

# Unlocking Neural Transparency: Jacobian Maps for Explainable AI in Alzheimer's Detection

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Presenter: Thomas Tie Luo

#### Introduction

#### Alzheimer's Disease

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- AD is a leading cause of dementia with rising global burden
- Progresses from Mild Cognitive Impairment (MCI) to severe functional loss
- Early detection is key to intervention



## EARLY STAGE:

- Trouble remembering events
- Difficulty recalling names
- Frequently loses personal items



# MIDDLE STAGE:

- Worsening memory loss
- Confusion about names and relationships
- Difficulty with daily tasks



#### LATE STAGE:

- Difficulty recognizing family members
- Wheelchair dependence
- Trouble eating and loss of bowl/bladder control
- Limited vocabulary & comprehension



# Neuroimaging + machine learning have shown promise



#### Introduction

# Role of Explainable Artificial Intelligence (XAI)

- Black-box nature of AI models causes skepticism in clinics
- Trust and adoption require transparent decision-making
- XAI provides insights into why/how a prediction is made



#### **XAI** categories:

#### Pre-model / ante-hoc:

 Data or feature engineering before training the model (e.g., identifying key brain biomarkers).

#### In-model / Intrinsic:

 Incorporate model design or training mechanism into model itself

#### Post-model / post-hoc:

 Explaining predictions after the model runs (e.g., Grad-CAM).

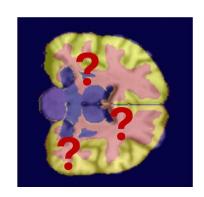


#### Introduction

# **Challenges in Medical XAI**

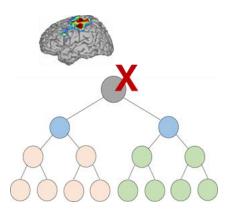
#### **Post-hoc approaches**

- Lack of ground truth to validate the explanation
- Lack of metrics for pathology alignment
- Post-hoc heatmaps (e.g., Grad-CAM) have limited reliability in brain scans (works better for natural images)



#### **Intrinsic approaches**

- While inherently interpretable (e.g., linear models or decision trees), they
- Struggle to capture complex patterns present in high-dimensional medical data





#### Our Method

# **Ante-hoc XAI with Jacobian Maps**

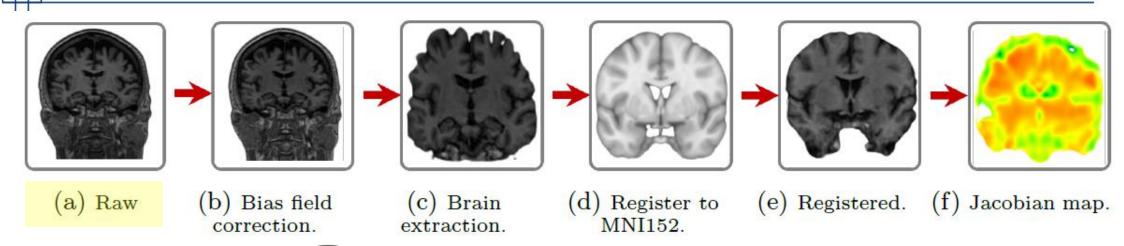
Introducing Jacobian Maps (JMs) as an ante-hoc explainability tool for AD detection.

#### How it works (overview):

- Compute Jacobian determinants, which measure how much each voxel
   (3D pixel in a brain scan) expands or shrinks compared to a healthy brain.
  - This creates a subject-specific map of brain structural changes.
  - This map serves as a kind of ground truth that highlights the locations of brain changes.
- and we apply it before training medical AI models.



