

SPIKY: A graphical user interface for monitoring spike train synchrony

Nebojsa Bozanic, Thomas Kreuz

Institute for complex systems, CNR, Sesto Fiorentino, Italy

Abstract

Recently, the SPIKE-distance has been proposed as a measure of spike train synchrony which is both parameter-free and time-scale independent. Since it relies on instantaneous estimates of spike train dissimilarity, it is also time-resolved which makes it possible to track changes in instantaneous clustering, i.e., time-localized patterns of (dis)similarity among multiple spike trains. Further features include selective and triggered temporal averaging as well as the instantaneous comparison of spike train groups. Besides the regular SPIKE-distance, there also exists a causal variant which is defined such that the instantaneous values of dissimilarity rely on past information only so that time-resolved spike train synchrony can be estimated in real-time. Finally, here we introduce the future SPIKE-distance which can be used in triggered temporal averaging in order to evaluate the effect of certain spikes or of certain stimuli features on future spiking. In the first part of this report we address some of the computational aspects in the calculation and implementation of the SPIKE-distance while in the second part we present SPIKY, a graphical user interface which facilitates the application of the SPIKE-distance and all its variants to both simulated and real data.

1. Introduction

A wide variety of approaches to quantify the dissimilarity, or distance, between two spike trains has been suggested. Among these is the metric introduced in ?, which evaluates the cost needed to transform one spike train into the other, using only certain elementary steps. Another metric proposed in ?, measures the Euclidean distance between the two spike trains after convolution of the spikes with an exponential function. Both methods involve one parameter that sets the time scale. In contrast, two more recent bivariate approaches, the ISI- and the SPIKE-distance are time scale independent and self-adaptive (??). These two measures are complementary: The ISI-distance relies on the relative length of simultaneous interspike intervals and is thus well-designed to quantify similarities in the neurons firing-rate profiles (??). The SPIKE-distance is based on differences between the spike times of the two spike trains and is therefore ideally suited to track synchrony that is mediated by spike timing (??).

XXXXX Computational aspects XXXXX

2. Measures

2.1. The SPIKE-distance

The SPIKE-distance (see ? for the original proposal and ? for the definite version presented here) is extracted from differences between the spike times of the two spike trains. It relies on instantaneous values in the sense that in a first step the two sequences of discrete spike times are transformed into a continuous dissimilarity profiles $S(t)$. This dissimilarity profile is based on three piecewise constant quantities which for each neuron $n = 1, 2$ are assigned to every time instant between 0 and T (see Fig. 1). These are the time of the preceding spike

$$t_P^n(t) = \max(t_i^n | t_i^n \leq t) \quad t_1^n \leq t \leq t_{M_n}^n, \quad (1)$$

the time of the following spike

$$t_F^n(t) = \min(t_i^n | t_i^n > t) \quad t_1^n \leq t \leq t_{M_n}^n, \quad (2)$$

as well as the interspike interval

$$x_{\text{ISI}}^n(t) = t_F^n(t) - t_P^n(t). \quad (3)$$

The ambiguity regarding the definition of the very first and the very last interspike interval is resolved by placing for each spike train auxiliary leading spikes at time $t = 0$ and auxiliary trailing spikes at time $t = T$. From these three quantities the dissimilarity profile is calculated in two steps: First for each spike the distance to the nearest spike in the other spike train is calculated, then for each time instant the

Email addresses: strance@gmail.com (Nebojsa Bozanic), thomas.kreuz@cnr.it (Thomas Kreuz).

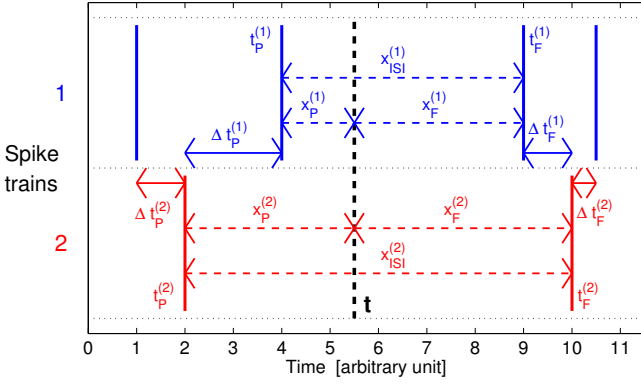


Fig. 1. SPIKE-distance. Illustration of the local quantities needed to define the dissimilarity profile $S(t)$ for an arbitrary time instant t .

