

Multivariate Convolutional Sparse Coding for Electromagnetic Brain Signals

Dupré La Tour T., TM, Mainak J., Gramfort A.
INRIA Saclay

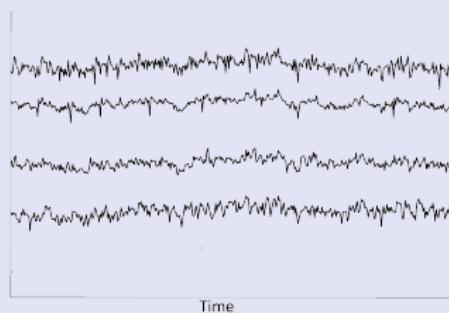
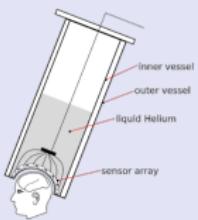
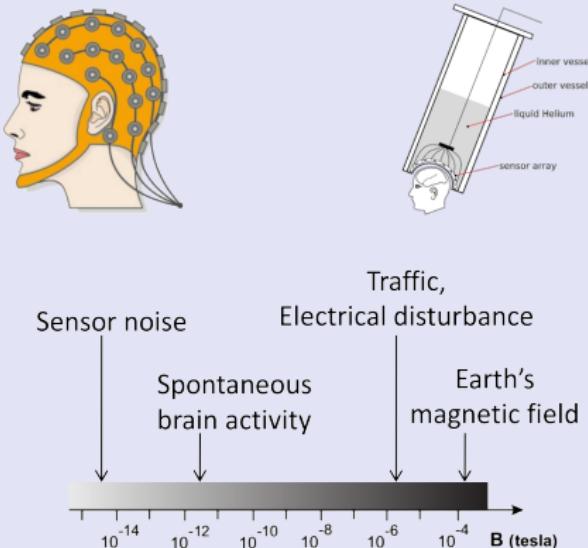


PARIETAL

inria
inventors for the digital world

Studying brain activity through electromagnetic signals

- ▶ Brain (electrical) activity produces an electromagnetic field.
- ▶ This can be measured with EEG or MEG.



Goal: Study Oscillation in Neural Data

Oscillations are believed to play an important role in cognitive functions.

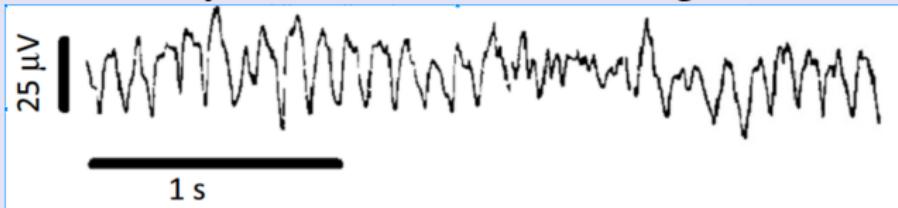
Many studies rely on Fourier or wavelet analyses:

- ▶ Easy interpretation,
- ▶ Standard analysis e.g. canonical bands alpha, beta or theta.

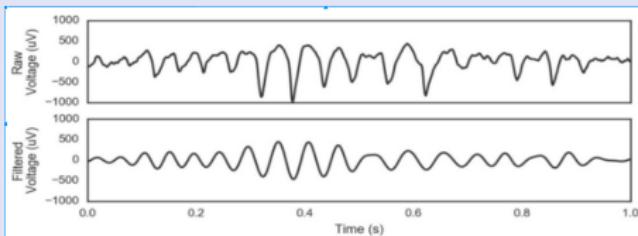
[Buzsáki, 2006]

Goal: Study Oscillation in Neural Data

However, some brain rhythms are not sinusoidal, e.g. mu-waves [Hari, 2006]



and filtering degrades waveforms

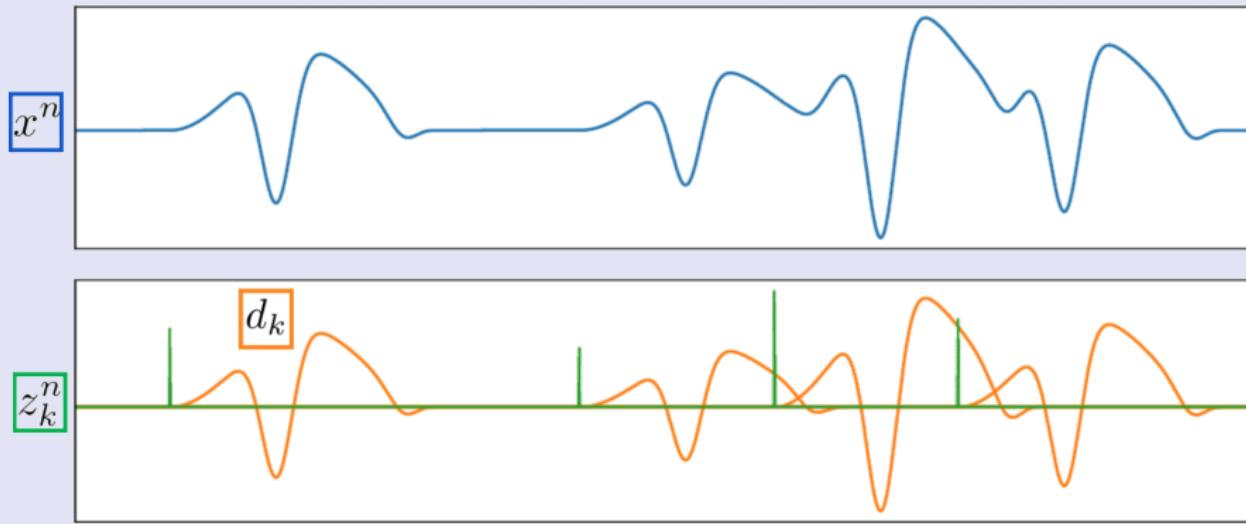


The shape of the waveform can be linked to the information flow between neurons.

⇒ Can extract them with an unsupervised data-driven approach?

