



THE OHIO STATE UNIVERSITY

Denoising E-Textile Sensors for Real-World Kinematics Monitoring

Yuxuan Han, Vigyanshu Mishra, and Asimina Kiourti

han.1454@osu.edu, mishra.186@osu.edu, kiourti.1@osu.edu

*ElectroScience Laboratory, Dept. of Electrical and Computer Engineering
The Ohio State University*

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- **Introduction**
 - Motivation and state-of-the-art
- **Operating Principle of E-Textile Kinematics Sensors**
- **Measuring the Fabric Drift Error**
 - Experimental setup
 - Measurement observations
 - Model analysis
- **Correcting the Fabric Drift Error**
 - STEP 1: Initial condition calibration
 - STEP 2: Machine learning aided calibration
- **Conclusion and Future Work**



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Motivation for Motion Capture “In-The-Wild”



Healthcare

- Detection and Rehabilitation
- Parkinson's, TBI, Concussion, Falls etc.



Sports

- Optimize fitness and prevent injuries
- Rehabilitate in real-time, faster recovery.



Healthy Individuals

- Maintain fitness and create baseline data.
- Pre-onset detection and relevant measures.



Human-Machine Interface, and Animation

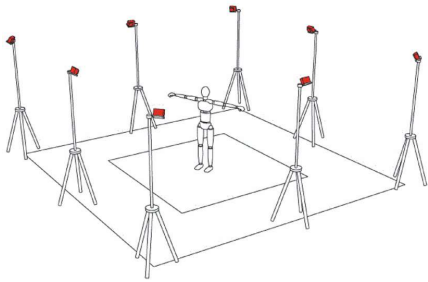
Widespread and significant impact



Biomedical Research



State-of-the-art Motion Capture Technologies



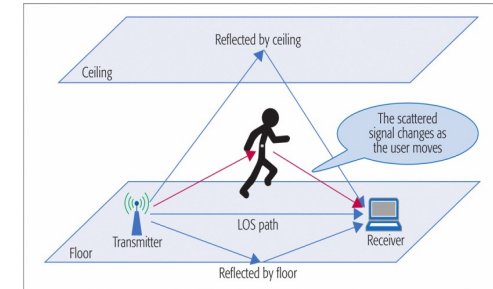
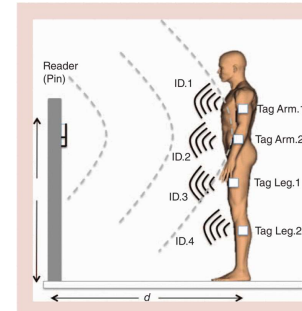
Motion Capture Labs

Restricted to contrived settings



IMUs

Not reliable due to drift issues



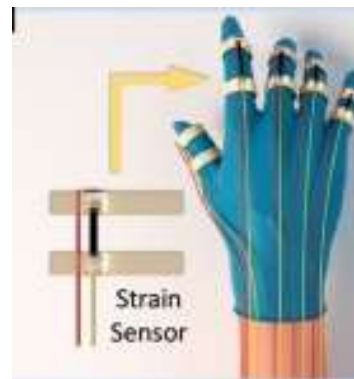
Electromagnetics-Based

Restricted and limited to activity classification



Time of Flight

Line of sight issues



Bending Sensors

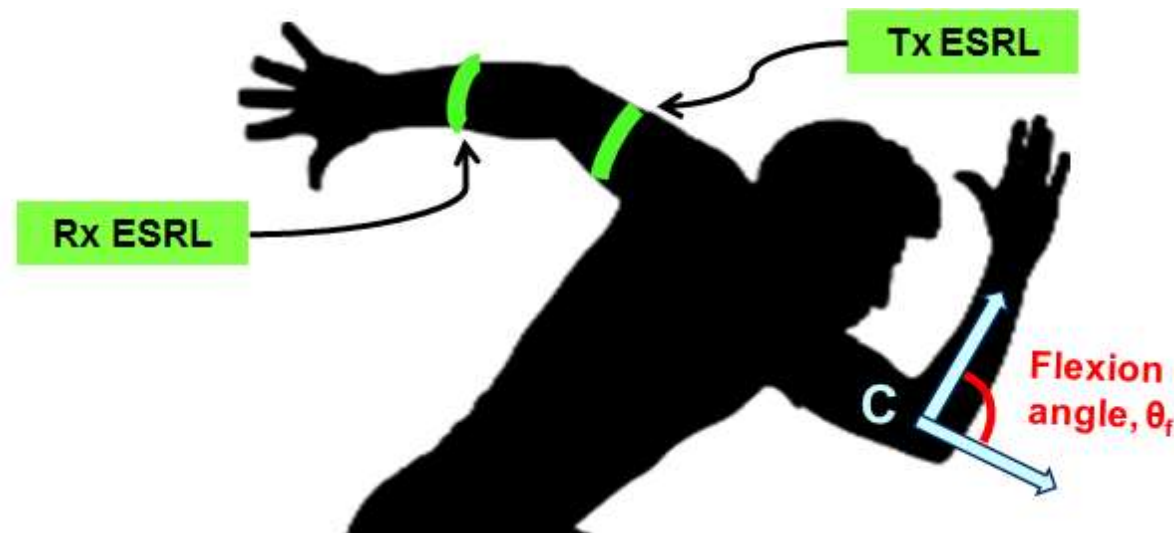
Restrict natural motion and limited by number of cycles of use.

