

Spatio-angular fluorescence microscopy

II. Paraxial 4f imaging

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Abstract: We investigate the properties of a single-view fluorescence microscope in a 4f geometry when imaging fluorescent dipoles without using the monopole or scalar approximations. We show that this imaging system has a spatio-angular band limit, and we exploit the band limit to perform efficient simulations. Notably, we show that information about the out-of-plane orientation of ensembles of in-focus fluorophores is recorded by paraxial fluorescence microscopes. Additionally, we show that the monopole approximation may cause biased estimates of fluorophore concentrations, but these biases are small when the sample contains either many randomly oriented fluorophores in each resolvable volume or unconstrained rotating fluorophores.

1. Introduction

In the first paper of this series we developed a new set of transfer functions that can be used to analyze spatio-angular fluorescence microscopes [1]. In this work we will demonstrate these transfer functions by analyzing a single-view fluorescence microscope in a 4f geometry.

A central goal of this work is to examine the validity of the monopole approximation in fluorescence microscopy. Although many works implicitly apply the monopole approximation, we have encountered two explicit justifications: (1) the sample contains many randomly oriented fluorophores within a resolvable volume or (2) the sample contains unconstrained rotating fluorophores. While both of these situations yield monopole-like emitters, neither yields emitters that are perfectly described by the monopole model. We investigate the dipole model of fluorophores in detail and find the conditions under which the monopole approximation is justified.

We begin in section 2 by specifying the imaging geometry and defining *pupil functions* for imaging systems with and without the monopole approximation. We explicitly relate the pupil functions to the coherent transfer functions to establish a connection between physical calculations and the transfer functions. Next, in section 3 we calculate the monopole and dipole transfer functions in closed form, and we use these transfer functions to perform efficient simulations with four numerical phantoms. Finally, in section 4 we discuss the results and expand on how the pupil functions can be used to develop improved models for spatio-angular microscopes.

2. Theory

During our initial modeling [1] we considered an aplanatic optical system imaging a sample of in-focus fluorophores—either a monopole density, $f(\mathbf{r}_o)$, or a dipole density, $f(\mathbf{r}_o, \hat{\mathbf{s}}_o)$ —by recording the scaled irradiance on a two-dimensional detector, $g(\mathbf{r}_d)$. A central result was that we could express the relationship between the object and the data as a linear Hilbert-space operator, and we showed that these operators took the form of an integral transform in a delta function

Quantity	Symbol	Relationships
Monopole density	$f(\mathbf{r}_o)$	—
Monopole spectrum	$F(\boldsymbol{\nu})$	$= \mathcal{F}_{\mathbb{R}^2}\{f(\mathbf{r}_o)\}$
Monopole coherent spread function	$c(\mathbf{r}_d - \mathbf{r}_o)$	—
Monopole coherent transfer function	$C(\boldsymbol{\tau})$	$= \mathcal{F}_{\mathbb{R}^2}\{c(\mathbf{r}_d - \mathbf{r}_o)\}$
Monopole point spread function	$h(\mathbf{r}_d - \mathbf{r}_o)$	$= c(\mathbf{r}_d - \mathbf{r}_o) ^2$
Monopole transfer function	$H(\boldsymbol{\nu})$	$= \mathcal{F}_{\mathbb{R}^2}\{h(\mathbf{r}_d - \mathbf{r}_o)\}$ $= \int_{\mathbb{R}^2} d\boldsymbol{\tau} C(\boldsymbol{\tau}) C^*(\boldsymbol{\tau} - \boldsymbol{\nu})$
Scaled irradiance	$g(\mathbf{r}_d)$	$= \int_{\mathbb{R}^2} d\mathbf{r}_o h(\mathbf{r}_d - \mathbf{r}_o) f(\mathbf{r}_o)$
Scaled irradiance spectrum	$G(\boldsymbol{\nu})$	$= \mathcal{F}_{\mathbb{R}^2}\{g(\mathbf{r}_d)\} = H(\boldsymbol{\nu}) F(\boldsymbol{\nu})$

Table 1. Summary of relevant quantities in fluorescence microscopy under the monopole approximation—see [1] for derivations. $\mathcal{F}_{\mathbb{R}^2}$ denotes a two-dimensional Fourier transform.

basis. For monopoles the integral transform takes the form

$$g(\mathbf{r}_d) = \int_{\mathbb{R}^2} d\mathbf{r}_o h(\mathbf{r}_d - \mathbf{r}_o) f(\mathbf{r}_o), \quad (1)$$

where $h(\mathbf{r}_d - \mathbf{r}_o)$ is the monopole point spread function. For dipoles the integral transform takes the form

$$g(\mathbf{r}_d) = \int_{\mathbb{S}^2} d\hat{\mathbf{s}}_o \int_{\mathbb{R}^2} d\mathbf{r}_o h(\mathbf{r}_d - \mathbf{r}_o, \hat{\mathbf{s}}_o) f(\mathbf{r}_o, \hat{\mathbf{s}}_o), \quad (2)$$

where $h(\mathbf{r}_d - \mathbf{r}_o, \hat{\mathbf{s}}_o)$ is the dipole point spread function. Note that we have written Eqs. (1) and (2) in their demagnified forms. We will use primes to denote the unscaled detector coordinate, \mathbf{r}'_d , and unscaled point spread functions, h' .

After expressing the operators in a delta function basis we explored the form of the operators with several other choices of basis functions. Tables 1 and 2 summarize our results.

Our task is to calculate the form of the monopole and dipole transfer functions for a specific imaging geometry. In this work we will consider an aplanatic optical system in a *4f configuration* with an arbitrary first lens (the objective lens) and a *paraxial second lens* (the tube lens) as shown in Fig. 1. A lens can be considered paraxial if the angle α between the optical axis of the lens and the marginal ray is small enough that $\sin \alpha \approx \alpha$. As a rule of thumb, non-paraxial effects only become significant when the numerical aperture of a lens exceeds 0.7 [2, ch. 6], but this is only a rough guideline. Commercial microscopes with infinity-corrected objectives can almost always be modeled by considering the tube lens as paraxial.

2.1. Monopole pupil functions

We define the *monopole pupil function* $p(\mathbf{r}_p)$ of the imaging system as the field immediately following the pupil plane created by an on-axis monopole, where \mathbf{r}_p is an unscaled two-dimensional coordinate in the pupil plane. In this section we will relate the monopole pupil function to the monopole transfer functions by adapting the treatment in Barrett and Myers [3, ch. 9.7].

Quantity	Symbol	Relationships
Dipole density	$f(\mathbf{r}_o, \hat{\mathbf{s}}_o)$	—
Dipole spatial spectrum	$F(\mathbf{v}, \hat{\mathbf{s}}_o)$	$= \mathcal{F}_{\mathbb{R}^2}\{f(\mathbf{r}_o, \hat{\mathbf{s}}_o)\}$
Dipole angular spectrum	$F_\ell^m(\mathbf{r}_o)$	$= \mathcal{F}_{\mathbb{S}^2}\{f(\mathbf{r}_o, \hat{\mathbf{s}}_o)\}$
Dipole spatio-angular spectrum	$F_\ell^m(\mathbf{v})$	$= \mathcal{F}_{\mathbb{R}^2}\{F_\ell^m(\mathbf{r}_o)\} = \mathcal{F}_{\mathbb{S}^2}\{F(\mathbf{v}, \hat{\mathbf{s}}_o)\}$
Dipole coherent spread function	$\mathbf{c}(\mathbf{r}_d - \mathbf{r}_o, \hat{\mathbf{s}}_o)$	—
Dipole coherent transfer function	$\mathbf{C}(\boldsymbol{\tau}, \hat{\mathbf{s}}_o)$	$= \mathcal{F}_{\mathbb{R}^2}\{\mathbf{c}(\mathbf{r}_d - \mathbf{r}_o, \hat{\mathbf{s}}_o)\}$
Dipole point spread function	$h(\mathbf{r}_d - \mathbf{r}_o, \hat{\mathbf{s}}_o)$	$= \mathbf{c}(\mathbf{r}_d - \mathbf{r}_o, \hat{\mathbf{s}}_o) ^2$
Dipole spatial transfer function	$H(\mathbf{v}, \hat{\mathbf{s}}_o)$	$= \mathcal{F}_{\mathbb{R}^2}\{h(\mathbf{r}_d - \mathbf{r}_o, \hat{\mathbf{s}}_o)\}$ $= \int_{\mathbb{R}^2} d\boldsymbol{\tau} \mathbf{C}(\boldsymbol{\tau}, \hat{\mathbf{s}}_o) \mathbf{C}^\dagger(\boldsymbol{\tau} - \mathbf{v}, \hat{\mathbf{s}}_o)$
Dipole angular transfer function	$H_\ell^m(\mathbf{r}_d - \mathbf{r}_o)$	$= \mathcal{F}_{\mathbb{S}^2}\{h(\mathbf{r}_d - \mathbf{r}_o, \hat{\mathbf{s}}_o)\}$
Dipole spatio-angular transfer function	$H_\ell^m(\mathbf{v})$	$= \mathcal{F}_{\mathbb{R}^2}\{H_\ell^m(\mathbf{r}_d - \mathbf{r}_o)\} = \mathcal{F}_{\mathbb{S}^2}\{H(\mathbf{v}, \hat{\mathbf{s}}_o)\}$
Scaled irradiance	$g(\mathbf{r}_d)$	$= \int_{\mathbb{S}^2} d\hat{\mathbf{s}}_o \int_{\mathbb{R}^2} d\mathbf{r}_o h(\mathbf{r}_d - \mathbf{r}_o, \hat{\mathbf{s}}_o) f(\mathbf{r}_o, \hat{\mathbf{s}}_o)$ $= \sum_{\ell m} \int_{\mathbb{R}^2} d\mathbf{r}_o H_\ell^m(\mathbf{r}_d - \mathbf{r}_o) F_\ell^m(\mathbf{r}_o)$
Scaled irradiance spectrum	$G(\mathbf{v})$	$= \mathcal{F}_{\mathbb{R}^2}\{g(\mathbf{r}_d)\}$ $= \int_{\mathbb{S}^2} d\hat{\mathbf{s}}_o H(\mathbf{v}, \hat{\mathbf{s}}_o) F(\mathbf{v}, \hat{\mathbf{s}}_o)$ $= \sum_{\ell m} H_\ell^m(\mathbf{v}) F_\ell^m(\mathbf{v})$

Table 2. Summary of relevant quantities in spatio-angular dipole imaging—see [1] for derivations. $\mathcal{F}_{\mathbb{R}^2}$ denotes a two-dimensional Fourier transform, and $\mathcal{F}_{\mathbb{S}^2}$ denotes a spherical Fourier transform.

