

Received 17 September 2016; revised 11 January 2017; accepted 11 February 2017.  
Date of publication 2 May 2017; date of current version 24 April 2017.

Digital Object Identifier 10.1109/JTEHM.2017.2679746

# Wearable Improved Vision System for Color Vision Deficiency Correction

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This work was supported by the Regione Campania under the research project Computer Improved VISus.

**ABSTRACT** Color vision deficiency (CVD) is an extremely frequent vision impairment that compromises the ability to recognize colors. In order to improve color vision in a subject with CVD, we designed and developed a wearable improved vision system based on an augmented reality device. The system was validated in a clinical pilot study on 24 subjects with CVD (18 males and 6 females, aged  $37.4 \pm 14.2$  years). The primary outcome was the improvement in the Ishihara Vision Test score with the correction proposed by our system. The Ishihara test score significantly improved ( $p = 0.03$ ) from  $5.8 \pm 3.0$  without correction to  $14.8 \pm 5.0$  with correction. Almost all patients showed an improvement in color vision, as shown by the increased test scores. Moreover, with our system, 12 subjects (50%) passed the vision color test as normal vision subjects. The development and preliminary validation of the proposed platform confirm that a wearable augmented-reality device could be an effective aid to improve color vision in subjects with CVD.

**INDEX TERMS** Augmented reality, color vision deficiency, wearable device, medical device.

## I. INTRODUCTION

Color vision deficiency (CVD), also referred to as color blindness, is defined as the “inability to distinguish certain shades of color or in more severe cases, see colors at all”. Around 5%–8% of men and 0.8% of women have certain kinds of CVD [1]. Unlike people with normal color vision, people with CVD report difficulties discriminating certain color combinations and color differences.

Human color vision is based on the response of three different classes of photoreceptors, called cones, located in the retina [2]. Each class of cones is sensitive to photons of different wavelengths: long-wavelength (L), middle wavelength (M), and short-wavelength (S) regions of the visible spectrum. CVD generally arises from either a complete lack of one of the three classes of cone pigments or the modification of one of them. The former is called dichromacy and the latter is called anomalous trichromacy. The dichromacies are distinguished in protanopia, deutanopia and tritanopia according to the missing class of cones. Similarly, anomalous

trichromacies are classified as protanomaly, deutanomaly and tritanomaly.

In the last decades several algorithms, applications and commercial products have been developed for subjects with CVD. In particular, special lenses have been developed to improve color vision [3], however, they are specific to a particular disability (deutanopia and protanopia) and require adaptation of the eye to be effective. Moreover, several apps for smartphones have been deployed in order to help people with CVD. Most of them are not designed for real-time applications and also those presenting real-time function are impractical, since using a smartphone during a real-life activity is often troublesome [4].

The advent of wearable augmented reality devices, such as the Google Glass, paves the way to the design and development of a wearable system to help people with CVD. Although several augmented reality solutions have been used in different health-related contexts [5]–[10], to the best of the authors’ knowledge, only one study explored the application

of this technology, based on an optical see-through device, to support subjects with CVD [4]. This may be related to the fact that most algorithms developed to improve color vision have been designed for asynchronous mode and not for real-time applications [11].

The current paper describes the design, development and clinical validation of a wearable augmented reality system to improve color vision for subjects with CVD.

## II. METHODS AND PROCEDURES

### A. SYSTEM DESIGN

We designed a wearable real-time augmented-reality system in order to improve color vision in subjects suffering from CVD.

Two approaches can be used for real-world manipulation: the optical see-through that combines computer-generated imagery with the image of the real world, and video see-through that presents video feeds from cameras inside head-mounted devices.

Video see-through systems suffer the latency (delay) from sensing to imaging. Optical see-through has no latency, which sounds great but it gives a mismatch or lack of synchronization between what you see through the glasses and the graphics. When the real world needs to be overlaid, this mismatch is annoying and distracting. In contrast, using video see-through allows you to synchronize the delay so that your video and graphics are always in sync.

