

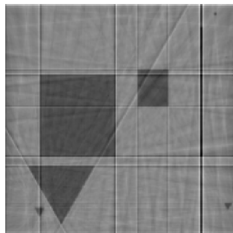
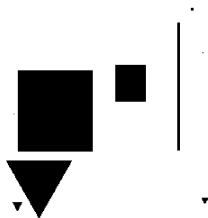
# Using Futhark for SIRT

Mette Bjerg Lindhøj

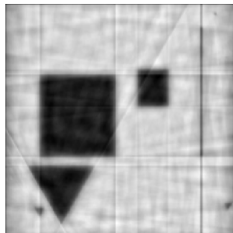
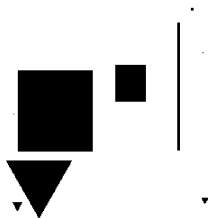
University of Copenhagen

17/12/2018

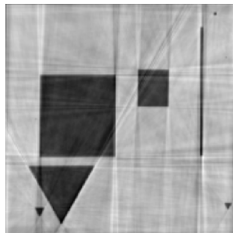
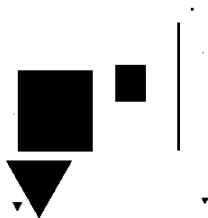
MSE: 0.21, SSIM: 0.60



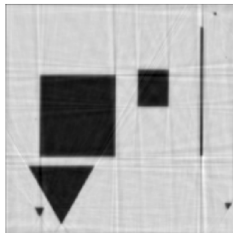
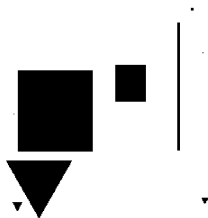
MSE: 0.08, SSIM: 0.69



MSE: 0.09, SSIM: 0.66



MSE: 0.05, SSIM: 0.73



# SIRT

Solve the problem:

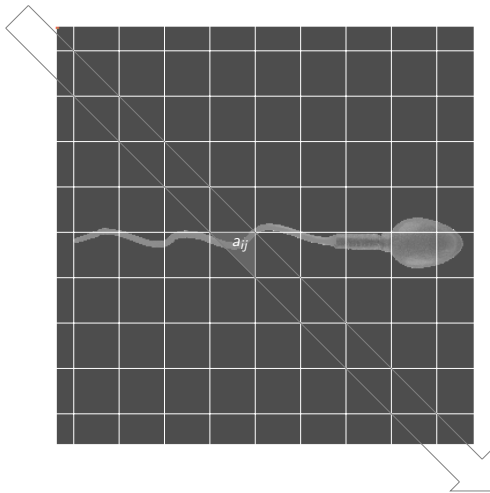
$$\mathbf{f}^* = \operatorname{argmin}_{\mathbf{f}} \|\mathbf{p} - \mathbf{A}\mathbf{f}\| \quad (1)$$

iteratively using this update step:

$$\mathbf{f}^n = \mathbf{f}^{(n-1)} + \mathbf{C}\mathbf{A}^T \mathbf{R}(\mathbf{p} - \mathbf{A}\mathbf{f}^{(n-1)}), \quad (2)$$

where  $\mathbf{C}$  and  $\mathbf{R}$  are the diagonal matrices containing the inverse column and row sums of the system matrix respectively.

# The system matrix



# The problem is in the size

- ▶ Consider reconstructing a single slice of a volume from a detector of size  $n \times n$
- ▶ The number of rays is  $n$
- ▶ The number of angles is  $\frac{n \cdot \pi}{2}$
- ▶ A typical value for  $n$  is 2048
- ▶ In semi sparse format the matrix will take up  $2 \cdot 4 \cdot 2048 \cdot \lceil \frac{2048 \cdot \pi}{2} \rceil \cdot (2 \cdot 2048 - 1) \approx 216GB$

# System matrix computation

```
1 for ray in rays
2     for i=-halfsize; i < halfsize; i++
3         (l1,pixel1) = intersection1 ray i
4         (l2,pixel2) = intersection2 ray i
5         A[ray][pixel1] = l1
6         A[ray][pixel2] = l2
```

Figure:  $W(r, n) = O(r \cdot n)$ ,  $D(r, n) = O(1)$

```
1 for pixel in pixels:
2     for angle in angles:
3         rays = rays that are within pixel
4         for ray in rays:
5             l = intersection ray pixel
```