Since monopoles emit scalar fields, the monopole pupil function is a scalar-valued function. The optical system is aplanatic, so we can write the field, $U_p(\mathbf{r}_p, \mathbf{r}_o)$, created at a point in the pupil plane \mathbf{r}_p by a monopole at position \mathbf{r}_o as

$$U_p(\mathbf{r}_p, \mathbf{r}_o) \propto p(\mathbf{r}_p) \exp\left[-2\pi i \frac{n_0}{\lambda f_0} \mathbf{r}_p \cdot \mathbf{r}_o\right], \quad (3)$$

where λ is the emission wavelength. Equation (3) is a restatement of the aplanatic condition for a $4f$ optical system—the fields in the pupil plane can be written as the pupil function multiplied by a linear phase factor that encodes the position of the object.

Since the second lens is paraxial, we can model the relationship between the field in the pupil plane and the field on the detector with a scaled Fourier transform [4–6]:

$$U_d(\mathbf{r}'_d, \mathbf{r}_o) \propto \int_{\mathbb{R}^2} d\mathbf{r}_p p(\mathbf{r}_p) \exp\left[-2\pi i \frac{n_0}{\lambda f_0} \mathbf{r}_p \cdot \mathbf{r}_o\right] \exp\left[-2\pi i \frac{n_1}{\lambda f_1} \mathbf{r}_p \cdot \mathbf{r}'_d\right], \quad (4)$$

where \mathbf{r}'_d is an unscaled detector coordinate.

If we define $P(\boldsymbol{\tau})$ as the two-dimensional Fourier transform of the pupil function then we can

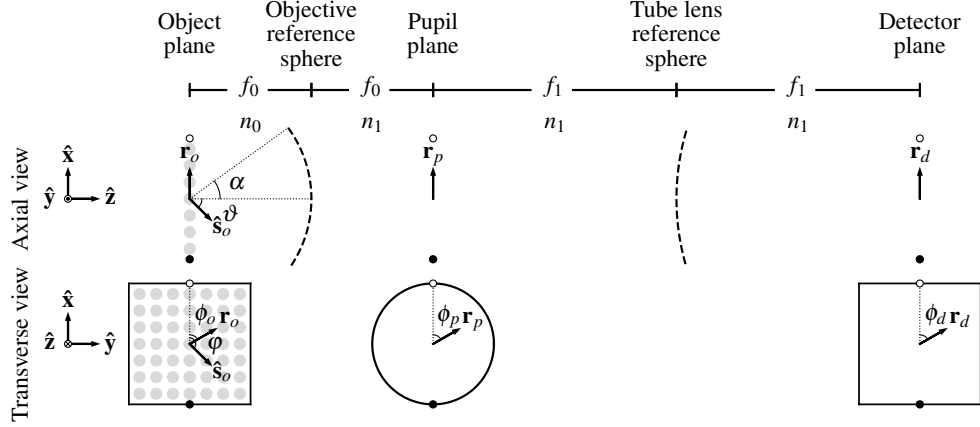


Fig. 1. Schematic of an aplanatic imaging system in a $4f$ geometry with a paraxial tube lens. We are considering an aplanatic optical system, so we only need to consider the image created by on-axis objects. The fluorescent object consists of ensembles of monopoles or dipoles embedded in a medium with index of refraction n_0 . An objective with focal length f_0 and numerical aperture $\text{NA} = n_0 \sin \alpha$ is trained on the object. A paraxial tube lens with focal length f_1 and a detector complete the $4f$ geometry, and all components except the object are embedded in a medium with index of refraction n_1 . The object, pupil, and detector planes are parameterized by vectors \mathbf{r}_o , \mathbf{r}_p , and \mathbf{r}_d with polar coordinates (r_o, ϕ_o) , (r_p, ϕ_p) , and (r_d, ϕ_d) , respectively. At each position \mathbf{r}_o in the object there is a sphere parameterized by a unit vector $\hat{\mathbf{s}}_o$ with spherical coordinates (ϑ, φ) .

rewrite Eq. (4) as

$$U_d(\mathbf{r}'_d, \mathbf{r}_o) \propto P\left(\frac{n_0}{\lambda f_0} \mathbf{r}_o + \frac{n_1}{\lambda f_1} \mathbf{r}'_d\right), \quad (5)$$

which we can simplify further by writing in terms of the magnification $m = -\frac{f_1 n_0}{f_0 n_1}$:

$$U_d(\mathbf{r}'_d - m\mathbf{r}_o) \propto P\left(\frac{n_1}{\lambda f_1} [\mathbf{r}'_d - m\mathbf{r}_o]\right). \quad (6)$$

The irradiance on the detector is the absolute square of the field so

$$h'(\mathbf{r}'_d - m\mathbf{r}_o) \propto \left| P\left(\frac{n_1}{\lambda f_1} [\mathbf{r}'_d - m\mathbf{r}_o]\right) \right|^2. \quad (7)$$

If we demagnify the coordinates with $\mathbf{r}_d = \mathbf{r}'_d/m$ and demagnify the irradiance with $h(\mathbf{r}_d - \mathbf{r}_o) \propto h'(m[\mathbf{r}_d - \mathbf{r}_o])$, we find that the monopole point spread function is related to the Fourier transform of the monopole pupil function by

$$h(\mathbf{r}_d - \mathbf{r}_o) \propto \left| P\left(-\frac{n_o}{\lambda f_o} [\mathbf{r}_d - \mathbf{r}_o]\right) \right|^2. \quad (8)$$

The monopole point spread function is the absolute square of the monopole coherent spread function so

$$c(\mathbf{r}_d - \mathbf{r}_o) \propto P\left(-\frac{n_o}{\lambda f_o} [\mathbf{r}_d - \mathbf{r}_o]\right). \quad (9)$$

Finally, the monopole coherent transfer function is the Fourier transform of the monopole coherent spread function so

$$C(\boldsymbol{\tau}) \propto p\left(\frac{\lambda f_o}{n_o} \boldsymbol{\tau}\right). \quad (10)$$

Equation (10) is the key result of this section—the monopole coherent transfer function is a scaled monopole pupil function.

2.2. Dipole pupil function

We define the *dipole pupil function* $\mathbf{p}(\mathbf{r}_p, \hat{\mathbf{s}}_o)$ of the imaging system as the electric field immediately following the pupil plane created by an on-axis dipole oriented along $\hat{\mathbf{s}}_o$. Since dipoles emit vector-valued electric fields, the dipole pupil function is a vector-valued function. Almost all of the arguments in the previous section carry over to the dipole case. Briefly, we can write the electric field created at a point in the pupil \mathbf{r}_p by a dipole at \mathbf{r}_o oriented along $\hat{\mathbf{s}}_o$ as

$$\mathbf{E}_p(\mathbf{r}_p, \mathbf{r}_o, \hat{\mathbf{s}}_o) \propto \mathbf{p}(\mathbf{r}_p, \hat{\mathbf{s}}_o) \exp\left[-2\pi i \frac{n_o}{\lambda f_0} \mathbf{r}_p \cdot \mathbf{r}_o\right]. \quad (11)$$

The second lens is paraxial, so we can find the field on the detector with a Fourier transform

$$\mathbf{E}_d(\mathbf{r}'_d, \mathbf{r}_o, \hat{\mathbf{s}}_o) \propto \int_{\mathbb{R}^2} d\mathbf{r}_p \mathbf{p}(\mathbf{r}_p, \hat{\mathbf{s}}_o) \exp\left[-2\pi i \frac{n_o}{\lambda f_0} \mathbf{r}_p \cdot \mathbf{r}_o\right] \exp\left[-2\pi i \frac{n_1}{\lambda f_1} \mathbf{r}_p \cdot \mathbf{r}'_d\right]. \quad (12)$$

Note that the Fourier transform of a vector field is the Fourier transform of its scalar-valued orthogonal components, so Eq. (12) specifies three two-dimensional Fourier transforms. We follow the same manipulations as the previous section and find that the dipole coherent transfer function is a scaled dipole pupil function

$$\mathbf{C}(\boldsymbol{\tau}, \hat{\mathbf{s}}_o) \propto \mathbf{p}\left(\frac{\lambda f_o}{n_o} \boldsymbol{\tau}, \hat{\mathbf{s}}_o\right). \quad (13)$$

We have restricted our analysis to paraxial tube lenses, but non-paraxial tube lenses (or a non-infinity-corrected objective) can be modeled with vector-valued three-dimensional pupil functions [2, 7–9].

2.3. Special functions

We adopt and generalize Bracewell's notation [10] for several special functions which will simplify our calculations. First, we define a *rectangle function* as

$$\Pi(x) = \begin{cases} 1 & \text{if } |x| < \frac{1}{2}, \\ 0 & \text{else.} \end{cases} \quad (14)$$

We also define the n^{th} -order *jinc function* as

$$\text{jinc}_n(r) = \frac{J_{n+1}(\pi r)}{2r}, \quad (15)$$

where $J_{n+1}(r)$ is the $(n+1)^{\text{th}}$ -order Bessel function of the first kind.

Although the rectangle and jinc functions are defined in one dimension, we will usually apply them in two dimensions. In Appendix A we derive the following two-dimensional Fourier transform relationships between the jinc functions and the weighted rectangle functions

$$i^n \begin{Bmatrix} \exp(in\phi_r) \\ \cos(n\phi_r) \\ \sin(n\phi_r) \end{Bmatrix} \text{jinc}_n(r) \xrightarrow{\mathcal{F}_{\mathbb{R}^2}} (2v)^n \begin{Bmatrix} \exp(in\phi_v) \\ \cos(n\phi_v) \\ \sin(n\phi_v) \end{Bmatrix} \Pi(v), \quad (16)$$

where the entries inside the curly braces are to be taken one at a time and $\{r, \phi_r\}/\{\nu, \phi_\nu\}$ are conjugate sets of polar coordinates.