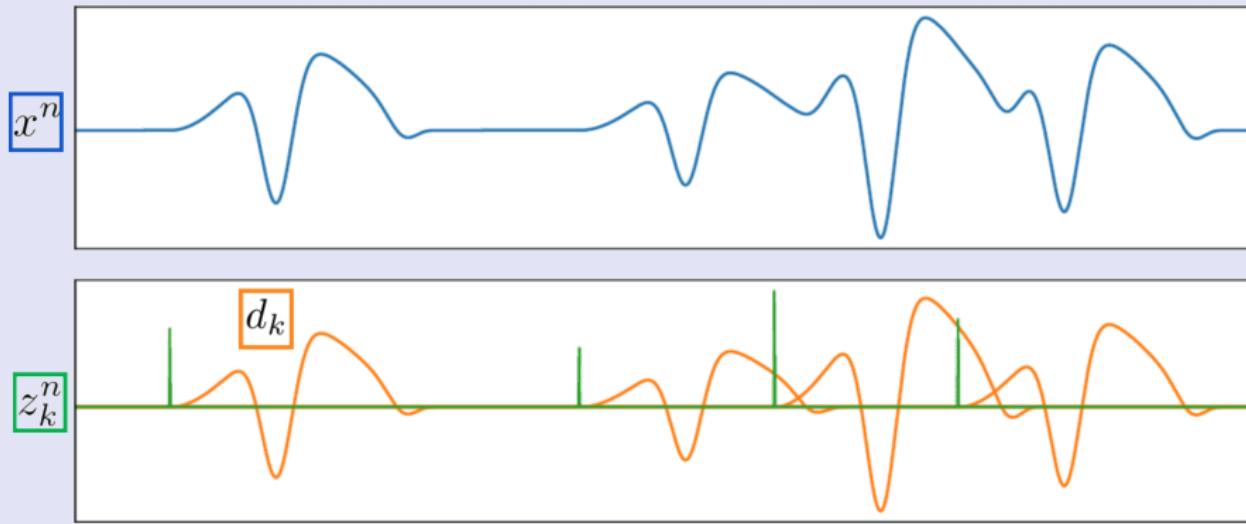
Extracting shift invariant patterns

Key idea: decouple the localization of the patterns and their shape



Extracting shift invariant patterns

Key idea: decouple the localization of the patterns and their shape

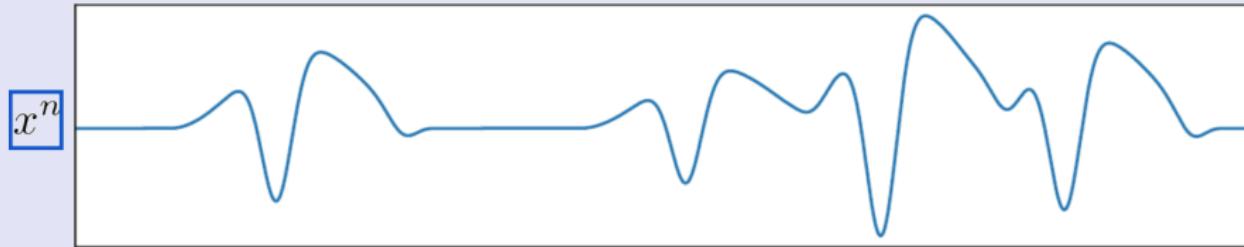


**Convolutional
Representation:**

$$x^n[t] = \sum_{k=1}^K (z_k^n * d_k)[t] + \varepsilon[t]$$

Extracting shift invariant patterns

Key idea: decouple the localization of the patterns and their shape



**Convolutional
Dictionary Learning:**

$$\begin{aligned} & \min_{d,z} \sum_{n=1}^N \frac{1}{2} \left\| x^n - \sum_{k=1}^K z_k^n * d_k \right\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1, \\ & \text{s.t. } \|d_k\|_2^2 \leq 1 \end{aligned}$$

Shift-invariant Patterns in images



Images also have shift-invariant patterns that we might want to detect.

Convolutional Dictionary Learning

Convolutional Dictionary Learning (CDL)

[Grosse et al., 2007]

For a set of N univariate signals x^n , solve

$$\min_{d_k, z_k^n} \sum_{n=1}^N \frac{1}{2} \|x^n - \sum_{k=1}^K z_k^n * d_k\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1 \quad (1)$$

Hypothesis: patterns d_k are not present everywhere in the signal. They are localized in time.

⇒ Sparse activation signals z

Extra hypothesis: the patterns are in the ℓ_2 -ball: $\|d_k\|_2^2 \leq 1$.

Optimization strategy

Bi-convex: The problem is not jointly convex in z_k^n , and d_k but it is convex in each block of coordinate.

Alternate minimization (a.k.a. Bloc Coordinate Descent):

- ▶ **Z-step:** given a fixed estimate of the atom, compute the activation signal z_k^n associated to each signal X^n .
- ▶ **D-step:** given a fixed estimate of the activation, update the atoms in the dictionary d_k .

Rank-1 constrained dictionary learning

References

- ▶ Dupré la Tour, T., Moreau, T., Jas, M., and Gramfort, A. (2018).
Multivariate Convolutional Sparse Coding for Electromagnetic Brain Signals.
In *Advances in Neural Information Processing Systems (NeurIPS)*, pages
3296–3306, Montreal, Canada

How to extend CSC to multivariate signals?

We can just use multivariate convolution,

$$\underbrace{X[t]}_{\in \mathbb{R}^P} = \sum_{k=1}^K (z_k * D_k)[t] = \sum_{k=1}^K \sum_{\tau=1}^L z_k[t - \tau] \underbrace{D_k[\tau]}_{\in \mathbb{R}^P}$$

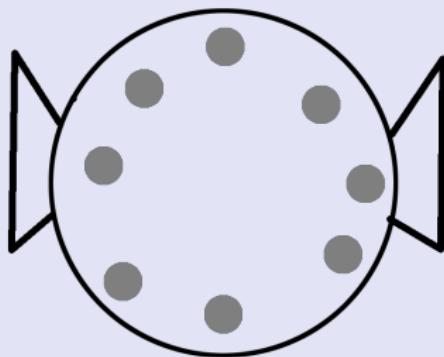
with:

- ▶ X a multivariate signal of length T in \mathbb{R}^P
- ▶ D_k a multivariate signal of length L in \mathbb{R}^P
- ▶ z_k a univariate activation signal of length $\tilde{T} = T - L + 1$

However, this model does not account for the physics of the problem.

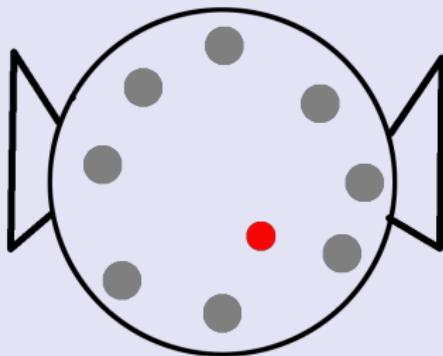
EM wave diffusion

- ▶ Recording here with 8 sensors



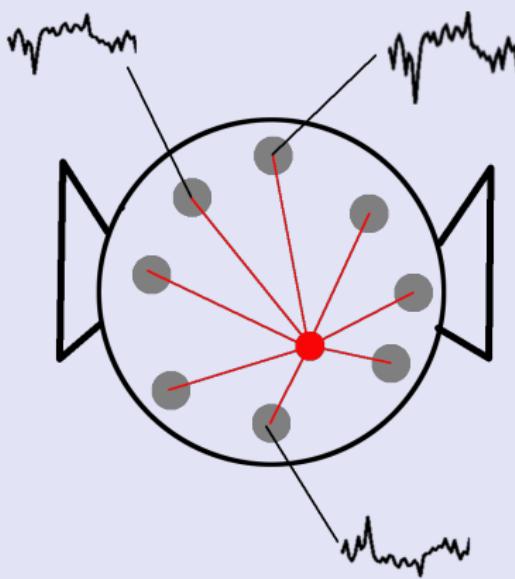
EM wave diffusion

- ▶ Recording here with 8 sensors
- ▶ EM activity in the brain



EM wave diffusion

- ▶ Recording here with 8 sensors
- ▶ EM activity in the brain
- ▶ The electric field is spread **linearly** and **instantaneously** over all sensors (Maxwell equations)



Multivariate CSC with rank-1 constraint

Idea: Impose a rank-1 constraint on the dictionary atoms D_k

To make the problem tractable, we decided to use auxiliary variables u_k and v_k s.t. $D_k = u_k v_k^\top$.

$$\begin{aligned} \min_{u_k, v_k, z_k^n} & \sum_{n=1}^N \frac{1}{2} \left\| X^n - \sum_{k=1}^K z_k^n * (u_k v_k^\top) \right\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1, \\ \text{s.t. } & \|u_k\|_2^2 \leq 1, \|v_k\|_2^2 \leq 1 \text{ and } z_k^n \geq 0. \end{aligned} \tag{2}$$

Here,

- ▶ $u_k \in \mathbb{R}^P$ is the spatial pattern of our atom
- ▶ $v_k \in \mathbb{R}^L$ is the temporal pattern of our atom

Optimization strategy

Tri-convex: The problem is not jointly convex in z_k^n , u_k and v_k but it is convex in each block of coordinate.

