) was largely predominant (>85%), with a small component of apparently dimeric particles ( $n = 2$ ; approximately 5–18%). This component was due to random colocalization of two particles below the resolution limit of our method and not to SNAP-CD86 dimerization, as indicated by the fact that the same fractions of apparent dimers were obtained at 10% labeling efficiency (Fig. S2)—these results were also consistent with those of computer simulations (*SI Results*, Movie S3 and Fig. S4). Moreover, because these simulations indicated that the method was accurate up to 0.45 particle/ $\mu\text{m}^2$  (Fig. S4), only movies with particle densities below this value were analyzed. The analysis of SNAP2x-CD86 image sequences (Fig. S2) showed a largely predominant peak with  $\mu$  and  $\sigma$  of intensity values approximately corresponding to two times those measured with SNAP-CD86. The mixed Gaussian fitting analysis correctly identified SNAP2x-CD86 particles as dimers. As expected for particles containing two fluorophores, particles were typically bleaching in two steps (Fig. S3). After partial photobleaching, a peak with the intensity of single fluorophores appeared in SNAP2x-CD86 image sequences (Fig. S2, dashed line). Such data obtained after partial photobleaching were used by the mixed Gaussian fitting algorithm to precisely estimate the intensity of single fluorophores in each image sequence (*SI Materials and Methods*). These results showed that the vast majority SNAP-tags were functional and were labeled with Alexa647-BG, thus excluding the presence of a relevant fraction of unlabeled, “dark” SNAP-tagged receptors. In addition, they indicated that the method was able to efficiently discriminate between populations of “monomeric” and “dimeric” receptors.

**$\beta_1$ - and  $\beta_2$ ARs Have Different Di/Oligomerization States.** We then applied our method to two prototypical family-A GPCRs, i.e.,  $\beta_1$ - and  $\beta_2$ ARs. Constructs coding for  $\beta_1$ - and  $\beta_2$ ARs with the SNAP-tag fused to their N termini were fully functional (Fig. S5). In CHO cells transfected with these constructs (Fig. 2 *A* and *F*) and labeled with Alexa647-BG, single fluorescent particles were detected by TIRF-M (Fig. S5). Although similar results were also obtained in HEK293 cells, CHO cells were chosen because they have no detectable  $\beta_1$ - $\beta_2$ ARs and we observed no agonist-dependent clustering of SNAP-tagged  $\beta_1$ - $\beta_2$ ARs. Typical intensity distributions of GPCR particles and mixed Gaussian fits are shown in Fig. 2 *B* and *G*. Data obtained at different particle densities were used to generate plots of the distribution of particle sizes over density, where the areas filled with different colors indicate the relative abundance of particles containing the indicated number of receptors (Fig. 2 *C* and *H*). Both receptors were present as mixtures of complexes with different size, which was increasing with particle density. The proportion of di-/oligomeric complexes and the dependency on particle density were much higher than in control SNAP-CD86 and simulated image sequences, as expected for true interactions. The effect of density was more prominent for the  $\beta_1$ AR, in which case the fraction of monomers was ~70% at low densities (0.15–0.3 particle/ $\mu\text{m}^2$ ), whereas dimers predominated over monomers and a small fraction of tri-/tetramers at the highest particle densities measured (Fig. 2*C*). The  $\beta_2$ AR had a higher tendency of forming dimers, which constituted ~60% at low densities (0.15–0.3 particle/ $\mu\text{m}^2$ ), the rest being represented by monomers (Fig. 2*H*). At higher densities,  $\beta_2$ AR contained a mixture of di-, tri-, and tetramers, which at 0.4–0.45 particle/ $\mu\text{m}^2$  accounted for ~50%, 30%, and 15%, respectively (Fig. 2*H*). The different abundance of monomers between  $\beta_1$ - and  $\beta_2$ ARs at low densities was highly statistically significant (Fig. 2*G*, *Inset*). These results were confirmed by a separate analysis based on the photobleaching steps (Fig. S3). For this purpose, the intensity profile of each particle was



**Fig. 1.** Detection and tracking of individual SNAP-tagged proteins on the surface of living cells. (*A*) Enlarged view of single SNAP-CD86 particles on the surface of a living cell visualized by TIRF-M. Particles were automatically detected and tracked. The current position (blue circle) and trajectory (blue spline) of each particle are indicated. Apparent merging and splitting events are shown as green and red segments, respectively. (Scale bar, 5  $\mu\text{m}$ .) (*B*) Same tracks on inverted image (white background). *Inset*, higher magnification.





