



Tutorial on Diffusion Models for Medical Imaging

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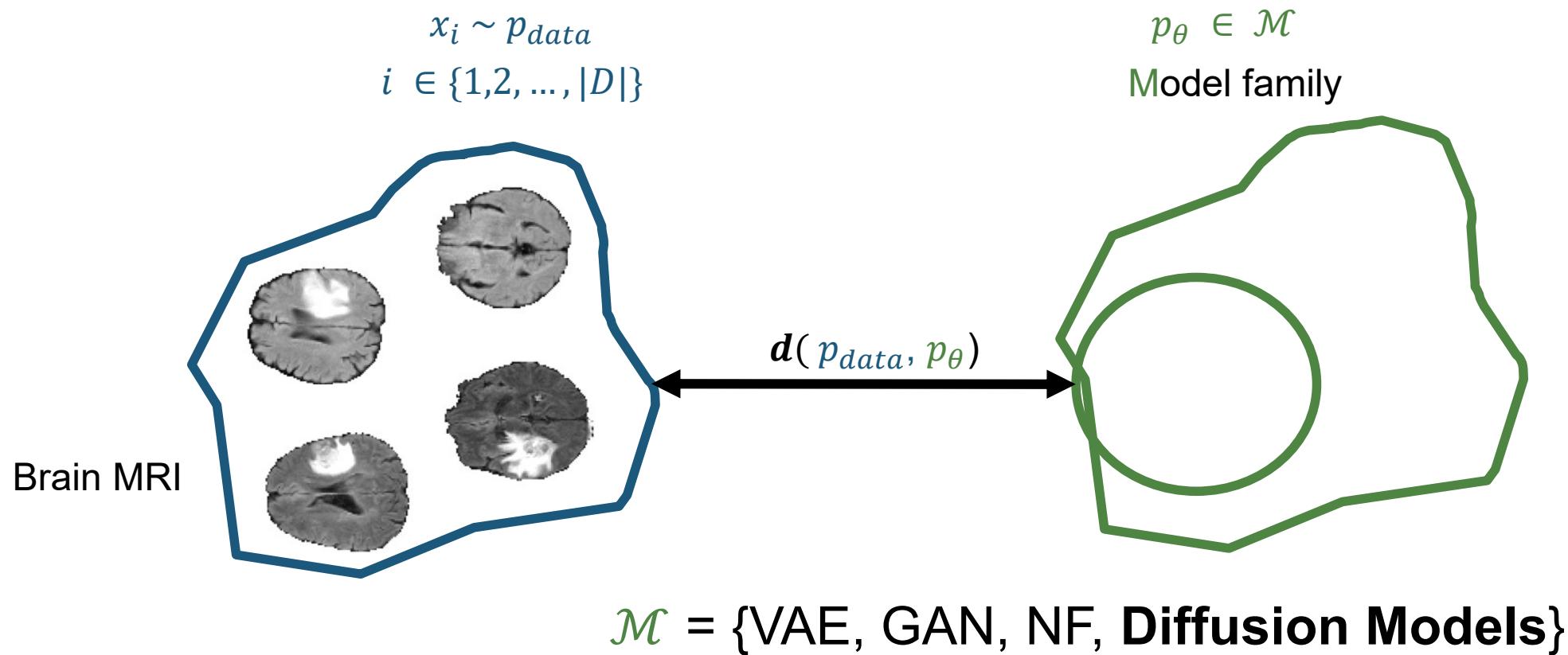
Tutorial Schedule

- ❑ Introduction [1:30pm-2:30pm]
 - ❑ What? Why? How?
 - ❑ Understanding and Intuition
 - ❑ DEMO - MONAI Generative Models
- [Coding tutorial on DDPM](#)
- ❑ Advanced Topics [2:30pm-3:30pm]
 - ❑ Sampling Strategies
 - ❑ Inference-time Conditioning
 - ❑ Training-time Conditioning
 - ❑ DEMO - MONAI Generative Models
- [DDIM Inversion + Classifier-free guidance](#)
- ❑ Applications in Medical Imaging [4pm-5pm]
 - ❑ Synthesis
 - ❑ Reconstruction
 - ❑ Segmentation
 - ❑ Registration
 - ❑ Inpainting
 - ❑ Anomaly Detection
 - ❑ Miscellaneous
- ❑ Panel Discussion [5pm-6pm]

Diffusion Models

What? Why? How?

What? Generative Models



What? Generative Models

Density Estimation

$$p_{\theta}(x)$$

$$p_{\theta} \in \mathcal{M}$$

Model family

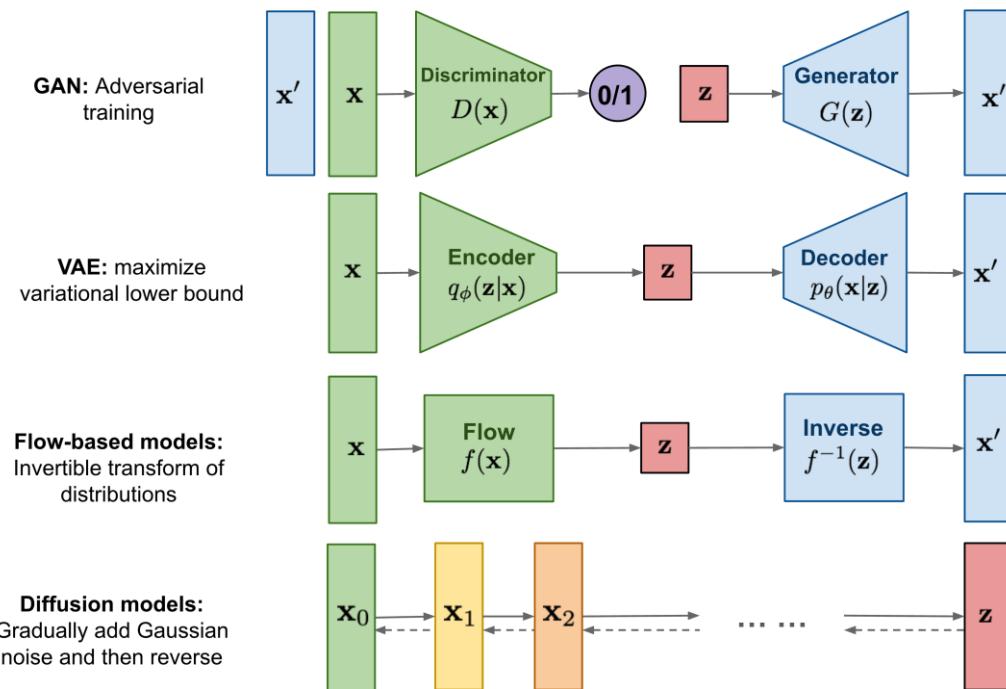
Sampling

$$x_{new} \sim p_{\theta}$$

Unsupervised Representation Learning

$$z \leftarrow p_{\theta}(x)$$

What? Generative models



likelihood-based models

Require

- inductive bias to ensure a tractable normalizing constant for likelihood computation; or
- surrogate objectives to approximate ML training.

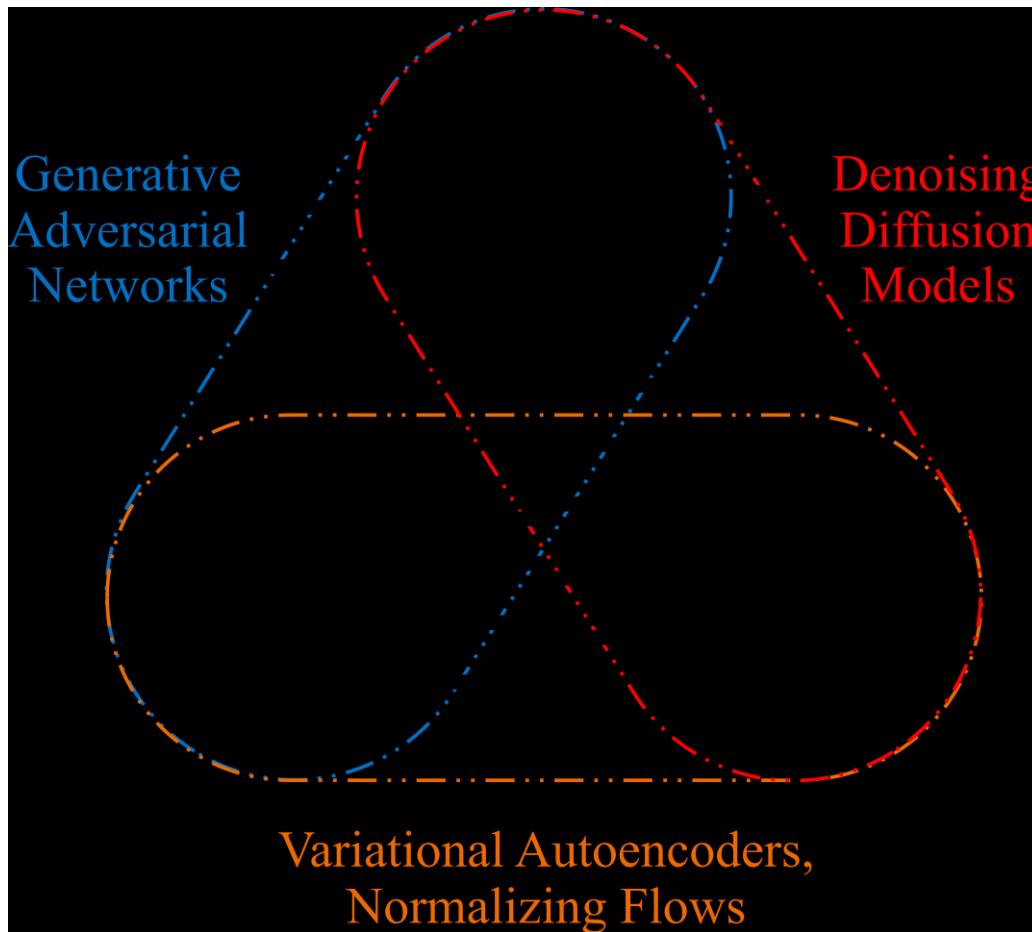
implicit generative models

Require adversarial training:

- notoriously unstable; leading to
- mode collapse

diffusion models bypass both with neat tricks

Sampling Trilemma



Why? Unprecedented Quality

1. Realism
2. Control
3. Prior

“realistic photo of a cybernetic Eagle”



“
...
Tribe taking a
selfie ...”

“A dystopian male face made of volcanic lava, mysterious, image containing secret codes”



Why? Community Push

Companies

Big models and data



stability.ai

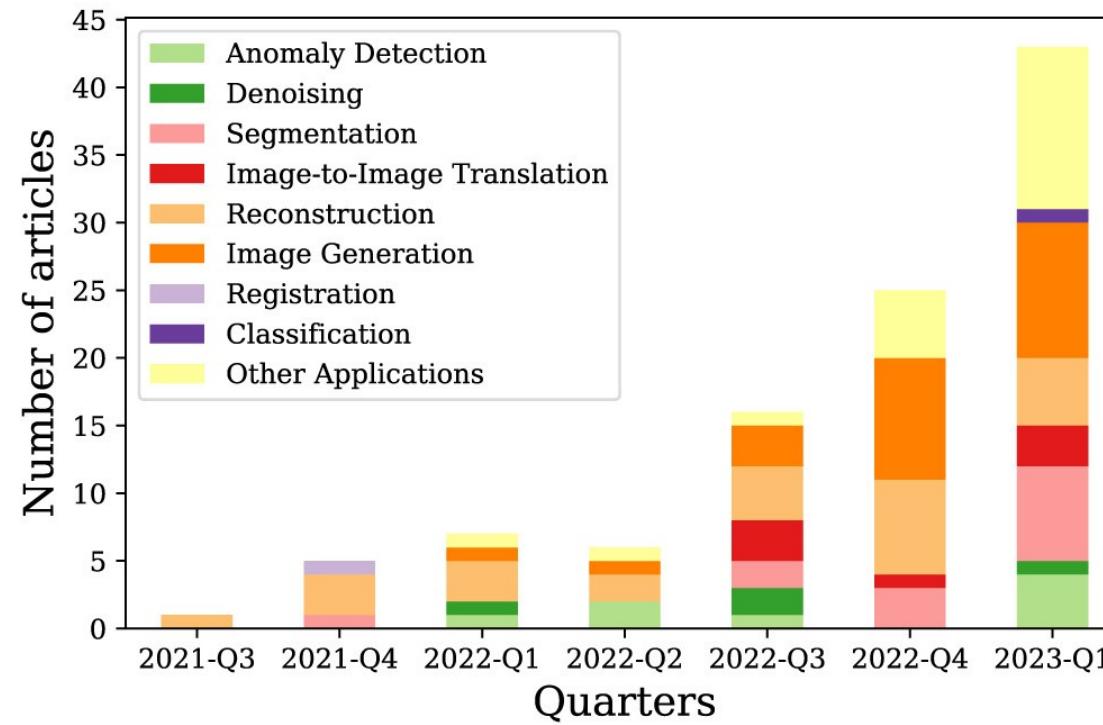


Open-Source

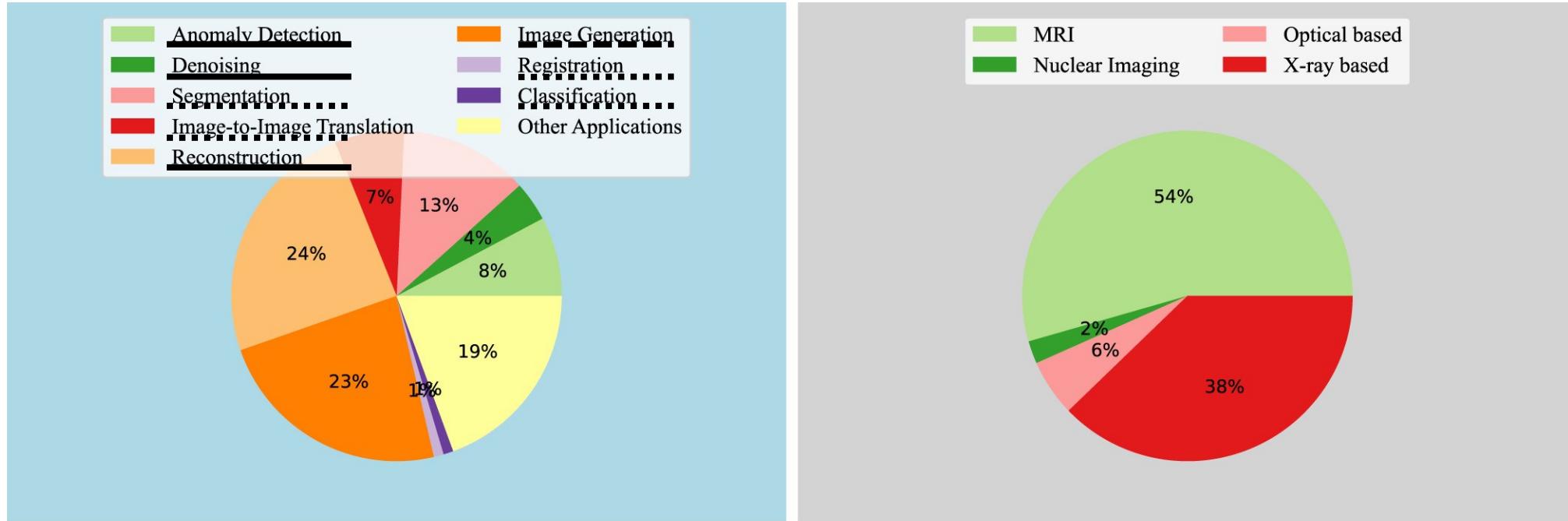
Ease of Use



Why? Medical Imaging Popularity



Why? Medical Imaging Applications

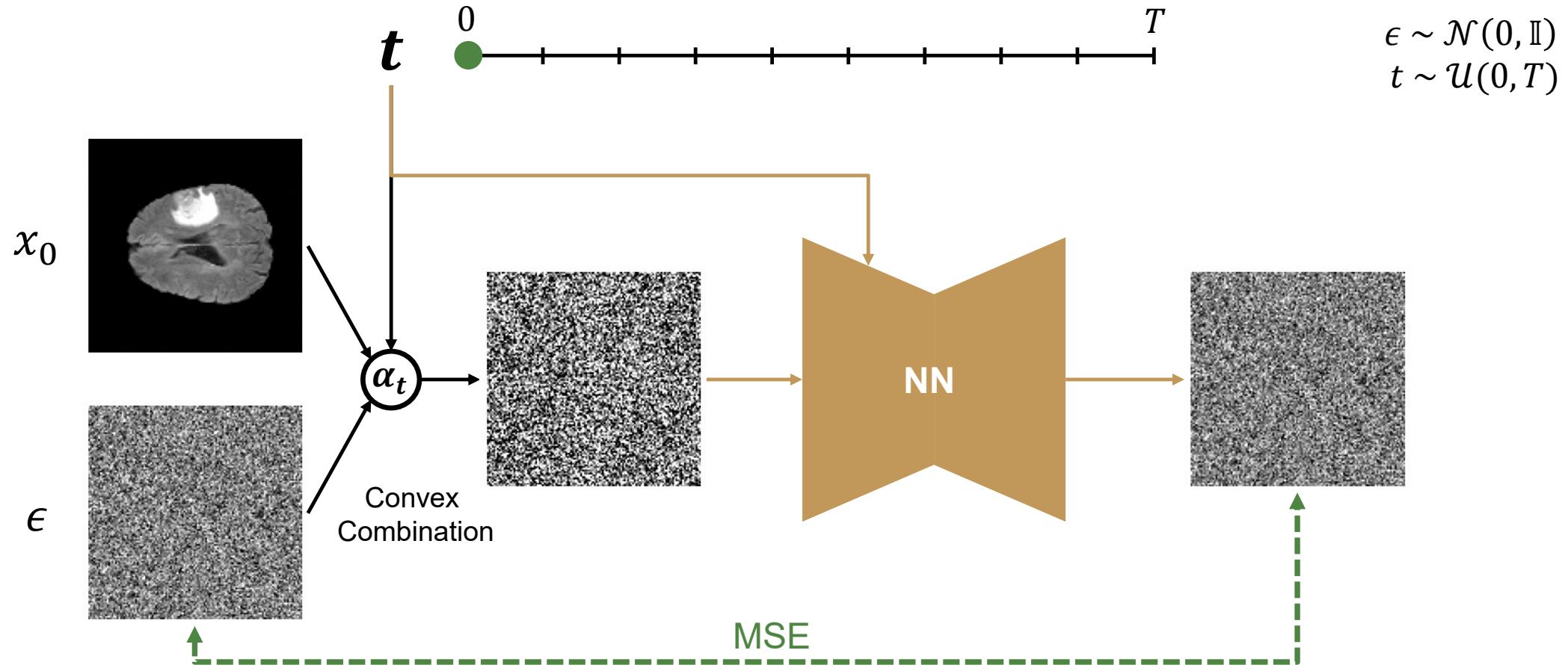


Realism

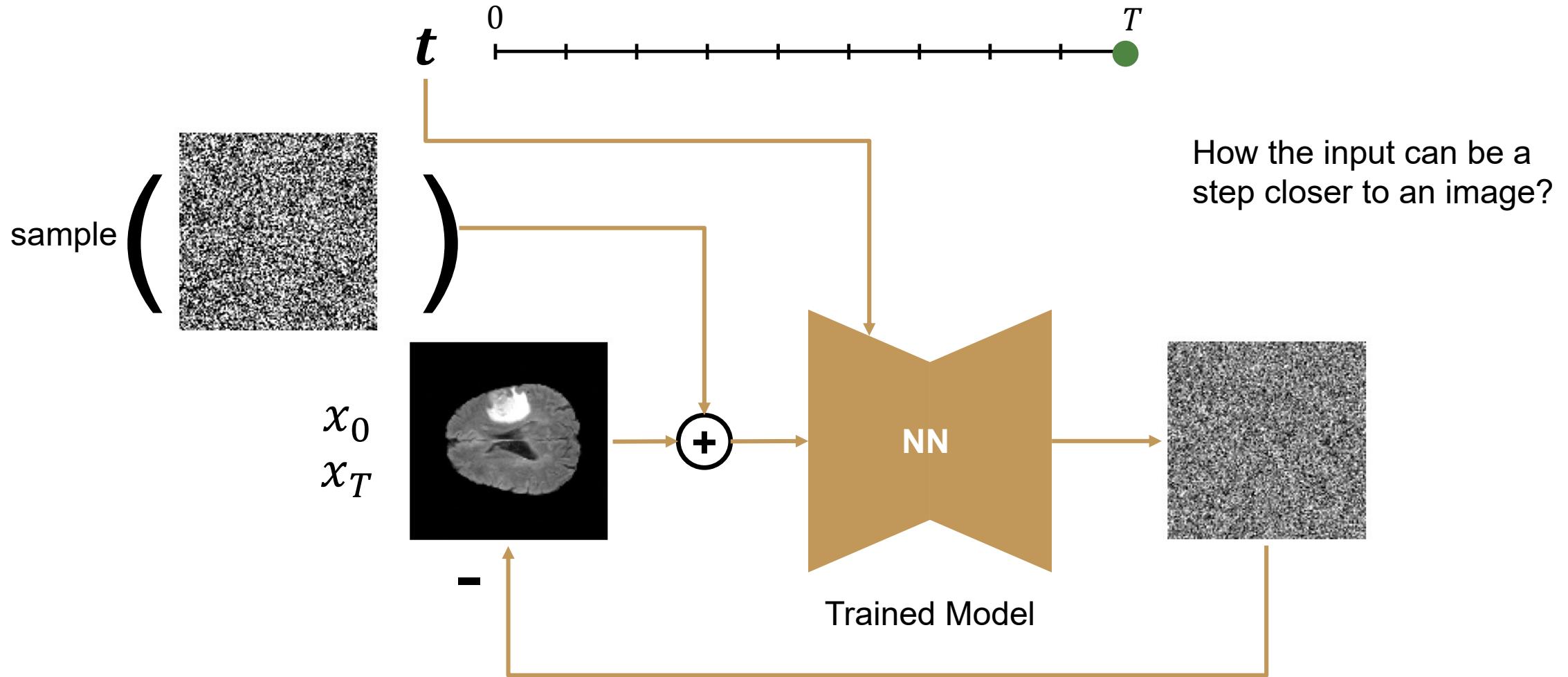
Control

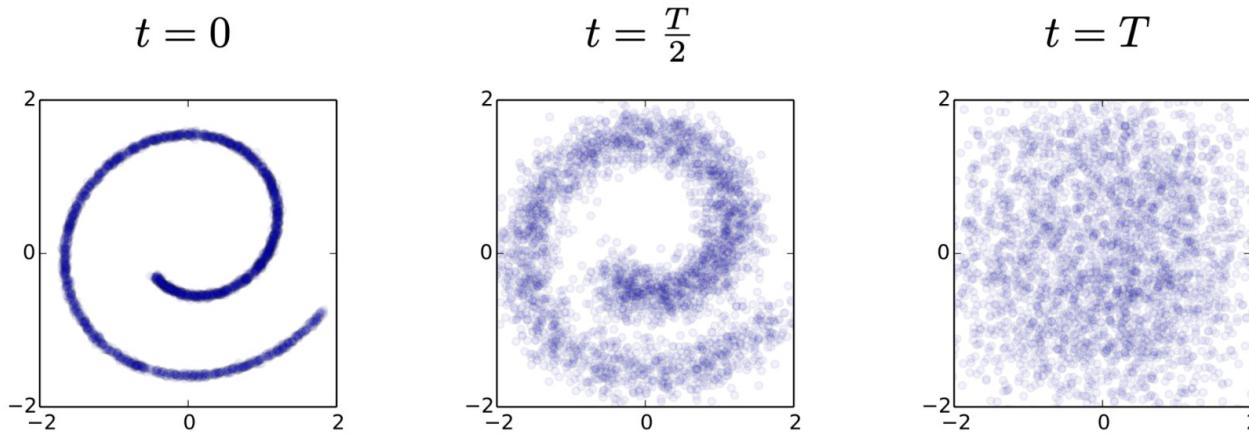
Prior

How? Training by Denoising



How? Inference





Understanding and Intuition

Score Function

$$p_\theta(x) = \frac{e^{-f_\theta(x)}}{Z_\theta}$$

$$\log p_\theta(x) = \log e^{-f_\theta(x)} - \log Z_\theta$$

$$\nabla_x \log p_\theta(x) = -\nabla_x f_\theta(x) - \nabla_x \log Z_\theta$$

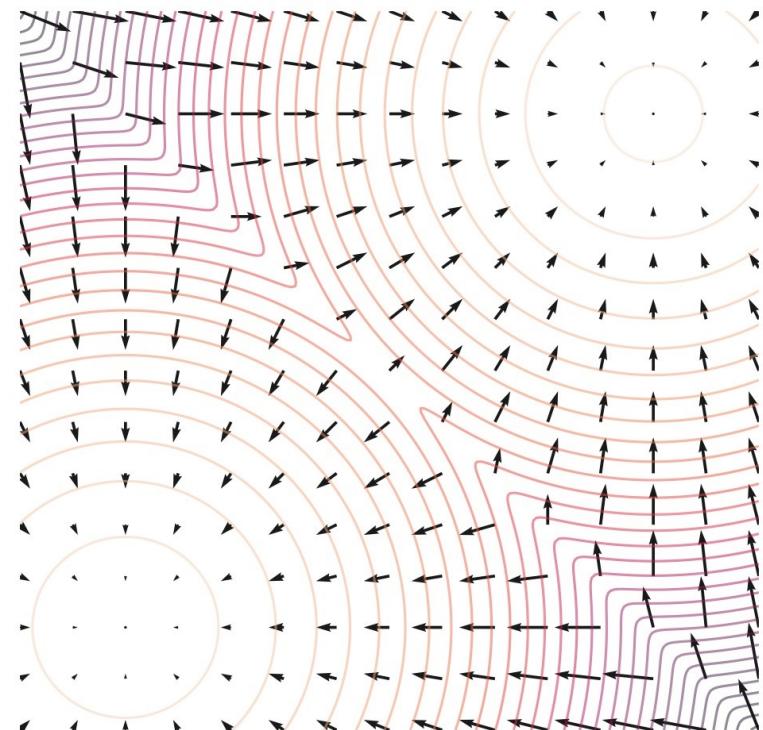
$\cancel{\epsilon_\theta}$

How to learn it?

Mixture of two Gaussians

Score function (the vector field)

Density function (contours)

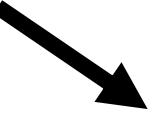


Denoising Score Matching

How to **learn** the score?

$$\mathbb{E}_{p(x)} \left\| \underbrace{\epsilon_{\theta}(x)}_{\text{Diffusion Model}} - \underbrace{\nabla_x \log p_{\theta}(x)}_{\text{Score}} \right\|_2^2$$

$$\mathbb{E}_{p(x)} \left\| \epsilon_{\theta}(x) - \nabla_x \log p_t(x_t | x) \right\|_2^2$$


 $\frac{x_t - x}{\sigma_t^2}$

Forward Process

$$p_t(x_t | x) \approx p_{data}(x)$$

$$p_t(x_t | x) = \mathcal{N}(\sqrt{\alpha_t}x, (1 - \alpha_t)\mathbf{I})$$

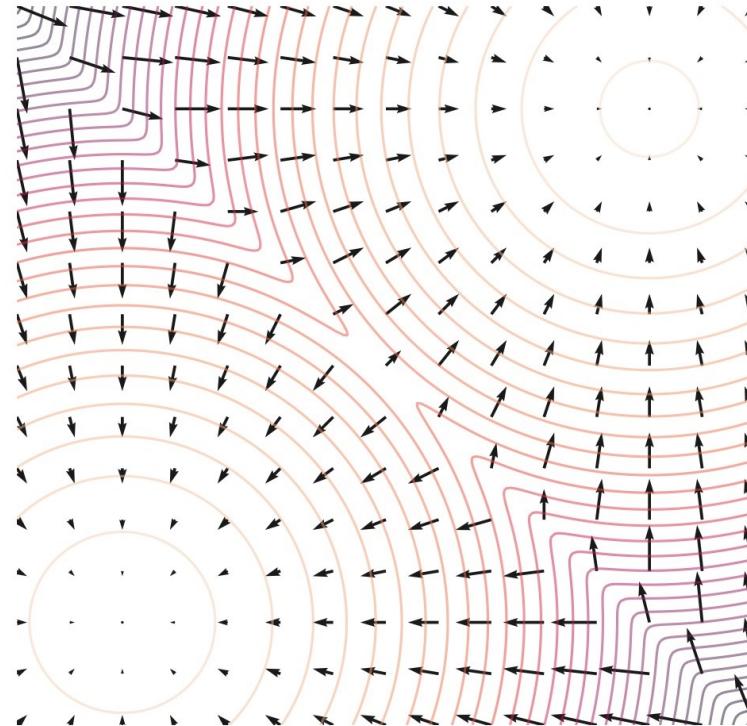
$$x_t = \sqrt{\alpha_t}x + \sqrt{1 - \alpha_t}\epsilon, \quad \epsilon \sim \mathcal{N}(0, \mathbf{I})$$

Gaussian is a common perturbation

Vincent, Pascal. "A connection between score matching and denoising autoencoders." Neural computation 23.7 (2011): 1661-1674.

Learning the Score

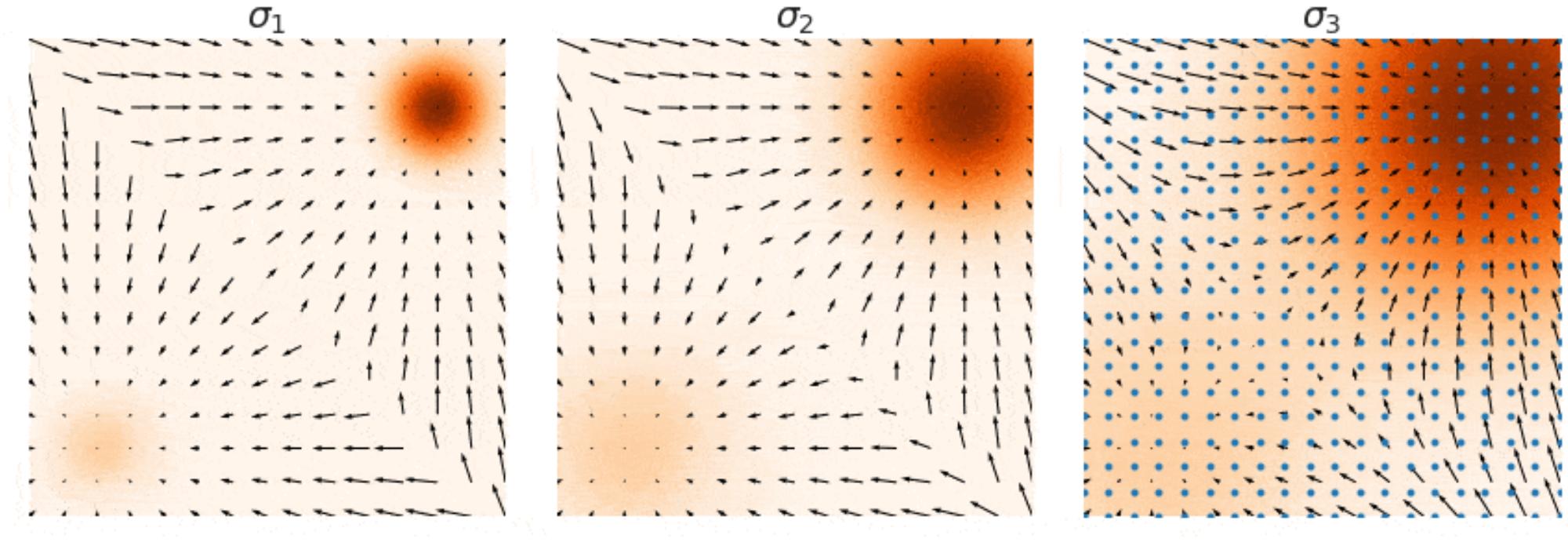
$$\mathbb{E}_{p(x)} \|\epsilon_{\theta}(x) - \nabla_x \log p_t(x_t | x)\|_2^2$$



Vincent, Pascal. "A connection between score matching and denoising autoencoders." *Neural computation* 23.7 (2011): 1661-1674.

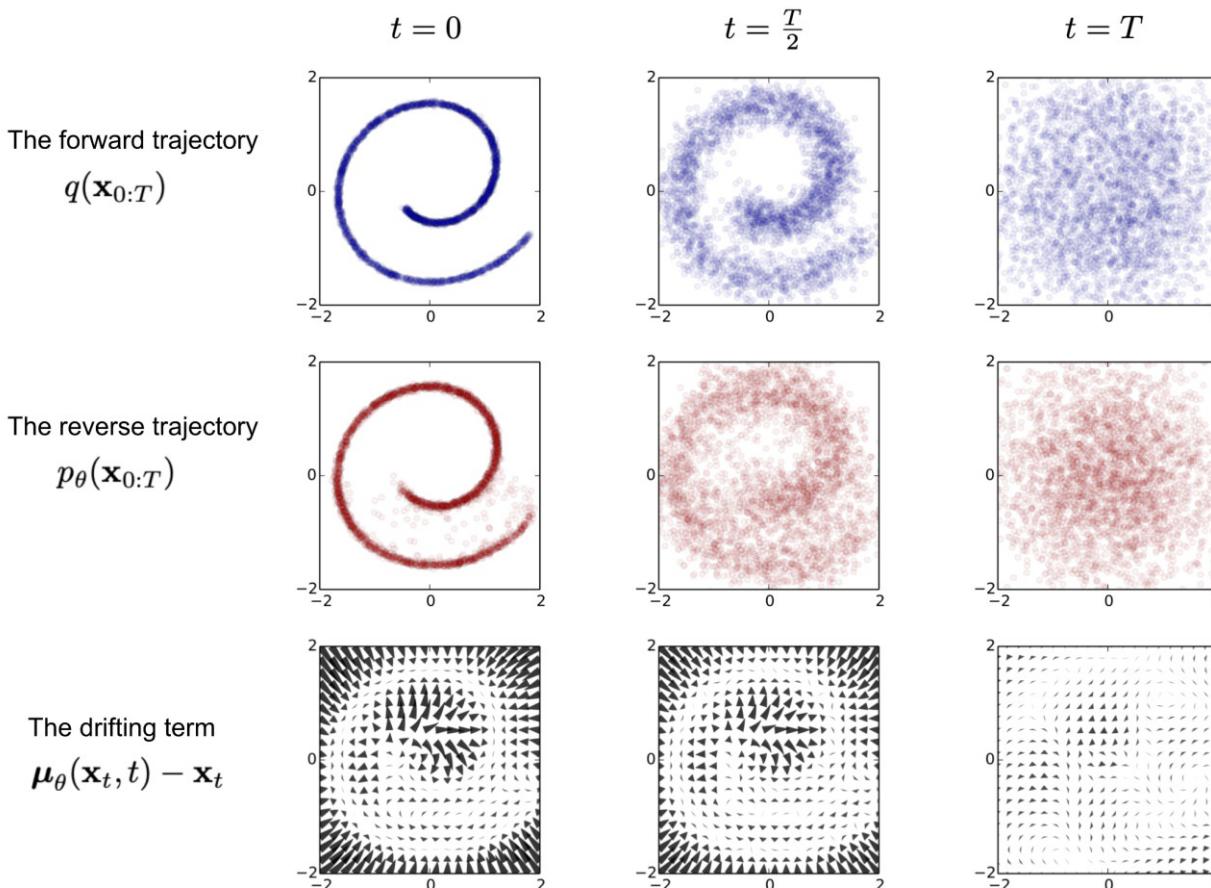
Image from blog post by Yang Song <https://yang-song.net/blog/2021/score/>

Perturbation at many scales



Learning in **low** density regions

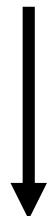
Diffusion Models Learn the Gradient



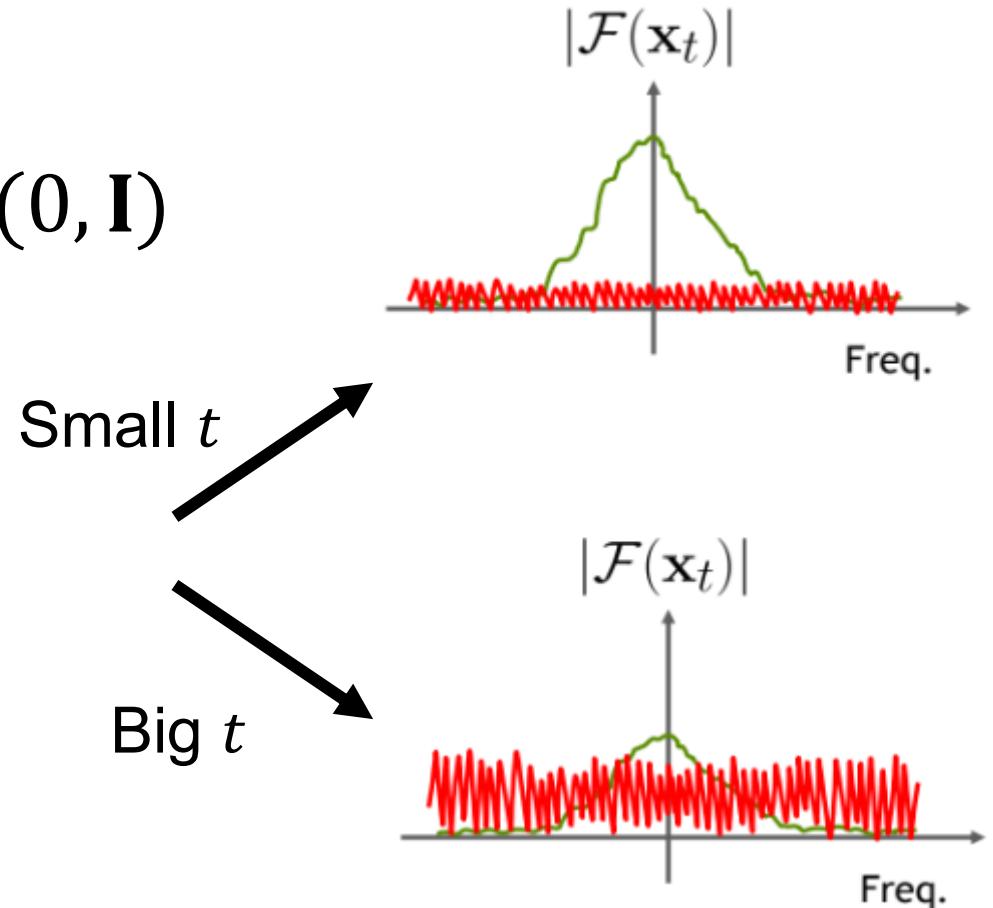
$$\nabla_{\mathbf{x}} \log p(\mathbf{x})$$

Fourier Transform

$$\mathbf{x}_t = \sqrt{\alpha_t} \mathbf{x} + \sqrt{1 - \alpha_t} \boldsymbol{\epsilon}, \quad \boldsymbol{\epsilon} \sim \mathcal{N}(0, \mathbf{I})$$

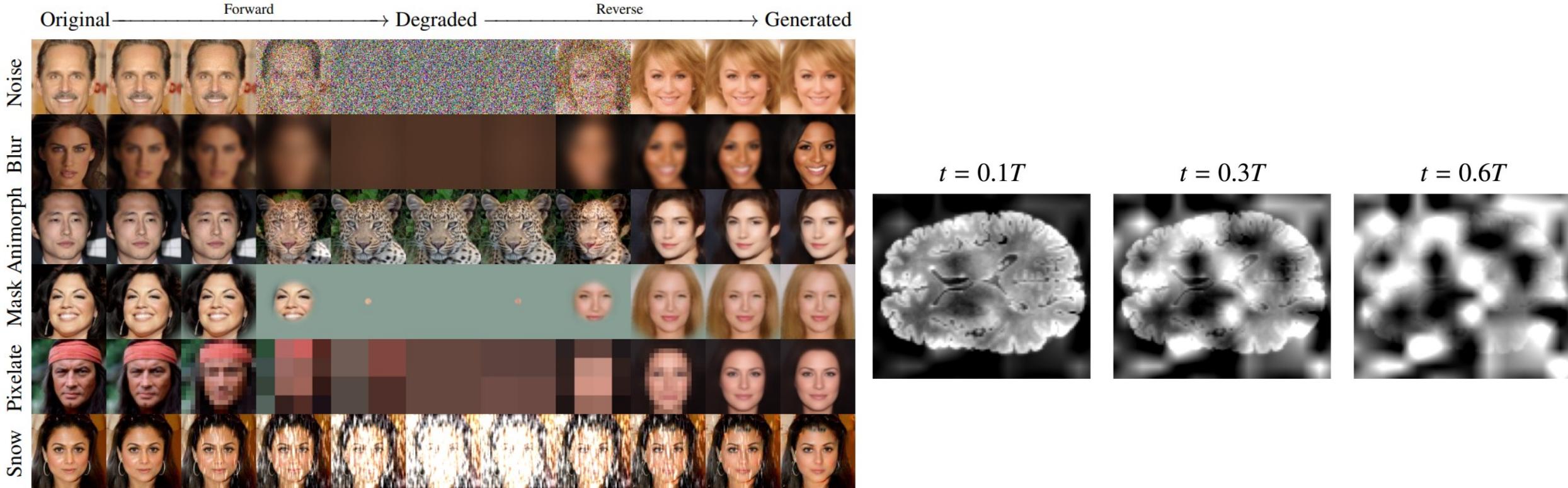


$$\mathcal{F}(\mathbf{x}_t) = \sqrt{\alpha_t} \mathcal{F}(\mathbf{x}) + \sqrt{1 - \alpha_t} \mathcal{F}(\boldsymbol{\epsilon})$$



Slide inspired in CVPRs 2022 tutorial on diffusion models

Gaussian Perturbation?