- [1] PC: Takeuchi et al., "Web-based avatar represented lecture viewer toward interactive e-lecture performed by 3d avatar," in 2015 IEEE Global Engineering Education Conference (EDUCON), Mar. 2015, pp. 283–286
- [2] PC: Gonz lez-Villanueva et al., "Design of a wearable sensing system for human motion monitoring in physical rehabilitation," Sensors, vol. 13, no. 6, pp. 7735–7755, Jun. 2013.
- [3] PC: Wang et al., "Wi-fi CSI-based behavior recognition: From signals and actions to activities," IEEE Communications Magazine, vol. 56, no. 5, pp. 109–115, May 2018.
- [4] PC: Amendola et al., "Movement detection of human body segments: Passive radio-frequency identification and machine-learning technologies," IEEE Antennas and Propagation Magazine, vol. 57, no. 3, pp. 23–37, Jun. 2015.
- [5] Y. Qi, C. B. Soh, E. Gunawan, K.-S. Low, and A. Maskooki, "A novel approach to joint flexion/extension angles measurement based on wearable UWB radios," IEEE Journal of Biomedical and Health Informatics, vol. 18, no. 1, pp. 300–308, Jan. 2014.
- [6] C. Li, Y.-L. Cui, G.-L. Tian, Y. Shu, X.-F. Wang, H. Tian, Y. Yang, F. Wei, and T.-L. Ren, "Flexible CNT-array double helices strain sensor with high stretchability for motion capture," Scientific Reports, vol. 5, no. 1, pp. 1–8, Nov. 2015

Loop-Based Textile Kinematics Sensors Developed in our Group

Advantages

- Real-time
- Non-contrived settings
- Seamless
- Unobtrusive
- Unrestricted natural movement
- Robust
- Reliable
- Injury Safe



ESRL: Electrically Small Resonant Loop (ESRL)

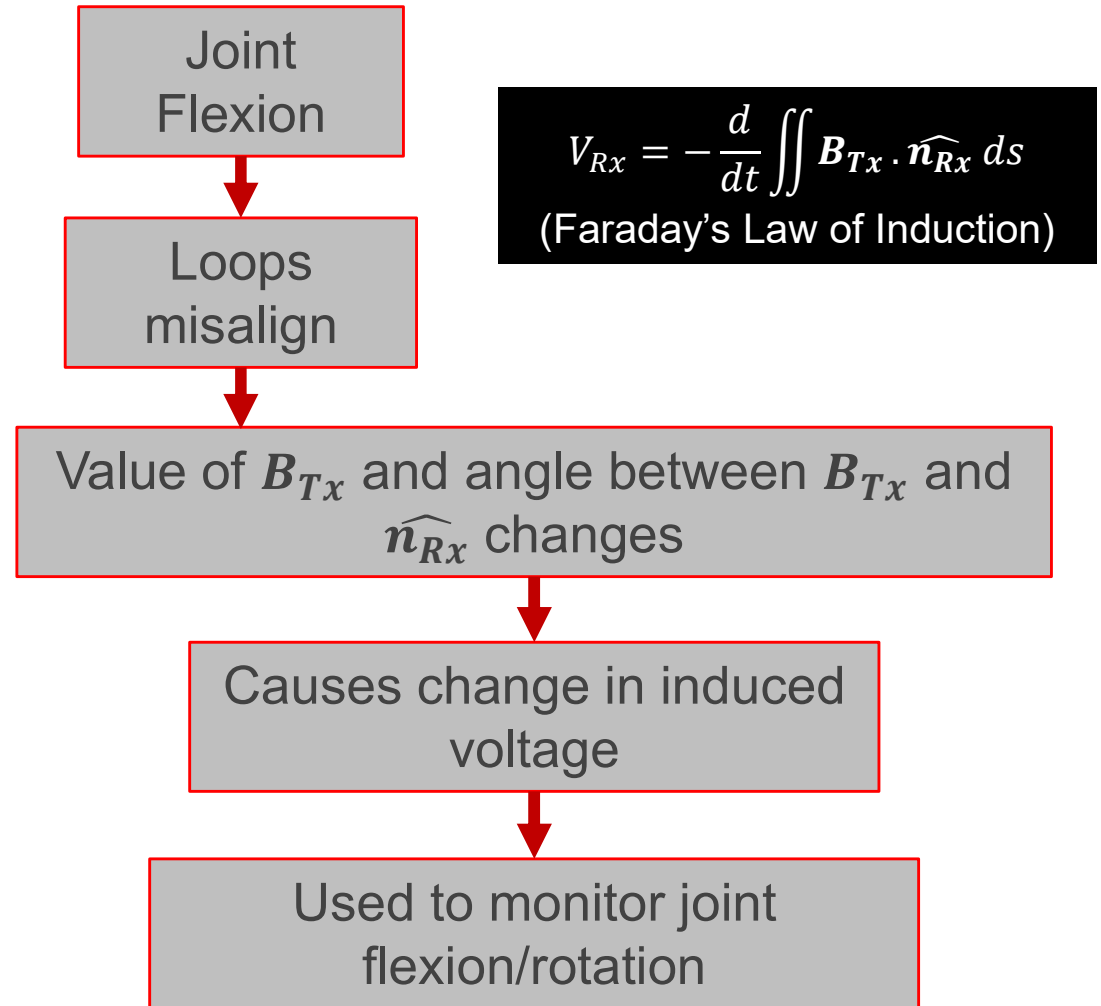
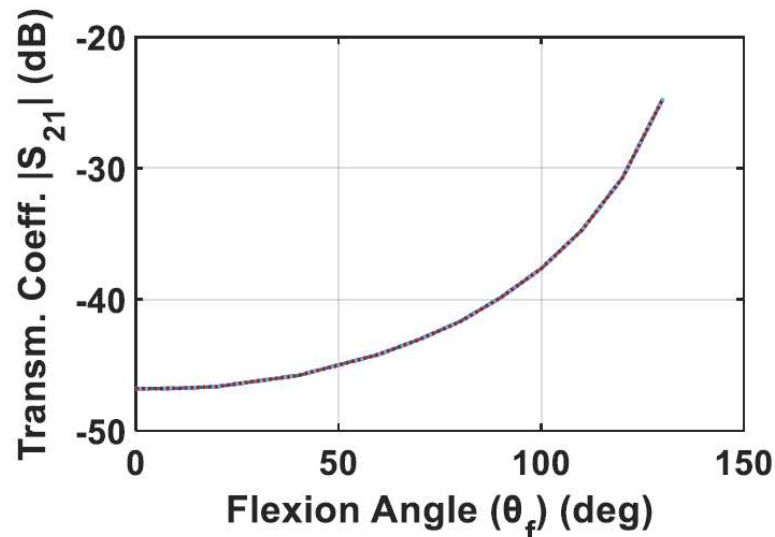
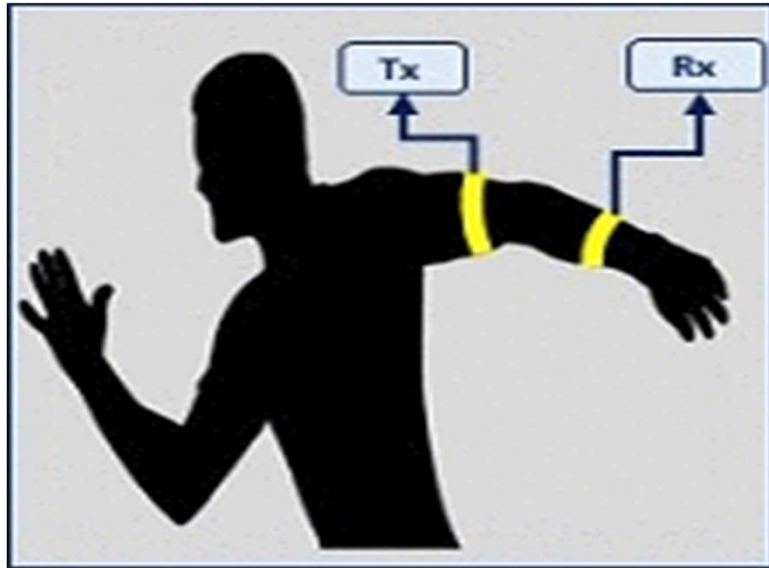
V. Mishra and A. Kiourti, "Wrap-Around Wearable Coils for Seamless Monitoring of Joint Flexion," *IEEE Transactions on Biomedical Engineering*, vol. 66, no. 10, pp. 2753–2760, Oct. 2019