relevant spike time differences are selected, weighted, and normalized. Here ‘relevant’ means local; each time instant is uniquely surrounded by four corner spikes: the preceding spike from the first spike train $t_P^{(1)}$, the following spike from the first spike train $t_F^{(1)}$, the preceding spike from the second spike train $t_P^{(2)}$, and, finally, the following spike from the second spike train $t_F^{(2)}$. Each of these corner spikes can be identified with a spike time difference, for example, for the previous spike of the first spike train

$$\Delta t_P^{(1)} = \min_i (|t_P^{(1)} - t_i^{(2)}|) \quad (4)$$

and analogously for $t_F^{(1)}$, $t_P^{(2)}$, and $t_F^{(2)}$ (see Fig. 1). For each spike train separately a locally weighted average is employed such that the differences for the closer spike dominate; the weighting factors depend on

$$x_P^{(n)}(t) = t - t_P^{(n)}(t) \quad (5)$$

and

$$x_F^{(n)}(t) = t_F^{(n)}(t) - t, \quad (6)$$

the intervals to the previous and the following spikes for each neuron $n = 1, 2$. The local weighting for the spike time differences of the first spike train reads

$$S_1(t) = \frac{\Delta t_P^{(1)} x_F^{(1)} + \Delta t_F^{(1)} x_P^{(1)}}{x_{\text{ISI}}^{(1)}} \quad (7)$$

and analogously $S_2(t)$ is obtained for the second spike train. Averaging over the two spike train contributions and normalizing by the mean interspike interval yields

$$S''(t) = \frac{S_1(t) + S_2(t)}{2\langle x_{\text{ISI}}^{(n)} \rangle_n}. \quad (8)$$

This quantity weights the spike time differences for each spike train according to the relative distance of the corner spike from the time instant under investigation. This way relative distances within each spike train are taken care of, while relative distances between spike trains are not. In order to get these ratios straight and to account for differences in firing rate, in a last step the two contributions from the two spike trains are locally weighted by their instan-

taneous interspike intervals. This leads to the definition of the dissimilarity profile

$$S(t) = \frac{S_1(t)x_{\text{ISI}}^{(2)} + S_2(t)x_{\text{ISI}}^{(1)}}{2\langle x_{\text{ISI}}^{(n)} \rangle_n^2}. \quad (9)$$

The SPIKE-distance is defined as the temporal average of this dissimilarity profile

$$D_S = \frac{1}{T} \int_0^T dt S(t). \quad (10)$$

The dissimilarity profile $S(t)$ and the SPIKE-distance D_S as its average are bounded in the interval $[0, 1]$. The distance value $D_S = 0$ is obtained for identical spike trains only. Since the dissimilarity profile is obtained from a linear interpolation of three piecewise constant quantities it is piecewise linear.

There exists a straightforward extension to the case of more than two spike trains (number of spike trains $N > 2$), the averaged bivariate distance. This average over all pairs of neurons commutes with the average over time, so it is possible to achieve the same kind of time-resolved visualization as in the bivariate case by first calculating the instantaneous average, e.g., $S^a(t)$ over all pairwise instantaneous values $S^{mn}(t)$,

$$S^a(t) = \frac{1}{N(N-1)/2} \sum_{n=1}^{N-1} \sum_{m=n+1}^N S^{mn}(t) \quad (11)$$

2.1.1. Edge effect

In previous versions of the SPIKE-distance the ambiguity regarding the definition of the initial (final) distance to the preceding (following) spike as well as the very first and the very last interspike intervals was resolved by adding to each spike train an auxiliary leading spike at time $t = 0$ and an auxiliary trailing spike at time $t = T$. This led to spurious synchrony at the edges where by construction the dissimilarity profile reached the zero value. Here we follow a suggestion by Conor Houghton (personal communication) and at least partly correct this edge effect. We describe the correction for the beginning of the recording, it is an analogous mirror image at the end of the recording.

We count the auxiliary spikes as normal spikes which can be nearest neighbor to other spikes. But instead of calculating their spike time distance (which is always zero) we use the spike time difference of the first real spike. For the first interspike interval we know that it is at least the distance to the first spike $t_1 - t_0 = t_1$ but it could be longer. So to take the local firing rate (or its inverse) into consideration we set

$$x_{\text{ISI}}(0) = \max(t_1, t_2 - t_1). \quad (12)$$

where we use the length of the first known interspike interval $t_2 - t_1$ as an upper limit of the inverse firing rate. This way we get at least a crude estimate of how much longer the first interspike interval could be.

