

# A Fast Proximal Gradient Algorithm For Single Particle Reconstruction of Cryo-EM

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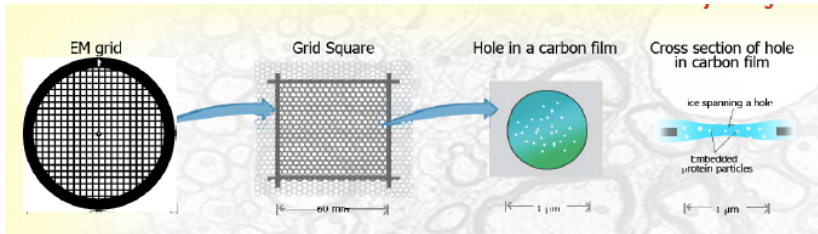
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## Sample preparation

- The particles of interest are embedded in the holes on this grid in **vitreous ice**
- a thin layer of sample suspended in water is rapidly frozen in liquid ethane to form vitreous ice
- The specimen is maintained continuously below  $-160^{\circ}\text{C}$  during storage and also during imaging in the electron microscope to prevent the formation of **ice crystals**

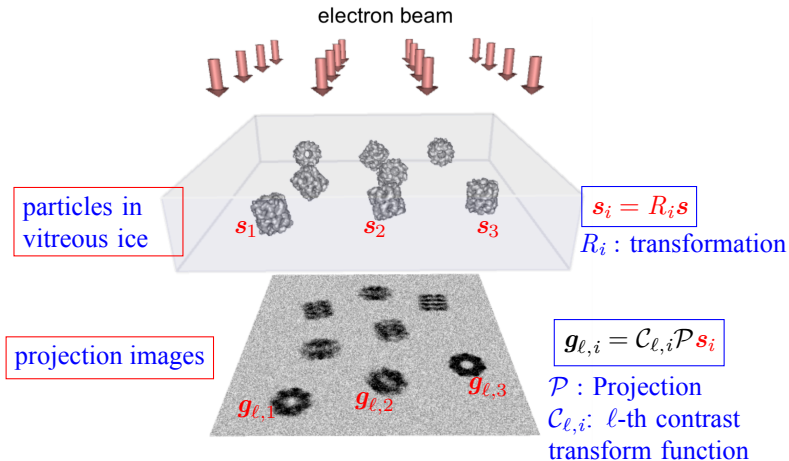


图: 2D projection images of 3D object are recorded with an EM. **The rotation parameters are unknown!** The goal of Cryo-EM is to reconstruct  $s$  from  $g_{l,i}$ .

## Forward Projection

- $\mathbf{s}(\mathbf{x})$  be the true particle with  $\mathbf{x} = (x_1, x_2, x_3)^T \in \mathbb{R}^3$ .
- $R$  be the rotation of each particle  $\mathbf{s}_R(\mathbf{x}) = \mathbf{s}(R^{-1}\mathbf{x})$
- Projection  $(\mathcal{P}\mathbf{s}_R)(x_1, x_2) = \int_{-\infty}^{\infty} \mathbf{s}_R(x_1, x_2, x_3) dx_3$ .
- Contrast Transfer function determination and correction

$$\text{CTF}(r) = \sin \left( -\pi \left( \frac{\text{defocus}}{2} \cdot r^2 - C_s \cdot \lambda^3 \cdot r^4 \right) - A \right) \exp \left( -\frac{r^2}{4B_{\text{factor}}} \right).$$

- $r$ : the magnitude of the frequency
- $C_s$ : the spherical aberration constant in mm
- $\lambda$ : the electron wavelength in picometers
- $A$ : amplitude contrast.

## Challenge in Cryo-EM

- **Low electron dose** vs. **noise**. Low electron dose to minimize radiation damage, **but** more noise in images.



Sample in vitreous ice



Sample inside EM

- **Number of Particles Required**. Thousands or millions of particles to improve the quality and resolution of 3D reconstruction, **but** thousands or millions **unknown parameters** in transformation.

