

Introduction to BCI: Decoding(1) - Artifacts and filtering

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Outline

Introduction

Pre-processing

Artifacts in BCI

Example artifacts

Rereferencing

Re-referencing

Data-Cleaning: Artifact Detection, and Rejection/Removal

Artifact Detection

Artifact Rejection/Removal

Artifact Removal

Signal Filtering

Spectral decompositions

Signal filtering

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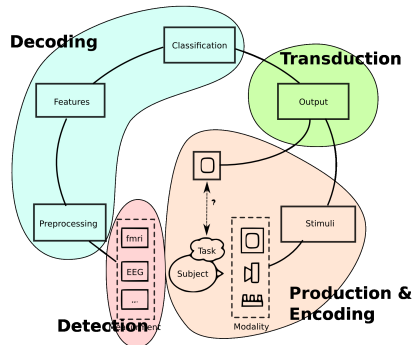
Spectral decompositions

Signal filtering

How does a BCI work?

Fundamentally, BCI is a **simple**(?) engineering problem;

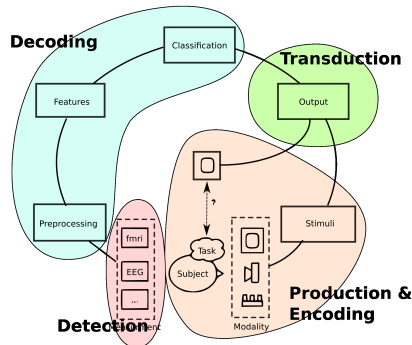
- 1 **Signal Production**: Get the person to **produce** a strong brain signal, either by performing an explicit **mental-task**, or through normal mental processes
- 2 **Detection**: Build a machine able to measure the properties of their brain, e.g. EEG, MEG, fMRI
- 3 **Decoding**: Build a machine able to **decode** the measurements to deduce the users mental state
- 4 **Transduction**: Communicate the mental-state to the outside world



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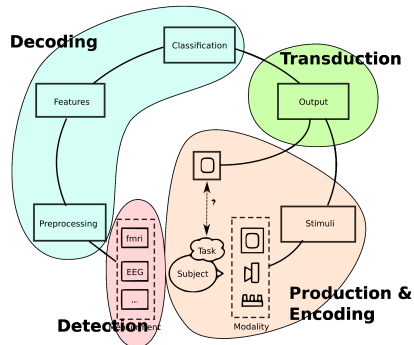
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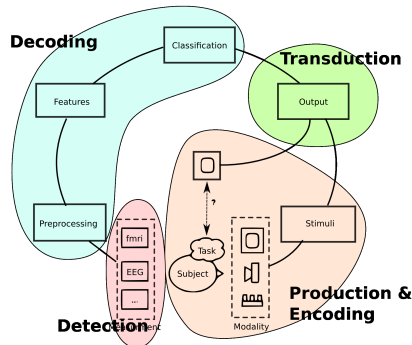
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The need for signal-processing

Just to re-iterate

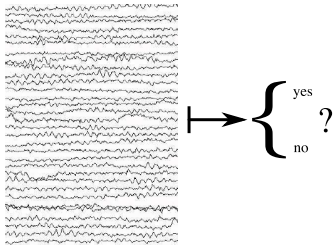
Defn. BCI

a system which allows someone to communicate information about their **mental state** without the use of the **peripheral nervous system**.

Note the emphasis. That means we **can't** use:

- ▶ muscles
- ▶ peripheral nerves, e.g. motor neurons
- ▶ **machine artifacts**

Decoding the neural code



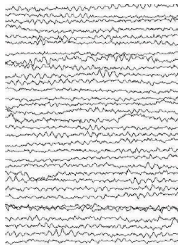
Further:

- ▶ non-brain sources generate much stronger signals than the brain
- ▶ Thus we must remove them to be sure our BCI has a B in it..
- ▶ and isn't a: MMI, EMI, CCI etc..

