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# Shapes analysis for time series.

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## Abstract

1 Analyzing inter-individual variability of physiological functions is particularly ap-  
2 pealing in medical and biological contexts to describe or quantify health conditions.  
3 Such analysis can be done by comparing individuals to a reference one with time  
4 series as biomedical data. This paper introduces an unsupervised representation  
5 learning (URL) algorithm for time series tailored to inter-individual studies. The  
6 idea is to represent time series as deformations of a reference time series. The  
7 deformations are diffeomorphisms parameterized and learned by our method called  
8 TS-LDDMM. Once the deformations and the reference time series are learned, the  
9 vector representations of individual time series are given by the parametrization of  
10 their corresponding deformation. At the crossroads between URL for time series  
11 and shape analysis, the proposed algorithm handles irregularly sampled multivariate  
12 time series of variable lengths and provides shape-based representations of  
13 temporal data. In this work, we establish a representation theorem for the graph  
14 of a time series and derive its consequences on the LDDMM framework. We  
15 showcase the advantages of our representation compared to existing methods using  
16 synthetic data and real-world examples motivated by biomedical applications.

## 1 Introduction

18 Our goal is to analyze the inter-individual variability of a time series dataset, which is of prime  
19 interest in medicine and biology [21, 46, 3, 17]. More specifically, we aim to find an unsupervised  
20 features representation method which encode the specificity of an individual compared to another. In  
21 physiology, studying the different *shapes* in a time series related to biological phenomena and their  
22 variations according to individual or pathology is common. However, a *shape* has no clear definition;  
23 it is more an intuitive way to speak about the silhouette of a pattern in a time series. In this paper, we  
24 refer to as the shape of a time series, the graph of this signal.

25 Although a community structure with representatives can be learned in an unsupervised way [44, 31]  
26 using contrastive loss [16, 43, 31] or similarity measures [1, 17, 37, 49], studying the inter-individual  
27 variability of shapes within a cluster [35, 41] is still an open problem in URL.

28 First, we propose not to see time series through their curve  $\{s_t : t \in I\}$ , but through their graph  
29  $G(s) = \{(t, s(t)) : t \in I\}$ . Then, building on the shape analysis literature [4, 45], we follow the  
30 Large Deformation Diffeomorphic Metric Mapping (LDDMM) framework [4, 45] to analyze these  
31 graphs. The idea is to represent each element  $(G(s^j))_{j \in [N]}$  of the dataset as the transformation of a  
32 reference graph  $G(s_0)$  by a diffeomorphism. Then, the diffeomorphism is learned by integrating an  
33 ordinary differential equation parameterized by a Reproducing Kernel Hilbert Space (RKHS). The  
34 parameters  $(\alpha_j)_{j \in [N]}$  encoding the diffeomorphisms  $(\phi_j)_{j \in [N]}$  yield the representation features of the  
35 graphs  $(G(s^j))_{j \in [N]}$ . Finally, these features encoding the shapes can feed any statistical or machine  
36 learning model as in URL.

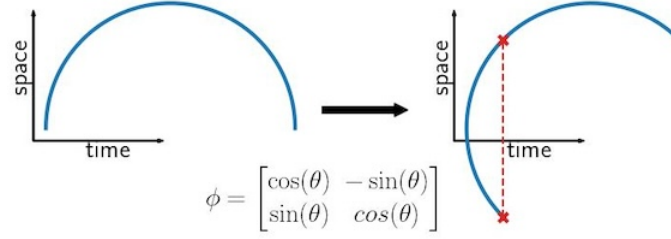


Figure 1: A time series' graph  $G = \{(t, s(t)) : t \in I\}$  can lose its structure after applying a general diffeomorphism  $\phi$ .  $G$ : a time value can be related to two values on the space axis.

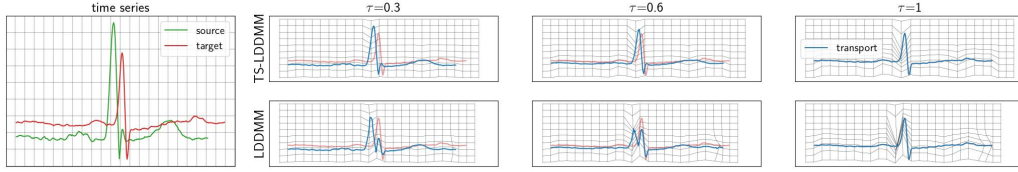


Figure 2: LDDMM and TS-LDDMM are applied to ECG data. We observe that LDDMM, using a general Gaussian kernel, does not learn the time translation of the first spike but changes the space values, i.e., one spike disappears before emerging at a translated position. At the same time, TS-LDDMM handles the time change in the shape. This difference of *deformations* implies differences in features *representations*.

However, a graph time series transformation by a general diffeomorphism is not always a graph time series, see e.g. Figure 1, thus a graph time series is more than a simple curve [19]. Our contributions arise from this observation. We solve this issue by specifying the class of diffeomorphisms to consider and showing how to learn them. This change is fruitful in representing time transformation as illustrated in Figure 2.

Our contributions can be summarized as follows:

- We propose an unsupervised method (TS-LDDMM) to analyze inter-individual variability of shapes in a time series dataset. In particular, the method can handle *irregularly sampled* time series with *variable sizes*.
- We motivate our extension of LDDMM to time series by introducing a theoretical framework with a representation theorem for time series graph (Theorem 1) and kernels related to their structure (Lemma 1).
- We demonstrate the identifiability of the model by estimating the true generating parameter of synthetic data, and we highlight the sensitivity of our method with respect to its hyperparameters, also providing guidelines for tuning. We highlight the *interpretability* of TS-LDDMM for studying the inter-individual variability in a clinical dataset. We illustrate the quantitative interest of the representation on classification tasks on real shape-based datasets.

## 2 Related Works

Shape analysis focus on the statistical analysis of various mathematical objects invariant under rotations, dilations, or time parameterization. The main idea is to represent these different objects in a complete Riemannian manifold  $(\mathcal{M}, g)$  with a metric  $g$  adapted to the geometry of the problem [32]. Then, any set of points in  $\mathcal{M}$  can be represented as points in the tangent space of their Frechet mean  $m_0$  [36, 28] by considering their logarithms. The goal is then to find a well suited Riemannian structure according to the studied object.

A time series graph can be seen as a curve and LDDMM structure is relevant to tackle curves as presented in [19]. However, time series graph has more structure than curves as depicted in Figure 1 due to the temporal evolution. [38] tracks anatomical shape changes in serial images using LDDMM, but distinguish from us by including the temporal evolution at a higher level: the goal is to perform longitudinal data modeling.

Leaving the LDDMM representation, [42, 22] address the representation of curves having unitary velocity by using the Square-Root Velocity (SRV) representation. However, the SRV representation applies after a reparametrization in time, such that the original time evolution of the time series is not represented in the final features. Again, the time series graph structure is not respected. Very recently in a functional data analysis framework, a paper [47] (Shape-FPCA) improved by giving a representation for the original time evolution. Nevertheless, this methods applies only on time series of *same size* and is made for *continuous objects*, making the estimation more sensitive to noise. [Ajouter littérature de URL demander à Sisi ?]

### 3 Notations

We denote by integer ranges by  $[k : l] = \{k, \dots, l\} \subset \mathcal{P}(\mathbb{Z})$  and  $[l] = [1 : l]$  with  $k, l \in \mathbb{N}$ , by  $C^m(I, E)$  the set of  $m$ -times continuously differentiable function defined on an open set  $U$  to a normed vector space  $E$ , by  $\|u\|_\infty = \sup_{x \in U} |u(x)|$  for any bounded function  $u : U \rightarrow E$ , and by  $\mathbb{N}_{>0}$  is the set of positive integers.

### 4 Background on LDDMM

In this part, there is no novelty, we simply expose how to learn the diffeomorphisms  $(\phi_j)_{j \in [N]}$  using LDDMM, initially introduced in [4]. In a nutshell, for any  $j \in [N]$ ,  $\phi_j$  corresponds to a differential flow related to a learnable velocity field belonging to a well-chosen Reproducing Kernel Hilbert Space (RKHS).

In the next section, the time series are going to be represented by diffeomorphism parameters  $(\alpha_j)_{j \in [N]}$ . That's why LDDMM is chosen since it offers a parametrization for diffeomorphisms which is sparse and interpretable, two features particularly relevant in the biomedical context.

The basic problem that we consider in this section is the following. Given a set of targets  $\mathbf{y} = (y_i)_{i \in [T_2]}$  in  $\mathbb{R}^{d'}$ , a set of starting points  $\mathbf{x} = (x_i)_{i \in [T_1]}$  in  $\mathbb{R}^{d'}$ , we aim to find a diffeomorphism  $\phi$  such that the finite set of points  $\mathbf{y}$  is similar in a certain sense to the set of finite sets of transformed points  $\phi \cdot \mathbf{x} = (\phi(x_i))_{i \in [T_1]}$ . The function  $\phi$  is occasionally referred to as a *deformation*. In general, these sets  $\mathbf{x}, \mathbf{y}$  are meshes of continous objects, e.g surfaces, curves, images and so on.