V. Mishra and A. Kiourti, "Wearable Electrically Small Loop Antennas for Monitoring Joint Flexion and Rotation," *IEEE Transactions on Antennas and Propagation*, vol. 68, no. 1, pp. 134–141, Jan. 2020



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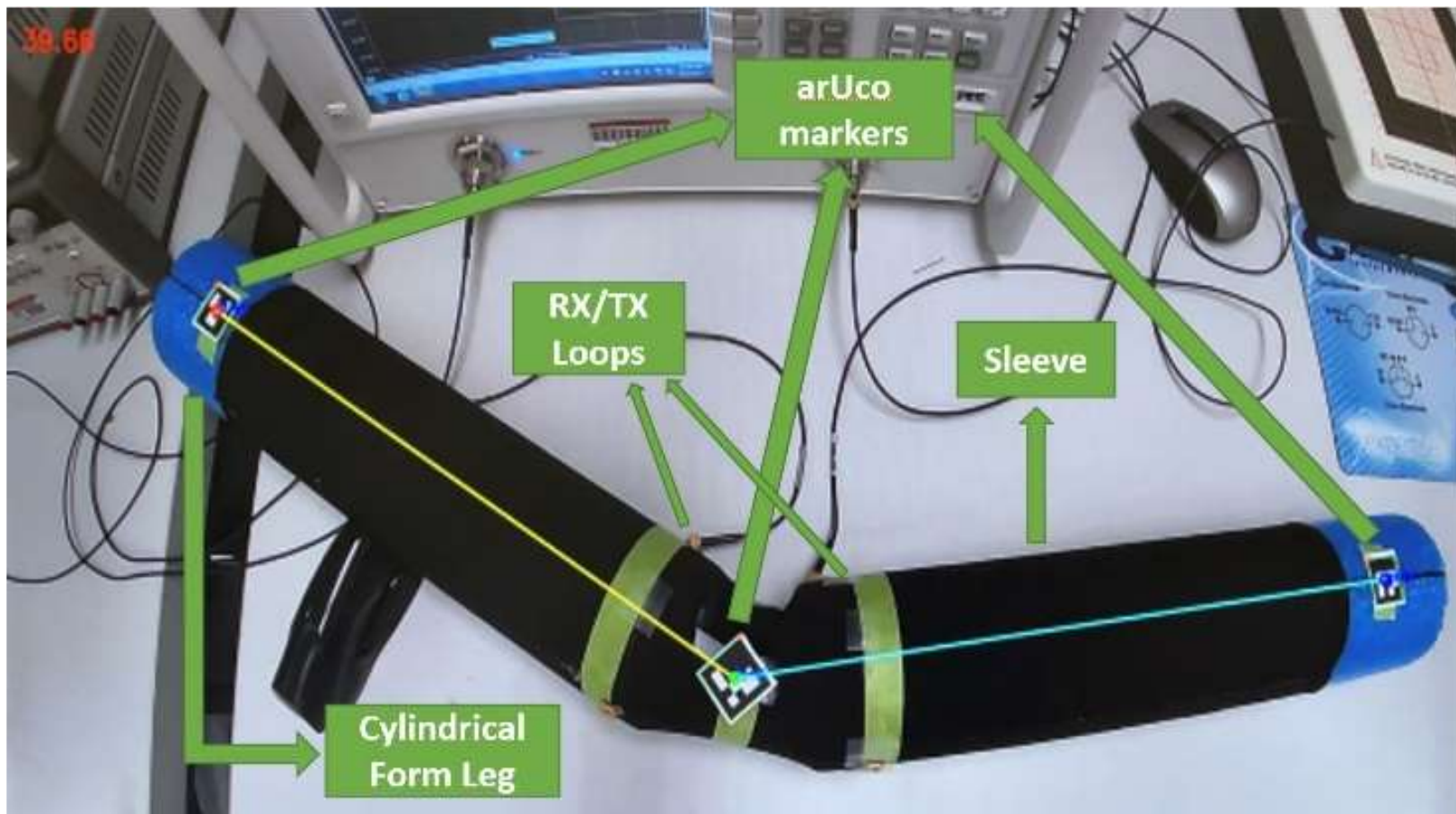
Operating Principle of E-Textile Kinematic Sensors