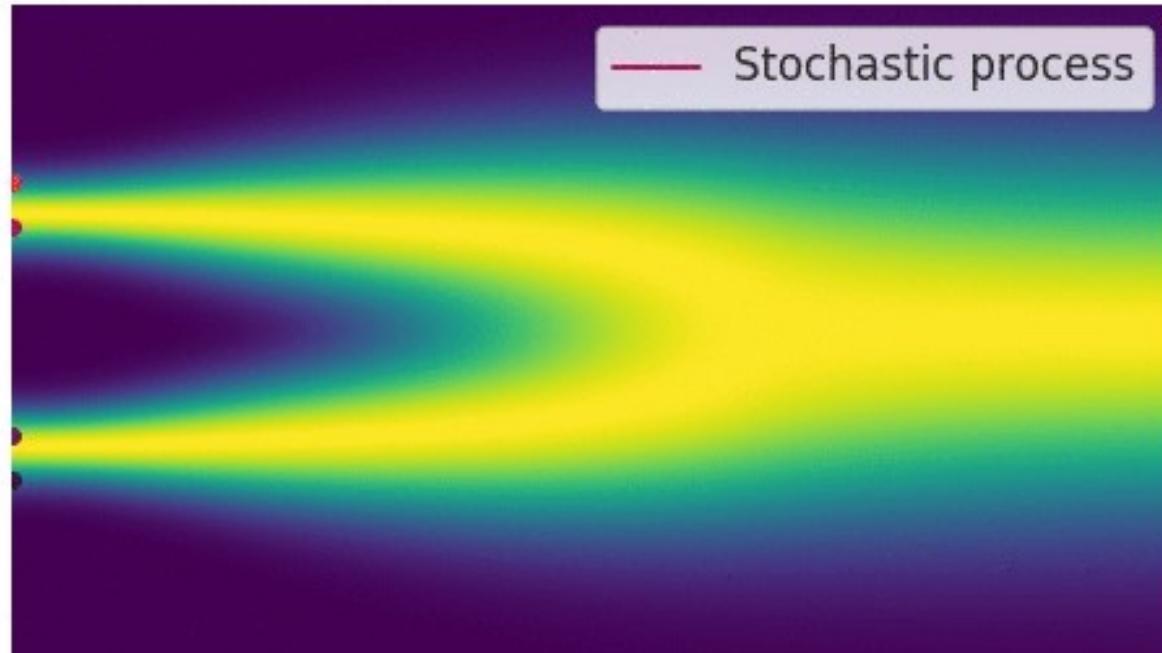
[1] Daras, Giannis, et al. "Soft diffusion: Score matching for general corruptions." arXiv preprint arXiv:2209.05442 (2022).

[2] Bansal, Arpit, et al. "Cold diffusion: Inverting arbitrary image transforms without noise." arXiv preprint arXiv:2208.09392 (2022).

[3] Kascenas, Antanas, et al. "The role of noise in denoising models for anomaly detection in medical images." Medical Image Analysis (2023): 102963.

Diffusion and Differential Equations

- ❑ Perturbation process is a Stochastic Differential Equation (SDE)
 - ❑ From complex to simple
 - ❑ Allow different values for SDE modelling

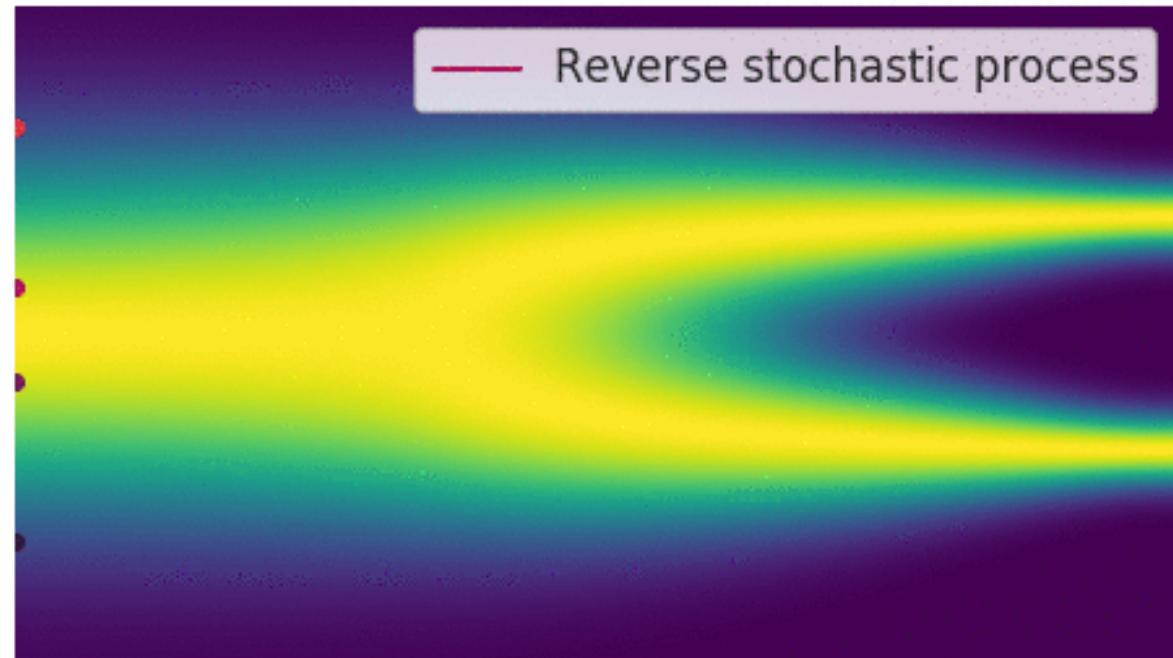


$$d\mathbf{x} = \mathbf{f}(\mathbf{x}, t)dt + g(t)d\mathbf{w}$$

Image from blog post by Yang Song <https://yang-song.net/blog/2021/score/>

Reversing the Process is Generation

- Samplers are discrete solutions of the reverse-time SDE



$$d\mathbf{x} = [\mathbf{f}(\mathbf{x}, t) - g^2(t) \nabla_{\mathbf{x}} \log p_t(\mathbf{x})] dt + g(t) d\mathbf{w}$$

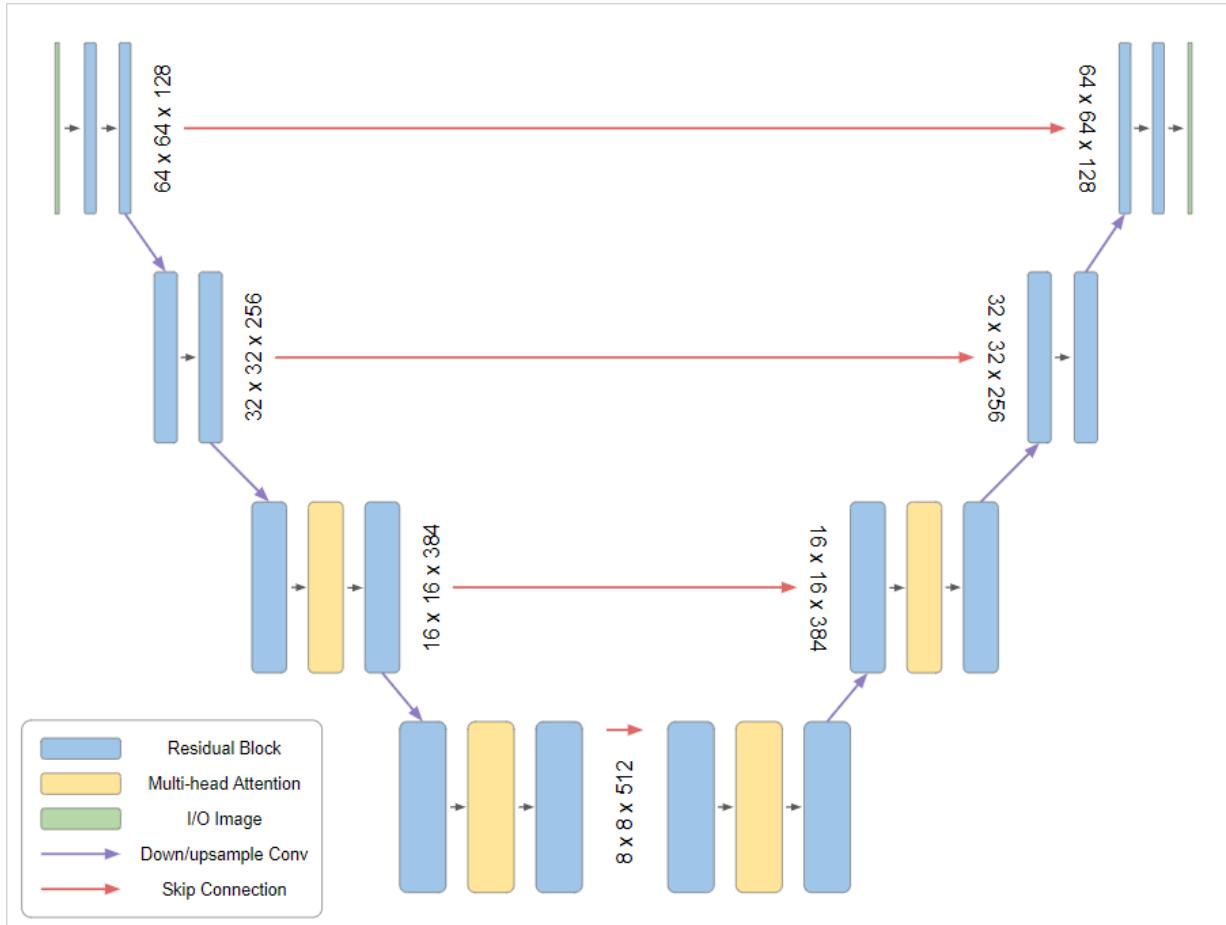
Image from blog post by Yang Song <https://yang-song.net/blog/2021/score/>

The Design Space

	VP [49]	VE [49]	iDDPM [37] + DDIM [47]	Ours (“EDM”)
Sampling (Section 3)				
ODE solver	Euler	Euler	Euler	2^{nd} order Heun
Time steps	$t_{i < N}$	$1 + \frac{i}{N-1}(\epsilon_s - 1)$	$\sigma_{\max}^2 (\sigma_{\min}^2 / \sigma_{\max}^2)^{\frac{i}{N-1}}$	$u_{\lfloor j_0 + \frac{M-1-j_0}{N-1} i + \frac{1}{2} \rfloor}, \text{ where } u_M = 0$ $u_{j-1} = \sqrt{\frac{u_j^2 + 1}{\max(\bar{\alpha}_{j-1}/\bar{\alpha}_j, C_1)} - 1}$
Schedule	$\sigma(t)$	$\sqrt{e^{\frac{1}{2}\beta_d t^2 + \beta_{\min} t} - 1}$	\sqrt{t}	t
Scaling	$s(t)$	$1/\sqrt{e^{\frac{1}{2}\beta_d t^2 + \beta_{\min} t}}$	1	1
Network and preconditioning (Section 5)				
Architecture of F_θ	DDPM++	NCSN++	DDPM	(any)
Skip scaling $c_{\text{skip}}(\sigma)$	1	1	1	$\sigma_{\text{data}}^2 / (\sigma^2 + \sigma_{\text{data}}^2)$
Output scaling $c_{\text{out}}(\sigma)$	$-\sigma$	σ	$-\sigma$	$\sigma \cdot \sigma_{\text{data}} / \sqrt{\sigma_{\text{data}}^2 + \sigma^2}$
Input scaling $c_{\text{in}}(\sigma)$	$1/\sqrt{\sigma^2 + 1}$	1	$1/\sqrt{\sigma^2 + 1}$	$1/\sqrt{\sigma^2 + \sigma_{\text{data}}^2}$
Noise cond. $c_{\text{noise}}(\sigma)$	$(M-1) \sigma^{-1}(\sigma)$	$\ln(\frac{1}{2}\sigma)$	$M-1 - \arg \min_j u_j - \sigma $	$\frac{1}{4} \ln(\sigma)$
Training (Section 5)				
Noise distribution	$\sigma^{-1}(\sigma) \sim \mathcal{U}(\epsilon_t, 1)$	$\ln(\sigma) \sim \mathcal{U}(\ln(\sigma_{\min}), \ln(\sigma_{\max}))$	$\sigma = u_j, \quad j \sim \mathcal{U}\{0, M-1\}$	$\ln(\sigma) \sim \mathcal{N}(P_{\text{mean}}, P_{\text{std}}^2)$
Loss weighting $\lambda(\sigma)$	$1/\sigma^2$	$1/\sigma^2$	$1/\sigma^2$ (note: *)	$(\sigma^2 + \sigma_{\text{data}}^2) / (\sigma \cdot \sigma_{\text{data}})^2$
Parameters				
	$\beta_d = 19.9, \beta_{\min} = 0.1$	$\sigma_{\min} = 0.02$	$\bar{\alpha}_j = \sin^2(\frac{\pi}{2} \frac{j}{M(C_2+1)})$	$\sigma_{\min} = 0.002, \sigma_{\max} = 80$
	$\epsilon_s = 10^{-3}, \epsilon_t = 10^{-5}$	$\sigma_{\max} = 100$	$C_1 = 0.001, C_2 = 0.008$	$\sigma_{\text{data}} = 0.5, \rho = 7$
	$M = 1000$		$M = 1000, j_0 = 8^\dagger$	$P_{\text{mean}} = -1.2, P_{\text{std}} = 1.2$

* iDDPM also employs a second loss term L_{vlb} [†] In our tests, $j_0 = 8$ yielded better FID than $j_0 = 0$ used by iDDPM

Architecture – Reusing the *classics*, and the SoTA



Unet!

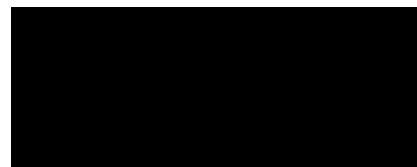
Or transformers
Or VQ-VAEs
Or...

DEMO



Generative Models

Allows researchers and developers to easily train, evaluate, and deploy generative models on medical imaging.



UNIVERSITAT DE
BARCELONA



Icahn School
of Medicine at
Mount
Sinai



Stanford
University



Features

- State-of-the-art models
- Losses and supporting classes to train models
- Evaluation metrics
- Tutorials
- Pre-trained models



Screenshot of the GitHub repository page for "GenerativeModels".

The repository has 43 issues, 9 pull requests, and 21 watchers. It contains 26 branches and 4 tags. The main branch is selected. The repository was created by marksgraham on Aug 16, 2023, with 415 commits.

The commit history shows the following changes:

File / Commit	Description	Date
github/workflows	Create python-publish.yml	5 months ago
generative	add spatial rescaler (#414)	2 months ago
model-zoo	Fix model zoo scheduler args (#398)	5 months ago
tests	add spatial rescaler (#414)	2 months ago
tutorials	373 add code for spade vae gan (#405)	3 months ago
.deepsource.toml	Update tests, CI and pre-commit (#193)	9 months ago
.gitignore	Modified .gitignore to account for all IteliJ tools.	last year
.pre-commit-config.yaml	Change num_res_channels and num_channels to Sequence[int] int (#2...)	8 months ago
CODE_OF_CONDUCT.md	Create CODE_OF_CONDUCT.md	last year

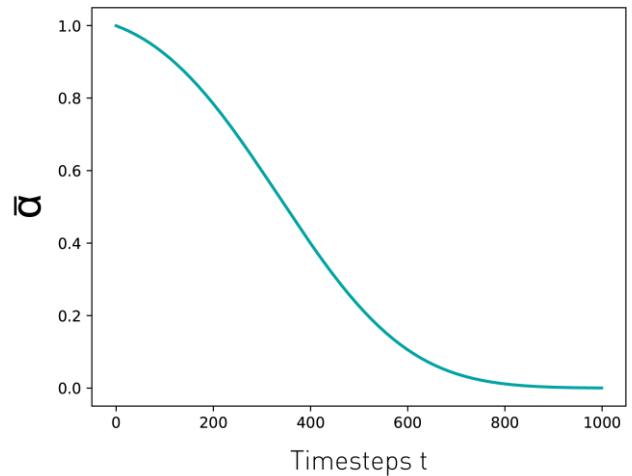
The repository is public and has 42 forks. It is associated with the MONAI project and includes tags for medical-imaging, generative-adversarial-network, image-translation, anomaly-detection, generative-models, image-synthesis, mri-reconstruction, diffusion-models, and monai. It includes links to Readme, Apache-2.0 license, Code of conduct, Activity, and 319 stars.

U-Net Architecture

```
from generative.networks.nets import DiffusionModelUNet

model = DiffusionModelUNet(
    spatial_dims=3,
    in_channels=1,
    out_channels=1,
    num_channels=[256, 256, 512],
    attention_levels=[False, False, True],
    num_head_channels=[0, 0, 512],
    num_res_blocks=2,
)
```

Noise Schedulers



$$\begin{aligned}\mathbf{x}_t &= \sqrt{\alpha_t} \mathbf{x}_{t-1} + \sqrt{1 - \alpha_t} \boldsymbol{\epsilon}_{t-1} \\ &= \sqrt{\alpha_t \alpha_{t-1}} \mathbf{x}_{t-2} + \sqrt{1 - \alpha_t \alpha_{t-1}} \boldsymbol{\epsilon}_{t-2} \\ &= \dots \\ &= \sqrt{\bar{\alpha}_t} \mathbf{x}_0 + \sqrt{1 - \bar{\alpha}_t} \boldsymbol{\epsilon}\end{aligned}$$
$$q(\mathbf{x}_t | \mathbf{x}_0) = \mathcal{N}(\mathbf{x}_t; \sqrt{\bar{\alpha}_t} \mathbf{x}_0, (1 - \bar{\alpha}_t) \mathbf{I})$$

```
from generative.networks.schedulers  
import DDPMscheduler
```

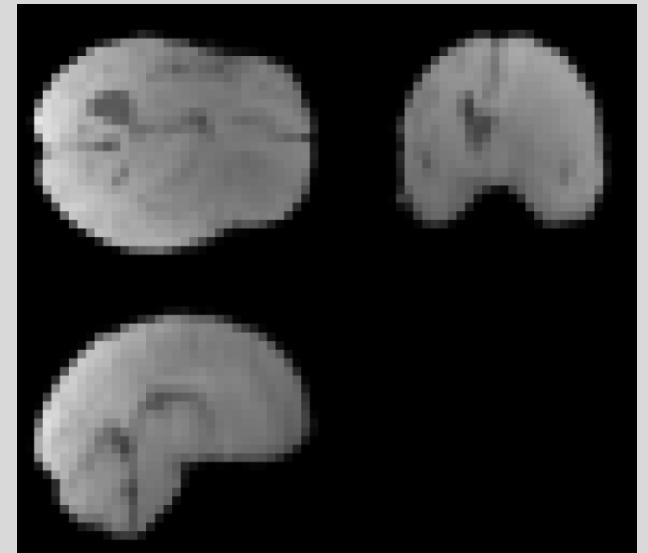
```
scheduler = DDPMscheduler(  
    num_train_timesteps=1000,  
    beta_schedule="scaled_linear",  
    beta_start=0.0005,  
    beta_end=0.0195,  
)
```

3D - Preprocessing

```
from monai import transforms
from monai.apps import DecathlonDataset
from monai.data import DataLoader

train_transform = transforms.Compose(
    [
        transforms.LoadImaged(keys=["image"]),
        transforms.Lambda(keys=["image"], func=lambda x: x[:, :, :, 1]),
        transforms.AddChanneld(keys=["image"]),
        transforms.ScaleIntensityd(keys=["image"]),
        transforms.CenterSpatialCropd(keys=["image"], roi_size=[160, 200, 155]),
        transforms.Resized(keys=["image"], spatial_size=(32, 40, 32)),
    ]
)

train_ds = DecathlonDataset(
    root_dir="./data", task="Task01_BrainTumour", transform=train_transform, section="training", download=True
)
train_loader = DataLoader(train_ds, batch_size=8, shuffle=True, num_workers=8, persistent_workers=True)
```



Training

```
...
for batch in train_loader:
    model.train()
    images = batch["image"].to(device)

    optimizer.zero_grad(set_to_none=True)

    noise = torch.randn_like(images).to(device)
    timesteps = torch.randint(0, scheduler.num_train_timesteps,(images.shape[0],))
    noisy_image = scheduler.add_noise(original_samples=images,
                                       noise=noise,
                                       timesteps=timesteps)

    noise_pred = model(x=noisy_image, timesteps=timesteps)

    loss = F.mse_loss(noise_pred.float(), noise.float())
...
```

Sampling Images

```
model.eval()
noise = torch.randn((1, 1, 32, 40, 32)) # BS, Channels, 3D
scheduler.set_timesteps(num_inference_steps=1000)

for t in iter(scheduler.timesteps):
    model_output = model(noise, timesteps=(t,))
    noise, _ = scheduler.step(model_output, t, noise)
image = noise
```



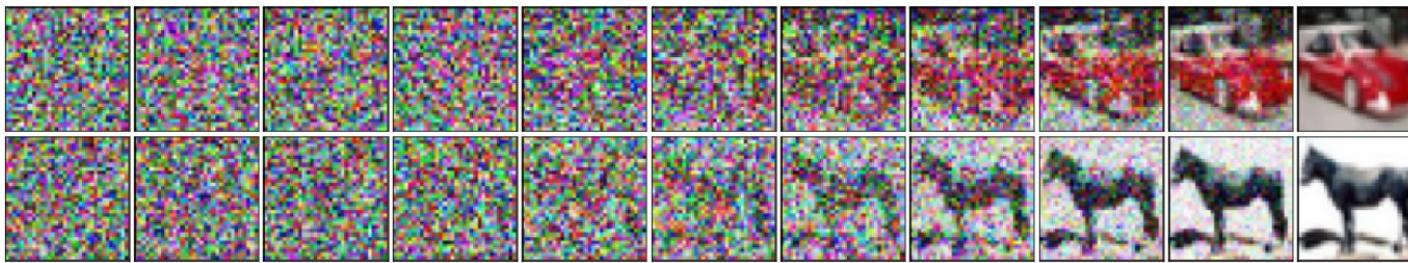
t=1000

Timestep [t]

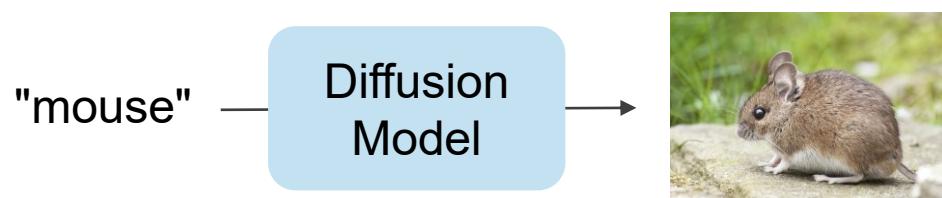
t=0

Part 2 – Advanced Topics

- Sampling Strategies



- Conditioning Mechanisms



Basic Idea of Denoising Diffusion Models



x_0

Diffusion Models Beat GANs on Image Synthesis

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x_0

$x_{t-1}, \beta_t \mathbf{I}$

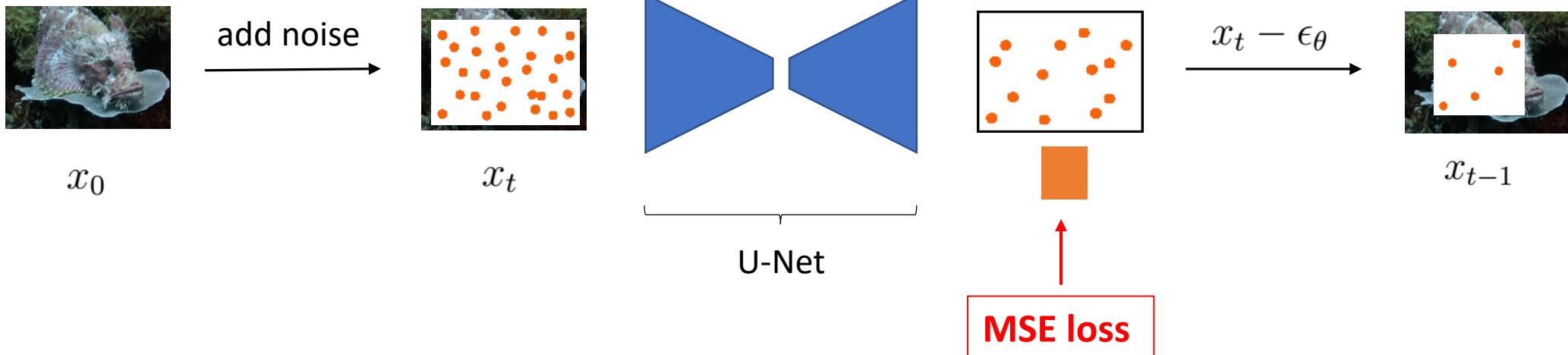
Abstract

We show that diffusion models can achieve image sample quality superior to the current state-of-the-art generative models. We achieve this on unconditional image synthesis by finding a better architecture through a series of ablations. For conditional image synthesis, we further improve sample quality with classifier guidance: a simple, compute-efficient method for trading off diversity for fidelity using gradients from a classifier. We achieve an FID of 2.97 on ImageNet 128×128 , 4.59 on ImageNet 256×256 , and 7.72 on ImageNet 512×512 , and we match

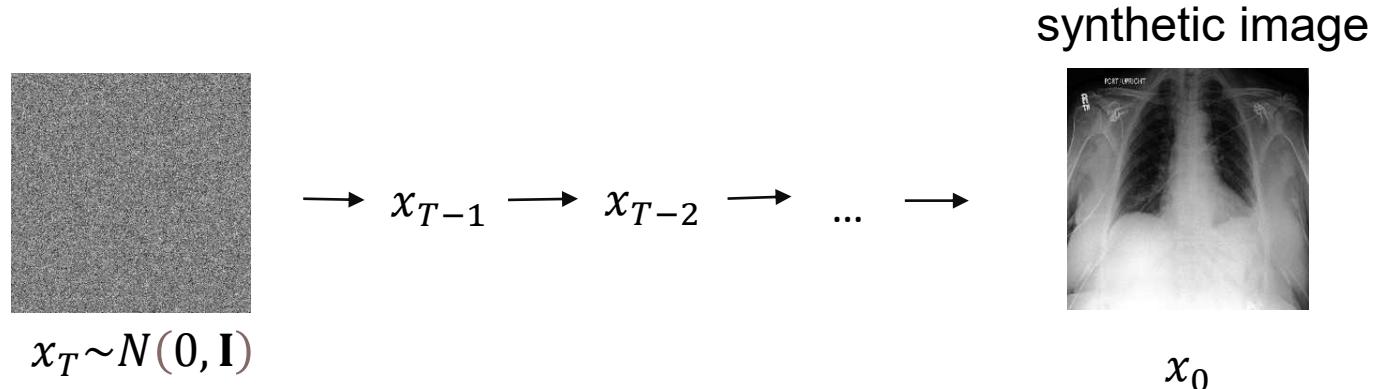
- The noising process is a Markov chain with forward and backward transitions.
- The noise is added to the image at each step.
- For this, we need to learn a denoising function.

Training Overview

- We choose a random step $t \in \{0, 1, \dots, T\}$.
- We add t steps of noise to our input image x_0 , and obtain a noisy image x_t .
- Our model predicts the noise pattern  that needs to be subtracted from x_t , to predict a slightly denoised x_{t-1} .



Fake Image Generation

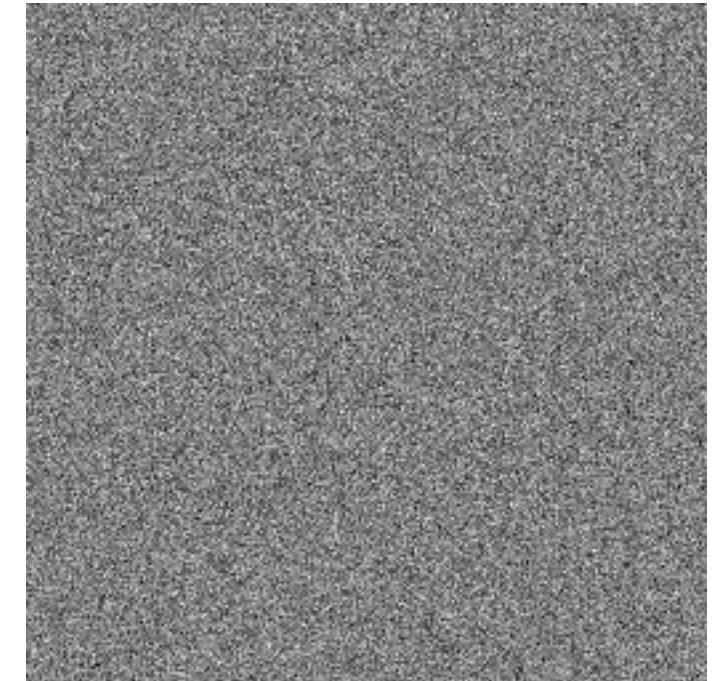


U-Net

$$x_{t-1} = \frac{1}{\sqrt{\alpha_t}} \left(x_t - \frac{1 - \alpha_t}{\sqrt{1 - \bar{\alpha}_t}} \right) + \sigma_t, \quad \text{with}$$

Random component

A green arrow points from the text "Random component" to the term σ_t in the equation.



DDPM Scheduler

Denoising Diffusion Probabilistic Models

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Abstract

We present high quality image synthesis results using diffusion probabilistic models, a class of latent variable models inspired by considerations from nonequilibrium thermodynamics. Our best results are obtained by training on a weighted variational bound designed according to a novel connection between diffusion probabilistic

Algorithm 1 Training

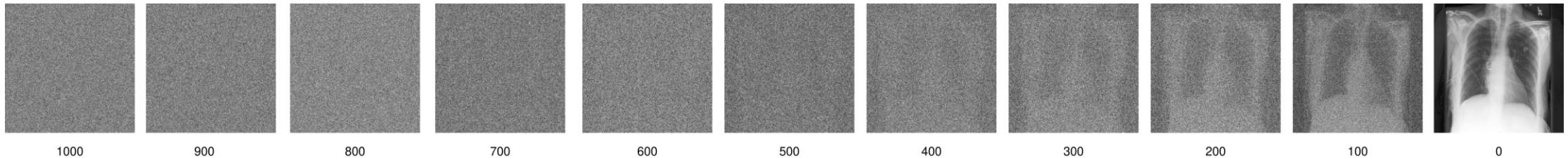
```
1: repeat
2:    $\mathbf{x}_0 \sim q(\mathbf{x}_0)$ 
3:    $t \sim \text{Uniform}(\{1, \dots, T\})$ 
4:    $\epsilon \sim \mathcal{N}(\mathbf{0}, \mathbf{I})$ 
5:   Take gradient descent step on
      
$$\nabla_{\theta} \|\epsilon - \epsilon_{\theta}(\sqrt{\bar{\alpha}_t} \mathbf{x}_0 + \sqrt{1 - \bar{\alpha}_t} \epsilon, t)\|^2$$

6: until converged
```

Algorithm 2 Sampling

```
1:  $\mathbf{x}_T \sim \mathcal{N}(\mathbf{0}, \mathbf{I})$ 
2: for  $t = T, \dots, 1$  do
3:    $\mathbf{z} \sim \mathcal{N}(\mathbf{0}, \mathbf{I})$  if  $t > 1$ , else  $\mathbf{z} = \mathbf{0}$ 
4:    $\mathbf{x}_{t-1} = \frac{1}{\sqrt{\alpha_t}} \left( \mathbf{x}_t - \frac{1 - \alpha_t}{\sqrt{1 - \bar{\alpha}_t}} \epsilon_{\theta}(\mathbf{x}_t, t) \right) + \sigma_t \mathbf{z}$ 
5: end for
6: return  $\mathbf{x}_0$ 
```

Schedulers: How to Accelerate Sampling?



Published as a conference paper at ICLR 2021

DENOISING DIFFUSION IMPLICIT MODELS

Jiaming Song, Chenlin Meng & Stefano Ermon
Stanford University
{tsong,chenlin,ermon}@cs.stanford.edu

ABSTRACT

Denoising diffusion probabilistic models (DDPMs) have achieved high quality image generation without adversarial training, yet they require simulating a Markov chain for many steps in order to produce a sample. To accelerate sampling, we present denoising diffusion implicit models (DDIMs), a more efficient class of iterative implicit probabilistic models with the same training procedure as DDPMs. In DDPMs, the generative process is defined as the reverse of a particular Markovian diffusion process. We generalize DDPMs via a class of non-Markovian diffusion processes that lead to the same training objective. These non-Markovian

"Denoising diffusion probabilistic models (DDPMs) have achieved high quality image generation, yet they require simulating a Markov chain for many steps in order to produce a sample."



We need to make the generation process faster.

From DDPMs to DDIMs

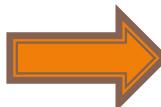
$$\mathbf{x}_{t-1} = \sqrt{\alpha_{t-1}} \underbrace{\left(\frac{\mathbf{x}_t - \sqrt{1-\alpha_t} \epsilon_\theta^{(t)}(\mathbf{x}_t)}{\sqrt{\alpha_t}} \right)}_{\text{“predicted } \mathbf{x}_0\text{”}} + \underbrace{\sqrt{1-\alpha_{t-1}-\sigma_t^2} \cdot \epsilon_\theta^{(t)}(\mathbf{x}_t)}_{\text{“direction pointing to } \mathbf{x}_t\text{”}} + \underbrace{\sigma_t \epsilon_t}_{\text{random noise}}$$

DDPM sampling scheme

$$\sigma_t = \sqrt{(1-\alpha_{t-1})/(1-\alpha_t)} \sqrt{1-\alpha_t/\alpha_{t-1}}$$

DDIM sampling scheme

$$\sigma_t = 0$$



We remove the random component

The training process stays the same.

An Excursion into ODEs

- The connection to ordinary differential equations (ODEs) can be seen when we rewrite the DDIM denoising step as

$$\text{prediction} = \text{previous value} + \text{step size} \cdot \text{derivative}.$$

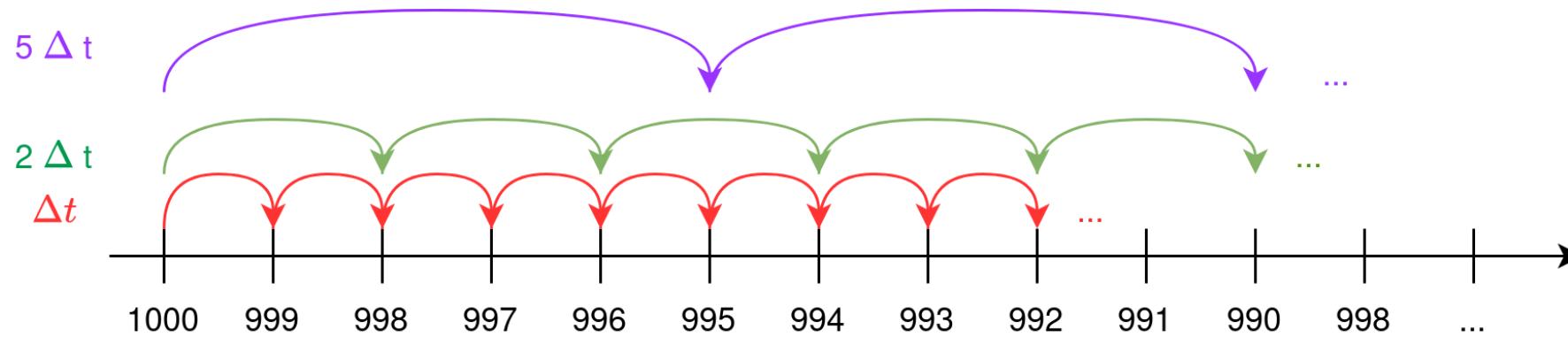
prediction previous value step size derivative

- This can be interpreted as the Euler approximation of an ODE.
- We can speed up the generation process by choosing a larger step size.
- DDIM is a **probability flow** ODE from a SDE [1].

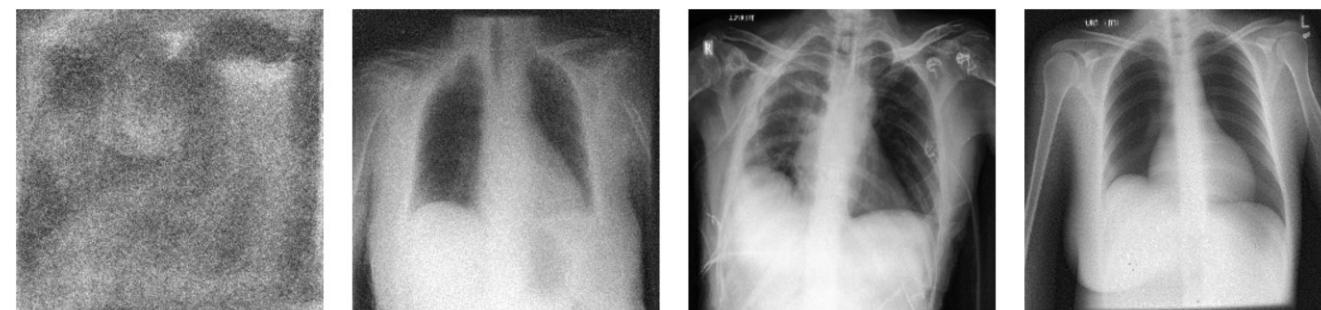


Faster, but less accurate

DDIM Accelerated Sampling



- By skipping k steps, we have a step size of $k\Delta t$.
- Sampling is k times faster.
- We trade image quality for speed.



Total amount of steps

→ 2

10

20

50

Various Schedulers...

Elucidating the Design Space of Diffusion-Based Generative Models

PSEUDO NUMERICAL METHODS FOR DIFFUSION MODELS ON MANIFOLDS

Luping Liu, Yi Ren
Zhejiang University
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Published as a conference paper at ICLR 2022

PROGRESSIVE DISTILLATION FOR FAST SAMPLING OF DIFFUSION MODELS

Tim Salimans & Jonathan Ho
Google Research, Brain team
{salimans,jonathanho}@google.com

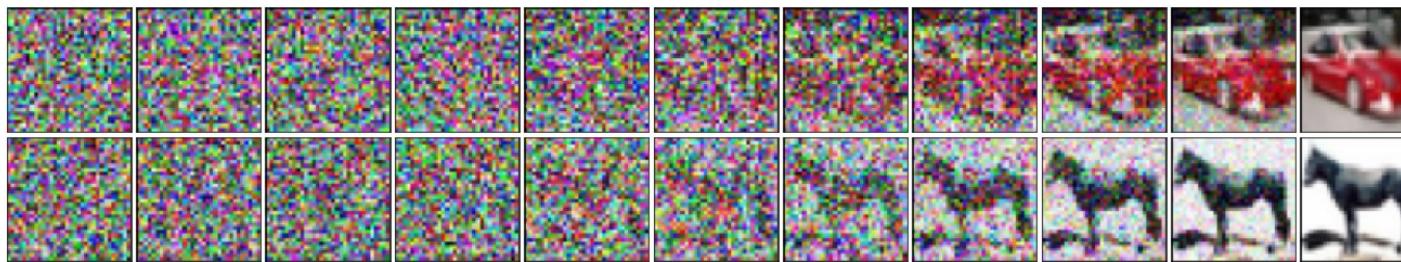
ABSTRACT

Diffusion models have recently shown great promise for generative modeling, outperforming GANs on perceptual quality and autoregressive models at density estimation. A remaining downside is their slow sampling time: generating high quality samples takes many hundreds or thousands of model evaluations. Here we make two contributions to help eliminate this downside: First, we present new parameterizations of diffusion models that provide increased stability when using few sampling steps. Second, we present a method to distill a trained deterministic diffusion sampler, using many steps, into a new diffusion model that takes half as many sampling steps. We then keep progressively refining this distillation process.