For this reason, our system is based on video see-through. The real world is acquired by a stereoscopic camera, then the left and right images are processed separately applying the algorithms described in the following and the new world is presented to the patient via the Liquid Crystal Display (LCD) of the Head Mount Display (HMD).

The architecture consists of three main modules:

- Video Acquisition Module (VAM);
- Video Processing Module (VPM);
- Video Rendering Module (VRM);

The VAM is based on an OVRVISION PRO camera (OVR VISION, Osaka, Japan), mounted in the front part of HMD, represented in Figure 1, with a resolution of  $960 \times 950 \times \text{eye}$  @ 60Hz with a horizontal field of view (FOV) of 100° and a vertical FOV of 98°.

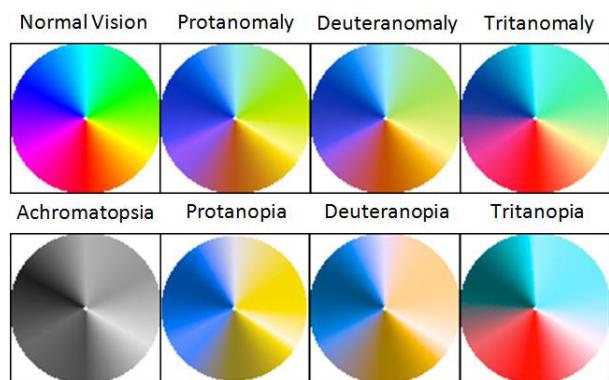
The VPM implements the three different algorithms (protanopia, deutanopia and tritanopia) using the openCV library and customized software ensuring an execution time less than the acquisition period (1/60 s) in order to avoid any loss of frames.

The VRM is based on an HMD display with a resolution of  $960 \times 1080 \times \text{eye}$  @ 75Hz, a diagonal FOV of 100°, a persistence <3 ms and a weight of 440 grams.

Subjects with CVD typically perceive a narrower color spectrum compared to people with normal color vision. The color spectrum seen by subjects with normal color vision and by people affected by CVD are shown in Figure 2. The proposed wearable system aims at improving color vision of



**FIGURE 1.** HMD with OVRVISION PRO camera mounted.



**FIGURE 2.** A comparison of the visible color spectrum in common types of color blindness.

visually impaired people and its function is to perform a remapping of the colors in the scene observed by a visually impaired subject in order to increase her/his ability to distinguish colors.

To this purpose, we designed an algorithm to redistribute the colors in the scene on the spectrum actually perceived by the subject. Since the system is requested to work real-time, the computational cost of the algorithm should be as limited as possible and this suggests the use of a linear transformation-based approach. The standard RGB color space is not the best choice to implement the desired remapping. A color space better modeling human color perception is the LMS which simulates the response of the three types of cones to long, medium and short wavelengths.

The color remapping process is inspired to the daltonization strategy suggested by Brettel *et al.* [12], which is mainly based on the transformation from RGB (LMS) to LMS (RGB) color spaces by means of linear transformation matrices. Actually, in [12] only protanopia has been taken into account for the correction of daltonization. In this work, we adopted the transformation matrix reported in [12] for protanopia, and, since we are also interested in correcting deutanopia and tritanopia, we further computed the relative transformation matrices by means of a regression approach.

The first step of our algorithm is the transformation from the RGB to LMS color space by means of the following

matrix:

$$\begin{bmatrix} L \\ M \\ S \end{bmatrix} = \begin{bmatrix} 17.8824 & 43.5161 & 4.11935 \\ 3.45565 & 27.1554 & 3.86714 \\ 0.0299566 & 0.184309 & 1.46709 \end{bmatrix} \begin{bmatrix} R \\ G \\ B \end{bmatrix}$$

The obtained LMS image undergoes a further linear transformation aimed at simulating the specific color blindness according to one of the following matrices:

Protanopia:

$$T_P = \begin{bmatrix} 0.0 & 2.02344 & -2.52581 \\ 0.0 & 1.0 & 0.0 \\ 0.0 & 0.0 & 1.0 \end{bmatrix}$$

