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# Speech enhancement using binary estimator selection applied to hearing aids with a remote microphone

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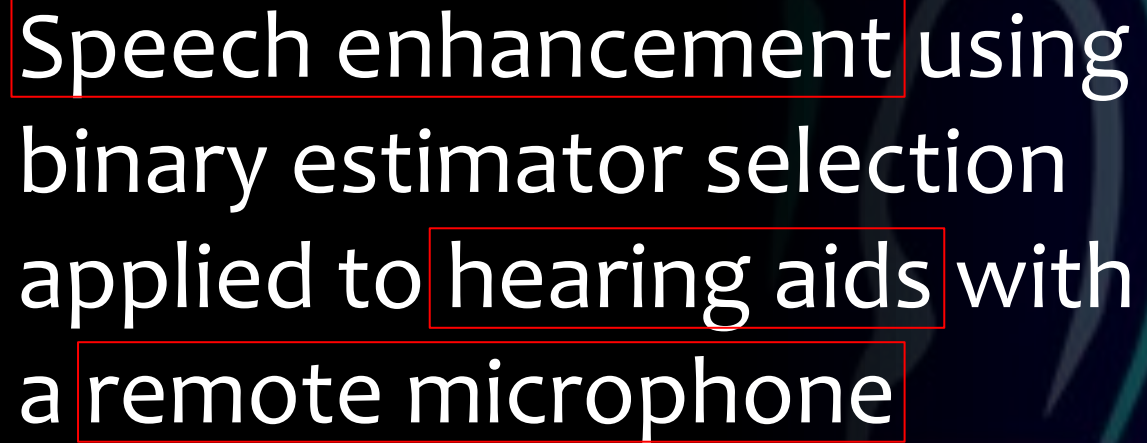
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A stylized illustration of a human ear in profile, facing right, rendered in a light blue color. Behind the ear, there are several concentric, wavy lines representing sound waves, also in light blue. The background is a solid dark blue.

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# Overview

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- Introduction
- Proposed Method
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# Overview

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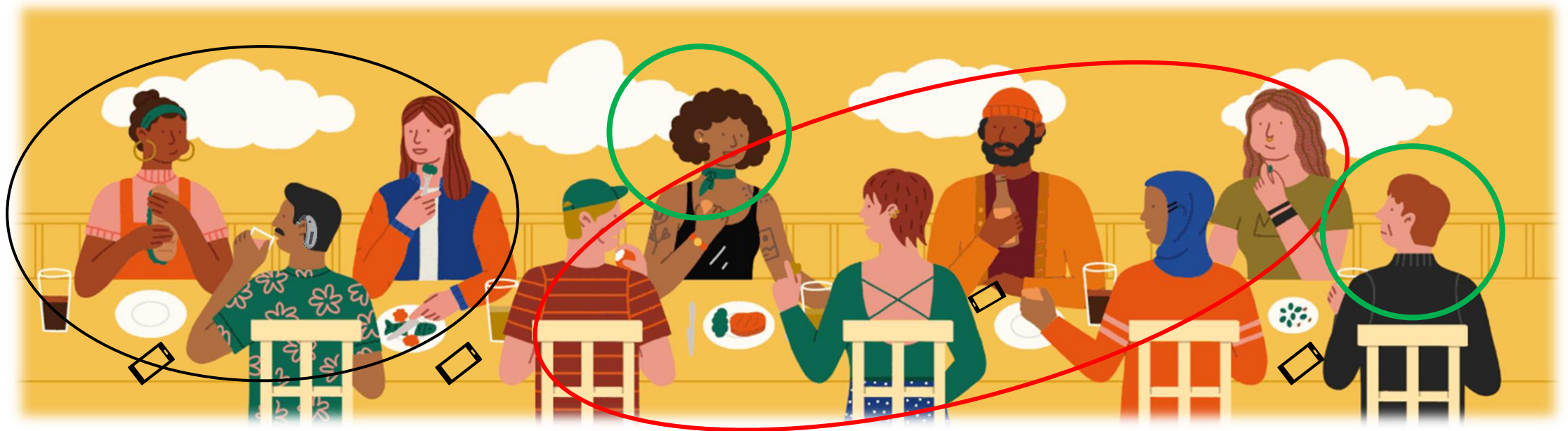
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# Motivation



