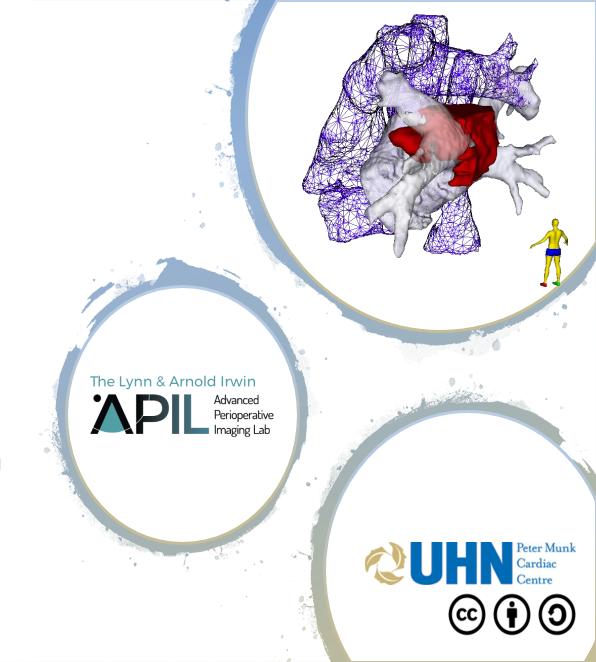
3D Modeling of Cardiac Tumors

Toronto Cardiac Tumor Symposium

2020.01.23

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Competing Interests

- No financial conflicts of interest.
- Research & educational work supported by the

Peter Munk Cardiac Center Foundation.

Objectives

At the completion of this session participants will be able to

- Define basic concepts related to patient-specific 3D models of cardiac tumors
- 2. Describe commonly used presentation formats for 3D models
- 3. Describe the **process for creation** of 3D models from medical imaging data
- 4. Describe the **appropriate uses** of such models
- 5. Describe the **limitations** of current modeling techniques

Outline

What are patient-specific 3D models?

How can you see them?

How are they made?

What can they do?

What can't they do?

What does the (near) future hold?

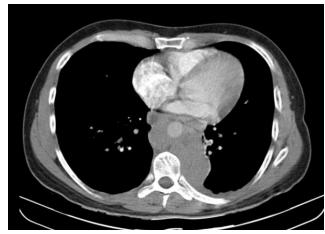
What are patient-specific 3D models?

Digital 3D models created from 3-dimenstional medical imaging data (**CT, MRI, 3D Ultrasound**)

Models can be **dynamic** or **static** depending on the source data

Multiple file formats (STL, OBJ etc.)

Digitally represented as a **mesh** (vertices and edges)





Digital 3D Model

solid ascii

facet normal 0.0927133 -0.0679498

0.993372

outer loop

vertex -54.8458 67.1663 -2.490

vertex -55.0673 67.1473 -2.4708

vertex -55.0497 66.8845 -24904

endloop

endfacet

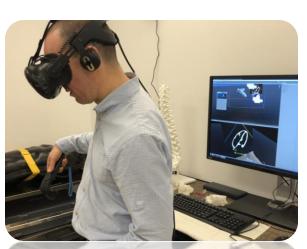
facet normal -0.665674 -0.09466

0.739557

How can you see them?

3D rendering (on 2D screen)
Stereoscopic & holographic displays
3D print
Virtual/augmented Reality





Digital 3D Model

solid ascii facet normal 0.0927133 -0.0679498 0.993372 outer loop vertex -54.8458 67.1663 -2.49017 vertex -55.0673 67.1473 -2.4708 vertex -55.0497 66.8845 -2.49042 endloop endfacet facet normal -0.665674 -0.0996668 0.739557

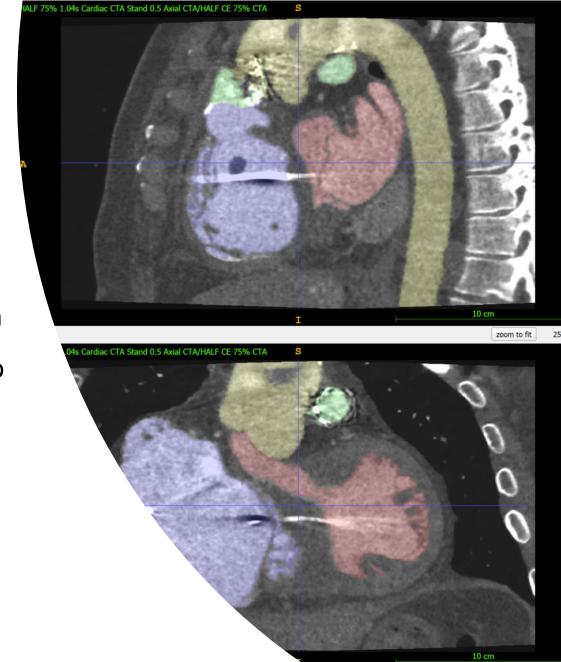


How are they made?