**Representing diffeomorphisms as deformations.** Such *deformations*  $\phi$  are constructed via differential flow equations, for any  $x_0 \in \mathbb{R}^{d'}$  and  $\tau \in [0, 1]$ :

$$\frac{dX(\tau)}{d\tau} = v_\tau(X(\tau)), \quad X(0) = x_0, \quad \phi_\tau^v(x_0) = X(\tau), \quad \phi^v = \phi_1^v, \quad (1)$$

where the velocity field is  $v : \tau \in [0, 1] \mapsto v_\tau \in V$  and  $V$  is a Hilbert space of continuously differentiable function on  $\mathbb{R}^{d'}$ . If  $\|du\|_\infty + \|u\|_\infty \leq \|u\|_V$  for any  $u \in V$  and  $v \in L^2([0, 1], V) = \{v \in C^0([0, 1], V) : \int_0^1 \|v_\tau\|_V^2 d\tau < \infty\}$ , by [18, Theorem 5]  $\phi^v$  exists and belongs to  $\mathcal{D}(\mathbb{R}^{d'})$ , where we denote by  $\mathcal{D}(O)$  the set of diffeomorphism defined on an open set  $O$  to  $O$ . Therefore, for any choice of  $v$ ,  $\phi^v$  defines a valid deformation. This offers a general recipe to construct diffeomorphism given a functional space  $V$ .

With this in mind, the velocity field  $v$  fitting the data can be estimated by minimizing  $v \in L^2([0, 1], V) \mapsto \mathcal{L}(\phi^v \cdot \mathbf{x}, \mathbf{y})$ , where  $\mathcal{L}$  is an appropriate loss function. However, two computational challenges arise. First, this optimization problem is ill-posed, and a penalty term is needed to obtain a unique solution. In addition, we have to find a parametric family  $V_\Theta \subset L^2([0, 1], V)$ , parameterized by  $\Theta$ , which allows us to solve this minimization problem efficiently.

<sup>1</sup>Note that we denote by  $d' \in \mathbb{N}$  the ambient space

106 It has been proposed in [32] to interpret  $V$  as a tangent space relative to the group of diffeomorphisms  
 107  $H = \{\phi^v : v \in L^2([0, 1], V)\}$ . Following this geometric point of view, geodesics can be constructed  
 108 on  $H$  by using the following squared norm

$$\mathcal{R}^2 : g \in H \mapsto \inf_{v \in L^2([0, 1], V) : g = \phi^v} \int_0^1 \|v_\tau\|_V^2 d\tau \quad (2)$$

109 By deriving differential constraints related to the minimum of (2) and using Cauchy lipshcitz condi-  
 110 tions, geodesics can be defined only by giving the starting point and the initial velocity  $v_0 \in V$  [32],  
 111 as straight lines in Euclidean space. Denoting by  $w(v_0)$  the geodesic starting from the identity with  
 112 initial velocity  $v_0$ , the exponential map is defined as  $\varphi^{\{v_0\}} \triangleq \phi^v$  and the previous matching problem  
 113 becomes a *geodesic shooting problem*:

$$\inf_{v_0 \in V} \mathcal{L}(\varphi^{\{v_0\}} \cdot \mathbf{x}, \mathbf{y}). \quad (3)$$

114 Using  $\varphi^{\{v_0\}}$  instead of  $\phi^v$  for any  $v \in L^2([0, 1], V)$  regularizes the problem and induces a sparse  
 115 representation for the learning diffeomorphisms. Moreover, by setting  $V$  as an RKHS, the geodesic  
 116 shooting problem has a unique solution and becomes tractable, as described in the next section.

117 **Discrete parametrization of diffeomorphism.** In this part,  $V$  is chosen as an RKHS [5] generated  
 118 by a smooth kernel  $K$  (e.g., Gaussian). We follow [13] and define a discrete parameterization of the  
 119 velocity fields to perform geodesics shooting (3). The initial velocity field  $v_0$  is chosen as a finite  
 120 linear combination of the RKHS basis vector fields,  $\mathbf{n}_0$  control points  $\mathbf{X}_0 = (x_{k,0})_{k \in [\mathbf{n}_0]} \in (\mathbb{R}^{d'})^{\mathbf{n}_0}$   
 121 and momentum vectors  $\alpha_0 = (\alpha_{k,0})_{k \in [\mathbf{n}_0]} \in (\mathbb{R}^{d'})^{\mathbf{n}_0}$  are defined such that for any  $x \in \mathbb{R}^{d'}$ ,

$$v_0(\alpha_0, \mathbf{X}_0)(x) = \sum_{k=1}^{\mathbf{n}_0} K(x, x_{k,0}) \alpha_{k,0}. \quad (4)$$

122 In our applications, the control points  $(x_{k,0})_{k \in [\mathbf{n}_0]}$  can be understood as the discretized graph  
 123  $(t_k, \mathbf{s}_0(t_k))_{k \in [\mathbf{n}_0]}$  of a starting time series  $\mathbf{s}_0$ . With this parametrization of  $v_0$ , (author?) [32] show  
 124 that the velocity field  $v$  of the solution of (3) keeps the same structure along time, such that for any  
 125  $x \in \mathbb{R}^{d'}$  and  $\tau \in [0, 1]$ ,

$$v_\tau(x) = \sum_{k=1}^{\mathbf{n}_0} K(x, x_k(\tau)) \alpha_k(\tau), \quad (5)$$

$$\begin{cases} \frac{dx_k(\tau)}{d\tau} = v_\tau(x_k(\tau)), & \frac{d\alpha_k(\tau)}{d\tau} = - \sum_{l=1}^{\mathbf{n}_0} d_{x_k(\tau)} K(x_k(\tau), x_l(\tau)) \alpha_l(\tau)^\top \alpha_k(\tau) \\ \alpha_k(0) = \alpha_{k,0}, & x_k(0) = x_{k,0}, k \in [\mathbf{n}_0] \end{cases}$$

126 These equations are derived from the hamiltonian  $H : (\alpha_k, x_k)_{k \in [\mathbf{n}_0]} \mapsto \sum_{k,l=1}^{\mathbf{n}_0} \alpha_k^\top K(x_k, x_l) \alpha_l$ ,  
 127 such that the velocity norm is preserved  $\|v_\tau\|_V = \|v_0\|_V$  for any  $\tau \in [0, 1]$ . By (5), the velocity  
 128 field related to a geodesic  $v^*$  is fully parametrized by its initial control points and momentum  
 129  $(x_{k,0}, \alpha_{k,0})_{k \in [\mathbf{n}_0]}$ . Thus, given a set of targets  $\mathbf{y} = (y_i)_{i \in [T_2]}$  in  $\mathbb{R}^{d'}$ , a set of starting points  $\mathbf{x} =$   
 130  $(x_{i,0})_{i \in [T_1]}$  in  $\mathbb{R}^{d'}$ , a RKHS's kernel  $K : \mathbb{R}^{d'} \times \mathbb{R}^{d'} \rightarrow \mathbb{R}^{d' \times d'}$ , a distance on sets  $\mathcal{L}$ , a numerical  
 131 integration scheme of ODE and a penalty factor  $\lambda > 0$ , the basic geodesic shooting step minimizes  
 132 the following function using a gradient descent method:

$$\mathcal{F}_{\mathbf{x}, \mathbf{y}} : (\alpha_k)_{k \in [T_1]} \mapsto \mathcal{L}(\varphi^{\{v_0\}} \cdot \mathbf{x}, \mathbf{y}) + \lambda \|v_0\|_V^2, \quad (6)$$

134 where  $v_0$  is defined by (4) and  $\varphi^{\{v_0\}} \cdot \mathbf{x}$  is the result of the numerical integration of (5) using control  
 135 points  $\mathbf{x}$  and initial momentums  $(\alpha_k)_{k \in [T_1]}$ .

136 **Relation to Continuous Normalizing Flows.** One particular popular choice to address the problem  
 137 of learning a diffeomorphism or a velocity field is Normalizing Flows [39, 27] (NF) or their continuous  
 138 counterpart [9, 20, 40] (CNF). However, we do not rely on this class of learning algorithms for several  
 139 reasons. Indeed, existing and simple normalizing flows are not suitable for the type of data that  
 140 we are interested in this paper [15, 12]. In addition, they are primarily designed to have tractable

Jacobian functions, while we do not require such property in our applications. Finally, the use of a differential flow solution of an ODE (1) trick is also at the basis of CNF, which then consists of learning a velocity field to address in fitting the data through a loss aiming to address the problem at hand. Nevertheless, the main difference between CNF and LDDMM lies in the parametrization of the velocity field. LDDMM uses kernels to derive closed form formula and enhance interpretability while NF and CNF take advantage of deep neural networks to scale with large dataset in high dimensions.