$$V_{Rx} = -\frac{d}{dt} \iint \mathbf{B}_{Tx} \cdot \hat{\mathbf{n}}_{Rx} ds$$

(Faraday's Law of Induction)

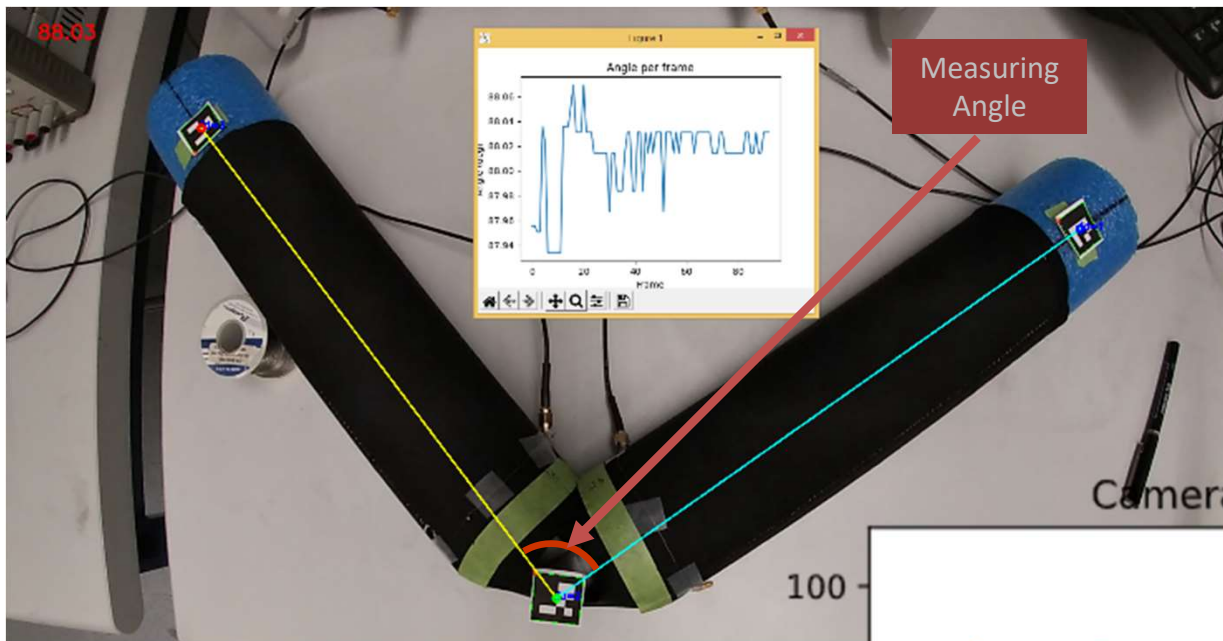
Experimental Setup



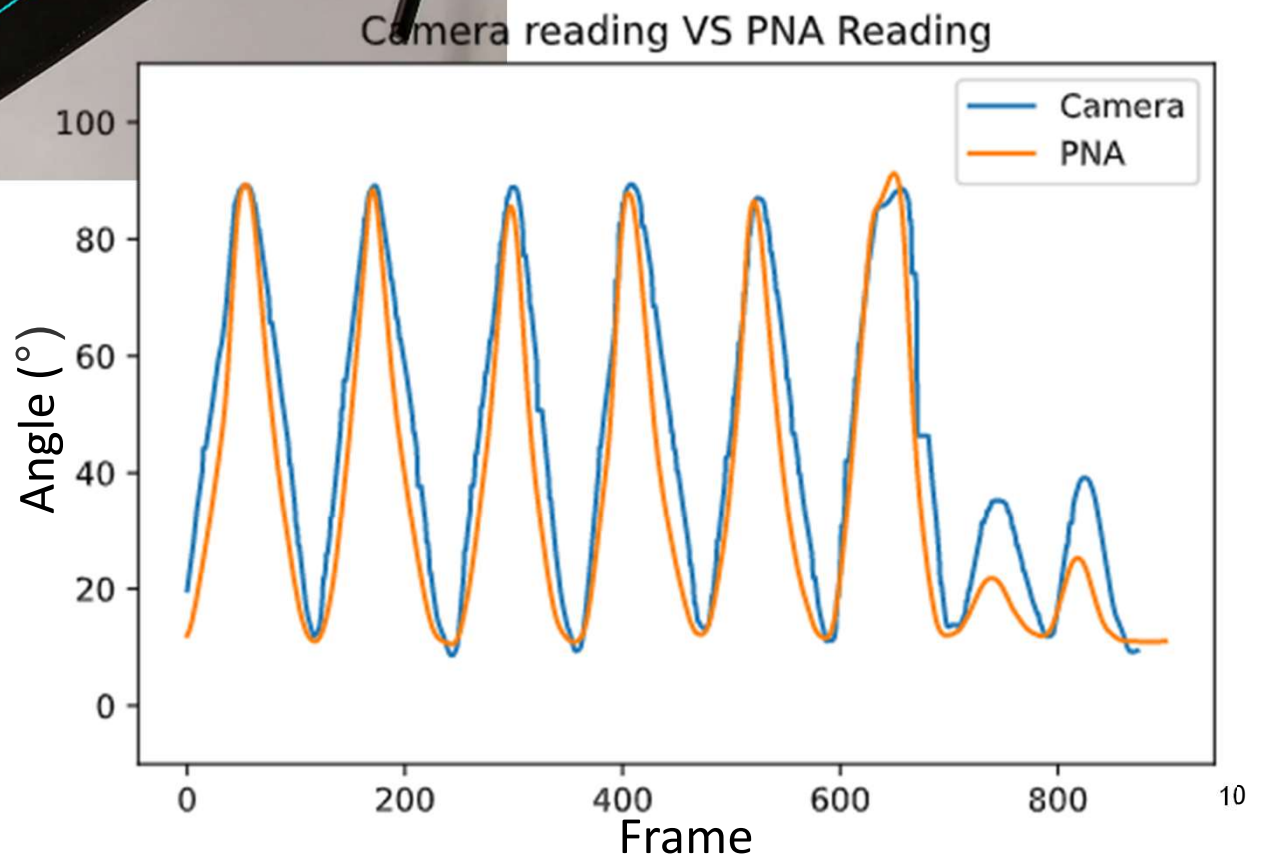
- Rotatable Styrofoam leg with loops on stretchy fit sleeve
- ArUco markers & computer vision for “gold standard” joint angle measurements
- Network analyzer for $|S_{21}|$ readings