- 1. Imaging
- 2. Resampling to isotropic resolution
- **3. Segmentation** of medical image to create voxel model

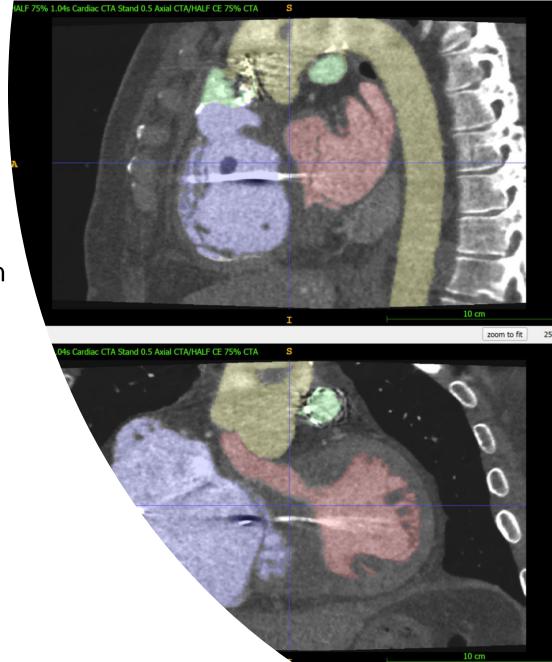
manual automatic

4. Modeling/Mesh generation from voxel model



Source Imaging: CT

- Most common, ~ 0.5 mm resolution
- Ideally cardiac-gated to reduce motion artifact, with contrast
- Soft-tissue boundaries can be challenging to model accurately
- Dual-energy CT (DECT) can improve soft tissue distinctions but not widely available yet



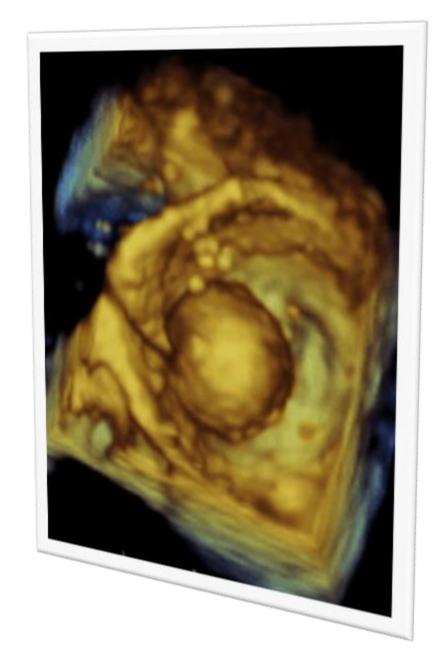
Source Imaging: MR

- Best soft tissue contrast
- Anisotropic resolution (with 5-8 mm slices) limited by time & storage space, patient tolerance
- Most common in **pediatric** cases



Source Imaging: 3D TEE

- Best temporal resolution: Ideal for valves and highly mobile masses.
- Limited spatial scope
- Frustum anisotropic voxel geometry requires resampling; resolution decreases with dept
- Non-standard DICOM format requires vendor-specific software



Voxel Geometry & Resolution: CT vs MRI vs Echo

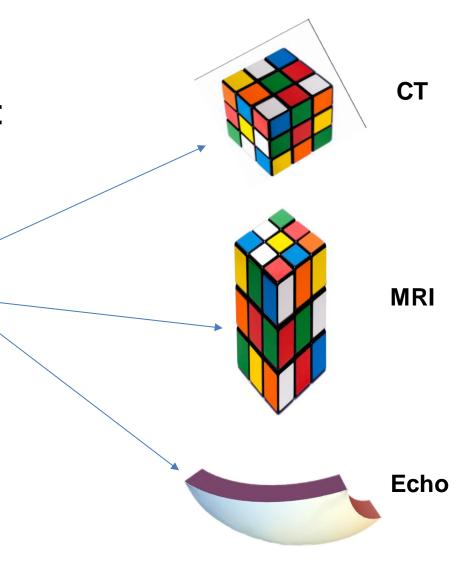
Isotropic: Same resolution in all 3 axis

