

# **Single-Molecule Color Sensing From PSF Fitting**

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# Single-Molecule Color Sensing Methods

## Goal

Sensing spectral mean of a single emitter along with its position

- Available options
  - Optical filter bank & lambda stack construction
  - PSF engineering based on chromatic dispersion (gratings<sup>1</sup>, prism<sup>2</sup>, programmable phase mask with 4f setup<sup>3</sup>, etc.)
- **What is desired?**

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<sup>1</sup>Ma, Y. *et al. Analytical Chemistry* **72**, 4640–4645 (2000).

<sup>2</sup>Zhang, Z. *et al. Nat Meth* **12**, 935–938 (2015).

<sup>3</sup>Shechtman, Y. *et al. Nat Photon* **10**, 590–594 (2016).

# Color Sensing Methods: Criteria

- Minimum overhead in the optical setup
  - Less aberration & insertion loss, easy to apply, avoid complicated calibration
- Minimum impact on lateral/axial localization accuracy
  - Localization accuracy degrades by  $\sqrt{N}$  for  $N \times$  less photons due to beam-split
- Avoid PSF footprint enlargement
  - In SMLM context, minimize the probability of overlap of PSFs (affects temporal resolution)
- Flexibility (no need for a priori wavelength info)
- Good  $\lambda$  estimation accuracy for given photon budget
- Avoid possibility of bias from non-idealities

# SM Color Sensing From PSF Fitting

- Diffraction-limited image of a single molecule already contains color information

$$\text{First minimum of Airy pattern} = 0.61 \frac{\lambda}{NA}$$

- In principle, it should be possible to estimate emitter color from the scale of the fitted PSF
- Spectrally resolved SMLM: just installation of a ImageJ plugin!
  - Literally zero impact on the optical setup/xyz accuracy
  - No PSF modification (more than whats required for 3D)
  - No a priori information

## Questions to be answered

- Good enough  $\lambda$  estimation accuracy in realistic scenario?
  - Axial position dependency in 2D situation
- Possibility of bias from non-idealities (not limited to)
  - Chromatic/spherical aberration
  - Spectral profile of the fluorophore (bandwidth, skewness)
  - Non-uniform background
  - Deconvolution artifacts
  - Motion blur
  - Fluorophore orientation

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# Performance of Measurement Method

## Task

Estimation of  $x, y, z, \bar{\lambda}$  of a single emitter from values of sensor array (EMCCD, sCMOS) within certain ROI

- A “measurement method” includes:
  - PSF design (how you encode the information to actual image: prism/grating, astigmatism, double helix, etc.)
  - Corresponding optical setting (affecting SNR, bias)
  - Reconstruction algorithm (LS/MLE, ROI selection, b/g correction, etc.)
- Performance metrics
  - Highest accuracy (smallest  $\sigma$ ) for given number of photons & noise profile
  - Unbiased
  - PSF footprint

# Design of Measurement Method

- Major design decisions in our context
  - PSF design/PSF model to use (optical setting is determined by this)
  - Deconvolution algorithm
- Today's question: what's the theoretical bound for wavelength estimation accuracy and the impact of PSF choice?
  - Fix everything other than PSF
    - Magnification, noise, pixel size, ROI, NA, illumination
  - Consider only major physical implication of PSF design choice
    - e.g. consider beam split, but not the insertion loss from additional optical elements



# Problem Setting

- PSF options
  - *Plain-vanilla* circular aperture
  - Multifocus (biplane)
  - Astigmatism
  - Double-helix
- Assumptions
  - $NA=1.4$ , effective pixel size=100nm, ROI=20x20 pixels
  - Only shot noise, uniform background of 10 photons/pixel
  - Ignore aberration
  - Model a fluorophore as an monochromatic/isotropic emitter
- Procedure
  - Compute Cramér-Rao lower bound (CRLB) for different  $z$  location & number of photons

## Circular Aperture Case

- 3D PSF model for simple circular aperture: Born & Wolf model

$$q_{z_0}(\vec{r} - \vec{r}_0) = \left\| A \int_0^1 J_0 \left( \frac{2\pi}{\lambda} \text{NA} \|\vec{r} - \vec{r}_0\| \rho \right) e^{-j \frac{\pi}{\lambda} \rho^2 z_0 \left( \frac{\text{NA}^2}{n_i} \right)} \rho d\rho \right\|^2$$

$A$ : normalization constant,  $n_i$ : refractive index of the immersion oil

$J_0$ : zeroth order Bessel function of the first kind

- Fisher information matrix with pixelation & shot noise<sup>4</sup>

$$I_{ij}(\boldsymbol{\theta}) = \sum_{k=1}^{N_{\text{pixel}}} \frac{1}{\mu_k(\boldsymbol{\theta}) + \beta} \left( \frac{\partial \mu_k(\boldsymbol{\theta})}{\partial \theta_i} \right) \left( \frac{\partial \mu_k(\boldsymbol{\theta})}{\partial \theta_j} \right)$$