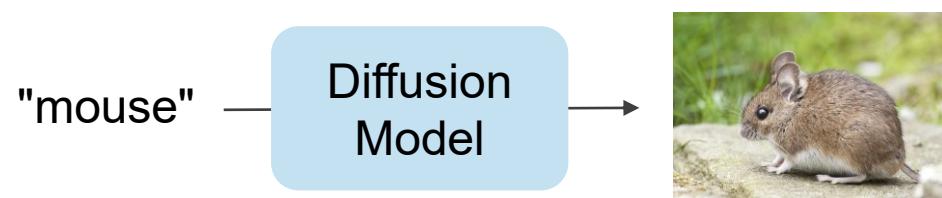
- Choosing a different solver for the given ODE can improve speed and image quality.
- Other numerical approaches such as **Heun's Method** or **Runge Kutta** solvers can be explored.
- Knowledge distillation techniques can be used for fast sampling.

Part 2 – Advanced Topics

- Sampling Strategies



- Conditioning Mechanisms



Conditioning

1. Inference-time

- 1. An inverse problem view
 - Classifier guidance
- 2. DDIM inversion
 - Interpolation
 - Gradient guidance

2. Training-time

- 1. Scalar inputs
- 2. Text
- 3. Images
- 4. ControlNet
- 5. DreamBooth



Inverse Problem

- We consider two random variables x and y .
- Suppose we know the forward process of generating y from x , represented by the transition probability distribution $p(y|x)$.
- We aim to solve the inverse problem $p(x|y)$.
- With the Bayes' rule, we have

$$p(\mathbf{x} \mid \mathbf{y}) = p(\mathbf{x})p(\mathbf{y} \mid \mathbf{x}) / \int p(\mathbf{x})p(\mathbf{y} \mid \mathbf{x}) d\mathbf{x}.$$

- Like in score-based models, we take the gradient of the log

$$\nabla_{\mathbf{x}} \log \text{[green box]} = \nabla_{\mathbf{x}} \text{[blue box]} + \nabla_{\mathbf{x}} \text{[red box]}$$

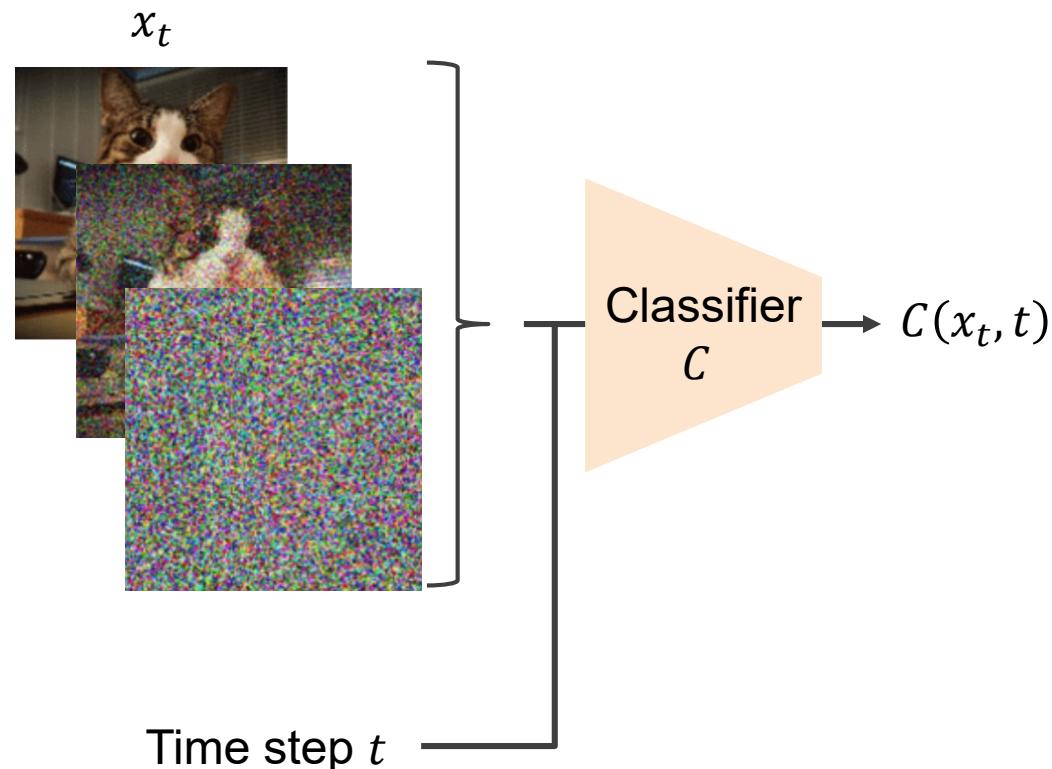
Image given the
condition

This is known
(diffusion model ϵ_θ)

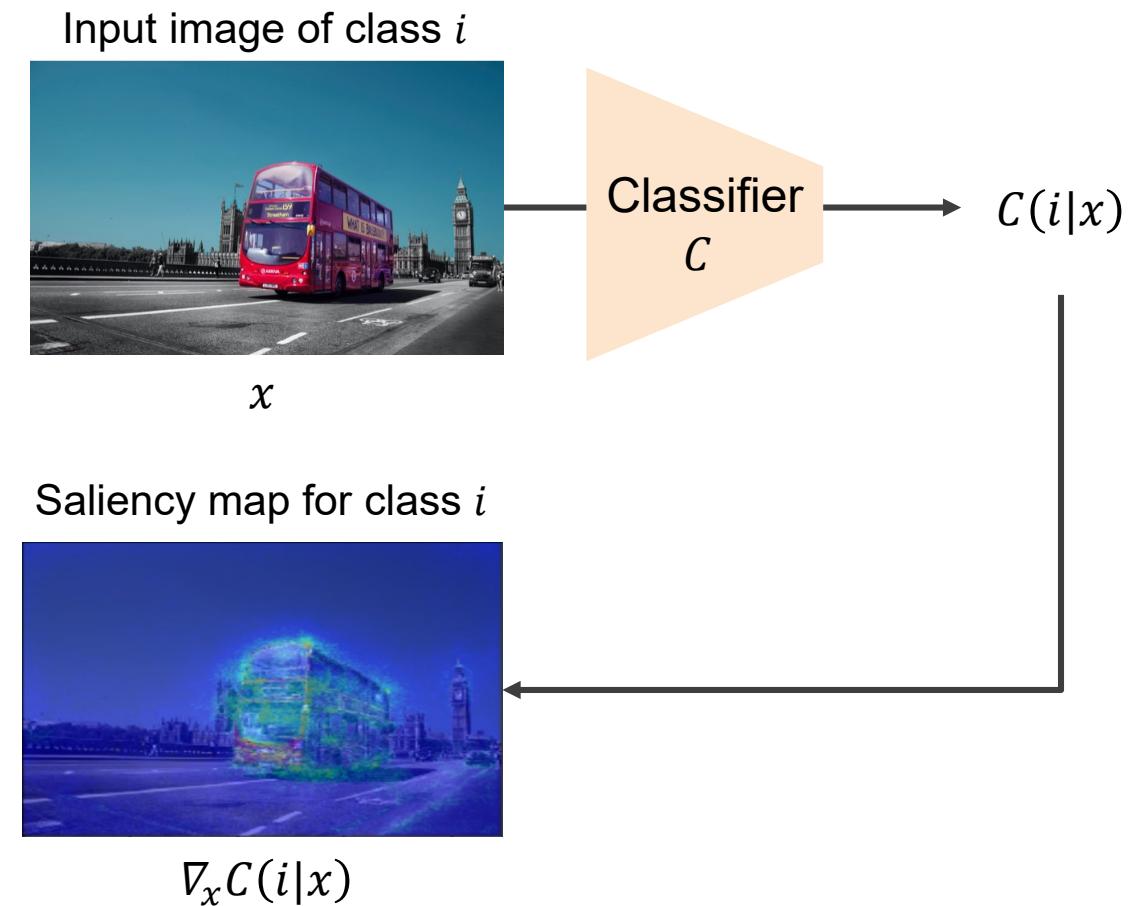
This is the condition
(classifier, ...)

Example: Classifier Guidance

We want a class-conditional diffusion model.

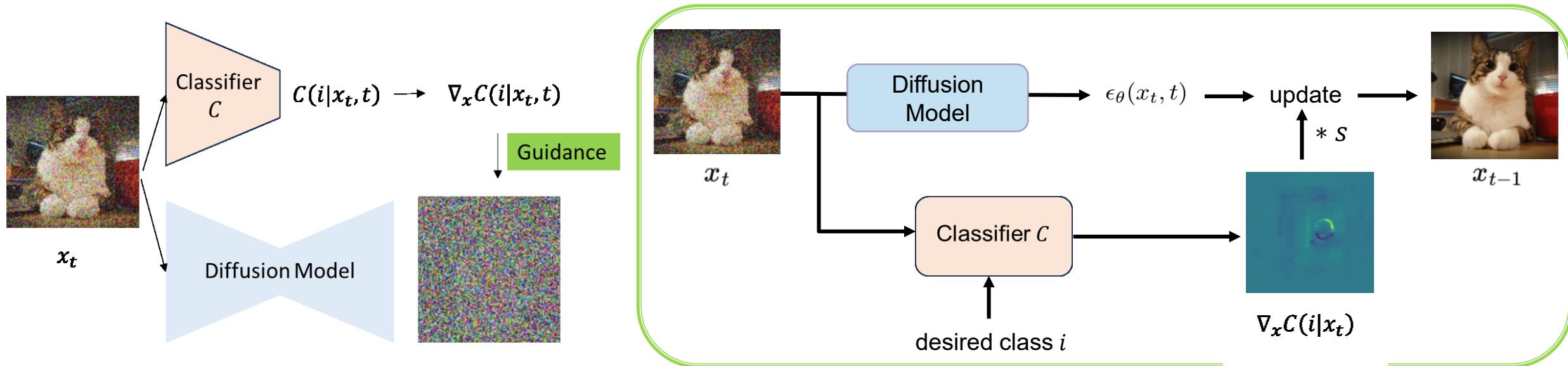


We consider the gradient with respect to the input pixels.



Classifier Guidance

We use the gradient to guide the generation process towards a desired class.



→ Gradient guidance is not restricted to classification models. Other models (e.g., regression, segmentation, ...) work just in the same way.

Classifier Guidance



goldfish

arctic fox

butterfly

African elephant

flamingo

tennis ball



cheeseburger

fountain

balloon

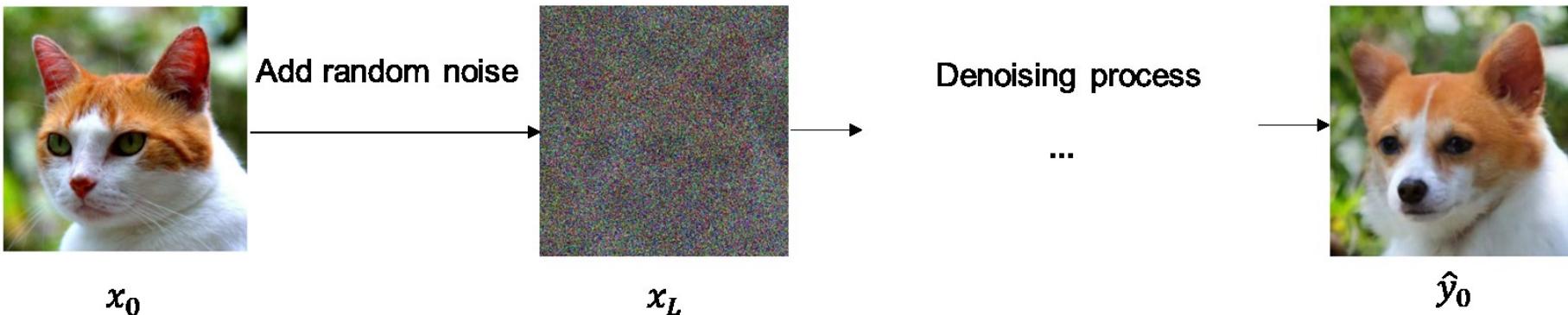
tabby cat

lorikeet

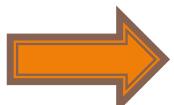
agaric

How can we preserve information?

We might want to translate an image to another...



- We add L steps of noise to an input image x_0 .
- The smaller L , the less the image can be changed.
- The higher L , the more information is destroyed.



We need to find a way to keep the information of x_0 .



We consider Denoising Diffusion Implicit Models (DDIMs).

DDIM Inversion

- Under the DDIM sampling scheme, we remove the random component.
- The connection to ordinary differential equations (ODEs) can be seen when we rewrite the denoising step as

$$\frac{x_{t-1}}{\sqrt{\bar{\alpha}_{t-1}}} = \frac{x_t}{\sqrt{\bar{\alpha}_t}} + \left(\sqrt{\frac{1 - \bar{\alpha}_{t-1}}{\bar{\alpha}_{t-1}}} - \sqrt{\frac{1 - \bar{\alpha}_t}{\bar{\alpha}_t}} \right) \epsilon_\theta(x_t, t). \quad \text{Noise decoding}$$

- This can be interpreted as the Euler approximation of an ODE.
- Given infinitely small steps t , the reversed ODE can then be solved with

$$\frac{x_{t+1}}{\sqrt{\bar{\alpha}_{t+1}}} = \frac{x_t}{\sqrt{\bar{\alpha}_t}} + \left(\sqrt{\frac{1 - \bar{\alpha}_{t+1}}{\bar{\alpha}_{t+1}}} - \sqrt{\frac{1 - \bar{\alpha}_t}{\bar{\alpha}_t}} \right) \epsilon_\theta(x_t, t). \quad \text{Noise encoding}$$

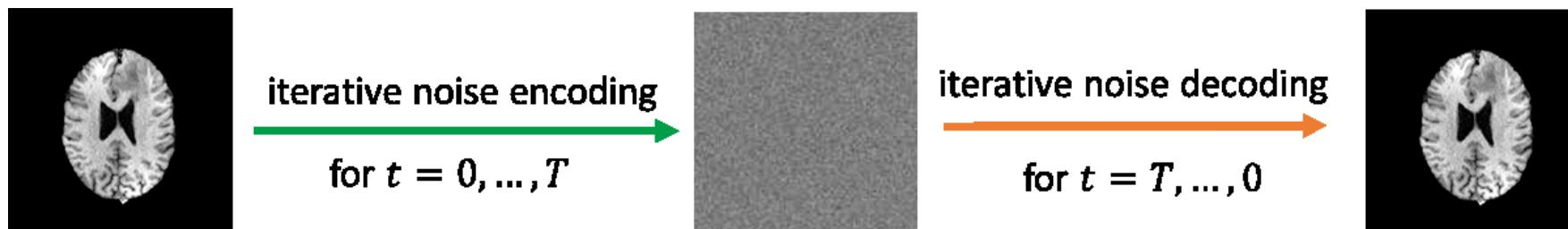
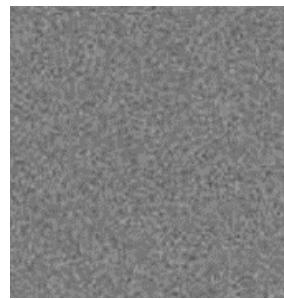


Image Interpolation



DDIM noise encoding

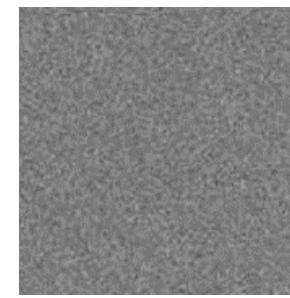
A



Linear Combination
 $(1-\alpha)A + \alpha B$

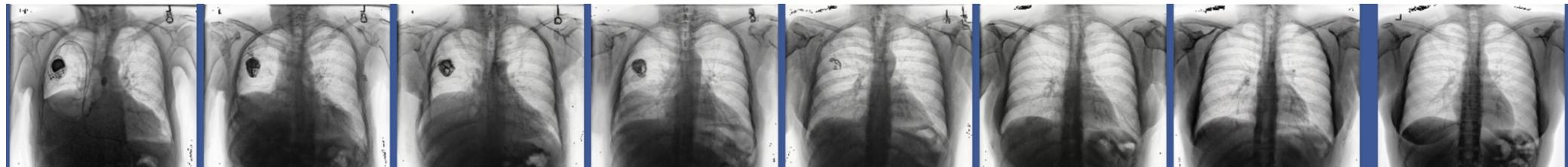


B



DDIM noise decoding

Output



α

0

0.1

0.2

0.4

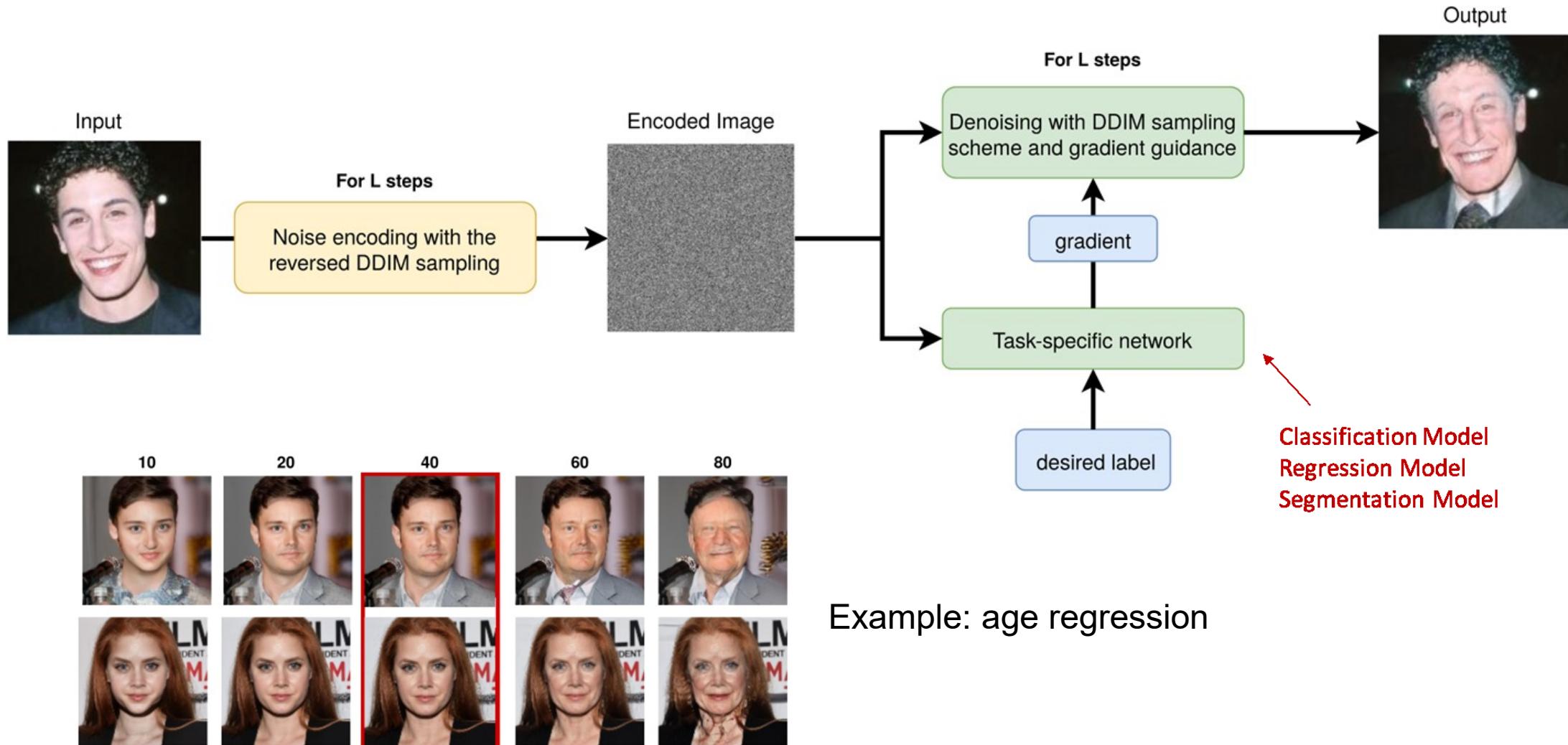
0.5

0.6

0.8

1

DDIM Inversion & Gradient Guidance



Conditioning

1. Inference-time

1. An inverse problem view
 - Classifier guidance
2. DDIM inversion
 - Interpolation
 - Gradient guidance

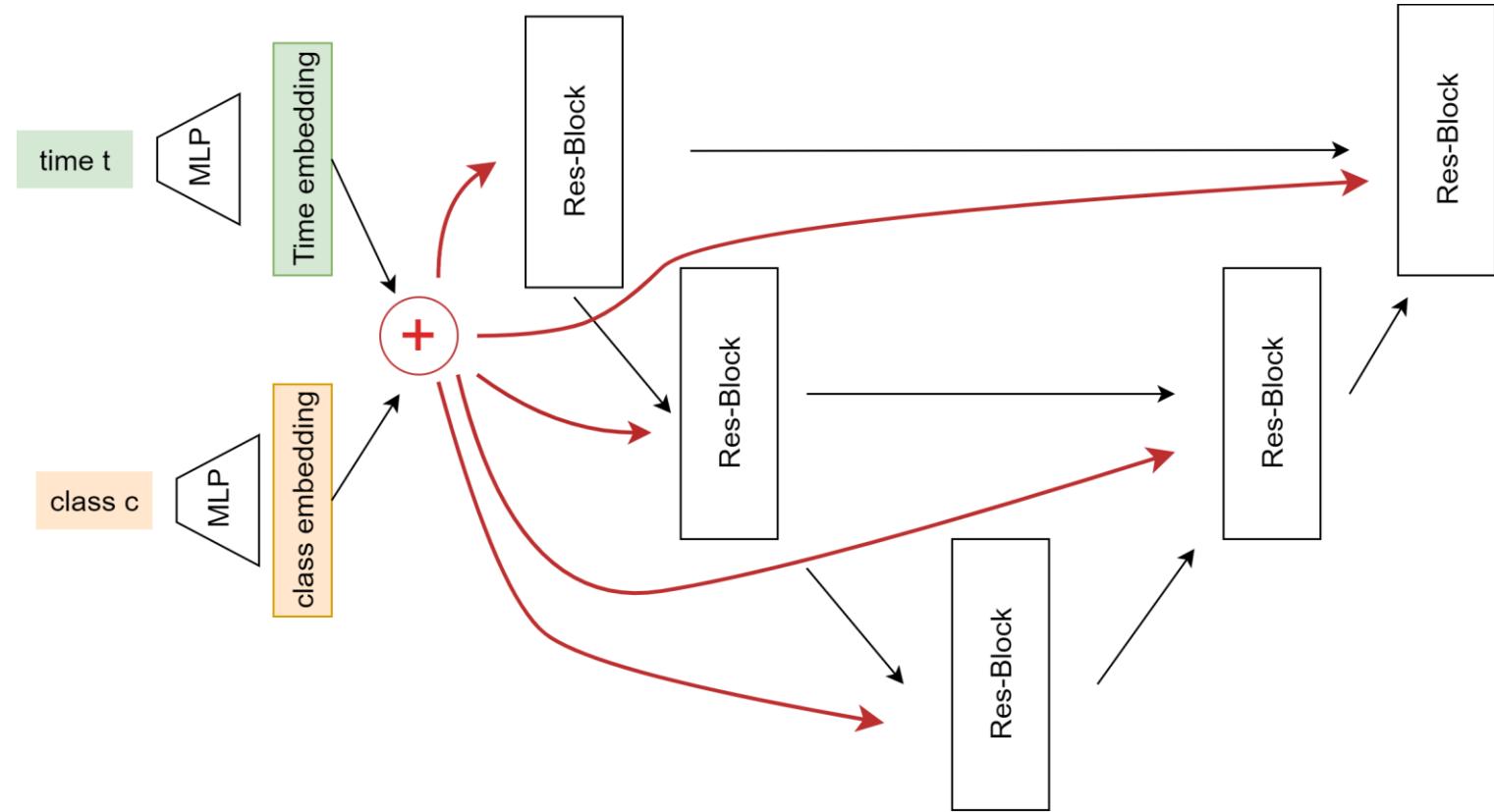
2. Training-time

1. Scalar inputs
2. Text
3. Images
4. ControlNet
5. DreamBooth

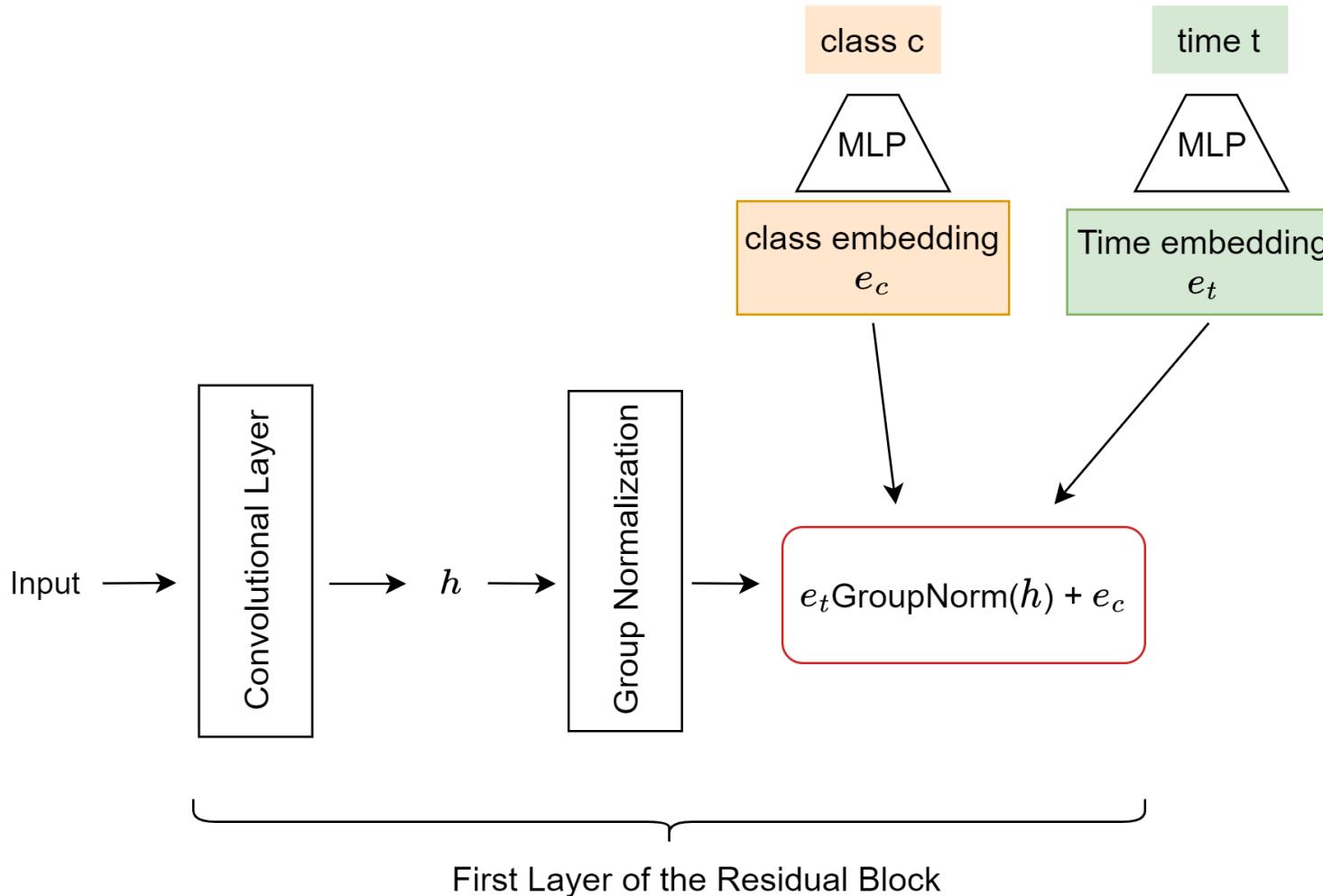


Scalar Conditioning via Spatial Addition

- We train a class-conditional diffusion model by including a class label c .
- We compute a class embedding, and pass it to the residual blocks by **spatial addition**.

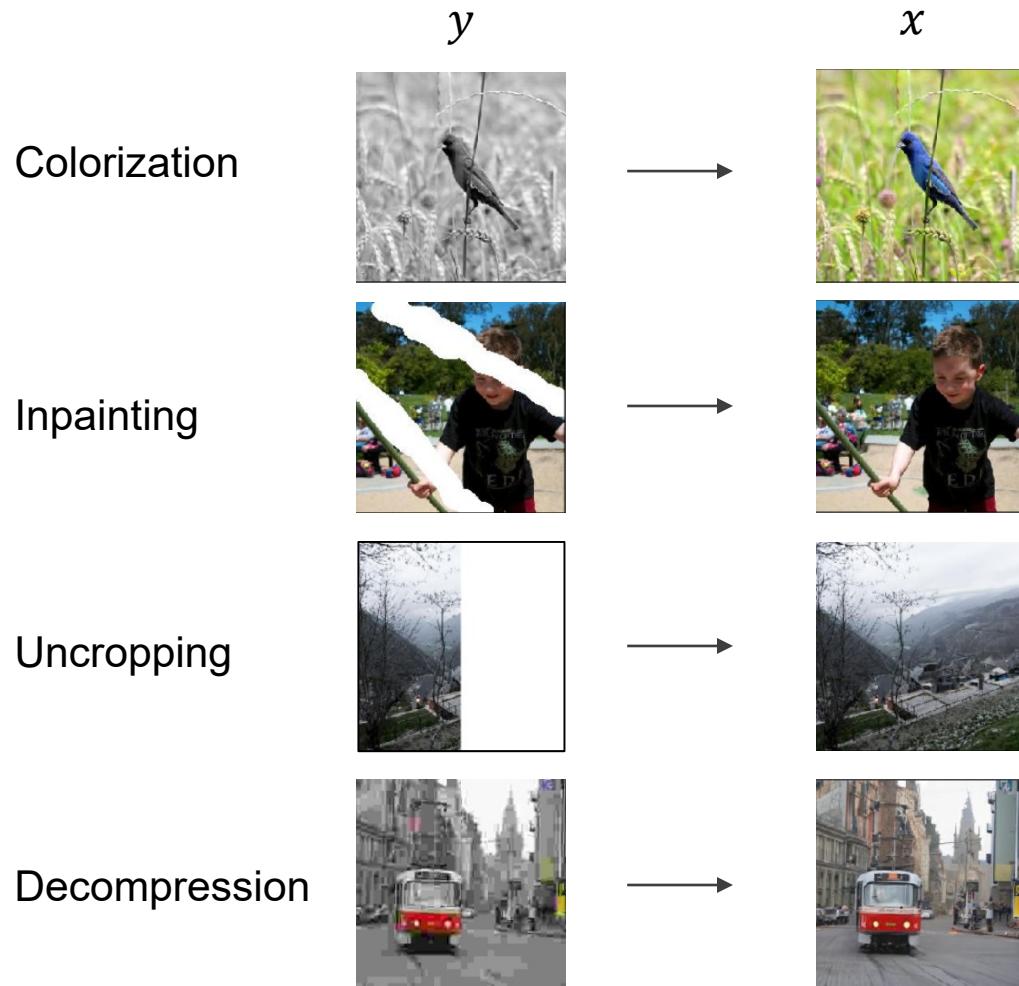


Scalar Conditioning via Adaptive Group Normalization



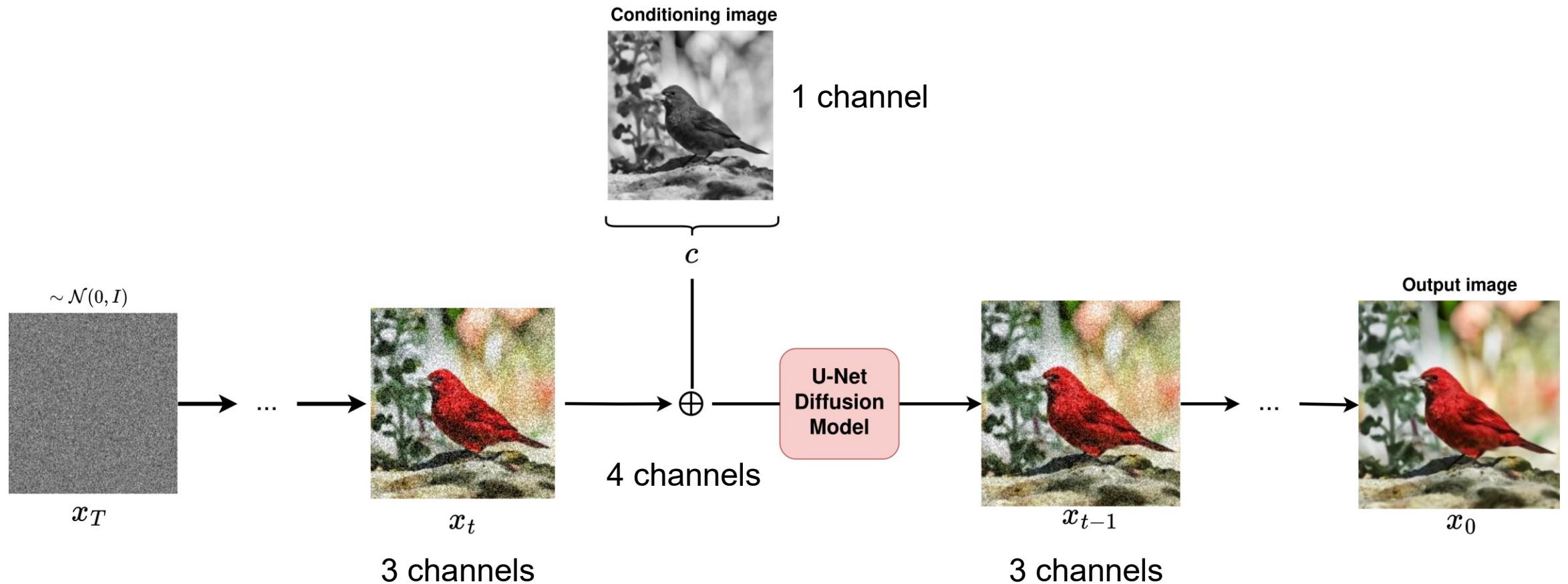
- Similar to StyleGAN, we add time and class information using a group normalization layer.
- This happens in all residual blocks of the U-Net.

Image Conditioning through Concatenation

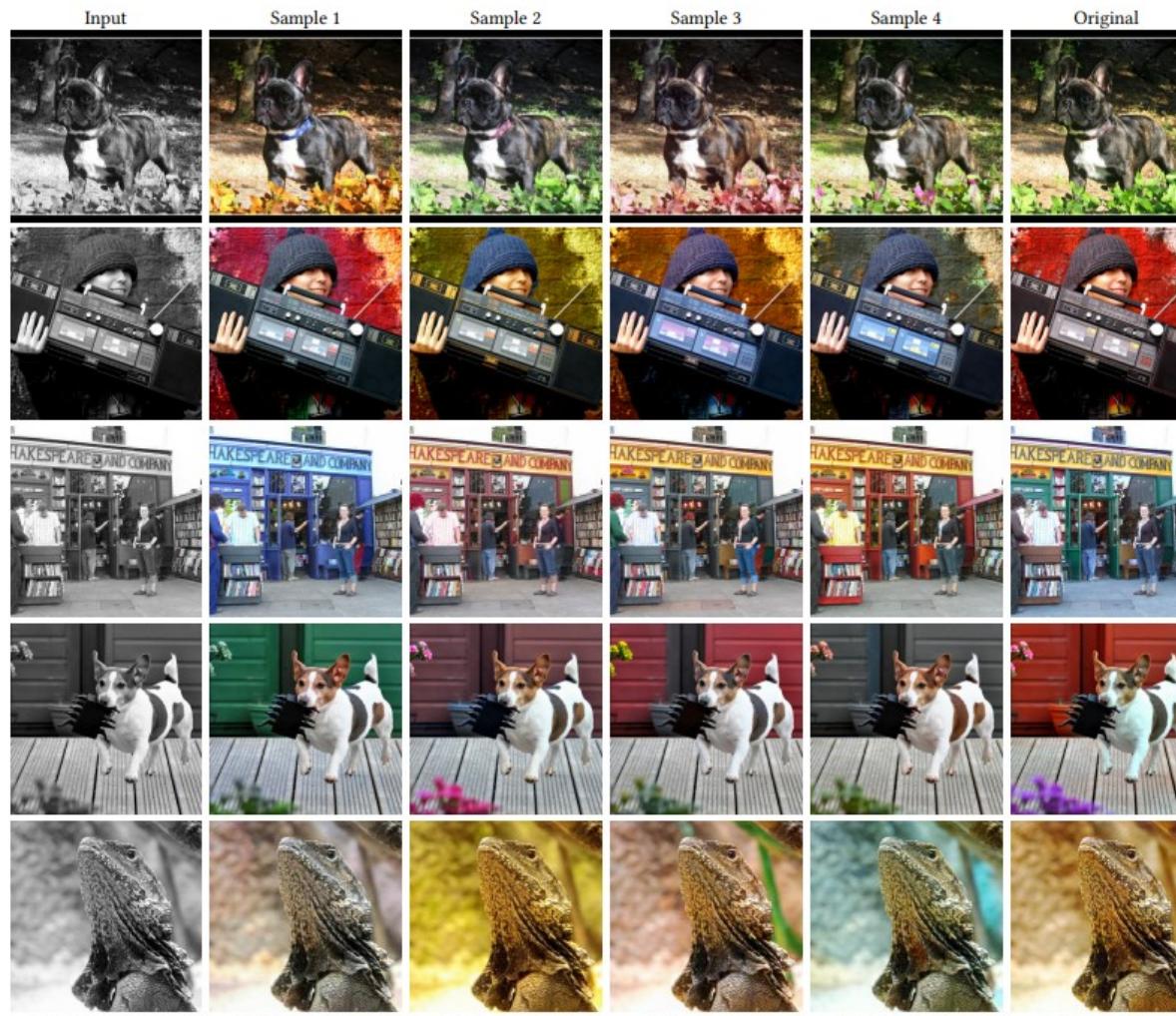


- For image generation of a fake image x , we can use a conditioning image y .
- This requires **paired** training.
- During training and sampling, we add information of the conditioning image x through **channel-wise concatenation**.

Image Conditioning through Concatenation



Palette: Image-to-Image Diffusion Models



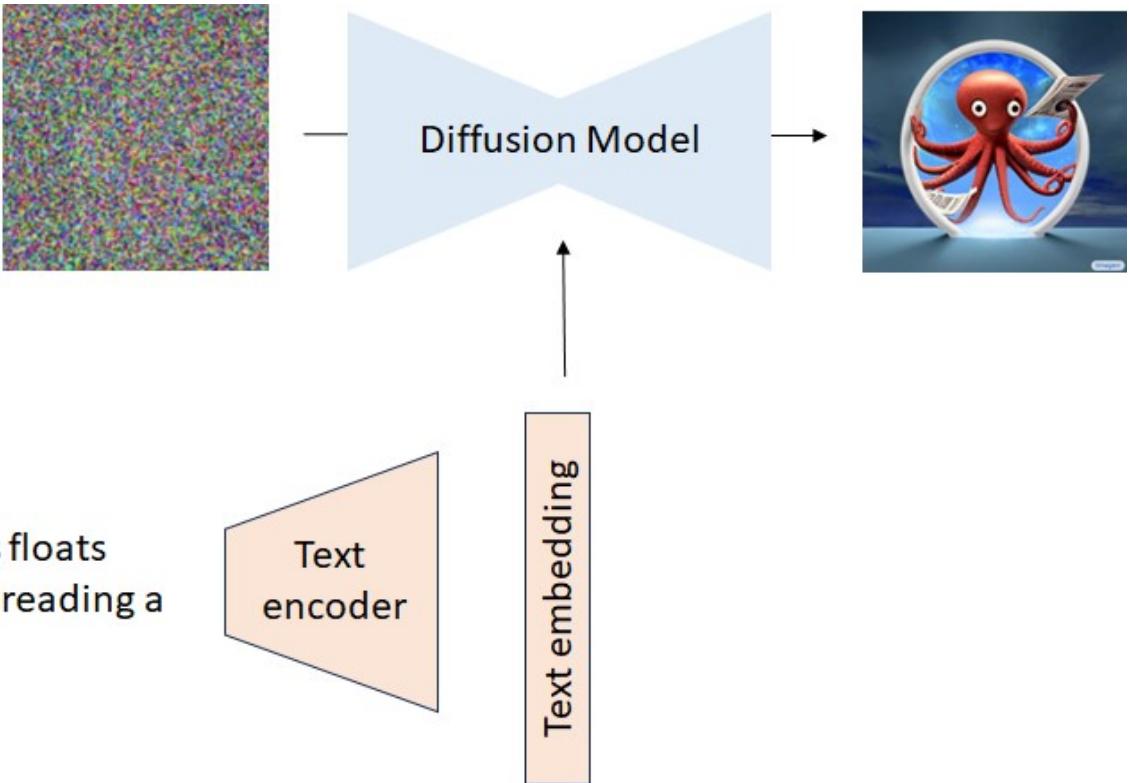
Text Conditioning



"A small cactus wearing a straw hat and neon sunglasses in the Sahara desert."