We can use a block coordinate descent, aka alternate minimization, to converge to a local minima of this problem. The 3 following steps are applied alternatively:

- ▶ **Z-step:** given a fixed estimate of the atom, compute the activation signal z_k^n associated to each signal X^n .
- ▶ **u-step:** given a fixed estimate of the activation and temporal pattern, update the spatial pattern u_k .
- ▶ **v-step:** given a fixed estimate of the activation and spatial pattern, update the temporal pattern v_k .

Z-step: Locally greedy coordinate descent (LGCD)

N independent problem such that

$$\min_{z_k^n \geq 0} \frac{1}{2} \left\| X^n - \sum_{k=1}^K z_k^n * D_k \right\|_2^2 + \lambda \sum_{k=1}^K \|z_k^n\|_1.$$

This problem is convex in z_k and can be solved with different techniques:

- ▶ Greedy CD [Kavukcuoglu et al., 2010]
- ▶ Fista [Chalasani et al., 2013]
- ▶ ADMM [Bristow et al., 2013]
- ▶ L-BFGS [Jas et al., 2017]

⇒ These methods can be slow for long signals as the complexity of each iteration is at least linear in the length of the signal.

Z-step: Locally greedy coordinate descent (LGCD)

For the Greedy Coordinate Descent, only 1 coordinate is updated at each iteration:

[Kavukcuoglu et al., 2010]

1. The coordinate $z_{k_0}[t_0]$ is updated to its optimal value $z'_{k_0}[t_0]$ when all other coordinate are fixed.

$$z'_k[t] = \max \left(\frac{\beta_k[t] - \lambda}{\|D_k\|_2^2}, 0 \right),$$

$$\text{with } \beta_k[t] = \left[D_k^\top * \left(X - \sum_{l=1}^K z_l * D_l + z_k[t] e_t * D_k \right) \right] [t]$$

For each coordinate update, it is possible to maintain the value of β with $\mathcal{O}(KL)$ operations.

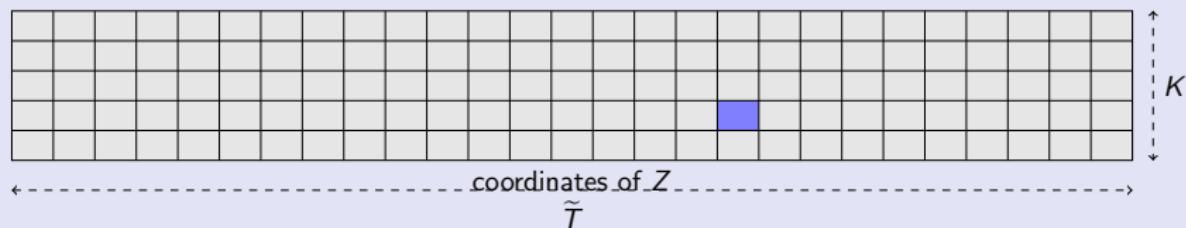
Z-step: Locally greedy coordinate descent (LGCD)

For the Greedy Coordinate Descent, only 1 coordinate is updated at each iteration:

[Kavukcuoglu et al., 2010]

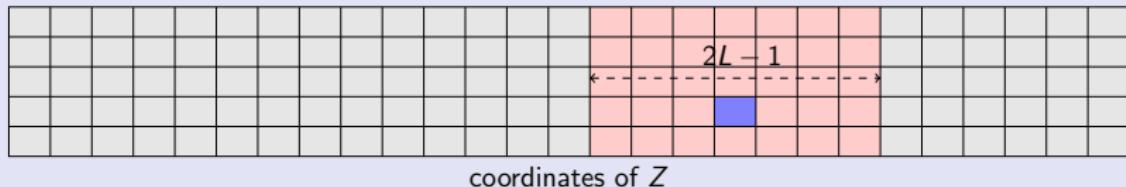
1. The coordinate $z_{k_0}[t_0]$ is updated to its optimal value $z'_{k_0}[t_0]$ when all other coordinate are fixed.
2. The updated coordinate is chosen
 - ▶ Cyclic selection: $\mathcal{O}(1)$ [Friedman et al., 2007]
 - ▶ Randomized selection: $\mathcal{O}(1)$ [Nesterov, 2010]
 - ▶ Greedy selection: $\mathcal{O}(K\tilde{T})$ [Osher and Li, 2009]
by maximizing $|z_k[t] - z'_k[t]|$

We introduced the LGCD method which is an extension of GCD.



GCD has $\mathcal{O}(K\tilde{T})$ computational complexity.

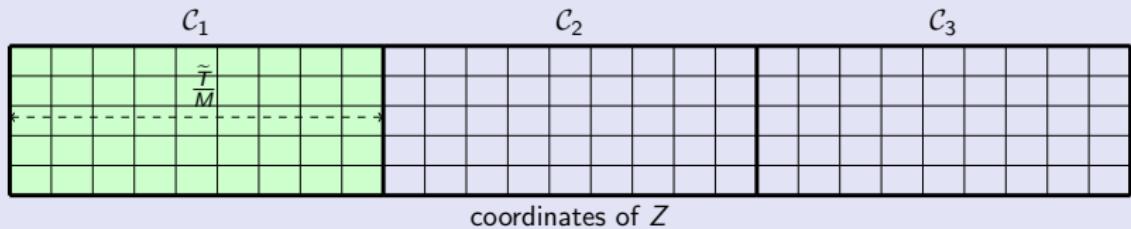
We introduced the LGCD method which is an extension of GCD.



GCD has $\mathcal{O}(K\tilde{T})$ computational complexity.

But the update itself has complexity $\mathcal{O}(KL)$

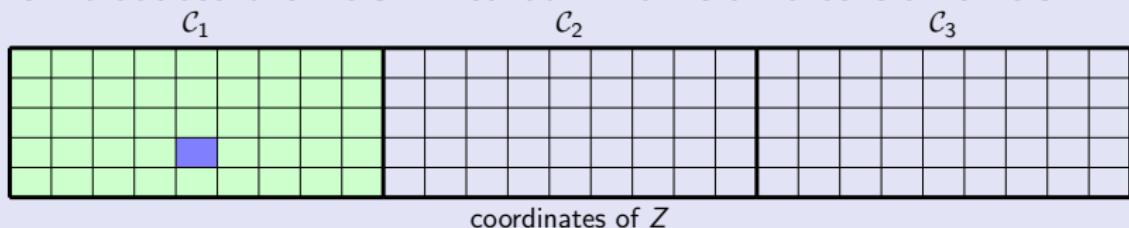
We introduced the LGCD method which is an extension of GCD.



With a partition \mathcal{C}_m of the signal domain $[1, K] \times [0, \tilde{T}]$,

$$\mathcal{C}_m = [1, K] \times \left[\frac{(m-1)\tilde{T}}{M}, \frac{m\tilde{T}}{M} \right]$$

We introduced the LGCD method which is an extension of GCD.



With a partition \mathcal{C}_m of the signal domain $[1, K] \times [0, \tilde{T}]$,

$$\mathcal{C}_m = [1, K] \times \left[\frac{(m-1)\tilde{T}}{M}, \frac{m\tilde{T}}{M} \right]$$

The coordinate to update is chosen greedily on a sub-domain \mathcal{C}_m

$$\frac{\tilde{T}}{M} = 2L - 1 \Rightarrow \mathcal{O}(\text{Coordinate selection}) = \mathcal{O}(\text{Coordinate Update})$$

The overall iteration complexity is $\mathcal{O}(KL)$ instead of $\mathcal{O}(K\tilde{T})$.