# Transforming Brain Images into Jacobian Maps (JM)



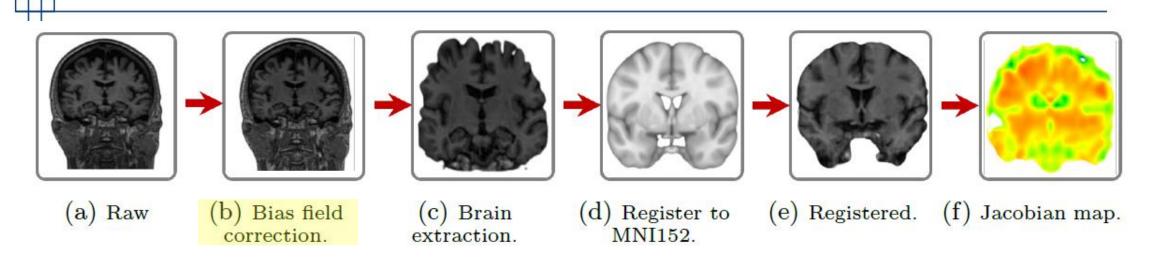
- Oasis dataset
- 3D images



- Participants include **755 cognitively normal (CN)** adults and **622 patients** at various stages of cognitive decline with age between 42-95 yrs.
- Based on clinical dementia rating (CDR) scores:

CDR	Class	
0	Normal	
0.5	MCI	
1	Mild	h
2	Moderate	Combine
3	Severe	

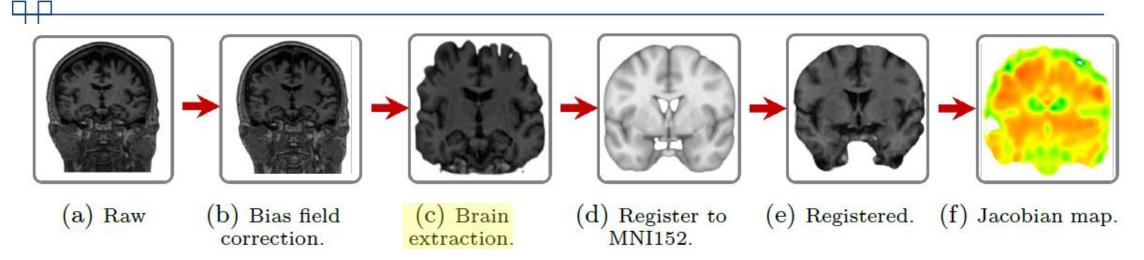
# **Transforming Brain Images into Jacobian Maps (JM)**



#### (b) Bias Field Correction

- Corrects non-uniform intensity caused by magnetic field inhomogeneities in the scanner.
- Ensures that tissue intensity is consistent across the brain.
- Tool: FLIRT (FMRIB's Linear Image Registration Tool)

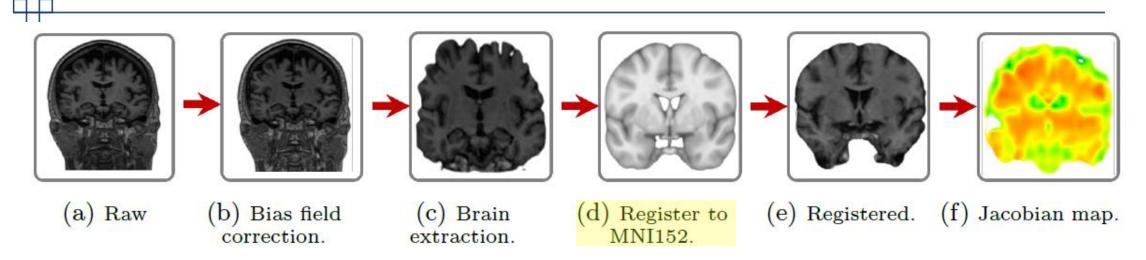
# Transforming Brain Images into Jacobian Maps (JM)



#### (c) Brain Extraction

- Removes non-brain tissues (skull, skin, etc.) to isolate the brain.
- Reduces irrelevant variability and computation.
- Tool: BET (Brain Extraction Tool)

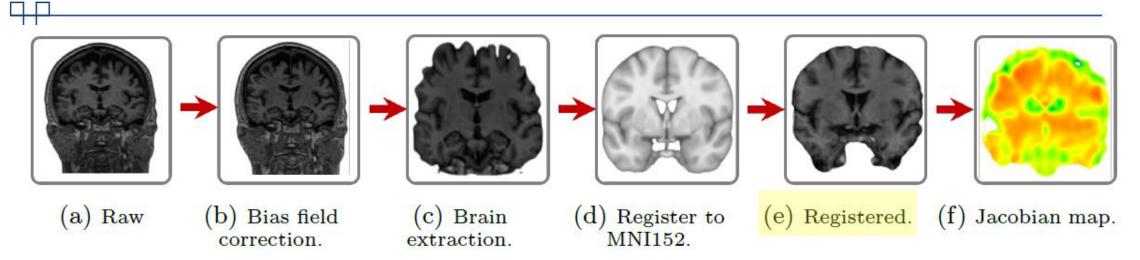
# **Transforming Brain Images into Jacobian Maps (JM)**