Data Collection Sample



Dynamic measurement of angle vs. time/frame

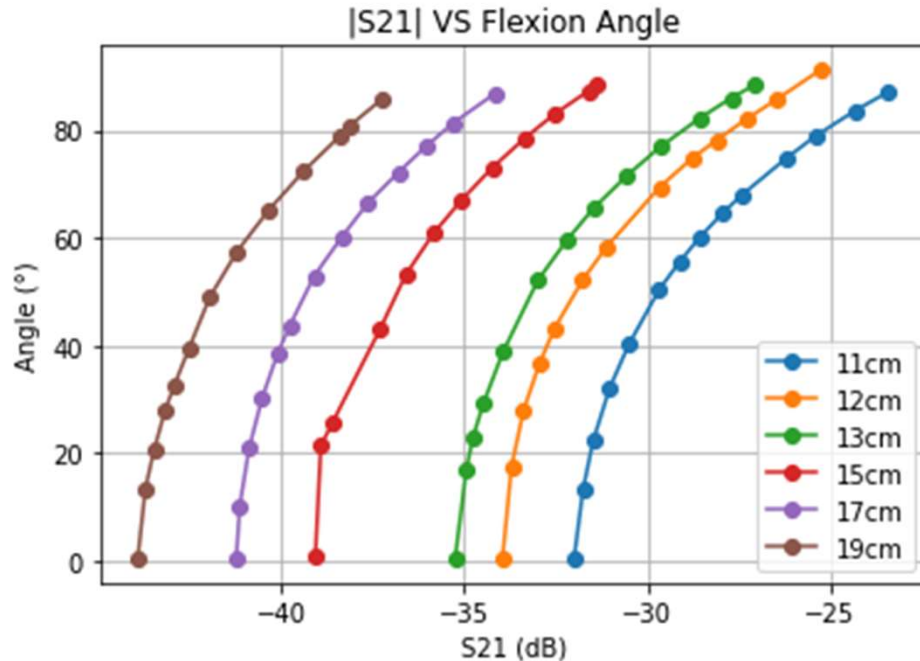




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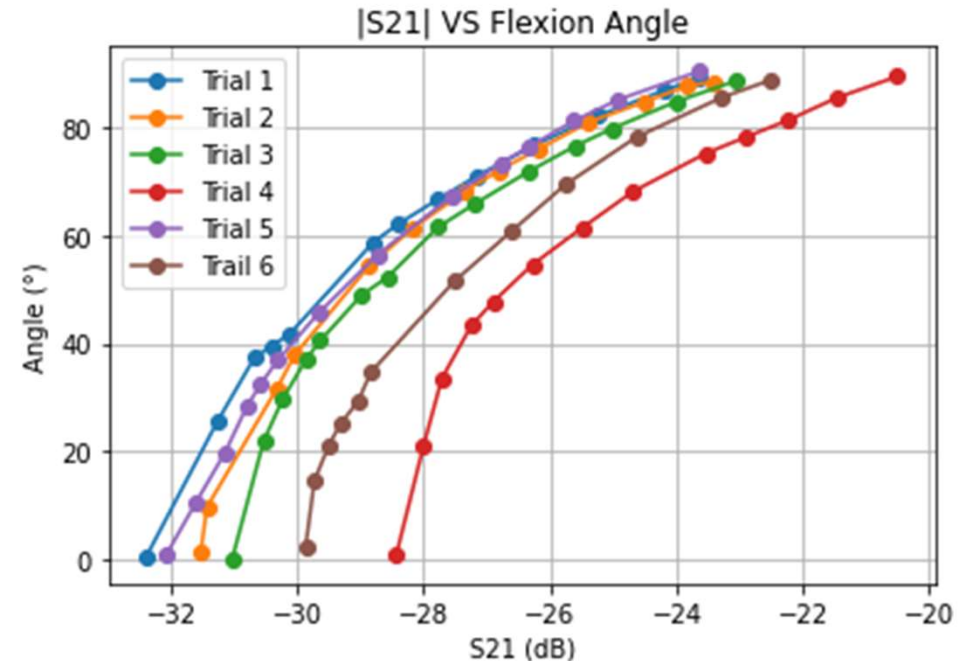


Fabric Drift Error: Measurement Observations



$|S_{21}|$ VS Angle **WITHOUT**
considering sleeve stretches

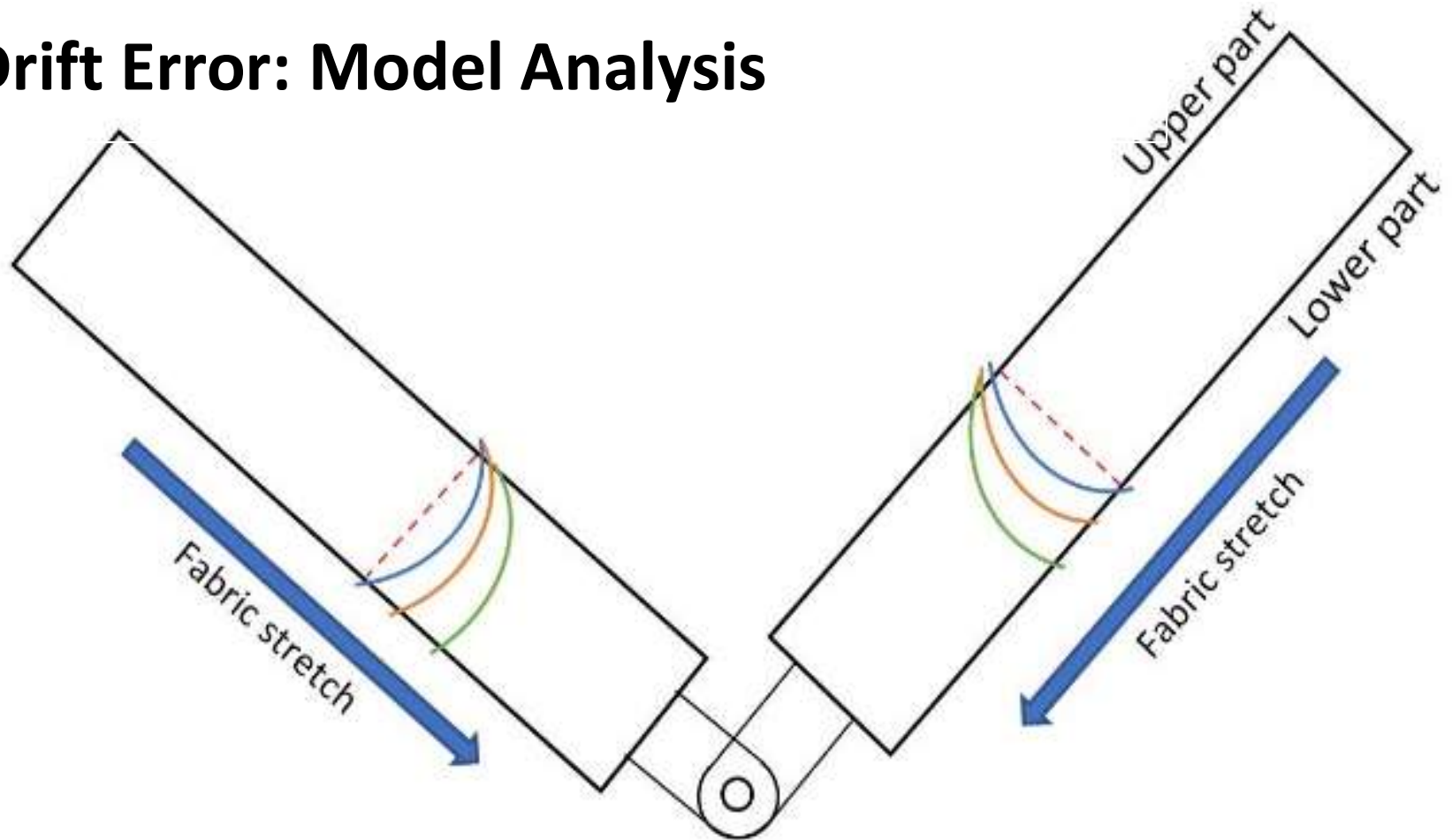
- Predictable
- Curvature hardly changes under different conditions
- Can shift left/right based on $|S_{21}|$ at 0°



$|S_{21}|$ VS Angle **WITH**
considering sleeve stretches

- Hard to predict
- Curvature changes significantly under different condition
- Cannot just shift left/right

Fabric Drift Error: Model Analysis



Fabric stretches unevenly with joint flexion, causing the loops' relative position to change over time.