Deuteranopia:

$$T_D = \begin{bmatrix} 1.42319 & -0.88995 & 1.77557 \\ 0.67558 & -0.42203 & 2.82788 \\ 0.00267 & -0.00504 & 0.99914 \end{bmatrix}$$

Tritanopia

$$T_T = \begin{bmatrix} 0.95451 & -0.04719 & 2.74872 \\ -0.00447 & 0.96543 & 0.88835 \\ -0.01251 & 0.07312 & -0.01161 \end{bmatrix}$$

After this, inverse transformation is performed to simulate the resulting image in the RGB color space, showing the original image as perceived by a person with CVD.

$$T_T = \begin{bmatrix} 0.08094 & -0.13050 & 0.11672 \\ -0.01024 & 0.05401 & -0.11361 \\ -0.00036 & -0.00412 & 0.69351 \end{bmatrix} \begin{bmatrix} l \\ m \\ s \end{bmatrix}$$

Starting from the simulated RGB image we compute the difference with respect to the original one:

$$\begin{bmatrix} R' \\ G' \\ B' \end{bmatrix} = \begin{bmatrix} r \\ g \\ b \end{bmatrix} - \begin{bmatrix} R \\ G \\ B \end{bmatrix}$$

The following step applies a shift so that R', G', B' are in the visible spectrum. Of course, the shift depends on the dichromacy:

Protanopia

$$\begin{bmatrix} RR \\ GG \\ BB \end{bmatrix} = \begin{bmatrix} 0.0 & 0.0 & 0.0 \\ 0.5 & 1.0 & 0.0 \\ 0.5 & 0.0 & 1.0 \end{bmatrix} \begin{bmatrix} R' \\ G' \\ B' \end{bmatrix}$$

Deuteranopia:

$$\begin{bmatrix} RR \\ GG \\ BB \end{bmatrix} = \begin{bmatrix} 1.0 & 0.5 & 0.0 \\ 0.0 & 0.0 & 0.0 \\ 0.0 & 0.5 & 1.0 \end{bmatrix} \begin{bmatrix} R' \\ G' \\ B' \end{bmatrix}$$

Tritanopia

$$\begin{bmatrix} RR \\ GG \\ BB \end{bmatrix} = \begin{bmatrix} 1.0 & 0.0 & 0.7 \\ 0.0 & 1.0 & 0.7 \\ 0.0 & 0.0 & 0.0 \end{bmatrix} \begin{bmatrix} R' \\ G' \\ B' \end{bmatrix}$$

The final step consists in compensating the components r, g, b obtained by the simulation as follows R''=RR+r, G''=GG+g e B''=BB+b. Since R'', G'', B'' could have



**FIGURE 3.** From left to right, original image, image perceived by a subject affected by protanopia, image perceived after correction.

values outside [0-255], their values undergo a saturation process. Figure 3 shows an example for protanopia. The image to the left is the original image, the one in the middle is what the subject affected by protanopia perceives and the one to the right is the perceived image after correction of protanopia.

## B. CLINICAL STUDY FOR VALIDATION

A sample of 100 patients visited at the Referral Centre for Inherited Retinal Diseases of the Academic Hospital “University of Campania Luigi Vanvitelli”, mainly affected by Retinitis Pigmentosa [13] and Stargardt Disease [14], who previously provided informed consent to participate in clinical experiments, was screened.

The following inclusion criteria were adopted for study eligibility:

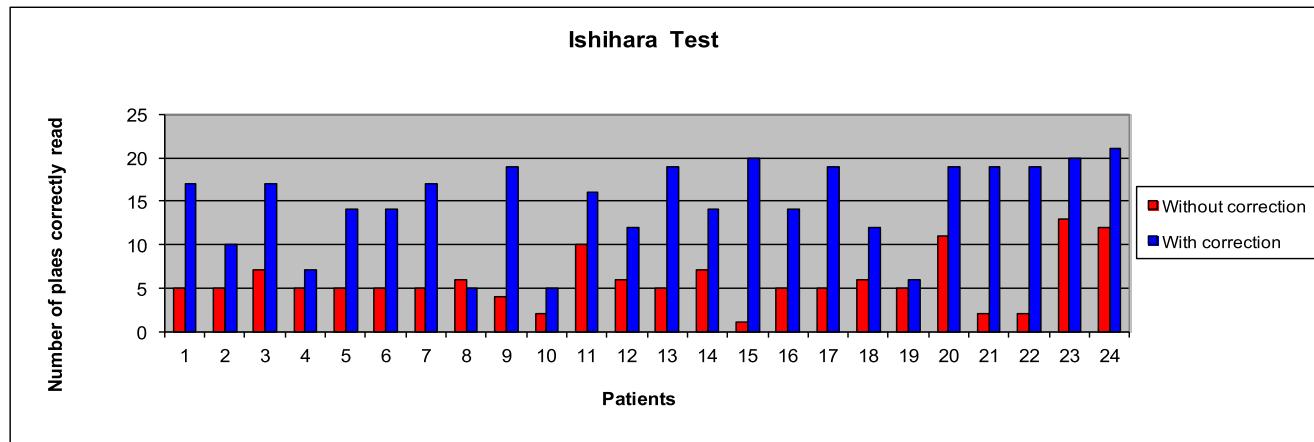
- CVD, as proven by a clinical test;
- a best corrected visual acuity (BCVA) of at least 20/200;
- living within 2-hours drive from the Hospital;
- willingness to be contacted for clinical experimentation.

A subset of 24 patients resulted eligible and accepted to be enrolled. The patients were asked to complete Farnsworth D15 test, in order to evaluate the entity of CVD. Since the latter was adopted as an additional test, unwillingness to perform Farnsworth D15 test did not affect subject inclusion. Only two subjects refused to perform the Farnsworth D15. The test score sheets were analyzed according to Bowman [15] and to moment of inertia methods [16], in particular, the following parameters were computed:

- Total Color Difference Score (TCDS), i.e., a quantitative index of colour confusion, which does not differentiate between different types of defects in individual subjects;
- Color Confusion Index (CCI), i.e., the ratio between the TCDS of the subject and the reference value. It ranges from 1 (for normal vision people) to 2 or more (for people with CVD);
- Total error score (TES), i.e., a combination of the major and minus radius used in the moment of inertia method to determine the severity of CVD (range from about 11 for normal vision, to 40 and above for severe CVD);
- Confusion Angle, i.e., the axis angle producing the minimum moment of inertia that measures the type of defect.

The above-cited parameters have been selected since they provide information about the entity and the type of CVD. Detailed description of the Farnsworth D15 parameters can be found elsewhere [15], [16].

Moreover, since BCVA is a parameter universally used to evaluate visual function in clinical trials [17], in the current study it is measured for each eye with Landolt rings [18].



**FIGURE 4.** Comparison of results of Ishihara test with and without the proposed correction for color vision deficiency.

After diagnostic testing, a computerized and modified version of the Ishihara test was performed in order to test which of the three matrices (i.e., for protanopia, deuteranopia, tritanopia) suited best for each subject. The Ishihara plates, corrected for each of the three algorithms, were randomly presented to each patient sitting in front of the monitor, and the algorithm which enabled the patient to achieve the highest score (i.e., number of Ishihara table correctly read) was selected.

Once the best matrix for the patient was chosen, the subject was invited to use the wearable system in a room with natural lighting and the luminance was measured with a luxmeter. The contrast and light intensity of the see-through system was adjusted and the subject was invited to explore the room for about 5 minutes. After that, the Ishihara test was repeated for each subject in the usual clinical manner (i.e., with Ishihara paper book), except for the use of the wearable system, without correction and with the correction suggested by the most suitable matrix for that subject. All the study procedures required about one hour and half for each subject.

The outcome measure is the difference between the score of Ishihara test conducted with and without correction for color vision deficiency.

The research followed the tenets of the Declaration of Helsinki, and informed consent was obtained before participant assessment. Ethics approval was obtained from the Institutional Review Board of the Second University of Naples.