#### (d) Registration to Template (MNI152)

- Align each brain to a common anatomical space to allow voxel-wise comparison.
- Uses non-linear image registration via Symmetric Normalization (SyN).
- Tool: ANTs (Advanced Normalization Tools)

# **Transforming Brain Images into Jacobian Maps (JM)**



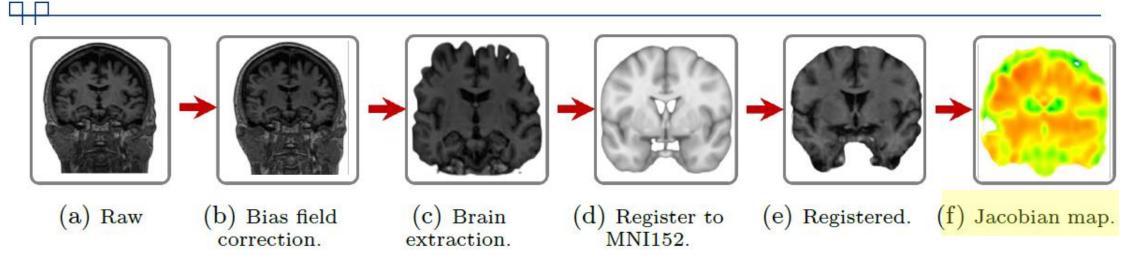
#### (e) Compute Deformation Vector Field

- After registration to MNI152, calculate how much each voxel has moved from the original brain.
- This deformation is expressed as a vector field:

$$v(x,y,z) = \phi(x,y,z) - (x,y,z)$$

where  $\phi$  is the transformation function.

# Transforming Brain Images into Jacobian Maps (JM)

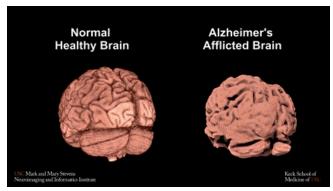


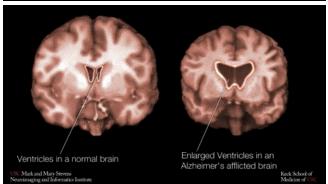
#### (f) Compute Jacobian Determinant

- A **Jacobian matrix** Is composed of the gradients of each deformation field v(.), and it captures the stretching, compression, and shearing of the voxel.
- We compute the determinant of this matrix.
- Doing this for all the voxels result in the Jacobian map.

# **Computing Jacobian Maps**

# Brain Volume Changes Denoting Dementia





#### **Deformation Field**

$$v(x,y,z) = \phi(x,y,z) - (x,y,z)$$

#### Jacobian Matrix (J):

$$J(v) = egin{pmatrix} rac{\partial v_x}{\partial x} & rac{\partial v_x}{\partial y} & rac{\partial v_x}{\partial z} \ rac{\partial v_y}{\partial x} & rac{\partial v_y}{\partial y} & rac{\partial v_y}{\partial z} \ rac{\partial v_z}{\partial x} & rac{\partial v_z}{\partial y} & rac{\partial v_z}{\partial z} \end{pmatrix}$$

#### **Jacobian Determinant:**

$$\mathrm{JM}(x,y,z) = \det(J(v(x,y,z)))$$

#### **Jacobian Map**

- Captures subtle brain volume changes
- Highlights local brain morphometry
- Provides informative representations for feature learning

#### **Semantics:**

Determinant of each voxel:

- >1 → local expansion
- =1 → no brain change
- <1 → local compression

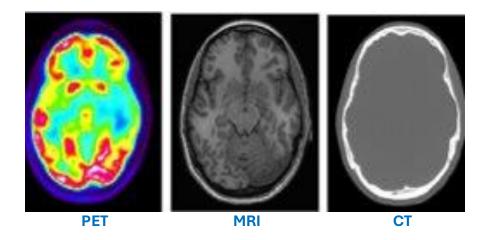
$$\begin{bmatrix} \vdots \\ \dots Det(J(v(x,y,z)) \dots \\ \vdots \end{bmatrix}_{ \begin{subarray}{c} x=1...W \\ y=1...H \\ z=1...D \end{subarray}$$