## 5 Methodology

We consider in this paper observations which consist in a population of  $N$  multivariate time series, for any  $j \in [N]$ ,  $s^j \in C^1(I_j, \mathbb{R}^d)$ . However, we can only access a  $n_j$ -samples  $\tilde{s}^j = (\tilde{s}_i^j = s^j(t_i^j))_{i \in [n_j]}$  collected at timestamps  $(t_i^j)_{i \in [n_j]}$  for any  $j \in [N]$ . Note that **the number of samples  $n_j$  is not necessary the same across individuals** and the timestamps can be **irregularly sampled**. We assume the time series population is globally homogeneous regarding their "shapes" even if inter-individual variability exists. Intuitively speaking, the "shape" of a time series  $s : I \rightarrow \mathbb{R}^d$  is encoded in its graphs  $G(s)$  defined as the set  $\{(t, s(t)) : t \in I\}$  and not only in its values  $s(I) = \{s(t) : t \in I\}$  since the time axis is crucial. As a motivating use-case,  $s^j$  can be the time series of a heartbeat extracted from an individual's electrocardiogram (ECG), see Figure 2. The homogeneity in a resulting dataset comes from the fact that humans have similar shapes of heartbeat [48, 30].

**The deformation problem.** In this paper, we aim to study the inter-individual variability in the dataset by finding a relevant representation of each time series. Inspired from the framework of shape analysis [45], addressing similar problems in morphology, we suggest to represent each time series' graph  $G(s^j)$  as the transformation of a reference graph  $G(s_0)$ , related to a time series  $s_0 : I \rightarrow \mathbb{R}^d$ , by a diffeomorphism  $\phi_j$  on  $\mathbb{R}^{d+1}$ , for any  $j \in [N]$ ,

$$\phi_j.G(s_0) = \{\phi_j(t, s_0(t)), t \in I\}. \quad (7)$$

$s_0$  will be understood as the typical representative shape common to the collection of time series  $(s^j)_{j \in [N]}$ . As  $s_0$  is supposed to be fixed, then the representation of the time series  $(s^j)_{j \in [N]}$  boils down to the one of the transformation  $(\phi_j)_{j \in [N]}$ . We aim to learn  $G(s_0)$  and  $(\phi_j)_{j \in [N]}$ .

**Optimization related to (7).** Defining the *discretized graphs* of the time series  $(s^j)_{j \in [N]}$  and a discretization of the reference graph  $G(s_0)$  as, for any  $j \in [N]$ ,

$$\mathbf{y}_j = G(\tilde{s}^j) = (t_i^j, \tilde{s}_i^j)_{i \in [n_j]} \in (\mathbb{R}^{d+1})^{n_j}, \quad \tilde{G}_0 = (t_i^0, \tilde{s}_i^0)_{i \in [\mathbf{n}_0]} \in (\mathbb{R}^{d+1})^{\mathbf{n}_0},$$

with  $\mathbf{n}_0 = \text{median}((n_j)_{j \in [N]})$ , the representation problem given in (7) boils down solving:

$$\text{argmin}_{\tilde{G}_0, (\alpha_k^j)_{k \in [\mathbf{n}_0]}^{j \in [N]}} \sum_{j=1}^N \mathcal{F}_{\tilde{G}_0, \mathbf{y}_j} \left( (\alpha_k^j)_{k \in [\mathbf{n}_0]} \right), \quad (8)$$

which is carried out by a gradient descent on the control points  $\tilde{G}_0$  and the momentums  $\alpha_j = (\alpha_k^j)_{k \in [\mathbf{n}_0]}$  for any  $j \in [N]$ , initialized by a dataset's time series graph of size  $\mathbf{n}_0$  and by  $0_{(d+1)\mathbf{n}_0}$  respectively. The optimization hyperparameter details are given in Appendix D.1. The result of the minimization  $\tilde{G}_0$  is then considered as the  $\mathbf{n}_0$ -samples of a common time series  $s_0$  and the momentums  $\alpha_j$  encoding  $\phi_j$  yields a feature vector in  $\mathbb{R}^{d\mathbf{n}_0}$  of  $s^j$  for any  $j \in [N]$ . Finally, the vectors  $(\alpha_j)_{j \in [N]}$  can be analyzed with any statistical or machine learning tools such as Principal Components Analysis (PCA), Latent Discriminant Analysis (LDA), longitudinal data analysis and so on.

Nevertheless, (8) ask to define a kernel and a loss in order to perform geodesic shooting 6, which is the purpose of the next subsection.

### 5.1 Application of LDDMM to time series analysis: TS-LDDMM

In this section, we present our theoretical contribution: we tailor the LDDMM framework to handle time series data. The reason is that applying a general diffeomorphism  $\phi$  from  $\mathbb{R}^{d+1}$  to a time series'

graph  $G(s)$  can result in a set  $\phi.G(s)$  that does not correspond to the graph of any time series, as illustrated in the Figure 1. Thus, Time series graph have more structure than a simple 1D curve [19] and deserve their special analysis which will prove fruitful as demonstrated in 6.

To address this challenge, we need to identify an RKHS kernel  $K : \mathbb{R}^{d+1} \times \mathbb{R}^{d+1} \rightarrow \mathbb{R}^{(d+1)^2}$  that generates deformations preserving the structure of the time series graph. This goal motivates us to clarify, in Theorem 1, the specific representation of diffeomorphisms we require before presenting a class of kernels that produce deformations with this representation.

Similarly, selecting a loss function on sets  $\mathcal{L}$  that considers the temporal evolution in a time series' graph is crucial for meaningful comparisons with time series data. Consequently, we introduce the oriented Varifold distance.

**A representation separating space and time.** We prove that two time series graphs can always be linked by a time transformation composed of a space transformation. Moreover, a time series graph transformed by this kind of transformation is always a time series graph. We define  $\Psi_\gamma \in \mathcal{D}(\mathbb{R}^{d+1}) : (t, x) \in \mathbb{R}^{d+1} \rightarrow (\gamma(t), x)$  for any  $\gamma \in \mathcal{D}(\mathbb{R})$  and  $\Phi_f : (t, x) \in \mathbb{R}^{d+1} \rightarrow (t, f(t, x))$  for any  $f \in C^1(\mathbb{R}^{d+1}, \mathbb{R}^d)$ . We have the following representation theorem. All proofs are given in Appendix A.

Denote by  $G(s) \triangleq \{(t, s(t)) : t \in I\}$  the graph of a time series  $s : I \rightarrow \mathbb{R}^d$  and  $\phi.G(s) \triangleq \{\phi(t, s(t)) : t \in I\}$  the action of  $\phi \in \mathcal{D}(\mathbb{R}^{d+1})$  on  $G(s)$ .

**Theorem 1.** *Let  $s : J \rightarrow \mathbb{R}^d$  and  $s_0 : I \rightarrow \mathbb{R}^d$  be two continuously differentiable time series with  $I, J$  two intervals of  $\mathbb{R}$ . There exist  $f \in C^1(\mathbb{R}^{d+1}, \mathbb{R}^d)$  and  $\gamma \in \mathcal{D}(\mathbb{R})$  such that  $\gamma(I) = J$  and  $\Phi_f \in \mathcal{D}(\mathbb{R}^{d+1})$ ,*

$$G(s) = \Pi_{\gamma, f}.G(s_0), \quad \Pi_{\gamma, f} = \Psi_\gamma \circ \Phi_f.$$

*Moreover, for any  $\bar{f} \in C^1(\mathbb{R}^{d+1}, \mathbb{R}^d)$  and  $\bar{\gamma} \in \mathcal{D}(\mathbb{R})$ , there exists a continuously differentiable time series  $\bar{s}$  such that  $G(\bar{s}) = \Pi_{\bar{\gamma}, \bar{f}}.G(s_0)$*

**Remark 2.** *that for any  $\gamma \in \mathcal{D}(\mathbb{R})$  and  $s \in C^0(I, \mathbb{R}^d)$ ,*

$$\{(\gamma(t), s(t)), t \in I\} = \{(t, s \circ \gamma^{-1}(t)) : t \in \gamma(I)\}.$$

*As a result,  $\Psi_\gamma$  can be understood as a temporal reparametrization and  $\Phi_f$  encodes the transformation about the space.*

**Choice for the kernel associated with the RKHS  $\mathcal{V}$**  As depicted on Figure 1-2, we can not use any kernel  $K$  to apply the previous methodology to learn deformations on time series' graphs. We describe and motivate our choice in this paragraph. Denote the one-dimensional Gaussian kernel by  $K_\sigma^{(a)}(x, y) = \exp(-|x - y|^2/\sigma)$  for any  $(x, y) \in (\mathbb{R}^a)^2$ ,  $a \in \mathbb{N}$  and  $\sigma > 0$ . To solve the geodesic shooting problem (6) on  $\mathbb{R}^{d+1}$ , we consider for  $\mathcal{V}$  the RKHS associated with the kernel defined for any  $(t, x), (t', x') \in (\mathbb{R}^{d+1})^2$ :

$$K_G((t, x), (t', x')) = \begin{pmatrix} c_0 K_{\text{time}} & 0 \\ 0 & c_1 K_{\text{space}} \end{pmatrix}, \quad (9)$$

$$K_{\text{space}} = K_{\sigma_{T,1}}^{(1)}(t, t') K_{\sigma_x}^{(d)}(x, x') I_d, \quad K_{\text{time}} = K_{\sigma_{T,0}}^{(1)}(t, t'),$$

parametrized by the widths  $\sigma_{T,0}, \sigma_{T,1}, \sigma_x > 0$  and the constants  $c_0, c_1 > 0$ . This choice for  $K_G$  is motivated by the representation Theorem 1 and the following result.