$\mu_k(\boldsymbol{\theta})$ : the value of the model PSF in pixel  $k$

$N_{\text{pixel}}$ : the number of pixels in the ROI

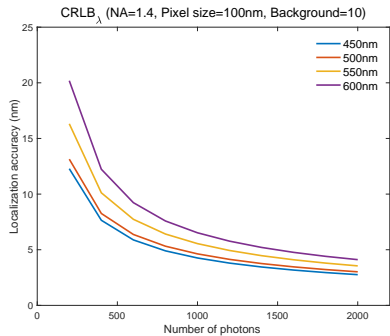
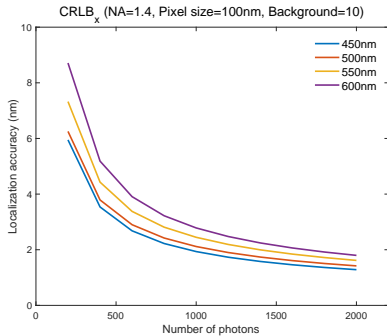
$\beta$ : background photons per pixel

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<sup>4</sup>Ober, R. J. *et al. Biophysical Journal* **86**, 1185–1200 (2004).

# Circular Aperture Case

- For  $z = 0$



## Impact of Defocusing

- Defocusing introduces biasing to wavelength estimation
  - Accuracy bound should take into account both bias & CRLB
- Generalized CRLB in presence of bias

$$\text{Var}(\hat{\lambda}) \geq \frac{[1 + b'(\lambda)]^2}{I(\lambda)}$$

$b(\lambda)$ : bias,  $I(\lambda)$ : Fisher information

- CRLB is  $z$  dependent

$$b(\lambda) = \lambda(M(z) - 1), \quad b'(\lambda) = M(z) - 1$$

$$\text{Var}(\hat{\lambda})|_z \geq \frac{M(z)^2}{I(\lambda)|_z}$$

$M(z)$ : magnification factor of the PSF at  $z$

## Impact of Defocusing

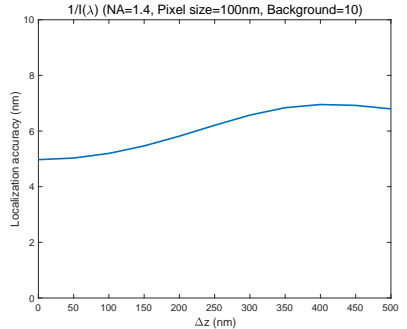
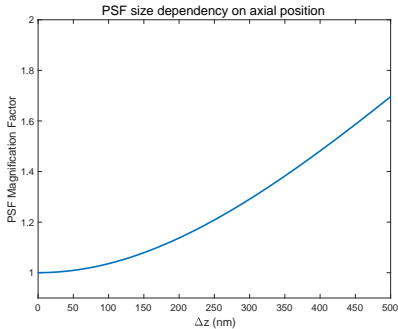
- Assuming certain distribution for  $z$ , performance bound in presence of  $z$  variation can be calculated
  - Mean squared error at  $z$ :  $E[(\hat{\lambda} - \lambda)^2]_z = \text{Var}(\hat{\lambda})_z + b(z)^2$
  - Final CRLB is calculated as a weighted sum over  $z$

$$\begin{aligned} CRLB_{\lambda} &= \int_{z_{min}}^{z_{max}} E[(\hat{\lambda} - \lambda)^2] f(z) dz \\ &= \int_{z_{min}}^{z_{max}} \left( \text{Var}(\hat{\lambda})_z + b(\lambda)^2 \right) f(z) dz \\ &\geq 2 \int_0^{\Delta z_{max}} \left( \frac{M(z)^2}{I(\lambda)_z} + \lambda^2 (M(z) - 1)^2 \right) f(z) dz \end{aligned}$$

- PSF Symmetry over  $z$ ,  $f(z)$ : probability distribution of  $z$
- For  $M(z) = 1$ , converges to the CRLB at  $z = 0$

# Impact of Defocusing

- Magnification factor & Fisher information vs.  $z$ 
  - $N_{\text{photon}}=1500$ ,  $\lambda=600\text{nm}$ ,  $n_i=1.5$ , Born & Wolf model



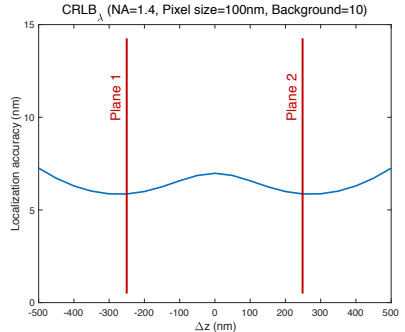
- For  $\Delta z_{\text{max}}=100\text{nm}$  &  $f(z)=\text{uniform}$ , CRLB=9.86nm (originally 4.97nm)
- For  $\Delta z_{\text{max}}=500\text{nm}$ , CRLB=177nm!