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#### Method

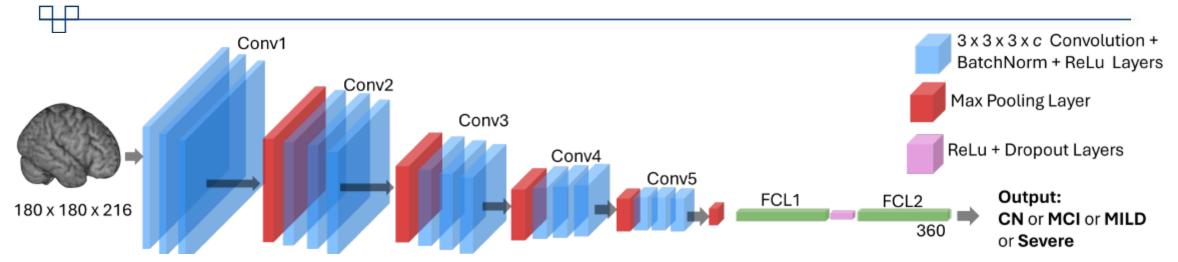
# **Key Advantages of JM for Ante-hoc XAI**

- No segmentation needed → avoids label noise and complexity
- Whole-brain coverage → no patch-based sampling
- Clinically intuitive → visualizes structural atrophy directly
- Quantitative → preserves local volume change metrics
- Generalizable → works across MRI, PET, or CT if deformation fields are computed





#### **Model Architecture**



- Input: 3D Jacobian Maps (or standard registered MRI images for comparison).
- Five 3D conv layers, each with a kernel of size 3×3×3.
- After each conv layer:
  - Batch Normalization: Stabilizes learning and accelerates convergence.
  - o ReLU Activation: Introduces non-linearity.
  - Max-Pooling (at selected layers): Downsamples the spatial resolution.
- Output is flattened and passed through two Fully Connected (FC) layers.
  - The first FC layer uses Dropout for regularization.
  - D The second FC layer outputs logits, normalized with Softmax to get class probabilities.