Unfortunately

- ▶ In general, we don't know how the users intentions are encoded in the neural signal
- ▶ we don't know how the signal may be encoded for this individual

Decoding the neural code



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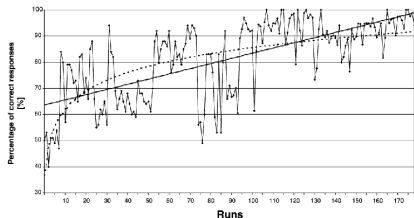
Further:

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- ▶ and isn't a: MMI, EMI, CCI etc..

Decoding Options

Thus we have two options:

1. **train** the **user** to generate a strong known signal, e.g. SCP, μ ERDS
2. **train** the machine to identify and extract the **signature** of this users mental state..



Thus:

We use **signal-processing** and **machine learning** to automatically decode the neural code for each new subject.

Learning Objectives

- ▶ Understand why pre-processing is necessary in BCI
- ▶ Describe the main sources of artifacts and their effects on the recorded signal; i.e. muscles, eyes, movement, hardware, line-noise etc.
- ▶ Describe the main types of pre-processing and what they are useful for; re-referencing, spectral-filtering, artifact-detection/rejection/removal
- ▶ Understand what is shown in the temporal, spectral and time-frequency representations of a signal
- ▶ Understand how signal filtering in these different representations can be used to suppress the noise in measured data, and hence make a signal more visible
- ▶ Understand how knowledge of the signal characteristics allows one to design signal filters to improve signal-to-noise

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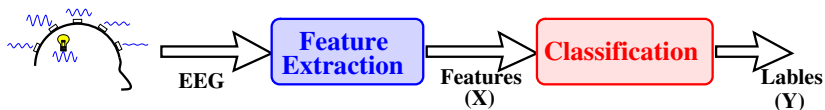
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Decoding Steps



The decoding process consists of 2 main steps:

1. Pre-processing and feature extraction - remove noise and focus on signal-characteristics of interest
2. Classification - learn a mapping from pre-processed features to decoded-mental states

Typical pre-processing pipeline

1. Pre-processing
 - ▶ re-reference
 - ▶ detect+reject bad-channels/epochs
 - ▶ data-cleaning - remove known artifact sources
 - ▶ spectrally/temporally filter
2. Feature Extraction : extract problem specific features based on knowledge of the signal characteristics, e.g. PSD for μ -ERD/S
3. Classification : train a classifier with the extracted features to learn the subject-specific signal

Golden rule of pre-processing

<rant on>

Don't **leak** label information into your data.

- ▶ BCI signal is **very small**
- ▶ Noise is big → after removal can still be larger than BCI signal
- ▶ class aware pre-processing can **leak** class information
- ▶ **clever** classifier will use this leaked information if available

The Golden Rule of Pre-Processing

Use **exactly** the same pre-processing for **all** epochs.

i.e.

- ▶ epoch-by-epoch pre-processing
- ▶ all-epochs pre-processing

</rant off>

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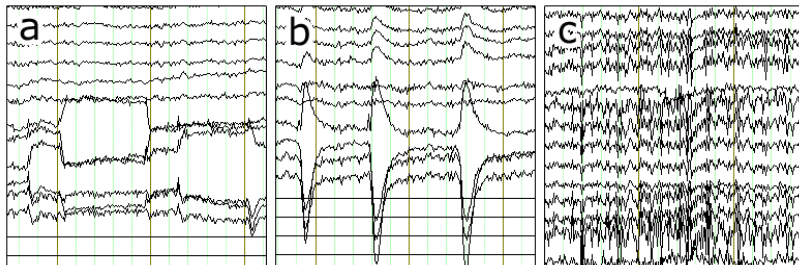
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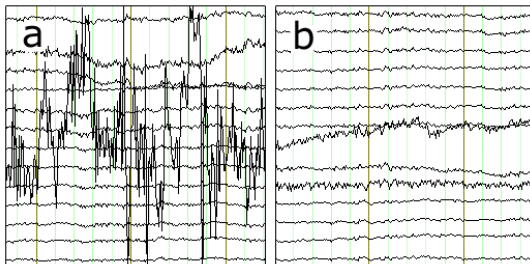
Signal filtering

Example Artifacts (1)