## Challenge in Cryo-EM

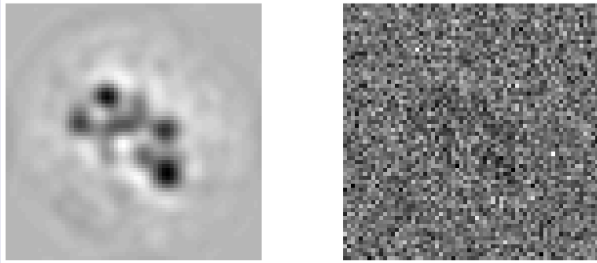


图: Projection image versus noisy image (SNR=0.05dB).



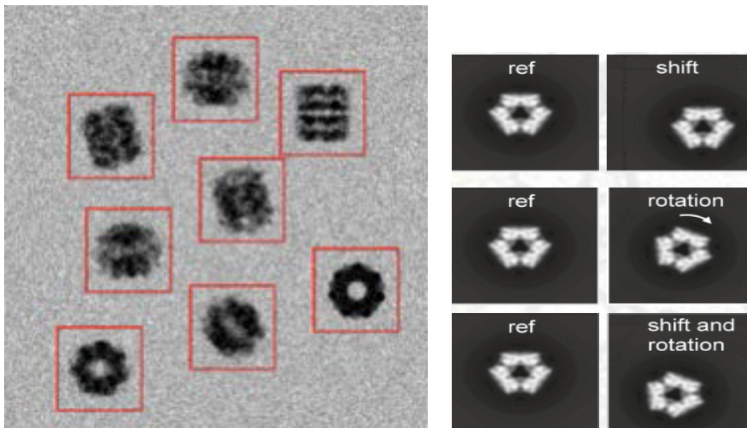


图: Particle selection and 2D classification to group similar images.

$b_{i,i_1} = T_{i,i_1} g_{i,i_1}$ ,  $T_{i,i_1}$  denotes shift and rotation.

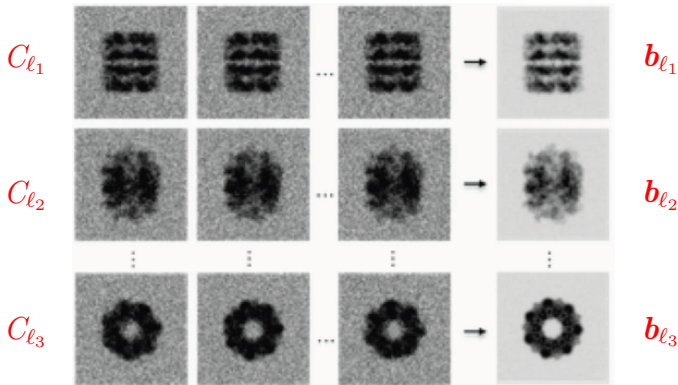


图: 使用低电子剂量需要对粒子群进行平均处理, 以提高信噪比

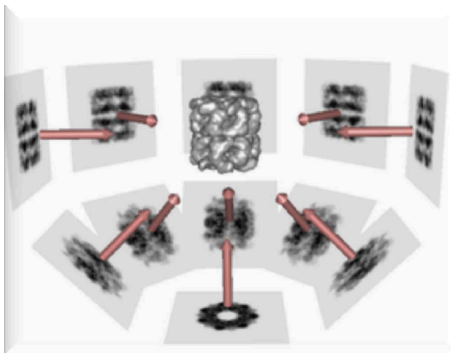
$\min_{b_\ell} \sum_{b_{i,i_1} \in C_\ell} \|b_{i,i_1} - b_\ell\|_2^2$ . **Multivariate Statistical Analysis** can be used to

generate a class average, i.e., one single image to represent a group of images that all look the same.