# **Training Details**



Optimizer: Adam

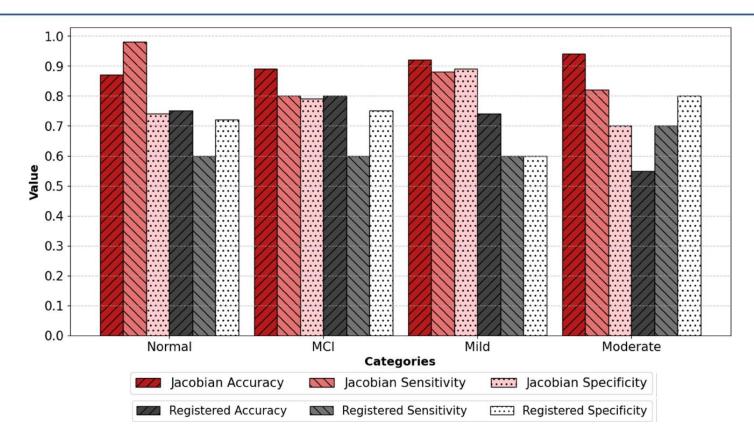
Cross-Entropy loss

Learning Rate: 1e-4

Batch Size: 15

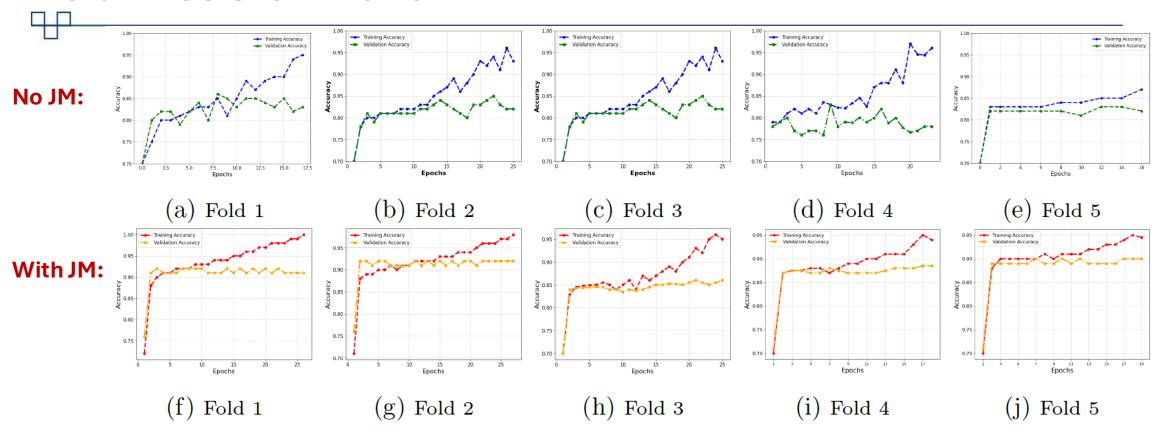
- 5-Fold Cross-Validation is used to ensure robust evaluation:
  - Data is split into 5 subsets: 4 for training and 1 for validation in each fold.
  - 50 epochs per fold
  - Early stopping if validation loss does not improve (to prevent overfitting)

# **Diagnostic Performance**



- JM-base approach outperforms those using standard registered MRIs in all metrics.
- JM contributes more discriminative information by capturing local volumetric brain changes.

#### **Fold-wise examination**

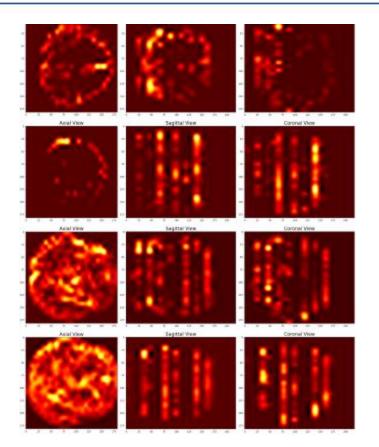


#### JM improves training stability:

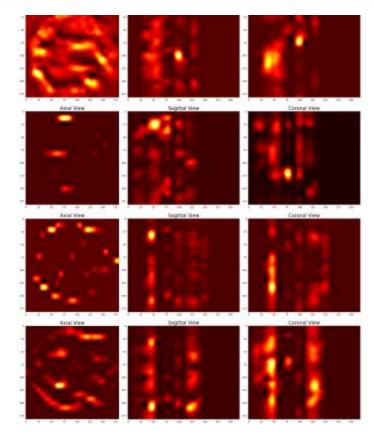
- no JM: More fluctuation and less consistent validation accuracy.
- with JM: Smoother, stabler convergence with better validation performance.

# Interpretations (Qualitative)

Grad-CAM is extended to 3D CNN to visualize the most influential regions.

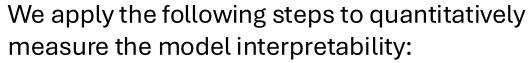


No JM: broader, less localized/focused activations.

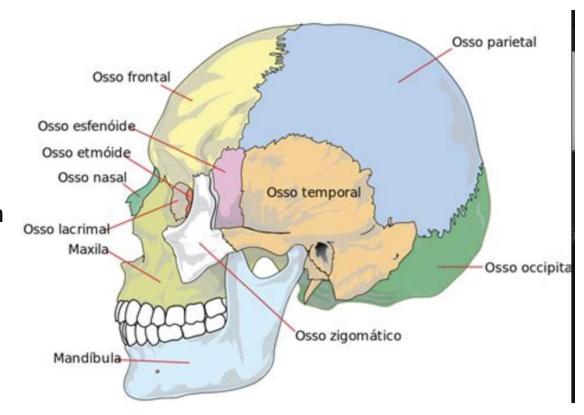


With JM: sharper focus on specific structural changes.

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- Register Grad-CAM heatmaps to MNI152 template.
- 2) Use the **Harvard-Oxford cortical atlas** to divide brain into anatomical regions.
- 3) Compute **average voxel intensity** within each region.
- 4) Rank regions by importance (activation level).





Avg. voxel intensity of each region

Table 1: Brain regions ranked by importance for each AD class based on heatmap intensity.