2.2. Sampling

Earlier versions of the codes for calculating the ISI- and the SPIKE-distance relied on sampled dissimilarity profiles. Typically the precision was set to the sampling interval of the neuronal recording. Since the dissimilarity profile has to be calculated and stored for each pair of spike trains, this resulted, for each measure, in a matrix of order 'number of sampled time instants s ' 'squared number of spike trains' (i.e., $\#(t_s)N^2$). For small sampling intervals and a large number of recorded spike trains this lead to memory problems. In SPIKY we use an optimized and more memory-efficient way of storing the data where we make use of the fact that the ISI-distance is piecewise constant and the SPIKE-distance is piecewise linear. For each interval in the pooled spike train (and each pair of spike trains) we have to store only one value for the ISI-distance and two values for the SPIKE-distance, one at the beginning and one at the end of the interval. For both dissimilarity profiles there are instantaneous jumps at the times of the spikes since this is where the lengths of the interspike intervals and the identity of the previous and the following spikes change abruptly. In contrast to the calculation based on sampling we get the exact result since each spike is both the previous and the next spike and there is no need anymore to cut the corners of the dissimilarity profiles.

2.3. Realtime SPIKE-distance

The realtime SPIKE-distance D_{S_r} is a modification of the SPIKE-distance with the key difference that the corresponding time profile $S_r(t)$ can be calculated online because it relies on past information only. From the perspective of an online measure, the information provided by the following spikes, both their position and the length of the interspike interval, is not yet available. Like the regular (improved) SPIKE-distance D_S , this causal variant is also based on local spike time differences but now only two corner spikes are available, and the spikes of comparison are restricted to past spikes, e.g., for the preceding spike of the first spike train

$$\Delta t_P^{(1)} = \min_i (|t_P^{(1)} - t_i^{(2)}|), t_i < t. \quad (13)$$

Since there are no following spikes available, there is no local weighting, and since there is no interspike interval, the normalization is achieved by dividing the average corner spike difference by twice the average time interval to the preceding spikes (Eq. 5). This yields a causal indicator of local spike train dissimilarity:

$$S_r(t) = \frac{\Delta t_P^{(1)} + \Delta t_P^{(2)}}{4\langle x_F^{(n)} \rangle_n}. \quad (14)$$

2.4. Future SPIKE-distance

The future SPIKE-distance D_{S_f} can be used in triggered temporal averaging in order to evaluate the effect of certain spikes or of certain stimuli features on future spiking. It is the inverse measure to the realtime SPIKE-distance but instead of relying on past information only it relies on future information only. Again for each time instant there are just two corner spikes and the potential nearest spikes in the other spike train are future spikes only. Thus the spike time difference for the following spike of the first spike train reads

$$\Delta t_F^{(1)} = \min_i (|t_F^{(1)} - t_i^{(2)}|), t_i > t, \quad (15)$$

and accordingly for the following spike of the second spike train. In analogy to Eq. 14, an indicator of local spike train dissimilarity is obtained as follows:

$$S_f(t) = \frac{\Delta t_F^{(1)} + \Delta t_F^{(2)}}{4\langle x_F^{(n)} \rangle_n}. \quad (16)$$

2.5. The ISI-distance

While the dissimilarity profile of the SPIKE-distance is extracted from differences between the spike times of the two spike trains, the dissimilarity profile of the ISI-distance (??) is calculated as the instantaneous ratio between the interspike intervals $x_{\text{ISI}}^{(1)}$ and $x_{\text{ISI}}^{(2)}$ (Eq. 3) according to:

$$I(t) = \begin{cases} x_{\text{ISI}}^{(1)}(t)/x_{\text{ISI}}^{(2)}(t) - 1 & \text{if } x_{\text{ISI}}^{(1)}(t) \leq x_{\text{ISI}}^{(2)}(t) \\ -(x_{\text{ISI}}^{(2)}(t)/x_{\text{ISI}}^{(1)}(t) - 1) & \text{otherwise.} \end{cases} \quad (17)$$

This ISI-ratio equals 0 for identical ISI in the two spike trains, and approaches -1 and 1 , respectively, if the first or the second spike train is much faster than the other. Since the ISI-values only change at the times of spikes, the dissimilarity profile is piecewise constant. For the ISI-distance the temporal averaging analogous to Eq. 10 is performed on the absolute value of the ISI-ratio, thus both kinds of deviations are treated equally. Since the ISI-distance relies on the instantaneous ISI-values and thus requires knowledge about the following spikes, no causal realtime extension is possible.