Finally, we define the n^{th} -order chat function as the two-dimensional Fourier transform of the squared n^{th} -order jinc function

$$\text{jinc}_n^2(r) \xrightarrow{\mathcal{F}_{\mathbb{R}^2}} \text{chat}_n(\nu). \quad (17)$$

In Appendix A we show that the zeroth- and first-order chat functions can be written in closed form as

$$\text{chat}_0(x) = \frac{1}{2} \left[\cos^{-1} |x| - |x| \sqrt{1 - x^2} \right] \Pi\left(\frac{x}{2}\right), \quad (18)$$

$$\text{chat}_1(x) = \frac{1}{2} \left[\cos^{-1} |x| - |x| (3 - 2x^2) \sqrt{1 - x^2} \right] \Pi\left(\frac{x}{2}\right). \quad (19)$$

3. Results

3.1. Monopole transfer functions

Our first step towards the monopole transfer functions is to calculate the monopole pupil function and coherent transfer function. Several works [11, 12] have modeled an aplanatic fluorescence microscope imaging monopole emitters with the scalar pupil function

$$p(\mathbf{r}_p) \propto \tilde{C}\left(\frac{r_p}{f_o}\right) \Pi\left(\frac{r_p}{2f_o \sin \alpha}\right), \quad (20)$$

where

$$\tilde{C}(x) = (1 - x^2)^{-1/4} = 1 + \frac{x^2}{4} + \frac{5x^4}{32} + \dots \quad (21)$$

The $\tilde{C}(x)$ function models the radial dependence of the field and ensures that power is conserved on either side of an aplanatic objective, and the rectangle function models the aperture stop of the objective. Applying Eq. (10) and collecting constants we find that the coherent monopole transfer function is

$$C(\boldsymbol{\tau}) \propto \tilde{C}\left(\frac{2\text{NA}}{n_o} \frac{\tau}{\nu_c}\right) \Pi\left(\frac{\tau}{\nu_c}\right), \quad (22)$$

where $\text{NA} = n_o \sin \alpha$ and $\nu_c = 2\text{NA}/\lambda$. This coherent transfer function models objectives with an arbitrary numerical aperture, but for our initial analysis we restrict ourselves to the paraxial regime. We drop second- and higher-order radial terms to find that

$$C(\boldsymbol{\tau}) \stackrel{(p)}{\propto} \Pi\left(\frac{\tau}{\nu_c}\right), \quad (23)$$

where (p) indicates that we have used the paraxial approximation for the objective lens.

We can find the monopole coherent spread function by taking the inverse Fourier transform of the monopole coherent transfer function

$$c(\mathbf{r}) \stackrel{(p)}{\propto} \text{jinc}_0(\nu_c r). \quad (24)$$

The monopole point spread function is the (normalized) absolute square of the monopole coherent spread function so

$$h(\mathbf{r}) \stackrel{(p)}{=} \frac{4}{\pi} \text{jinc}_0^2(\nu_c r), \quad (25)$$

which is the well-known *Airy disk*.

Finally, we can calculate the monopole transfer function as the two-dimensional Fourier transform of the monopole point spread function (or the autocorrelation of the coherent transfer function) and find that

$$H(\mathbf{v}) \stackrel{(p)}{=} \frac{4}{\pi} \text{chat}_0\left(\frac{\mathbf{v}}{v_c}\right). \quad (26)$$

3.2. Dipole transfer functions

To calculate the dipole transfer function we proceed similarly to the monopole case—we find the pupil function, scale to find the coherent dipole transfer function, then calculate the remaining transfer functions.

Backer and Moerner [6] have calculated the dipole pupil function for a high-NA objective as

$$\mathbf{p}(\mathbf{r}_p, \hat{\mathbf{s}}_o) \propto \begin{bmatrix} \tilde{C}_0\left(\frac{r_p}{f_o}\right) + \tilde{C}_2\left(\frac{r_p}{f_o}\right)c(2\phi_p) & \tilde{C}_2\left(\frac{r_p}{f_o}\right)s(2\phi_p) & \tilde{C}_1\left(\frac{r_p}{f_o}\right)c(\phi_p) \\ \tilde{C}_2\left(\frac{r_p}{f_o}\right)s(2\phi_p) & \tilde{C}_0\left(\frac{r_p}{f_o}\right) - \tilde{C}_2\left(\frac{r_p}{f_o}\right)c(2\phi_p) & \tilde{C}_1\left(\frac{r_p}{f_o}\right)s(\phi_p) \\ 0 & 0 & 0 \end{bmatrix} \begin{bmatrix} s_x \\ s_y \\ s_z \end{bmatrix} \Pi\left(\frac{r_p}{2f_o s(\alpha)}\right), \quad (27)$$

where $c(x)$ and $s(x)$ are shorthand for $\cos(x)$ and $\sin(x)$, $\{s_x, s_y, s_z\}$ are the Cartesian components of $\hat{\mathbf{s}}_o$ when $\hat{\mathbf{z}}$ is aligned with the optical axis, and

$$\tilde{C}_0(x) = \frac{1}{2}(\sqrt{1-x^2} + 1)(1-x^2)^{-1/4} = 1 + \frac{x^4}{32} + \frac{x^6}{32} + \dots, \quad (28)$$

$$\tilde{C}_1(x) = x(1-x^2)^{-1/4} = x + \frac{x^3}{4} + \frac{5x^5}{32} + \dots, \quad (29)$$

$$\tilde{C}_2(x) = \frac{1}{2}(\sqrt{1-x^2} - 1)(1-x^2)^{-1/4} = -\frac{x^2}{4} - \frac{x^4}{8} - \frac{11x^6}{128} - \dots. \quad (30)$$

Similar to the monopole case, the dipole pupil function conserves power and has a cutoff at the objective aperture, but the dipole pupil function is vector-valued to model the complete electric field in the pupil plane. The fields in the pupil plane have a negligible $\hat{\mathbf{z}}$ component which is a consequence of our assumption that the tube lens is paraxial—modeling a non-paraxial tube lens would require a three-dimensional vector-valued pupil function [2, 7–9].

Scaling the dipole pupil function using Eq. (13) yields the dipole coherent transfer function

$$\mathbf{C}(\boldsymbol{\tau}, \hat{\mathbf{s}}_o) \propto \begin{bmatrix} \tilde{C}_0\left(\frac{\lambda r_p \tau}{n_o}\right) + \tilde{C}_2\left(\frac{\lambda r_p \tau}{n_o}\right)c(2\phi_\tau) & \tilde{C}_2\left(\frac{\lambda r_p \tau}{n_o}\right)s(2\phi_\tau) & \tilde{C}_1\left(\frac{\lambda r_p \tau}{n_o}\right)c(\phi_\tau) \\ \tilde{C}_2\left(\frac{\lambda r_p \tau}{n_o}\right)s(2\phi_\tau) & \tilde{C}_0\left(\frac{\lambda r_p \tau}{n_o}\right) - \tilde{C}_2\left(\frac{\lambda r_p \tau}{n_o}\right)c(2\phi_\tau) & \tilde{C}_1\left(\frac{\lambda r_p \tau}{n_o}\right)s(\phi_\tau) \\ 0 & 0 & 0 \end{bmatrix} \begin{bmatrix} s_x \\ s_y \\ s_z \end{bmatrix} \Pi\left(\frac{\tau}{v_c}\right). \quad (31)$$

We restrict our analysis to the paraxial regime by dropping second- and higher-order radial terms to find that

$$\mathbf{C}(\boldsymbol{\tau}, \hat{\mathbf{s}}_o) \stackrel{(p)}{\propto} \begin{bmatrix} 1 & 0 & \frac{2\text{NA}}{n_o} \frac{\tau}{v_c} \cos \phi_\tau \\ 0 & 1 & \frac{2\text{NA}}{n_o} \frac{\tau}{v_c} \sin \phi_\tau \\ 0 & 0 & 0 \end{bmatrix} \begin{bmatrix} s_x \\ s_y \\ s_z \end{bmatrix} \Pi\left(\frac{\tau}{v_c}\right). \quad (32)$$

Under the paraxial approximation the transverse components of the dipole $\{s_x, s_y\}$ create purely transverse fields in the pupil plane and the axial component of the dipole $\{s_z\}$ creates purely radial fields in the pupil plane. The paraxial approximation may seem crude compared to Backer and Moerner's numerical results, but the approximation will allow us to calculate the transfer functions in closed form so that we can build an intuition for the limits of the microscope. We also note that many existing works in ensemble polarized fluorescence microscopy make stronger approximations than ours. For example, Fourkas only considers the total irradiance in the pupil plane while ignoring the propagation of fields to the detector [13].

The dipole coherent spread function is the inverse Fourier transform of the dipole coherent transfer function. Applying Eq. (16) in reverse yields

$$\mathbf{c}(\mathbf{r}, \hat{\mathbf{s}}_o) \stackrel{(p)}{\propto} \begin{bmatrix} \text{jinc}_0(v_c r) & 0 & \frac{\text{NA}}{n_o} i \cos \phi \text{jinc}_1(v_c r) \\ 0 & \text{jinc}_0(v_c r) & \frac{\text{NA}}{n_o} i \sin \phi \text{jinc}_1(v_c r) \\ 0 & 0 & 0 \end{bmatrix} \begin{bmatrix} s_x \\ s_y \\ s_z \end{bmatrix}. \quad (33)$$

Notice that the radial component of the dipole coherent spread function has a $\pi/2$ phase shift relative to the transverse component. This phase factor arises because the Fourier transform of a real and odd function is purely imaginary.

3.2.1. Paraxial dipole point spread function

The dipole point spread function is the (normalized) absolute square of the coherent dipole spread function

$$h(\mathbf{r}, \hat{\mathbf{s}}_o) \propto \mathbf{c}(\mathbf{r}, \hat{\mathbf{s}}_o) \mathbf{c}^\dagger(\mathbf{r}, \hat{\mathbf{s}}_o). \quad (34)$$

Plugging in the paraxial dipole coherent spread function and normalizing yields

$$h(\mathbf{r}, \hat{\mathbf{s}}_o) \stackrel{(p)}{=} N \left[\text{jinc}_0^2(v_c r) \sin^2 \vartheta + \left(\frac{\text{NA}}{n_o} \right)^2 \text{jinc}_1^2(v_c r) \cos^2 \vartheta \right], \quad (35)$$

where $\sin^2 \vartheta = s_x^2 + s_y^2$, $\cos^2 \vartheta = s_z^2$, and the normalization factor is

$$N = 6v_c^2 \pi^{-3/2} \left[2 + \left(\frac{\text{NA}}{n_o} \right)^2 \right]^{-1}. \quad (36)$$

As discussed above, the transverse and radial fields are out of phase on the detector, so the total irradiance is the sum of the contributions from the transverse and radial components. In Fig. 2 we plot the dipole point spread function for several dipole orientations and numerical apertures, and in Fig. 3 we compare the monopole point spread function to the dipole point spread function. The paraxial monopole and dipole models are only equivalent when the sample consists of transverse dipoles, which is clear if we notice that Eq. (35) reduces to an Airy disk when $\vartheta = \pi/2$ —see Novotny and Hecht for a similar observation [14, ch. 4].