## Main advantages of 2D classifications

- Cryo-EM images are noisy (low contrast), averaging similar looking images enhance the contrast by increases signal to noise ratio
- identifying the features and helping in alignment during 3D reconstruction
- helping in identifying bad or unwanted images thereby improving the quality of data
- Its an unbiased process with less user interference

# 3D Reconstruction



$$\mathbf{s}_i = R_i \mathbf{s}$$

$$\mathbf{g}_{i,i_1} = C_{i,i_1} P \mathbf{s}_i$$

$$\mathbf{b}_{i,i_1} = T_{i,i_1} \mathbf{g}_{i,i_1}$$

$$\min_{\mathbf{b}_\ell} \sum_{\mathbf{b}_{i,i_1} \in C_\ell} \|\mathbf{b}_{i,i_1} - \mathbf{b}_\ell\|_2^2$$

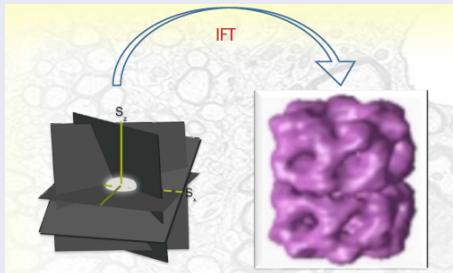
$\mathbf{b}_\ell$ : back projection

图: 3D reconstruction.

## Central slice theorem

$$(\mathcal{F}_2 \mathcal{P} s_R)(\omega_1, \omega_2) = (\mathcal{F}_3 s_R)(\omega_1, \omega_2, 0).$$

$\mathcal{F}_2$  : 2D-Fourier transform,  $\mathcal{F}_3$  : 3D-Fourier transform.



## Main steps of SPR in Cryo-EM

- Sample Preparation
- Electron Microscopy Imaging,
- EM Image Processing
  - Data quality assessment
  - CTF determination and correction
  - Particle selection
  - 2D Classification: **determine shift and rotation parameter  $T_{i,i_1}$ .**
- 3D Classification: **determine rotation parameter  $R_i$ .**
- **3D Reconstruction**

## References



Allison Doerr.

Single-particle electron cryomicroscopy.  
*Nature Methods*, 11:30EP, 12 2013.



Richard Gordon, Robert Bender, and Gabor T Herman.

Algebraic reconstruction techniques (art) for three-dimensional electron microscopy and x-ray photography.  
*Journal of Theoretical Biology*, 29(3):471–481, 1970.



Frank Joachim.

*Three-dimensional electron microscopy of macromolecular assemblies*.  
Elsevier, 1996.



Alp Kucukelbir, Fred J Sigworth, and Hemant D Tagare.

A bayesian adaptive basis algorithm for single particle reconstruction.  
*Journal of Structural Biology*, 179(1):56–67, 2012.



Sjors HW Scheres.

Relion: implementation of a bayesian approach to cryo-em structure determination.  
*Journal of Structural Biology*, 180(3):519–530, 2012.



Lanhui Wang, Amit Singer, and Zaiwen Wen.

Orientation determination of cryo-em images using least unsquared deviations.  
*SLAM journal on Imaging Sciences*, 6(4):2450–2483, 2013.

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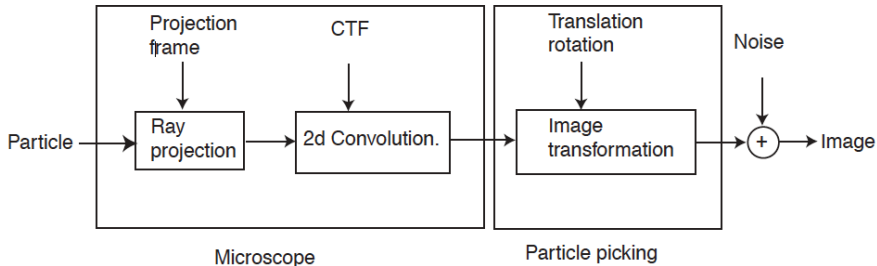


图: Signal Flow for Cryo-EM

## Mathematical Model of SPR

$$\mathbf{b}_k = T_k C_k \Omega_k \mathbf{s} + \eta_k$$

- $\mathbf{b}_k$ : the 2-D observed Cryo-EM image with size  $P \times P$ .
- $\mathbf{s}$ : the 3D particle density map with size  $N \times N \times N$ .
- $T_k$ : the 2-D transformation operator. and the rotation  $\gamma_k$  parameters.
- $C_k$ : the contrast transfer function.
- $\Omega_k$ : the projection operator with  $\Omega_k = PR_k$ .
- $\eta_k$ : the Gaussian noise with standard deviation  $\sigma$ .