# 3D+Color: Multifocal Plane

- Total Fisher information matrix is the sum of FI from each imaging plane<sup>5</sup>

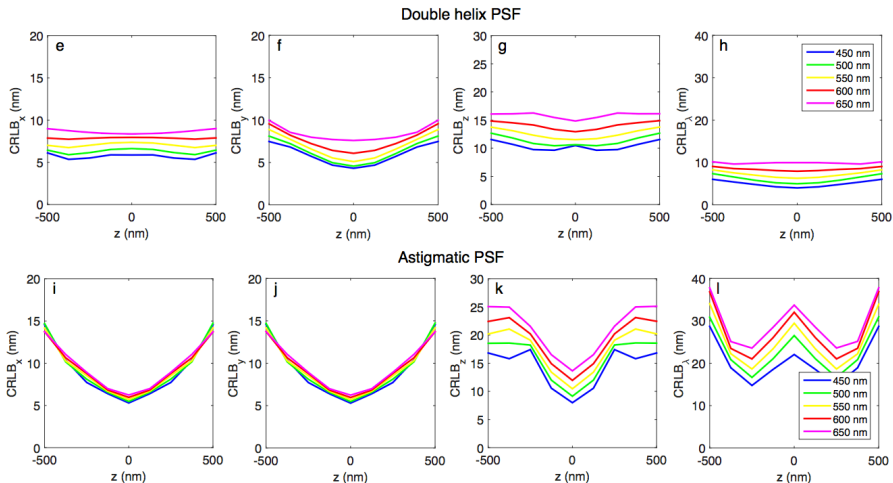
$$I_{tot}(\boldsymbol{\theta}) = \sum_{i=1}^{N_{plane}} I_i(\boldsymbol{\theta})$$

- Biplane setting
  - $N_{photon}=1500$ ,  $\lambda=600\text{nm}$
  - 50/50 beam split (750 photons/plane)
  - Distance between planes: 500nm



<sup>5</sup>Ram, S. *et al. Biophysical Journal* **95**, 6025–6043 (2008).

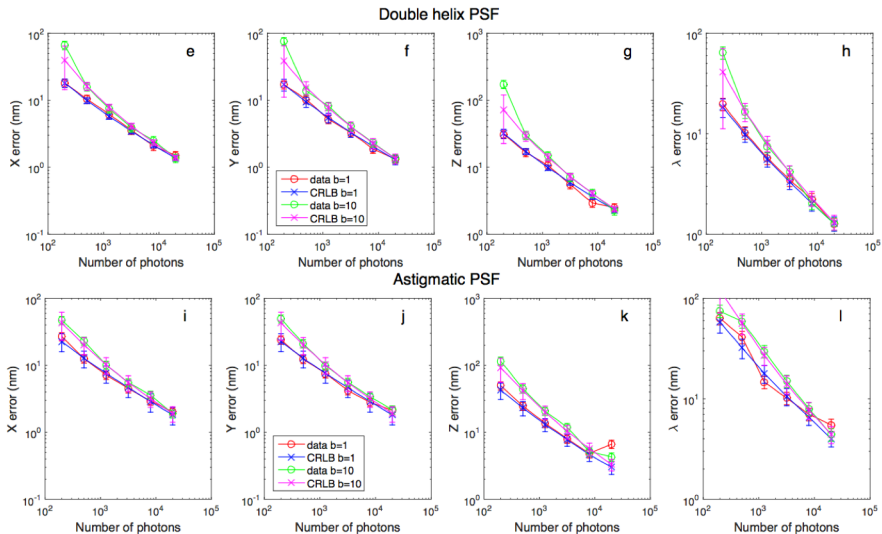
# 3D+Color: Double Helix/Astigmatic<sup>6</sup>



<sup>6</sup>Smith, C. et al. *Optics Express* **24** (2016).



# 3D+Color: Double Helix/Astigmatic<sup>6</sup>



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# Conclusions

- Takeaways from CRLB calculation
  - Can work with useful accuracy ( $\sim 10\text{nm}$ ) only when  $z$  &  $\lambda$  are disentangled
  - Looks promising for biplane & dual helix PSF
- Next steps:
  - Fluorophore spectrum/dipole moment dependence
    - If there's a performance difference between beads and single molecule, this could be the reason
  - Quantitative comparison with chromatic dispersion-based methods
  - Characterize readout noise
  - Actual PSF & chromatic aberration analysis for microscopes in the lab
    - Tools such as PSFj<sup>7</sup> can be applied
  - Compare to the fitted simulation dataset or experimental data
  - Right fitting algorithm to achieve close-CRLB performance

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<sup>7</sup>Theer, P. *et al. Nat Meth* **11**, 981–982 (2014).