**Lemma 1.** *If we denote by  $\mathcal{V}$  the RKHS associated with the kernel  $K_G$ , then for any vector field  $v$  generated by (5) with  $v_0$  satisfying (4), there exist  $\gamma \in \mathcal{D}(\mathbb{R})$  and  $f \in C^1(\mathbb{R}^{d+1}, \mathbb{R}^d)$  such that  $\phi^v = \Psi_\gamma \circ \Phi_f$ .*

[Parler des Cauchy kernel en appndice et du choix de la loss](#)

**Remark 3.** *With this choice of kernel, the features associated to the time transformation can be extracted from the momentums  $(\alpha_{k,0})_{k \in [n_0]} \in (\mathbb{R}^{d+1})^{n_0}$  in (4) by taking the coordinates related to time. However, the features related to the space transformation are not only in the space coordinates since the related kernel  $K_{\text{space}}$  depends on time as well.*

In Appendix C, we give guidelines for selecting the hyperparameters  $(\sigma_{T,0}, \sigma_{T,1}, \sigma_x, c_0, c_1)$ .

225 **Loss** This section specifies the distance function  $\mathcal{L}$  introduced in the loss function defined in (6).

226 In practice, we can only access discretized graphs of time series,  $(t_i^j, \tilde{s}_i^j)_{i \in [n_j]}$  for any  $j \in [N]$ , that are  
 227 potentially of different sizes  $n_j$  and sampled at different timestamps  $(t_i^j)_{i \in [n_j]}$  for any  $j \in [N]$ . Usual  
 228 metrics, such as the Euclidean distance, are not appealing as they make the underlying assumptions  
 229 of equal size sets and the existence of a pairing between points. Distances between measures on sets  
 230 (taking the empirical distribution), such as Maximum Mean Discrepancy (MMD) [14, 6], alleviate  
 231 those issues; however, MMD only accounts for positional information and lacks information about  
 232 the time evolution between sampled points. A classical data fidelity metric from shape analysis  
 233 corresponding to the distance between *oriented varifolds* associated with curves alleviates this last  
 234 issue [26]. Intuitively, an oriented varifold is a measure that accounts for positional and tangential  
 235 information about the underlying curves at sample points. More details and information about  
 236 *oriented varifolds* can be found in Appendix B.

237 More precisely, given two sets  $G_0 = (g_i^0)_{i \in [T_0]}$ ,  $G_1 = (g_i^1)_{i \in [T_1]} \in (\mathbb{R}^{d+1})^{T_1}$  and a kernel<sup>2</sup>  $k :$   
 238  $(\mathbb{R}^{d+1} \times \mathbb{S}^d)^2 \rightarrow \mathbb{R}$  verifying [26, Proposition 2 & 4], for any  $\xi \in \{0, 1\}$  and  $i \in [T_\xi - 1]$ , denoting  
 239 the center and length of the  $i^{th}$  segment  $[g_i^\xi, g_{i+1}^\xi]$  by  $c_i^\xi = (g_i^\xi + g_{i+1}^\xi)/2$ ,  $l_i^\xi = \|g_{i+1}^\xi - g_i^\xi\|$ , and  
 240  $\vec{v}_i^\xi = (g_{i+1}^\xi - g_i^\xi)/l_i^\xi$ , the varifold distance between  $G_0$  and  $G_1$  is defined as,

$$\begin{aligned} d_{W^*}^2(G_0, G_1) &= \sum_{i,j=1}^{T_0-1} l_i^0 k((c_i^0, \vec{v}_i^0), (c_j^0, \vec{v}_j^0)) l_j^0 - 2 \sum_{i=1}^{T_0-1} \sum_{j=1}^{T_1-1} l_i^0 k((c_i^0, \vec{v}_i^0), (c_j^1, \vec{v}_j^1)) l_j^1 \\ &+ \sum_{i,j=1}^{T_1-1} l_i^1 k((c_i^1, \vec{v}_i^1), (c_j^1, \vec{v}_j^1)) l_j^1 \end{aligned}$$

241 In practice, we set the kernel  $k$  as the product of two anisotropic Gaussian kernels,  $k_{\text{pos}}$  and  $k_{\text{dir}}$ ,  
 242 such that for any  $(x, \vec{u}), (y, \vec{v}) \in (\mathbb{R}^{d+1} \times \mathbb{S}^d)^2$

$$k((x, \vec{u}), (y, \vec{v})) = k_{\text{pos}}(x, y) k_{\text{dir}}(\vec{u}, \vec{v}).$$

243 The specific kernels  $k_{\text{pos}}, k_{\text{dir}}$  that we use in our experiments are given Appendix B.1. Note that  
 244 the loss kernel  $k$  has nothing to do with the velocity field kernel denoted by  $K_G$  or  $K$  specified in  
 245 Section 5.1. Finally, we define the data fidelity loss function,  $\mathcal{L}$ , as  $d_{W^*}^2$ , which is differentiable with  
 246 regards to its first variable. For further readings on curves and surfaces representation as varifolds,  
 247 readers can refer to [26, 8].

248 [Parler de méthode adaptatif ici](#)

## 249 6 Experiments

250 [L'intro est ce necessaire ?]

251 First, we show on synthetic data that the proposed representation is identifiable provided that the  
 252 hyperparameters and the reference graph are wisely selected, i.e., the parameter  $v_0^*$  generating a  
 253 deformation  $\varphi^{\{v_0^*\}}$  of a time series graph  $G$  can be estimated from the data  $G, \varphi^{\{v_0^*\}}.G$  by solving  
 254 the geodesic shooting problem (6). Secondly, we illustrate the qualitative interest of TS-LDDMM in  
 255 studying inter-individual variability on a clinical dataset. Thirdly, we demonstrate the quantitative  
 256 performance of our representation by performing classification on shape-based datasets. The method  
 257 is implemented on Python using the library JAX<sup>3</sup>. The code was compiled on a server with NVIDIA  
 258 RTX A2000 12GB GPU, Intel(R) Xeon(R) Gold 5220R CPU @ 2.20GHz, and 250 GB of RAM. The  
 259 code will be available on Github.

### 260 6.1 Synthetic experiments

261 First, we show the model identifiability when the kernel  $K_G$  is well specified: the estimated param-  
 262 eter is a good approximation of the generating parameter when the generation and the estimation

<sup>2</sup> $\mathbb{S}^d = \{x \in \mathbb{R}^{d+1} : |x| = 1\}$

<sup>3</sup><https://github.com/google/jax>

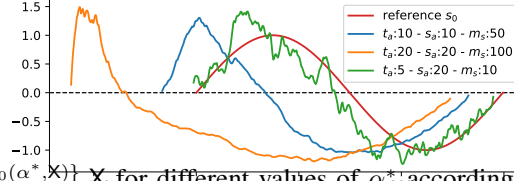


Figure 3: Plots of  $\varphi^{\{v_0(\alpha^*, X)\}} \cdot X$  for different values of  $\alpha^*$  according to its sampling parameter  $t_a, s_a, m_s$ , taking  $X = G(s_0)$  with  $s_0 : k \in [300] \rightarrow \sin(2\pi k/300)$ .

Table 1: Values of  $\mathcal{L}(\varphi^{\{v_0(\alpha^*, X)\}} \cdot X, \varphi^{\{\hat{v}_0\}} \cdot X)$  as  $\alpha^*$  is sampled according to  $\text{Gen}(10, 10, 50)$  and  $\hat{v}_0$  is estimated using  $K_G$  with varying parameters  $\sigma_{T,1}, \sigma_x$ .