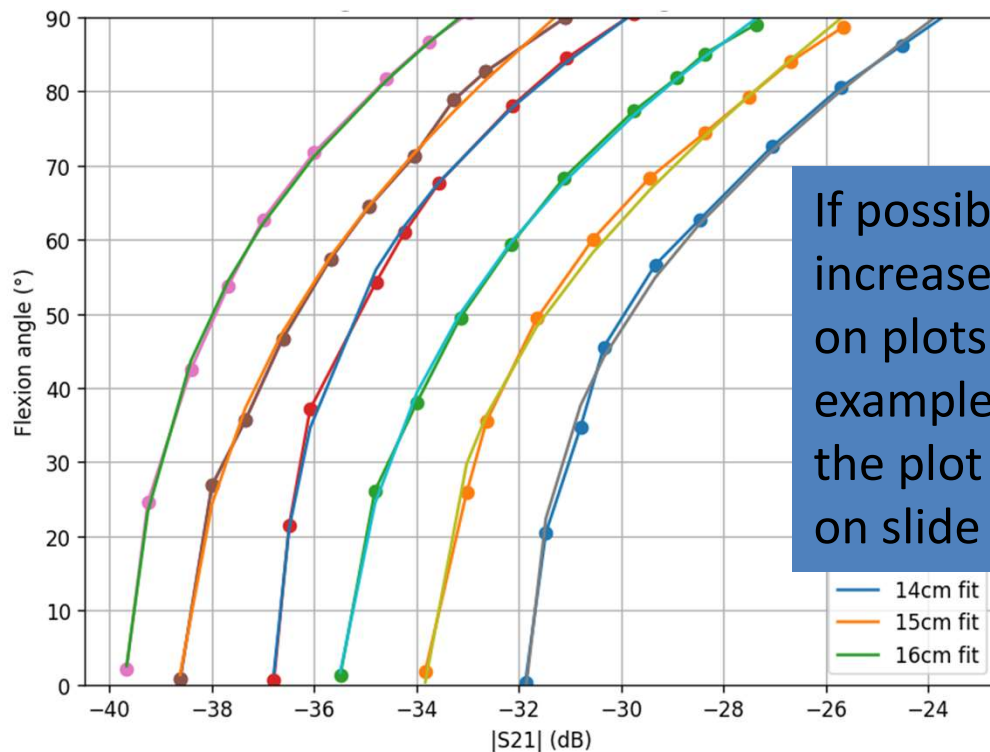
How can we calibrate out this error?



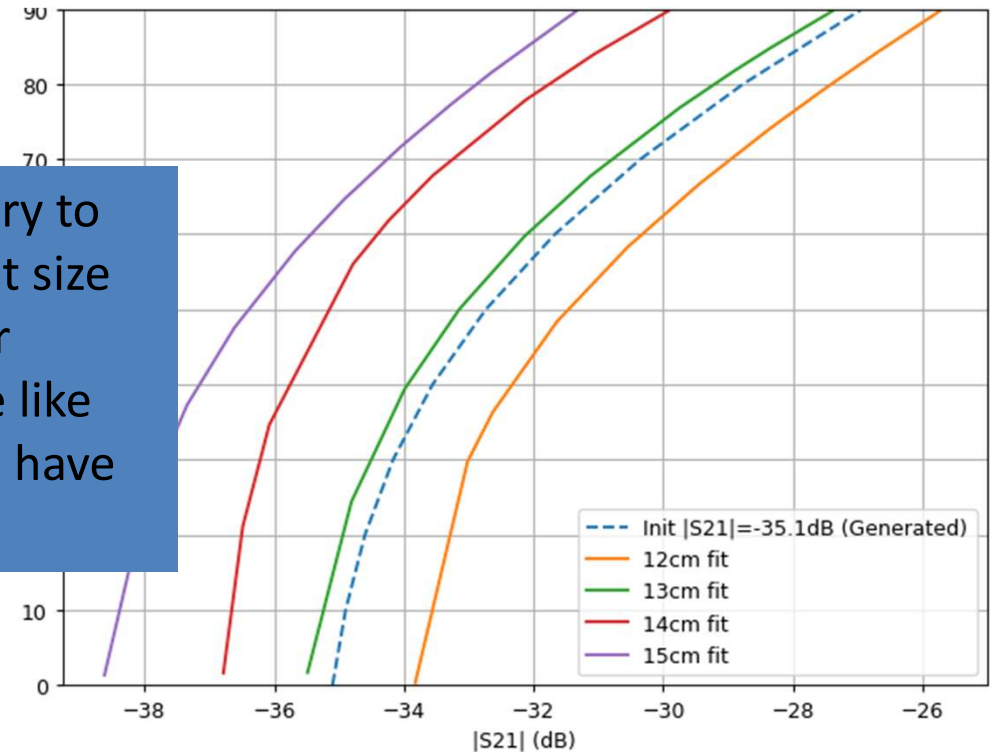
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STEP 1: Initial Condition Calibration



If possible, try to increase font size on plots. For example the like the plot you have on slide 8



Collect $|S_{21}|$ VS Angle w/o considering sleeve stretches → convert into logarithmic equation