2.6. Representations

The ISI- and the SPIKE-distance combine a variety of properties that make them well suited for applications to real data. In particular, they are conceptually simple, computationally efficient, and easy to visualize in a time-resolved manner. By taking into account only the preceding and the following spike in each spike train, these distances rely on local information only. They are also time-scale-adaptive since the information used is not contained within a window of fixed size but rather within a time frame whose size depends on the local rate of each spike train.

Moreover, the sensitivity to spike timing and the instantaneous reliability achieved by the SPIKE-distance opens up many new possibilities in multi-neuron spike train analysis (?). These build upon the fact that there are several levels of information reduction.

2.6.1. Full matrix and cross sections

The starting point is the most detailed representation in which one instantaneous value is obtained for each pair of spike trains (see Eq. 9). For multineuron data, this results in a matrix of size 'number of sampled time instants s ' 'squared number of spike trains' (i.e., $\#(t_s)N^2$).

From this matrix, it is possible to extract any desired information. By selecting a pair of spike trains, one obtains the bivariate dissimilarity profile $S(t)$ for this pair of spike trains. Selecting a time instant t_s instead yields an instantaneous matrix of pairwise spike train dissimilarities $S_{mn}(t_s)$. This matrix can be used to divide the spike trains into instantaneous clusters, that is, groups of spike trains with low intra-group and high inter-group dissimilarity.

2.6.2. Spatial and temporal averaging

Another way to reduce the information of the dissimilarity matrix is averaging. There are two possibilities that commute: the spatial average over spike train pairs and the temporal average.

The local average over spike train pairs yields a dissimilarity profile for the whole population. Temporal averaging over certain (continuous or noncontinuous) intervals on the other hand leads to a bivariate distance matrix (in real data, these intervals could be chosen to correspond to different external conditions such as normal vs. pathological, asleep vs. awake, target vs. non-target stimulus, or presence/absence of a certain channel blocker). Finally, in both cases, application of the respective remaining average results in one distance value that describes the overall level of synchrony for a group of spike trains over a given time interval.

2.6.3. Triggered averaging

The fact that there are no limits to the temporal resolution allows further analyses such as internally or externally triggered temporal averaging. Here, the matrices are averaged over certain trigger time instants only. The idea is to check whether this triggered temporal average is significantly different from the global average since this would indicate that something peculiar is happening at these trigger instants. These trigger times can either be obtained from internal conditions (such as the spike times of a certain spike train) or from external influences (such as the occurrence of certain features in a stimulus). In real multi-neuron data, internal triggering might help to uncover the connectivity in neural networks or to detect converging or diverging patterns of firing propagation. External triggering might be helpful in addressing questions of neuronal coding, for example, it could be used to evaluate the influ-

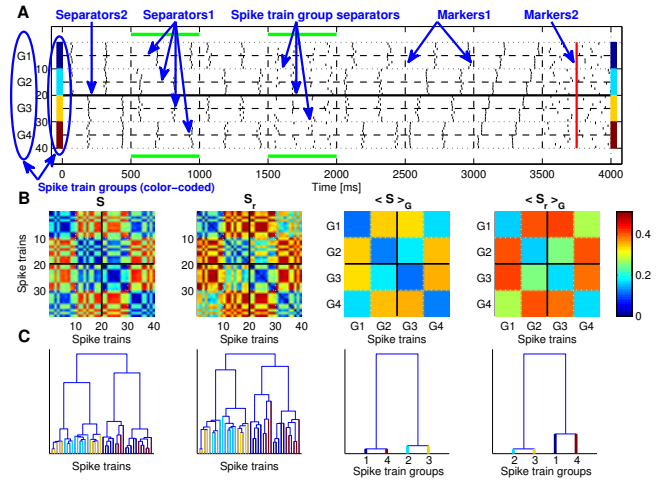


Fig. 2. Annotated screenshot from a movie. A. Artificially generated spike trains. B. Dissimilarity matrices obtained by averaging over two separate time intervals for both the regular and the real-time SPIKE-distance as well as their averages over subgroups of spike trains (denoted by $< >_G$). C. Corresponding dendrograms.

ence of localized stimulus features on the reliability of real neurons under repeated stimulation.