**Fig. 2.** Analysis of  $\beta_1$ - (A–E) and  $\beta_2$ - (F–J) AR oligomerization and lateral mobility by single-molecule TIRF-M. (A and F) Schematic representation of the used SNAP-tagged constructs. (B and G) Representative intensity distributions of Alexa647-labeled particles. Particle densities were 0.24 (B) and 0.25 (G) particle/ $\mu\text{m}^2$ . Data were fitted with a mixed Gaussian model. A mixed Gaussian fit after partial photobleaching (dashed lines) was used to precisely estimate the intensity of single fluorophores in each image sequence. (G, Inset) Comparison of the fraction of monomeric  $\beta_1$ AR and  $\beta_2$ AR particles at low density (0.15–0.3 particle/ $\mu\text{m}^2$ ). Each data point represents one cell.  $*P = 0.0003$  by Mann–Whitney test. (C and H) Dependency of the distribution of particle components on particle density. Shown is the cumulative distribution of mono-, di-, tri-, and tetramers of Alexa647-labeled receptors, based on mixed Gaussian fitting analyses like those shown in B and G, as a function of particle density. Data were fitted using third-order polynomial functions to provide an indication of their trend. Each data point represents one cell. [ $n = 6,181$  particles from 27 different cells (C) and 7,419 particles from 30 different cells (H)]. (D and I) Distribution of diffusion coefficients of receptor particles calculated from their mean square displacement (MSD). Insets, MSD plots; shown are the mean (red) as well as the 10% and 90% percentiles (shaded area) of particles that were tracked for at least 3 s; black, data of representative individual particles. (E and J) Effect of the size of GPCR complexes on their lateral diffusion. The size of individual particles was estimated on the basis of the number of bleaching steps. Shown are box plots of diffusion coefficients measured for particles of different size. The boxes encompass the 25% and 75% percentiles and median values are indicated by red lines. Differences in E and J are statistically significant by a Kruskal–Wallis test ( $P < 0.0001$ ) followed by Dunn's test ( $*P < 0.001$ ).

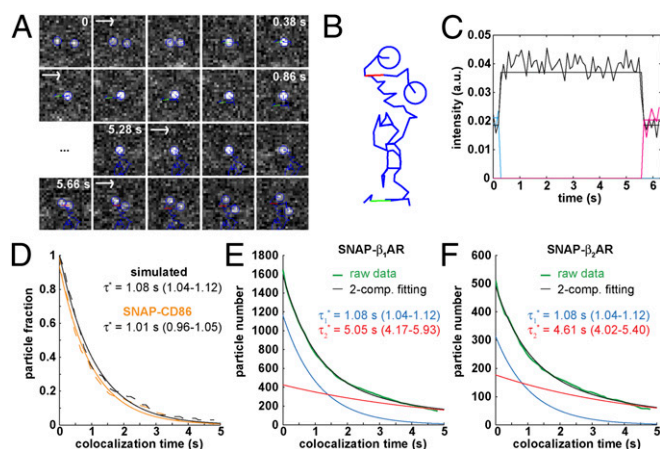
fitted with a stepwise model and the number of receptors in each particle was estimated on the basis of the number and size of steps. The results were in very good agreement with those of the mixed Gaussian fitting analyses.

