A missing data method for deconfounding in neuroimaging studies

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Accounting for motion in fMRI: What part of the spectrum are we characterizing in autism?

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Functional connectivity and resting-state fMRI

- Functional connectivity: spontaneous correlations between brain regions.
- Resting-state fMRI scans from Kennedy Krieger Institute and JHU SOM (either 5:20 or 6:45 seconds in length).
- Children are asked to remain motionless while staring at crosshairs.
- This is challenging, particularly for children with autism.
- Motion in the scanner produces artifacts.



Motion quality control exclusion

- Goal: E[Y|A=1] E[Y|A=0].
- Connectivity hypothesis of autism: short-range connections increased at the expense of long-range connections (Deen and Pelphrey, 2012; Just et al., 2004).
- Motion looks like an increase in shortand decrease in long-range (Power et al., 2012).
- Lenient: < 5 min data after removing frames > 3 mm or 3° from previous frame (Fassbender et al., 2017).
- Strict: mean framewise displacement > .2 mm or < 5 min data after excluding FD > .25 mm (Ciric et al., 2017).

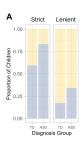


Figure: Quality control removes 30-83% of children with ASD and 12-60% of typically developing.

The problem: motion exclusion criteria causes sampling bias

• Motion quality control reduces one problem but creates a new problem: sample bias.

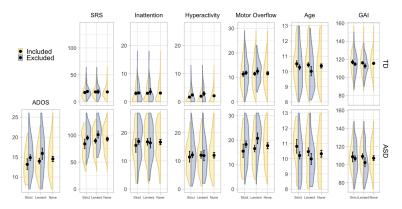


Figure: During QC, more severe cases of autism are excluded.

The problem: some behavioral measures are related to functional connectivity.

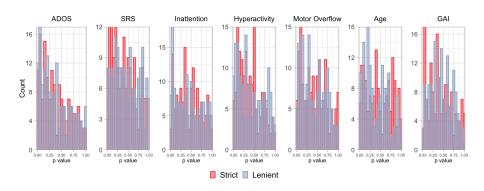


Figure: Some covariates related to rs-fMRI exclusion probability are also related to functional connectivity. Histograms of p-values from univariate GAMs at 153 brain connections.

The problem: confounding due to motion exclusion

- Y(1) is the counterfactual that a participant's scan is usable; A is diagnosis; W are behavioral measures.
- Define a novel parameter of interest:

$$\psi^* = E^* \left\{ E^* \left(Y(1) | A = 1, W \right) | A = 1 \right\}$$
$$- E^* \left\{ E^* \left(Y(1) | A = 0, W \right) | A = 0 \right\}$$

• The naïve estimator:

$$\begin{split} \psi_{naive} &= E\left\{ E\left(Y|\Delta=1, A=1, W\right) | \ \Delta=1, A=1 \right\} \\ &- E\left\{ E\left(Y(1) | \Delta=1, A=0, W\right) | \Delta=1, A=0 \right\} \end{split}$$

• Confounding: $\psi_{naive} \neq \psi^*$, e.g., Greenland et al. (1999).

The solution: Deconfounded group difference

- $\Delta = 0$ (unusable data) are treated as missing data.
- We define the target parameter, which we call the **deconfounded** group difference:

$$\psi = E\{E(Y \mid \Delta = 1, A = 1, W) \mid A = 1\}$$

$$-E\{E(Y \mid \Delta = 1, A = 0, W) \mid A = 0\}.$$

- $\psi = \psi^*$ under assumptions:
 - (A1.1) Conditional Randomization: for a = 0, 1,

$$E^*\{Y(1) \mid A = a, W\} = E\{Y \mid \Delta = 1, A = a, W\}.$$

• (A1.2) Positivity: for a = 0, 1 and all possible w,

$$P(\Delta = 1 \mid A = a, W = w) > 0.$$

• (A1.3) Consistency: for all i such that $\Delta_i = 1$, $Y_i(1) = Y_i$,

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Deconfounded group difference