A last possibility is spatial averaging such that the spike trains are manually assigned to subgroups, and a block matrix (and the corresponding dendrogram) is obtained by averaging over the respective submatrices of the original dissimilarity matrix. In applications to real data, these groups could be different neuronal populations or responses to different stimuli, depending on whether the spike trains were recorded simultaneously or successively.

2.7. Spike train surrogates and significance

One important question that has not yet been addressed is the one of statistical significance.

Daniel's Email 13.07.2011:

Regarding the use of Poisson processes to have a benchmark it will have different implications depending on the structure of your data. If the rate is almost constant then comparing to processes with the same estimated average rate is the best option. If the rate is time-dependent you may want to compare with processes which are Poisson but mimic the same time-dependent profile of the rate. These are just alternatives that give you complementary information on the structure of the reliability.

Surrogate data with the same time dependent rate can be obtained by randomly reassigning each spike to any of the spike trains.

How can I estimate the significance of my results? Please have a look at the program 'Spiky_loop_surro.m'. This is similar to 'SPIKY_loop.m' only that you do not look at different datasets, rather you can compare the results obtained for one dataset against the results obtained for spike train surrogates generated from that dataset.

(???)

3. SPIKY

SPIKY is a graphical user interface (GUI) for monitoring synchrony between artificially simulated or experimentally recorded neuronal spike trains. It is based on two recently proposed methods to measure spike train (dis)similarity, the ISI- and the SPIKE-distance. SPIKY is a free software package programmed by Thomas Kreuz and Nebojsa Bozanic. All source codes are written in Matlab (Math-Works Inc, MA) with the most time-consuming loops coded in MEX-files. It is not stand-alone but requires Matlab to run.

3.1. Structure of SPIKY

First extract the zip-package (all files should be in one directory named SPIKY), then within Matlab go to this directory or add it to the path (addpath). Compile the MEX-files using 'SPIKY_compile_MEX', finally run SPIKY.

Typically the suggested element for the next user action is marked by a bold font. The most complete initial example is the entry 'Clustering' in the Data listbox. We suggest to follow this example through till the end advancing from panel to panel by pressing the highlighted button. With the same example in a second step you can start to change some parameters and see the consequences. Later, if you do not want to set all the parameters each time when you start SPIKY with a new dataset have a look at the file 'SPIKY_f_user_interface' and try to understand how for this example the spike train and the parameter values have been created. Hopefully you should then be able to do similar things with your own datasets. For quick information about the individual elements of the GUI activate the Hints-checkbox in the Options-Menu and then hover with the mouse cursor above the elements of interest and you will see short hints. An overview of all this information can be found in the file SPIKY-Elements.doc.

3.2. Input

There are three possibilities:

1. In the Selection: Data panel there is a listbox containing predefined examples. Initially these are the examples used in (?) but you can delete them and/or add your own data via the Matlab file 'SPIKY_f_user_interface'. Just make sure that the listbox entries defined in the variable listbox_str match the examples detailed below that.

2. You can load your own data via the Load button in the toolbar (left upper corner) or in the menu. Currently two different file formats are allowed, '.mat' and '.txt' (ASCII) files. For the mat-files SPIKY allows three different kinds of input formats: - cell arrays (ca) with just the spike times (this is the preferred format used by SPIKY since it is most memory efficient. The two other formats will internally be converted into this format) - regular matrices with each row being a spike train and zero padding (zp) in case the spike

numbers are different. - matrices representing time bins where each zero/one (01) indicates the absence/presence of a spike. If the spikes are stored in a Mat-file SPIKY looks for a variable called 'spikes', if it cannot find it you have the chance to select the variable name (or field name) which contains the spikes via some input mask which provides a hierarchical structure tree. In the text format spike times should be written as a matrix with each row being one spike train. The package contains one example file for each format ('testdata_ca.mat', 'testdata_zp.mat', 'testdata_01.mat' as well as 'testdata.txt').