$\sigma_{T,0} \backslash \sigma_x$	1	10	50	100	200	300
0.1	2e+0	3e-4	1e-5	4e-6	7e-4	4e-3
1	4e-2	1e-4	1e-5	4e-6	7e-4	4e-3
100	4e-2	2e-4	1e-5	4e-6	7e-4	4e-3

procedure use the same hyperparameters for the RKHS kernel  $K_G$ . All the hyperparameter values for generation and estimation are given in Appendix D.2. We fix the initial control points as  $X = (x_k = (k, \sin(2\pi k/300)))_{k \in [300]}$ . Given  $m_s \in \mathbb{N}_{>0}$  and  $t_a, s_a > 0$ , we randomly generate initial momentums  $\alpha^* = (\alpha_k^*)_{k \in [n_0]}$  with the following sampling, called  $\text{Gen}(m_s, t_a, s_a)$ : For any  $k \in [n_0]$ ,  $\alpha_k^*$  is sampled according to a Gaussian normal distribution  $\mathcal{N}(0_{d+1}, I_{d+1})$ . Then,  $(\alpha_k^*)_{k \in [n_0]}$  is regularized by a rolling average of size  $m_s$ , we get  $\bar{\alpha}' = (\bar{\alpha}'_k)_{k \in [n_0]}$ . Finally, we normalize  $\bar{\alpha}'$  to derive  $\alpha^*$  such that  $|([\alpha_k^*]_t)_{k \in [n_0]}| = t_{\text{amp}}$  and  $|([\alpha_k^*]_s)_{k \in [n_0]}| = s_{\text{amp}}$  for any  $k \in [n_0]$ , denoting by  $[\alpha_k^*]_t, [\alpha_k^*]_s$  the time and space coordinates of  $\alpha_k^*$  respectively. Note that the regularizing step  $(\alpha_k^*)_{k \in [n_0]} \rightarrow \bar{\alpha}'$  is necessary to obtain realistic deformations which take into account the regularity induced by the RKHS  $V$ . Then, using  $v_0(\alpha^*, X)$  as defined in (4) with initial momentums  $\alpha^*$  and control points  $X$ , we apply the induced deformation  $\varphi^{\{v_0\}}$  by (5) to  $X$  and obtain  $\varphi^{\{v_0\}} \cdot X$ . Finally, we solve (6) to recover an estimation  $\hat{\alpha}$  of  $\alpha^*$  and report the average relative error (ARE)  $|v_0(\hat{\alpha}, X) - v_0(\alpha^*, X)|_V / |v_0(\alpha^*, X)|_V$  on 50 repetitions. This procedure is performed for any  $m_s, t_a, s_a \in \{10, 50, 100\} \times \{5, 10, 15, 20\}^2$ . Mean, standard deviation, and maximum of the ARE on all these hyperparameters choices are respectively **0.10, 0.03, 0.17**. Therefore, the estimation procedure (6) offers a good approximation of the true parameter when the kernel  $K_G$  is well specified. We observe that the estimation is difficult when  $t_a \ll s_a$  because the time series can be very noisy as illustrated in Figure 3: this impacts the Varifold loss which is sensitive to tangents.

Secondly, we demonstrate a weak identifiability when the kernel  $K_G$  is misspecified: we can reconstruct the graph time series' after deformations even if the hyperparameters of  $K_G$  are different during the generation and the estimation. The hyperparameters of  $K_G$  during generation are  $(c_0, c_1, \sigma_{T,0}, \sigma_{T,1}, \sigma_x) = (1, 0.1, 100, 1, 1)$  and we fix  $\sigma_{T,1}, c_0, c_1 = (1, 1, 0.1)$  for  $K_G$  during estimation. We aim to understand the impact of  $\sigma_{T,1}, \sigma_x$  on the reconstruction since they are encoding the smoothness of the transformation according to time and space.

For any choice of the hyperparameters  $\sigma_{T,1}, \sigma_x \in \{1, 10, 50, 100, 200, 300\} \times \{0.1, 1, 100\}$  related to  $K_G$  in the estimation, we average  $\mathcal{L}(\varphi^{\{v_0(\alpha^*, X)\}} \cdot X, \varphi^{\{\hat{v}_0\}} \cdot X)$  on 50 repetitions when  $\alpha^*$  is sampled according to  $\text{Gen}(10, 10, 50)$  and  $\hat{v}_0 = v_0(\hat{\alpha}, X)$  denoting by  $\hat{\alpha}$  the result of the minimization (6). We observe in Table 1 that the reconstruction is almost perfect except in the case when  $\sigma_{t,0} = 1$  during estimation, while  $\sigma_{t,0} = 100$  during generation. Compared to  $\sigma_{T,0}$ ,  $\sigma_x$  has nearly no impact on the reconstruction. In Appendix B.1-C, we propose guidelines to drive future hyperparameters tuning and further discussions related to  $\sigma_{T,1}, c_0, c_1$ .

## 6.2 Qualitative analysis of respiratory behavior in mice

This experiment highlights the *interpretability* of TS-LDDMM for studying the inter-individual variability in a clinical dataset. We consider a time series dataset recording the evolution of the respiratory airflow of mice exposed to an irritant molecule altering respiratory functions [34]. The dataset is divided into two groups, one composed of 7 control mice (**wt**) and the other of 7 mice (**colq**) deficient in an enzyme involved in the control of respiration. For each mouse, the respiratory airflow was recorded for 15 to 20 minutes before exposure to the irritant molecule and then for 35



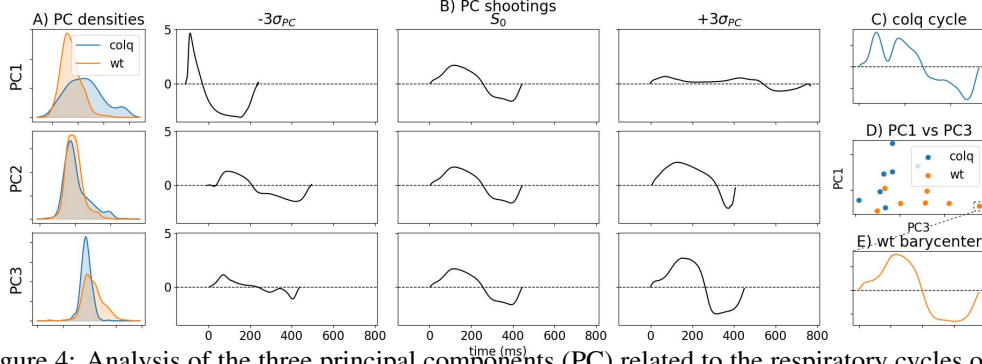


Figure 4: Analysis of the three principal components (PC) related to the respiratory cycles of the mouse before exposure. In Figure A), the densities of each genotype according to each PC are displayed. In Figure B), the deformations of the reference graph  $S_0$  along each PC are given. In Figure D), the graph of reference  $S^j$ , also called barycenter, related to each mouse, is displayed according to their coordinates on PC1 and PC3. In Figure C) et E), illustrations of respiratory cycles related to mice coming from the **wt** and **colq** group are displayed.

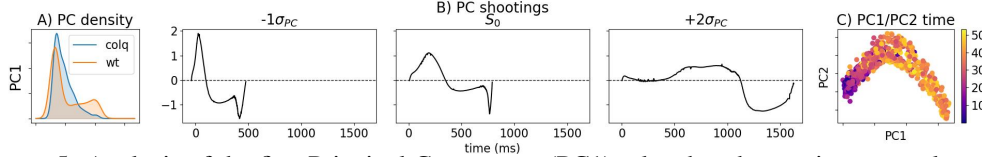


Figure 5: Analysis of the first Principal Component (PC1) related to the respiratory cycles of the mouse before and after exposure. In Figure A), the densities of each genotype according are displayed. In Figure B), the deformations of the reference graph  $S_0$  PC1 is given. In Figure C), respiratory cycles displayed with respect to time and according to their coordinates on PC1 and PC2

301 to 40 minutes. A complete description of the dataset is given in the Appendix E. By comparing  
 302 the shape of individual respiratory cycles (inspiration + expiration, see Figure 4-C)), we show that  
 303 TS-LDDMM features can encode genotype distinctive breathing behaviors and their evolution after  
 304 exposure to the irritant molecule.

305 We first compare breathing behaviors before exposure. Solving (8), we derive the reference respiratory  
 306 cycle's graph  $S_0$  and the TS-LDDMM features representations  $(\alpha_j)_{j \in [N_1]}$  related to  $N_1 = 700$   
 307 respiratory cycles extracted according to the procedure [17]. Then, we perform a kernel PCA on the  
 308 initial velocity field  $(v_0(\alpha_j, S_0))_{j \in [N_1]} \in V^{N_1}$  defined in (4). In Figure 4, we focus on the analysis  
 309 of the three Principal Components (PC).

310 As observable from Figure 4-B), principal components refer to different types of deformations. By  
 311 interpreting Figure 4-B): Only PC1 accounts for time warping, PC2 expresses the trade-off between  
 312 inspiration and expiration duration, and PC3 corresponds to a change in signal amplitude. Compared  
 313 to **wt** mice, the distribution of **colq** mice TS-LDDMM feature representation along the PC1 axis  
 314 has a heavy tail and the associated deformation (+3  $\sigma_{PC}$ ) shows an inspiration with two peaks. As  
 315 illustrated in Figure 4-A), such respiratory cycles are preponderant with **colq** mice and may be caused  
 316 by motor impairment due to their enzyme deficiency, [17]. In addition, the **colq** mice were smaller  
 317 than the **wt** mice due to a delay in growth caused by their lack of an enzyme. This difference can be  
 318 seen on PC3 since the volumes of air (area under the curve) inspired and exhaled are smaller for the  
 319 smaller mice. In correlation, the distribution of **wt** mice TS-LDDMM feature representations along  
 320 the PC3 axis have a heavy tail corresponding to large air volume as depicted by the deformation  
 321 (+3  $\sigma_{PC}$ ) in Figure 4-B). Finally, Figure 4-D) shows that PC1 and PC3 capture the main differences  
 322 between the two groups as their respective reference graphs  $S^j$  are located in different parts of the  
 323 space.