Next we analyzed the movement of receptor particles on the cell surface (Fig. 2 D and I). Plots of their mean square displacement (MSD) against time gave linear relationships, suggesting that the receptors were freely diffusing. MSD data of individual particles indicated no corraling at this temporal resolution. A calculation of their diffusion coefficients from MSD data showed that  $\beta_1$ ARs were diffusing quickly on the cell surface (median diffusion coefficient =  $0.052 \mu\text{m}^2\text{s}^{-1}$ ; peak =  $0.032$ – $0.043 \mu\text{m}^2\text{s}^{-1}$ ) (Fig. 2D).  $\beta_2$ ARs had a slightly slower diffusion speed (median diffusion coefficient =  $0.039 \mu\text{m}^2\text{s}^{-1}$ ; peak =  $0.021$ – $0.032 \mu\text{m}^2\text{s}^{-1}$ ) (Fig. 2I). Overall, these values are similar to those reported on  $\beta_2$ ARs with other methods (30) as well as on other receptors by TIRF-M (26). The speed of receptor diffusion was negatively correlated with the size of receptor complexes (Fig. 2 E and J).

**$\beta_1$ - and  $\beta_2$ ARs Undergo Transient Interactions.** Because the observed increase of receptor di-/oligomerization with receptor density was suggesting the presence of transient interactions, we attempted to directly observe and characterize such interactions. An example of a transient colocalization between two  $\beta_1$ AR particles is shown in Fig. 3 A–C. For each pair of colocalizing particles, the colocalization time ( $\Delta t$ ), i.e., the time between merging and splitting, was automatically calculated and  $\Delta t$  values were used to estimate the apparent lifetime of particle colocalizations ( $\tau^*$ ) by fitting the data to an exponential decay function. Colocalization of  $\beta_1$ ARs should result from both random colocalizations and true receptor–receptor interactions. To distinguish these true interactions from random colocalizations, we simulated particles with the same characteristics (diffusion coefficients, intensity distribution, and bleaching rate) of  $\beta_1$ ARs, but showing no interactions. The estimated  $\tau^*$ -value for these random colocalizations ( $\tau_1^*$ ) was 1.08 s (95% confidence interval: 1.04–1.12) and served as a background value (Fig. 3D). Almost identical  $\tau^*$ -values (1.01 s; 95% confidence interval, 0.96–1.05) were

obtained with control monomeric (SNAP-CD86) receptors. Then,  $\beta_1$ AR data were fitted to the sum of two exponential functions, the first one with a lifetime equal to  $\tau_1^*$  (Fig. 3E). The apparent lifetime of the second component ( $\tau_2^*$ ), i.e., the one resulting from receptor–receptor interactions, was estimated to be 5.05 s (95% confidence interval: 4.17–5.93). Similar results ( $\tau_2^* = 4.61$  s; 95% confidence interval, 4.02–5.40) were obtained for low-density  $\beta_2$ AR movies (Fig. 3F). Knowing  $\tau_1^*$  and  $\tau_2^*$ , the true lifetime of receptor–receptor interactions can be roughly estimated as  $\tau_{\text{int}} = \tau_2^* - \tau_1^* \approx 4$  s at 20 °C (27).

**Functional GABA<sub>B</sub> Heterodimers Form Large Complexes Tethered to the Cortical Actin Cytoskeleton.** We then applied our method to the GABA<sub>B</sub> receptor, a prototypical family-C GPCR, consisting of heteromers between GABA<sub>B1</sub> and GABA<sub>B2</sub> subunits (10–12). Initially, we transfected CHO cells with N-terminally SNAP-tagged GABA<sub>B1</sub> and GABA<sub>B2</sub> subunits (31). As expected, the SNAP-tagged GABA<sub>B1</sub> subunit alone did not reach the cell surface, whereas the SNAP-tagged GABA<sub>B2</sub> subunit alone was detectable on the cell surface, where it formed a mixture of mono-/di-/oligomers with high lateral mobility (Fig. S6). Thus, cells cotransfected with both SNAP-tagged subunits (Fig. S7) most likely contained a mixture of labeled homomeric (composed of GABA<sub>B2</sub>) and heteromeric complexes. Therefore, to selectively analyze functional GABA<sub>B</sub> complexes, we took advantage of the fact that the GABA<sub>B1</sub> subunit requires dimerization with the GABA<sub>B2</sub> subunit to reach the cell surface and analyzed cells cotransfected with SNAP-tagged GABA<sub>B1</sub> and untagged GABA<sub>B2</sub> subunits (Fig. 4 A and B). Note that in these experiments the labeling stoichiometry is one fluorophore per heterodimer (h.d.). At low densities (0.15–0.2 particle/ $\mu\text{m}^2$ ), GABA<sub>B</sub> complexes prevalently consisted of heterodimers ( $n = 1$  h.d.) (Fig. 4 C and D). The proportion of higher-order oligomers increased with particle density. At the highest density analyzed (0.4–0.45 particle/ $\mu\text{m}^2$ ), tetramers (dimers of dimers;  $n = 2$  h.d.) and octamers (tetramers of dimers;  $n = 4$  h.d.) constituted a large fraction (30–40% each) of the detected complexes. Very similar results were obtained after correction for random colocalization (SI Results and Fig. S8). These findings were confirmed by an