3. You can generate your own spike trains via the Spike Train Generator. After setting some defining variables (number of spike trains, start and end time, sampling rate) you can build your spike trains by using predefined spike train patterns (such as periodic, Splay, uniform or Poisson) and/or by manually adding, shifting and deleting individual spikes or groups of spikes. For an overview of the general structure of the spike train generator please have a look at the file STG-flowchart.pdf, more detailed information can be found in the file STG-Elements.doc.

Input: Matrix 'spikes' with two or more spike trains (if trains have different numbers of spikes, fill with zeros) Parameter structure 'para' that describe the data (see below) tmin: Beginning of recording tmax: End of recording dts: Sampling interval, precision of spike times [!!! Please take care that this value is not larger than the actual sampling size, otherwise two spikes can occur at the same time instant and this can lead to problems in the algorithm !!!] select_measures: Vector with order of measures

3.3. Output

How can I extract the spike trains and the results of the analysis (measure profiles, matrices) to the workspace? By clicking (left mouse button) on the element whose data you wish to extract. Results will be stored in variables such as 'SPIKY_spikes', 'SPIKY_profile_X_1', 'SPIKY_profile_Y_1', 'SPIKY_profile_name_1' as well as 'SPIKY_matrix_1' and 'SPIKY_matrix_name_1'. In addition, the results obtained during an analysis will automatically be stored in the structure 'SPIKY_results' which will have one field for each measure selected.

How do I save/print figures? Press the Print to postscript button in the toolbar (left upper corner).

Output (Structure 'SPIKY_results'): SPIKY_results.jMeasure.j.name: Name of selected measures (helps to identify the order within all other variables) SPIKY_results.jMeasure.j.distance: Level of dissimilarity over all spike trains and the whole interval. This is just one value, obtained by averaging over both spike trains and time SPIKY_results.jMeasure.j.matrix: Pairwise distance matrices, obtained by averaging over time SPIKY_results.jMeasure.j.x: Time-values of overall dissimilarity profile SPIKY_results.jMeasure.j.y: Overall dissimilarity profile obtained by averaging over spike train pairs

Note: For the ISI-distance the function 'SPIKY_f_pico.m' can be used to obtain the average value as well as x- and y-vectors for plotting:

3.4. Figure-Layout

To change elements (fonts, lines, etc.) in the figure simply click the right mouse button on the element you wish to change. Please use the file 'SPIKY_f_user_interface' to set the standard values for all the parameters that describe the layout of the figure (mainly the parameter structure 'p_para').

How can I move subplots (spikes and profiles subplot, matrices) in the figure? How can I change their size?

Move the cursor to the respective axis (either just left or just below the subplot) and click the right mouse button. Now you can either edit all position variables by hand or change the x-position, the y-position, the width and the height individually. In case there are several matrices/dendrograms you can do this either for an individual matrix/dendrogram or for all of them at the same time.

3.5. GUI vs. loop

How can I get the statistics of a certain quantity over a large number of datasets?

For this purpose you can use the program SPIKY_loop which is complementary to the graphical user interface SPIKY'. Both programs can be used to calculate time-resolved spike train distances (ISI and SPIKE) between two (or more) spike trains. However, whereas SPIKY was mainly designed to facilitate the detailed analysis of one dataset, SPIKY_loop is meant to be used in order to compare the 'SPIKY_results' for many different datasets (e.g. in some kind of loop). Note that the new program 'SPIKY_loop' uses the full functionality of SPIKY (access to time instants, selective and triggered averages as well as averages over spike train groups).

3.6. Computational aspects

3.7. MEX-files

XXXXXX Rewrite and extend, add part on MEX-files
XXXXXX

The dissimilarity profile $S(t)$ of the SPIKE-distance is piecewise linear (with each linear interval running from one spike of the pooled spike train to the next) rather than piecewise constant as is the case for the ISI-distance. Therefore, when the localized visualization is desired, a new value has to be calculated for each sampling point and not just once per each interval in the pooled spike train. In cases where the distance value itself is sufficient, the short computation time can be even further decreased by representing each interval by the value of its center and weighting it