- a Eye movement
- b Eye blink
- c Muscle tension

Example Artifacts (2)



a bad channel

b baseline drift

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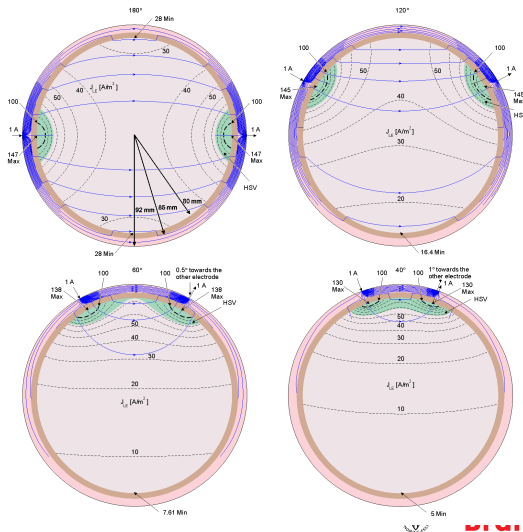
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Reference Sensitivity

- ▶ EEG measures **voltage differences** between electrode and reference
- ▶ Thus, EEG signal is sensitive to selection of reference location



Re-referencing

- ▶ Amplifier internally uses a particular reference/ground
- ▶ re-reference in s/w to change sensitivity region of each electrode
- ▶ **assume** the recorded signal at each electrode the combination of true signal, s , and common artifact, n , i.e.

$$x(t) = s(t) + n(t)$$

- ▶ thus, re-referencing to a new reference channel, $r(t)$, can remove the artifact

$$x_r(t) = s(t) + n(t) - r(t)$$

- ▶ re-referencing changes how your data **looks**
- ▶ removes common parts of the reference, e.g. $n(t)$, from x ,
- ▶ spreads non-common parts of the reference into all electrodes

Thus

ideal reference contains only the common **noise** component

Commonly used references (1)

- ▶ Ear - far from brain
- ▶ (Linked)-mastoids - far from brain
- ▶ Common-average / Common-mode
 - ▶ assuming signals s are **zero-mean**,

$$\langle \mathbf{x}(t) \rangle = \langle \mathbf{s}(t) \rangle - \langle n(t) \rangle = n(t)$$

- ▶ Note: non-zero-mean part of signal gets spread over all electrodes

Commonly used references (2)

- ▶ local-reference
 - ▶ assuming signals s_I is locally zero-mean, but noise is not

$$\mathbf{x}_I(t) = \mathbf{s}_I(t) - \mathbf{n}_I(t)$$

- ▶ where I is some local group of electrodes
- ▶ thus, $\langle \mathbf{x}_I(t) \rangle = \langle \mathbf{s}_I(t) \rangle - \langle \mathbf{n}_I(t) \rangle = \mathbf{n}_I(t)$
- ▶ N.B. vol-conducted signal nearby sources also tends to be **locally** non-zero mean, thus improves spatial-selectivity
- ▶ surface-laplacian (SLAP)
 - ▶ special form of local-reference
 - ▶ estimate of the local-divergence of the scalp current
 - ▶ shown to be good approx. to dura potential [Nunez 1987]
 - ▶ significant increase in spatial selectivity
 - ▶ estimated using spline interpolation, see [Perrin 1989]

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Data-Cleaning

- ▶ **Detection** – find where the artifacts are in the data, **easy->hard**
- ▶ **Rejection** – delete data containing artifacts, **easy**
- ▶ **Removal** – remove the artifact leaving signal intact, **hard**

Mk 1 - eyeball

Visually scan the data and hand mark artifacts

- ▶ Slow
- ▶ Tedious and prone to errors
- ▶ good as a final check

Outlier Detection

- ▶ Assume **most** data is artifact free
- ▶ Look for data which is **significantly** different from the rest
- ▶ treat these as artifacts

Note

need some measure of **similarity** between data-segments to assess significance

Example: variance based bad-electrode detection

- ▶ bad channels tend to have more noise than good ones
- ▶ this noise increases the variance/power of the data, i.e. variance is our similarity measure

Processing Steps:

1. estimate the variance of each electrode
2. compute the mean and variance of these estimates
3. electrodes more than (say) 4-std-deviations from mean are detected as bad