To demonstrate the paraxial dipole point spread function we simulate a set of equally spaced dipoles with varying orientation:

$$f_{(ph1)}(r_x, r_y, \vartheta, \varphi) = \sum_{j=0}^3 \sum_{k=0}^3 \delta(r_x - j) \delta(r_y - k) \delta(\cos \vartheta - \cos \vartheta_j) \delta(\varphi - \varphi_k), \quad (37)$$

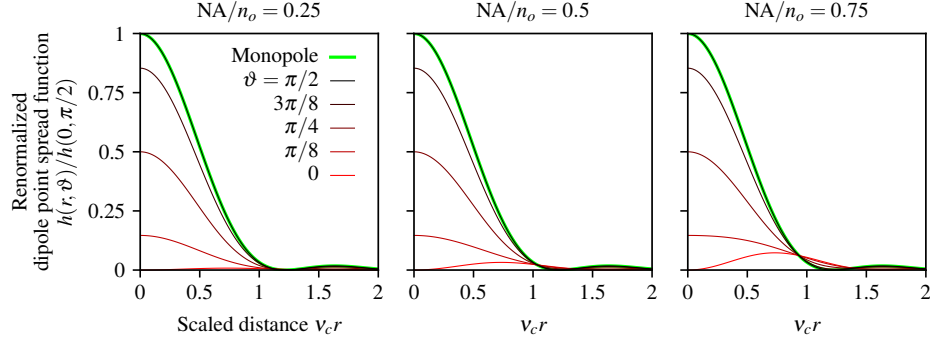


Fig. 2. Renormalized paraxial dipole point spread function as a function of the scaled radial coordinate $v_c r$, the dipole inclination angle ϑ , and NA/n_o . For small numerical apertures (left) the irradiance pattern created by axial dipoles (**red**) is small compared to transverse dipoles (**black**), but the relative contribution of axial dipoles increases with the numerical aperture (see **red** lines from left to right). Additionally, we plot the monopole point spread function (**green**) and observe that the paraxial monopole and dipole models are identical for transverse dipoles (the **green** and **black** lines are coincident).

where $\vartheta_j = j\frac{\pi}{6}$, $\varphi_k = k\frac{\pi}{4}$, the subscript (*ph1*) indicates that this is the first phantom, and the spatial coordinates are expressed in μm . To find the irradiance pattern created by the phantom we plug Eq. (37) into Eq. (2) and use the sifting property to find that

$$g_{(ph1)}(r_x, r_y) = \sum_{j=0}^3 \sum_{k=0}^3 h\left(\sqrt{(r_x - j)^2 + (r_y - k)^2}, \vartheta_j\right). \quad (38)$$

In Fig. 4 we plot the phantom and scaled irradiance for an imaging system with $\text{NA} = 0.75$, $\lambda = 500 \text{ nm}$, and $n_o = 1.33$. We sample and plot the scaled irradiance at $20\times$ the Nyquist rate, $\Delta x = 1/[20(2v_c)]$, so the irradiance patterns are free of aliasing. The output demonstrates that the irradiance pattern depends on the dipole inclination, but not its azimuth.

3.2.2. Paraxial dipole spatial transfer function

The dipole spatial transfer function is the spatial Fourier transform of the dipole point spread function (or the complex autocorrelation of the dipole coherent transfer function). Applying the Fourier transform to Eq. (35) we find that

$$H(\mathbf{v}, \vartheta) \stackrel{(p)}{=} \frac{N}{v_c^2} \left[\text{chat}_0\left(\frac{v}{v_c}\right) \sin^2 \vartheta + \left(\frac{\text{NA}}{n_o}\right)^2 \text{chat}_1\left(\frac{v}{v_c}\right) \cos^2 \vartheta \right]. \quad (39)$$

In Fig. 5 we plot the dipole spatial transfer function for several dipole orientations and numerical apertures. We find that the dipole spatial transfer function is negative for axial dipoles at high spatial frequencies, especially for larger numerical apertures. The negative dipole spatial transfer function corresponds to a contrast inversion for high-frequency patterns of axial dipoles because the irradiance minimum corresponds to the position of the dipole.

To demonstrate the dipole spatial transfer function we simulate a set of equally spaced disks with varying diameter containing fluorophores with varying orientation

$$f_{(ph2)}(r_x, r_y, \vartheta) = \sum_{j=0}^3 \sum_{k=0}^3 \frac{1}{D_k^2} \Pi\left(\frac{1}{D_k} \sqrt{(r_x - j)^2 + (r_y - k)^2}\right) \delta(\cos \vartheta - \cos \vartheta_j) \quad (40)$$

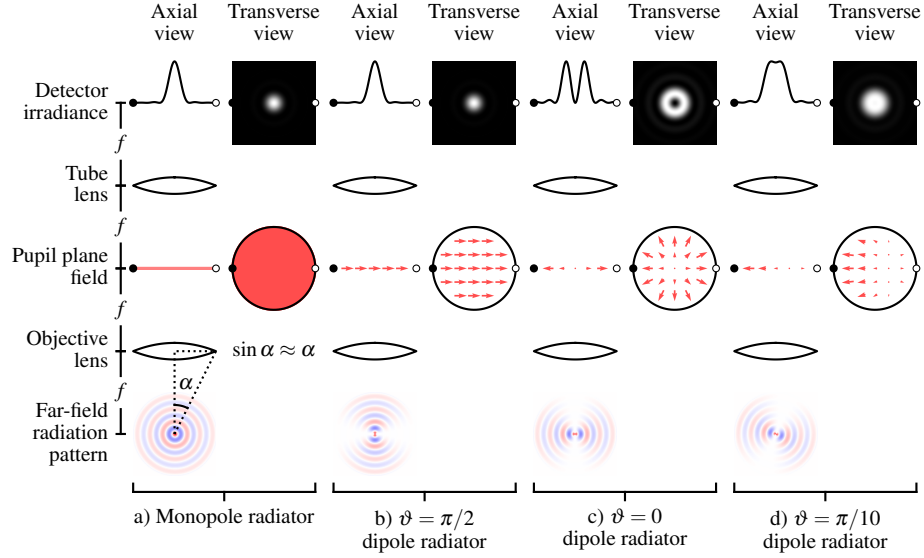


Fig. 3. Comparison of paraxial models for monopole radiators a) and dipole radiators b)–d). a) Monopole radiators fill the pupil plane with a uniform scalar field which gives rise to an Airy disk on the detector. b) A transverse dipole radiator also creates an Airy disk, but the pupil plane is filled with a uniform vector field. c) An axial dipole radiator creates a radial electric field pattern in the back focal plane that creates a $\text{jinc}_1^2(r)$ pattern on the detector. d) Dipoles that are not transverse or axial still create radially symmetric irradiance patterns under the paraxial approximation. Fields from transverse dipoles are real and even while fields from axial dipoles are real and odd, which causes a relative $\pi/2$ phase shift for the fields on the detector. This phase shift means that the fields from transverse and axial components of the dipole do not interfere, which causes radially symmetric irradiance patterns.

where $D_k = 0.15(1 + k) \mu\text{m}$ and $\vartheta_j = j \frac{\pi}{6}$. Notice that we have scaled the disks so that the total number of fluorophores in each disk is constant. Also notice that the disk can model a spatial distribution of many fluorophores or a single molecule undergoing spatial diffusion within a well.

We can calculate the scaled irradiance by taking the spatial Fourier transform of each orientation in the phantom, multiplying the result with the dipole spatial transfer function, summing over the orientations, then taking the inverse spatial Fourier transform

$$g_{(ph2)}(r_x, r_y) = \mathcal{F}_{\mathbb{R}^2}^{-1} \left\{ \sum_j H(\nu, \vartheta_j) \mathcal{F}_{\mathbb{R}^2} \{ f_{(ph2)}(r_x, r_y, \vartheta_j) \} \right\}. \quad (41)$$

In Fig. 6 we plot the phantom and scaled irradiance with the same imaging parameters as the previous section. The small disks create irradiance patterns that are similar to the point sources in the previous section, while larger disks create increasingly uniform irradiance patterns that hide the orientation of the fluorophores.

3.2.3. Paraxial dipole angular transfer function

To calculate the angular dipole transfer function we take the spherical Fourier transform of the dipole point spread function

$$H_l^m(\mathbf{r}) = \int_{\mathbb{S}^2} d\hat{\mathbf{s}}_o h(\mathbf{r}, \hat{\mathbf{s}}_o) Y_l^{m*}(\hat{\mathbf{s}}_o). \quad (42)$$

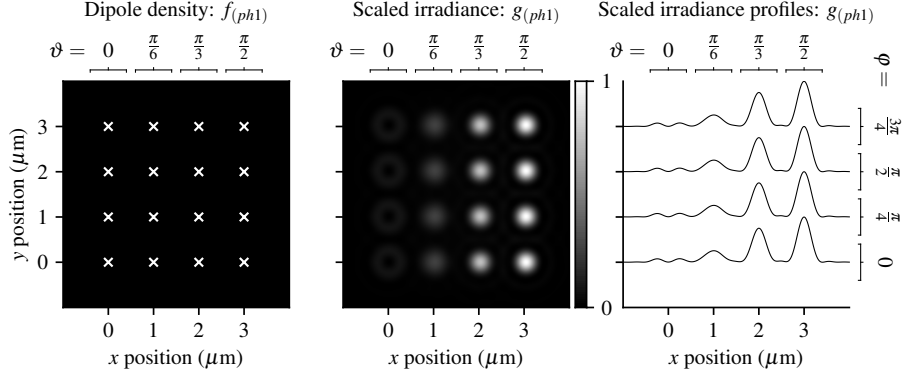


Fig. 4. **Left:** A spatially and angularly sparse phantom—uniformly spaced single dipoles with varying orientations (increasing ϑ from left to right and increasing φ from bottom to top). White crosses mark the positions of the dipoles. **Center:** Scaled irradiance for an imaging system with $\text{NA} = 0.75$, $\lambda = 500$ nm, and $n_o = 1.33$ sampled at $20\times$ the Nyquist rate. **Right:** x profiles through the scaled irradiance. The response is independent of the azimuth angle and strongly dependent on the inclination angle.