Since this is a pilot study, no formal sample size computation was performed and a sample of 24 patients was considered to be satisfactory to test feasibility, usability and performance of the system. Differences in the main outcome measurement (i.e., the number of correctly read plates) were evaluated by paired t-test. Moreover, the correlation between the outcome measurement and other features, such as Best Corrected Visual Acuity (BCVA), Farnsworth D15 parameters, light level, was explored by Pearson correlation. A p-value lower than 5% was considered statistically significant.

### III. RESULTS

A sample of 24 patients (18 males and 6 females), aged  $37.4 \pm 14.2$ , accepted to be enrolled in the clinical experimentation to validate the system. All the subjects completed the experiment without reporting any particular problems. Table 1 shows the main clinical and demographic features of the selected sample of patients. BCVA on average was  $0.6 \pm 0.3$  in both eyes. Farnsworth D15 test, performed in 22 out of 24 patients showed:

- 8 (36.4%) patients with diffuse alteration;
- 7 (31.8%) patients with prevalent CVD in protan axis;
- 1 (4.5%) patient with prevalent CVD in deutan axis;
- 5 (22.7%) patients with prevalent CVD in tritan axis;
- 1 (4.5%) borderline patient.

The Ishihara score (i.e., number of correctly read plates) significantly improved ( $p=0.03$ ) from  $5.8 \pm 3.0$  without correction to  $14.8 \pm 5.0$  with correction for CVD which best suited the subject. As shown in Figure 4, all but one subject showed an improvement in the number of correctly read plates. In particular, 12 subjects (50%) passed the Ishihara test (i.e., more than 16 correctly read plates) with the system on, while 5 (21%) achieved a borderline result (14-16 correctly read plates), and the remaining 6 patients (25%), in spite of the color vision improvement, continued to fail the Ishihara test.

Among the three different matrices, the one for deuteranopia correction achieved the highest results in most subjects ( $n=18$  - 80%). The correlation analysis, reported in Table II, showed that the improvement in the Ishihara test score was significantly ( $p<0.01$ ) correlated with BCVA and light level, but not with Farnsworth D15 parameters.

### IV. DISCUSSION

In the current study, the design, development and clinical validation of a novel wearable system for improving color vision in CVD subjects was presented. The results achieved in the pilot experimental study are encouraging and confirm that a wearable augmented-reality platform could be feasible

