A thermodynamic framework for modelling membrane transporters using bond graphs

Michael Pan¹, Peter J. Gawthrop¹, Kenneth Tran², Joseph Cursons^{3,4}, Edmund J. Crampin^{1,5,6,*}

¹Systems Biology Laboratory, School of Mathematics and Statistics, and Department of Biomedical Engineering, Melbourne School of Engineering, University of Melbourne, Parkville, Victoria 3010, Australia

²Auckland Bioengineering Institute, University of Auckland

³Bioinformatics Division, Walter and Eliza Hall Institute of Medical Research, Parkville, Victoria 3052, Australia

⁴Department of Medical Biology, School of Medicine, University of Melbourne, Parkville, Victoria 3010, Australia

⁵School of Medicine, Faculty of Medicine, Dentistry and Health Sciences, University of Melbourne, Parkville, Victoria 3010

⁶ARC Centre of Excellence in Convergent Bio-Nano Science and Technology, Melbourne School of Engineering, University of Melbourne, Parkville, Victoria 3010, Australia

*Corresponding author. Email: edmund.crampin@unimelb.edu.au

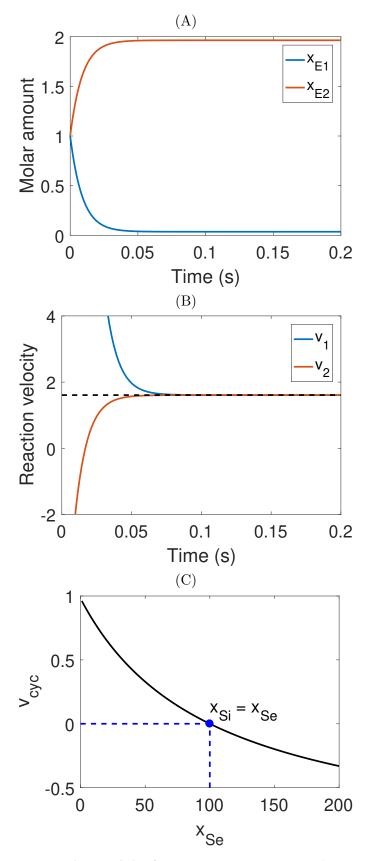


Figure 1: Enzyme cycle model. A passive transporter can be modelled using the enzyme cycle $E_1 + S_i \rightleftharpoons E_2 \rightleftharpoons E_2 + S_e$. We simulate this model, and plot how the enzyme states (A) and reaction velocities (B) change with respect to time. (C) The transporter reaches a steady state, with the direction of steady-state transport dictated by the concentration gradient of the substrate.

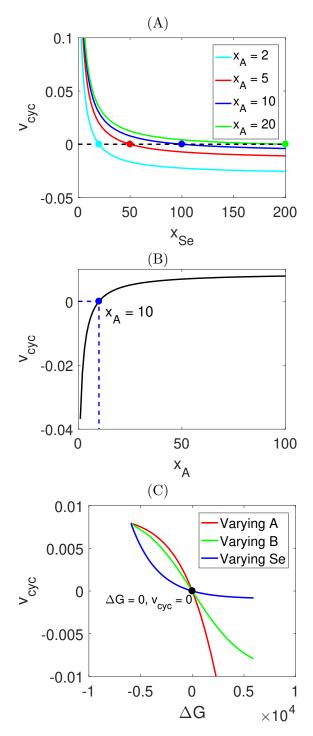


Figure 2: Coupled transport. In order for a transporter to move a substrate against a concentration gradient, it must couple the transport to a process that generates sufficient energy for the transport to occur. Here we model a transporter that couples the transport of substrate to another biochemical reaction $A \rightleftharpoons B$, giving rise to the overall reaction $S_i + A \rightleftharpoons S_e + B$. We simulate this system to steady state. The plots show that the amount of A affects the ability of the transporter to move a substrate against a chemical gradient, shifting the equilibrium point to a higher concentration of Se (A) and increasing the cycling rate (B). (C) By modelling this system as a bond graph, fundamental thermodynamic constraints are captured, therefore the pump only operates in the direction of decreasing chemical potential, and stops cycling at equilibrium.