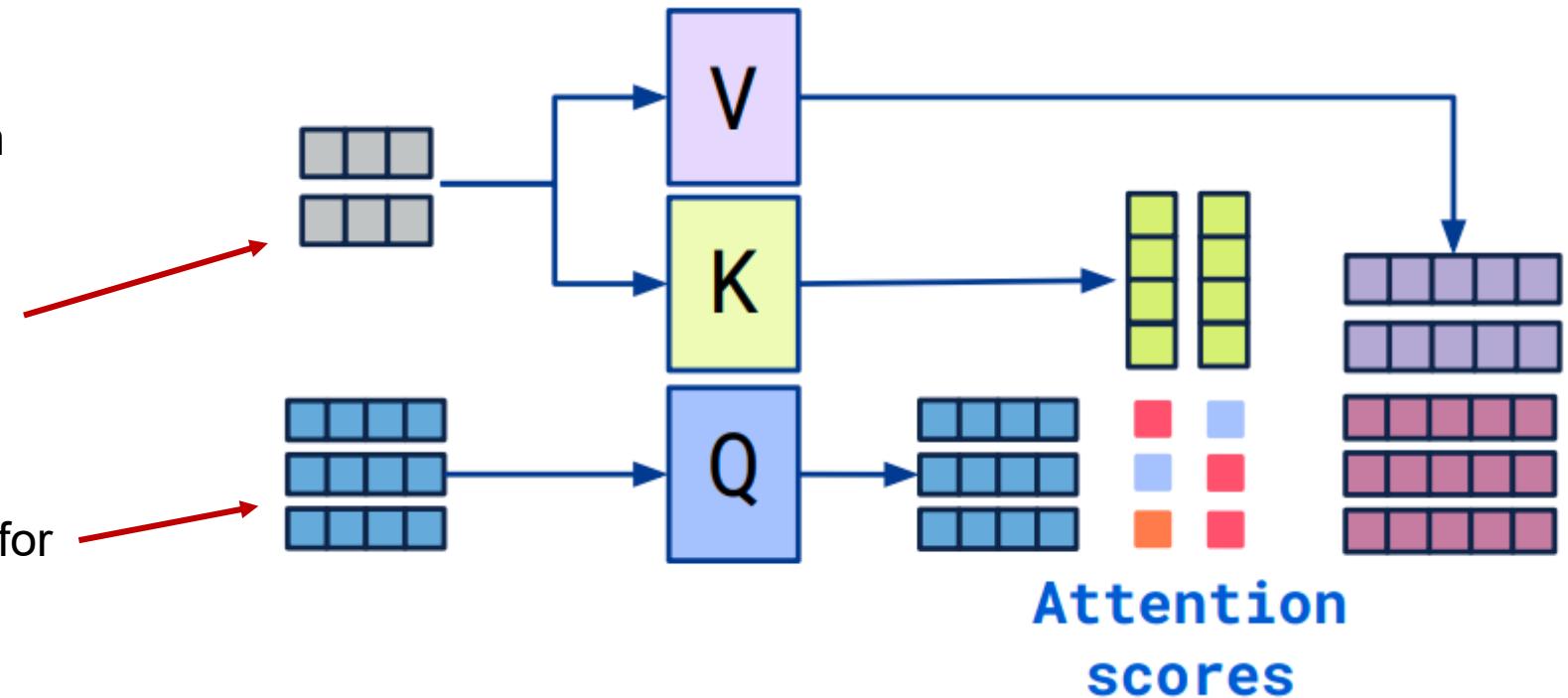
- CLIP
- Dall-E
- Stable Diffusion
- Imagen
- ...

An alien octopus floats through a portal reading a newspaper.

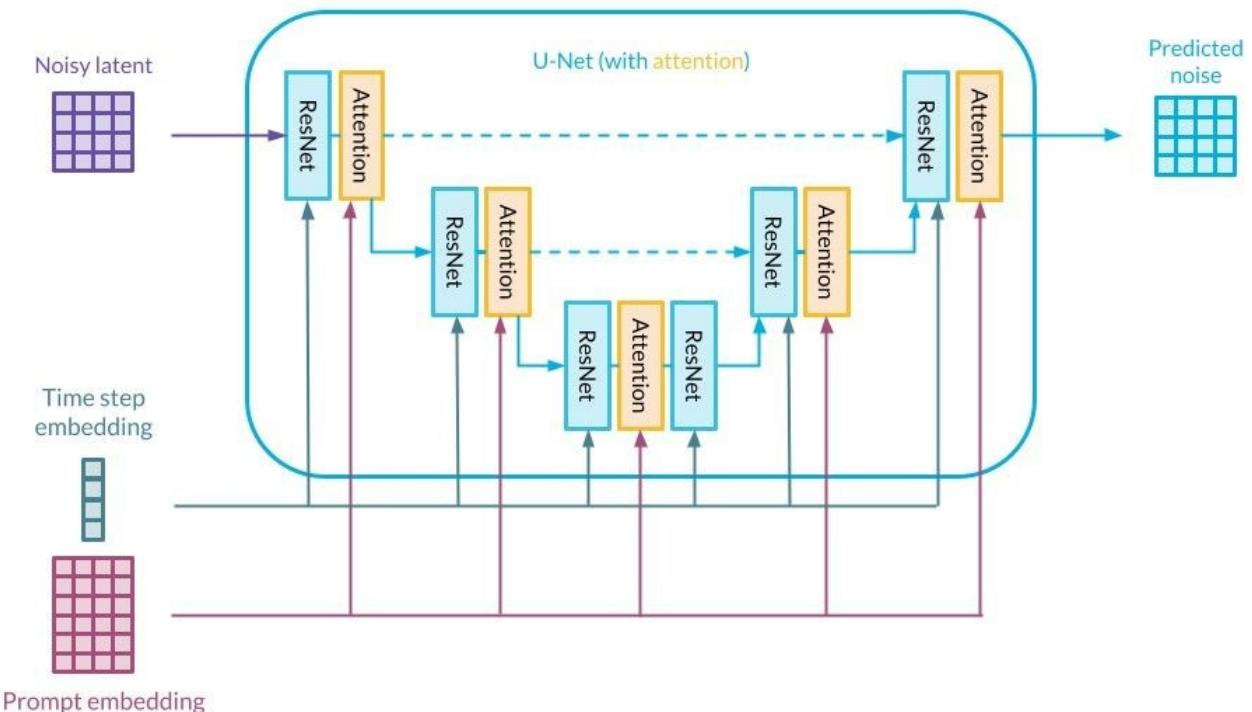
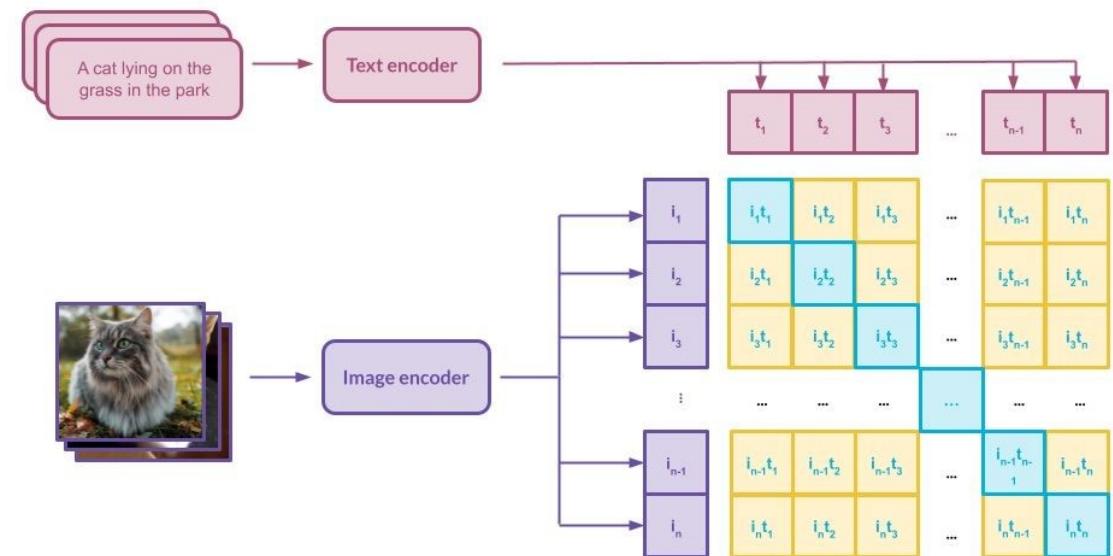


Architecture - Conditioning

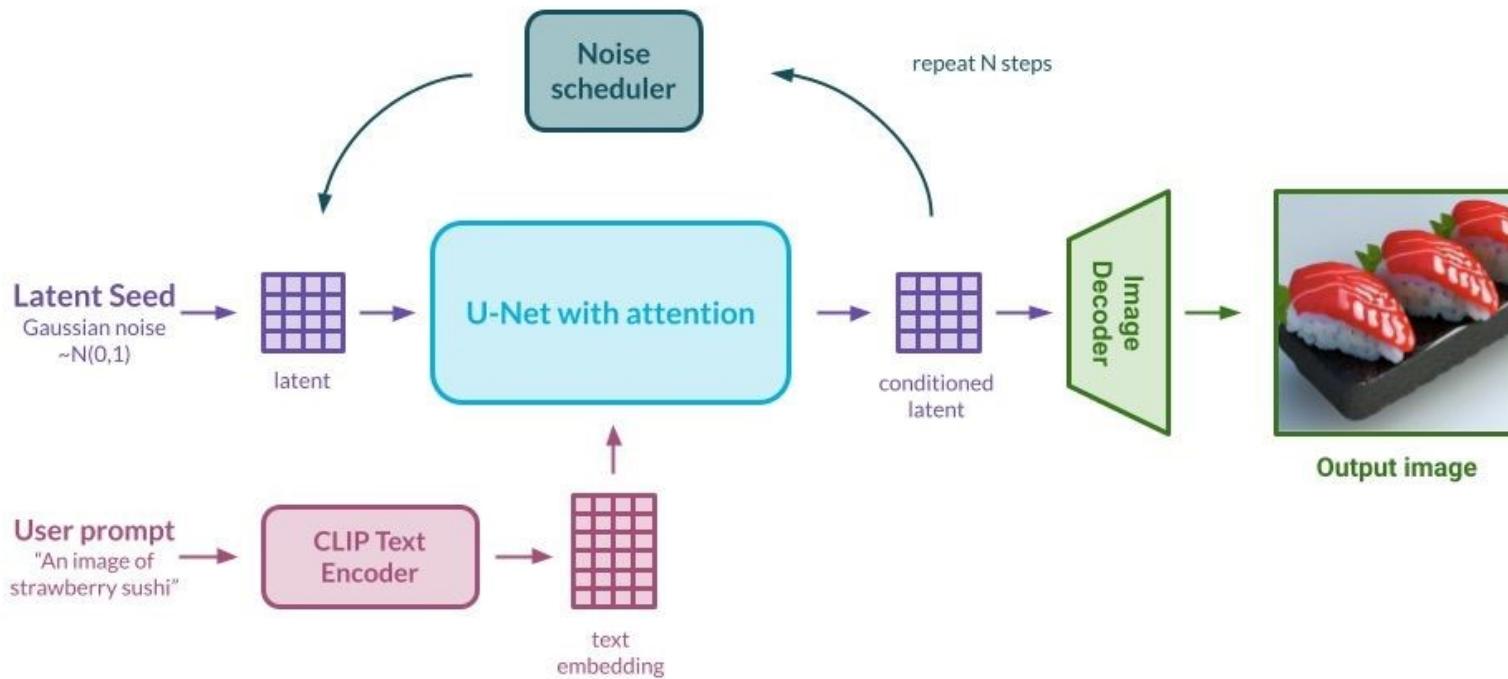
- Transformers **Cross-Attention**
- We use the text embedding to generate the key / value pair.
- We use the image embedding for the query.



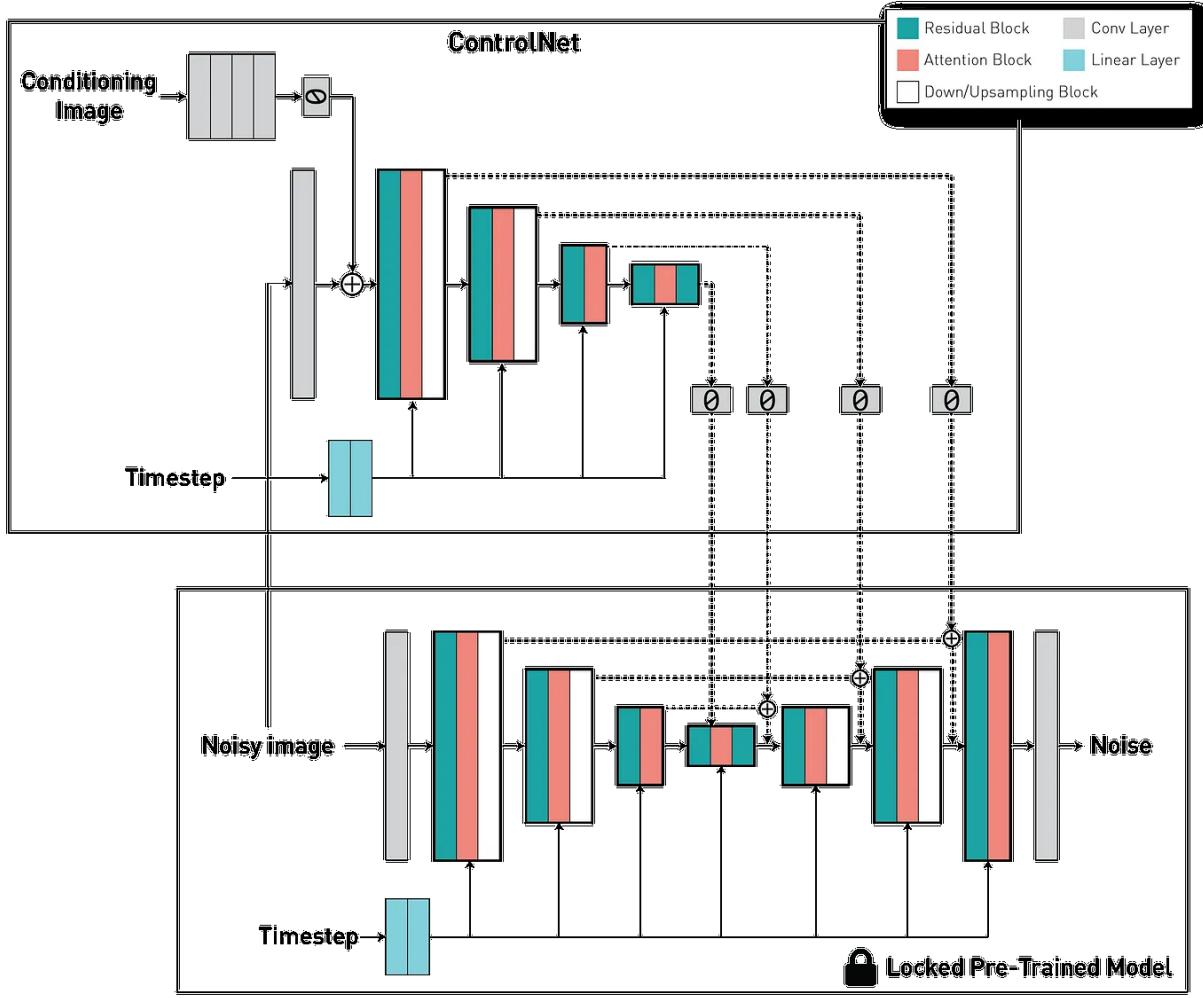
Text Conditioning



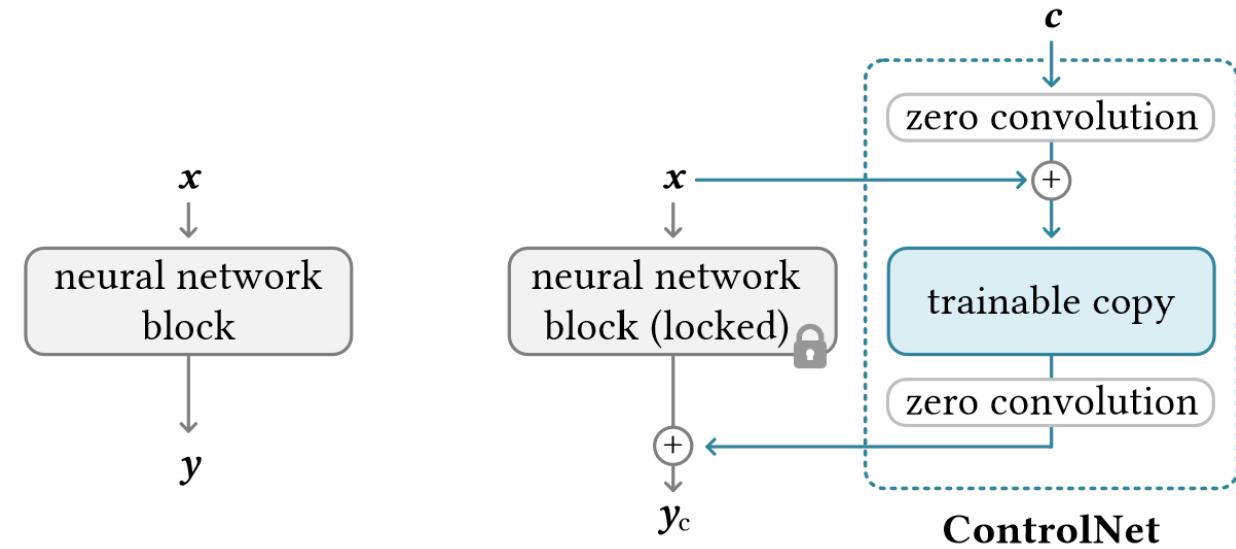
Text Conditioning



ControlNet

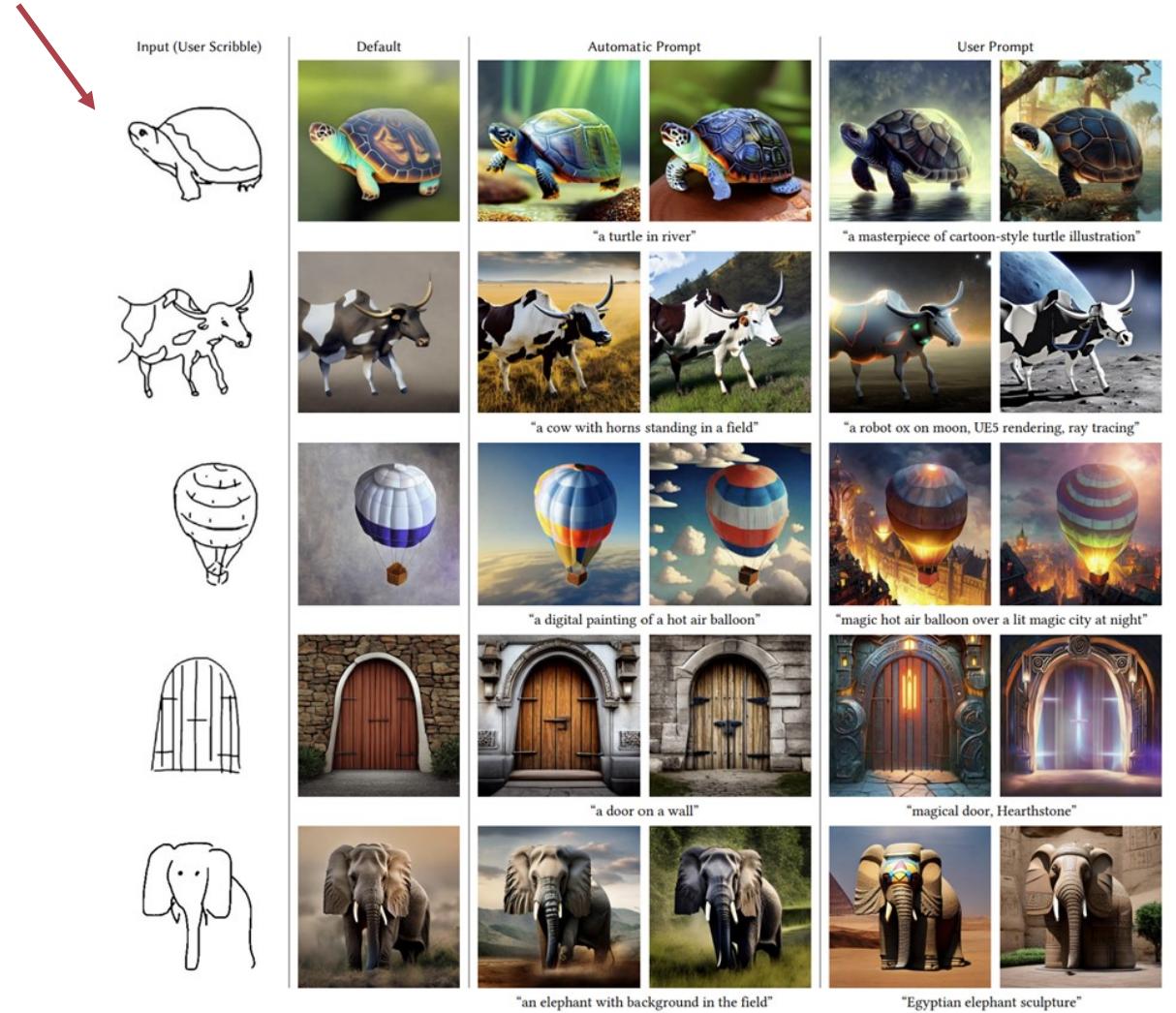
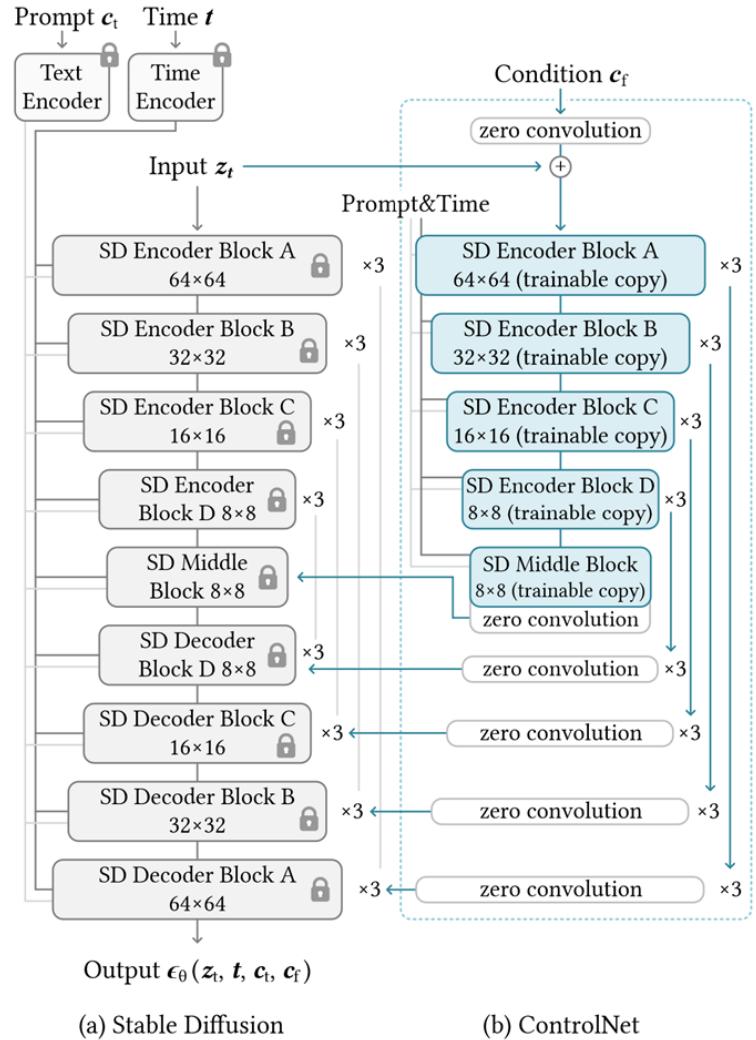


- We pretrain a diffusion model with text prompts.
- We freeze this model.
- We fine-tune a copy conditioned on c .
- We pass information through skip connections.

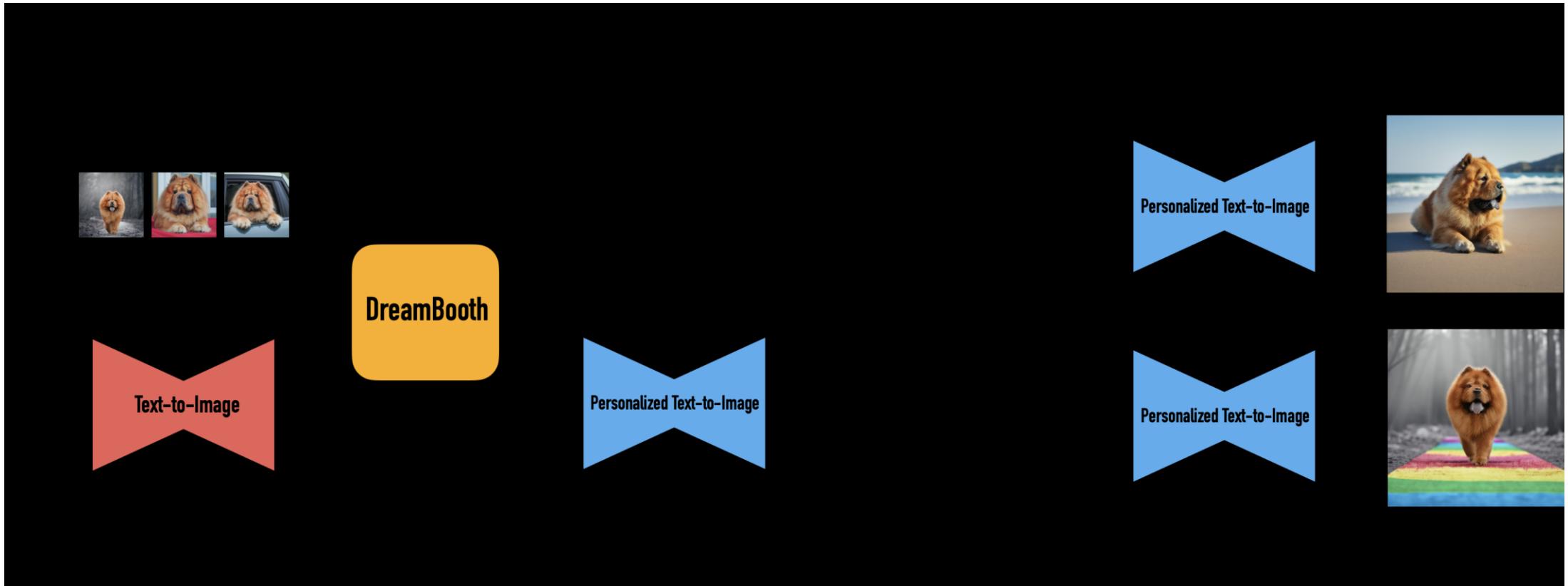


ControlNet

conditioning image



DreamBooth

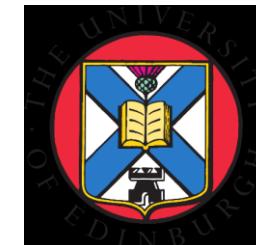
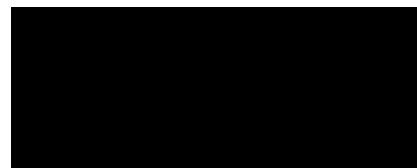


DEMO



Generative Models

DDIM Inversion + Classifier-Free Guidance



UNIVERSITAT DE
BARCELONA



Icahn School
of Medicine at
**Mount
Sinai**

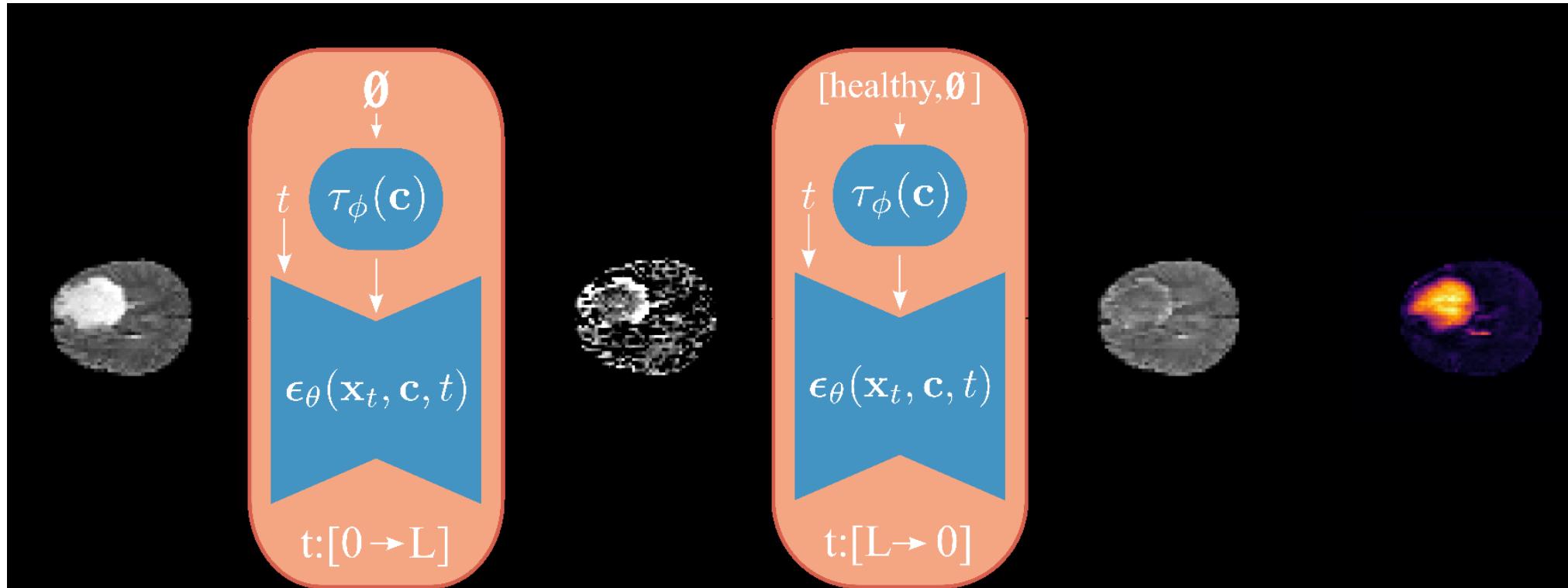


Stanford
University

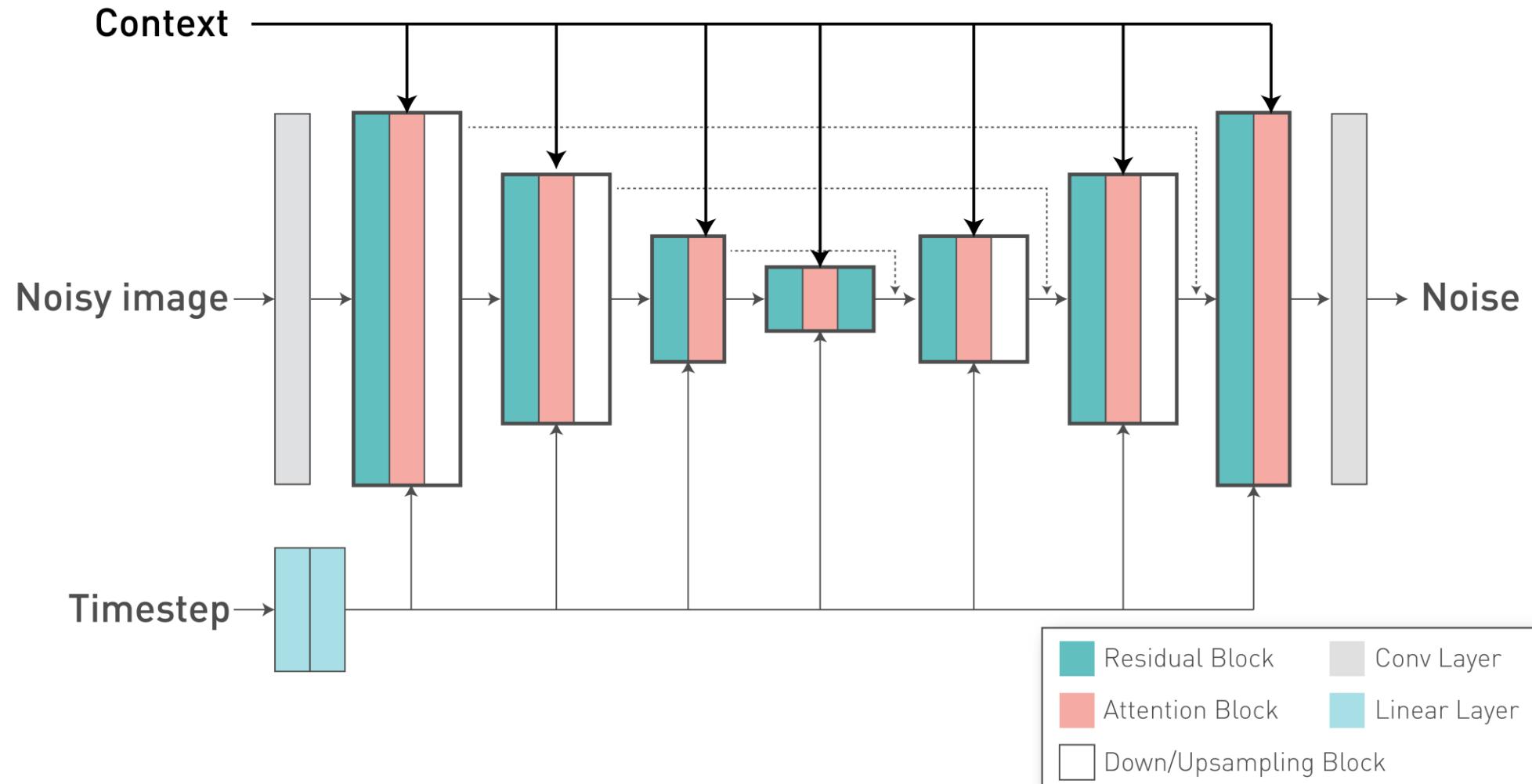


DEMO - Conditioning

1. Scalar Conditioning
2. Classifier-free guidance
3. DDIM Inversion



Conditional Unet

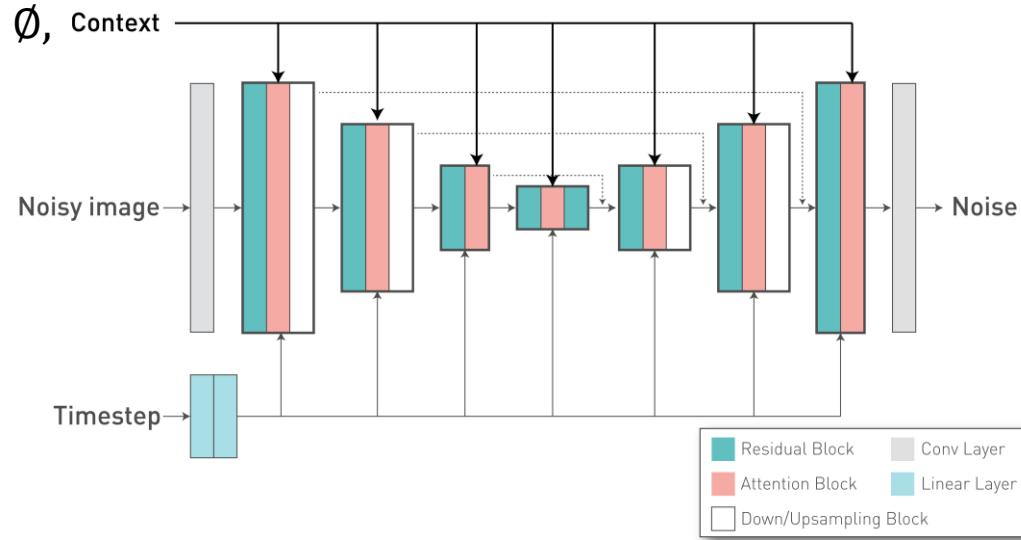


Conditional Unet

```
from generative.networks.nets import DiffusionModelUNet

model = DiffusionModelUNet(
    ...
    num_channels=[256, 256, 512],
    attention_levels=[False, True, True],
    num_head_channels=[0, 256, 512],
    with_conditioning=True,
    cross_attention_dim=768,
)
...
noise_pred = model(x=noisy_image,
                    timesteps=timesteps,
                    context=context)
```

Classifier-free Guidance

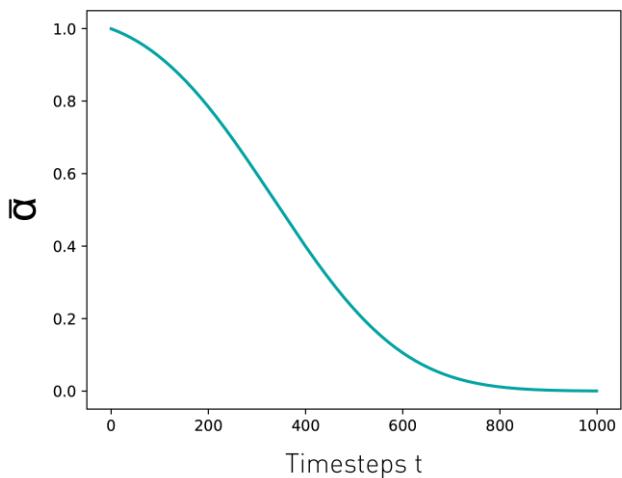


$$\widetilde{\epsilon}_{\theta}(x_t|y) = \epsilon_{\theta}(x_t|\emptyset) + w[\epsilon_{\theta}(x_t|y) - \epsilon_{\theta}(x_t|\emptyset)]$$

Classifier-free Guidance

```
def classifier_free_guidance(noise, t, conditioning, w):  
  
    conditioning = torch.cat([torch.zeros(1), conditioning])  
    noise_input = torch.cat([noise] * 2)  
    model_output = model(noise_input, timesteps=t, context=conditioning)  
    noise_pred_uncond, noise_pred_text = model_output.chunk(2)  
  
    noise_pred = noise_pred_uncond + w * (noise_pred_text - noise_pred_uncond)  
  
    return noise_pred
```

Noise Schedulers



```
from generative.networks.schedulers import  
DDIMScheduler  
  
scheduler = DDIMScheduler(  
    num_train_timesteps=1000,  
    beta_schedule="scaled_linear",  
    beta_start=0.0005,  
    beta_end=0.0195,  
)
```

Training

```
...
for batch in train_loader:
    # classes {1: unhealthy, 2: unhealthy}
    images, classes = batch["image"], batch["classes"]
    # dropout classes 15% of the time
    classes = classes * (torch.rand_like(classes) > 0.15)
    optimizer.zero_grad(set_to_none=True)

    noise = torch.randn_like(images).to(device)
    timesteps = torch.randint(0, scheduler.num_train_timesteps,(images.shape[0],))
    noisy_image = scheduler.add_noise(original_samples=images,
                                       noise=noise,
                                       timesteps=timesteps,)

    noise_pred = model(x=noisy_image, timesteps=timesteps, context=classes)

    loss = F.mse_loss(noise_pred.float(), noise.float())
...
```