Note

Note: Fieldtrip has a mode for performing this type of analysis visually jointly over electrodes and epochs

Template Matching Detection

- ▶ Some artifacts have a particular **shape**
e.g. eye-blink, saccads
- ▶ look for that shape in data to detect the artifact

Note

Need a good (subject-specific) template **shape**

Note

Can match templates in frequency-domain, or over multiple electrodes

Template Matching

Processing Steps:

1. **visually** select a set of example artifacts
2. **average** these together to generate a **template** artifact, $a(t)$
3. **convolve** the template with the data to compute a similarity measure

[animation](#)

$$\text{sim}(t) = \sum_{\tau} x(t + \tau) a(\tau)$$

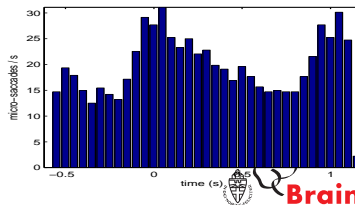
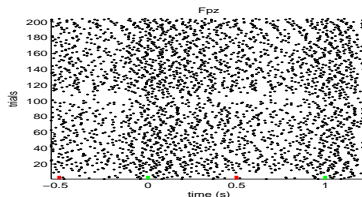
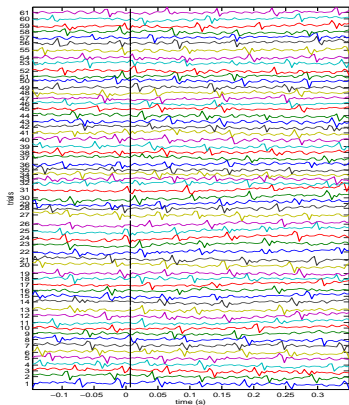
4. **peak-detect & threshold** to detect artifacts

Note

Related idea is to train a **classifier** to recognise the artifact

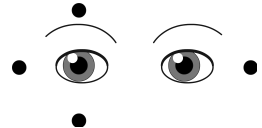
Saccade detection

- ▶ saccades have a characteristic shape+location
- ▶ anywhere this shape occurs at that location is an artifact



Sensor Based Detection

- ▶ Many artifacts are generated by known physical processes, e.g. eye-blinks, arm-movements, external-stimulation
- ▶ record the generating process to identify the artifact



Example: eye-blink detection

- ▶ add extra EOG channels to the montage
- ▶ threshold (or template match) the EOG data to detect eye-blinks

Note

Record everything you can, e.g. eye, muscle, heart, audio/video stimulus, so you identify causes of artifacts

Artifact Removal

Now that we have detected our artifacts we must remove them from the data

- ▶ **Rejection** – just throw away the data with artifacts
- ▶ **Removal** – attempt to clean the artifacts from the data

Linear Artifact removal

- ▶ say we have detected an artifact and extracted a template, n
- ▶ this could be from any of the methods presented above, i.e. template match, extra-sensor, virtual-sensor etc.
- ▶ **assume** the recorded signal is a weighted combination of true signal, s , and the artifact, n , i.e.

$$x(t) = s(t) + an(t)$$

- ▶ then by simply subtracting $an(t)$ from x we remove the artifact!
- ▶ the problem is we don't know the weighting a
- ▶ the weight of a source over all electrodes is called its **spatial pattern**

Two main ways to estimate a

1. correlation-based
2. volume-conduction based

Correlation-based artifact removal

- ▶ **assume** the signal, s , is **un-correlated** with the artifact, n , i.e. $s^\top n = 0$, then

$$x^\top n = (s + an)^\top n = an^\top n$$

- ▶ Hence,

$$a = \frac{x^\top n}{n^\top n}$$

- ▶ Combining with artifact removal gives,

$$s = x - an = x - n \frac{n^\top x}{n^\top n} = \left(I - \frac{nn^\top}{n^\top n} \right) x$$

Note: This operation is also called deflation, and de-correlation of the 2 signals x and n .