**TABLE 1. Main clinical and demographic features.**

ID	Age	Sex	TCDS	CCI	TES	Angle	Alteration	BCVA RE	BCVA LE	Best Correction algorithm	baseline	Ishihara score with correction	Light level
1	27	M	231.5	1.98	26.4	64.6	diffuse	0.9	0.9	Deuteranopia	5 (fail)	17 (pass)	53
2	32	M	381.3	3.26	39.9	52.5	diffuse	0.2	0.2	Deuteranopia	5 (fail)	10 (fail)	40
3	23	M	307.1	2.62	35.7	72.4	diffuse	0.8	0.8	Deuteranopia	7 (fail)	17 (pass)	88
4	36	F	315.1	2.69	33	-88.9	tritan	0.3	0.3	Deuteranopia	5 (fail)	7 (fail)	50
5	42	M	296.1	2.53	29.7	-86.3	tritan	0.2	0.2	Deuteranopia	5 (fail)	14 (borderline)	49
6	66	M	323.6	2.77	33.1	-77.7	tritan	0.8	0.8	Deuteranopia	5 (fail)	14 (borderline)	48
7	62	F	216.7	1.85	23.1	-88.2	tritan	0.9	0.9	Protanopia	5 (fail)	17 (pass)	69
8	67	M	246.5	2.11	27	-68.2	tritan	0.4	0.4	Protanopia	6 (fail)	5 (fail)	30
9	30	M	374.3	3.2	41	12.7	protan	1	1	Deuteranopia	4 (fail)	19 (pass)	100
10	21	F	318.4	2.72	34.6	55.2	diffuse	0.8	0.7	Protanopia	2 (fail)	5 (fail)	40
11	19	M	318.1	2.72	37.4	65	diffuse	0.7	0.7	Deuteranopia	10 (fail)	16 (borderline)	46
12	23	F	299.8	2.56	31.9	3.3	protan	0.4	0.4	Deuteranopia	6 (fail)	12 (fail)	25
13	33	M	415.4	3.55	43	6.7	protan	0.9	1	Deuteranopia	5 (fail)	19 (pass)	59
14	48	M	252.5	2.16	27.9	-9.8	deutan	1	1	Deuteranopia	7 (fail)	14 (borderline)	49
15	23	M	410.4	3.51	43.9	12.1	protan	1	1	Deuteranopia	1 (fail)	20 (pass)	48
16	38	M	n/a	n/a	n/a	n/a	n/a	0.4	0.3	Deuteranopia	5 (fail)	14 (borderline)	n/a
17	39	M	n/a	n/a	n/a	n/a	n/a	0.4	0.1	Deuteranopia	5 (fail)	19 (pass)	n/a
18	24	M	473	4.04	45.5	0.3	protan	0.3	0.2	Deuteranopia	6 (fail)	12 (fail)	41
19	37	M	204.9	1.75	21.6	85.6	diffuse	0.8	0.5	Deuteranopia	5 (fail)	6 (fail)	40
20	56	M	242.1	2.07	29.6	23	protan	0.1	0.1	Tritanopia	11 (fail)	19 (pass)	44
21	30	M	315.2	2.69	35.9	16.9	protan	1	1	Deuteranopia	2 (fail)	19 (pass)	115
22	34	M	145.9	1.25	16.6	76	bordeline	1	1	Deuteranopia	2 (fail)	19 (pass)	40
23	49	F	205	1.75	21.8	73	diffuse	0.3	0.7	Protanopia	13 (fail)	20 (pass)	55
24	39	F	295.6	2.53	31.3	82.4	diffuse	0.5	0.7	Protanopia	12 (fail)	21 (pass)	56

TCDS: Total Colour Difference Score; CCI: Color Confusion Index; TES: Total Error Score; BCVA: Best Corrected Visual Acuity; RE: Right Eye; LE: Left Eye; n/a: not available

**TABLE 2. Main clinical and demographic features.**

Parameter	Pearson Correlation	p-value
TCDS (Farnsworth D15)	0.122	0.589
CCI (Farnsworth D15)	0.122	0.587
TES (Farnsworth D15)	0.172	0.443
Angle (Farnsworth D15)	0.112	0.619
BCVA RE	0.524	0.009
BCVA LE	0.533	0.007
BCVA in the best-seeing eye	0.524	0.009
Light level	0.562	0.006

TCDS: Total Color Difference Score; CCI: Color Confusion Index; TES: Total Error Score; BCVA: Best Corrected Visual Acuity; RE: Right Eye; LE: Left Eye;

and helpful for people suffering from CVD. In particular, 50% of the subjects passed the Ishihara vision color test, which is usually adopted in clinical practice to identify the most common CVD and to disqualify those affected by color blindness from certain occupations [19].

As recently reported in a review on high-tech aids for the visually impaired, one of the challenges in the field is the choice and development of appropriate outcome measurements for the evaluation of the various techniques [20]. Previous studies evaluated the proposed algorithms by subjective evaluations [21] or error metrics designed to evaluate differences between the original and corrected images [11]. Only one study adopted a computerized version of the Ishihara test, associated with other *ad hoc* designed general or specialized tests [4]. We strongly believe that, for this kind of platform, which may be considered a medical device since its aim is to restore a compromised function, a well-designed clinical study, based on a clearly defined outcome, is required for CE marking (the conformity marking within the European

Economic Area). We therefore chose the improvement in the score of Ishihara test with and without the algorithm correction as primary outcome. Since the system would be used in real-life conditions, the setting of the experiments is chosen as a room with natural light condition and the level of light was recorded. Since light level could influence the performance, we checked that, when corrected for BCVA, the correlation was not significant. For that reason, the BCVA is the main predictor of the expected improvement at the Ishihara test. Actually, the six subjects failing Ishihara test with the correction showed a significantly (p-value = 0.04) lower BCVA ( $0.46 \pm 0.27$ ) than subjects passing the test with the correction ( $0.79 \pm 0.28$ ). To this regard, we underline that it is well known in ophthalmological clinical practice that worst BCVA implies a lower discrimination ability (independently from the CVD) and a less preserved cone function [22]. Consequently, it is expected that subjects with lower BCVA could benefit less from the proposed correction.