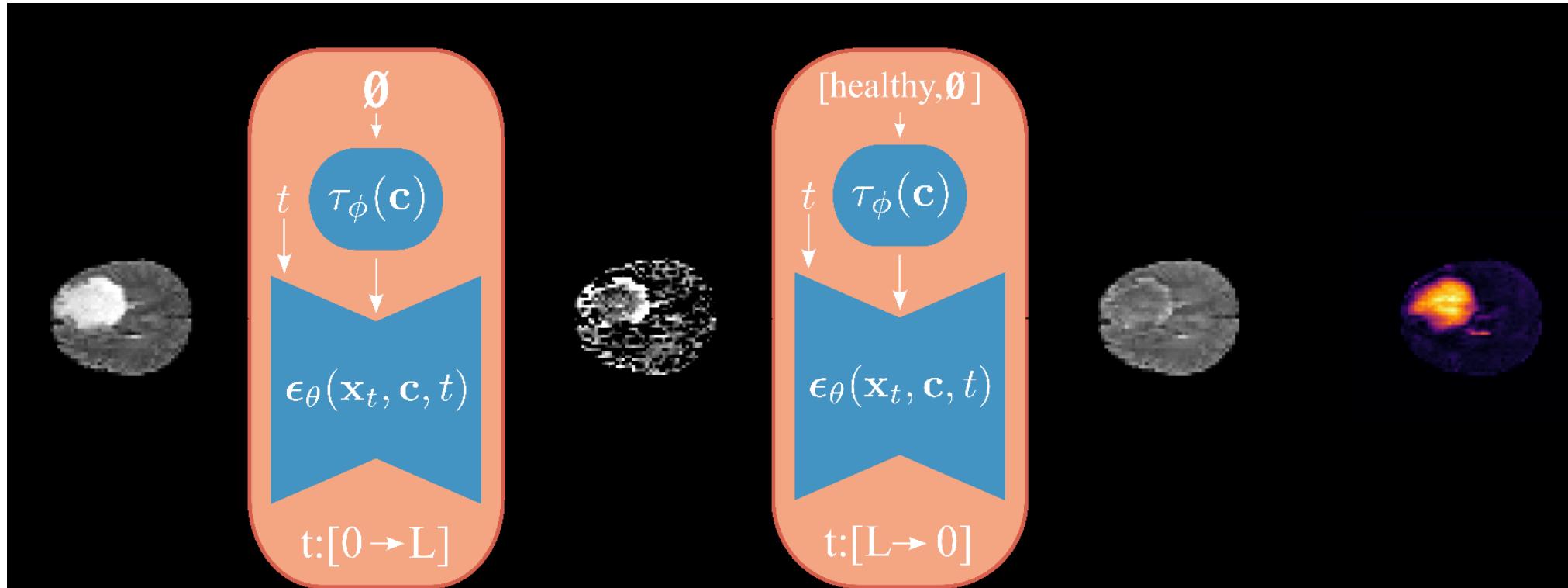
Sampling – DDIM Inversion + Guidance

```
L = 200
conditioning = torch.zeros(1)
scheduler.set_timesteps(num_inference_steps=1000)
current_img = batch["image"]
for t in range(L): # 0 -> L timesteps
    with torch.no_grad():
        model_output = model(current_img, timesteps=(t,), context=conditioning)
    current_img, _ = scheduler.reversed_step(model_output, t, current_img)
latent_space_L = current_img
```

```
conditioning = torch.ones(1) # Manipulate to be healthy
noise = latent_space_L
for i in range(L):
    t = L - i # t goes from L -> 0
    noise_pred = classifier_free_guidance(noise, t, conditioning, w)
    noise, _ = scheduler.step(noise_pred, t, noise)
image = noise
```

DEMO – Recap

1. Scalar Conditioning
2. Classifier-free guidance
3. DDIM Inversion



Part 2 – Q&A



Part 3 – Medical Image Applications

Image Reconstruction

Image Registration

Anomaly Detection

Image Segmentation

Image-to-Image Translation

Inpainting

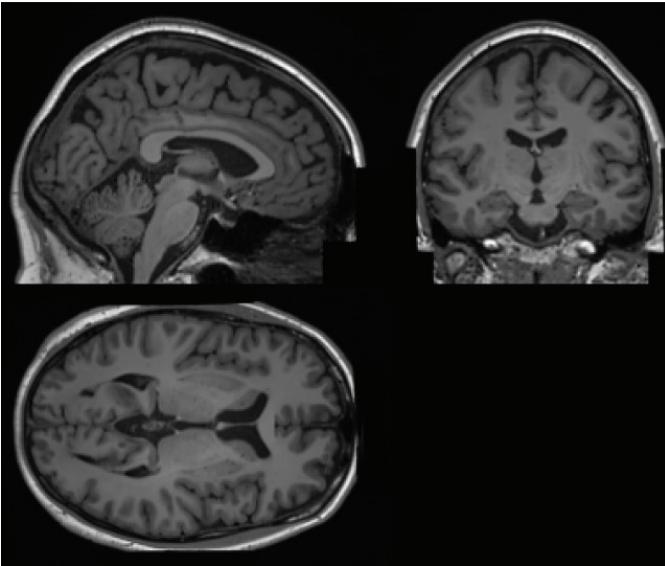
Image Synthesis

Image synthesis

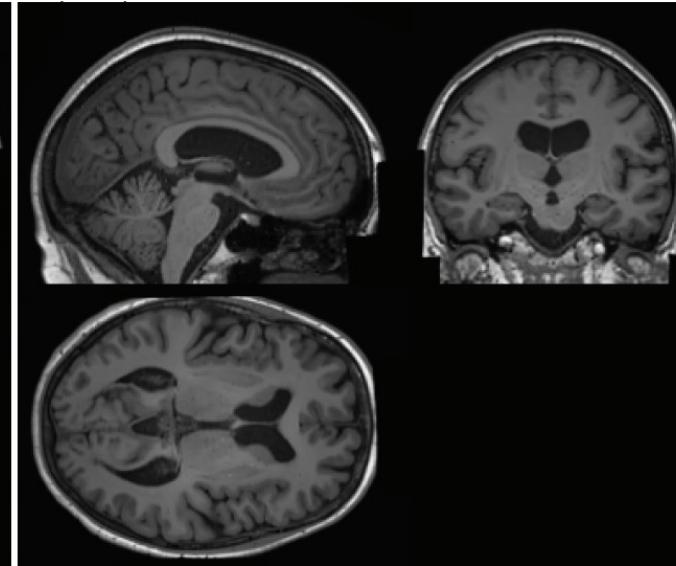
Examples from the community

The simple setup of the problem

Real



Synthetic

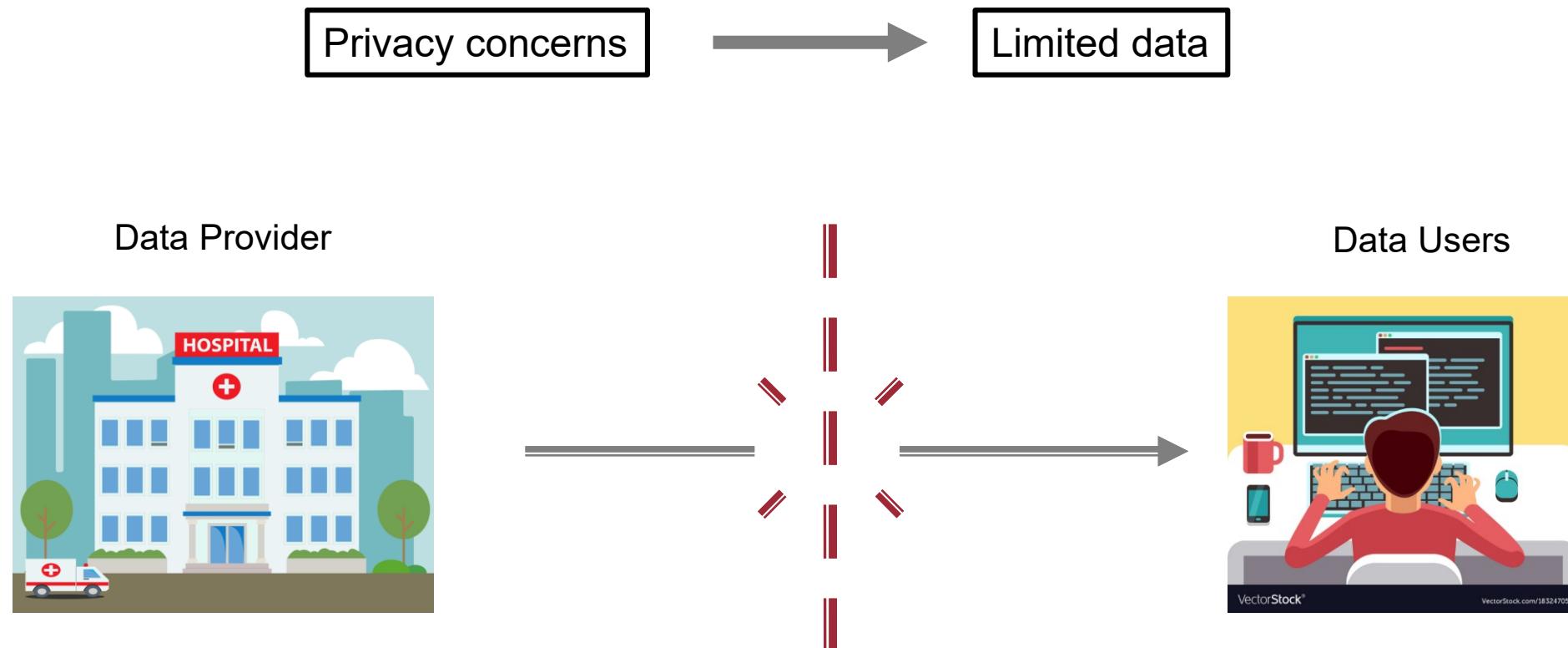


PAPERS

- Pinaya et al (2022) Brain Imaging Generation with Latent Diffusion Models. MICCAI workshop
Kim et al. (2022) Diffusion Deformable Model for 4D Temporal Medical Image Generation. MICCAI
Khader et al. (2022) Medical Diffusion -- Denoising Diffusion Probabilistic Models for 3D Medical Image Generation. arXiv:2211.03364
Packhäuser et al. (2022) Generation of Anonymous Chest Radiographs Using Latent Diffusion Models for Training Thoracic Abnormality Classification Systems. arXiv:2211.01323
Ali et al. (2022) Spot the fake lungs: Generating Synthetic Medical Images using Neural Diffusion Models. arXiv:2211.00902
Rouzrokh et al. (2022) Multitask Brain Tumor Inpainting with Diffusion Models: A Methodological Report. arXiv:2210.12113
Chambon et al (2022) Adapting Pretrained Vision-Language Foundational Models to Medical Imaging Domains. arXiv:2210.04133
Lyu et al. (2022) Conversion Between CT and MRI Images Using Diffusion and Score-Matching Models. arXiv:2209.12104
Ozbey et al. (2022) Unsupervised Medical Image Translation with Adversarial Diffusion Models. arXiv:2207.08208
Meng et al. (2022) A Novel Unified Conditional Score-based Generative Framework for Multi-modal Medical Image Completion. arXiv:2207.03430

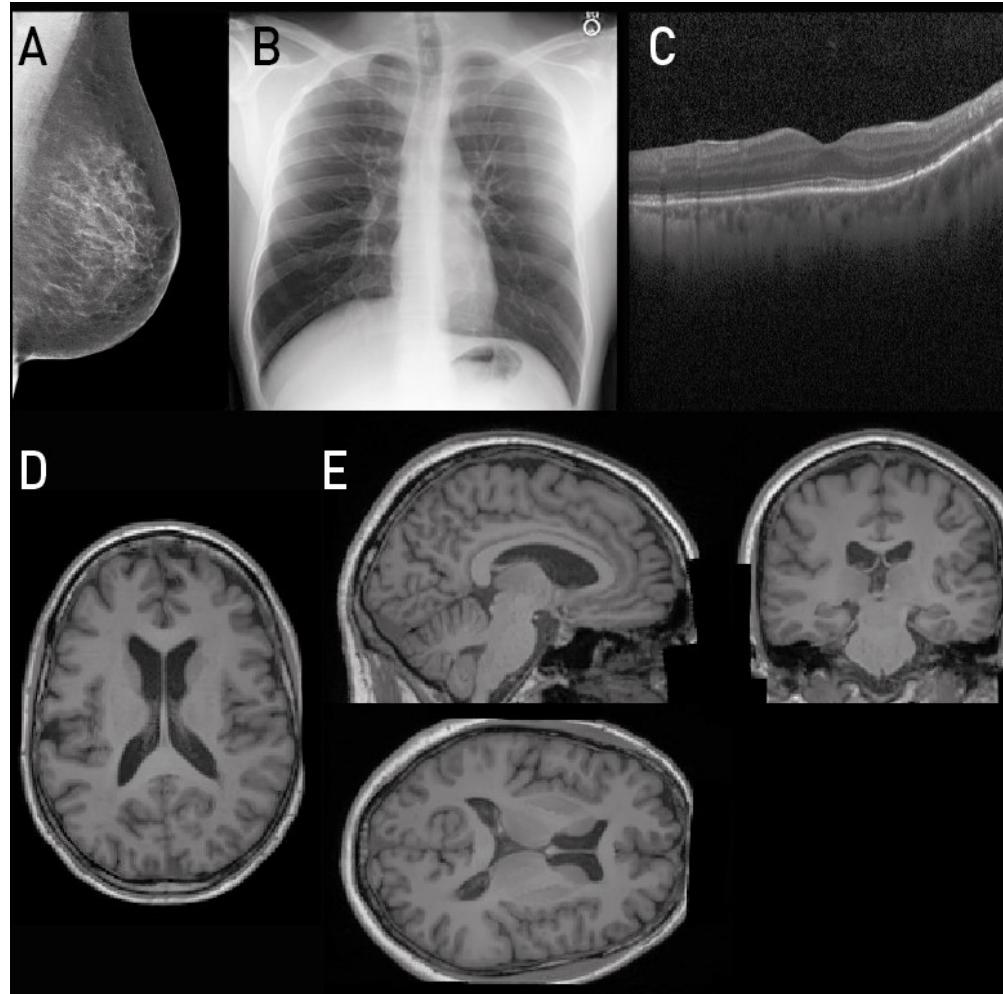
Figure by Song et al ICLR 2022.
Copyright rests with the authors.

Why? Medical Image Data is Scarce



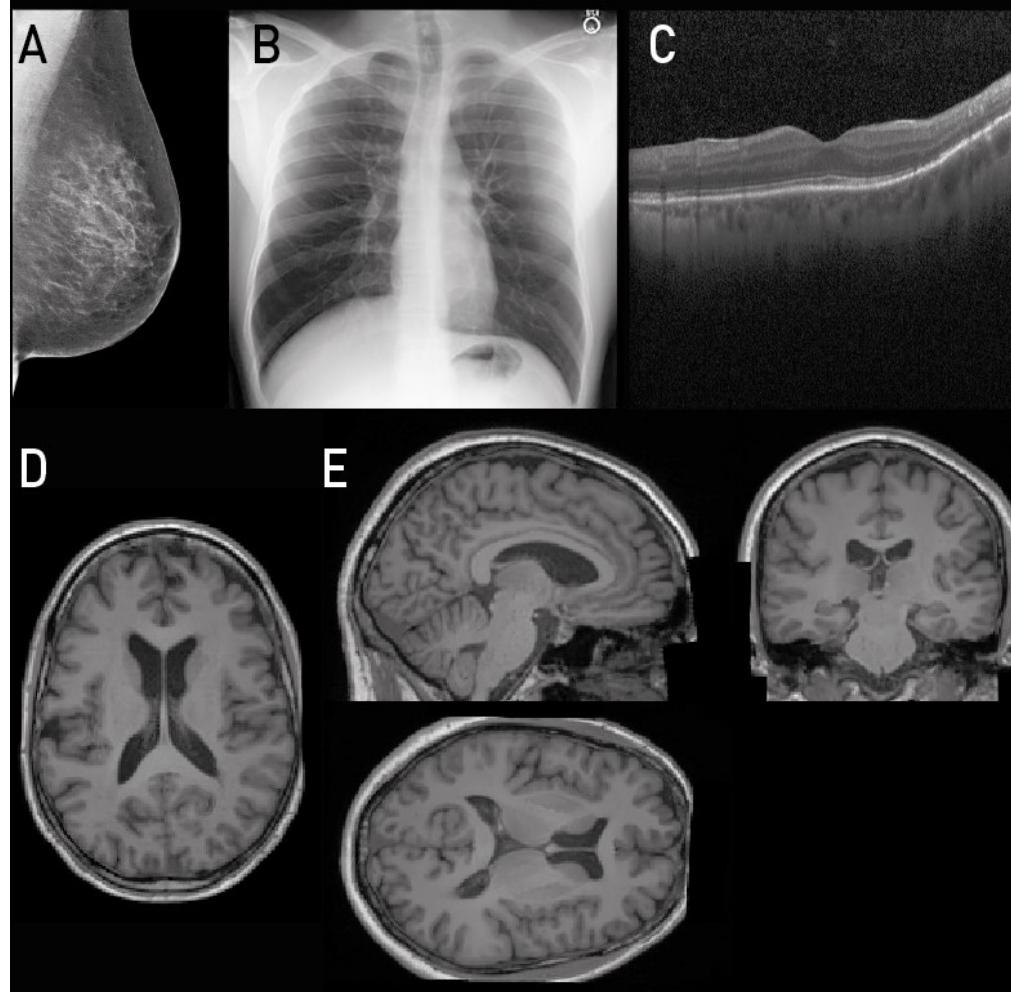
Use of Synthetic Data

- Full “private” training
- Data augmentation
- Test-time augmentation
- Testing edge cases



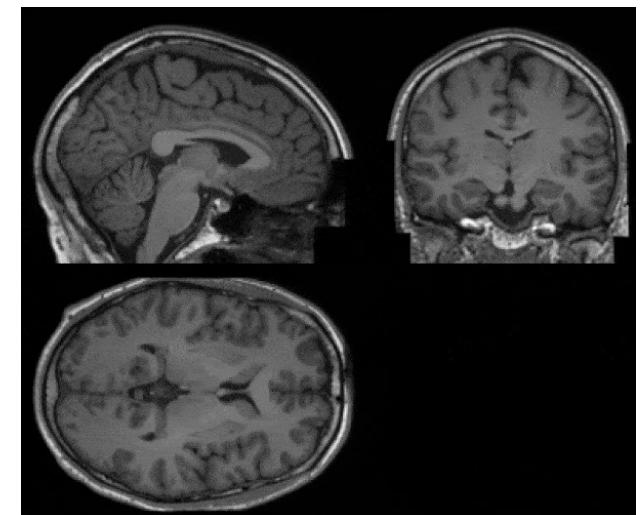
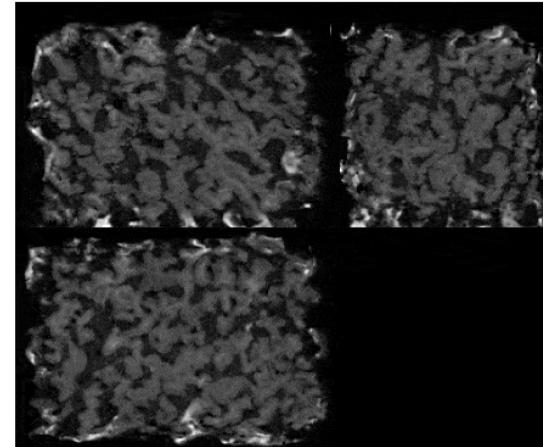
Evaluation of Synthetic Data

- Realism
- Diversity
- Privacy
- Benchmark

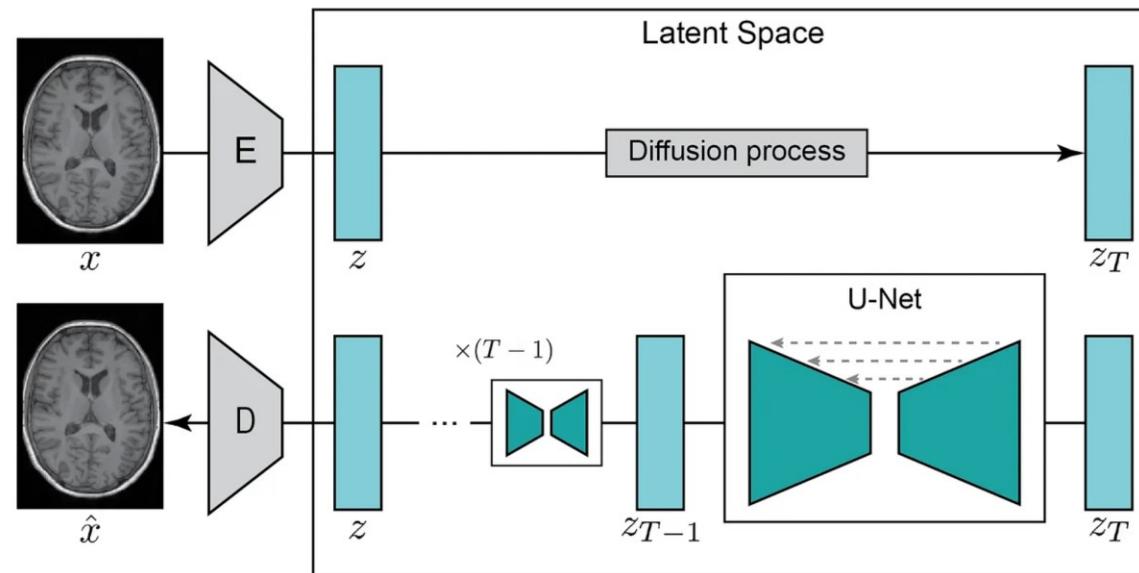


Generating high-resolution 3D brain data

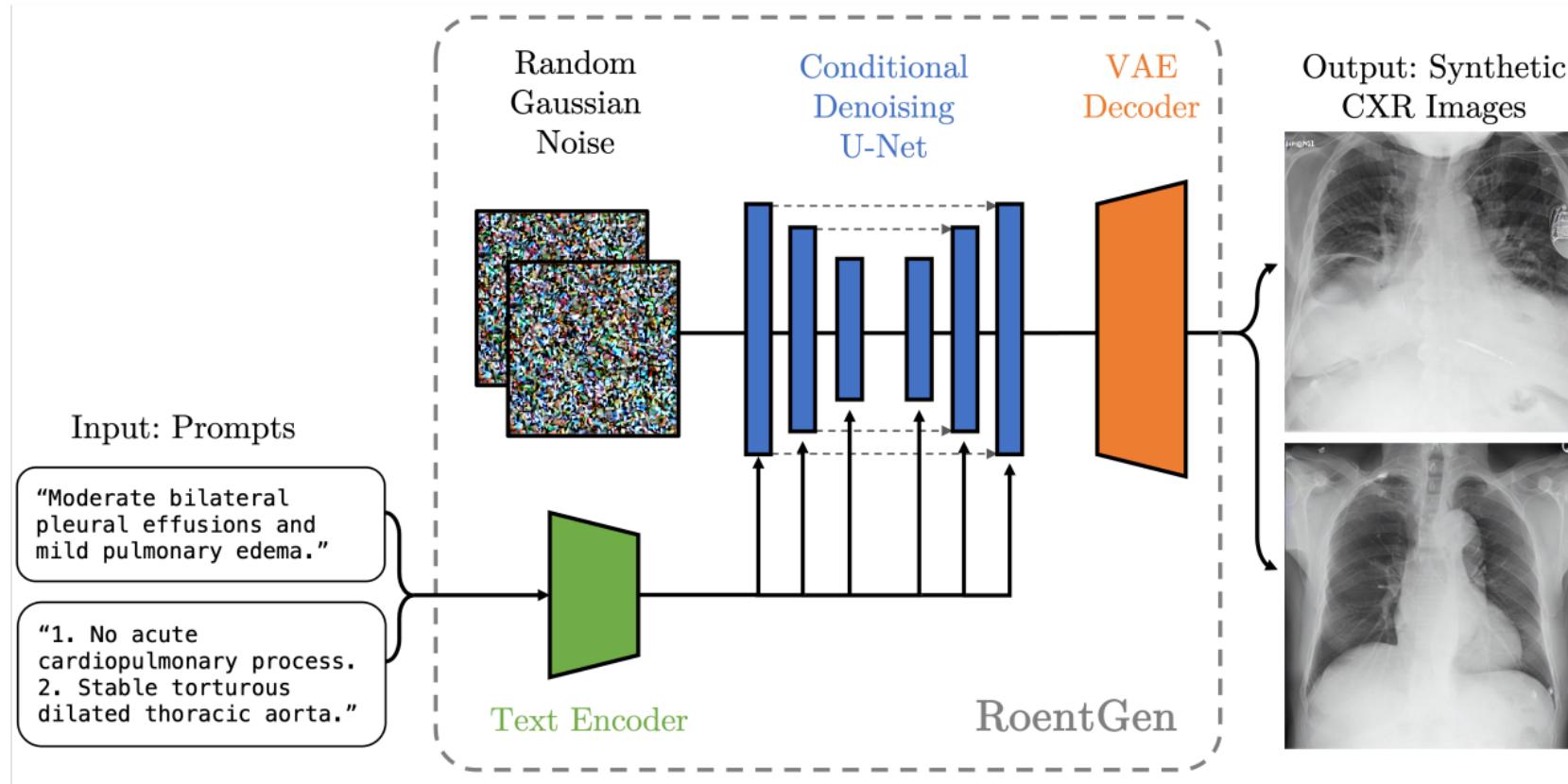
- Latent Diffusion Models trained on data from UK Biobank ($N = 31,740$)
 - T1 MRI brain images with 1 mm^3 voxel size ($160 \times 224 \times 160$ voxels)
- Conditioned on covariates, such as:
 - Age
 - Gender
 - Ventricular and Brain volumes



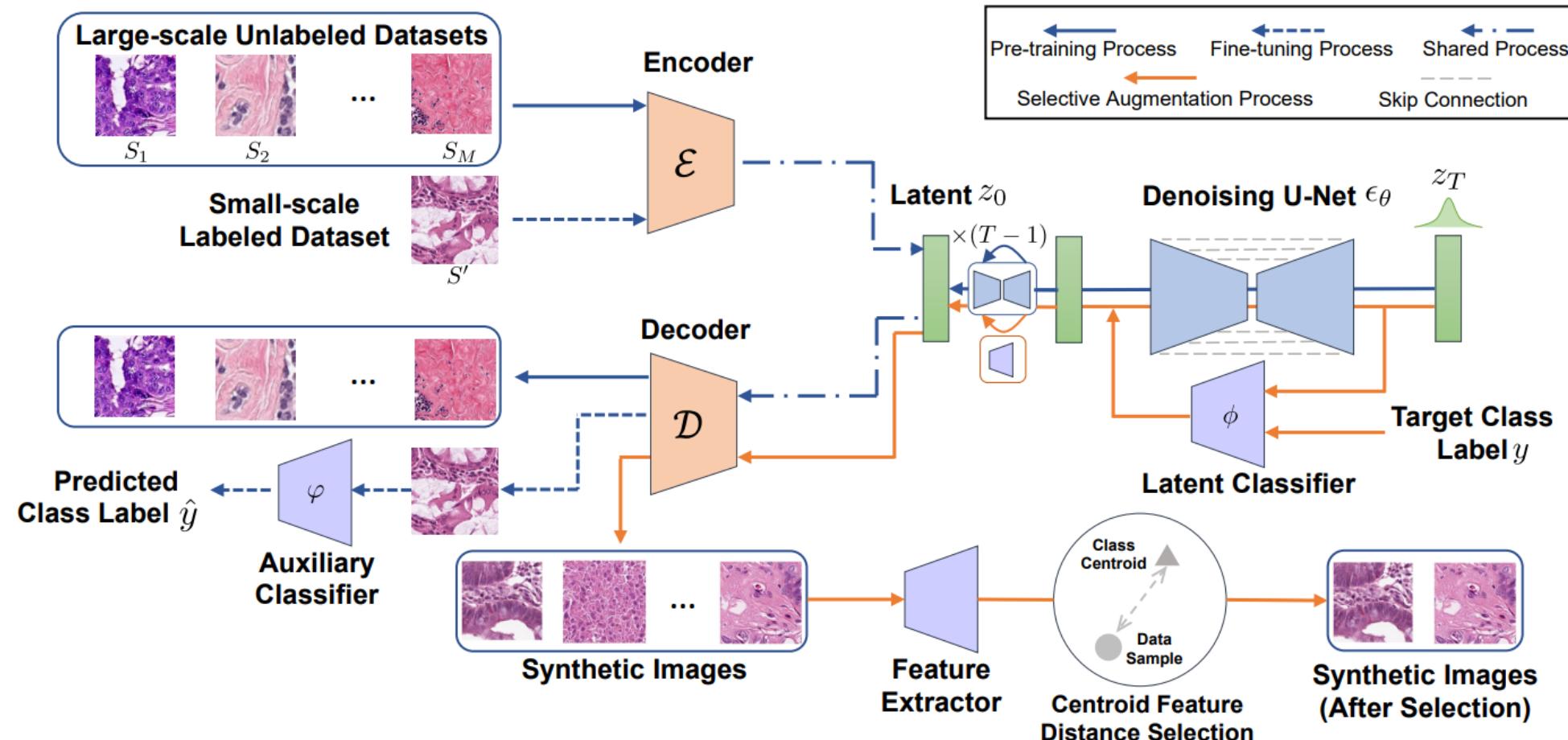
Diffusion Model in the Latent Space



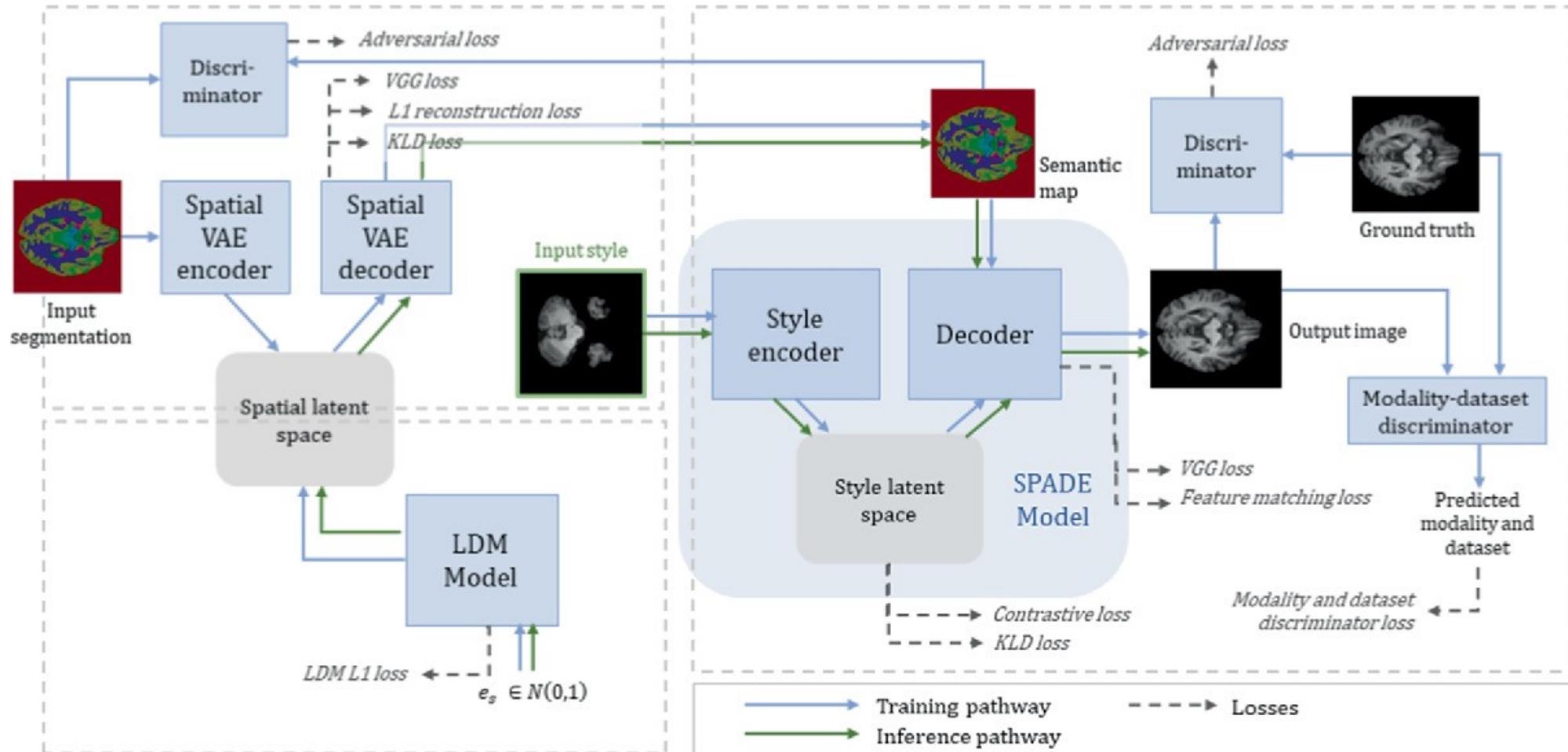
Fine-tuning Stable Diffusion



Unlabelled Pre-training



Generating Segmentation Masks



Generation of Anonymous Chest Radiographs

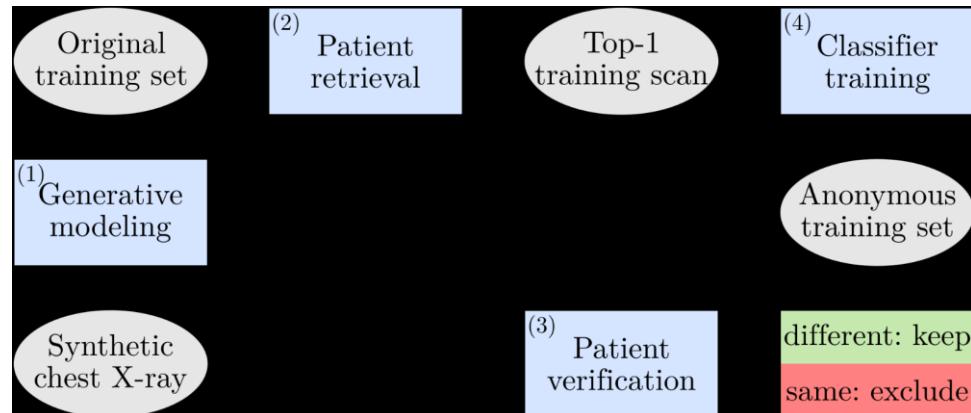


Fig. 1: Proposed privacy-enhancing image sampling strategy. Image taken from [1].

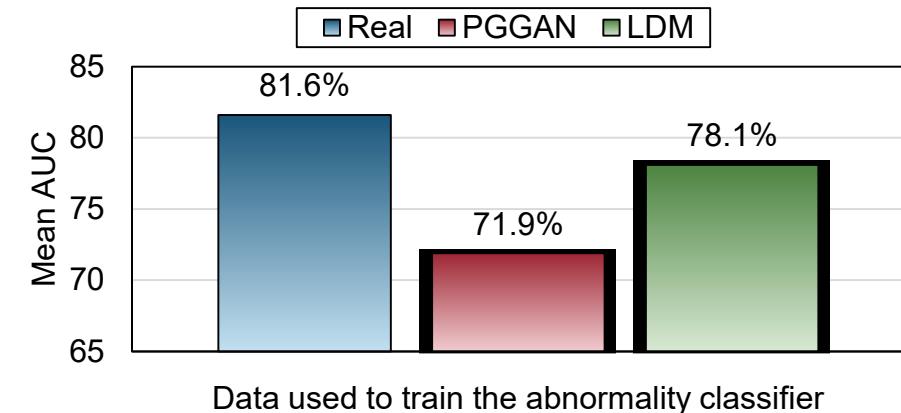


Fig. 2: Comparison of the classification performance of CheXNet.

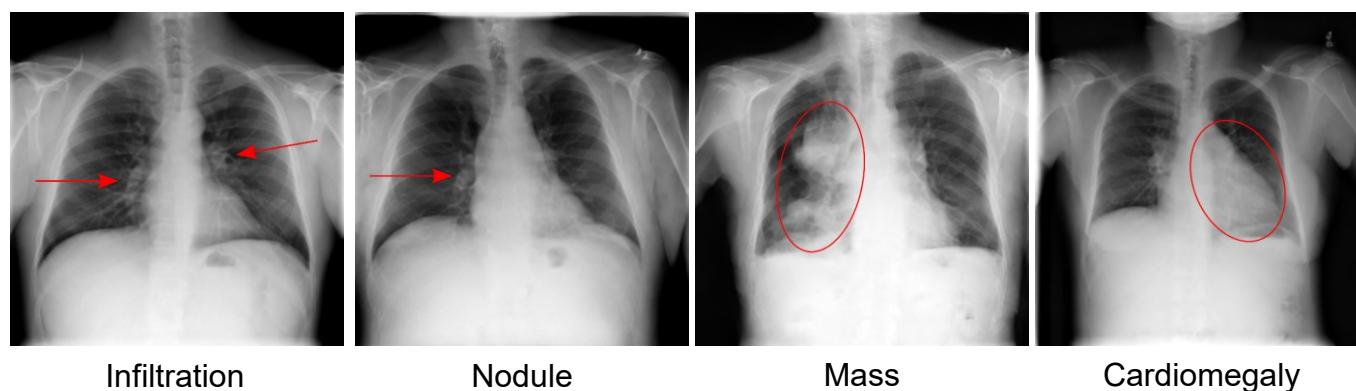
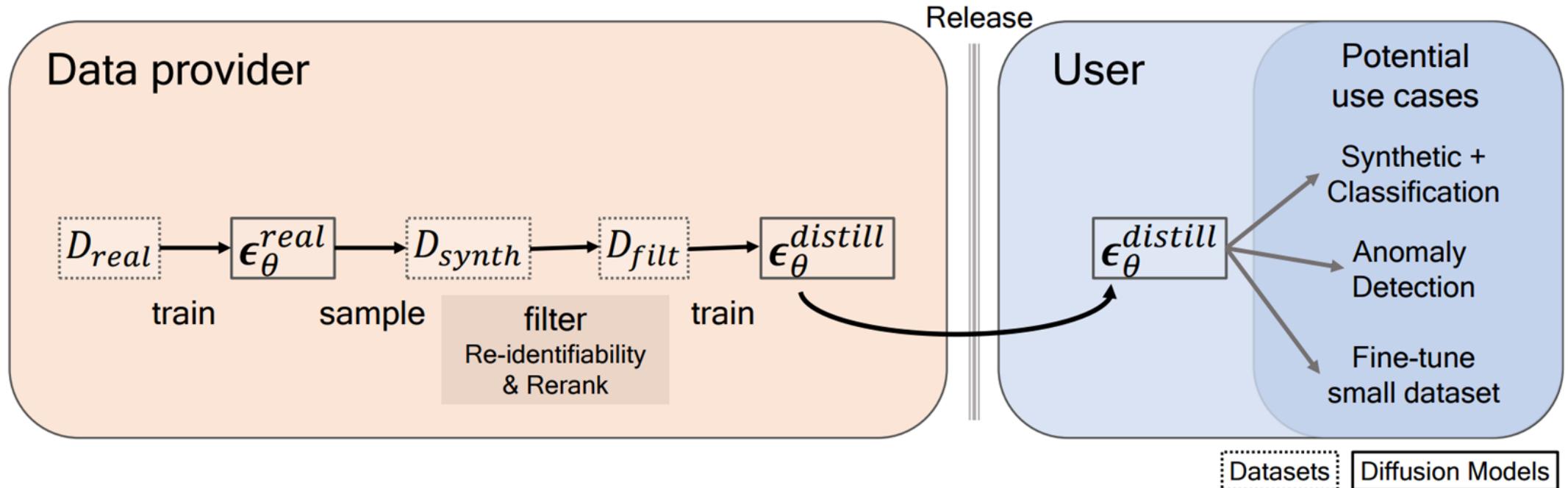


Fig. 3: Randomly selected images generated by the trained LDM. Images taken from [1].