After evaluating the integrals and normalizing, the angular dipole transfer function is

$$H_l^m(\mathbf{r}) \stackrel{(p)}{=} \frac{N}{3} \left[2\text{jinc}_0^2(\nu_c r) + \left(\frac{\text{NA}}{n_o} \right)^2 \text{jinc}_1^2(\nu_c r) \right] \Lambda_0 \delta_{\ell 0} \delta_{m 0} + \frac{N}{3} \left[-2\text{jinc}_0^2(\nu_c r) + 2 \left(\frac{\text{NA}}{n_o} \right)^2 \text{jinc}_1^2(\nu_c r) \right] \Lambda_2 \delta_{\ell 2} \delta_{m 0}, \quad (43)$$

where $\Lambda_\ell = \sqrt{4\pi/(2\ell + 1)}$.

In Fig. 7 we plot the dipole angular transfer function for both spherical harmonic terms and several numerical apertures. Note that the dipole angular transfer function can be negative because the spherical harmonics can take negative values. The $\ell = 0$ term shows that angularly uniform distributions of dipoles create spatial irradiance patterns that are similar but not identical to the Airy disk, while the $\ell = 2$ term shows a negative pattern because of the large contribution of the transverse negative values in the Y_2^0 spherical harmonic.

To demonstrate the dipole angular transfer function we simulate a set of equally spaced fluorophore distributions with varying orientation and angular distributions

$$f_{(ph3)}(r_x, r_y, \vartheta) = \sum_{j=0}^3 \sum_{k=0}^3 \delta(r_x - j) \delta(r_y - k) f_{(\text{cone})}(\vartheta, \varphi; \vartheta_j, 0, \Delta_k), \quad (44)$$

where

$$f_{(\text{cone})}(\hat{\mathbf{s}}_o; \hat{\mathbf{s}}'_o, \Delta) = f_{(\text{cone})}(\vartheta, \varphi; \vartheta', \varphi', \Delta) = \frac{1}{4\pi(1 - \cos \Delta)} \Pi\left(\frac{\hat{\mathbf{s}} \cdot \hat{\mathbf{s}}'}{2 \cos \Delta}\right) \quad (45)$$

is an angular double cone distribution with central direction $\hat{\mathbf{s}}'$ and cone half-angle Δ ; $\vartheta_j = j\frac{\pi}{6}$; and $\Delta_k = k\frac{\pi}{6}$. Notice that when $\Delta = 0$ the angular double cone reduces to a single direction, and when $\Delta = \pi/2$ the angular double cone reduces to an angularly uniform distribution. Also notice that the double cone can model angular diffusion or the angular distribution of many fluorophores within a resolvable volume.

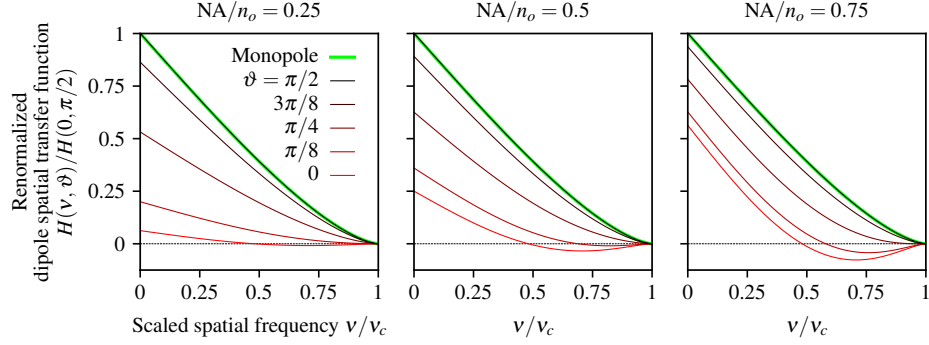


Fig. 5. Dipole spatial transfer function as a function of the scaled spatial frequency v/v_c , the dipole inclination angle ϑ , and NA/n_o . For small numerical apertures (left) the dipole spatial transfer function for axial dipoles (**red**) is small compared to transverse dipoles (**black**), but the relative contribution of axial dipoles increases with the numerical aperture (see **red** lines from left to right). The spatial dipole transfer function of axial dipoles is negative at high spatial frequencies because the central minimum of the axial dipole point spread function corresponds to the position of the dipole. Equivalently, a high-spatial-frequency pattern of axial dipoles will generate an irradiance pattern where the minimum irradiance corresponds to the peak of the axial dipole density. Additionally, we plot the monopole transfer function (**green**) and observe that the paraxial monopole and dipole models are identical for transverse dipoles (the **green** and **black** lines are coincident).

Our first step towards the irradiance pattern is to calculate the dipole angular spectrum of the phantom. In Appendix B we calculate the spherical Fourier transform of the double cone distribution $F_{\ell,(\text{cone})}^m(\vartheta', \varphi'; \Delta)$ which we can use to express the dipole angular spectrum as

$$F_{\ell,(ph3)}^m(r_x, r_y, \vartheta) = \sum_{j=0}^3 \sum_{k=0}^3 \delta(r_x - j) \delta(r_y - k) F_{\ell,(\text{cone})}^m(\vartheta_j, 0, \Delta_k). \quad (46)$$

To calculate the scaled irradiance we multiply the dipole angular spectrum by the dipole angular transfer function and sum over the dipoles and spherical harmonics

$$g_{(ph3)}(r_x, r_y) = \sum_{\ell m} \sum_{j=0}^3 \sum_{k=0}^3 H_{\ell}^m \left(\sqrt{(r_x - j)^2 + (r_y - k)^2} \right) F_{\ell,(\text{cone})}^m(\vartheta_j, 0, \Delta_k). \quad (47)$$

In Fig. 8 we plot the phantom and scaled irradiance with the same imaging parameters as the previous sections. For small cone angles the irradiance patterns are similar to the point sources in the previous sections, while larger cone angles create increasingly uniform irradiance patterns that hide the angular information about the distributions.

3.2.4. Paraxial dipole spatio-angular transfer function

We can calculate the dipole spatio-angular transfer function by taking the spatial Fourier transform of the dipole angular transfer function (or the spherical Fourier transform of the dipole spatial

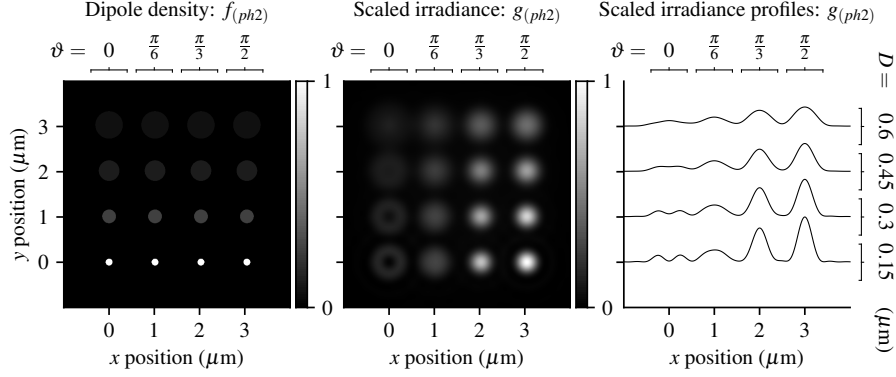


Fig. 6. **Left:** A spatially dense and angularly sparse phantom—uniformly spaced disks with varying size (increasing D from bottom to top) and dipole orientation (increasing ϑ from left to right) **Center:** Scaled irradiance for an imaging system with $\text{NA} = 0.75$, $\lambda = 500$ nm, and $n_o = 1.33$ sampled at $20\times$ the Nyquist rate. **Right:** x profiles through the scaled irradiance. Larger disks generate increasingly uniform irradiance patterns with fewer details that may indicate the orientation of fluorophores.

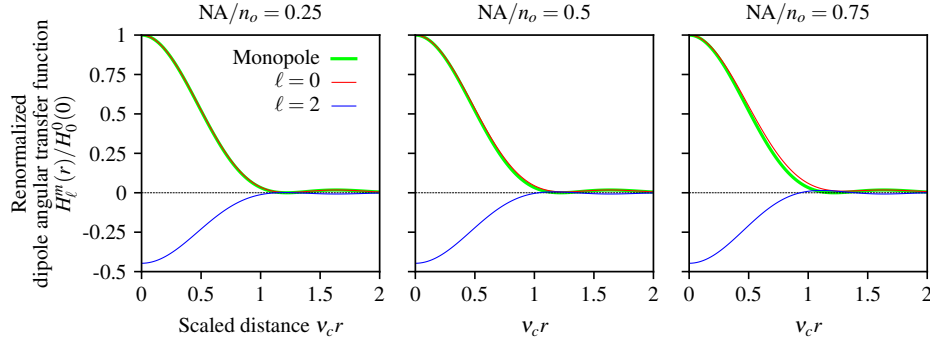


Fig. 7. Paraxial dipole angular transfer function in terms of a scaled radial detection coordinate $v_c r$, the spherical harmonic degree ℓ , and NA/n_o . Angularly uniform distributions of dipoles $\ell = 0$ generate a spatial pattern that is similar but not identical to the Airy disk created by a monopole (green), and this discrepancy increases with the numerical aperture. $\ell = 2$ distributions have a negative response because $Y_2^0(\hat{s})$ is negative for transverse directions. As the numerical aperture increases, the relative contribution of positive axial dipoles in the $\ell = 2$ distribution increases.

transfer function) to find that

$$H_\ell^m(v) \stackrel{(p)}{=} \frac{N}{3v_c^2} \left[2\text{chat}_0\left(\frac{v}{v_c}\right) + \left(\frac{\text{NA}}{n_o}\right)^2 \text{chat}_1\left(\frac{v}{v_c}\right) \right] \Lambda_0 \delta_{\ell 0} \delta_{m 0} + \frac{N}{3v_c^2} \left[-2\text{chat}_0\left(\frac{v}{v_c}\right) + 2\left(\frac{\text{NA}}{n_o}\right)^2 \text{chat}_1\left(\frac{v}{v_c}\right) \right] \Lambda_2 \delta_{\ell 2} \delta_{m 0}. \quad (48)$$