Example: EOG electrode based eye-blink removal

- ▶ use the raw EOG data as the noise signal n to subtract

Volume conduction-based artifact removal

- ▶ Vol-conduction means that the weight a depends (mainly) on the distance between the artifact source and the electrode
- ▶ Thus a can be computed given an assumed artifact source location using a forward model

Example: Common-Average-Referencing

- ▶ **re-referencing** to common average is a special case
- ▶ assume artifact **far** enough away that **all** electrodes have the same weight a
- ▶ then because all the other sources will tend to cancel out
- ▶ averaging the electrode activations leaves only the weighted artifact
- ▶ thus, subtracting average activation removes this artifact

Note

The **spatial patterns** computed by some Spatial-filtering methods, e.g. PCA, ICA, CSP, directly gives us the electrode weights.

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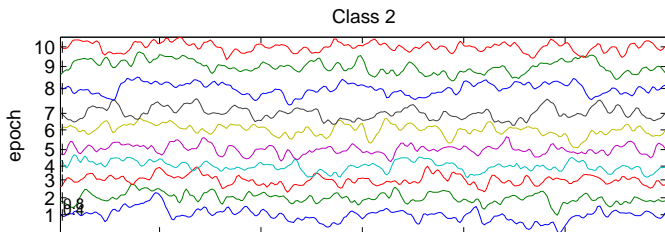
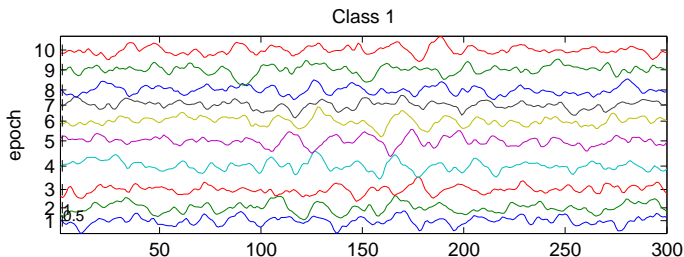
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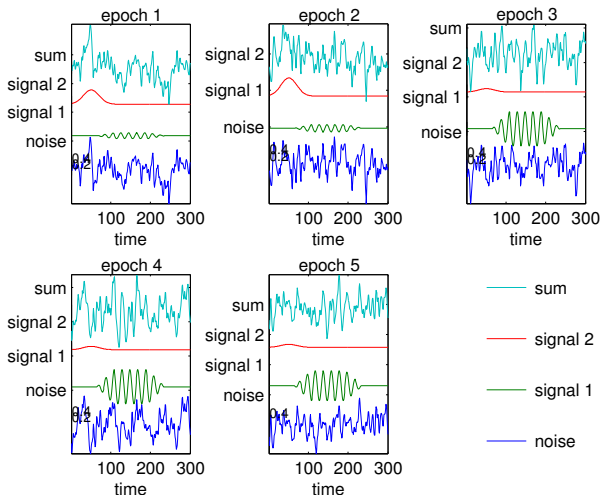
Introduction to BCI signal pre-processing

- ▶ BCI data = signal + noise
- ▶ usually the signal is much smaller than the noise
- ▶ signal processing techniques are used to suppress the noise to make the signal detectable
- ▶ most common technique is to use a spectral decomposition of the signal

Example Signals: Simulated 1-ch BCI



Simulated 1-ch BCI Signals



Spectral Decomposition of Signals

- Re-represents the data as a sum of sine and cosine terms

$$x(t) = \sum_{\nu=0:1/T:F/2} f_{\cos}(\nu) \cos(2\pi\nu t) + f_{\sin}(\nu) \sin(2\pi\nu t)$$

- or equivalently, as sum of **phase**-shifted sines

$$x(t) = \sum_{\nu=0:1/T:F/2} f_A(\nu) \sin(2\pi\nu t + f_{\omega}(\nu))$$

- more commonly written using complex numbers as:

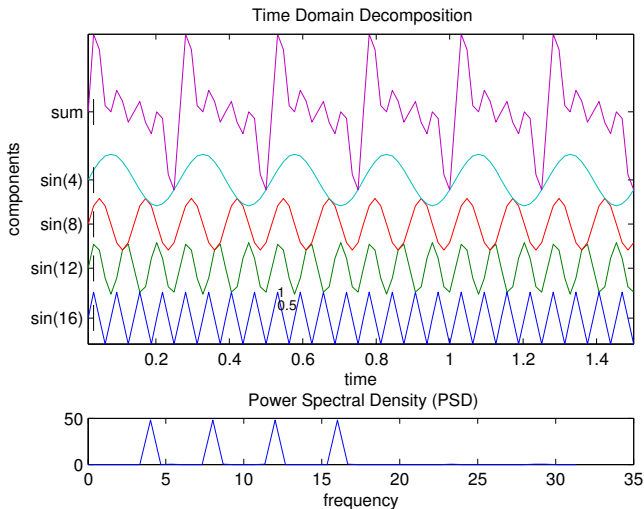
$$x(t) = \sum_{\nu=-F/2:(1/T):F/2} f(\nu) \exp(i2\pi\nu t)$$

where $f(\nu) = f_A(\nu) \exp(\text{sgn}(\nu)if_{\omega}(\nu))$

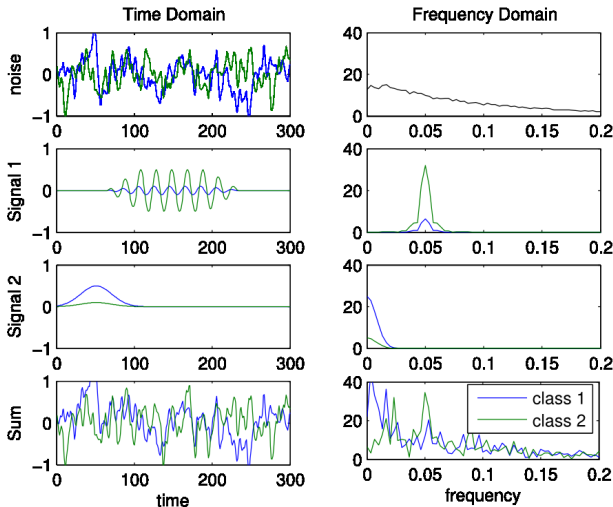
- Frequency Resolution: determined by signal duration, $\Delta f = 1/T$
- Frequency Range: determined by sampling rate, $0 : F/2$



Spectral decomposition of signals - easy



Spectral decomposition of signals - sim data



Time-Frequency Decompositions

Time-Frequency Decomposition

Given information about the **magnitude** (and possibly **phase**) of the signal at a particular **frequency** and **time**.

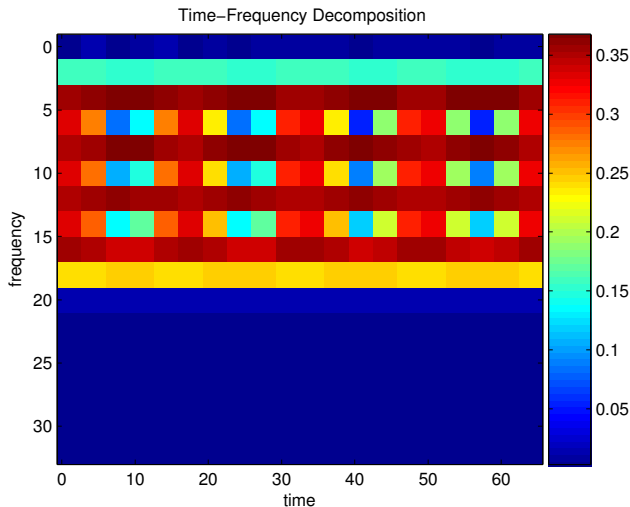
Many possible ways of computing this:

- ▶ Short-time-Fourier-transform (STFT)
- ▶ Hilbert Transform
- ▶ Multi-Taper-Method
- ▶ Wavelet-Transform

All essentially the same and only talk about the STFT here.