324 We perform a second experiment to analyze the evolution of breathing behaviors when mice are  
 325 exposed to the irritant molecule. We follow the same procedure as before. However, we take  
 326  $N_2 = 1400$  with 25% (resp. 75%) before (resp. after) exposure. In Figure 5, we focus on the first  
 327 principal component PC since it encodes the effect of the irritant molecule as depicted in Figure 5-C)  
 328 (the exposure occurs at 20 minutes). Figure 5-B) shows that the deformation (+3  $\sigma_{PC}$ ) leads to

Table 2: Classification results in f1-score (U: unsupervised, S: supervised, DL: deep learning, ML: machine learning).  $\mathbf{x}$  best unsupervised method,  $\underline{x}$  best supervised method.

		ArrowHead	ECG200	GunPoint	NATOPS
U	TS-LDDMM-SVC	<b>0.84</b>	<b>0.82</b>	<b>0.94</b>	<b>0.93</b>
	T-loss-SVC	0.57	0.76	0.82	0.88
	DTW-kNN	0.70	0.75	0.91	0.88
DL	CNN	0.70	0.79	0.85	<u>0.96</u>
	ResNet	0.77	0.87	0.97	0.95
S	ML Catch22	0.73	0.81	0.96	0.89
	Rocket	<u>0.81</u>	<u>0.91</u>	<u>1.00</u>	0.88

longer respiratory cycles that include pauses, as observed in [17]. As well, Figure 5-A) shows that TS-LDDMM features distributions are less spread out for **colq** mice compared to **wt** mice. Indeed, the irritant molecule inhibits the action of the deficient enzyme, **wt** mice strongly react to the irritant molecule, whereas **colq** mice are better adapted due to their deficiency.

### 6.3 Quantitative performances of the TS-LDDMM representation in classification

Combined with a Support Vector Classifier (SVC) [24], TS-LDDMM representation can be used for classification tasks using the kernel associated with the initial velocity space  $V$ . We compare TS-LDDMM-SVC classification performances with another SVC using representation learned with T-loss [16], an unsupervised deep learning feature representation method for time series. We also include fully supervised methods in deep learning -ResNet, CNN [25]- and machine learning: Catch22 [29], Rocket [11], Dynamic Time Wrapping k-Nearest Neighbors (DTW-kNN) [33]. Methods are compared using f1-score on several shape-based UCR/UEA datasets [10, 2] introduced in Appendix F. All implementation details are given in Appendix D.4. Table 2 presents the results. TS-LDDMM-SVC consistently outperforms the other unsupervised methods. It is ranked 1,3,4,3 for all methods combined, demonstrating its competitiveness as an unsupervised method on time series dataset homogeneous regarding shape.

## 7 Conclusion

In this paper, we propose a feature representation method, TS-LDDMM, designed for shape comparison in homogeneous time series datasets. We show on a real dataset its ability to study, with high interpretability, the inter-individual shape variability. As an unsupervised approach, it is user-friendly and enables knowledge transfer for different supervised tasks such as classification. Although TS-LDDMM is already competitive for classification, its performances can be leveraged on more heterogeneous datasets using a hierarchical clustering extension, which is relegated for future work.

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## A Proofs

Denote by  $G(s) \triangleq \{(t, s(t)) : t \in I\}$  the graph of a time series  $s : I \rightarrow \mathbb{R}^d$  and  $\phi.G(s) \triangleq \{\phi(t, s(t)) : t \in I\}$  the action of  $\phi \in \mathcal{D}(\mathbb{R}^{d+1})$  on  $G(s)$ .

**Theorem 4.** Let  $s : J \rightarrow \mathbb{R}^d$  and  $s_0 : I \rightarrow \mathbb{R}^d$  be two continuously differentiable time series with  $I, J$  two intervals of  $\mathbb{R}$ . There exist  $f \in C^1(\mathbb{R}^{d+1}, \mathbb{R}^d)$  and  $\gamma \in \mathcal{D}(\mathbb{R})$  such that  $\gamma(I) = J$  and  $\Phi_f \in \mathcal{D}(\mathbb{R}^{d+1})$ ,

$$G(s) = \Pi_{\gamma, f}.G(s_0), \quad \Pi_{\gamma, f} = \Psi_\gamma \circ \Phi_f.$$

Moreover, for any  $\bar{f} \in C^1(\mathbb{R}^{d+1}, \mathbb{R}^d)$  and  $\bar{\gamma} \in \mathcal{D}(\mathbb{R})$ , there exists a continuously differentiable time series  $\bar{s}$  such that  $G(\bar{s}) = \Pi_{\bar{\gamma}, \bar{f}}.G(s_0)$

*Proof.* Let  $s : J \rightarrow \mathbb{R}^d$  and  $s_0 : I \rightarrow \mathbb{R}^d$  be two continuously differentiable time series with  $I = (a, b)$ ,  $J = (\alpha, \beta)$  two intervals of  $\mathbb{R}$ . By setting  $\gamma : t \in \mathbb{R} \mapsto (\beta - \alpha)(t - a)/(b - a) + \alpha \in \mathbb{R}$ , we have  $\gamma(I) = J$  and  $\gamma \in \mathcal{D}(\mathbb{R})$ . By defining  $f : (t, x) \in \mathbb{R}^{d+1} \mapsto x - s_0(t) + s \circ \gamma(t)$ , the map  $\Phi_f \in \mathcal{D}(\mathbb{R}^{d+1})$ , indeed, its inverse is  $\Phi_f^{-1} : (t, x) \in \mathbb{R}^{d+1} \mapsto (t, x + s_0(t) - s(t))$  and is continuously differentiable. Moreover, we have  $\Pi_{\gamma, f}.G(s_0) = \{(\gamma(t), s \circ \gamma(t)) : t \in I\} = G(s)$ .

Let  $\bar{f} \in C^0(\mathbb{R}^{d+1}, \mathbb{R}^d)$ ,  $\bar{\gamma} \in \mathcal{D}(\mathbb{R})$  and  $s_0 \in C^0(I, \mathbb{R}^d)$  with  $I$  an interval of  $\mathbb{R}$ . We have :

$$\begin{aligned} \Pi_{\gamma, f}.G(s_0) &= \{(\gamma(t), f(t, s_0(t))), t \in I\} \\ &= \{(t, f(\gamma^{-1}(t), s_0(\gamma^{-1}(t))), t \in \gamma(I)\}. \end{aligned} \quad (10)$$

By defining  $\bar{s} : t \in \gamma(I) \rightarrow f(\gamma^{-1}(t), s_0(\gamma^{-1}(t)))$ , we have  $\bar{s} \in C^0(\gamma(I), \mathbb{R}^d)$  by composition of continuous functions and  $G(\bar{s}) = \Pi_{\gamma, f}.G(s_0)$  by (10), which concludes the proof.  $\square$

**Lemma 2.** *If we denote by  $V$  the RKHS associated with the kernel  $K_G$ , then for any vector field  $v$  generated by (5) with  $v_0$  satisfying (4), there exist  $\gamma \in D(\mathbb{R})$  and  $f \in C^1(\mathbb{R}^{d+1}, \mathbb{R}^d)$  such that  $\phi^v = \Psi_\gamma \circ \Phi_f$ .*

*Proof.* Let  $v$  be a vector field generated by (5) with  $v_0$  satisfying (4). We remark that the first coordinate of the velocity field  $v_\tau$  denoted by  $v_\tau^{\text{time}}$  only depends on the time variable  $t$  for any  $\tau \in [0, 1]$ . Thus, when computing the first coordinate of the deformation  $\phi^v$ , denoted by  $\gamma$ , we integrate (1) with  $v_\tau$  replaced by  $v_\tau^{\text{time}}$ , thus  $\gamma$  is independant of the variable  $x$ . Moreover,  $\gamma \in D(\mathbb{R})$  since a Gaussian kernel induced an Hilbert space  $V$  satisfying  $|f|_V \leq |f|_\infty + \|df\|_\infty$  for any  $f \in V$  by [18, Theorem 9]. For the same reason, we have  $\phi^v \in D(\mathbb{R}^{d+1})$ , and thus its last coordinates denoted by  $f$  belongs to  $C^1(\mathbb{R}^{d+1}, \mathbb{R}^d)$ , and by construction  $\phi^v = \Psi_\gamma \circ \Phi_f$ .  $\square$

## B Oriented varifold

In this section, we introduce the *oriented varifold* associated with curves. For further readings on curves and surfaces representation as varifolds, readers can refer to [26, 8]. We associate to  $\gamma \in C^1((a, b), \mathbb{R}^{d+1})$  an *oriented varifold*  $\mu_\gamma$ , i.e. a distribution on the space  $\mathbb{R}^{d+1} \times \mathbb{S}^d$  defined as follows, for any smooth test function  $\omega : \mathbb{R}^{d+1} \times \mathbb{S}^d \rightarrow \mathbb{R}$ ,

$$\mathbb{E}_{Y \sim \mu_\gamma} [\omega(Y)] = \mu_\gamma(\omega) = \int_a^b \omega\left(\gamma(t), \frac{\dot{\gamma}(t)}{|\dot{\gamma}(t)|}\right) |\dot{\gamma}(t)| dt.$$