In Fig. 9 we plot the dipole spatio-angular transfer function for both spherical harmonic terms and several numerical apertures. The $\ell = 0$ term shows that an angularly uniform distribution of dipoles has a transfer function that is similar but not identical to the monopole transfer function

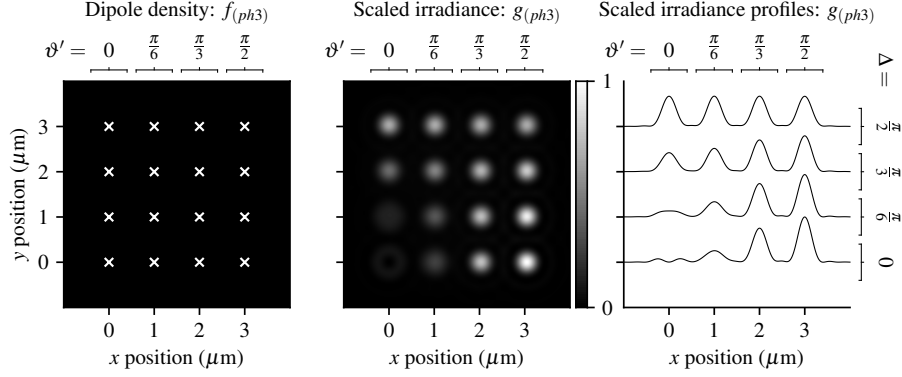


Fig. 8. **Left:** A spatially sparse and angularly dense phantom—uniformly spaced double cone distributions of fluorophores with varying central direction (increasing ϑ' from left to right) and varying cone half-angle (increasing Δ from bottom to top). **Center:** Scaled irradiance for an imaging system with $\text{NA} = 0.75$, $\lambda = 500$ nm, and $n_o = 1.33$ sampled at 20 \times the Nyquist rate. **Right:** x profiles through the scaled irradiance. Small cone angles have irradiance patterns that vary with the central direction, while larger cones angles have increasingly uniform irradiance patterns that hide angular information.

with high frequencies increasingly suppressed as the numerical aperture increases. The $\ell = 2$ term shows a negative pattern because of the large contribution of the transverse negative values in the Y_2^0 spherical harmonic. As the numerical aperture increases the relative contribution of the positive axial values increases and the $\ell = 2$ term becomes less negative.

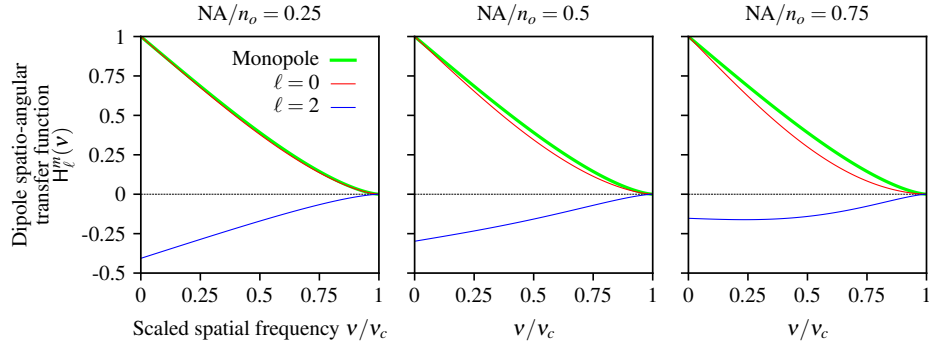


Fig. 9. Spatio-angular dipole transfer function as a function of the scaled spatial frequency v/v_c , the spherical harmonic degree ℓ , and NA/n_o . When the numerical aperture is small the transverse dipoles contribute the most to the signal which gives rise to a positive $\ell = 0$ component and a negative $\ell = 2$ component. As the numerical aperture increases, the relative contribution of axial dipoles increases and the $\ell = 2$ component becomes less negative. Additionally, we plot the monopole transfer function (green) and observe that the $\ell = 0$ term is similar but not identical to the monopole transfer function, and this discrepancy increases with the numerical aperture.

To demonstrate the spatio-angular transfer function, we simulate a set of equally spaced disks

of fluorophores with varying radius and angular distributions

$$f_{(ph4)}(r_x, r_y, \vartheta, \varphi) = \sum_{j=0}^3 \sum_{k=0}^3 \frac{1}{D_k^2} \Pi\left(\frac{1}{D_k} \sqrt{(r_x - j)^2 + (r_y - k)^2}\right) f_{(\text{cone})}\left(\vartheta, \varphi; \frac{\pi}{2}, 0, \Delta_j\right), \quad (49)$$

where $D_k = 0.15(1 + k) \mu\text{m}$, and $\Delta_j = j \frac{\pi}{6}$.

Our first step towards calculating the irradiance pattern is to calculate the dipole spatio-angular spectrum given by the spatial Fourier transform of the dipole angular spectrum

$$F_{\ell, (ph4)}^m(\nu_x, \nu_y) = \mathcal{F}_{\mathbb{R}^2} \left\{ \sum_{j=0}^3 \sum_{k=0}^3 \frac{1}{D_k^2} \Pi\left(\frac{1}{D_k} \sqrt{(r_x - j)^2 + (r_y - k)^2}\right) F_{\ell, \text{cone}}^m\left(\frac{\pi}{2}, 0, \Delta_j\right) \right\}. \quad (50)$$

To calculate the scaled irradiance we multiply the dipole spatio-angular spectrum by the dipole spatio-angular transfer function, sum over the spherical harmonics, then take an inverse Fourier transform

$$g_{(ph4)}(r_x, r_y) = \mathcal{F}_{\mathbb{R}^2}^{-1} \left\{ \sum_{\ell m} H_{\ell}^m(\nu_x, \nu_y) F_{\ell, (ph4)}^m(\nu_x, \nu_y) \right\}. \quad (51)$$

In Fig. 10 we plot the phantom and scaled irradiance with the same imaging parameters as the previous sections. Small cone angles and small disks create relatively unique irradiance patterns, while increasing the cone angle or disk size creates increasingly similar irradiance patterns.

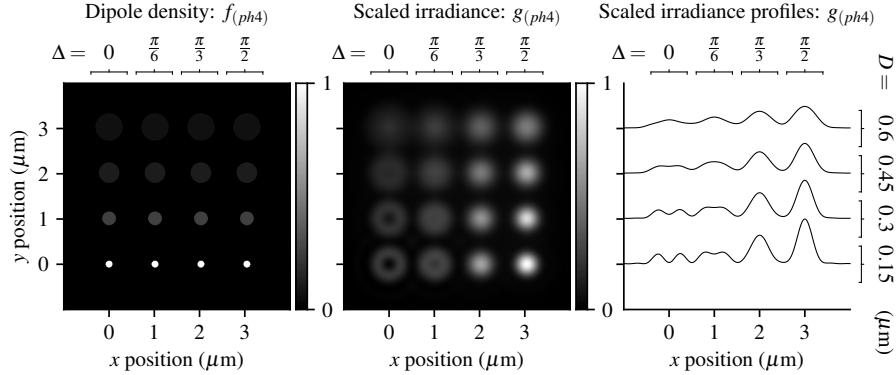


Fig. 10. **Left:** A spatially and angularly dense phantom—uniformly spaced disks with varying size (increasing D from bottom to top) and double cone half angle (increasing Δ from left to right) **Center:** Scaled irradiance for an imaging system with $\text{NA} = 0.75$, $\lambda = 500 \text{ nm}$, and $n_o = 1.33$ sampled at $20\times$ the Nyquist rate. **Right:** x profiles through the scaled irradiance.

4. Discussion

4.1. Comparing monopole and dipole models

The only case when the dipole and monopole transfer functions match exactly is when the sample consists of dipoles that are completely constrained to the transverse plane of a paraxial imaging system. Applying the monopole approximation in any other situation can lead to biased estimates of the fluorophore concentrations. To see how these biases manifest, consider the irradiance pattern created by an ensemble of dipoles oriented along the optic axis—see Figs. 4, 6, 8,

or 10. Any reconstruction scheme that uses the monopole approximation would attribute the irradiance doughnut to a doughnut of monopoles instead of axially oriented dipoles, which is a clear example of a biased estimate caused by model mismatch.

However, the common justifications for the monopole approximation—that the fluorophores are rotationally unconstrained or that there are many randomly oriented fluorophores in a resolvable volume—are good justifications in all but the highest SNR regimes. The effects of the dipole model become apparent in lower SNR regimes as the rotational constraints on the dipoles increase (assuming there are out-of-plane dipole components).

4.2. What determines the angular bandwidth?

Spatial imaging systems have a spatial bandwidth that characterizes the highest spatial frequency that the system can transfer between object and data space. Similarly, angular imaging systems have an angular bandwidth that characterizes the highest angular frequency that the system can transfer, but in the angular case there are two different types of angular bandwidths that we call the ℓ - and m -bandwidth. The ℓ -bandwidth can be interpreted in a similar way to the spatial bandwidth—it characterizes the smallest angular features that the imaging system can measure. The m -bandwidth does not have a direct analog in the spatial domain—it characterizes the angular uniformity of the imaging system. If the ℓ - and m -bandwidths are equal then the imaging system can be said to have an *isotropic angular bandwidth*.

The spatial bandwidth of a fluorescence microscope is well known to be $\nu_c = \frac{2\text{NA}}{\lambda}$. In other words, we can increase the spatial resolution of a fluorescence microscope by increasing the NA of the instrument or by choosing a fluorophore with a shorter emission wavelength. Similarly, the angular bandwidth of a fluorescence microscope depends on both the instrument and the choice of fluorophore.

The microscope we considered in this work has an ℓ -bandwidth of $\ell_c = 2$ and an m -bandwidth of $m_c = 0$, so it does not have an isotropic angular bandwidth. In future work we will consider several approaches to improving the angular bandwidths in detail, but we briefly mention that non-paraxial microscopes, microscopes with polarizers in the illumination or detection paths, and multiview microscopes all have higher angular bandwidths than the microscope considered here.

The angular bandwidth is also fluorophore dependent. Monopoles emit light isotropically so they have an ℓ -bandwidth of $\ell_c = 0$, while dipoles have an ℓ -bandwidth of $\ell_c = 2$, and higher-order excitation and detection moments will have even higher bandwidths. Multi-photon excitation and other non-linear methods can also increase the ℓ -bandwidth [15].