Anisotropic: Varies with orientation

CT: Cubic or near-cubic voxels >> No or minimal resampling required (low distortion risk). Typical 0.5x0.5x0.5 mm

MRI: Rectangular prism 0.5 x 0.5 x 5-8 mm

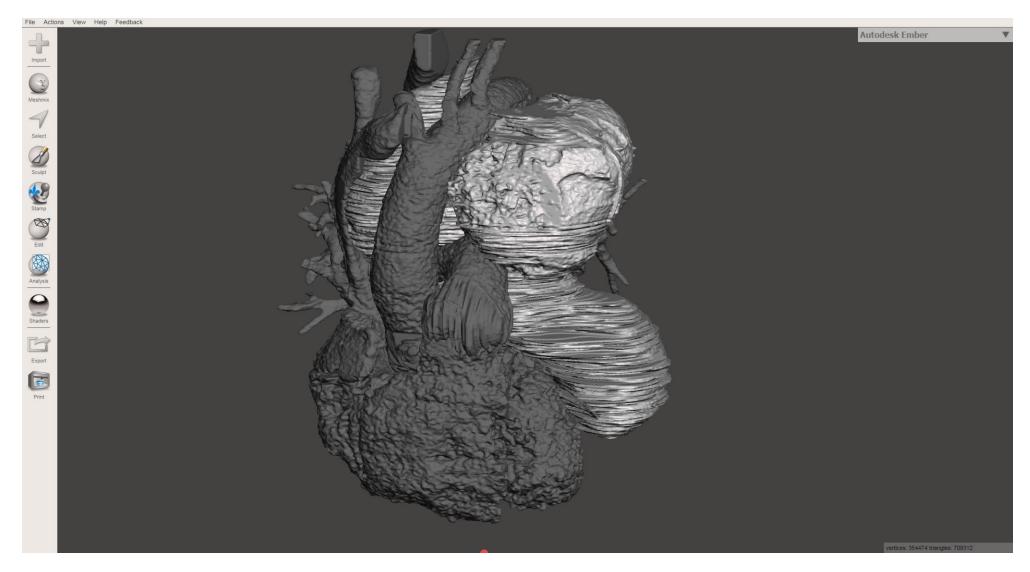
Echo: Spherical segment voxels which grow with distance from probe