CN	MCI	MLD	SEV		
Frontal-Temporal (2.71)	Frontal-Temporal (2.45)	Frontal-Temporal (2.76)	Frontal-Temporal (2.76)		
Sub-lobar $(2.51)$	Temporal Lobe (1.94)	Temporal Lobe (2.33)	Frontal Lobe (2.28)		
Temporal Lobe $(2.43)$	Frontal Lobe (1.89)	Frontal Lobe (2.28)	Parietal Lobe (1.77)		
Limbic Lobe $(2.40)$	Sub-lobar $(1.78)$	Sub-lobar $(2.20)$	Limbic Lobe (2.01)		
Frontal Lobe $(2.37)$	Background (1.73)	Occipital Lobe (2.02)	Occipital Lobe (2.02)		
Midbrain (2.29)	Limbic Lobe (1.67)	Pons (1.82)	Pons (1.82)		
Pons $(2.26)$	Occipital Lobe (1.59)	Posterior Lobe (1.91)	Posterior Lobe (1.91)		
Background (2.08)	Anterior Lobe (1.53)	Background (1.73)	Background (1.73)		
Parietal Lobe (2.07)	Medulla (1.37)	Anterior Lobe (1.53)	Medulla (1.43)		
Posterior Lobe (1.98)	Midbrain (1.61)	Medulla (1.43)	Anterior Lobe (1.53)		
Medulla (1.76)	Frontal-Temporal (2.45)	Parietal Lobe (1.77)	Midbrain (1.90)		
Anterior Lobe (1.97)	Parietal Lobe (1.33)	Frontal Lobe (1.89)	Pons (1.82)		

- Frontal-temporal region is a key area involved in memory, decision-making and language.
- Changes / degenerates early, even starting from CN and MCI.

Avg. voxel intensity of each region

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- Rank of temporal lobe increases in MCI and MLD.
- Temporal lobe includes hippocampus (海马体) and entorhinal cortex (内嗅皮层), and is among the first regions to show atrophy, with **memory loss** being a key symptom.

Avg. voxel intensity of each region

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- In late AD, neurodegeneration becomes widespread.
- Frontal lobe handles planning, judgment, social behavior.
- Parietal (顶骨) lobe controls spatial orientation, attention.
- These areas are affected less during early stages but more in late stages.

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# Interpretations (Quantitative)

Table 1: Brain regions ranked by importance for each AD class based on heatmap intensity.

Avg. voxel intensity of each region

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- Limbic system is crucial for emotion and memory.
- Appears to be involved more in early and late stages while less in intermediate stages

# Skip if running short on time

## **Experiments**

# Interpretations (Quantitative) - Summary

- Frontal-Temporal regions are dominant across all classes → Key biomarkers in AD.
- As AD progresses, Temporal Lobe becomes more important in MCI and MLD stages.
- Parietal and Frontal Lobes gain importance in SEV → reflects widespread neurodegeneration.
- Sub-lobar and Limbic regions show varying importance, capturing non-linear disease progression.
- Consistency with clinical evidence is observed in our experiments.



# **Extension to Multi-modal Setting**

- Why Multi-modal Imaging?
  - Different imaging modalities capture complementary information:
    - o MRI: Excellent soft tissue contrast—shows structural brain changes like atrophy.
    - CT: Captures bone and dense tissue differences; helps with structural localization and calcification, and can fill in missing contrast in certain brain areas.
- We extend our study by combining MRI + CT:
  - Concatenate MRI and CT images along the channel dimension.
  - The fused volume is treated as a single input to the 3D CNN.
  - The model learns from joint features from the very beginning of processing.

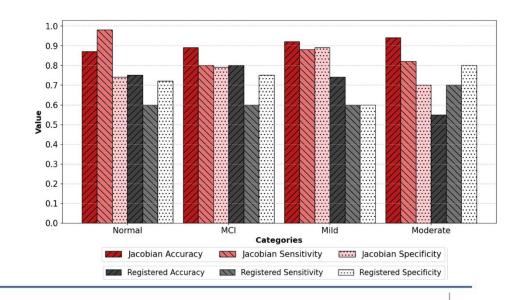


# **Extension to Multi-modal Setting**

Results

	Accuracy		Precision			Recall						
	$\mathbf{C}\mathbf{N}$	MCI	MLD	SEV	$\mathbf{CN}$	MCI	MLD	SEV	$\mathbf{C}\mathbf{N}$	MCI	MLD	SEV
REG	88.3	90.5	83.4	83.4	86.8	82.8	80	95.5	83.3	64.0	69.3	84.4
$\mathbf{J}\mathbf{M}$	95.2	96.3	90.2	90.2	92.8	100	83.33	98.6	94.96	89.6	78.6	90.2