\Rightarrow Efficient for sparse Z

D-step: solving for the atoms

The dictionary update is performed by minimizing

$$\min_{\|D_k\|_2 \leq 1} E(D) \triangleq \sum_{n=1}^N \frac{1}{2} \|X^n - \sum_{k=1}^K z_k^n * D_k\|_2^2 . \quad (3)$$

Computing $\nabla_{d_k} E(\{d_k\}_k)$ can be done efficiently

$$\nabla_D E(D) = \sum_{n=1}^N (z_k^n)^\top * \left(X^n - \sum_{l=1}^K z_l^n * D_l \right) = \Phi_k - \sum_{l=1}^K \Psi_{k,l} * D_l ,$$

⇒ Save with Projected Gradient Descent (PGD) with an Armijo backtracking line-search for the D-step [Wright and Nocedal, 1999].

D-step: solving for the atoms

We use the projected gradient descent with an Armijo backtracking line-search [Wright and Nocedal \[1999\]](#) for both u-step and v-step for

$$\min_{\substack{\|u_k\|_2 \leq 1 \\ \|v_k\|_2 \leq 1}} E(u_k, v_k) \triangleq \sum_{n=1}^N \frac{1}{2} \|X^n - \sum_{k=1}^K z_k^n * (u_k v_k^\top)\|_2^2 . \quad (4)$$

One important computation trick is for fast computation of the gradient.

$$\begin{aligned}\nabla_{u_k} E(u_k, v_k) &= \nabla_{D_k} E(u_k, v_k) v_k \in \mathbb{R}^P , \\ \nabla_{v_k} E(u_k, v_k) &= u_k^\top \nabla_{D_k} E(u_k, v_k) \in \mathbb{R}^L ,\end{aligned}$$

Computing $\nabla_{D_k} E(u_k, v_k)$ can be done efficiently

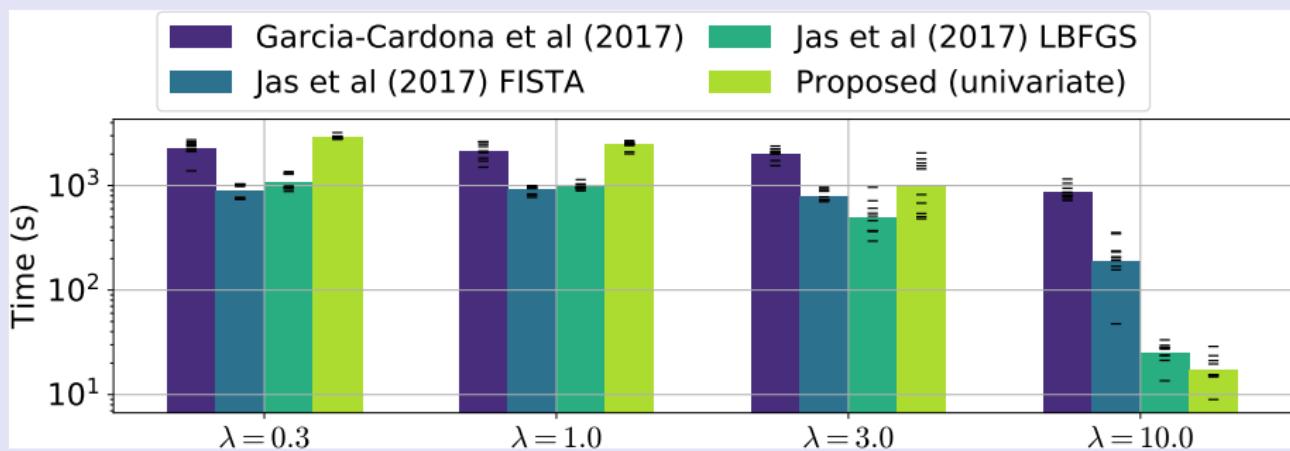
$$\nabla_{D_k} E(u_k, v_k) = \sum_{n=1}^N (z_k^n)^\top * \left(X^n - \sum_{l=1}^K z_l^n * D_l \right) = \Phi_k - \sum_{l=1}^K \Psi_{k,l} * D_l ,$$

Experiments

Good time to wake-up if you got lost in the previous section!

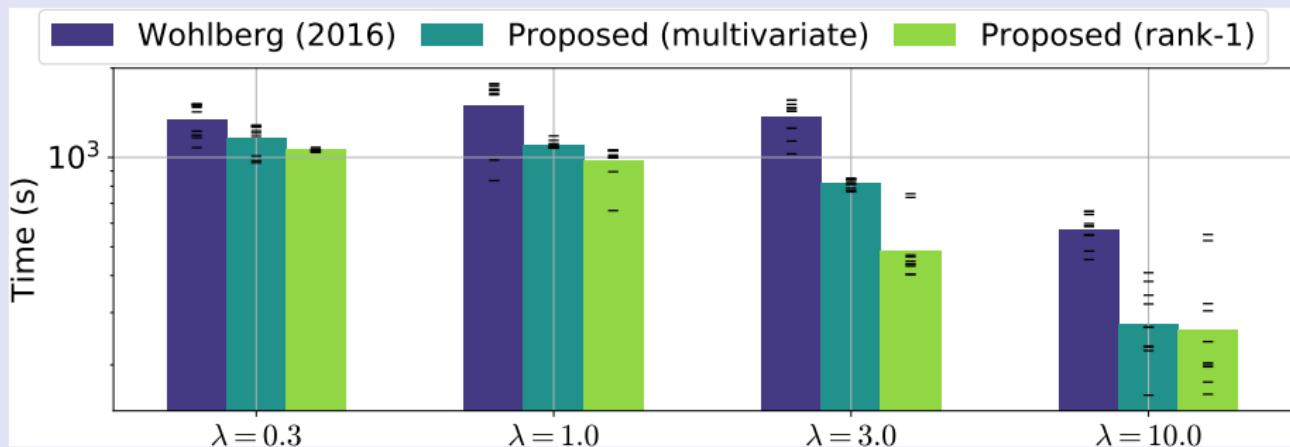
Fast optimization

Comparison with univariate methods on somato dataset with
 $T = 134,700$, $K = 8$ and $L = 128$



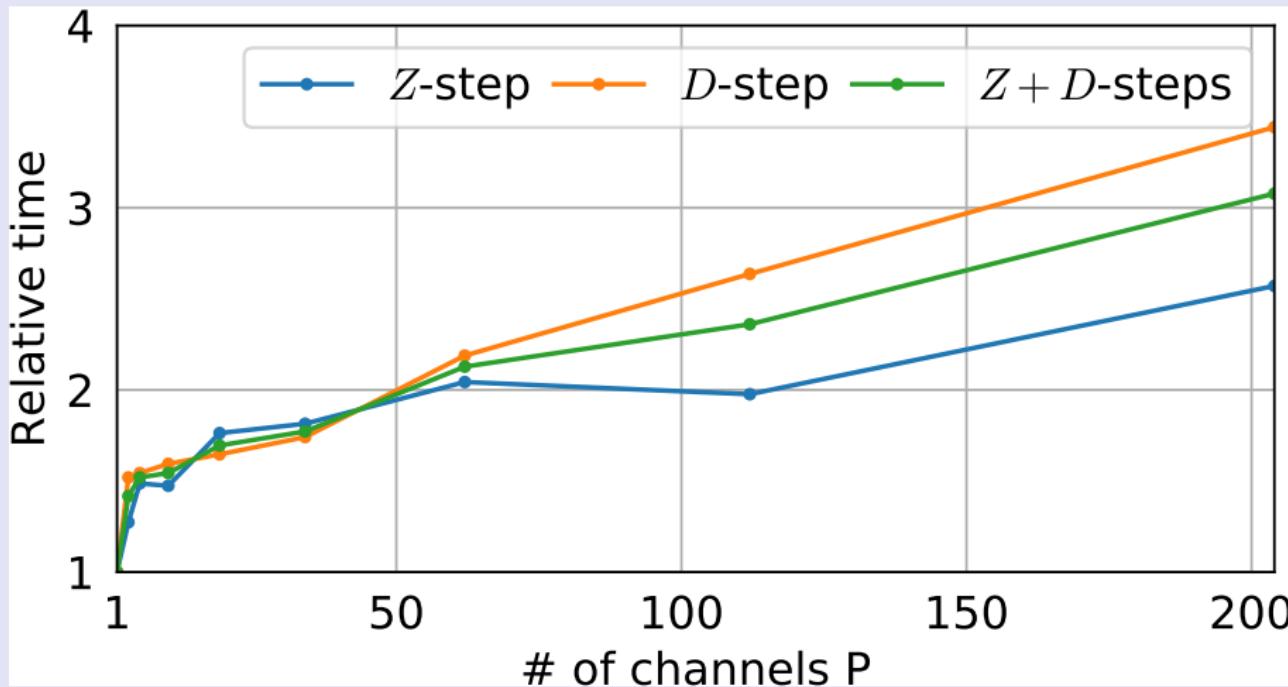
Fast optimization

Comparison with multivariate methods on somato dataset with
 $T = 134,700$, $K = 8$, $P = 5$ and $L = 128$