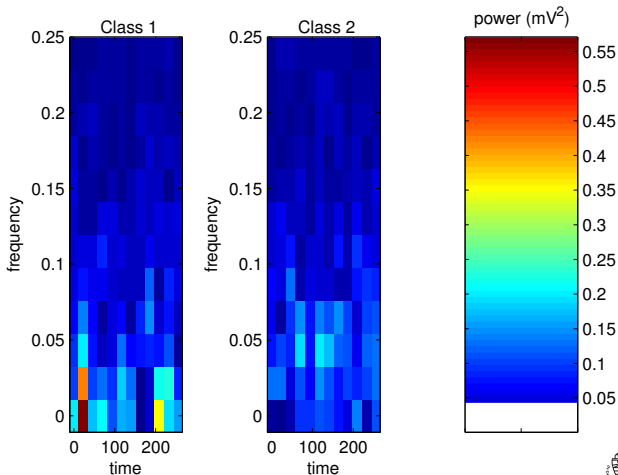


Time-Frequency Decomposition - easy



Time-Frequency Decomposition - sim data

Time-Frequency Decomposition

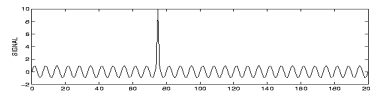


Time-Frequency trade-offs

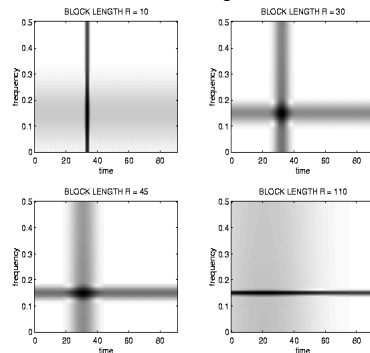
Time-Frequency trade-off

Time-Resolution (ΔT) and Frequency-Resolution (ΔF) are **inversely** related to each other by: $\Delta f = 1/\Delta T$.

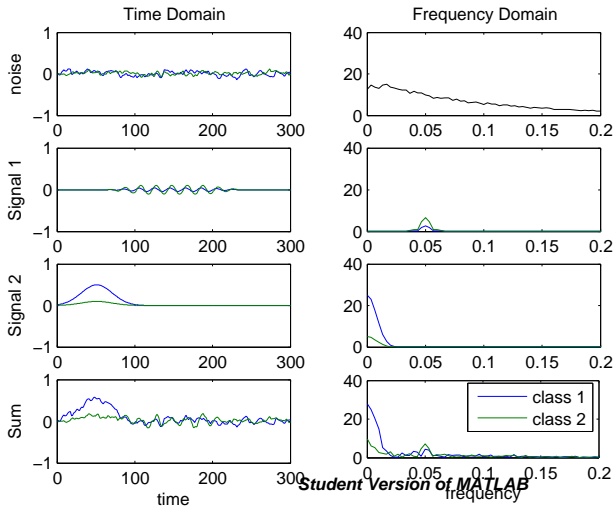
- ▶ Increasing time resolution decrease frequency resolution
- ▶ Increasing frequency resolution decreases time resolution
- ▶ Intuitively \rightarrow need >1 cycle to reliably identify phase+amplitude