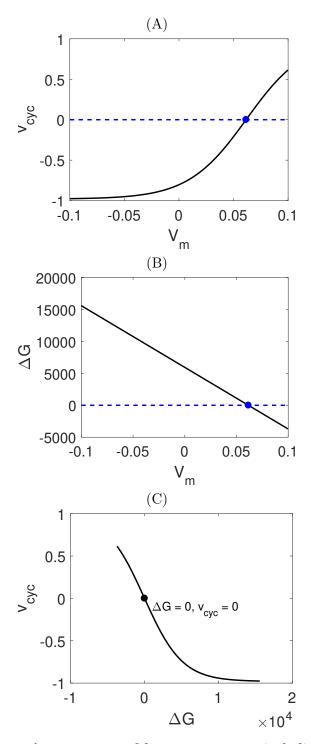


Figure 3: Electrogenic transport. Many transporters, including ion transporters, move charged species across a membrane that is charged. For these transporters, the membrane potential contributes to the thermodynamics and kinetics of the system. Because bond graphs are domain-independent, they are able to model the interaction between chemical and electrochemical power in electrogenic systems. Here we simulate the transporter model $E_1 + S_i^+ \rightleftharpoons E_2 \rightleftharpoons E_2 + S_e^+$, where the substrate is charged. (A) A plot of the cycling rate against voltage shows the bond graph model captures the equilibrium point (Nernst potential) of this transporter. (B) The membrane voltage has a linear contribution to the Gibbs free energy of the transporter. (C) Plotting cycling rate against Gibbs free energy verifies that the equilibrium point corresponds to a Gibbs free energy of zero.

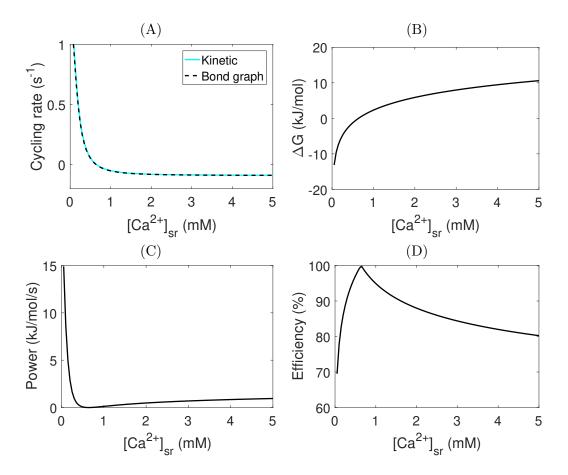


Figure 4: Simulation of the SERCA pump. (A) Comparison of cycling rates for kinetic and bond graph models, reproducing part of Fig. 13 in Tran et al. (2009); (B) Gibbs free energy; (C) Power consumption per mol of pump; (D) Pump efficiency. Simulations were run with $[Ca^{2+}]_i = 150$ nM, pH = 4, [MgADP] = 0.0363 mM, [MgATP] = 0.1 mM, [Pi] = 15 mM. Cycling rates were estimated by initialising each pump state to 1/9 fmol, and running the simulation to its steady state.