**Aim:** reconstruct a three-dimension structure of the particle  $\mathbf{s}$  from its two-dimension observed projections  $\mathbf{b}_k$ .

## Least Square Method

$$\min g(\mathbf{s}) \equiv \sum_{k=1}^K \frac{1}{2} \|\mathbf{b}_k - T_k C_k \Omega_k \mathbf{s}\|_F^2$$

## Regularization Approach

- Assume that the particle  $s$  can be sparse under some orthogonal basis vectors:  $s = \Phi\alpha$ .
- Regularization approach

$$\min_{\alpha} J(\alpha) \equiv \sum_{k=1}^K \frac{1}{2} \|b_k - T_{\tau_k} C_k \Omega_{p_k} \Phi \alpha\|_2^2 + \lambda \|\alpha\|_1.$$

- Denote  $h(\alpha) = \lambda \|\alpha\|_1$ , we have

$$\mathcal{J}(\alpha) = g(\Phi\alpha) + h(\alpha).$$

## Proximal Gradient Method

- starting with an initial guess  $\alpha_0$ , the iterate is given by

$$\alpha_k = \text{prox}_{t_k h}(\alpha_k - t_k \nabla_{\alpha} g(\Phi \alpha_k)).$$

- The proximal operator of the function  $h$  is defined by

$$\text{prox}_h(\mathbf{v}) = \underset{\alpha}{\operatorname{argmin}} \frac{1}{2} \|\mathbf{v} - \alpha\|_2^2 + h(\alpha).$$

- Notice that  $h(\alpha) = \lambda \|\alpha\|_1$ , we have

$$(\text{prox}_h(\mathbf{v}))_i = \begin{cases} \mathbf{v}_i - \lambda, & \mathbf{v}_i \geq \lambda. \\ 0, & |\mathbf{v}_i| \leq \lambda. \\ \mathbf{v}_i + \lambda, & \mathbf{v}_i \leq -\lambda. \end{cases}$$

## Accelerated Proximal Gradient Method

- When an extrapolation step is used in the iterate, the convergence can be improve.
- The iterate becomes to

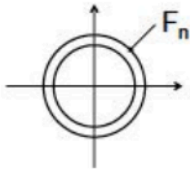
$$\beta_k = \alpha_{k-1} + \omega^k(\alpha_{k-1} - \alpha_{k-2}).$$

$$\alpha_k = \text{prox}_{t_k h}(\beta_k - t_k \nabla_{\alpha} g(\beta_k)).$$

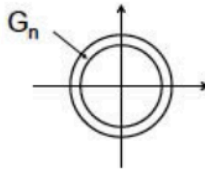
where  $\omega^k \in [0, 1)$  is an extrapolation parameter, one simple choice takes

$$\omega^k = \frac{k-1}{k+2}.$$

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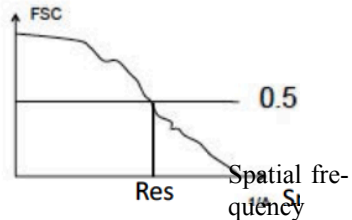


Reconstruction 1



Reconstruction 2

$$FSC(R) = \frac{\sum_{n \in R} F_n G_n}{\left\{ \sum_{n \in R} |F_n|^2 \sum_{n \in R} |G_n|^2 \right\}^{1/2}}$$





- The tested original volume is the 50S ribosomal subunit structure published(PDB ID: 8523), available online at the Protein Data Bank in Europe (PDBe) website <sup>a</sup>.
- The PDBe volume is  $64 \times 64 \times 64$  voxels with resolution of  $16.9 \text{ \AA}$ .
- The structure is projected along direction randomly chosen from sampling on the sphere.
- Defocus values of  $1.4 \text{ }\mu\text{m}$  CTFs with 120 keV electrons.
- A soft, spherical mask with a Gaussian fall-off at the edge was applied to each volume.