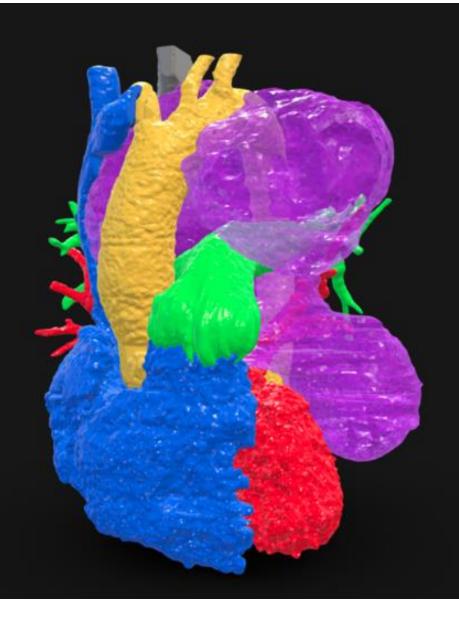


Segmentation



Modeling / Mesh generation / Editing





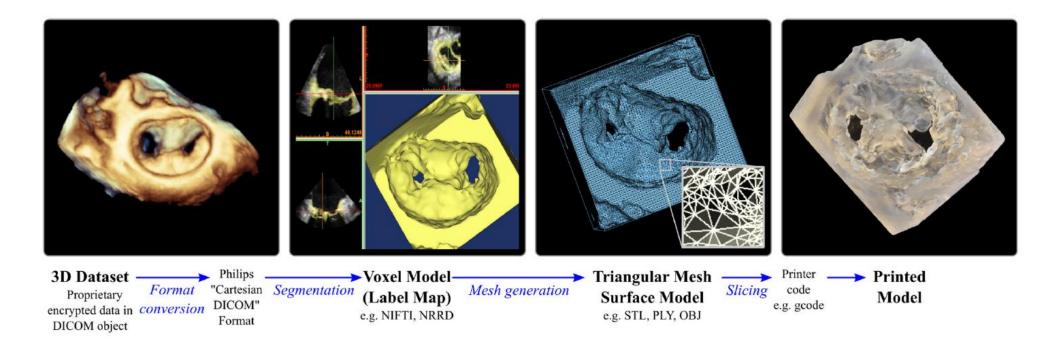


Figure 1

Summarized workflow for 3D printing of a 3D TEE data set of a mitral valve after a MitraClip procedure. Examples of file formats used are included where applicable. From left to right: After export from the ultrasound system, the data set is converted to the Philips Cartesian DICOM format (first panel). Using segmentation software the voxels in the region of interest are labeled, creating a 'solid' voxel model (second panel). A triangular surface mesh model is generated based on the voxel model (third panel). The mesh model is processed by the slicing software, generating a printer code, which directs the printing of the final model (fourth panel). (File formats: NIFTI, Neuroimaging Informatics Technology Initiative; NRRD, Nearly Raw Raster Data; STL, Stereolithography; PLY, Polygon; OBJ, Wavefront Object.)

Applications: Visualization

3D rendering (on screen)

3D print

Virtual/augmented Reality

Stereoscopic & holographic displays

Digital 3D Model

solid ascii facet normal 0.0927133 -0.0679498 0.993372

outer loop

vertex -54.8458 67.1663 -2.49017 vertex -55.0673 67.1473 -2.4708 vertex -55.0497 66.8845 -2.49042 endloop...



Rendering

https://apilnextcloud.ams3.digitaloceanspaces.com/2018003-02/2018003VIEWER.html









3D Printing

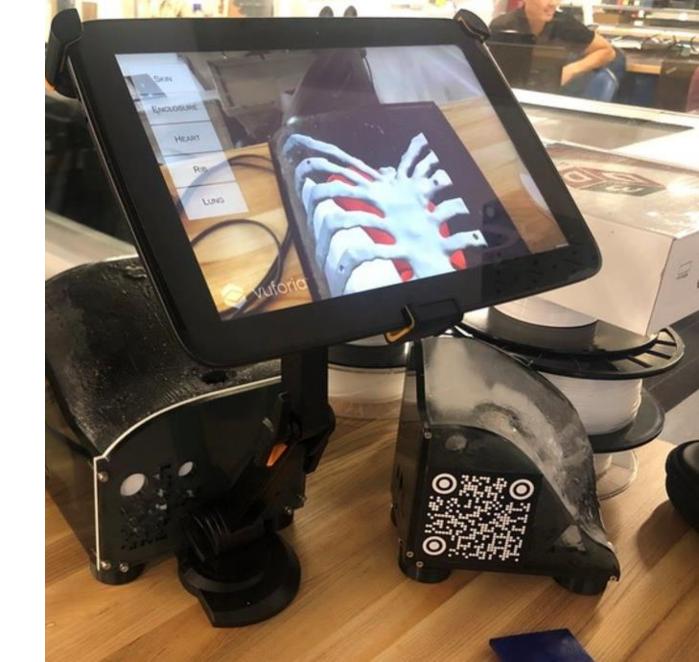
Most accessible in terms of use and interaction Least accessible in terms of resources / cost Wide range of materials, including biocompatible and tissue Growing rapidly, cost decreasing

Limited interaction: scaling, material properties

Virtual Reality



Augmented / Mixed Reality



Procedural Simulation (physical)

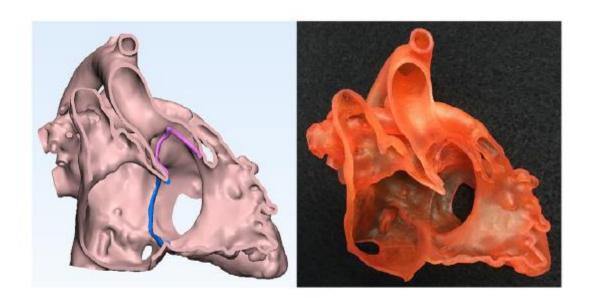
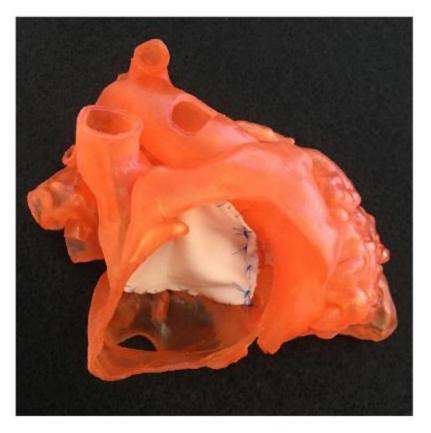


FIGURE 3 | Graphic representation and photograph of the endocardial surface anatomy model made of soft material (TangoPlus, Stratasys Ltd., MN, USA) of the right ventricle of the case shown in **Figure 1**.