Source Signal

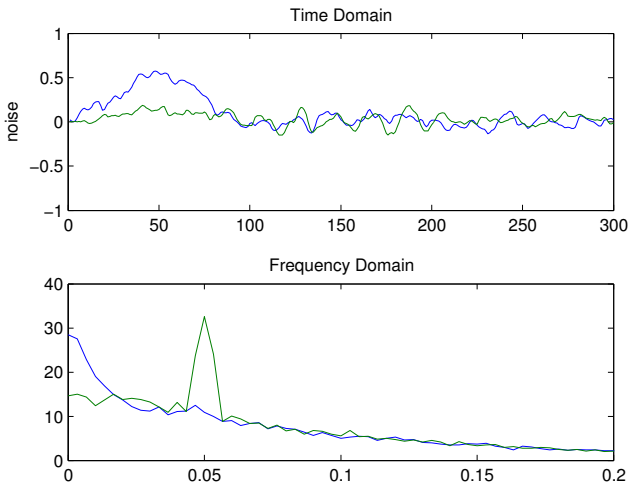


Averaging signals



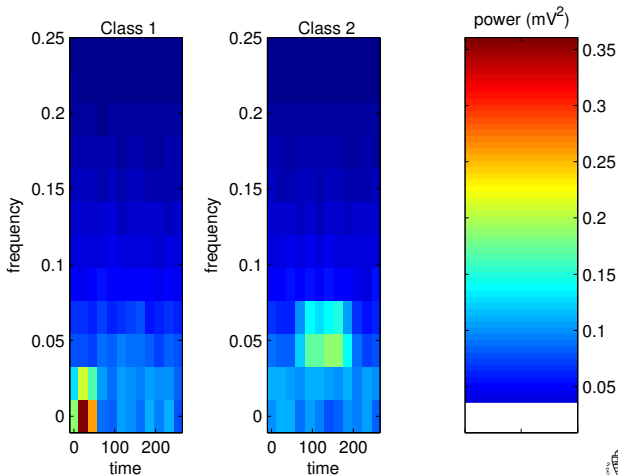
Student Version of MATLAB

Averaging: Time-domain vs. Freq-domain

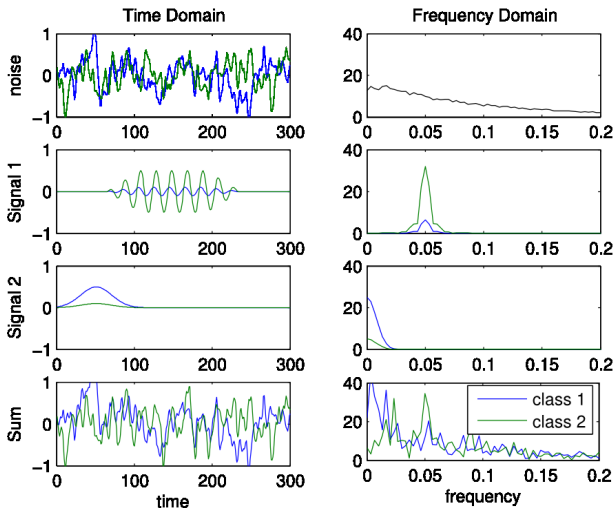


Averaging: Time-Frequency-Domain (sim-data)

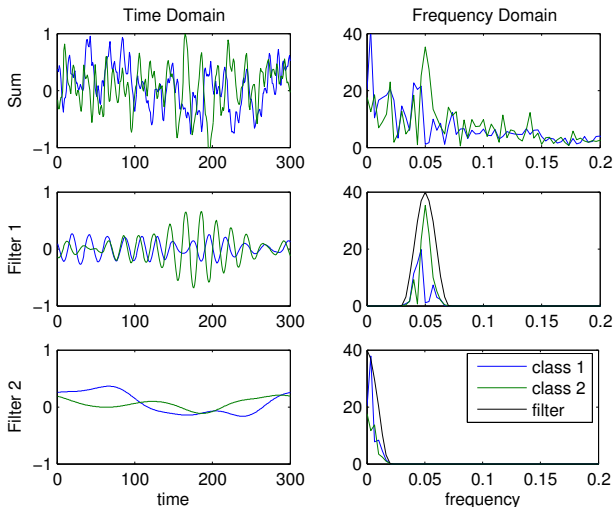
Average Time-Frequency Decomposition



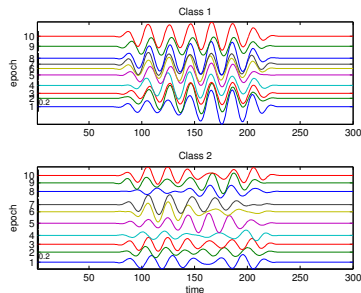
Spectral-filtering



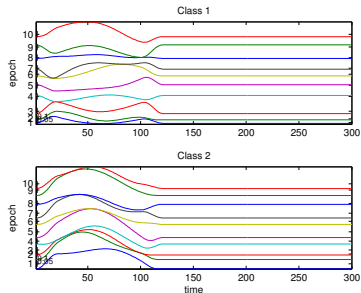
Spectral-filtering (2)



Spectral-filtering



Spectral filter 1



Spectral filter 2

Summary signal filtering

- ▶ signal filtering is used to attenuate background noise...
- ▶ ... and hence make the target signal easier to detect

Most commonly used filters:

1. temporal – focus 'when' signal is expected
2. spectral – focus on frequency signal is expected to have
3. spatial – focus on where signal is expected to come from
4. averaging – special type of temporal which attenuates uncorrelated noise.

Note:

To use design optimal filters need to know the expected characteristics of the target signal (and noise).

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