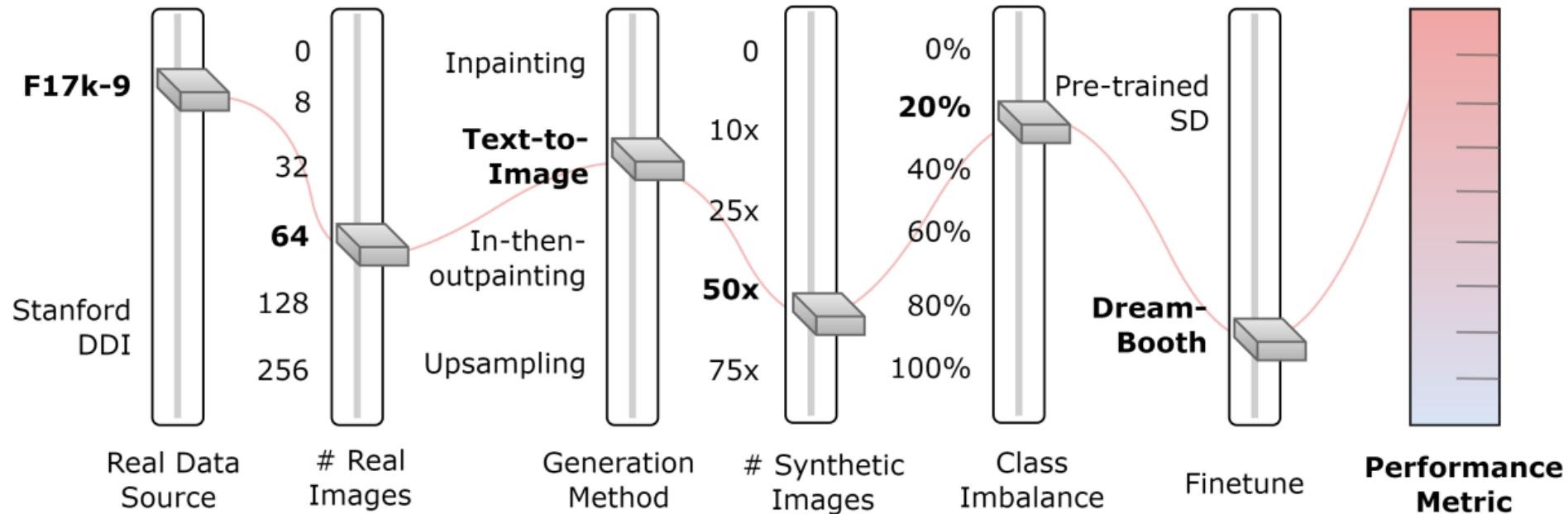
Slides courtesy of Kai Packhäuser

Privacy Distillation



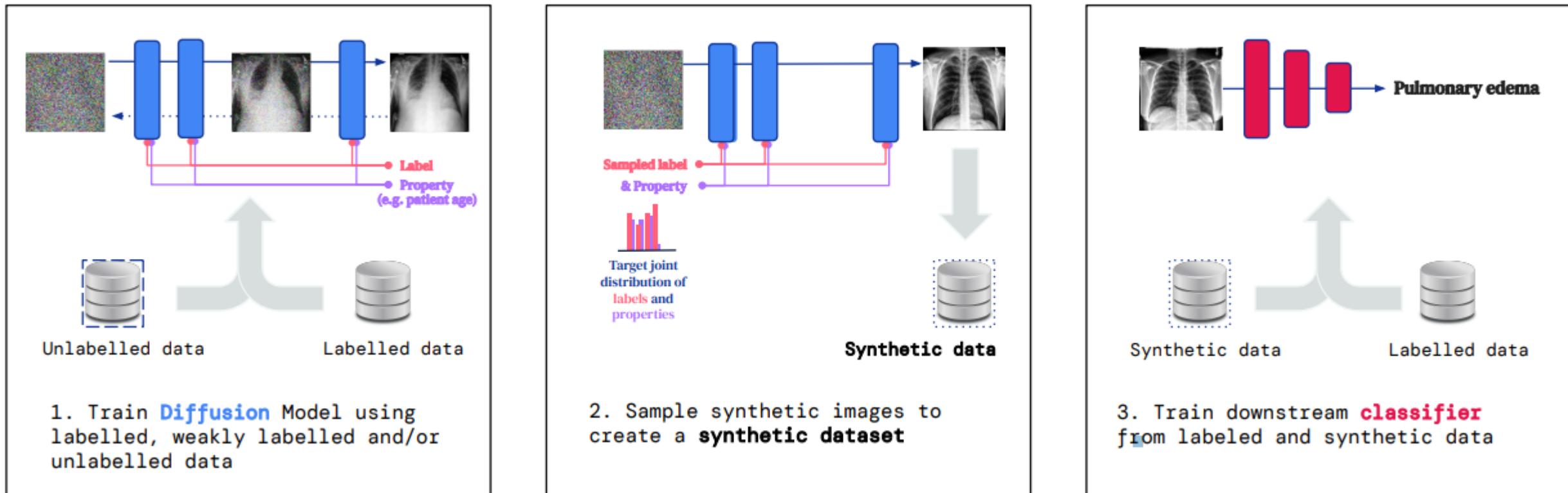
Synthetic Image Augmentation

Synthetic-to-real ratio of 10:1



Sagers, Luke W., et al. (2023) Augmenting medical image classifiers with synthetic data from latent diffusion models. arXiv:2308.12453

Synthetic Data for Distribution Shifts



Synthesising Rare Samples

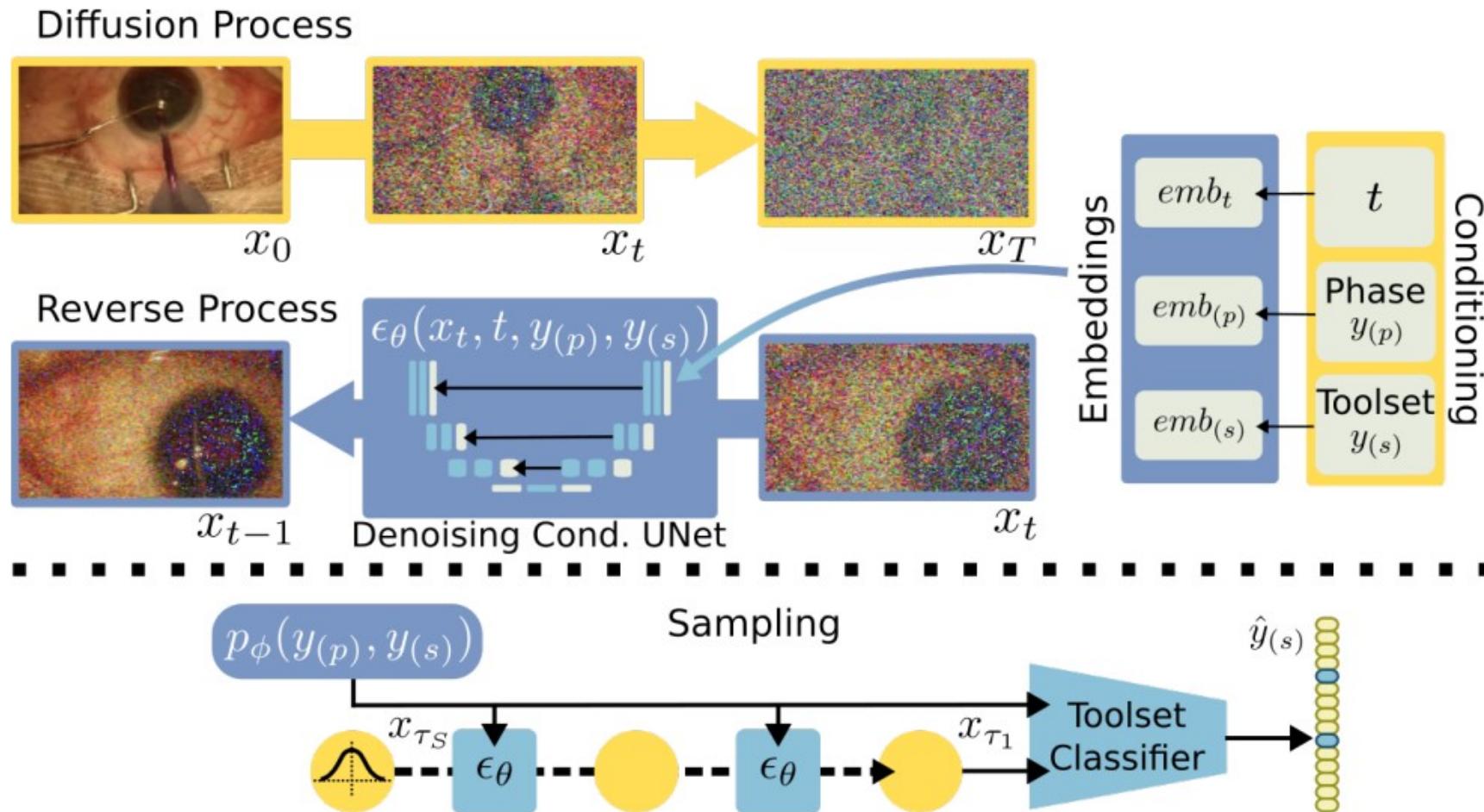
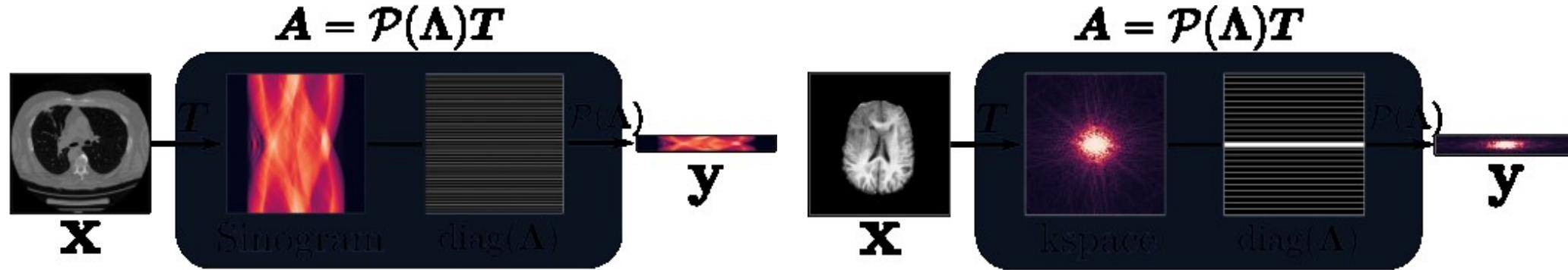


Image reconstruction

Examples from the community

Setup



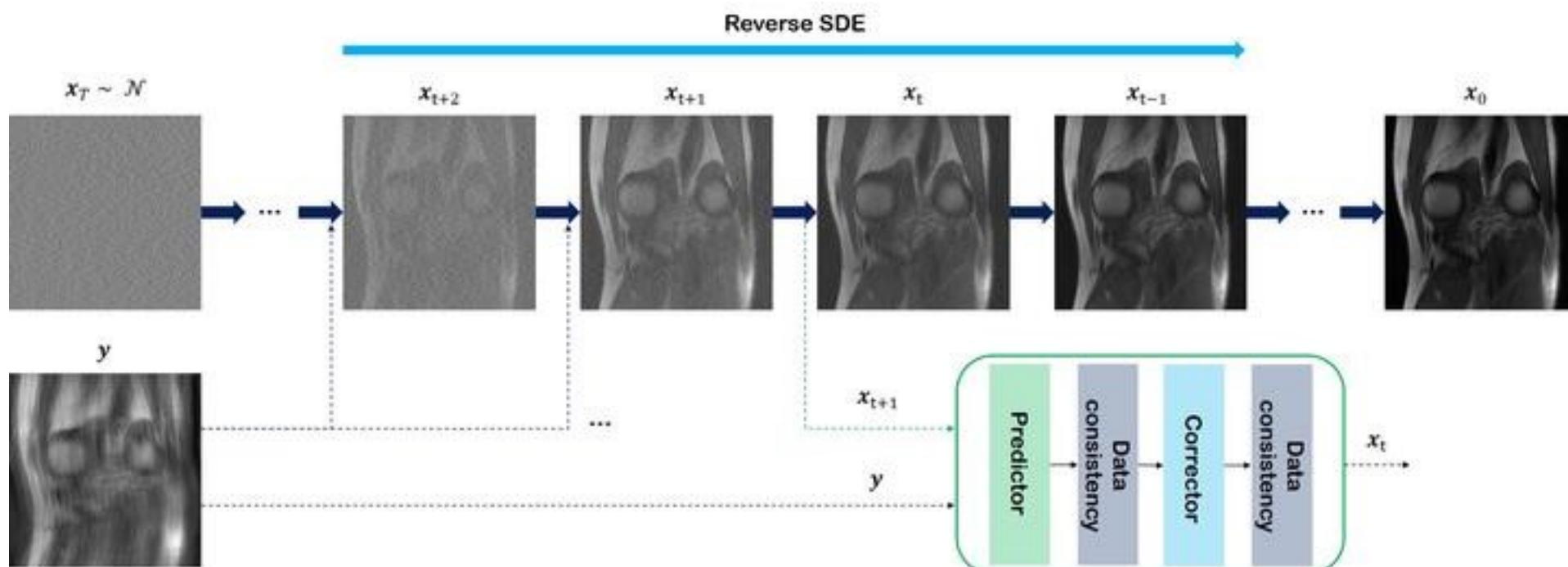
PAPERS

- Song et al (2022) Solving Inverse Problems in Medical Imaging with Score-Based Generative Models. ICLR
Chung et al. (2022) Come-Closer-Diffuse-Faster: Accelerating Conditional Diffusion Models for Inverse Problems through Stochastic Contraction. CVPR
Luo et al. (2022) MRI Reconstruction via Data-Driven Markov Chains with Joint Uncertainty Estimation arxiv:2202.01479
Xie et al. (2022) Measurement-Conditioned Denoising Diffusion Probabilistic Model for Under-Sampled Medical Image Reconstruction. MICCAI
Peng et al. (2022) Towards Performant and Reliable Undersampled MR Reconstruction via Diffusion Model Sampling. MICCAI
Gungor et al. (2022) Adaptive Diffusion Priors for Accelerated MRI Reconstruction. arxiv:2207.05876
Cui et al. (2022) Self-Score: Self-Supervised Learning on Score-Based Models for MRI Reconstruction. Arxiv:2209.00835
Cao et al. (2022) High-Frequency Space Diffusion Models for Accelerated MRI. arxiv:2208.05481
Chung et al.(2022) Improving Diffusion Models for Inverse Problems using Manifold Constraints. arxiv:2206.00941
Chung et al. (2022) MR Image Denoising and Super-Resolution Using Regularized Reverse Diffusion. arxiv:2203.12621
Chung et al. (2021) Score-based diffusion models for accelerated MRI. MIA 2021
Hu et al. (2022) Unsupervised Denoising of Retinal OCT with Diffusion Probabilistic Model. arxiv:2201.11760
Gong et al (2022) PET image denoising based on denoising diffusion probabilistic models. arxiv:2209.06167

Figure by Song et al ICLR 2022.
Copyright rests with the authors.

Reconstruction with Data Consistency

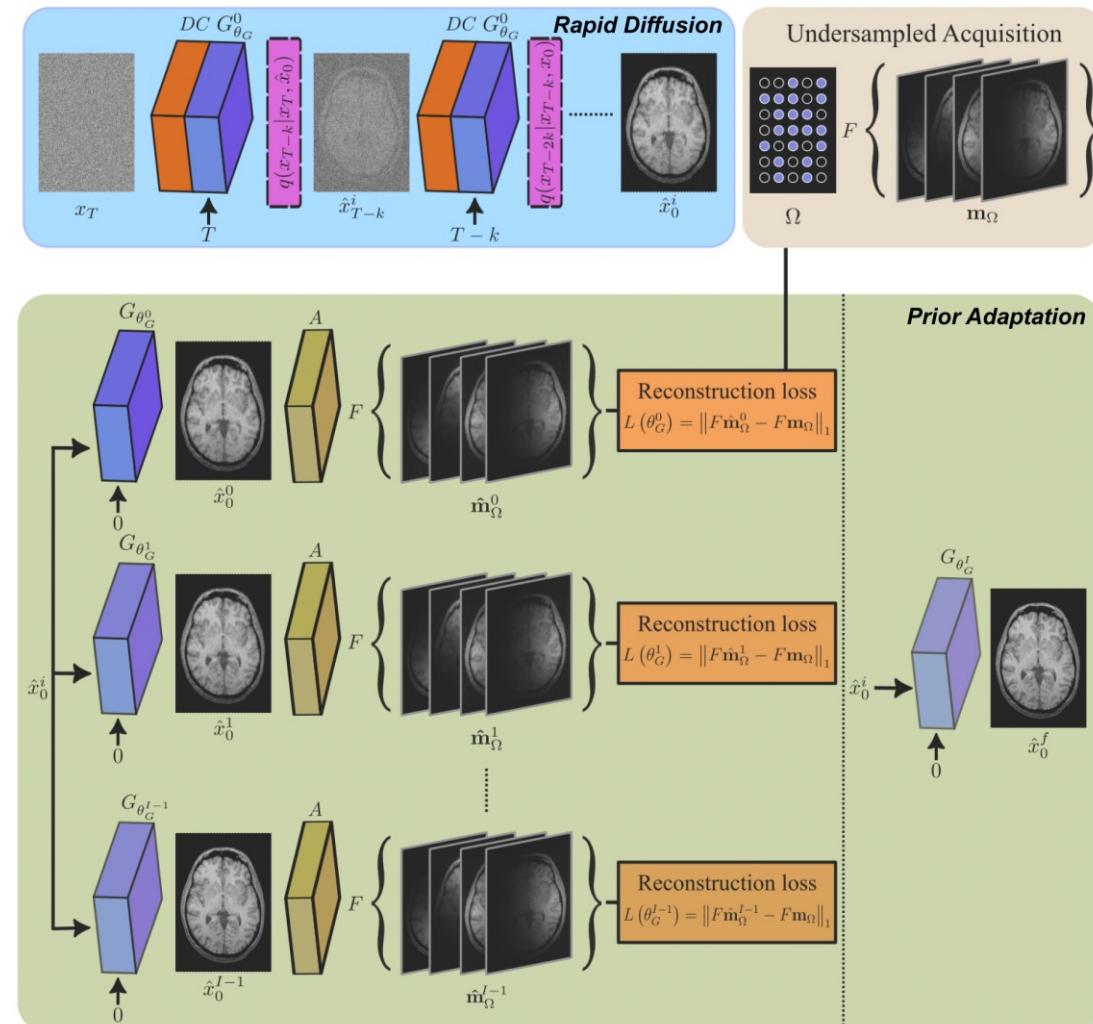
An unconditional diffusion prior is trained on fully-sampled MR acquisitions



Add a **data consistency** term at each sampling step:

$$x_i \leftarrow x_i + \lambda A^*(y - Ax_i)$$

MRI Reconstruction with Adaptive Diffusion Priors



Slides courtesy of Tolga Cukur

General Inverse Problems

$$\mathbf{y} = \mathcal{A}(\mathbf{x}_0) + \mathbf{n}, \quad \mathbf{y}, \mathbf{n} \in \mathbb{R}^n, \mathbf{x} \in \mathbb{R}^d$$

Algorithm 1 DPS - Gaussian

Require: $N, \mathbf{y}, \{\zeta_i\}_{i=1}^N, \{\tilde{\sigma}_i\}_{i=1}^N$

```

1:  $\mathbf{x}_N \sim \mathcal{N}(\mathbf{0}, \mathbf{I})$ 
2: for  $i = N - 1$  to 0 do
3:    $\hat{\mathbf{s}} \leftarrow \mathbf{s}_\theta(\mathbf{x}_i, i)$ 
4:    $\hat{\mathbf{x}}_0 \leftarrow \frac{1}{\sqrt{\bar{\alpha}_i}}(\mathbf{x}_i + (1 - \bar{\alpha}_i)\hat{\mathbf{s}})$ 
5:    $\mathbf{z} \sim \mathcal{N}(\mathbf{0}, \mathbf{I})$ 
6:    $\mathbf{x}'_{i-1} \leftarrow \frac{\sqrt{\alpha_i}(1 - \bar{\alpha}_{i-1})}{1 - \bar{\alpha}_i}\mathbf{x}_i + \frac{\sqrt{\bar{\alpha}_{i-1}}\beta_i}{1 - \bar{\alpha}_i}\hat{\mathbf{x}}_0 + \tilde{\sigma}_i \mathbf{z}$ 
7:    $\mathbf{x}_{i-1} \leftarrow \mathbf{x}'_{i-1} - \zeta_i \nabla_{\mathbf{x}_i} \|\mathbf{y} - \mathcal{A}(\hat{\mathbf{x}}_0)\|_2^2$ 
8: end for
9: return  $\hat{\mathbf{x}}_0$ 

```

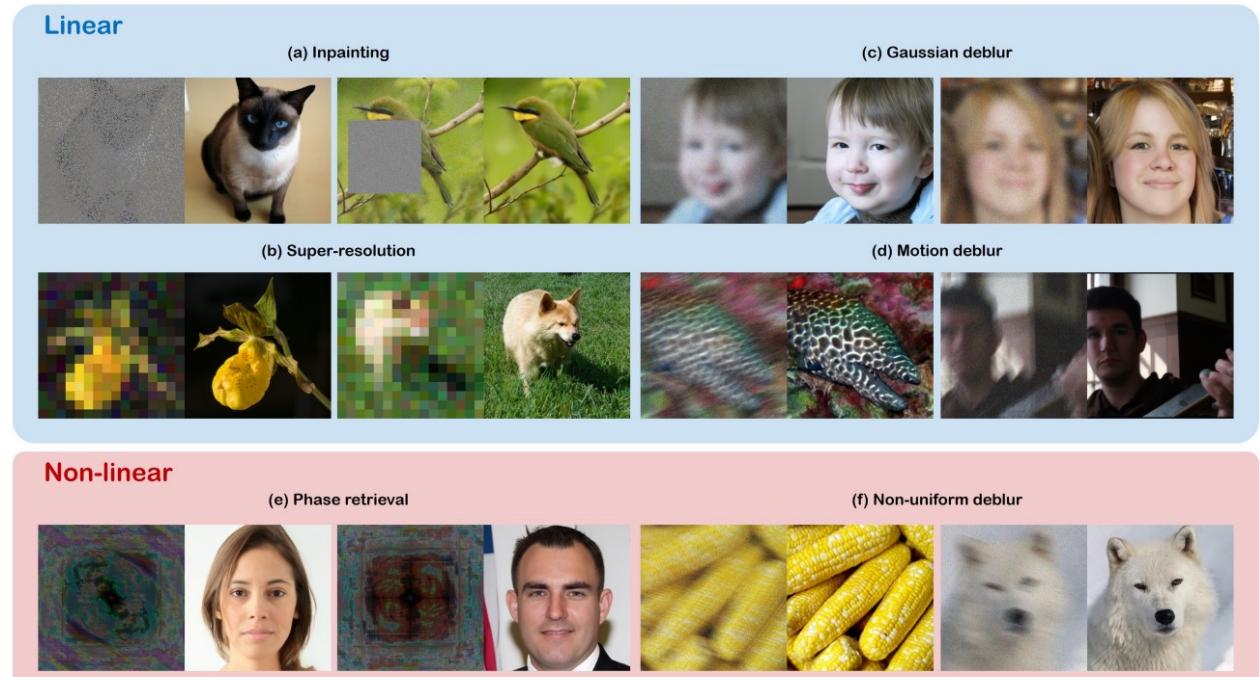


Image registration

Examples from the community

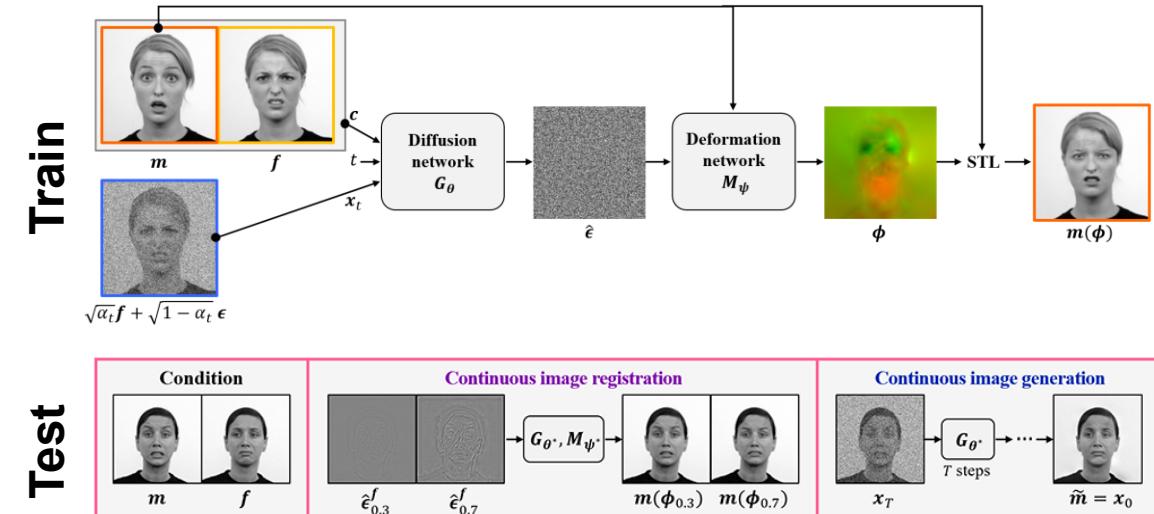
DiffuseMorph

- To perform image registration along the continuous trajectory
- **Diffusion network:** To estimate a conditional score function
- **Deformation network:** To yield the registration fields & provide the deformed image

Loss function

$$\min_{G_\theta, M_\psi} L_{diffusion}(c, x_t, t) + \lambda L_{regist}(m, f)$$

$L_{diffusion}(c, x_t, t) = \mathbb{E}_{\epsilon, x_t, t} \|G_\theta(c, x_t, t) - \epsilon\|_2^2$
 $L_{regist}(m, f) = -(m(\phi) \otimes f) + \lambda_\phi \sum \|\nabla \phi\|^2$



Algorithm 1 Continuous image registration

```

1: Input: Conditional images,  $c = (m, f)$ 
2: Output: Deformed moving image,  $m(\phi_\eta)$ 
3: Set the latent feature  $\hat{\epsilon}^f = G_{\theta^*}(c, f, 0)$ 
4: for  $\eta \in [0, 1]$  do
5:    $\hat{\epsilon}_\eta^f \leftarrow \eta \cdot \hat{\epsilon}^f$ 
6:    $\phi_\eta \leftarrow M_{\psi^*}(m, \hat{\epsilon}_\eta^f)$ 
7: end for=
8: return  $m(\phi_\eta)$ 

```

Algorithm 2 Synthetic image generation process

```

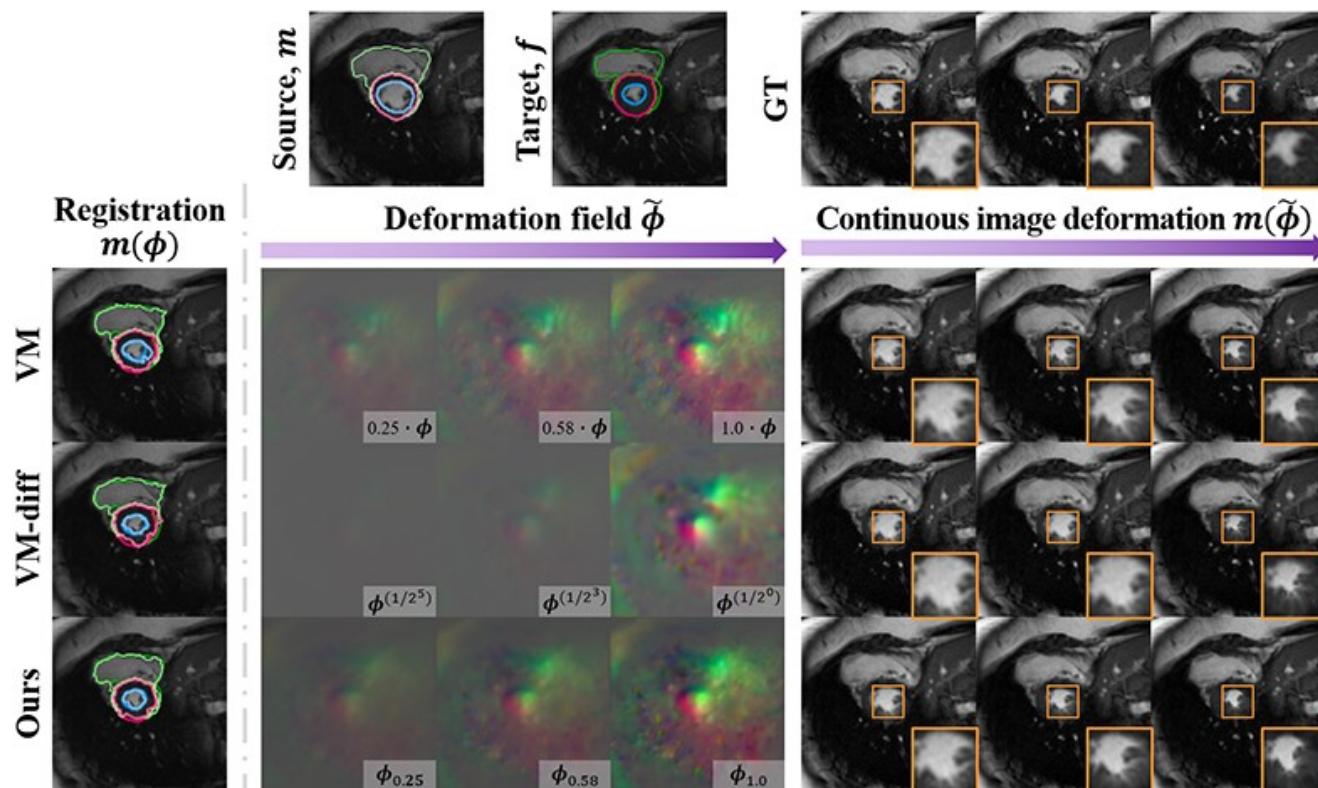
1: Input: Conditional images,  $c = (m, f)$ 
2: Output: Synthetic deformed image,  $x$ 
3: Set  $T \in (0, T_{train})$ 
4: Sample  $x_T = \sqrt{\alpha_T}m + \sqrt{1 - \alpha_T}\epsilon$ , where  $\epsilon \sim \mathcal{N}(0, I)$ 
5: for  $t = T, T - 1, \dots, 1$  do
6:    $z \sim \mathcal{N}(0, I)$ 
7:    $x_{t-1} \leftarrow \frac{1}{\sqrt{1 - \beta_t}}(x_t - \frac{\beta_t}{\sqrt{1 - \alpha_t}}G_{\theta^*}(c, x_t, t)) + \sigma_t z$ 
8: end for
9: return  $x_0$ 

```

Slides courtesy of Boah Kim & Jong Chul Ye

DiffuseMorph

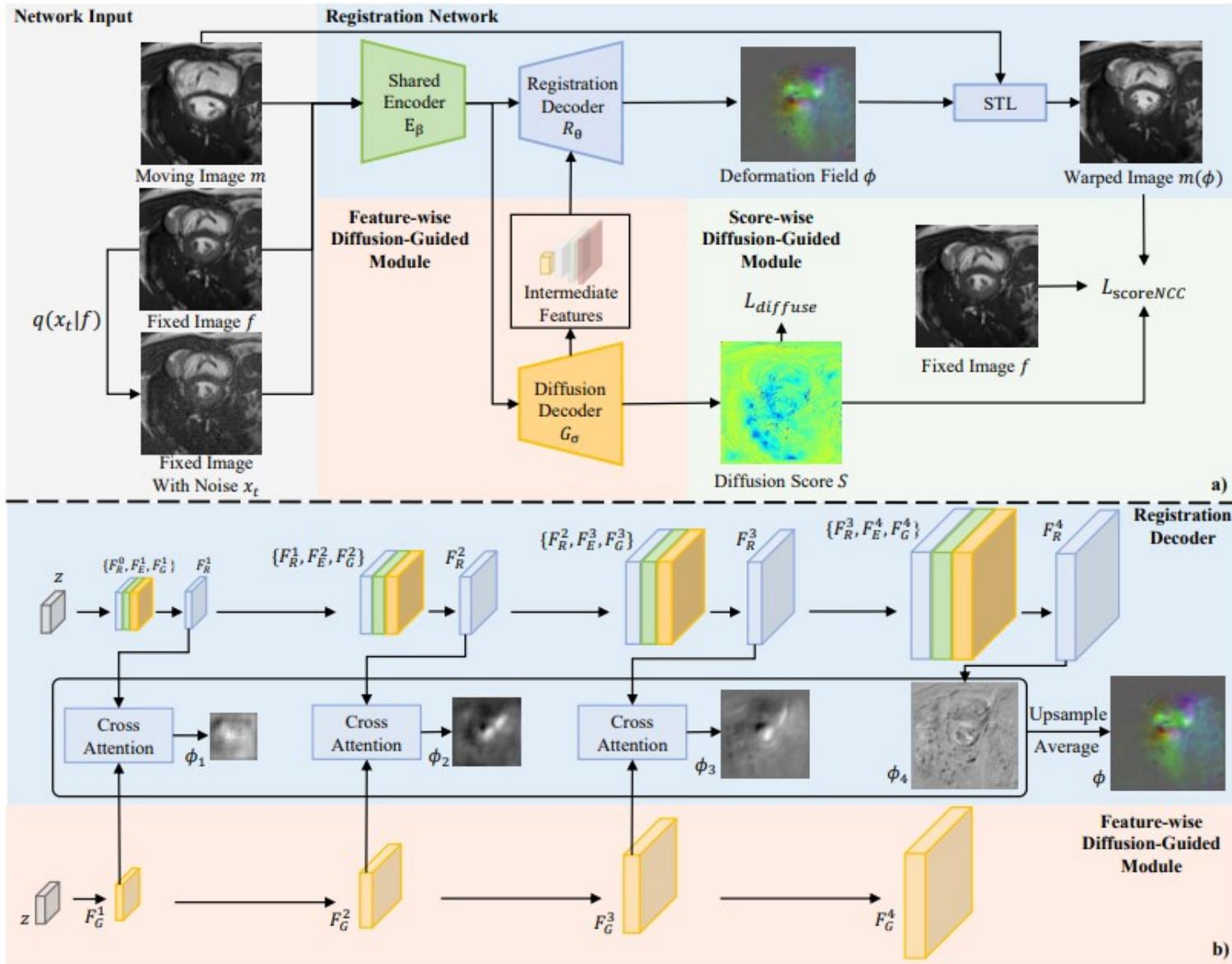
- Intra-subject 3D cardiac MR image registration



Methods	Dice	$ J_\phi \leq 0 (\%)$
Initial	0.642 (0.188)	-
VM [1]	0.787 (0.113)	0.169 (0.109)
VM-diff [2]	0.794 (0.104)	0.291 (0.188)
Ours	0.802 (0.109)	0.161 (0.082)

Slides courtesy of Boah Kim & Jong Chul Ye

Feature-wise Diffusion-Guided

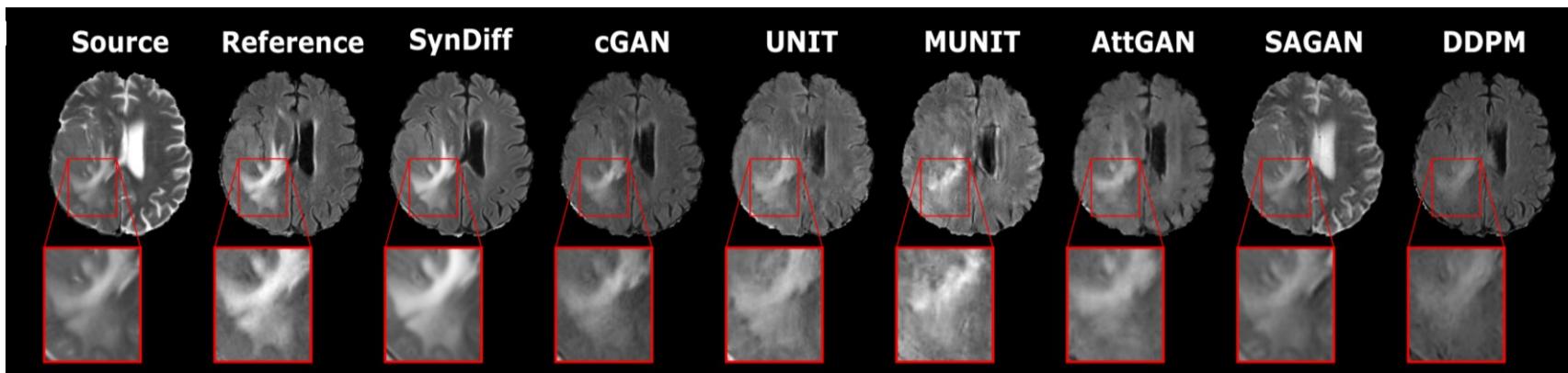


Qin et al. (2023) FSDiffReg: Feature-wise and Score-wise Diffusion-guided Unsupervised Deformable Image Registration for Cardiac Images.
Miccai 2023

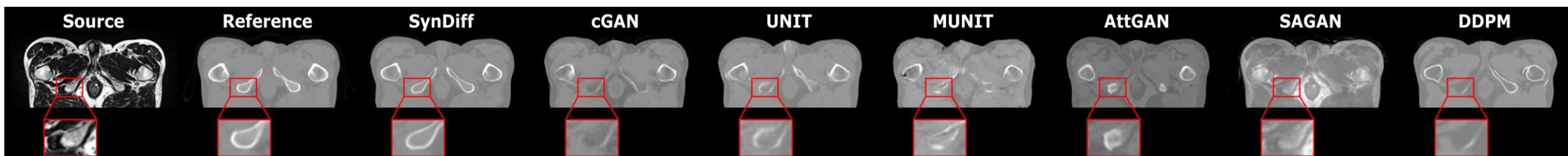
Image-to-Image translation

Setup

MRI Contrast Translation



MRI to CT Translation

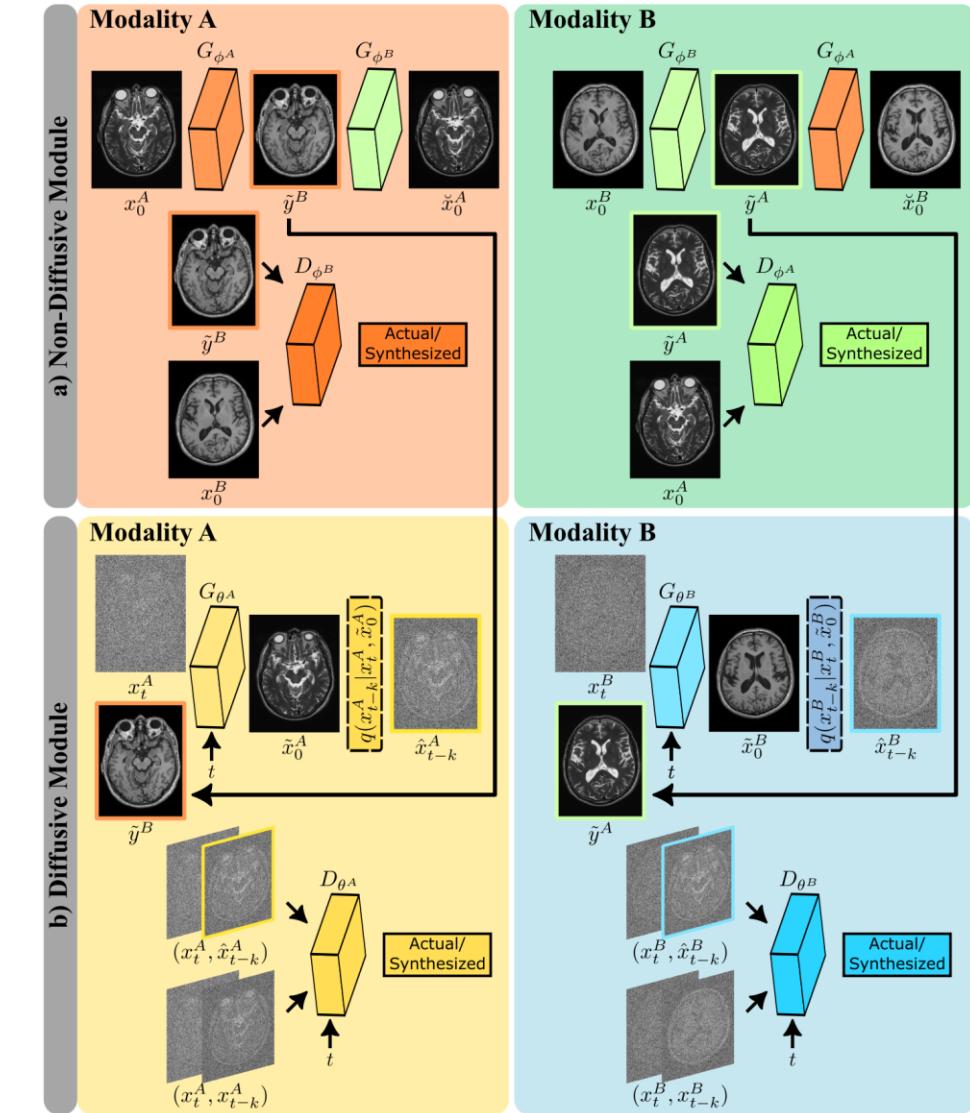


Slides courtesy of Tolga Cukur

Medical Image Translation with Adversarial Diffusion

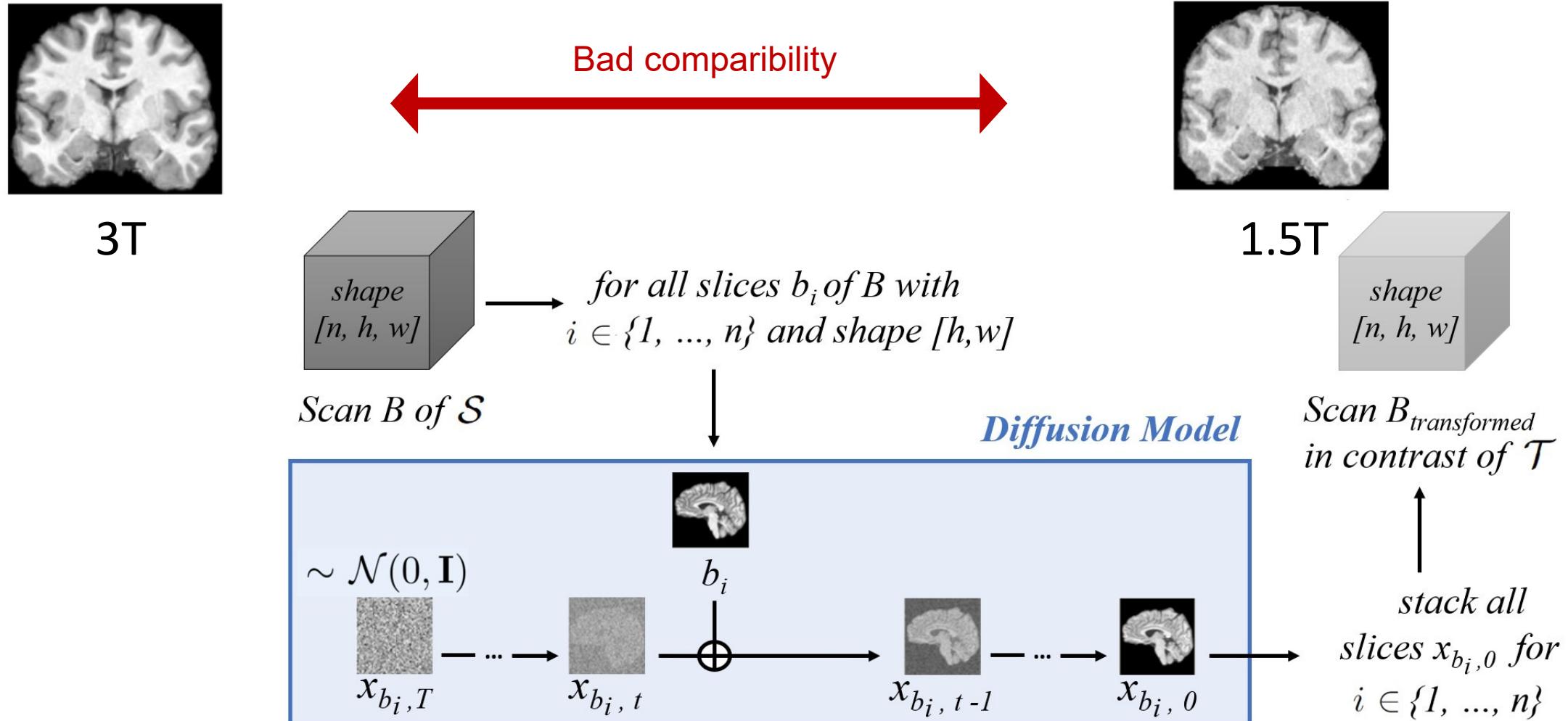
SynDiff: an unsupervised diffusion model
for medical image translation