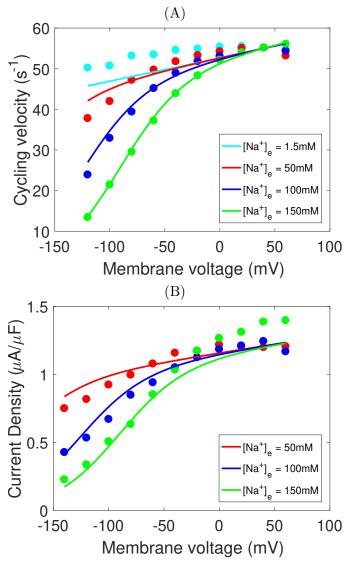


Figure 5: Fit of the cardiac Na⁺/K⁺ ATPase model to current-voltage measurements. (A) Comparison of the model to extracellular sodium and voltage data (Nakao and Gadsby, 1989, Fig. 3), with cycling velocities scaled to a value of 55 s⁻¹ at V=40 mV. (B) Comparison of the model to whole-cell current measurements (Nakao and Gadsby, 1989, Fig. 2A). [Na⁺]_i = 50 mM, [K⁺]_i = 0 mM, [K⁺]_e = 5.4 mM, pH = 7.4, [Pi]_{tot} = 0 mM, [MgATP] = 10 mM, [MgADP] = 0 mM, T=310 K.

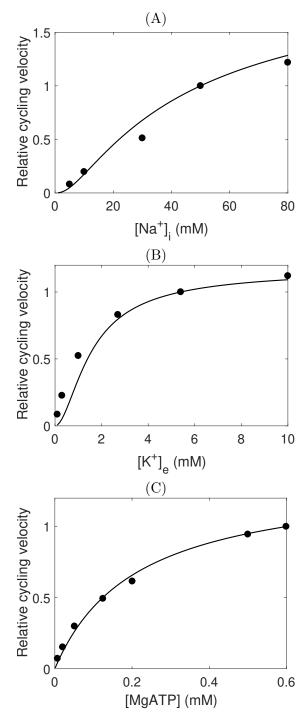


Figure 6: Fit of the cardiac Na^+/K^+ ATPase model to metabolite dependence data. (A) Comparison of the model to data with varying intracellular sodium concentrations (Hansen et al., 2002, Fig. 7A), normalised to the cycling velocity at $[Na^+]_i = 50$ mM. (B) Comparison of the model to data with varying extracellular potassium (Nakao and Gadsby, 1989, Fig. 11A), normalised to the cycling velocity at $[K^+]_e = 5.4$ mM. (C) Comparison of the model to data with varying ATP (Friedrich et al., 1996, Fig. 3B), normalised to the cycling velocity at [MgATP] = 0.6 mM.

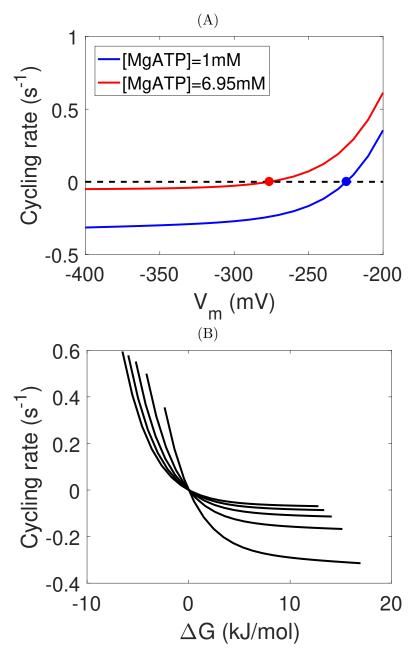


Figure 7: Simulation of the Na^+/K^+ ATPase. (A) Cycling rates of the pump near reversal potential; (B) Relationship between Gibbs free energy and cycling rate. The curves represent different concentrations of MgATP, from a concentration of 1 mM on the right, with increments of 1 mM up to a concentration of 5mM on the left. The Gibbs free energy was varied by changing the membrane potential. For (A) and (B), simulations were run using $[Na^+]_i = 10$ mM, $[Na^+]_e = 140$ mM, $[K^+]_i = 145$ mM, $[K^+]_e = 5.4$ mM, pH = 7.095, [Pi] = 0.3971 mM, [MgATP] = 6.95 mM, [MgADP] = 0.035 mM. Each pump state was initialised to 1/15 fmol, and steady states were estimated by running each simulation to steady state.