Differently from previous studies, which mainly focused on the most frequent CVD (i.e., deuteranopia and protanopia), our system is designed to deal with all kinds of CVD. For that reason, we tested the three proposed correction matrices in all subjects and we noticed that the one for correction of deuteranopia achieved the best results in almost all patients, independently from the classification obtained by Farnsworth D15 test. In particular, we noticed that also patients, classified according to Farnsworth D15 test as probably protanomaly / protanopia; or as probably tritanomaly / tritanopia, achieved the best improvement with correction for deuteranopia. This could be explained considering the following issues: alterations in the deutan axis may be present in almost all patients with CVD, consistently with the findings of epidemiological studies [23]; the classification

provided by the Farnsworth D15 test should be confirmed by more complex tests for assessment of CVD (i.e., Farnsworth-Munsell 100 Hue Tests); the correction matrix should be adapted to deal with alterations in more than one axis. To this regard, the results of this pilot study are very useful for the development of further clinical experimentations: from the clinical point of view, they showed the need of a more accurate screening of CVD, i.e., Farnsworth-Munsell 100 Hue Tests; consequently, from the technical point of view, a future development could be the tuning of the correction matrix in order to be customized for the specific alteration of each subject.

Finally, the development of the proposed system uncovered some limitations of the state-of-art devices, such as the limited resolution of stereoscopic cameras ( $960 \times 950 \times \text{eye} @ 60\text{fps}$ ) and of HMD ( $960 \times 1080 \times \text{eye} @ 75\text{Hz}$ ), the unpleasant ghosting effect caused by a slow response time of LCD mounted on HMD. Nevertheless, new HMD based on OLED technology are coming on the market with higher resolution and refresh rate and lighter weight. The good results achieved using our prototype can be easily improved upgrading the hardware technology and adding to the developed software the management of new devices.

## V. CONCLUSIONS

The present study shows the design, development and clinical validation of a wearable system based on augmented reality devices to improve color vision in subjects with any type of CVD. Almost all subjects (96%) showed an improvement in color vision and 50%, with the system on, passed the Ishihara color vision test, which is usually adopted to identify CVD and to disqualify those affected by color blindness from certain occupations.

From the experimental results we observed that, in most cases, subjects show color vision alterations in more than one axis, suggesting that tuning the correction matrix may further improve color vision. In particular, designing new combination policies as well as weighting strategies would be of high interest.

## ACKNOWLEDGMENT

The authors would like to thank Dr Carmela Acerra for English editing on the manuscript.