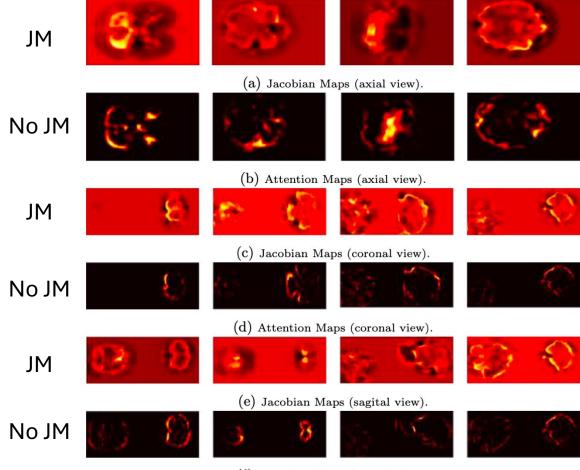
- Across all stages (CN, MCI, MLD, SEV), the use of Jacobian Maps still significantly improves all the metrics.
- Compared to the unimodal (MRI) case, performance improves overall, especially in early stages (which is important)



# **Extension to Multi-modal Setting**

#### **Interpretability Results**

Jacobian Maps enhance interpretability further by elevating the intensity level of AD-relevant regions; i.e., making the volumetric deformations more pronounced.



## **Conclusion**



#### Clinical Challenge

- Alzheimer's Disease (AD) is progressive (over multiple stages) and complex.
- Early, accurate diagnosis is critical yet explainability is key to adoption as well.

#### Our Contributions

- Introduced Jacobian Maps (JMs) as an ante-hoc XAI approach
  - o Capturing subtle, localized brain deformations to enable more interpretable model
- Integrated JMs into a 3D CNN and provided visual + quantitative interpretability using JM + Grad-CAM.
- Extended to a multimodal (MRI + CT) setting.

#### **Key Outcomes**

- Improved diagnostic performance across all AD stages.
- Enhanced interpretation consistent with clinical evidence (e.g., frontal-temporal lobes)
- Bridges the gap between deep learning and clinical interpretability.
- Scalable to other neurodegenerative diseases (e.g. Parkinson) and modalities (e.g., PET).



תודה Dankie Gracias Спасибо Köszönjük Grazie Dziękujemy Dėkojame Dakujeme Vielen Dank Paldies
Kiitos Täname teid 油油 Kiitos . 感謝您 Obrigado Σας Ευχαριστούμ Bedankt Děkujeme vám ありがとうございます Tack

# Comparison with VBM



#### What is VBM:

- **Voxel Based Morphometry** (VBM) is a neuroimaging analysis technique that compares local brain anatomy across individuals or groups.
- It helps detect structural differences in brain tissues.

#### **Key Difference:**

- While VBM uses JMs statistically to compare anatomical differences across groups (e.g., Alzheimer's vs. control) as a modulation technique,
- We repurpose JMs:
  - As a pre-model input to directly train deep learning models, to enhance both performance and explainability.



# Key novelties over VBM

#### 4

#### 1. Pre-model use of JMs in a deep learning pipeline

- Instead of using JMs after training for statistical analysis (as in VBM), we compute JMs and feed them as input images to a model.
- This is different from VBM's GLM or voxel-wise t-tests.

#### 2. Explainability through 3D Grad-CAM on JMs

- We apply Grad-CAM on a JM-based 3D CNN to generate heatmaps.
- Because JMs already represent deformation, the Grad-CAM heatmaps are **more anatomically grounded** (i.e., the interpretability is *meaningfully tied to real morphometric change*).

#### 3. Avoidance of segmentation and patch-based limitations

- VBM often depends on accurate segmentation and group-wise statistics.
- Our method bypasses those steps, offering **full-volume learning without patching or tissue segmentation**, which reduces preprocessing artifacts.