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<sup>a</sup><http://www.ebi.ac.uk/pdbe/entry/emdb/EMD-8523/>

# Results

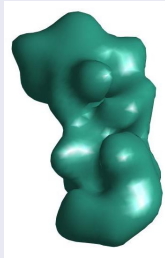


图: original volume from EMD-8523 in PDDBE

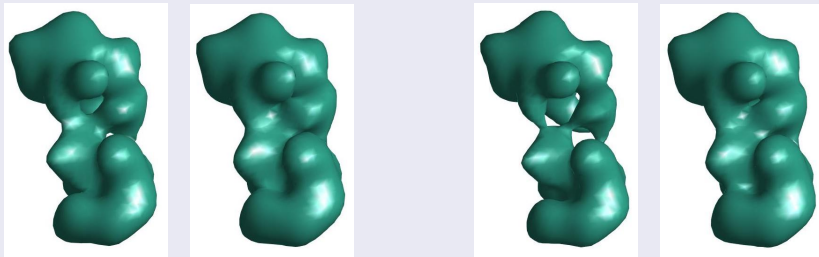


图: Left:  $\sigma=1$ , right:  $\sigma=2$ . Reconstruction volume by AB and FISTA respectively .

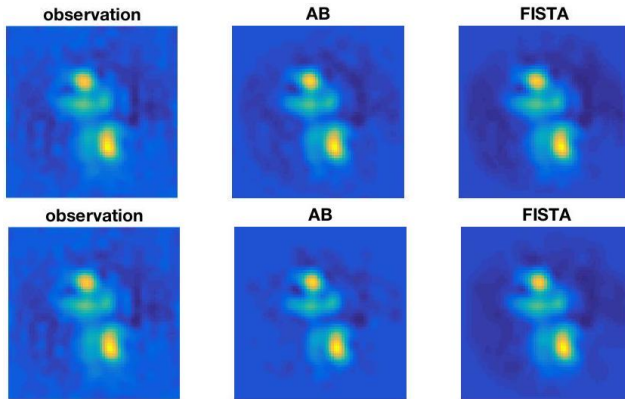


图: Central slices at  $n = 32$  from the simulated data reconstructions for 50S ribosomal subunit (PDB ID: 8523). Top:  $\sigma=1$ , Below:  $\sigma=2$ .

$\sigma$	Error		CPU Time	
	AB	FISTA	AB	FISTA
1	0.2871	0.1834	178.46	82.18
2	0.3839	0.2200	164.08	74.37

**Table:** run time and relative error Comparison of AB algorithm and FISTA method at  $\sigma=1$  and  $\sigma=2$  respectively

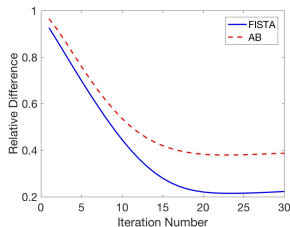
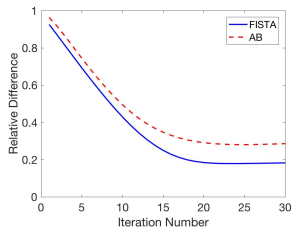


图: Relative error curves for AB and FISTA for  $\sigma = 1$  (left) and  $\sigma = 2$  (right) respectively.

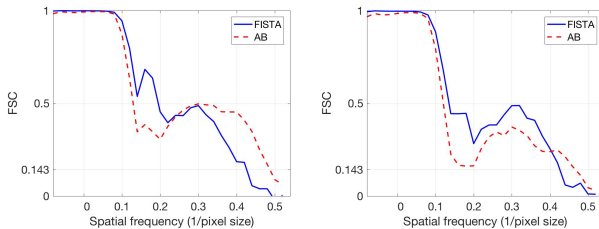


图: FSC curves for AB and FISTA  $\sigma = 1$  (left) and  $\sigma = 2$  (right) respectively.

## Conclusion

- The relative errors obtained the proposed method is less than that obtained by AB.
- The FSCs confirm that the FISTA algorithm reconstructions contain more detail than the AB algorithm results.
- The FISTA methods shows improved performance for simulated data when compared to the adaptive basis reconstruction algorithm (AB).



Thank You! Questions?