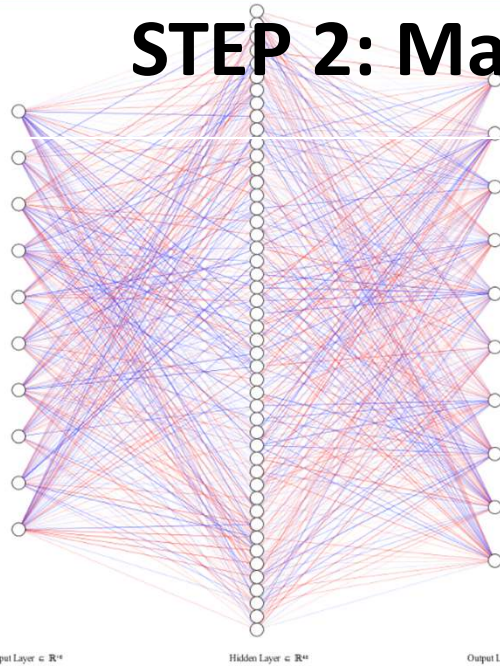


Generate $|S_{21}|$ VS Angle curves w/o considering sleeve stretches based on their $|S_{21}|$ value @ 0° (initial condition)

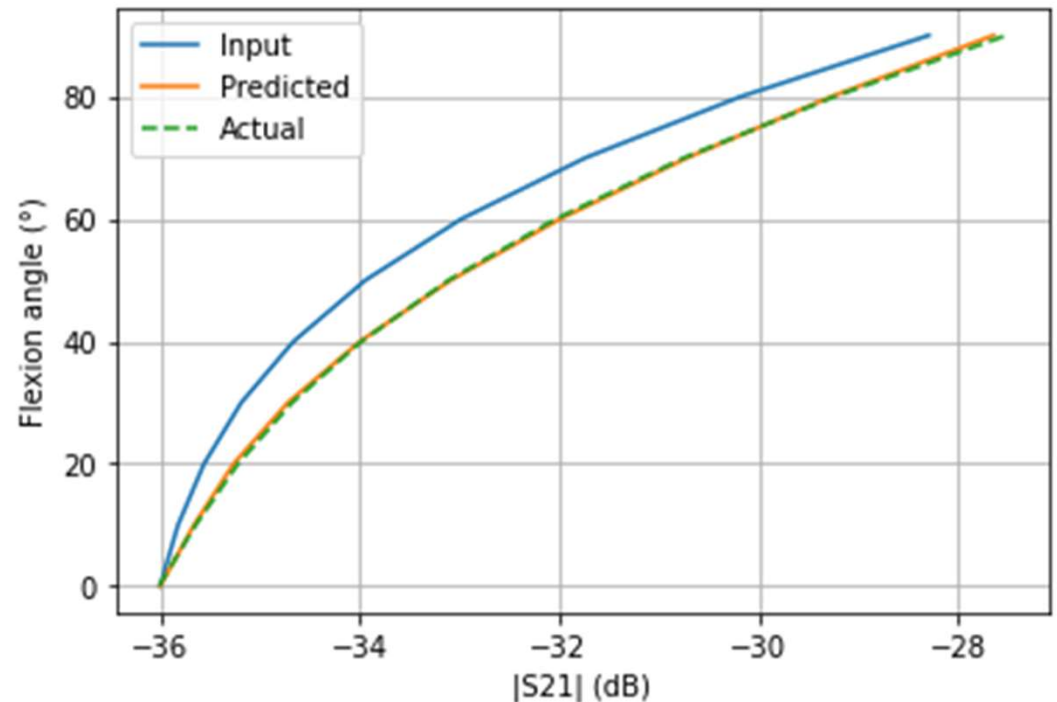
$$\hat{y} = a \cdot \log_{10}x + b \cdot x + d$$



STEP 2: Machine Learning Aided Calibration



10 nodes for input and output (10 data points of $|S_{21}|$ VS Flexion Angle curve), 48 nodes for hidden layer

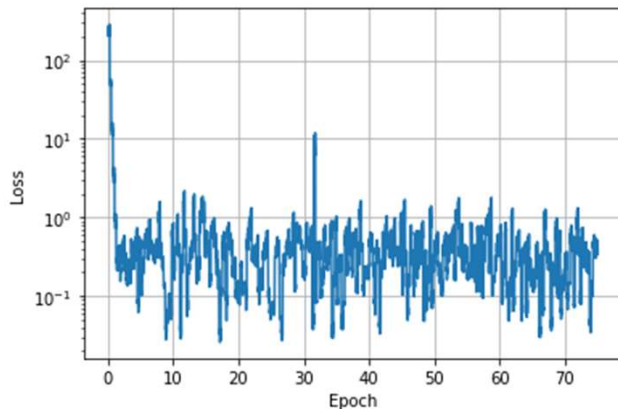


Using trained network to get calibrated $|S_{21}|$ VS Flexion Angle curve at a specific initial condition (-36dB @ 0°).

Error after calibration $\leq 0.3^\circ$

Input = $|S_{21}|$ VS Flexion Angle w/o sleeve

Predicted = $|S_{21}|$ VS Flexion Angle w/ sleeve



Test loss after 300 epochs
(2000 data samples), $lr=0.005$



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- **Conclusion**

- Fabric drift can be detrimental in the operation of loop-based textile kinematics sensors
- Proposed 2-step methodology can calibrate out this error
- Preliminary results show errors below 0.5°

- **Future Work**

- Adapt to dynamic motion measurements (i.e., joint flexing during sensor sampling)
- Improve accuracy



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Thank you!

Questions?

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