- An adversarial diffusive module maps fast source → target
- A non-diffusive module with cycle-consistency loss enables training on unpaired datasets



Slides courtesy of Tolga Cukur

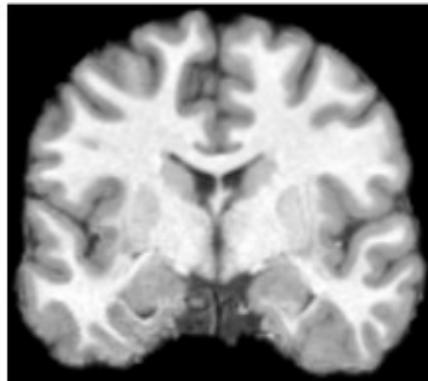
Diffusion Models for Contrast Harmonization



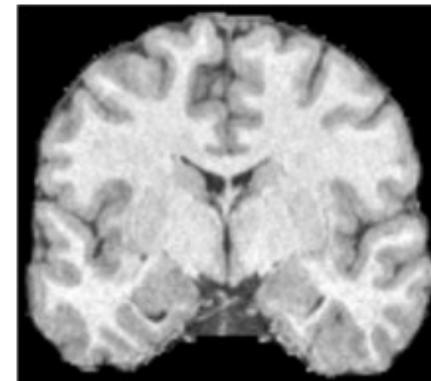
Contrast Harmonization Results

3 T to 1.5 T

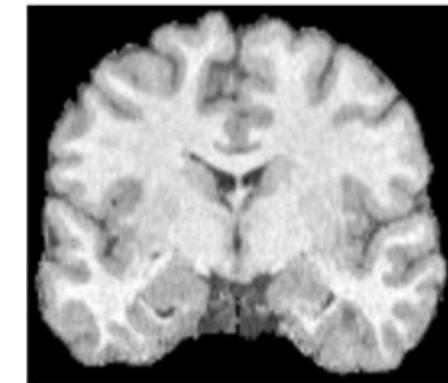
Input



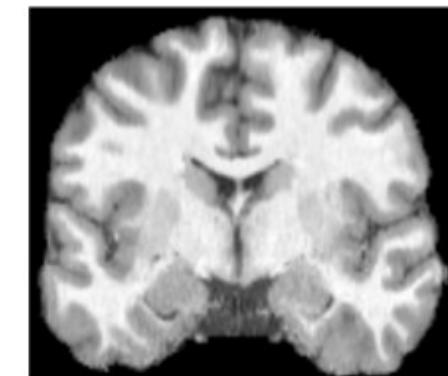
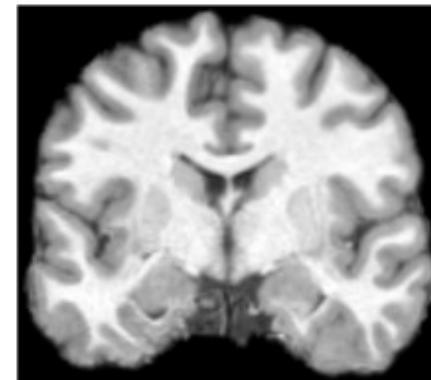
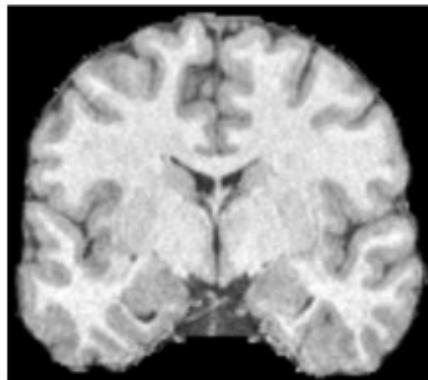
Ground Truth



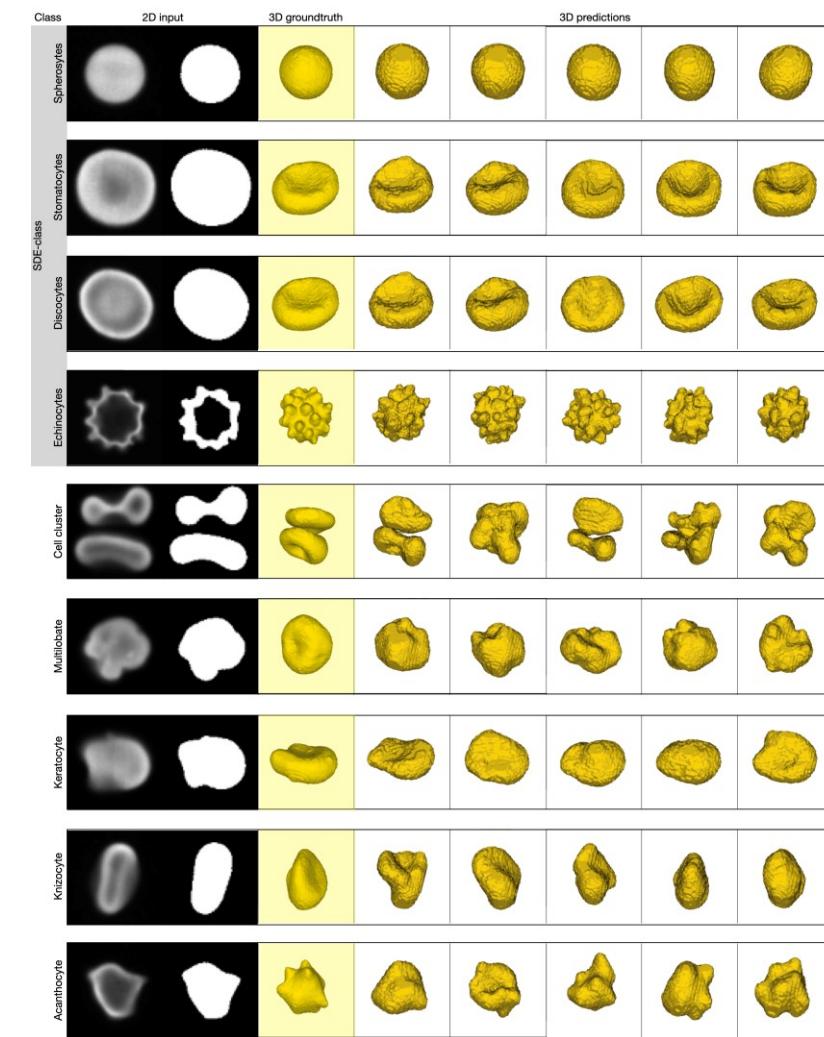
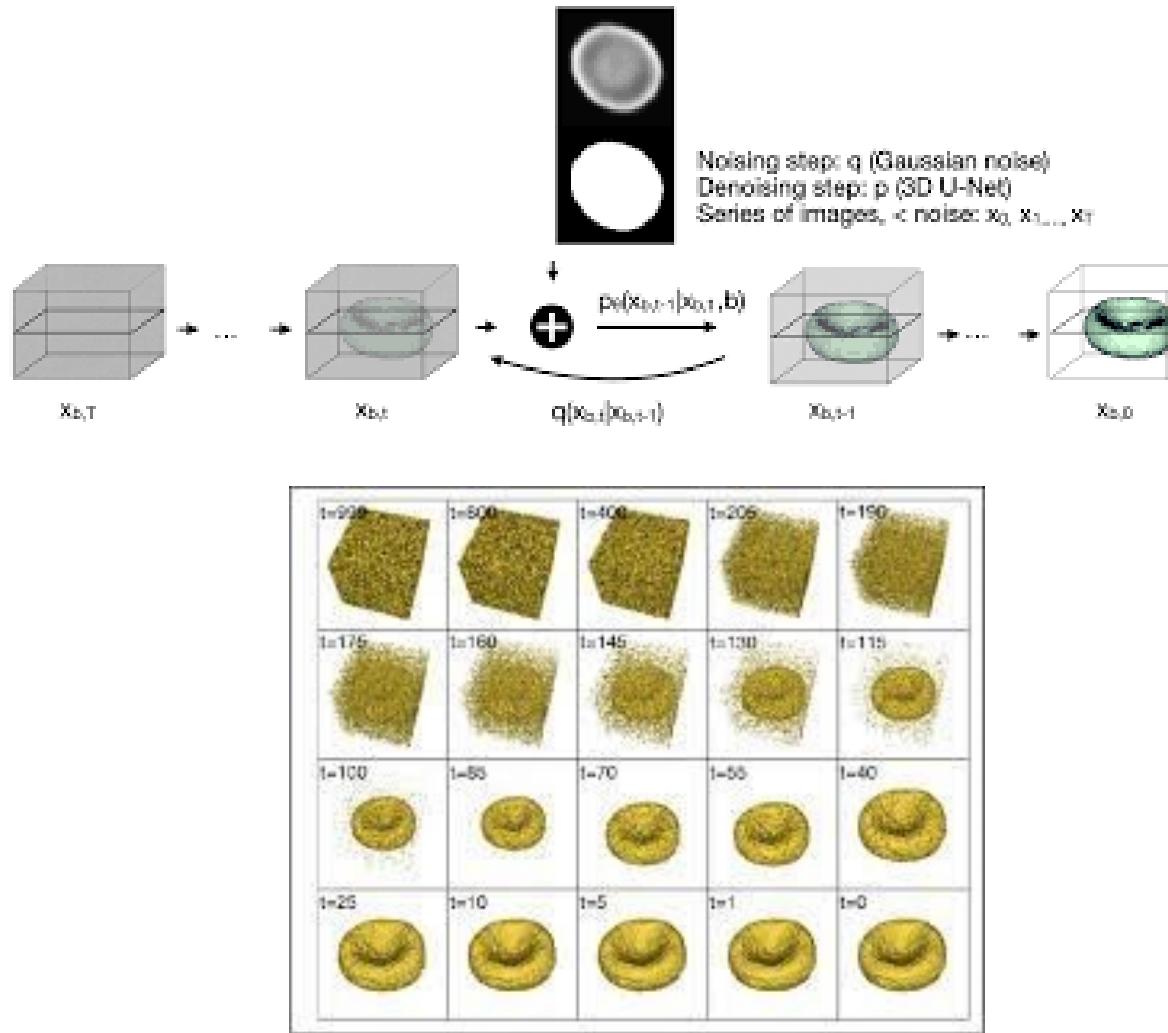
Diffusion Model Output



1.5 T to 3 T

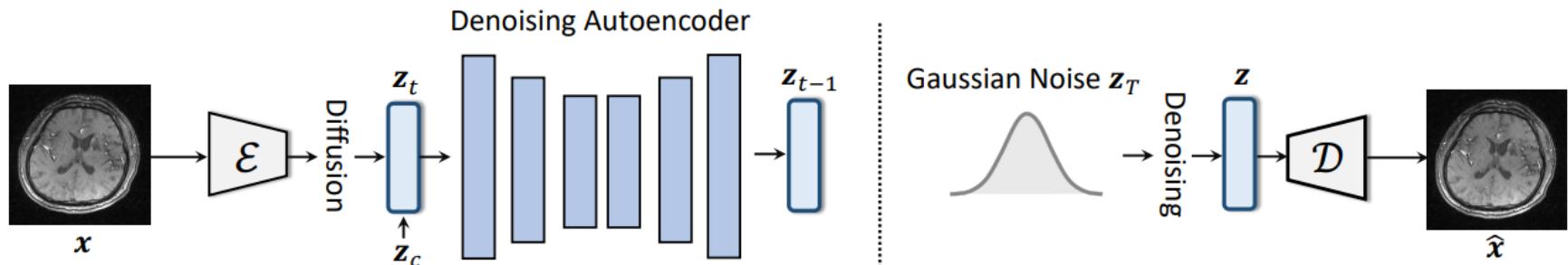


3D Shapes from 2D Microscopy Images

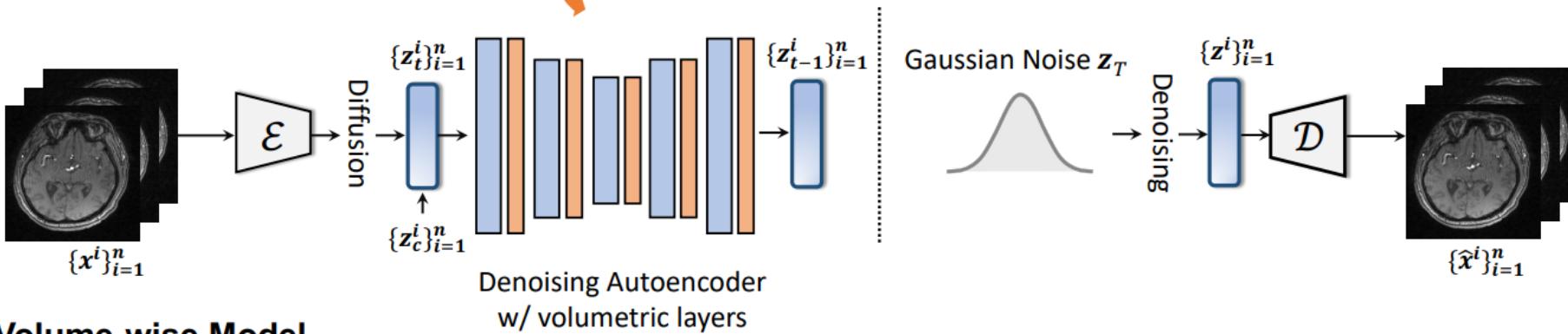


3D with 2D model

Slice-wise Model



Insert & Quick Fine-tuning

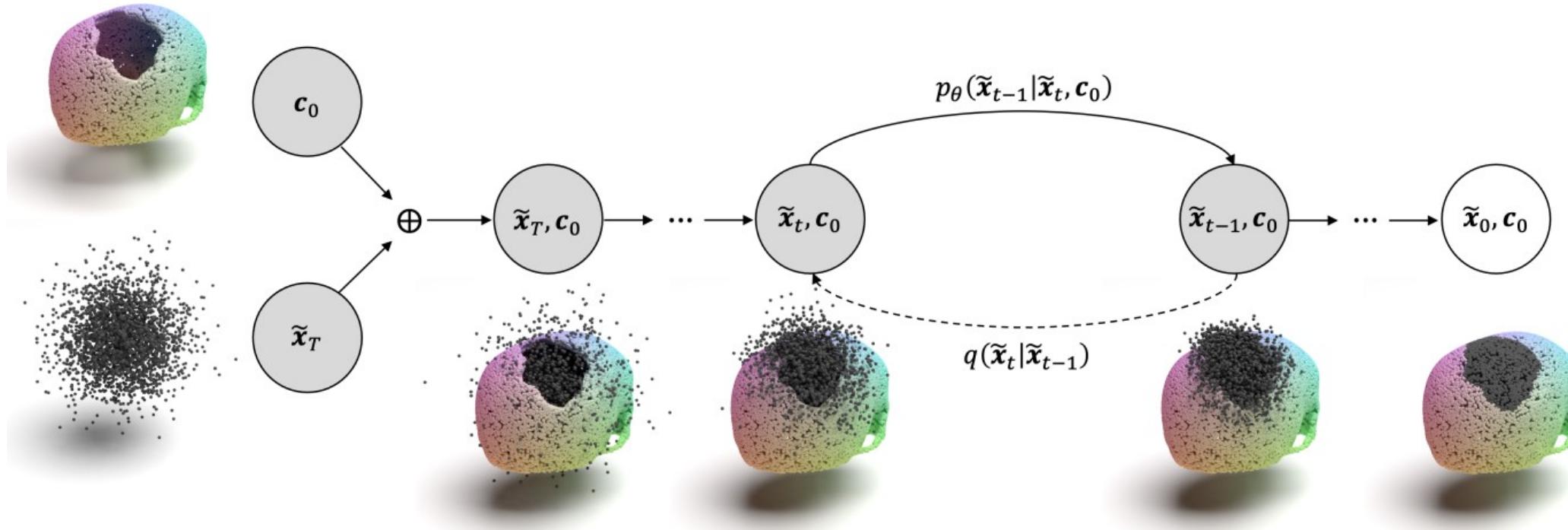


Volume-wise Model

Inpainting

Examples from the community

Point Cloud Diffusion Models for Implant Generation



- For automatic implant generation, we aim to complete a defective skull.
- The diffusion process is applied on a **point cloud representation** due to memory and computation time restrictions.
- We condition the generation process on the skull with a defect.

Point Cloud Completion

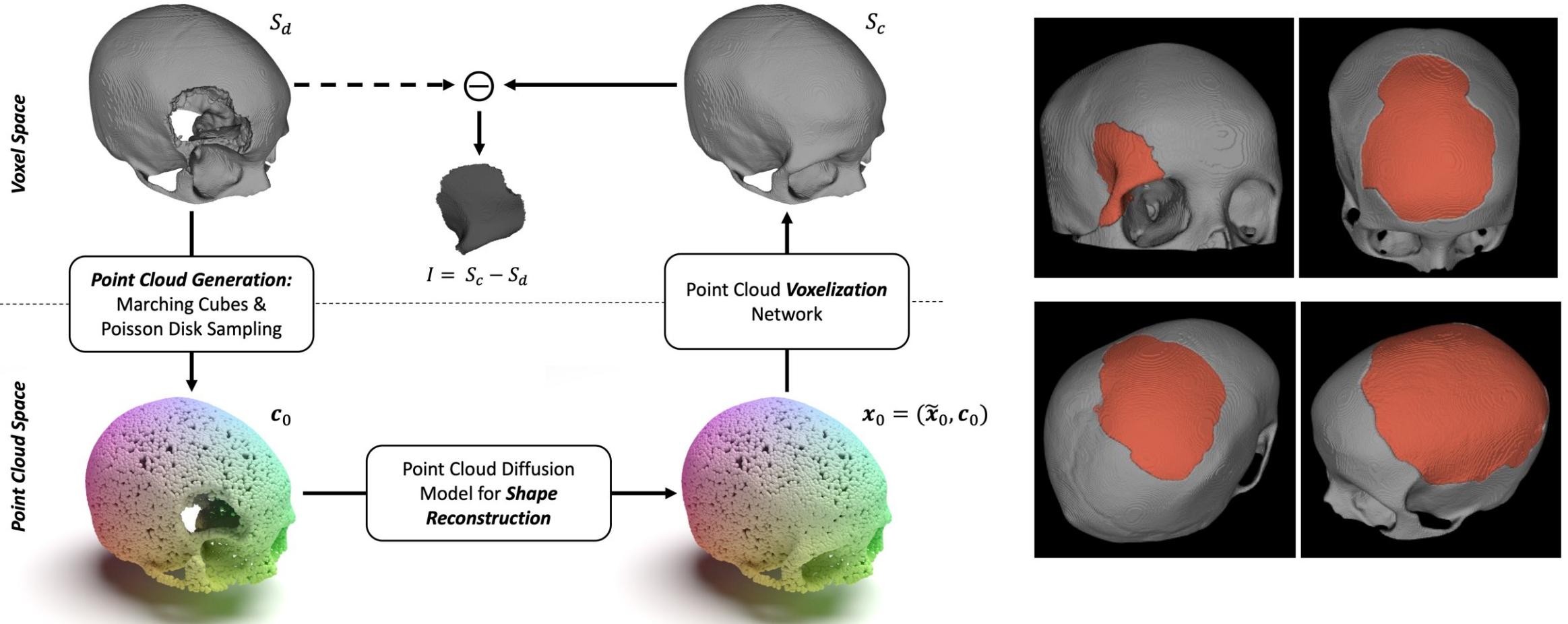
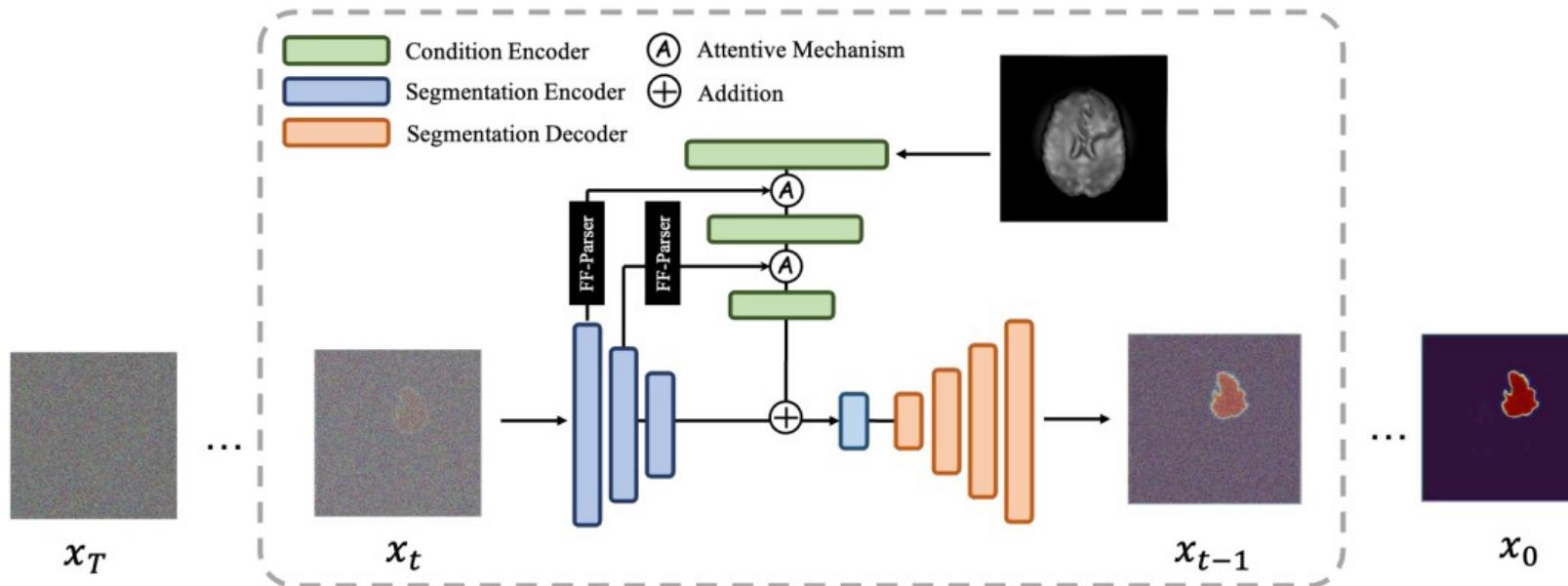


Image segmentation

Examples from the community

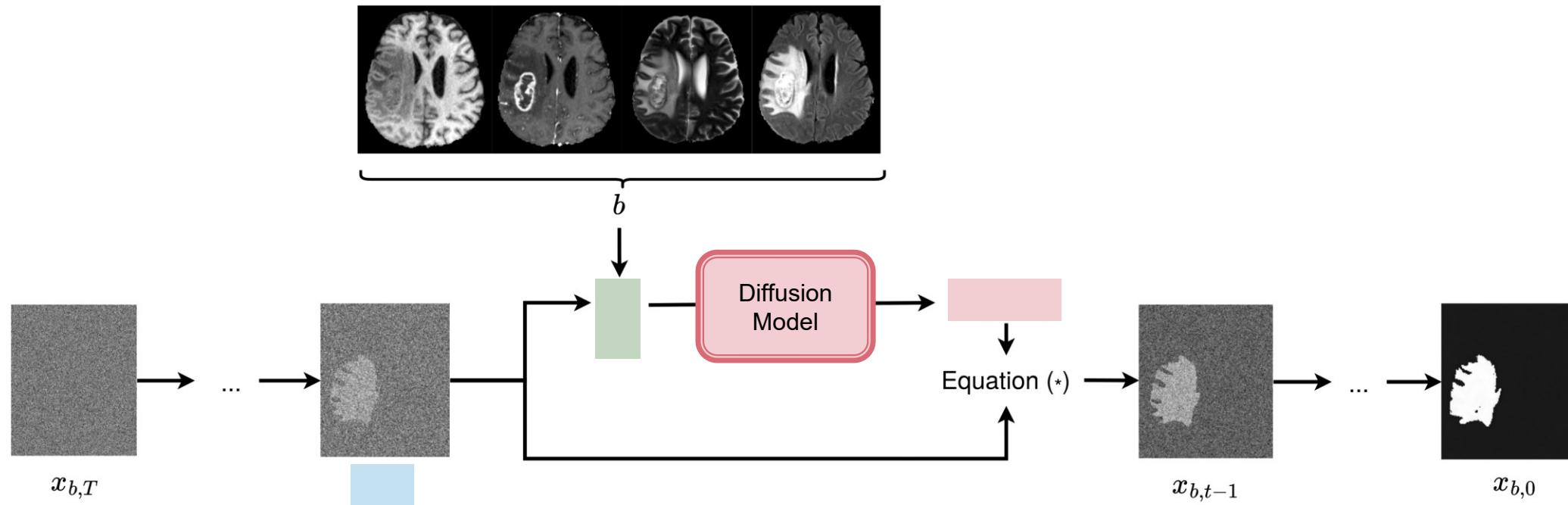
Setup



PAPERS

- Wolleb et al (2022). Diffusion Models for Implicit Image Segmentation Ensembles, *MIDL* 2022. arXiv:2112.03145
Guo et al (2022) Accelerating Diffusion Models via Pre-segmentation Diffusion Sampling for Medical Image Segmentation. arXiv:2210.17408
La Barbera et al. (2022) Anatomically constrained CT image translation for heterogeneous blood vessel segmentation. arXiv:2210.01713
Kim et al. (2022) Diffusion Adversarial Representation Learning for Self-supervised Vessel Segmentation. arXiv:2209.14566
Wu et al (2022) MedSegDiff: Medical Image Segmentation with Diffusion Probabilistic Model. arXiv:2211.00611
Rahman, Aimon, et al. (2023) Ambiguous medical image segmentation using diffusion models. CVPR
Bieder et al. (2023) Memory-Efficient 3D Denoising Diffusion Models for Medical Image Processing. Medical Imaging with Deep Learning
Rousseau et al. (2023) Pre-Training with Diffusion models for Dental Radiography segmentation. Miccai 2023

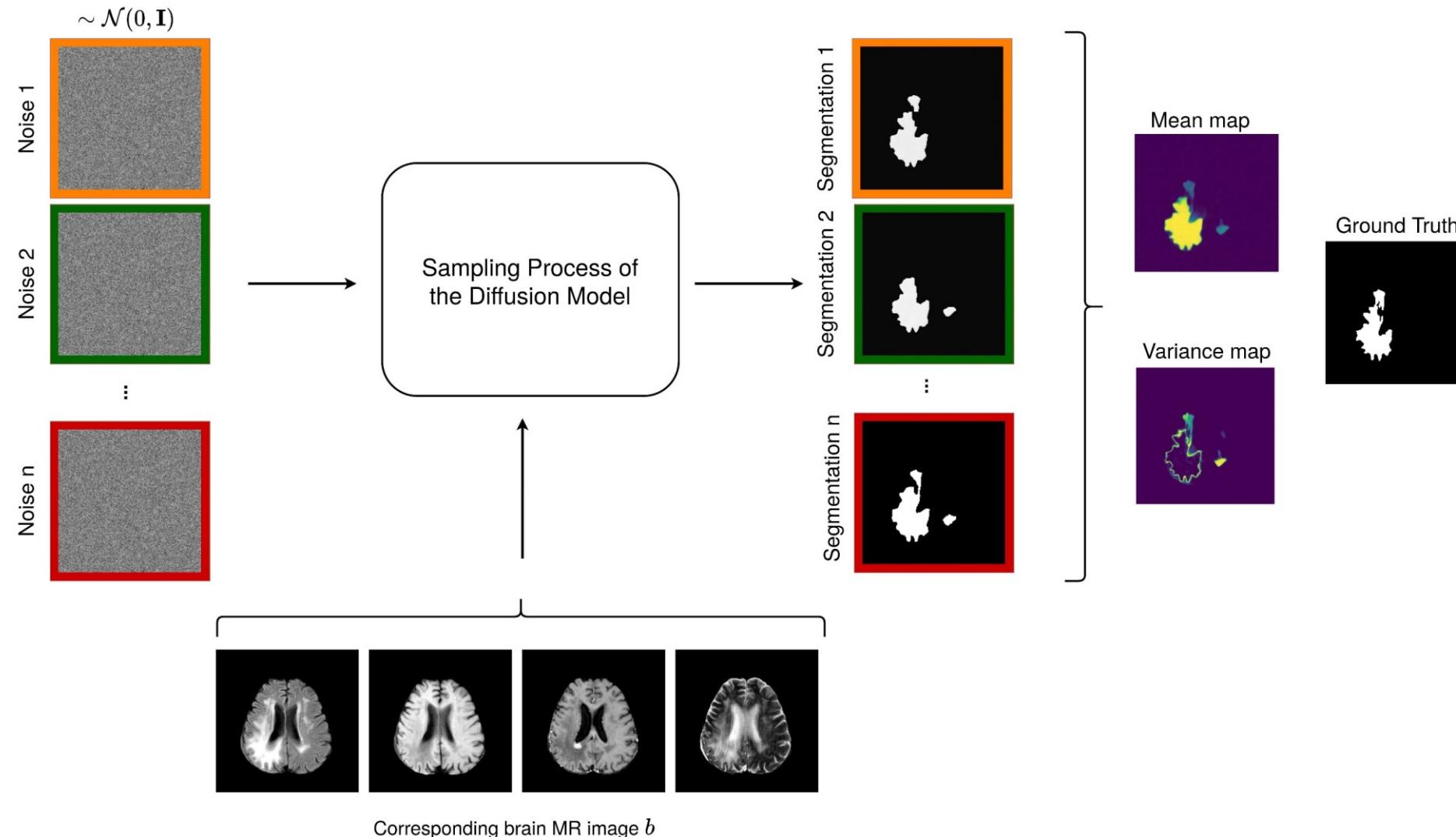
Diffusion Models for Segmentation Mask Generation



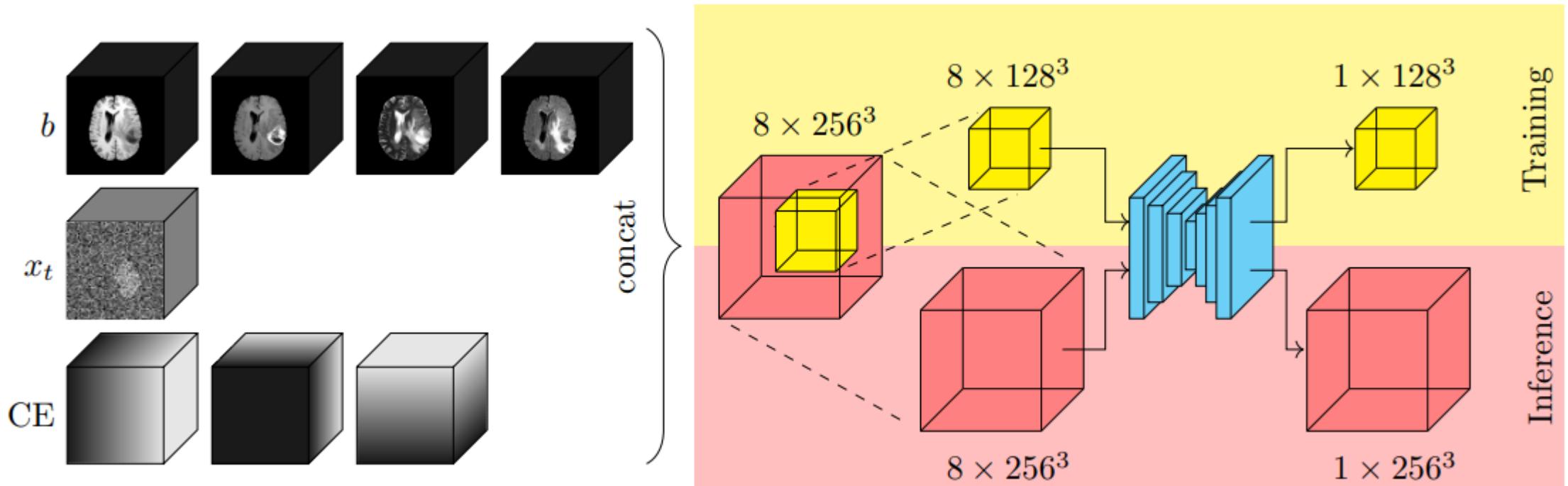
$$(*) \quad x_{b,t-1} = \frac{1}{\sqrt{\alpha_t}} \left(\text{[blue box]} - \frac{1 - \alpha_t}{\sqrt{1 - \alpha_t}} \text{[pink box]} \right) + \sigma_t \mathbf{z}, \quad \text{with } \mathbf{z} \sim \mathcal{N}(0, \mathbf{I})$$

The anatomical information is added by concatenating the input images b to the noisy segmentation mask [blue box] in every step t .

Generation of Segmentation Ensembles



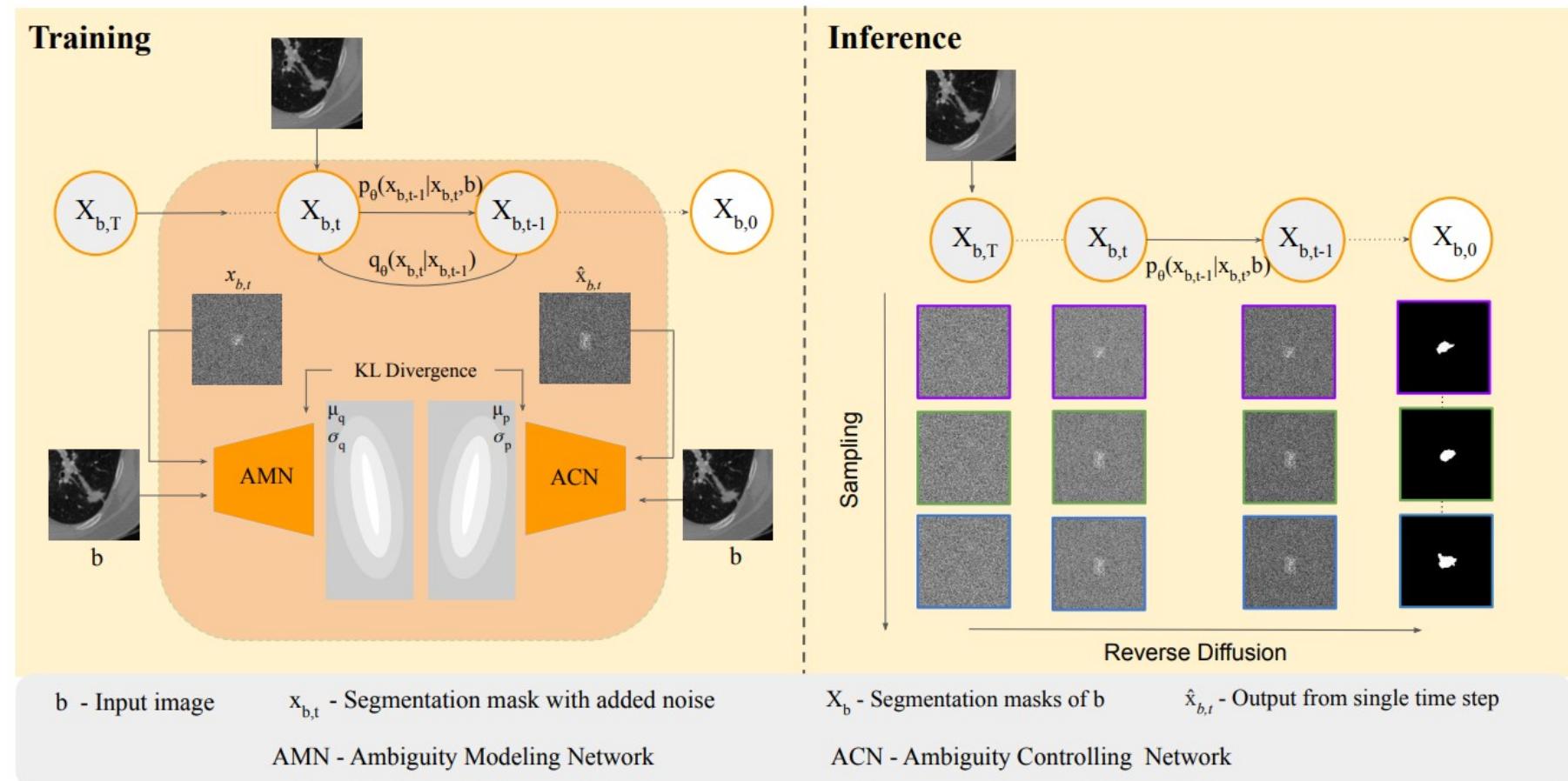
3D Segmentation with PatchDDM



- We add a position encoding in all 3 spatial dimensions.
- Training is on patches only, and saves memory and training time.
- Inference runs over the whole 3D volume.

Ambiguous Segmentation

- Ambiguity Modelling Network (AMN) models the distribution of ground truth masks given an input image.
- Ambiguity Controlling Network (ACN) models the noisy output from the diffusion model conditioning on an input image.