Good scaling in the number of channels P

Scaling relative to P on somato dataset with $T = 134,700$, $K = 2$, and $L = 128$



Pattern recovery

Test the pattern recovery capabilities of our method on simulated data,

$$X^n = \sum_{k=1}^2 z_k * (u_k v_k^\top) + \mathcal{E}$$

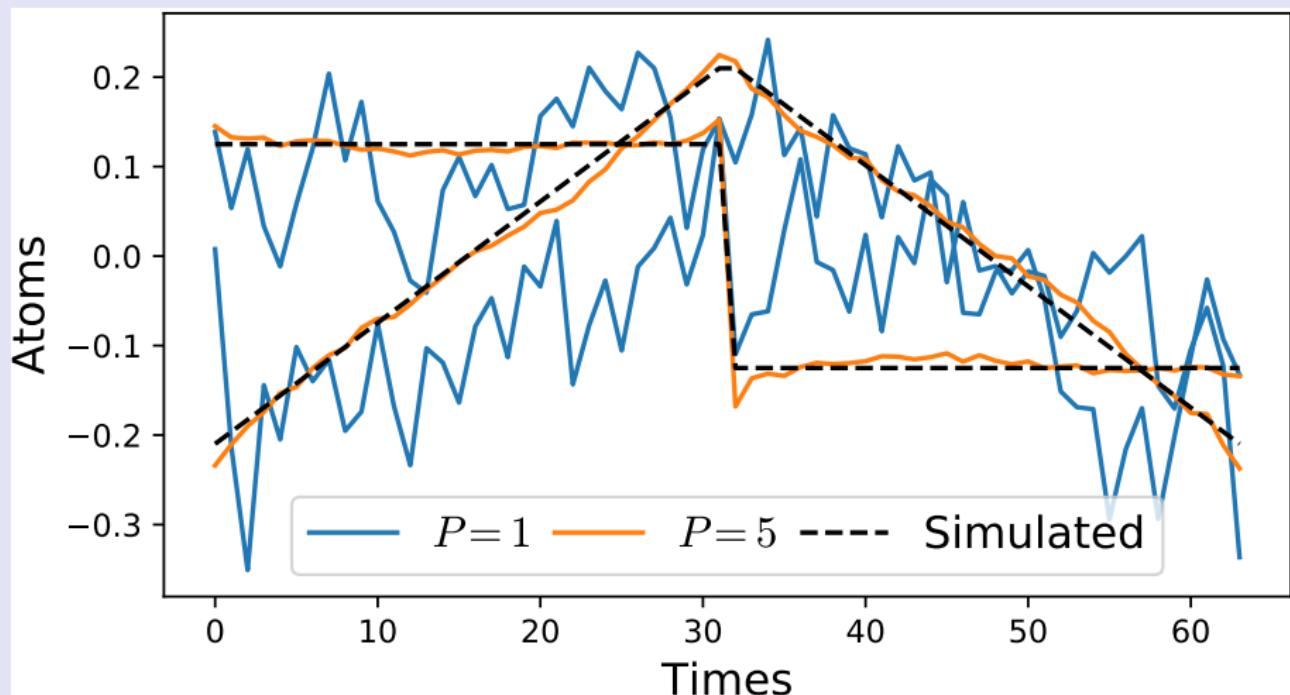
where (u_k, v_k) are chosen patterns of rank-1 and the activated coefficient $z_k^n[t]$ are drawn uniformly and their value are uniform in $[0, 1]$.

The noise \mathcal{E} is generated as a gaussian white noise with variance σ .

We set $N = 100$, $L = 64$ and $\tilde{T} = 640$

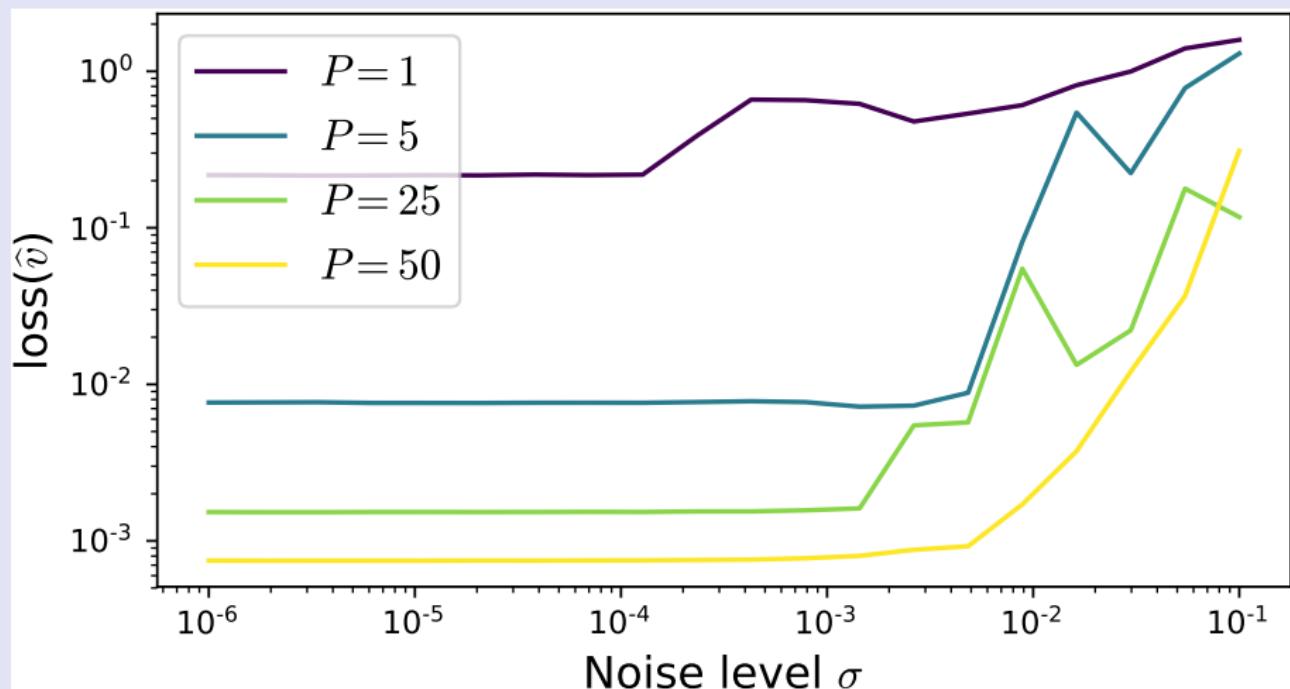
Pattern recovery

Patterns recovered with $P = 1$ and $P = 5$. The signals were generated with the two simulated temporal patterns and with $\sigma = 10^{-3}$.