**Fig. 3.** Dynamic visualization of receptor-receptor interactions. (A) Example of two Alexa647-labeled  $\beta_1$ AR particles showing a transient colocalization. A merging event (green) is followed after some frames by a splitting event (red). Images are centered on the particles' position. (Scale bar, 1  $\mu$ m.) (B) Same traces as in A on a white background and without centering. (C) Intensity profiles of the traces in A, showing intensity doubling upon merging. (D) Colocalizations between control particles devoid of true interactions. Black, simulated particles with diffusion coefficients, intensity distribution, and bleaching rate analogous to those of  $\beta_1$ AR particles. Orange, monomeric SNAP-CD86 receptors. The apparent lifetime of particle colocalizations ( $\tau^*$ ; 95% confidence intervals in parentheses) was calculated by fitting colocalization time data with an exponential decay function. (E) Lifetime of  $\beta_1$ AR colocalizations. Colocalization time data derived from experiments as in A (green) were fitted to the sum (black) of two exponential decays (blue and red, respectively). The obtained apparent lifetimes of particle colocalizations ( $\tau_1^*$  and  $\tau_2^*$ ; 95% confidence intervals in parentheses) were then used to estimate the true lifetime of receptor-receptor interactions. (F) Same as E with low-density ( $<0.35$  particle/ $\mu$ m<sup>2</sup>)  $\beta_2$ AR movies. Data in E and F were fitted better with two components than with one, as judged by an *F*-test ( $P < 1.0 \times 10^{-8}$ ).

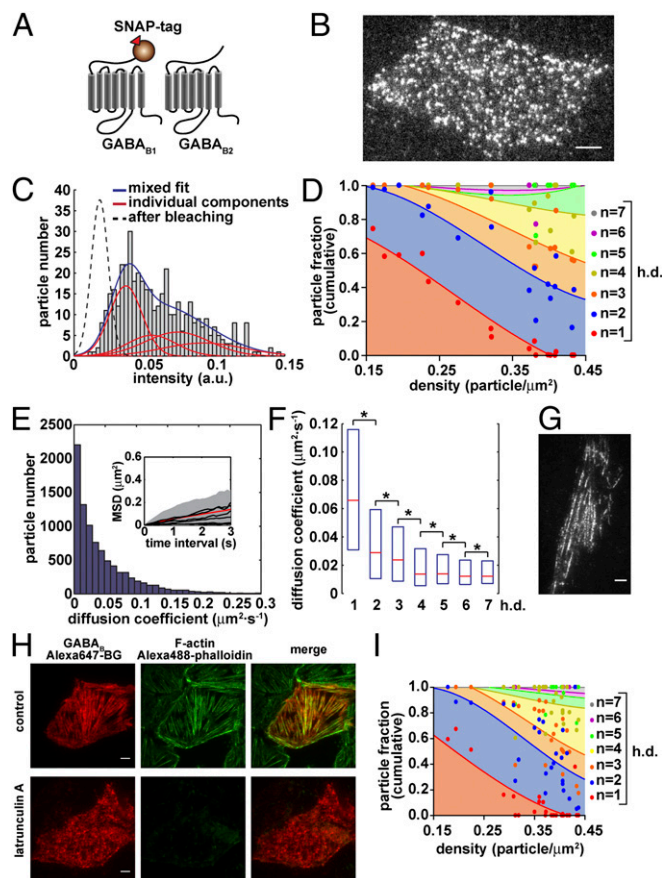
additional analysis, in which the intensity profiles of each receptor particle were fitted with a stepwise model and the number and size of steps were used to estimate the size of the receptor particles (Fig. S3).