Denoting by  $W$  the space of smooth test function, we have that  $\mu_\gamma$  belongs to its dual  $W^*$ . Thus, a distance on  $W^*$  is sufficient to set a distance on oriented varifolds associated to curve and thus on  $C^1((a, b), \mathbb{R}^{d+1})$  by the identification  $\gamma \rightarrow \mu_\gamma$ . Remark that in (TS-LDDMM),  $\gamma$  should be the parametrization of a time series' graph  $G(s)$ , i.e.  $\gamma : t \in I \rightarrow (t, s(t)) \in \mathbb{R}^{d+1}$  denoting by  $s : I \rightarrow \mathbb{R}^d$  the time series. However, in practice, we work with discrete objects. That is why, we set  $W$  as an RKHS to use its representation theorem. More specifically [26, Proposition 2 & 4] encourages us to consider a kernel  $k : (\mathbb{R}^{d+1} \times \mathbb{S}^d)^2 \rightarrow \mathbb{R}$  such that there exist two positive and continuously differentiable kernels  $k_{\text{pos}}$  and  $k_{\text{dir}}$ , such that for any  $(x, \vec{u}), (y, \vec{v}) \in (\mathbb{R}^{d+1} \times \mathbb{S}^d)^2$

$$k((x, \vec{u}), (y, \vec{v})) = k_{\text{pos}}(x, y) k_{\text{dir}}(\vec{u}, \vec{v}),$$

with moreover  $k_{\text{dir}} > 0$  and  $k_{\text{pos}}$  which admits an RKHS  $W_{\text{pos}}$  dense in the space of continuous function on  $\mathbb{R}^{d+1}$  vanishing at infinite [7].

Given such a kernel  $k : (\mathbb{R}^{d+1} \times \mathbb{S}^d)^2 \rightarrow \mathbb{R}$  verifying [26, Proposition 2 & 4], we have that for any  $(x, v) \in \mathbb{R}^{d+1} \times \mathbb{S}^d$ ,  $\delta_{(x, \vec{v})}$  belongs to  $W^*$  as a distribution and that the dual metric  $\langle \cdot, \cdot \rangle_{W^*}$  satisfies for any  $(x_1, v_1), (x_2, v_2) \in (\mathbb{R}^{d+1} \times \mathbb{S}^d)^2$ ,

$$\langle \delta_{(x_1, \vec{v}_1)}, \delta_{(x_2, \vec{v}_2)} \rangle_{W^*} = k((x_1, \vec{v}_1), (x_2, \vec{v}_2)).$$

Thus, given two sets of triplets  $X = (l_i, x_i, \vec{v}_i)_{i \in [T_0-1]} \in (\mathbb{R} \times \mathbb{R}^{d+1} \times \mathbb{S}^d)^{T_0-1}$ ,  $Y = (l'_i, y_i, \vec{w}_i)_{i \in [T_1]} \in (\mathbb{R} \times \mathbb{R}^{d+1} \times \mathbb{S}^d)^{T_1-1}$  and denoting by

$$\mu_X = \sum_{i=1}^{T_0} l_i \delta_{(x_i, \vec{v}_i)}, \mu_Y = \sum_{i=1}^{T_1} l'_i \delta_{(y_i, \vec{w}_i)}, \quad (11)$$

we have,

$$|\mu_X - \mu_Y|_{W^*}^2 = \sum_{i,j=1}^{T_0-1} l_i k((x_i, \vec{v}_i), (x_j, \vec{v}_j)) l_j - 2 \sum_{i=1}^{T_0-1} \sum_{j=1}^{T_1-1} l_i k((x_i, \vec{v}_i), (y_j, \vec{w}_j)) l'_j + \sum_{i,j=1}^{T_1-1} l'_i k((y_i, \vec{w}_i), (y_j, \vec{w}_j)) l'_j.$$

Then, using the identification  $X \rightarrow \mu_X, Y \rightarrow \mu_Y$ , we can define a distance on sets of triplets as  $d_{W^*,3}(X, Y) = |\mu_X - \mu_Y|_{W^*}^2$ .

Now, we aim to discretize the oriented varifold  $\mu_G$  related to a time series' graph  $G(s)$  by using a set of triplets. This is carried out by using a discretized version of  $G(s)$ , i.e.  $\tilde{G} = (g_i = (t_i, s(t_i)))_{i \in [T]} \in (\mathbb{R}^{d+1})^T$ , in the following way: For any  $i \in [T-1]$ , denoting the center and length of the  $i^{th}$  segment  $[g_i, g_{i+1}]$  by  $c_i = (g_i + g_{i+1})/2$ ,  $l_i = \|g_{i+1} - g_i\|$ , and the unit norm vector of direction  $\overrightarrow{g_i g_{i+1}}$  by  $\vec{v}_i = (g_{i+1} - g_i)/l_i$ , we define the set of triplets  $X(\tilde{G}) = (l_i, c_i, \vec{v}_i)_{i \in [T-1]}$  and its related oriented varifold  $\mu_{X(\tilde{G})} = \sum_{i=1}^{T-1} l_i \delta_{c_i, \vec{v}_i}$  as in (11). This is a valid discretization of the oriented varifold  $\mu_G$  according to [26, Proposition 1]:  $\mu_{X(\tilde{G})}$  converges towards  $\mu_G$  as the size of the discretization mesh  $\sup_{i \in [T-1]} |t_{i+1} - t_i|$  converges to 0.

Finally, we define a distance on discretized time series' graphs  $\tilde{G}_1, \tilde{G}_2$  as  $d_{W^*}(\tilde{G}_1, \tilde{G}_2) = d_{W^*,3}(X(\tilde{G}_1), X(\tilde{G}_2))$ .

## B.1 Varifold kernels

Denote the one-dimensional Gaussian kernel by  $K_\sigma^{(a)}(x, y) = \exp(-|x - y|^2/\sigma)$  for any  $(x, y) \in (\mathbb{R}^a)^2$ ,  $a \in \mathbb{N}$  and  $\sigma > 0$ . In the implementation, we use the following kernels, for any  $((t_1, x_1), (t_2, x_2)) \in (\mathbb{R}^{d+1})^2, ((w_1, v_1), (w_2, v_2)) \in (\mathbb{S}^d)^2$ ,

$$k_{\text{pos}}(x, y) = K_{\sigma_{\text{pos},t}}^{(1)}(t_1, t_2) K_{\sigma_{\text{pos},x}}^{(d)}(x_1, x_2), \quad k_{\text{pos}}(x, y) = K_{\sigma_{\text{dir},t}}^{(1)}(w_1, w_2) K_{\sigma_{\text{dir},x}}^{(d)}(v_1, v_2),$$

where  $\sigma_{\text{pos},t}, \sigma_{\text{pos},x}, \sigma_{\text{dir},t}, \sigma_{\text{dir},x} > 0$  are hyperparameters. In practice, we select  $\sigma_{\text{pos},x} \approx \sigma_{\text{dir},x} \approx 1$  when the time series are centered and normalized. Otherwise we select  $\sigma_{\text{pos},x} \approx \sigma_{\text{dir},x} \approx \bar{\sigma}_s$  with  $\bar{\sigma}_s$  the average standard deviation of the time series. We choose  $\sigma_{\text{pos},t} \approx \sigma_{\text{dir},t} = m f_e$  with  $f_e$  the sampling frequency of the time series and  $m \in [5]$  an integer depending on the time change between the starting and the target time series graph. The more significant the time change, the higher  $m$  should be. The intuition comes from the fact that the width  $\sigma_{\text{pos},t}, \sigma_{\text{dir},t}$  rules the time windows used to perform the comparison, and  $\sigma_{\text{pos},x}, \sigma_{\text{dir},x}$  affects the space window. The size of the windows should be selected depending on the variations in the data.

## C Tuning the hyperparameters of the TS-LDDMM kernel given in (9)

The parameter  $\sigma_{T,0}$  should be chosen *large* compared the sampling frequency  $f_e$  and compared to average standard deviation  $\bar{\sigma}_s$  of the time series, e.g  $\sigma_{T,0} = 100$  as  $\bar{\sigma}_s \approx f_e \approx 1$ . It makes the time transformation smoother. If  $\sigma_{T,0}$  is too small, for instance,  $\sigma_{T,0} = f_e$ , the effect of the time deformation is too localized, and there are not enough samples to make it visible.

The parameter  $\sigma_{T,1}$  should be of the same order as  $f_e$ : two different points in time can have various space transformations.  $\sigma_x$  should be of the same order of  $\bar{\sigma}_s$ : two points with a big difference regarding space compared to  $\bar{\sigma}_s$  can have very different space transformations.

We take  $c_0 \approx 10c_1$ , we want to encourage time transformation before space transformation. We take  $(c_0, c_1) = (1, 0.1)$  in all experiments.

## D Numerical details

A report of all the hyperparameters selected is given in Table 3.

### D.1 Optimization details of (8)

**Initialization** At the initialization of (8), all the momentums parameter are set to 0 and the graph of reference is set to the graph of a time series in the dataset having a median samples size.