Pattern recovery

Evolution of the recovery loss with σ for different values of P . Using more channels improves the recovery of the original patterns.



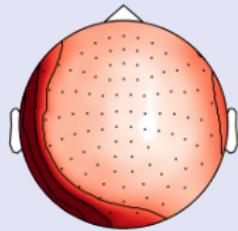
Experiments on MEG data

Even better time to wake-up!

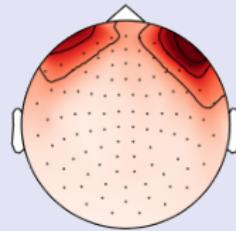
MNE somatosensory data

A selection of temporal waveforms of the atoms learned on the MNE sample dataset.

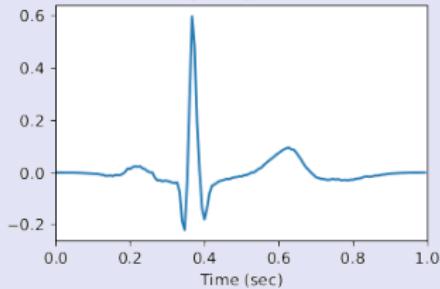
Spatial pattern 0
Explained variance 5.62 %



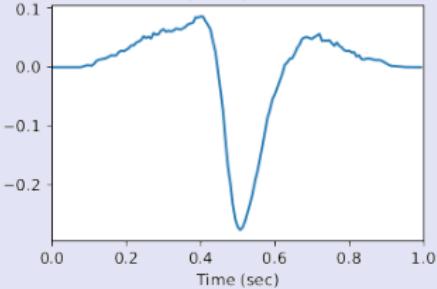
Spatial pattern 1
Explained variance 2.38 %



Temporal pattern 0

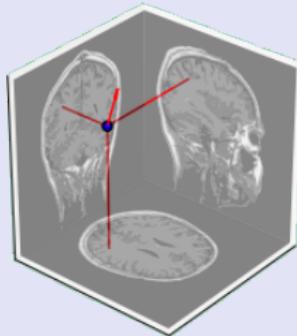
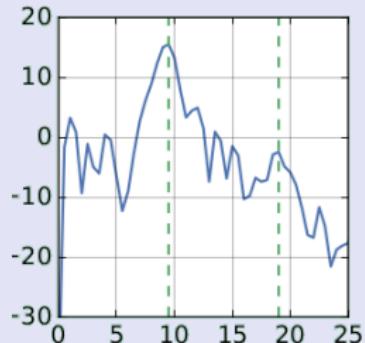
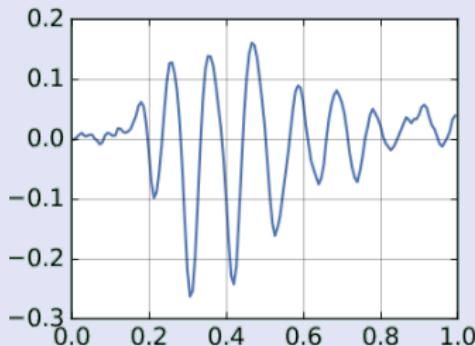


Temporal pattern 1



MNE somatosensory data

Atoms revealed using the MNE somatosensory data. Note the non-sinusoidal comb shape of the mu rhythm.



Conclusion

- ▶ We proposed a model for multivariate CSC with rank-1 constraint.
This model makes sense for different type of data.
- ▶ We proposed a fast algorithm to solve the optimization problem involved in this model.
- ▶ We demonstrated numerically the performance of our algorithm on both simulated and real datasets.
- ▶ We illustrated the benefit of such method to study electromagnetic signals form recorded from brain activity.

DiCoDiLe: Distributed Convolutional Dictionary Learning

References

- ▶ Moreau, T., Oudre, L., and Vayatis, N. (2018). [DICOD: Distributed Convolutional Sparse Coding](#).
In *International Conference on Machine Learning (ICML)*, pages 3626–3634, Stockholm, Sweden. PMLR (80)
- ▶ Moreau, T. and Gramfort, A. (2019). [Distributed Convolutional Dictionary Learning \(DiCoDiLe\): Pattern Discovery in Large Images and Signals](#).
preprint ArXiv, 1901.09235

Weak dependence of the coordinate updates

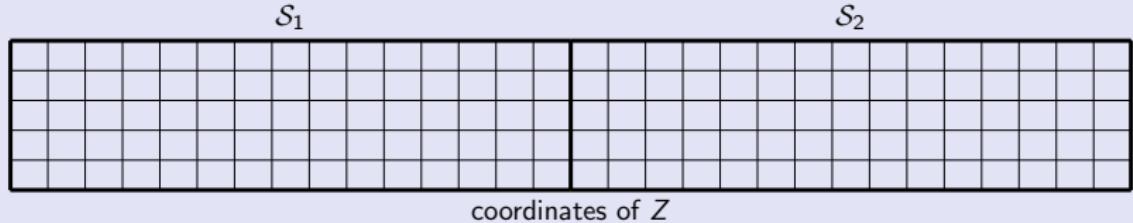
The update of the W coordinates $(k_w, \omega_w)_{w=1}^W$ with additive update $\Delta Z_{k_w}[\omega_w]$ changes the cost by:

$$\Delta E = \underbrace{\sum_{i=1}^W \Delta E_w}_{\text{iterative steps}} - \underbrace{\sum_{w \neq w'} (d_{k_w} * d_{k_{w'}}^\top) [\omega_{w'} - \omega_w] \Delta Z_{k_w}[\omega_w] \Delta Z_{k_{w'}}[\omega_{w'}]}_{\text{interference}},$$

⇒ If the updates are far enough, they can be considered as independent.

DICOD: Distributed Convolutional Coordinate Descent

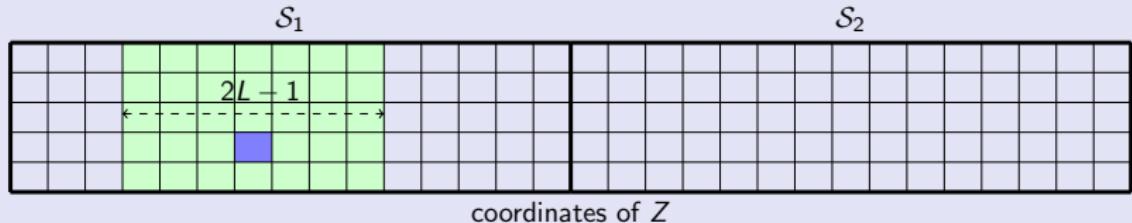
[Moreau et al., 2018]



- ▶ Split the coordinates in continuous sub-segment $\mathcal{S}_w = \left[\frac{(w-1)T}{W}, \frac{wT}{W} \right]$.

DICOD: Distributed Convolutional Coordinate Descent

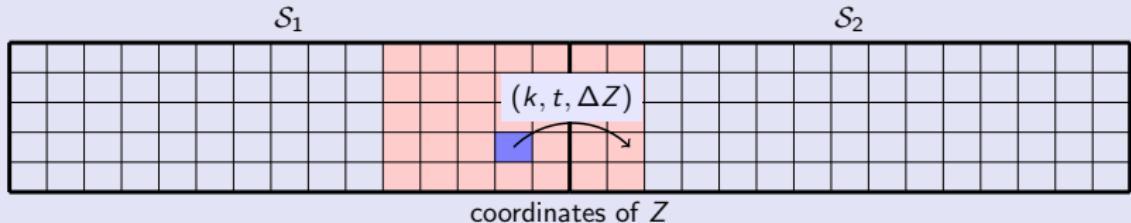
[Moreau et al., 2018]



- ▶ Split the coordinates in continuous sub-segment $\mathcal{S}_w = \left[\frac{(w-1)T}{W}, \frac{wT}{W} \right]$.
- ▶ Use CD updates in parallel in each sub-segment.