4.3. Towards more realistic models

The theoretical model we presented in this work is an extreme simplification of a real microscope. We have ignored the effects of thick samples, refractive-index mismatch, aberration, scattering, finite fluorescence lifetimes, and interactions between fluorophores among others. Because of this long list of unconsidered effects, real experiments will likely require extensions of the models developed here.

The dipole pupil function provides the simplest way to create more realistic models from the simple model in this paper. Phase aberrations can be added to the dipole pupil function with Zernike polynomials, and refractive index boundaries can be modeled by applying the work of Gibson and Lanni to the dipole pupil function [16]. These additions will model phase aberrations, but modeling polarization aberrations will also be necessary, and we anticipate that vector Zernike polynomials and the Jones pupil [17–19] will be essential tools for modeling dipole imaging systems. We plan to use the dipole pupil function to include the effects of non-paraxial objectives, polarizers, and defocus in future papers of this series.

The dipole pupil function also provides an enormous set of design opportunities. The dipole imaging problem may benefit from spatially varying diattenuating and birefringent masks—a

much larger set of possibilities than the well-explored design space of amplitude and phase masks. The dipole pupil function is a step towards Green's tensor engineering [20], and the dipole transfer functions provide a strong framework for evaluating dipole imaging designs.

In the simple case considered here we focused on the emission path of the microscope, but the excitation path is equally important. Complete models will need to consider the spatio-angular dependence of excitation. Zhenghao et. al. [21] have taken steps in this direction by considering polarized structured illumination microscopy. Rotational dynamics and the fluorescence lifetime are also important to consider when incorporating models of the excitation process [22–24].

5. Conclusions

We have calculated the monopole and dipole transfer functions for paraxial $4f$ imaging systems and demonstrated these transfer functions with efficient simulations. We found that the monopole and scalar approximations are good approximations when the sample consists of unconstrained rotating fluorophores or many randomly oriented fluorophores within a resolvable volume. We also found that dipole and vector optics effects become larger as rotational order increases, and in these cases the dipole transfer functions become valuable tools.

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Disclosures

The authors declare that there are no conflicts of interest related to this article.

References

1. T. Chandler, H. Shroff, R. Oldenbourg, and P. J. La Rivière, "Spatio-angular fluorescence microscopy I. basic theory," <https://arxiv.org/abs/1812.07093> (2018).
2. M. Gu, *Advanced Optical Imaging Theory*, Springer Series in Optical Sciences (Springer, 2000).
3. H. Barrett and K. Myers, *Foundations of Image Science* (Wiley-Interscience, 2004).
4. J. Goodman, *Introduction to Fourier Optics* (McGraw-Hill, 1996).
5. D. Axelrod, "Fluorescence excitation and imaging of single molecules near dielectric-coated and bare surfaces: a theoretical study," *J. Microsc.* **247** 2, 147–60 (2012).
6. A. S. Backer and W. E. Moerner, "Extending single-molecule microscopy using optical Fourier processing," *J. Phys. Chem. B* **118**, 8313–8329 (2014).
7. C. J. R. Sheppard, M. Gu, Y. Kawata, and S. Kawata, "Three-dimensional transfer functions for high-aperture systems," *J. Opt. Soc. Am. A* **11**, 593–598 (1994).
8. M. R. Arnison and C. J. Sheppard, "A 3D vectorial optical transfer function suitable for arbitrary pupil functions," *Opt. Commun.* **211**, 53–63 (2002).
9. M. R. Foreman and P. Török, "Computational methods in vectorial imaging," *J. Mod. Opt.* **58**, 339–364 (2011).
10. R. Bracewell, *Fourier Analysis and Imaging* (Springer US, 2004).
11. P. N. Petrov, Y. Shechtman, and W. E. Moerner, "Measurement-based estimation of global pupil functions in 3D localization microscopy," *Opt. Express* **25**, 7945–7959 (2017).
12. M. P. Backlund, Y. Shechtman, and R. L. Walsworth, "Fundamental precision bounds for three-dimensional optical localization microscopy with Poisson statistics," *Phys. Rev. Lett.* **121**, 023904 (2018).
13. J. T. Fourkas, "Rapid determination of the three-dimensional orientation of single molecules," *Opt. Lett.* **26**, 211–213 (2001).
14. L. Novotny and B. Hecht, *Principles of Nano-Optics* (Cambridge University Press, 2006).
15. S. Brasselet, "Polarization-resolved nonlinear microscopy: application to structural molecular and biological imaging," *Adv. Opt. Photon.* **3**, 205 (2011).

16. S. F. Gibson and F. Lanni, “Diffraction by a circular aperture as a model for three-dimensional optical microscopy,” *J. Opt. Soc. Am. A* **6**, 1357–1367 (1989).
17. C. Zhao and J. H. Burge, “Orthonormal vector polynomials in a unit circle, part I: basis set derived from gradients of Zernike polynomials,” *Opt. Express* **15**, 18014–18024 (2007).
18. X. Xu, W. Huang, and M. Xu, “Orthogonal polynomials describing polarization aberration for rotationally symmetric optical systems,” *Opt. Express* **23**, 27911–27919 (2015).
19. R. A. Chipman, “Polarization analysis of optical systems,” *Opt. Eng.* **28**, 28 – 28 – 10 (1989).
20. A. Agrawal, S. Quirin, G. Grover, and R. Piestun, “Limits of 3D dipole localization and orientation estimation for single-molecule imaging: towards Green’s tensor engineering,” *Opt. Express* **20**, 26667–26680 (2012).
21. K. Zhanghao, X. Chen, W. Liu, M. Li, C. Shan, X. Wang, K. Zhao, A. Lai, H. Xie, Q. Dai, and P. Xi, “Structured illumination in spatial-orientational hyperspace,” <https://arxiv.org/abs/1712.05092>.
22. M. D. Lew, M. P. Backlund, and W. E. Moerner, “Rotational mobility of single molecules affects localization accuracy in super-resolution fluorescence microscopy,” *Nano Lett.* **13**, 3967–3972 (2013).
23. O. Zhang, J. Lu, T. Ding, and M. D. Lew, “Imaging the three-dimensional orientation and rotational mobility of fluorescent emitters using the tri-spot point spread function,” *Appl. Phys. Lett.* **113**, 031103 (2018).
24. O. Zhang and M. D. Lew, “Fundamental limits on measuring the rotational constraint of single molecules using fluorescence microscopy,” <https://arxiv.org/abs/1811.09017>.
25. I. S. Gradshteyn and I. M. Ryzhik, *Table of Integrals, Series, and Products* (Elsevier/Academic Press, Amsterdam, 2007).
26. J. Mertz, *Introduction to Optical Microscopy* (W. H. Freeman, 2009).
27. R. Ramamoorthi, “Modeling illumination variation with spherical harmonics,” in *Face Processing: Advanced Modeling and Methods*, (Academic Press, 2005).

A. Relationships between special functions

Our first task is to show that

$$i^n \begin{Bmatrix} \exp(in\phi_r) \\ \cos(n\phi_r) \\ \sin(n\phi_r) \end{Bmatrix} \text{jinc}_n(r) \xrightarrow{\mathcal{F}_{\mathbb{R}^2}} (2\nu)^n \begin{Bmatrix} \exp(in\phi_\nu) \\ \cos(n\phi_\nu) \\ \sin(n\phi_\nu) \end{Bmatrix} \Pi(\nu). \quad (52)$$

Writing the inverse Fourier transform in polar coordinates yields

$$= 2^n \int_0^{1/2} d\nu \nu^{n+1} \int_0^{2\pi} d\phi_\nu \begin{Bmatrix} \exp(in\phi_\nu) \\ \cos(n\phi_\nu) \\ \sin(n\phi_\nu) \end{Bmatrix} \exp[2\pi i \nu r \cos(\phi_\nu - \phi_r)]. \quad (53)$$

The azimuthal integral can be evaluated in terms of an n^{th} order Bessel function (for the complex case see [3, ch. 4.111]).

$$= 2^n 2\pi i^n \begin{Bmatrix} \exp(in\phi_r) \\ \cos(n\phi_r) \\ \sin(n\phi_r) \end{Bmatrix} \int_0^{1/2} d\nu \nu^{n+1} J_n(2\pi \nu r). \quad (54)$$

We can use the following identity [25, ch. 6.561-5]

$$\int_0^1 du u^{n+1} J_n(au) = a^{-1} J_{n+1}(a) \quad (55)$$

with a change of variable $u = 2\nu$ to find the final result

$$= 2^n 2\pi i^n \begin{Bmatrix} \exp(in\phi_r) \\ \cos(n\phi_r) \\ \sin(n\phi_r) \end{Bmatrix} \int_0^1 \frac{du}{2} \left(\frac{u}{2}\right)^{n+1} J_n(\pi u r) = i^n \begin{Bmatrix} \exp(in\phi_r) \\ \cos(n\phi_r) \\ \sin(n\phi_r) \end{Bmatrix} \frac{J_{n+1}(\pi r)}{2r} = i^n \begin{Bmatrix} \exp(in\phi_r) \\ \cos(n\phi_r) \\ \sin(n\phi_r) \end{Bmatrix} \text{jinc}_n(r). \quad (56)$$

We can use the relationship in Eq. (52) to express the chat functions in terms of a complex autocorrelation—see the diagram in Fig. 11. Starting with the definition of the n^{th} -order chat function

$$\text{chat}_n(\nu) = \int_{\mathbb{R}^2} d\mathbf{r} \text{jinc}_n^2(|\mathbf{r}|) \exp[-2\pi i \mathbf{r} \nu], \quad (57)$$

$$\begin{array}{ccc}
i^n \exp[in\phi_r] \text{jinc}_n(r) & \xrightarrow{|\cdot|^2} & \text{jinc}_n^2(r) \\
\downarrow \mathcal{F}_{\mathbb{R}^2} & & \downarrow \mathcal{F}_{\mathbb{R}^2} \\
(2\tau)^n \exp[in\phi_\tau] \Pi(\tau) & \xrightarrow{\star_2} & \text{chat}_n(\nu)
\end{array}$$

Fig. 11. The relationships between special functions. The chat functions are defined as the two-dimensional Fourier transform of the squared jinc functions, and they can be calculated with the two-dimensional complex autocorrelations (denoted by \star_2) of the complex-weighted rectangle functions.