Next, we evaluated the diffusion speed of functional GABA<sub>B</sub> complexes. Most particles had limited mobility (median diffusion coefficient =  $0.028 \mu\text{m}^2 \cdot \text{s}^{-1}$ ; peak  $< 0.01 \mu\text{m}^2 \cdot \text{s}^{-1}$ ; particles with diffusion coefficients  $< 0.01 \mu\text{m}^2 \cdot \text{s}^{-1} = 24.6\%$ ; Fig. 4E), which was negatively correlated with particle size (Fig. 4F). Interestingly, GABA<sub>B</sub> receptors showed a tendency to arrange in rows. This was already visible at receptor densities used for the single-molecule analysis and was even better appreciated at higher receptor densities (Fig. 4G). Moreover, GABA<sub>B</sub> receptors colocalized with actin fibers stained with fluorescent phalloidin, suggesting an interaction between these receptors and the cortical actin cytoskeleton. Actin depolymerization with latrunculin A abolished the arrangement of GABA<sub>B</sub> receptors in rows (Fig. 4H), but did not modify the size of GABA<sub>B</sub> complexes (Fig. 4I).

**Agonist Stimulation Increases the Lateral Mobility of GABA<sub>B</sub> Receptors, but not of  $\beta_1$ -/ $\beta_2$ ARs.** Labeling the receptors themselves rather than the ligands allowed us to investigate whether the di-/oligomerization or mobility of GPCRs was affected by agonists. CHO cells expressing SNAP-tagged  $\beta_1$ -/ $\beta_2$ ARs or GABA<sub>B</sub> receptors were stimulated with 10  $\mu$ M isoproterenol or 50  $\mu$ M GABA, respectively. Agonist stimulation had no effect on the di-/oligomerization state of any receptor (Fig. S9) or on the mobility of  $\beta_1$ - and  $\beta_2$ ARs (Fig. 5A and B). However, it did increase the mobility of GABA<sub>B</sub> receptors (median diffusion coefficient from  $0.027$  to  $0.056 \mu\text{m}^2 \cdot \text{s}^{-1}$ ; Fig. 5C).

## Discussion

The extent and functional relevance of GPCR di-/oligomerization is highly debated. Whereas monomeric GPCRs, including rhodopsin (19, 20) and the  $\beta_2$ AR (21), efficiently activate G proteins, several studies suggest that GPCRs can form di-/oligomers (6–10). The exact size and stability of such complexes are largely unknown. We used single-molecule TIRF-M combined with direct labeling of the