Segmentation with Diffusion Pre-training

Diffusion

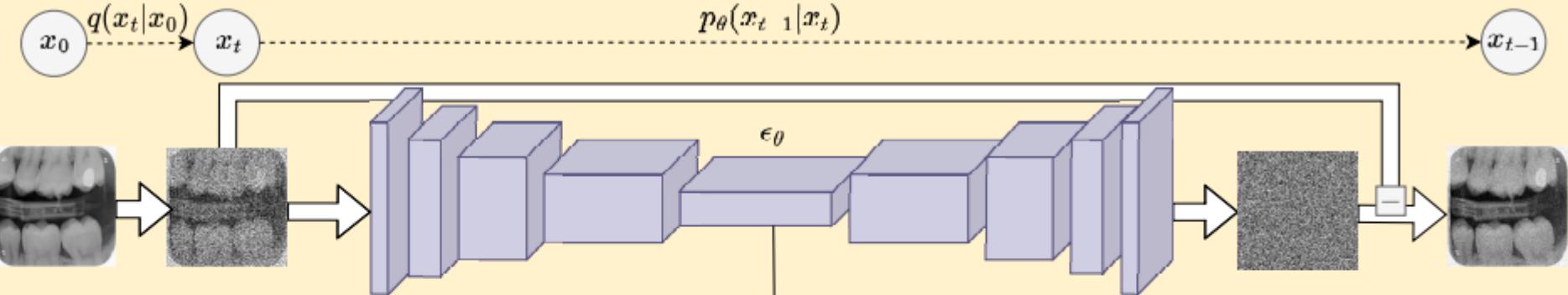
$$x_0 \in X_1$$

$$\epsilon \sim \mathcal{N}_{0,I}$$

$$t \sim \mathcal{U}_{1,T}$$

$$\nabla_{\theta} \|\epsilon_{\theta}(x_t, t) - \epsilon\|^2$$

Pre-training



Few label

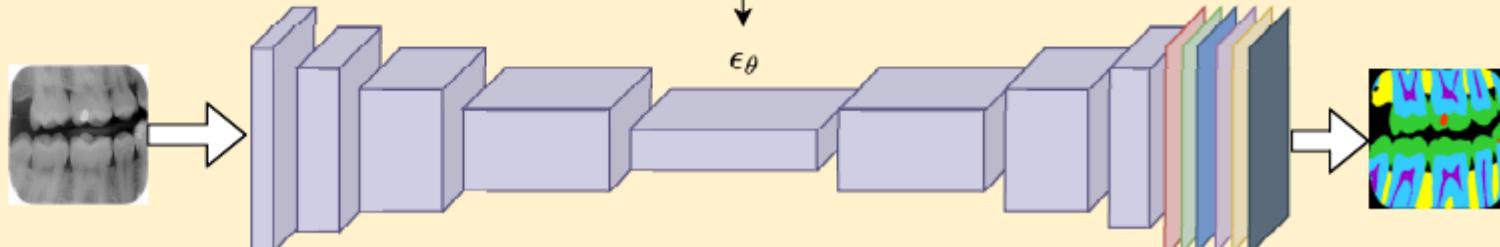
$$X_1 \cap X_2 = \emptyset$$

$$(x, y) \in X_2 \times Y$$

$$\hat{y} = \epsilon_{\theta}(x)$$

$$\nabla_{\theta} Loss(\hat{y}, y)$$

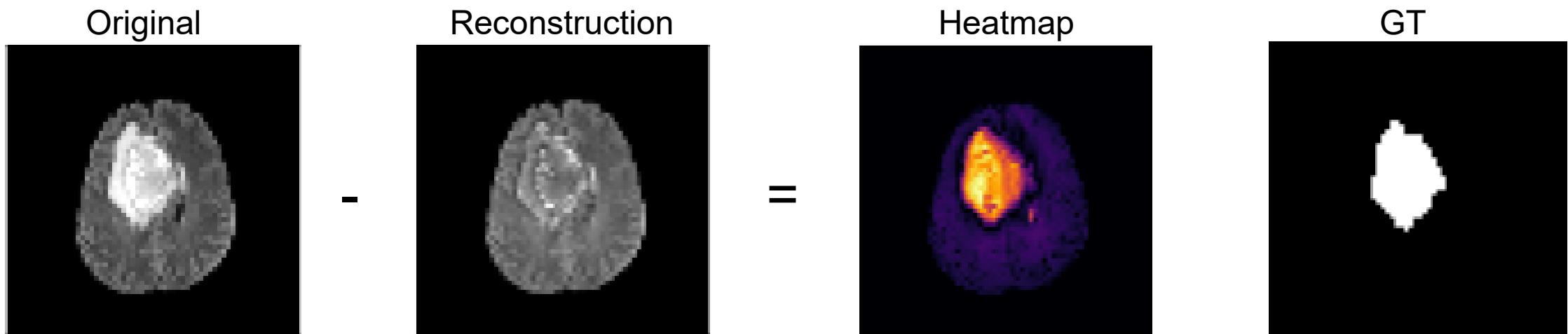
Finetuning



Anomaly detection

Examples from the community

The simple setup of the problem

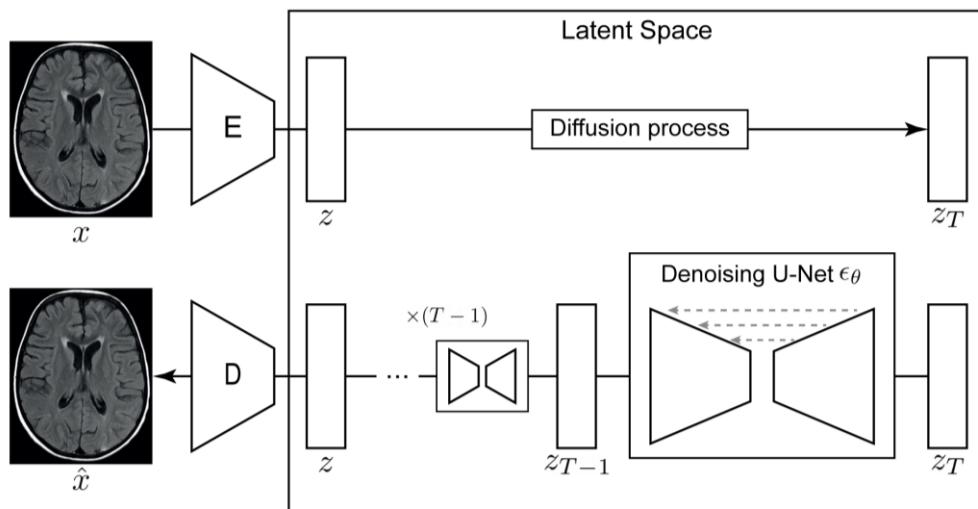


PAPERS

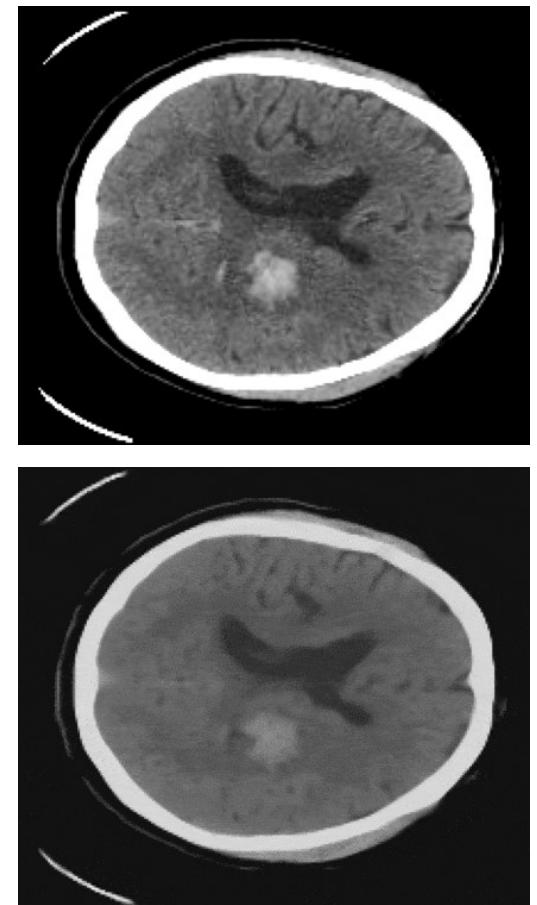
- Sanchez et al. (2022) What is Healthy? Generative Counterfactual Diffusion for Lesion Localization. MICCAI workshop
Pinaya et al (2022) Fast Unsupervised Brain Anomaly Detection and Segmentation with Diffusion Models. MICCAI
Wolleb et al (2022) Diffusion Models for Medical Anomaly Detection. MICCAI
Wyatt et al (2022) AnoDDPM: Anomaly Detection with Denoising Diffusion Probabilistic Models using Simplex Noise. CVPR workshop
Kascenas et al (2023) The role of noise in denoising models for anomaly detection in medical images. Medical Image Analysis
Behrendt, Finn, et al. (2023) "Patched diffusion models for unsupervised anomaly detection in brain mri." Medical Imaging with Deep Learning
Liang, Ziyun, et al. (2023) "Modality Cycles with Masked Conditional Diffusion for Unsupervised Anomaly Segmentation in MRI." arXiv preprint arXiv:2308.16150.

Unsupervised Anomaly Segmentation

- Latent Diffusion Model (LDM) learns the distribution of healthy brain data
- Compression (Vector-Quantised VAE) scales for high-resolution images



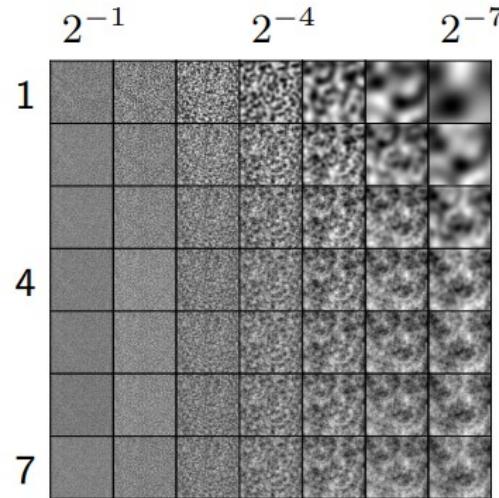
LDM identify regions with a low likelihood of being part of the healthy dataset



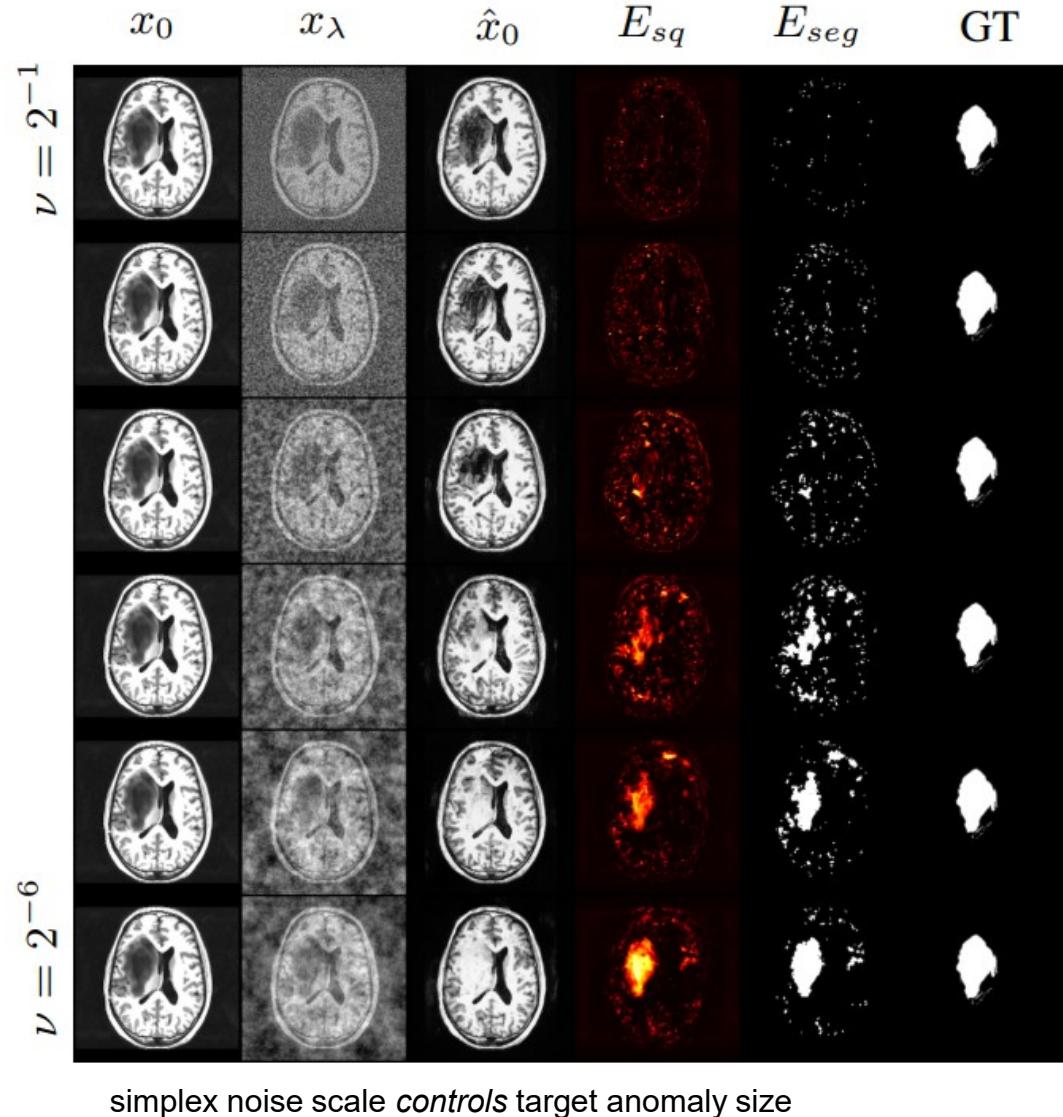
Reverse/denoising process is used to **inpaint** these regions and “heal” the possible anomalies

Anomaly Detection with Simplex Noise

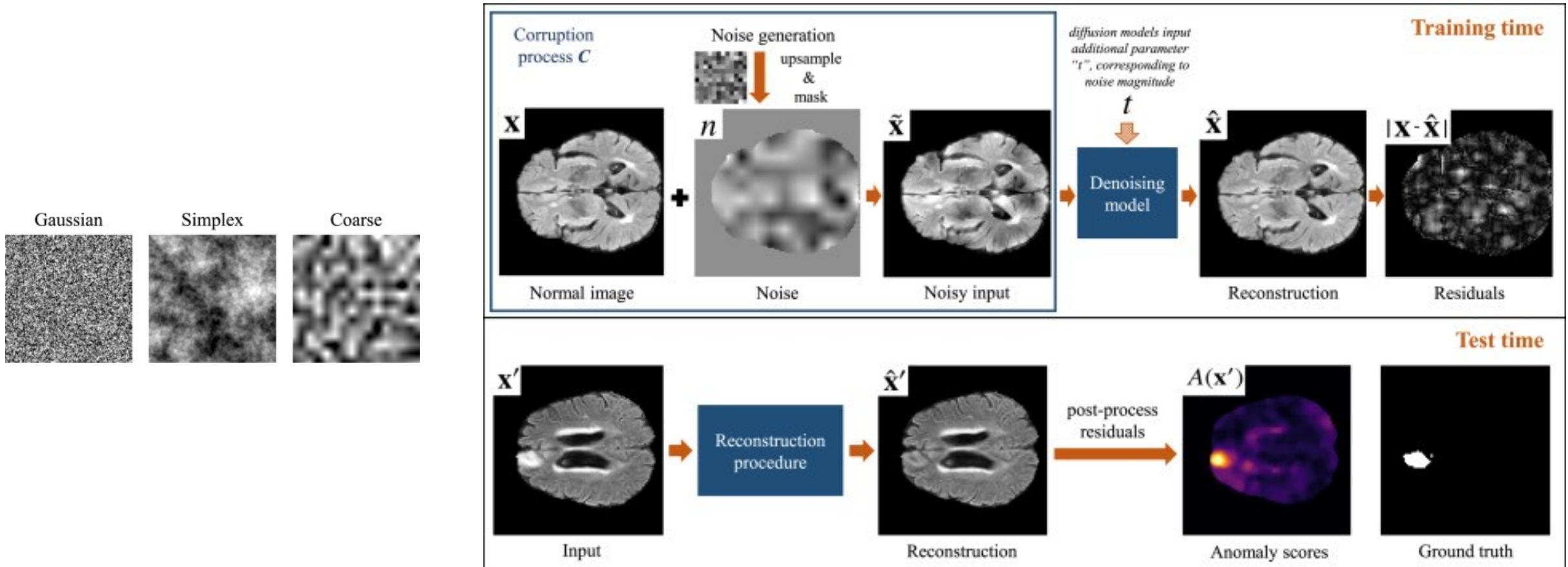
- Typical Gaussian noise is found to be insufficient for anomaly detection.
- Therefore, we explore the use of simplex noise for the corruption and sample generation of medical images.



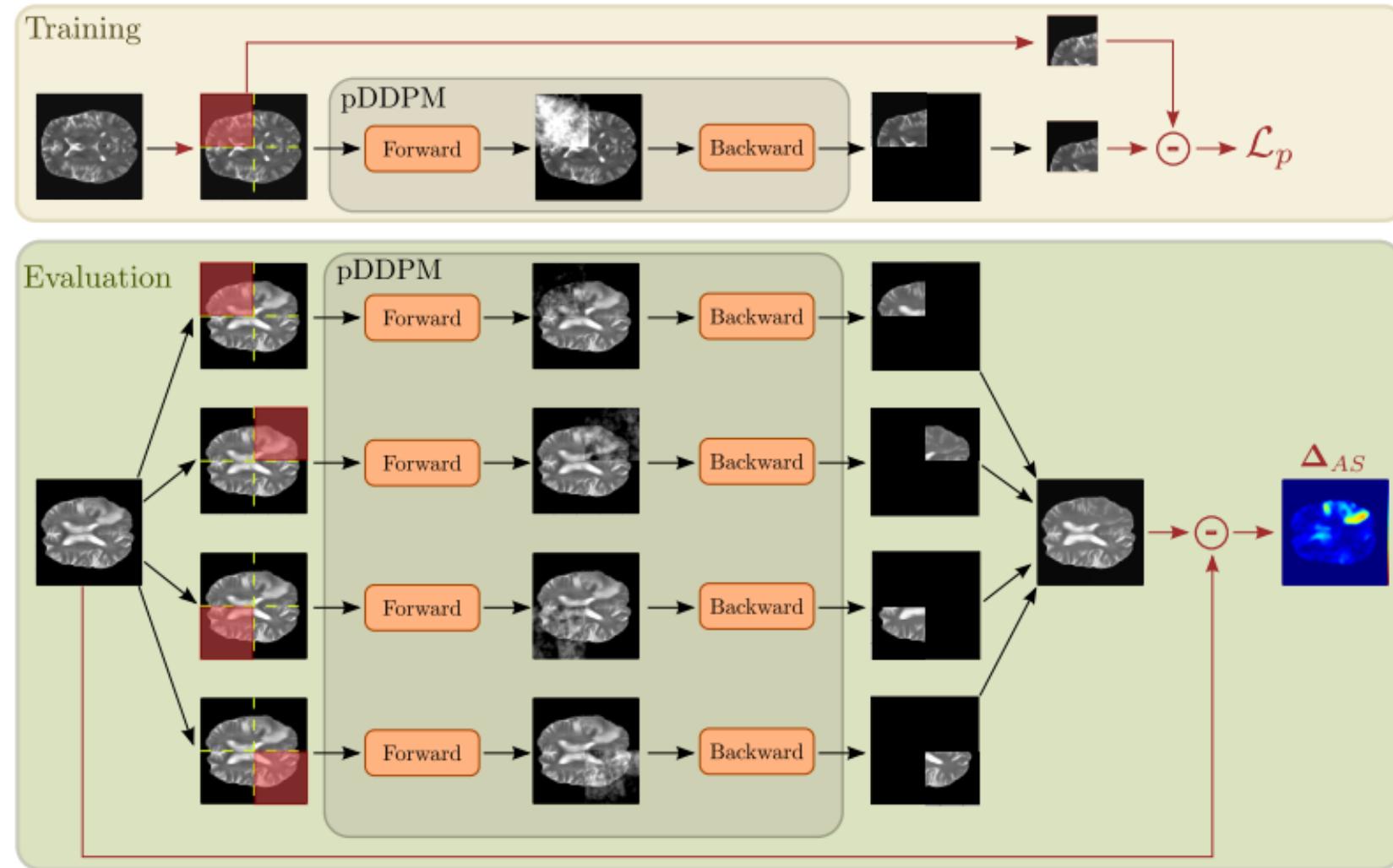
(a) Structures of simplex noise



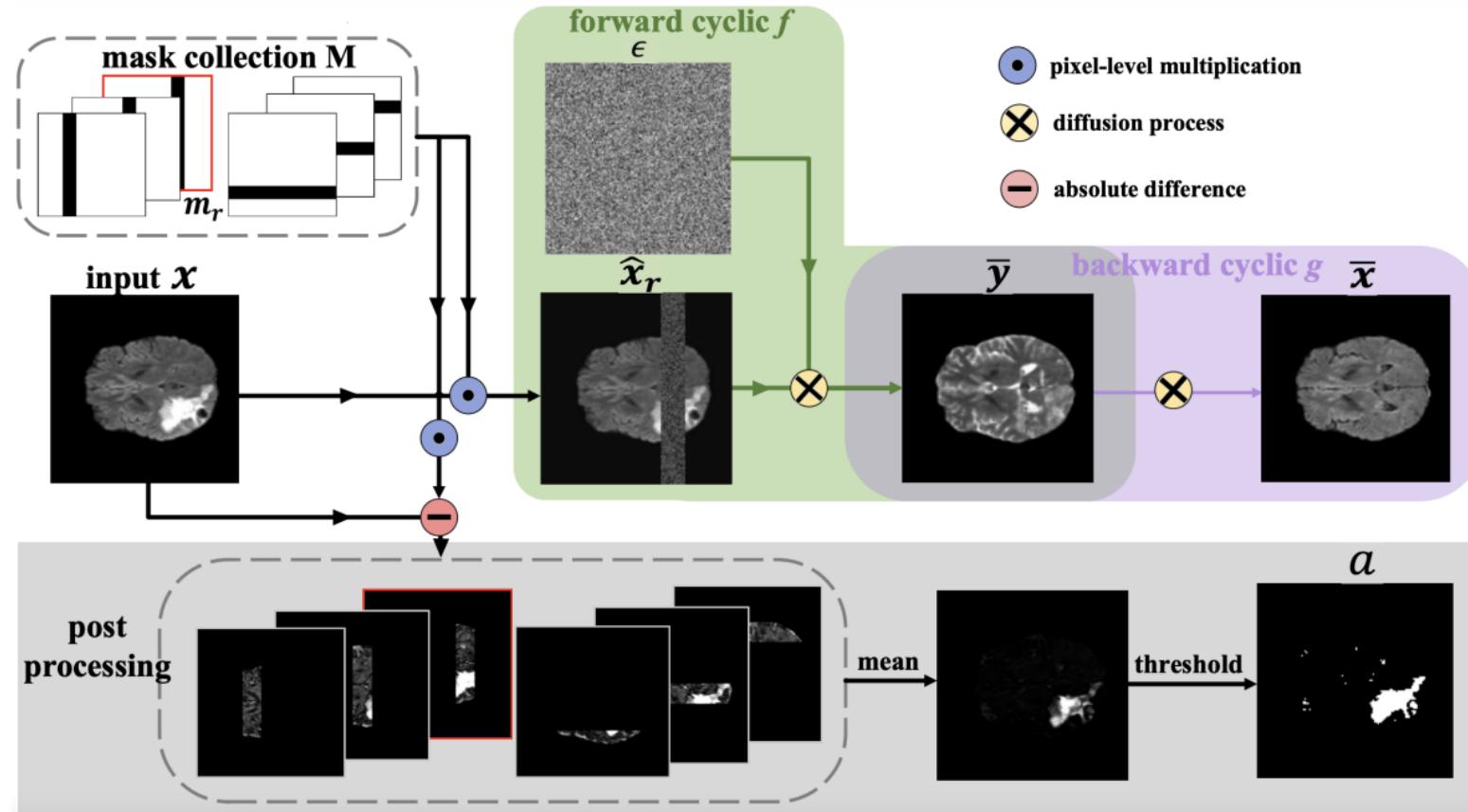
Anomaly Detection with Coarse Noise



Anomaly Detection from Patches

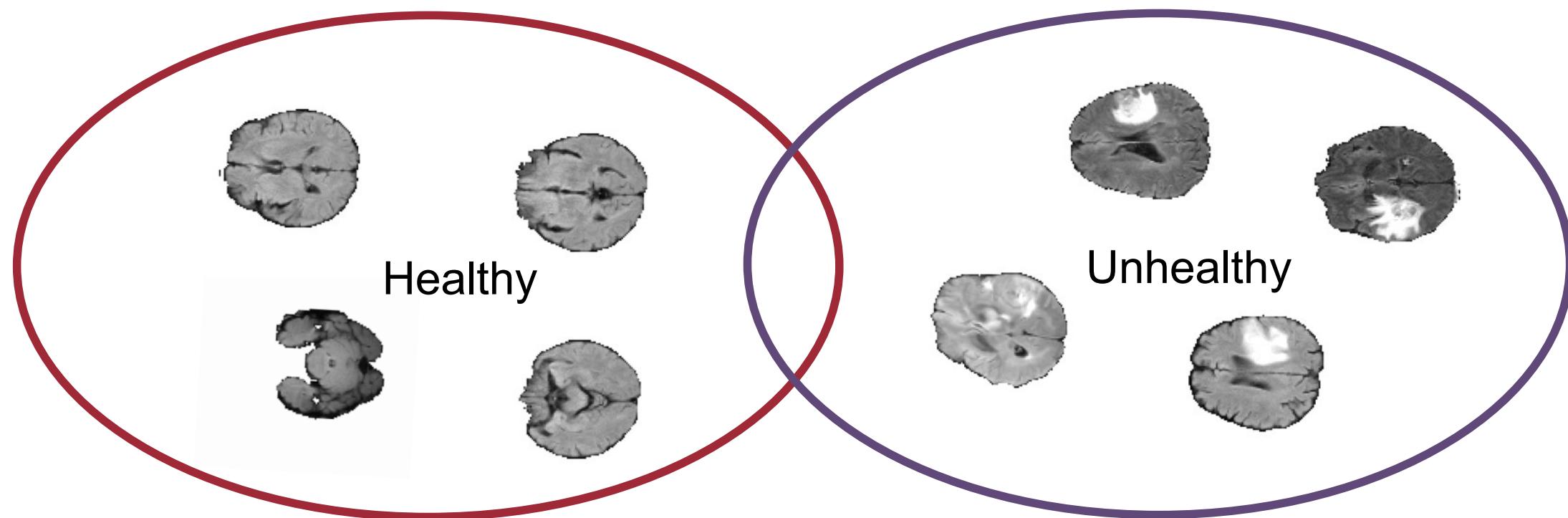


Anomaly Detection from Modality Cycles

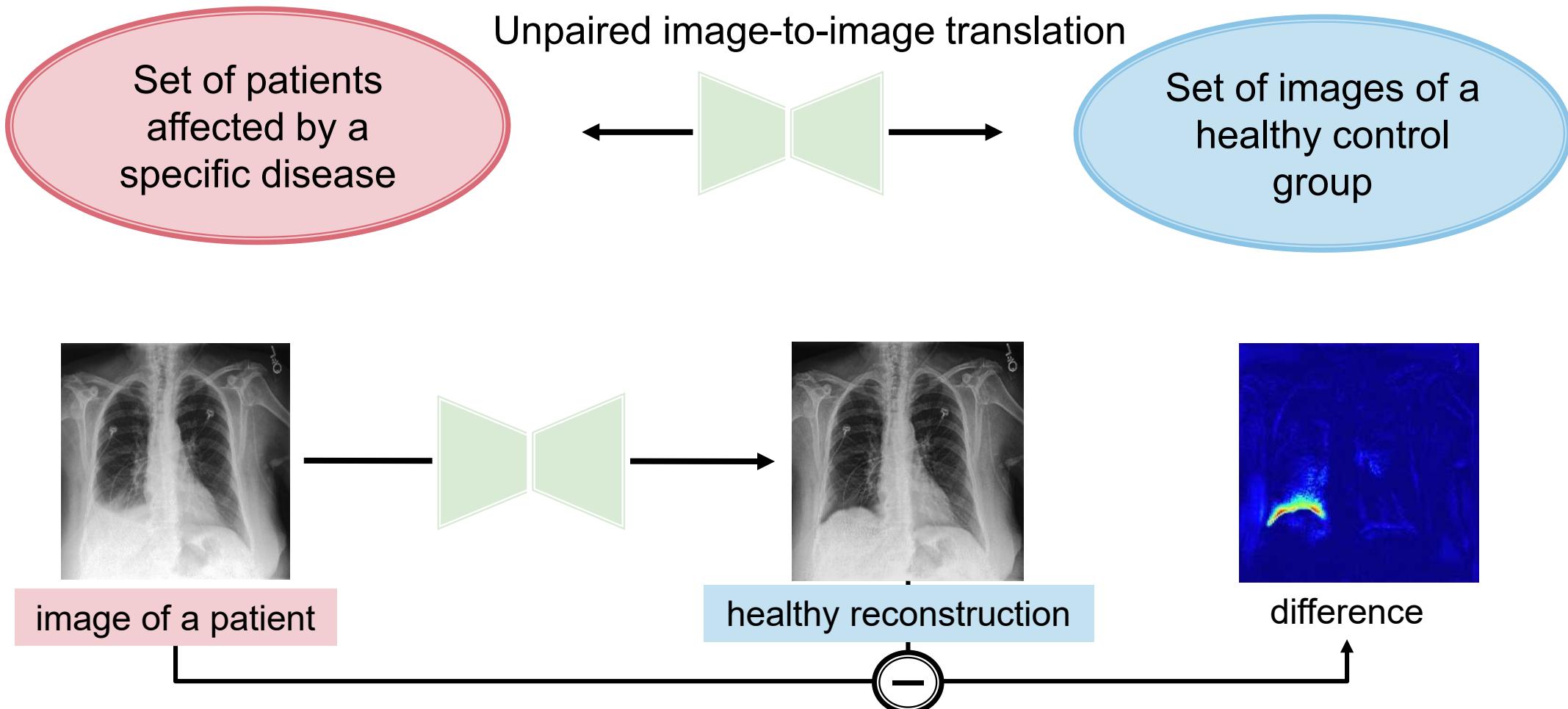


Weakly Supervised Lesion Detection

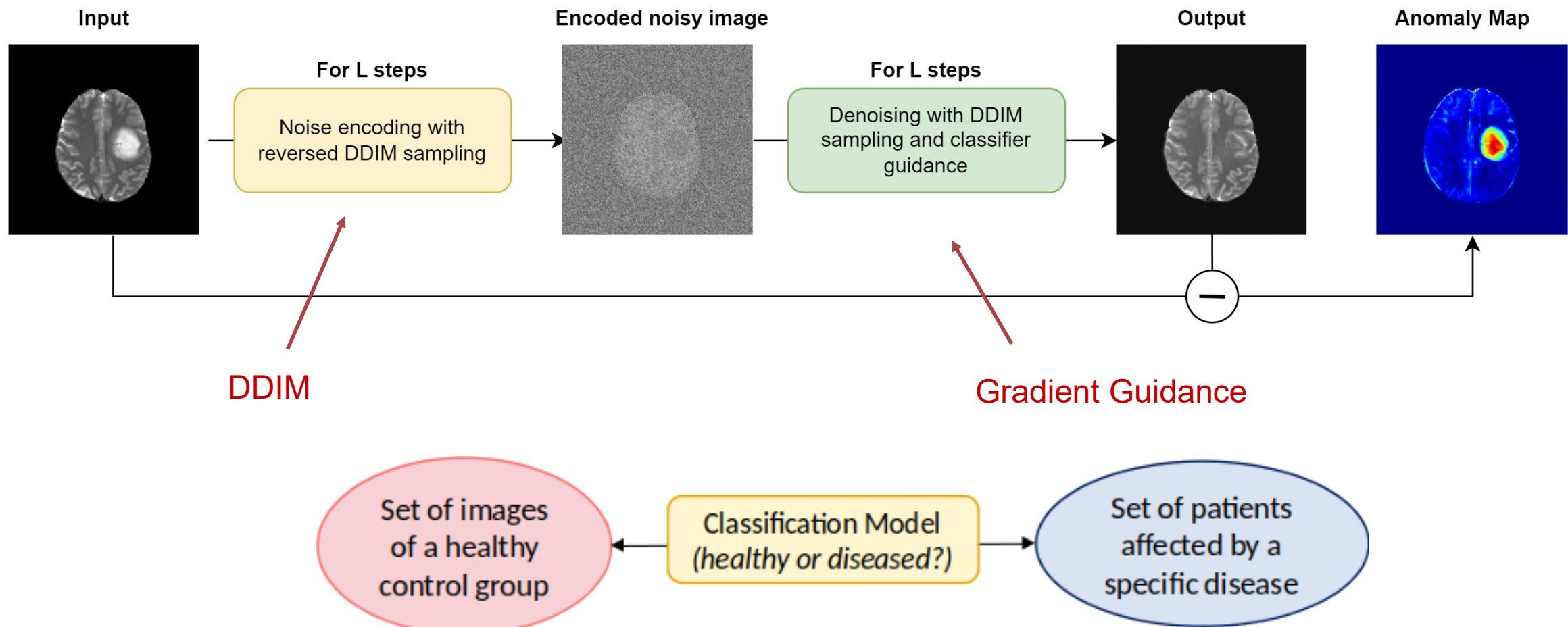
- **Goal:** Pixel-wise anomaly detection using image-level labels only



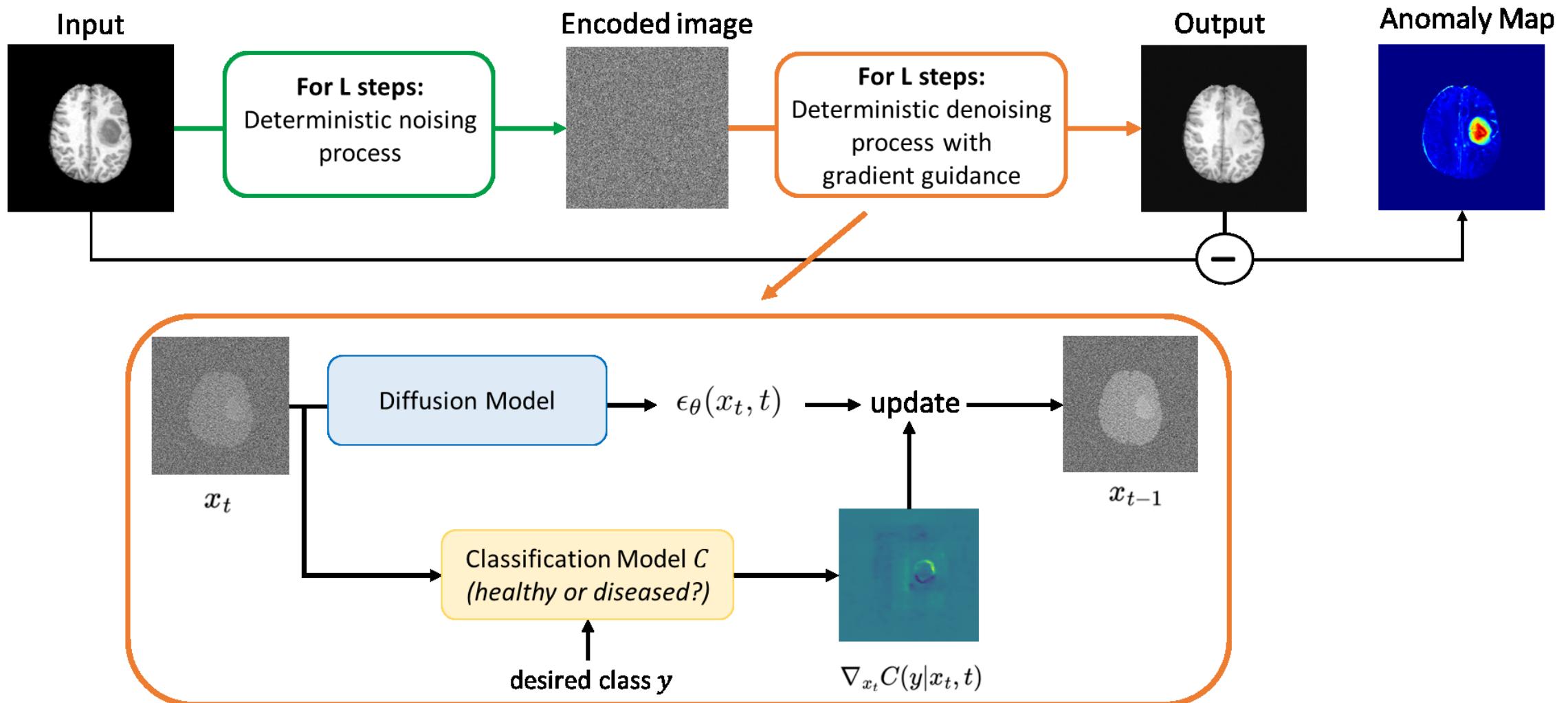
Weakly Supervised Lesion Detection



Weakly Supervised Lesion Detection



Gradient Guidance



Lesion Localization with Diffusion Models

Classifier-free guidance

1. DDIM Encoding - Empty condition
2. DDIM Decoding - Target class

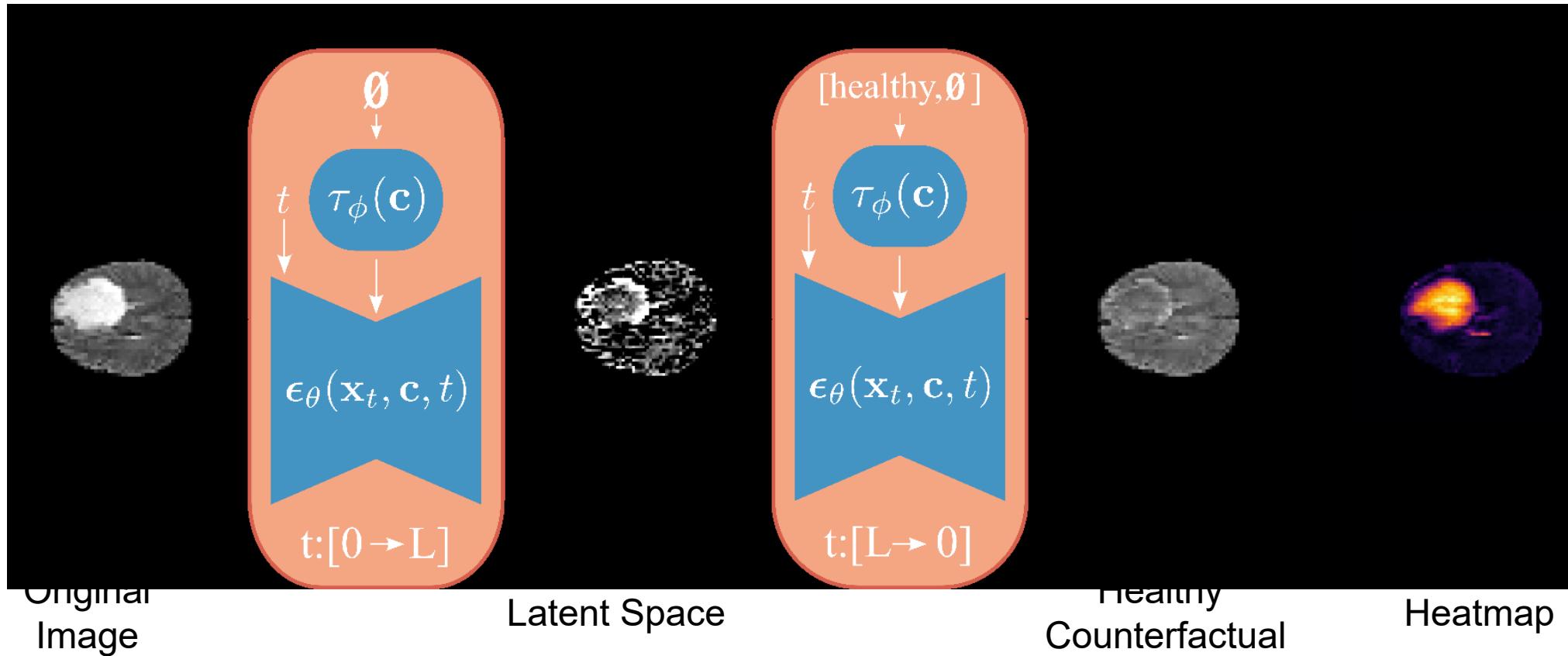


Image Reconstruction

Image Registration

Anomaly Detection

Image Segmentation

Image-to-Image Translation

Image Synthesis

Inpainting



Dr. Walter Pinaya



synthesia

Dr. Julia Wolleb



Universität
Basel

Prof. Jong Chul Yoo



Prof. Jorge Cardoso



Prof. Dorit Merhof



Panel Discussion

Diffusion Models for Medical Images

Prof. Bernhard Kainz



FAU
Friedrich-Alexander-Universität
Erlangen-Nürnberg

Imperial College
London

Dr. Alison O'Neil



Canon
CANON MEDICAL

Prof. Sotirios A. Tsaftaris



THE UNIVERSITY
of EDINBURGH

Useful key references, gits to watch etc

- Surveys
 - <https://arxiv.org/abs/2209.02646>
 - <https://arxiv.org/abs/2209.00796>
- Github
 - <https://github.com/heejkoo/Awesome-Diffusion-Models>
- Tutorial
 - <https://cvpr2022-tutorial-diffusion-models.github.io>
 - <https://huggingface.co/blog/annotated-diffusion>
 - <https://huggingface.co/docs/diffusers>