- Consider group specific targets: $\psi_{A=1}$ and $\psi_{A=0}$.
- Propensity model:

$$g(a,w) = P(\Delta = 1|A=a, W=w)$$

• Classic IPW. For $a_i = 1$,

$$\hat{\psi}_{IPW,A=1} = \mathbb{E}_{n,a=1} \left\{ \frac{I(\Delta_i = 1)}{g_n(a_i = 1, w_i)} y_i \right\}$$

• Outcome model:

$$\bar{Q}(a, w) = E(Y | \Delta = 1, A = a, W = w)$$

• Classic G-computation estimator:

$$\hat{\psi}_{G,A=1} = \mathbb{E}_{n,a=1} \left\{ \bar{Q}_n(\Delta = 1, a_i = 1, w_i) \right\}$$

Doubly robust targeted minimum loss based estimation

- Use ensemble of machine learning methods to fit the propensity and outcome models (Van Der Laan et al., 2007).
- Estimate using doubly robust targeted minimum loss based estimation.
- DRTMLE from Benkeser et al. (2017) combines propensity and outcome models in a manner that
 - is efficient when both outcome and propensity models are consistent;
 - is consistent when at least one of the outcome or propensity models is consistent;
 - asymptotically normal with a variance that is consistent if at least one of the outcome or propensity models is consistent.

Data Analysis: Functional connectivity

- Resting-state fMRI scans from Kennedy Krieger Institute (either 5:20 or 6:45 seconds in length).
- 151 ASD children and 353 typically developing.
- Used lenient criteria.
- 107 ASD and 296 TD pass lenient criteria.
- Defined a "parcellation" using group ICA via GIFT with 30 components (Calhoun et al., 2001).
- Resulted in a time course for 30 components.
- Calculated partial correlation matrix for each child.
- Identified 18 signal components, looked at 153 partial correlations = functional connectivity.
- FConn processing follows a recent study of ASD in toddlers (Lombardo et al., 2019).

Data Analysis: Propensity and outcome models

- Input to drtmle: for each edge, residuals from a linear regression of functional connectivity vs motion variables, race, SES, sex, and dx with dx added back in.
- SuperLearner with 10-fold CV for propensity and outcome models: SL.earth, SL.glmnet, SL.gam, SL.glm, SL.ranger, SL.ridge, SL.step, SL.step.interaction, SL.svm, SL.xgboost.
- Predictors: Primary diagnosis, Head coil, ADHD secondary, Age at scan, Handedness, Stimulants, Motor overflow, General ability index, Inattention, Hyperactivity, Autism diagnostic observation schedule.

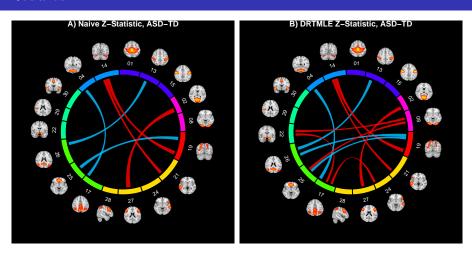


Figure: The deconfounded group difference via DRTMLE reveals more extensive differences between ASD and TD. Z-stats from partial correlations from the group ICA parcellation. Thresholded at FDR=0.20. Blue: ASD>TD. Naive: 6 edges, DRTMLE: 11 edges.

Discussion

- Participant exclusion due to motion quality control creates large sampling biases.
- We use DRTMLE to estimate the deconfounded group difference in a large study of autism spectrum disorder.
- More extensive differences between ASD and TD when accounting for sampling biases via DRTMLE.
- Future directions: develop estimator allowing for covariates that we balance between groups (demographics such as race, SES, sex) versus covariates for which we condition on diagnosis (measures of autism severity).
- Improved inference for finite samples.
- Additional info: https://github.com/thebrisklab/DeconfoundedFMRI
- Thank you!



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