we can rewrite the integrand in terms of the absolute square of a simpler function with a known Fourier transform

$$\text{chat}_n(\nu) = \int_{\mathbb{R}^2} d\mathbf{r} |t_n(\mathbf{r})|^2 \exp[-2\pi i \mathbf{r} \nu]. \quad (58)$$

$$t_n(\mathbf{r}) = i^n \exp[in\phi_r] \text{jinc}_n(r). \quad (59)$$

Now we can apply the autocorrelation theorem to rewrite the Fourier transform as

$$\text{chat}_n(\nu) = \int_{\mathbb{R}^2} d\tau T_n(\tau) T_n^*(\tau - \nu), \quad (60)$$

where the function to be autocorrelated can be found with the help of Eq. (52)

$$T_n(\tau) = \int_{\mathbb{R}^2} d\mathbf{r} t_n(\mathbf{r}) \exp[-2\pi i \mathbf{r} \cdot \tau] = (2\tau)^n \exp[in\phi_\tau] \Pi(\tau). \quad (61)$$

It will be more convenient to set up the autocorrelation in Cartesian coordinates

$$T_n(\tau) = 2^n (\tau_x + i\tau_y)^n \Pi\left(\sqrt{\tau_x^2 + \tau_y^2}\right). \quad (62)$$

Plugging Eq. (62) into Eq. (60) gives

$$\text{chat}_n(\nu) = 4^n \int_{\mathbb{R}^2} d\tau (\tau_x^2 + \tau_y^2 - \nu \tau_x)^n \Pi\left(\sqrt{\tau_x^2 + \tau_y^2}\right) \Pi\left(\sqrt{(\tau_x - \nu)^2 + \tau_y^2}\right). \quad (63)$$

We can interpret the autocorrelation as an integral over a region of overlap between a circle centered at the origin and a circle shifted to the right by ν (a geometric lens). Using the construction in Fig. 12 we can express this region as

$$\begin{aligned}
\text{chat}_n(\nu) = 4^{n+1} \left[\int_0^{1/2} \tau d\tau \int_0^{\cos^{-1} \nu} d\phi_\tau (\tau^2 - \nu \tau \cos \phi_\tau)^n - \right. \\
\left. \int_0^{\nu/2} d\tau_x \int_0^{\frac{\tau_x}{\nu} \sqrt{1-\nu^2}} d\tau_y (\tau_x^2 + \tau_y^2 - \nu \tau_x)^n \right] \Pi\left(\frac{\nu}{2}\right). \quad (64)
\end{aligned}$$

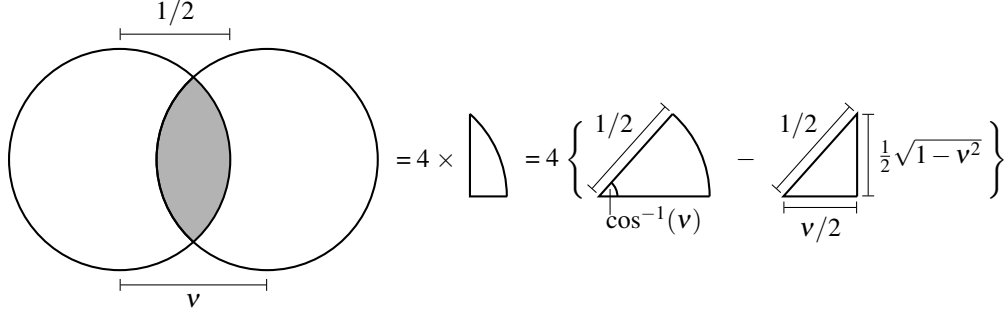


Fig. 12. Geometric construction for evaluating the autocorrelation. We need to integrate over the overlapping region of two circles with radius $1/2$ and distance v between their centers. The region is four times the difference in area between a sector of angle $\cos^{-1}(v)$ and radius $1/2$ and a right triangle with base $v/2$ and hypotenuse $1/2$.

For $n = 0$:

$$\text{chat}_0(v) = 4 \left[\int_0^{1/2} \tau d\tau \int_0^{\cos^{-1} v} d\phi_\tau - \int_0^{v/2} d\tau_x \int_0^{\frac{\tau_x}{v} \sqrt{1-v^2}} d\tau_y \right] \Pi\left(\frac{v}{2}\right), \quad (65)$$

$$\text{chat}_0(v) = \frac{1}{2} \left[\cos^{-1} |v| - |v| \sqrt{1-v^2} \right] \Pi\left(\frac{v}{2}\right), \quad (66)$$

which is a well-known result [4, 10, 26]. For $n = 1$:

$$\begin{aligned} \text{chat}_1(v) = 16 \left[\int_0^{1/2} \tau d\tau \int_0^{\cos^{-1} v} d\phi_\tau (\tau^2 - v\tau \cos \phi_\tau) - \right. \\ \left. \int_0^{v/2} d\tau_x \int_0^{\frac{\tau_x}{v} \sqrt{1-v^2}} d\tau_y (\tau_x^2 + \tau_y^2 - v\tau_x) \right] \Pi\left(\frac{v}{2}\right), \end{aligned} \quad (67)$$

$$\text{chat}_1(v) = \frac{1}{2} \left[\cos^{-1} |v| - |v| (3 - 2v^2) \sqrt{1-v^2} \right] \Pi\left(\frac{v}{2}\right). \quad (68)$$

B. Spherical Fourier transform of a double cone

In this appendix we evaluate the spherical Fourier transform of a normalized double-cone angular distribution with central direction $\hat{\mathbf{s}}'$ and cone half-angle Δ

$$f_{(\text{cone})}(\hat{\mathbf{s}}; \hat{\mathbf{s}}', \Delta) = \frac{1}{4\pi(1 - \cos \Delta)} \Pi\left(\frac{\hat{\mathbf{s}} \cdot \hat{\mathbf{s}}'}{2 \cos \Delta}\right). \quad (69)$$

The spherical Fourier transform is

$$F_{\ell(\text{cone})}^m(\hat{\mathbf{s}}', \Delta) = \int_{\mathbb{S}^2} d\hat{\mathbf{s}} f_{(\text{cone})}(\hat{\mathbf{s}}; \hat{\mathbf{s}}', \Delta) Y_\ell^{m*}(\hat{\mathbf{s}}). \quad (70)$$

The limits of integration will be difficult to find unless we change coordinates to exploit the axis of symmetry $\hat{\mathbf{s}}'$. Since the spherical function is rotationally symmetric about $\hat{\mathbf{s}}'$ we can rotate the function so that the axis of symmetry is aligned with $\hat{\mathbf{z}}$ and multiply by $\sqrt{\frac{4\pi}{2l+1}} Y_\ell^{m*}(\hat{\mathbf{s}}')$ to account for the rotation [27]

$$F_{\ell(\text{cone})}^m(\hat{\mathbf{s}}', \Delta) = \sqrt{\frac{4\pi}{2l+1}} Y_\ell^{m*}(\hat{\mathbf{s}}') \int_{\mathbb{S}^2} d\hat{\mathbf{s}} f_{(\text{cone})}(\vartheta; \hat{\mathbf{z}}, \Delta) Y_\ell^0(\hat{\mathbf{s}}). \quad (71)$$

In this coordinate system the double cone is independent of the azimuthal angle, so we can evaluate the azimuthal integral and express the function in terms of an integral over ϑ :

$$F_{\ell(\text{cone})}^m(\hat{\mathbf{s}}', \Delta) = 2\pi Y_{\ell}^{m*}(\hat{\mathbf{s}}') \int_0^{\pi} d\vartheta \sin \vartheta f_{(\text{cone})}(\vartheta; \hat{\mathbf{z}}, \Delta) P_{\ell}(\cos \vartheta). \quad (72)$$

The function $f_{(\text{cone})}(\vartheta; \hat{\mathbf{z}}, \Delta)$ is only non-zero on the intervals $\vartheta \in [0, \Delta]$ and $\vartheta \in [\pi - \Delta, \pi]$ so

$$F_{\ell(\text{cone})}^m(\hat{\mathbf{s}}', \Delta) = \frac{Y_{\ell}^{m*}(\hat{\mathbf{s}}')}{2(1 - \cos \Delta)} \left[\int_0^{\Delta} d\vartheta \sin \vartheta P_{\ell}(\cos \vartheta) + \int_{\pi-\Delta}^{\pi} d\vartheta \sin \vartheta P_{\ell}(\cos \vartheta) \right]. \quad (73)$$

Applying a change of coordinates with $u = \cos \vartheta$ yields

$$F_{\ell(\text{cone})}^m(\hat{\mathbf{s}}', \Delta) = \frac{Y_{\ell}^{m*}(\hat{\mathbf{s}}')}{2(1 - \cos \Delta)} \left[\int_{\cos \Delta}^1 d\vartheta P_{\ell}(u) + \int_{-1}^{-\cos \Delta} d\vartheta P_{\ell}(u) \right]. \quad (74)$$

The Legendre polynomials $P_{\ell}(u)$ are even (odd) on the interval $[-1, 1]$ when ℓ is even (odd), so the pair of integrals will be identical when ℓ is even and cancel when ℓ is odd. For even ℓ ,

$$F_{\ell(\text{cone})}^m(\hat{\mathbf{s}}', \Delta) = \frac{Y_{\ell}^{m*}(\hat{\mathbf{s}}')}{1 - \cos \Delta} \int_{\cos \Delta}^1 d\vartheta P_{\ell}(u). \quad (75)$$

The integral evaluates to [25, ch. 7.111]

$$\int_{\cos \Delta}^1 d\vartheta P_{\ell}(u) = \begin{cases} 1 - \cos \Delta, & \ell = 0, \\ \sin \Delta P_l^{-1}(\cos \Delta), & \text{else,} \end{cases} \quad (76)$$

where $P_l^{-1}(\cos \Delta)$ is the associated Legendre polynomial with order $m = -1$, not an inverse Legendre polynomial. Bringing everything together

$$F_{\ell(\text{cone})}^m(\hat{\mathbf{s}}', \Delta) = \begin{cases} \sqrt{1/(4\pi)}, & \ell = 0, \\ 0, & \ell \text{ odd,} \\ Y_{\ell}^{m*}(\hat{\mathbf{s}}') \cot\left(\frac{\Delta}{2}\right) P_l^{-1}(\cos \Delta), & \ell > 0 \text{ even.} \end{cases} \quad (77)$$