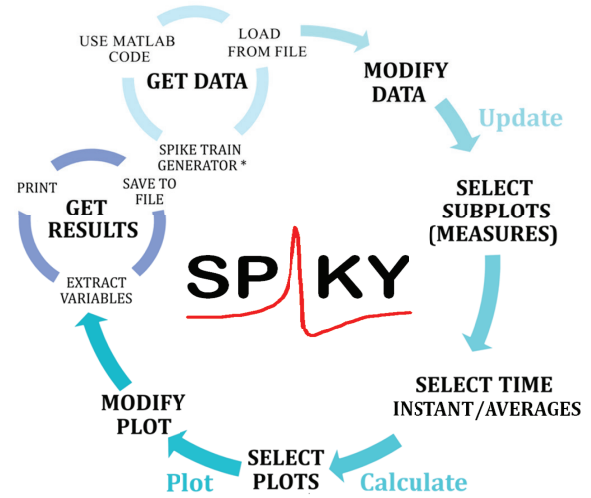


Fig. 3. SPIKY-Flowchart

by its length. This is not only faster, but it actually gives the exact result, whereas the time-resolved calculation is a very good approximation only for sufficiently small sampling intervals dt (imagine the example of a rectangular function, at some point any sampled representation has to cut the right angle). The dissimilarity profiles $S_r(t)$ and $S_f(t)$ of the real-time and the future SPIKE-distances are hyperbolic and not linear but here also the exact result can be obtained by piecewise integration over all intervals of the pooled spike train.

The calculation of the SPIKE-distance consists of three steps: In a precalculation step, for each spike the distance to the nearest spike in all the other spike trains is calculated. Successively, for each time instant and each pair of spike trains, the distances of the four corner spikes are first locally weighted and then normalized. These latter steps involve matrices of the order 'number of time instants' 'number of spike train pairs', which for very long datasets with many spike trains can lead to memory problems. The solution to these problems is to make the calculation sequential, i.e., to cut the recording interval into smaller segments, and to perform the averaging over all pairs of spike trains for each segment separately (no additional auxiliary spikes are needed except for very huge datasets for which even the calculation of the first matrix is too memory-demanding). In the end the dissimilarity profiles for the different segments (already averaged over pairs of spike trains) are concatenated, and its temporal average yields the distance value for the whole recording interval.

The computational load scales with the number of spike trains N as N^2 .

3.8. Comparison with other implementations

Python-Implementation of SPIKE-distance courtesy of Jeremy Fix:

<http://jeremy.fix.free.fr/Softwares/spike.html>

Python-Implementation of the pairwise ISI-distance courtesy of Michael Chary:

<https://pypi.python.org/pypi/ISIpy/1.0.1>

Răzvan Florian:

<https://github.com/modulus-metric/spike-train-metrics>

(?)

HRLAnalysisTM (?)

XXX Nebojsa figure (Performance comparison) XXX

We also thank Thomas Alderson, Black Square, Mayte Bonilla Quintana, Hamid Charkhkar, Didier Desaintjan, Mario DiPoppa, Mahboubah Etemadi, Marion Najac, Matthew Phillips, Eugenio Piasini, Robert Rein, Rodrigo Salazar, Michael Schaub, Eitan Schechtman, Matthew Williams, Yunguo Yu for advice and user feedback.

3.9. Access to SPIKY

SPIKY is distributed under a BSD licence (Copyright (c) 2014, Thomas Kreuz, Nebojsa Bozanic. All rights reserved.). A zip-package containing all the necessary files can be accessed for free on the download page (<http://www.fi.isc.cnr.it/users/thomas.kreuz/Source-Code/SPIKY.html>). This package also contains a folder with lots of documentation (such as a FAQ-file). Further information and some demonstrations (both images and movies) can be found on the download page and on the SPIKY Facebook-page (<https://www.facebook.com/SPIKYgui>). Both of these pages will be used to announce updates and distribute the latest information about new features. The Facebook-page also provides the user with an opportunity to provide feedback and ask questions. Finally, the movies can also be viewed on the SPIKY Youtube-channel (https://www.youtube.com/channel/UCgSz0YQ51WdVF0_Z1FNN0Bw).

4. Discussion

4.1. Summary

4.2. Limits

4.3. Outlook

Acknowledgements NB and TK acknowledge funding support from the European Commission through the Marie Curie Initial Training Network 'Neural Engineering Transformative Technologies (NETT)', project 289146. TK also acknowledges the Italian Ministry of Foreign Affairs regarding the activity of the Joint Italian-Israeli Laboratory on Neuroscience.

We thank Emily Caporello, Daniel Chicharro, Tim Genter, Conor Houghton, Jutta Kretzberg, Stefano Luccioli, Florian Mormann, Leon Paz, Friederice Pirschel, Alessandro Torcini, Jonathan Victor for useful discussions.