**Gradient descent.** The chosen gradient descent method is "adabelief" [50] implemented in the library OPTAX<sup>4</sup>. There are two main parameters in the gradient descent: the number of steps `nb_steps`, and the maximum value of step size  $\eta_M$ . The stepsize has a particular scheduling:

<sup>4</sup><https://optax.readthedocs.io/en/latest/>

578 • Warmup period on  $0.1 \times \text{nb\_steps}$  steps: the stepsize increases linearly from 0 to  $\eta_M$ . The  
579 goal is to learn progressively the parameters. If the stepsize is too large at the start, smaller  
580 steps at the end can't make up for the mistakes made at the beginning.

581 • Fine tuning periode on  $0.9 \times \text{nb\_steps}$  : the stepsize decreases from  $\eta_M$  to 0 with a cosine  
582 decay implemented in the OPTAX scheduler, i.e. the decreasing factor as the form  $0.5(1 +$   
583  $\cos(\pi t/T))$ .

584 The sharper the deformations, the larger the number of steps and the maximum value of step size  
585 should be selected. We suggest  $\text{nb\_steps}=300$ ,  $\eta_M = 0.1$  for small deformations and  $\text{nb\_steps}=800$ ,  
586  $\eta_M = 0.3$  for big ones (time dilation with a factor  $\lambda \geq 2$ ).

## 587 D.2 Synthetic experiments

588 For any deformations generation in both experiments (well-specified and misspecified), we take  
589  $\sigma_{T,0}, \sigma_{T,1}, \sigma_x = (100, 1, 1)$  and  $c_0, c_1 = (1, 0.1)$  for the kernel  $K_G$  and  $\sigma_{\text{pos},t}, \sigma_{\text{pos},t}, \sigma_{\text{dir},t}, \sigma_{\text{dir},x} =$   
590  $(2, 1, 2, 0.6)$  for the varifold kernels  $k_{\text{pos}}, k_{\text{dir}}$  related to the loss  $\mathcal{L}$ .

591 In both experiments, we have  $\text{nb\_steps}=300$  and  $\eta_M = 0.1$ .

## 592 D.3 Mouse experiments

593 The number of steps is larger in the second experiment (before/after injection) because the deforma-  
594 tions are sharper.

## 595 D.4 Classification experiments

596 We defined a default parametrization for all classifiers.

597 For classifiers: CNN, ResNet, Catch22, DTW-KNN, Rocket we used the aeon<sup>5</sup> implementations with  
598 their default settings.

599 For Tloss-SVC we used the implementation provided on github<sup>6</sup> with the following parameters for  
600 learning representations: batch\_size: 10, channels: 40, depth: 10, nb\_steps: 200, in\_channels: 1, ker-  
601 nel\_size: 3, lr: 0.001, nb\_random\_samples: 10, negative\_penalty: 1, out\_channels: 320, reduced\_size:  
602 160. We used the Support Vector Classifier (SVC) from scikit-learn with the regularization term C:  
603 1. Others parameters are set to default.

604 For TS-LDDMMM-SVC, all kernels' parameters et optimizer parameter are presented in Table 3.  
605 As well, we used the Support Vector Classifier from scikit-learn with the regularization term C: 1.  
606 Others parameters are set to default.

Table 3: Parameters used in all the experiments. For synthetic data,  $K_G$  refers to the kernel used in the generation, which is the same for the estimation only in the well-specified case.  $\bar{l}$  refers to the average time series length and  $N_d$  refers to the number of dimensions.

objects	Optimizer	$k_{\text{pos}}, k_{\text{dir}}$	$K_G$
Parameter	$(\text{nb\_steps}, \eta_M)$	$(\sigma_{\text{pos},t}, \sigma_{\text{pos},t}, \sigma_{\text{dir},t}, \sigma_{\text{dir},x})$	$(c_0, c_1, \sigma_{T,0}, \sigma_{T,1}, \sigma_x)$
Synthetic data well-specified	(300,0.1)	(2, 1, 2, 0.6)	(1, 0.1, 100, 1, 1)
Synthetic data misspecified	(300,0.1)	(2, 1, 2, 0.6)	(1, 0.1, 100, 1, 1)
Mouse before injection	(400,0.3)	(2, 1, 2, 0.6)	(1, 0.1, 100, 1, 1)
Mouse before/after injection	(800,0.3)	(5, 1, 5, 0.6)	(1, 0.1, 150, 1, 1)
classification	(400,0.1)	$(\max(2, 0.03\bar{l}), N_d, \max(2, 0.03\bar{l}), 0.6)$	$(1, 0.1, 0.33\bar{l}, 1, N_d)$



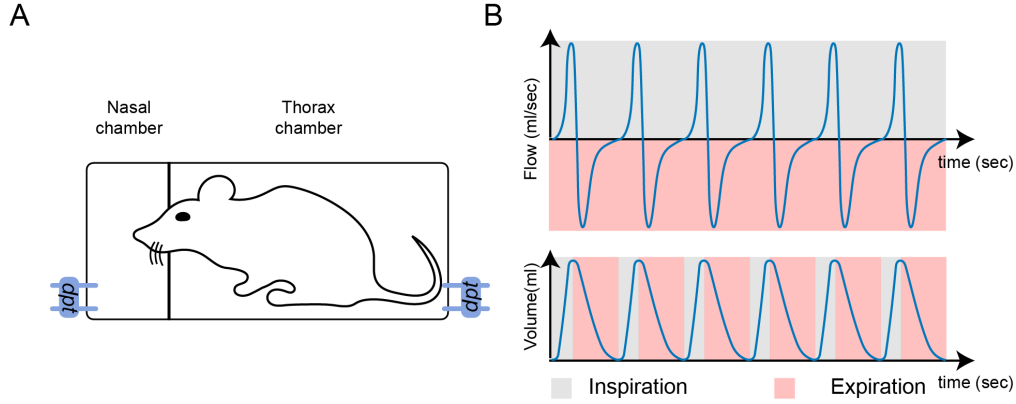


Figure 6: A: Illustration of a double-chamber plethysmograph. The term *dpt* stands for differential pressure transducer which measures the pressure in each compartment, the pressure then being converted to flow. B: Nasal airflow (top) and lung volume (bottom). During inspiration, airflow is positive (grey) and during expiration, airflow is negative (pink).

## E Mouse respiratory dataset

Ventilation is a simple physiological function that ensures a vital supply of oxygen and the elimination of CO<sub>2</sub>. Acetylcholine (ACh) is a neurotransmitter that plays an important role in muscular activity, notably for breathing. Indeed, muscle contraction information passes from the brain to the muscle through the nervous system. AChs are located in synapses of the nervous system (central and peripheral) and skeletal muscles. They ensure the information transmission from nerve to nerve. However, the transmission cannot end without the hydrolysis of ACh by the enzyme Acetylcholinesterase (AChE), allowing nerves to return to their resting state. Inhibition of (AChE) with, for instance, nerve gas, pesticide, or drug intoxication leads to respiratory arrests.

The dataset comes from the experiment [34], where they studied the consequences of partial deficits in AChE and AChE inhibition on mice respiration. AChE inhibition was induced with an irritant molecule called physostigmine (an AChE inhibitor). Mice nasal airflows were sampled at 2000Hz with a Double Chamber plethysmograph [23], as depicted in Figure 6-A). The flow is expressed in  $ml.s^{-1}$ ; it has a positive value during inspiration and a negative value expiration Figure 6-B). Among the mice population, we selected 7 control mice (**wt**) and 7 ColQ mice (**colq**), which do not have AChE anchoring in muscles and some tissues. As described in [34], mice experiments were as follows:

1. The mouse is placed in a DCP for 15 or 20 min to serve as an internal control.
2. The mouse is removed from the DCP and injected with physostigmine.
3. The mouse is placed back into the DCP, and its nasal flow is recorded for 35 or 40 min.

Respiratory cycles were extracted following procedure [17]. We removed respiratory cycles whose duration exceeds 1 second; the average respiratory cycle duration is 300 ms. We randomly sampled 10 respiratory cycles per minute and mouse. It leads to a dataset of 12,732 (time, genotype)-annotated respiratory cycles.

## F Classification datasets

All datasets were taken from UCR/UEA archives [10, 2]. Among all available datasets<sup>7</sup>, we selected 4 datasets related to time series shape comparison. All datasets were downloaded with the python

<sup>5</sup><https://www.aeon-toolkit.org/en/stable/index.html>

<sup>6</sup><https://github.com/mqwfrog/ULTS>

<sup>7</sup><https://timeseriesclassification.com>

package `aeon`<sup>8</sup> which already includes the train test split. Essential dataset information is summarized in Table 4.

Table 4: Time series datasets summary for shape based classification.

Dataset	Train size	test size	Length	Number of classes	Number of dimensions	Type
ArrowHead	36	175	251	3	1	IMAGE
ECG200	100	100	96	2	1	ECG
GunPoint	50	150	150	2	1	MOTION
NATOPS	180	180	51	6	24	MOTION

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<sup>8</sup><https://www.aeon-toolkit.org/en/stable/>

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