DICOD: Distributed Convolutional Coordinate Descent

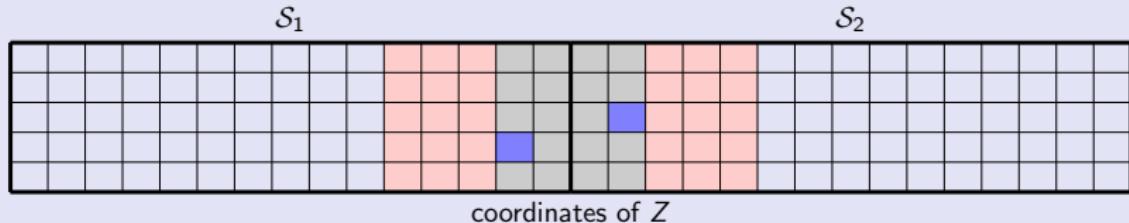
[Moreau et al., 2018]



- ▶ Split the coordinates in continuous sub-segment $\mathcal{S}_w = \left[\frac{(w-1)T}{W}, \frac{wT}{W} \right]$.
- ▶ Use CD updates in parallel in each sub-segment.
- ▶ Notify neighbor workers when the update is on the border of \mathcal{S}_w .

DICOD: Distributed Convolutional Coordinate Descent

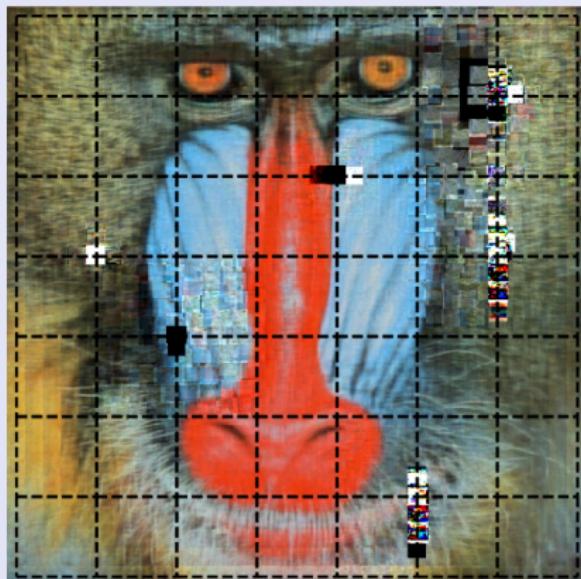
[Moreau et al., 2018]



- ▶ Split the coordinates in continuous sub-segment $\mathcal{S}_w = \left[\frac{(w-1)T}{W}, \frac{wT}{W} \right]$.
- ▶ Use CD updates in parallel in each sub-segment.
- ▶ Notify neighbor workers when the update is on the border of \mathcal{S}_w .
- ▶ What do we do when two updates are interfering?

Distributed Convolutional Dictionary Learning (DiCoDiLe-Z)

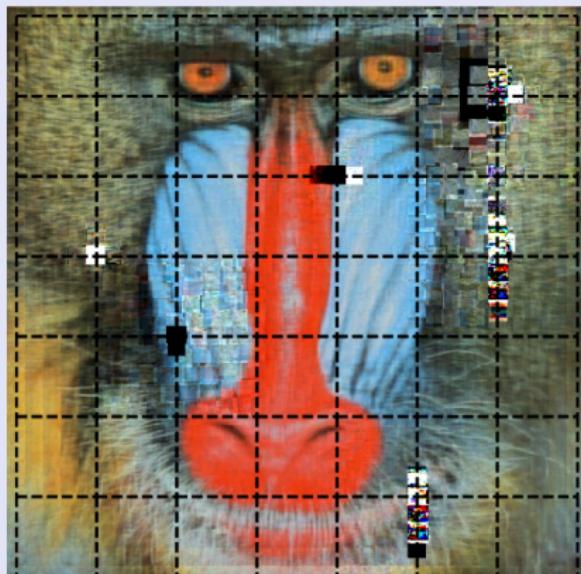
[Moreau and Gramfort, 2019]



- ▶ DICOD does not work for splits in dimension > 1 .

Distributed Convolutional Dictionary Learning (DiCoDiLe-Z)

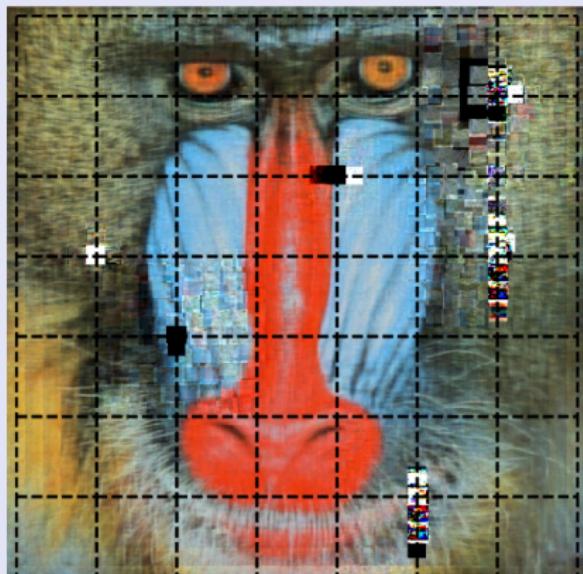
[Moreau and Gramfort, 2019]



- ▶ DICOD does not work for splits in dimension > 1 .
- ▶ Extension require to control interferences.

Distributed Convolutional Dictionary Learning (DiCoDiLe-Z)

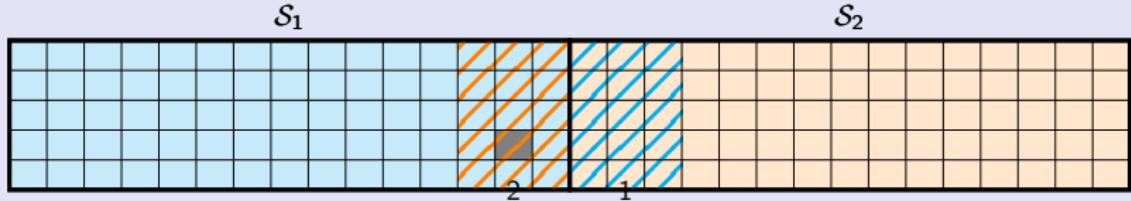
[Moreau and Gramfort, 2019]



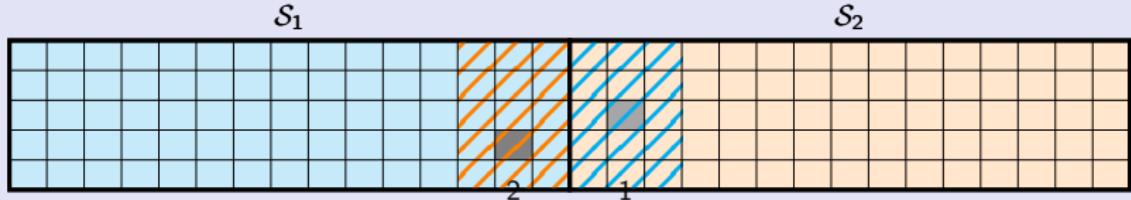
- ▶ DICOD does not work for splits in dimension > 1 .
- ▶ Extension require to control interferences.
- ▶ Use asynchronous mechanism: Soft-lock.