## REFERENCES

1. B. Wong, "Points of view: Color blindness," *Nature Methods*, vol. 8, p. 441, May 2011.
2. B. A. Wandell, *Foundations of Vision*. Sunderland, MA, USA: Sinauer Associates, 1995.
3. X. Chen and Z. Lu, "Method and eyeglasses for rectifying color blindness," Google Patents US 5 369 453 A, Nov. 29, 1994.
4. E. Tanuwidjaja *et al.*, "Chroma: A wearable augmented-reality solution for color blindness," in *Proc. ACM Int. Joint Conf. Pervasive Ubiquitous Comput.*, Sep. 2014, pp. 799–810.
5. A. Widmer, R. Schaeer, D. Markonis, and H. Müller, "Facilitating medical information search using Google Glass connected to a content-based medical image retrieval system," in *Proc. 36th Annu. Int. Conf. IEEE Eng. Med. Biol. Soc.*, Aug. 2014, pp. 4507–4510.
6. A. Abushakra and M. Faezipour, "Augmenting breath regulation using a mobile driven virtual reality therapy framework," *IEEE J. Biomed. Health Informat.*, vol. 18, no. 3, pp. 746–752, May 2014.
7. A. V. Dowling, O. Barzilay, Y. Lombrozo, and A. Wolf, "An adaptive home-use robotic rehabilitation system for the upper body," *IEEE J. Transl. Eng. Health Med.*, vol. 2, 2014, Art. no. 2100310.
8. V. Subbian, J. J. Ratcliff, J. M. Meunier, J. J. Korfhagen, F. R. Beyette, and G. J. Shaw, "Integration of new technology for research in the emergency department: Feasibility of deploying a robotic assessment tool for mild traumatic brain injury evaluation," *IEEE J. Transl. Eng. Health Med.*, vol. 3, 2015, Art. no. 3200109.
9. R. Schaeer *et al.*, "Live ECG readings using Google Glass in emergency situations," in *Proc. 37th Annu. Int. Conf. IEEE Eng. Med. Biol. Soc. (EMBC)*, Aug. 2015, pp. 315–318.
10. D. Fortmeier, A. Mastmeyer, J. Schroder, and H. Handels, "A virtual reality system for PTCD simulation using direct Visuo-haptic rendering of partially segmented image data," *IEEE J. Biomed. Health Informat.*, vol. 20, no. 1, pp. 355–366, Jan. 2016.
11. G. M. Machado and M. M. Oliveira, "Real-time temporal-coherent color contrast enhancement for Dichromats," *Comput. Graph. Forum*, vol. 29, no. 3, pp. 933–942, Jun. 2010.
12. H. Brettel, F. Viénot, and J. D. Mollon, "Computerized simulation of color appearance for Dichromats," *J. Opt. Soc. Amer. A*, vol. 14, no. 10, pp. 2647–2655, 1997.
13. F. Testa *et al.*, "Macular abnormalities in Italian patients with retinitis pigmentosa," *Brit. J. Ophthalmol.*, vol. 98, pp. 946–950, Feb. 2014.
14. S. Rossi *et al.*, "Subretinal fibrosis in stargardt's disease with fundus flavimaculatus and ABCA4 gene mutation," *Case Rep. Ophthalmol.*, vol. 3, pp. 410–417, Dec. 2012.
15. K. J. Bowman, "A method for quantitative scoring of the farnsworth panel D-15," *Acta Ophthalmol.*, vol. 60, no. 6, pp. 907–916, Dec. 1982.
16. A. J. Vingrys and P. E. King-Smith, "A quantitative scoring technique for panel tests of color vision," *Invest. Ophthalmol. Vis. Sci.*, vol. 29, pp. 50–63, Jan. 1988.
17. G. A. Fishman *et al.*, "Outcome measures and their application in clinical trials for retinal degenerative diseases: Outline, review, and perspective," *Retina*, vol. 25, pp. 772–777, Sep. 2005.
18. C. Kniestedt and R. L. Stamper, "Visual acuity and its measurement," *Ophthalmol. Clin. North Amer.*, vol. 16, pp. 155–170, Jun. 2003.
19. A. Almagambetov, S. Velipasalar, and A. Baitassova, "Mobile standards-based traffic light detection in assistive devices for individuals with color-vision deficiency," *IEEE Trans. Intell. Transp. Syst.*, vol. 16, no. 3, pp. 1305–1320, Jun. 2015.
20. H. Moshtael, T. Aslam, I. Underwood, and B. Dhillon, "High tech aids low vision: A review of image processing for the visually impaired," *Transl. Vis. Sci. Technol.*, vol. 4, no. 4, p. 6, Aug. 2015.
21. S. Yang, Y. M. Ro, J. Nam, J. Hong, S. Y. Choi, and J.-H. Lee, "Improving visual accessibility for color vision deficiency based on MPEG-21," *Etri J.*, vol. 26, no. 3, pp. 195–202, 2004.
22. A. Krill, A. Deutman, and M. Fishman, "The cone degenerations," *Documenta Ophthalmol.*, vol. 35, no. 1, pp. 1–80, Jan. 1973.
23. M. P. Simunovic, "Color vision deficiency," *Eye (Lond)*, vol. 24, no. 5, pp. 747–755, May 2010.



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