**Fig. 4.** Selective analysis of GABA<sub>B</sub> receptor heterodimers. (A) Schematic representation of the used constructs. Cells were cotransfected with SNAP-GABA<sub>B1</sub> and wild-type GABA<sub>B2</sub> subunits. (B) Representative image of a cell transfected with both constructs, labeled with Alexa647-BG and visualized by TIRF-M. Particle density =  $0.43$  particle/ $\mu$ m<sup>2</sup>. (C) Intensity distribution of the particles in B. Data were fitted with a mixed Gaussian model. (D) Dependency of the distribution of particle components on particle density. Data are based on mixed Gaussian fitting analyses like those shown in C and are represented as in Fig. 2C and H. Because only the GABA<sub>B1</sub> subunit is labeled, one fluorophore ( $n = 1$ ) corresponds to one heterodimer (h.d.) [ $n = 4,472$  particles from 17 different cells]. (E) Distribution of diffusion coefficients of GABA<sub>B</sub> heteromeric particles on the cell surface. Inset, MSD plot; shown are the mean (red) as well as the 10% and 90% percentiles (shaded area) of particles that were tracked for at least 3 s; black, representative data of individual mobile and immobile particles. (F) Effect of the size of GABA<sub>B</sub> heteromeric particles on their lateral diffusion. The size of individual particles was estimated on the basis of the number of bleaching steps. Shown are box plots of diffusion coefficients measured for particles of different size. The boxes encompass the 25% and 75% percentiles and median values are indicated by red lines. Differences are statistically significant by a Kruskal–Wallis test ( $P < 0.0001$ ) followed by Dunn's test ( $*P < 0.001$ ). (G) Image of a cell with  $\sim 15$  times higher receptor density than in B, showing GABA<sub>B</sub> receptors arranged in rows. (H) Interaction of GABA<sub>B</sub> receptors with the cortical actin cytoskeleton. Cells were cotransfected with SNAP-GABA<sub>B1</sub> and wild-type GABA<sub>B2</sub> subunits, treated or not (control) with latrunculin A and labeled with Alexa647-BG. After fixation, actin filaments were stained with Alexa488-phalloidin. (Scale bars, 5  $\mu$ m.) (I) Same as D in cells pretreated with latrunculin A [ $n = 7,748$  particles from 26 different cells].





## Materials and Methods

**Cell Culture and Transfection.** For single-molecule experiments, CHO cells were cultured in DMEM/F12 medium supplemented with 10% (vol/vol) FCS, penicillin, and streptomycin at 37 °C, 5% (vol/vol) CO<sub>2</sub>. Cells were plated at a density of  $3 \times 10^5$  cells per well onto 24-mm clean glass coverslips and transfected using the Lipofectamine 2000 reagent (Invitrogen), following the manufacturer's protocol. For each well, 2  $\mu$ g DNA and 6  $\mu$ L Lipofectamine 2000 were used. Cells were analyzed 8–12 h after transfection to achieve low expression levels.

**SNAP Labeling.** Cells were labeled with 1  $\mu$ M Alexa647-BG (Alexafluor 647-SNAP Surface; New England Biolabs) in complete (+FCS) phenol-red-free medium for 30 min at 37 °C. At the end of the incubation, the cells were washed three times with complete phenol-red-free medium and immediately imaged. These conditions resulted in saturating labeling of cell-surface SNAP-tagged receptors (Fig. S2).

**Total Internal Reflection Fluorescence Microscopy.** A commercial TIRF microscope (Leica AM TIRF) equipped with an EM-CCD camera (Cascade 512B; Roper Scientific), a 100 $\times$  oil-immersion objective (HCX PL APO 100 $\times$ /1.46), and a 635-nm diode laser was used. To avoid photobleaching before image acquisition, cells were searched and focused in bright field and a fine focus adjustment in TIRF mode was performed using only 2% laser power, an

intensity insufficient for detecting single molecules. This procedure resulted in negligible photobleaching. Afterward, laser power was set to 83% and image sequences (400–600 frames) were acquired with an exposure time of 50 ms, resulting in the acquisition of an image every 96 ms. The penetration depth of the evanescent field was  $\sim 110$  nm. Illumination intensity was homogeneous over the imaged area (maximum difference = 10%). Under these conditions, the photobleaching half-life was  $6.82 \pm 0.12$  s. The microscope was equipped with an incubator and a temperature control unit. Experiments were performed at  $20.5 \pm 0.3$  °C. Cells were imaged in a buffer containing 137 mM NaCl, 5.4 mM KCl, 2 mM CaCl<sub>2</sub>, 1 mM MgCl<sub>2</sub>, and 10 mM Hepes, pH 7.3. Only cells with less than 0.45 receptor particle/ $\mu$ m<sup>2</sup> were analyzed.

**Additional Methods.** Details about plasmids, coverslip cleaning, determination of Alexa647-BG labeling efficiency, radioligand binding, measurement of cAMP concentrations, Latrunculin A treatment/actin staining, and computational analyses are available in *SI Materials and Methods*.

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