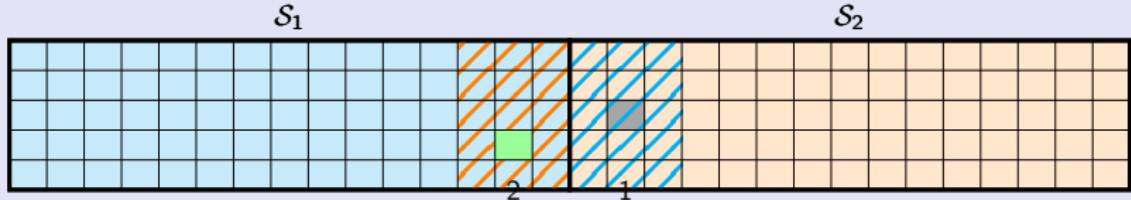
- ▶ Keep track of the value of the optimal update in an extended zone of size $L - 1$.



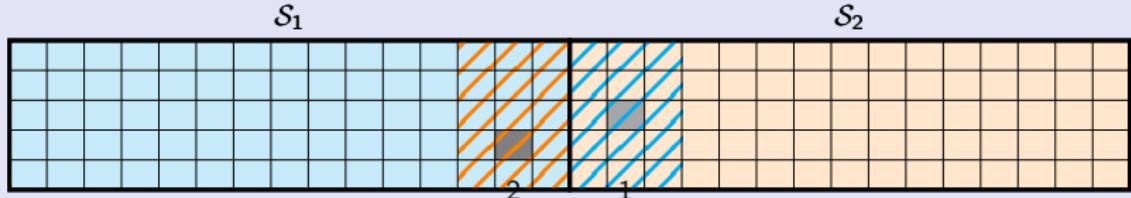
- ▶ Keep track of the value of the optimal update in an extended zone of size $L - 1$.
- ▶ Select an update candidate with LGCD.



- ▶ Keep track of the value of the optimal update in an extended zone of size $L - 1$.
- ▶ Select an update candidate with LGCD.
- ▶ If it is in the interfering zone, compare the value of the update with the value potential updates in the other worker.



- ▶ Keep track of the value of the optimal update in an extended zone of size $L - 1$.
- ▶ Select an update candidate with LGCD.
- ▶ If it is in the interfering zone, compare the value of the update with the value potential updates in the other worker.
- ▶ Only perform the update if it is larger than the other update.

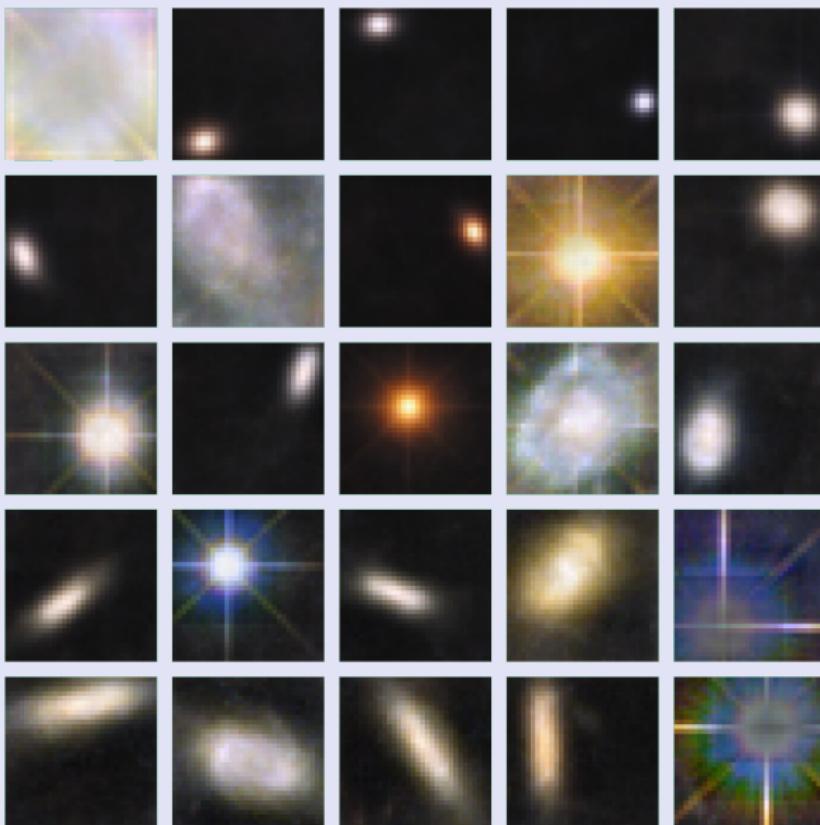


- ▶ Keep track of the value of the optimal update in an extended zone of size $L - 1$.
- ▶ Select an update candidate with LGCD.
- ▶ If it is in the interfering zone, compare the value of the update with the value potential updates in the other worker.
- ▶ Only perform the update if it is larger than the other update.
⇒ Give an update order asynchronously.

Images from Hubble Space Telescope



Images from Hubble Space Telescope



Thanks for your attention!

Code available online:

⌚ **alphacsc** : alphacsc.github.io

⌚ **DiCoDiLe** : github.com/tommoral/dicodile

Slides are on my web page:

🌐 tommoral.github.io

⌚ [@tomamoral](#)

Reference

- Bristow, H., Eriksson, A., and Lucey, S. (2013). Fast convolutional sparse coding. In *IEEE Conference on Computer Vision and Pattern Recognition (CVPR)*, pages 391–398, Portland, OR, USA.
- Buzsáki, G. (2006). *Rhythms of the Brain*. Oxford University Press.
- Chalasani, R., Principe, J. C., and Ramakrishnan, N. (2013). A fast proximal method for convolutional sparse coding. In *International Joint Conference on Neural Networks (IJCNN)*, pages 1–5, Dallas, TX, USA.
- Dupré la Tour, T., Moreau, T., Jas, M., and Gramfort, A. (2018). Multivariate Convolutional Sparse Coding for Electromagnetic Brain Signals. In *Advances in Neural Information Processing Systems (NeurIPS)*, pages 3296–3306, Montreal, Canada.
- Friedman, J., Hastie, T., Höfling, H., and Tibshirani, R. (2007). Pathwise coordinate optimization. *The Annals of Applied Statistics*, 1(2):302–332.
- Grosse, R., Raina, R., Kwong, H., and Ng, A. Y. (2007). Shift-Invariant Sparse Coding for Audio Classification. *Cortex*, 8:9.
- Hari, R. (2006). Action–perception connection and the cortical mu rhythm. *Progress in brain research*, 159:253–260.
- Jas, M., Dupré la Tour, T., Şimşekli, U., and Gramfort, A. (2017). Learning the Morphology of Brain Signals Using Alpha-Stable Convolutional Sparse Coding. In *Advances in Neural Information Processing Systems (NIPS)*, pages 1–15, Long Beach, CA, USA.
- Kavukcuoglu, K., Sermanet, P., Boureau, Y.-I., Gregor, K., and Le Cun, Y. (2010). Learning Convolutional Feature Hierarchies for Visual Recognition. In *Advances in Neural Information Processing Systems (NIPS)*, pages 1090–1098, Vancouver, Canada.
- Moreau, T. and Gramfort, A. (2019). Distributed Convolutional Dictionary Learning (DiCoDiLe): Pattern Discovery in Large Images and Signals. *preprint ArXiv*, 1901.09235.
- Moreau, T., Oudre, L., and Vayatis, N. (2018). DICOD: Distributed Convolutional Sparse Coding. In *International Conference on Machine Learning (ICML)*, pages 3626–3634, Stockholm, Sweden. PMLR (80).
- Nesterov, Y. (2010). Efficiency of coordinate descent methods on huge-scale optimization problems. *SIAM Journal on Optimization*, 22(2):341–362.
- Osher, S. and Li, Y. (2009). Coordinate descent optimization for ℓ_1 minimization with application to compressed sensing; a greedy algorithm. *Inverse Problems and Imaging*, 3(3):487–503.
- Wright, S. and Nocedal, J. (1999). *Numerical optimization*. Science Springer.