Figure:  $W(r, n) = O(r \cdot n)$ ,  $D(r, n) = O(1)$

# Benefits of Futhark

```
1 % Input: sparse system matrix A, data b.
2 % Output: SIRT reconstruction x.
3 x = zeros(d * d, 1);
4 [rows cols] = size(A);
5 C = sparse(1 : cols, 1 : cols, 1 ./ sum(A));
6 R = sparse(1 : rows, 1 : rows, 1 ./ sum(A')));
7 CATR = C * A' * R;
8 for i = 1 : 100
9     x = x + CATR * (b - A * x);
10 end
```

Figure: Example of high level implementation

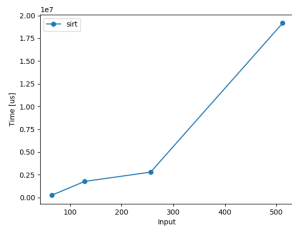
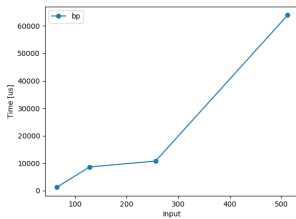
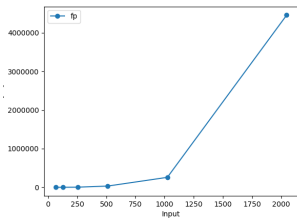


```

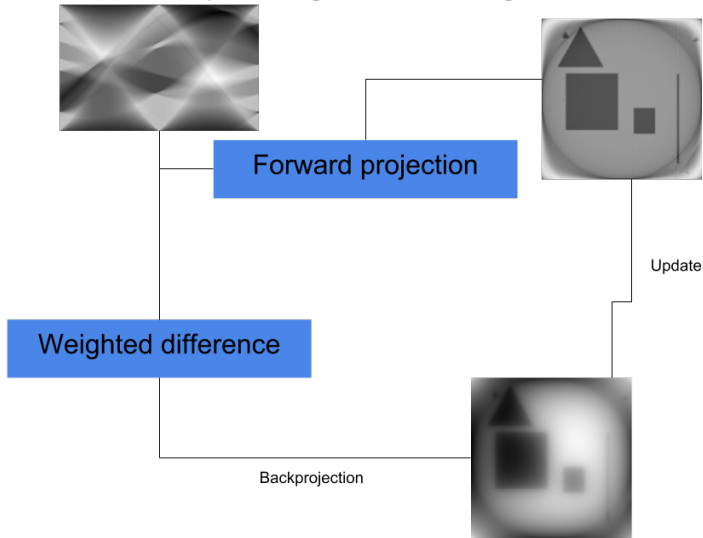
1 unsigned int blockStart = 0;
2 unsigned int blockEnd = 0;
3 bool blockVertical = false;
4 for (unsigned int a = 0; a <= dims.iProjAngles; ++
    a) {
5     bool vertical = false;
6     if (a != dims.iProjAngles)
7         vertical = (fabsf(angles[a].fRayX) <= fabsf(
            angles[a].fRayY));
8     if (a == dims.iProjAngles || vertical !=
        blockVertical) {
9
10        blockEnd = a;
11        if (blockStart != blockEnd) {
12            dim3 dimGrid((blockEnd-blockStart+
                g_anglesPerBlock-1)/g_anglesPerBlock,
13                        (dims.iProjDets+g_detBlockSize
                            -1)/g_detBlockSize); //
                            angle blocks, detector
                            blocks...

```

Figure: Example of CUDA implementation



Input: sinogram and initial guess





Hao Gao.

Fast parallel algorithms for the x-ray transform and its adjoint.  
*Medical physics*, 39(23127102):7110–7120, November 2012.



Y. Long, J. A. Fessler, and J. M. Balter.

3d forward and back-projection for x-ray ct using separable footprints.  
*IEEE Transactions on Medical Imaging*, 29(11):1839–1850, Nov 2010.



F. Natterer.

*The Mathematics of Computerized Tomography*.  
Society for Industrial and Applied Mathematics, 2001.



Z. Xue, L. Zhang, and J. Pan.

A new algorithm for calculating the radiological path in ct image reconstruction.  
*In Proceedings of 2011 International Conference on Electronic Mechanical Engineering and Information Technology*, volume 9, pages 4527–4530, Aug 2011.