3D Printing in Surgical Management of Double Outlet Right Ventricle



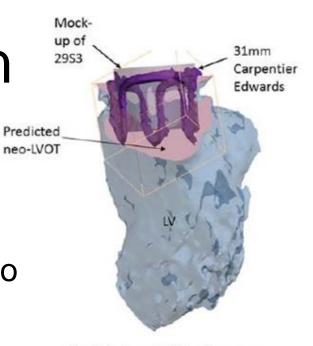
Virtual/Mixed Simulation

Simulation of procedure in virtual environment (VR, AR)

- Limited haptic feedback
- Mechanical properties of tissue difficult to capture

Computational Simulation +/- visualization

- Prosthesis sizing (TAVI)
- Prediction of complications
- Complex measurements
- Optimal geometric solutions (theoretical)



Predicted neo-LVOT surface area 630.7 mm²

Catheter Cardiovasc Interv. 2018;92:379-387

Validating a prediction modeling tool for left ventricular outflow tract (LVOT) obstruction after transcatheter mitral valve replacement (TMVR)

Dee Dee Wang, MD¹ O | Marvin H, Eng. MD¹ O | Adam B, Greenbaum, MD¹ |

... evidence

Three-dimensional printing of models for surgical planning in patients with primary cardiac tumors

Daniel Schmauss, MD, a Nicolas Gerber, MSc, b and Ralf Sodian, MD

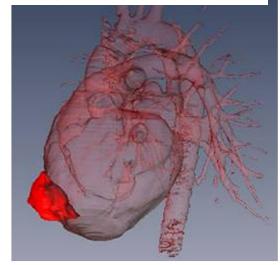
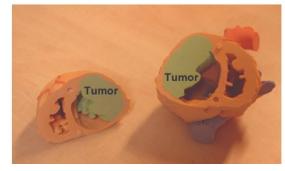
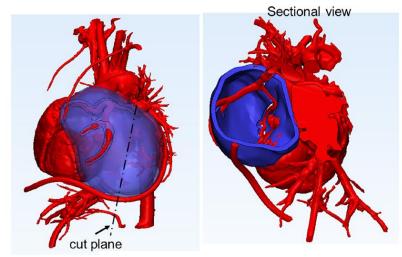


FIGURE 2. A 3-dimensional reconstruction of the heart with the tumor on the right ventricle.



Jacobs et al. Interact Cardiovasc Thorac Surg. 2008;7: 6–9.



Riggs et al. Transl Pediatr. 2018;7: 196-202.

DOI 10.1111/jocs.12812

NEW TECHNOLOGIES

WILEY Cardiac Surgery

Use of three-dimensional models to assist in the resection of malignant cardiac tumors

Odeaa Al Jabbari, M.D.^{1*} | Walid K. Abu Saleh, M.D.² | Avni P. Patel, M.E.¹ | Stephen R. Igo, B.S.¹ | Michael J. Reardon, M.D.¹

Tumor Solid LA Tumor Cross Section LA Tumor

Surgical Planning by 3D Printing for Primary Cardiac Schwannoma Resection

Kuk Hui Son 1* , Kun-Woo Kim 1* , Chi Bum Ahn 2 , Chang Hu Choi 1 , Kook Yang Park 1 , Chul Hyun Park 1 , Jae-Ik Lee 1 , and Yang Bin Jeon 1

Three-dimensional printed models for surgical planning of complex congenital heart defects: an international multicentre study

Israel Valverde^{a,b,c,d,*}, Gorka Gomez-Ciriza^a, Tarique Hussain^{c,e}, Cristina Suarez-Mejias^a,

METHODS: A prospective case-crossover study involving 10 international centres and 40 patients with complex CHD (median age 3 years, range 1 month–34 years) was conducted. Magnetic resonance imaging and computed tomography were used to acquire and segment the 3D cardiovascular anatomy. Models were fabricated by fused deposition modelling of polyurethane filament, and dimensions were compared with medical images. Decisions after the evaluation of routine clinical images were compared with those after inspection of the 3D model and intraoperative findings. Subjective satisfaction questionnaire was provided.

RESULTS: 3D models accurately replicate anatomy with a mean bias of -0.27 ± 0.73 mm. Ninety-six percent of the surgeons agree or strongly agree that 3D models provided better understanding of CHD morphology and improved surgical planning. 3D models changed the surgical decision in 19 of the 40 cases. Consideration of a 3D model refined the planned biventricular repair, achieving an improved surgical correction in 8 cases. In 4 cases initially considered for conservative management or univentricular palliation, inspection of the 3D model enabled successful biventricular repair.

CONCLUSIONS: 3D models are accurate replicas of the cardiovascular anatomy and improve the understanding of complex CHD. 3D models did not change the surgical decision in most of the cases (21 of 40 cases, 52.5% cases). However, in 19 of the 40 selected complex cases, 3D model helped redefining the surgical approach.



Radiological Society of North America (RSNA) 3D printing Special Interest Group (SIG): guidelines for medical 3D printing and appropriateness for clinical scenarios

Leonid Chepelev^{1†}, Nicole Wake^{2,3†}, Justin Ryan^{4†}, Waleed Althobaity^{1†}, Ashish Gupta^{1†}, Elsa Arribas^{5†}, Lumarie Santiago^{5†}, David H Ballard⁶, Kenneth C Wang⁷, William Weadock⁸, Ciprian N Ionita⁹, Dimitrios Mitsouras¹, Jonathan Morris¹⁰, Jane Matsumoto¹⁰, Andy Christensen¹, Peter Liacouras¹¹, Frank J Rybicki^{1*}, Adnan Sheikh¹ and RSNA Special Interest Group for 3D Printing

Cardiac Arrhythmias		
Cardiac Arrhythmia/atrial fibrillation	6	99,100
Cardiac Pacing	6	101,102
Cardiac Neoplasm		
Cardiac Tumors	7	103-110
Cardiac Transplant and Mechanical Circulatory Support		
Cardiac transplant	7	111
Left Ventricular Assist device	7	112-114
Total Artificial Heart	3	-
Heart Failure		
Heart Failure	2	-

- **1–3, rarely appropriate**: There is a lack of a clear benefit or experience that shows an advantage over usual practice.
- **4–6, maybe appropriate**: There may be times when there is an advantage, but the data is lacking, or the benefits have not been fully defined.
- **7–9**, **usually appropriate**: Data and experience shows an advantage to 3D printing as a method to represent and/or extend the value of data contained in the medical imaging examination.

Limitations & Challenges

Only (at best) as accurate as source imaging

Illusion of certainty: Margins of error and uncertainty in image interpretation difficult to capture (esp 3D Print)

Multi-step process = **multiple sources of error**: verification of critical details against source or other imaging is crucial

Mechanical properties poorly captured

Limited access, frequently on experimental basis

Limited evidence base. Lack of guidelines / appropriate use criteria*.

Infrasture needs to be developed for integration into regular clinical workflows: Organizational model of modeling services; PACS/EMR integration; cost recovery

The Near Future

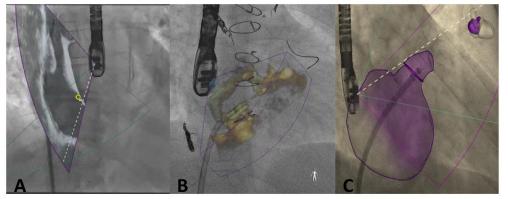


Figure 2 Different echocardiography imaging, such as 2D echocardiography with a *yellow marker* placed at the transseptal puncture site (A), 3D echocardiography (B), and 3D display of automatically rendered structures (C), can be overlaid onto the fluoroscopic screen to guide different procedural tasks. The tip of the catheter is in the LAA.

Multimodal image fusion to combine benefits of different modalities Modeling of **mechanical properties** of tissue for better physical & virtual simulation

Dynamic modeling to capture mobility of structures

Increased automation of process to increase speed and reduce cost

Procedural guidance: Fusion of model with intra-operative imaging; projection onto surgical field

Improved **infrastucture**: evidence base, guidelines, PACS support; remuneration

Acknowledgements

Joshua Qua Hiansen
Massimiliano Meineri,
Patricia Murphy
Department of Anesthesia & Pain
Management; and Division of Cardiac
Surgery, TGH
Peter Munk Cardiac Center Foundation

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Thank You!