Source: Behance.net

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# Motivation

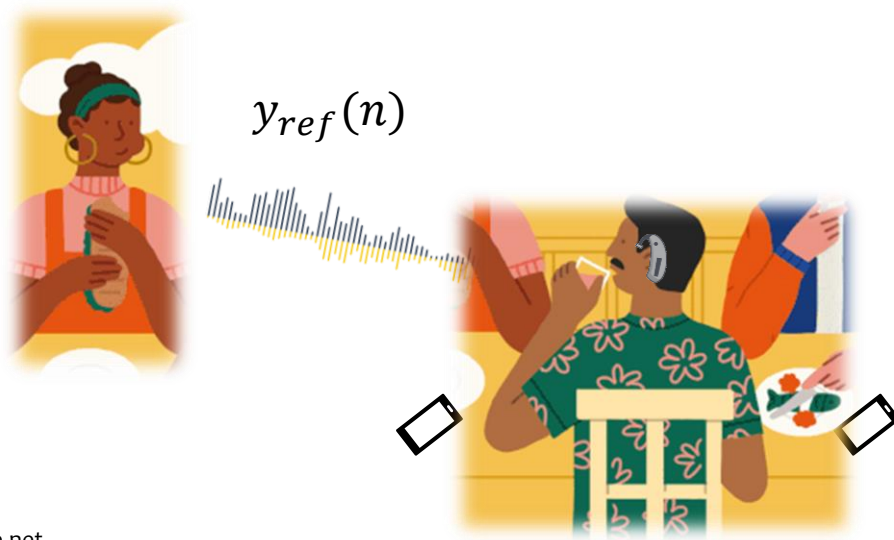


Introduction

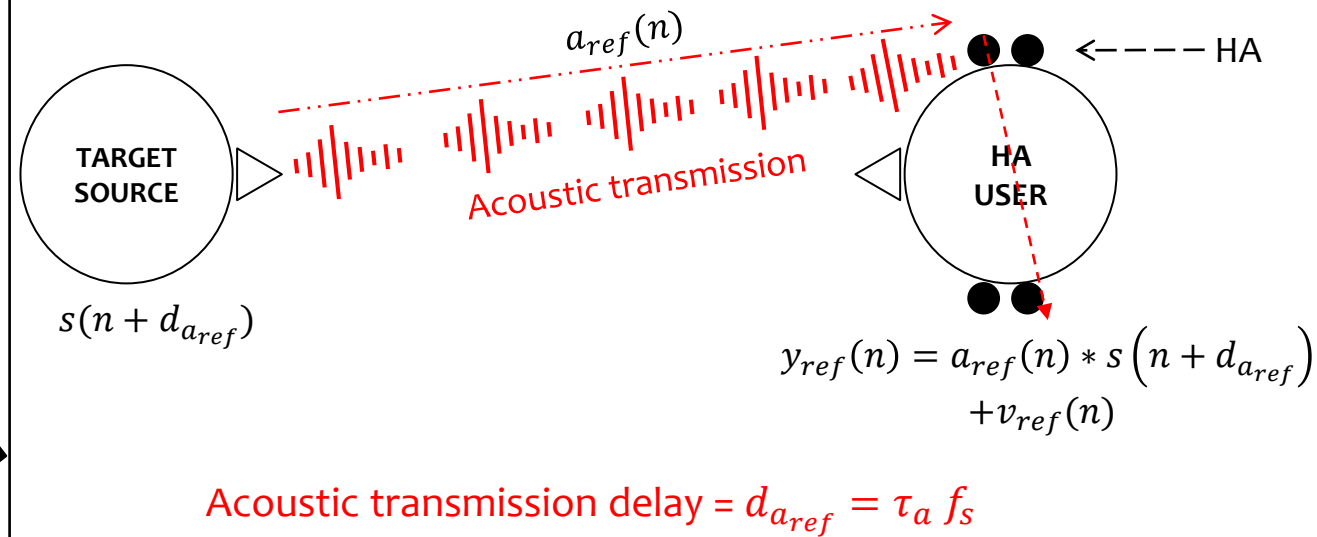
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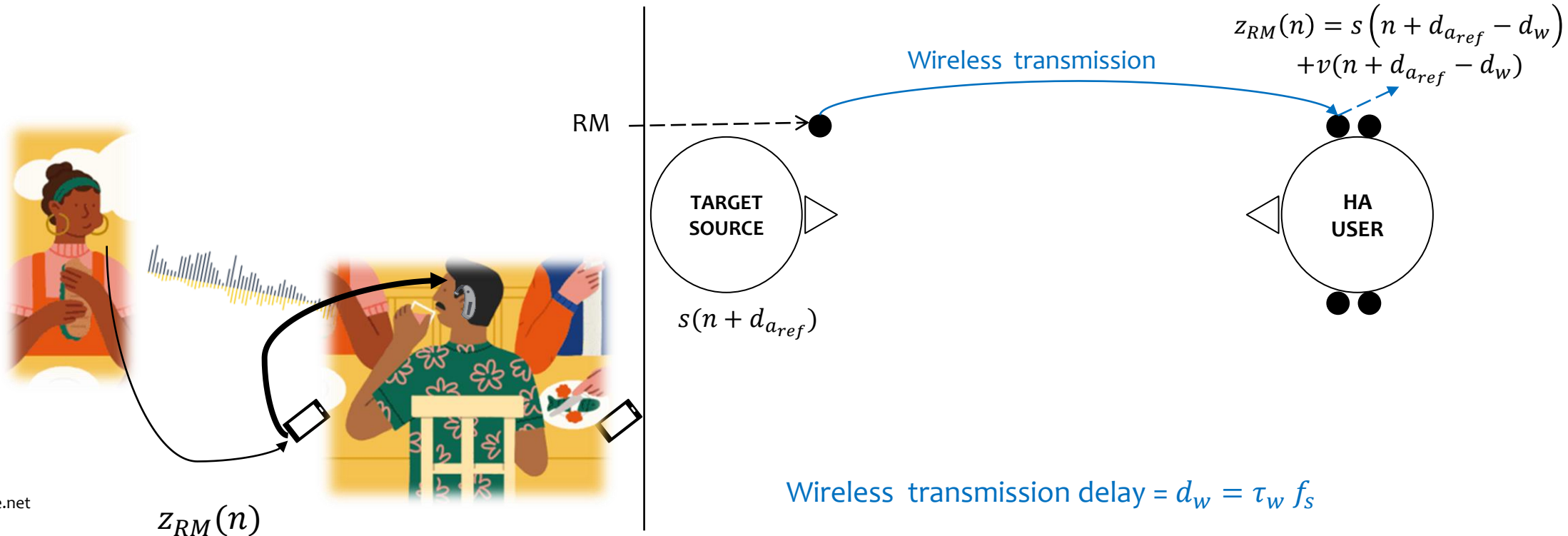


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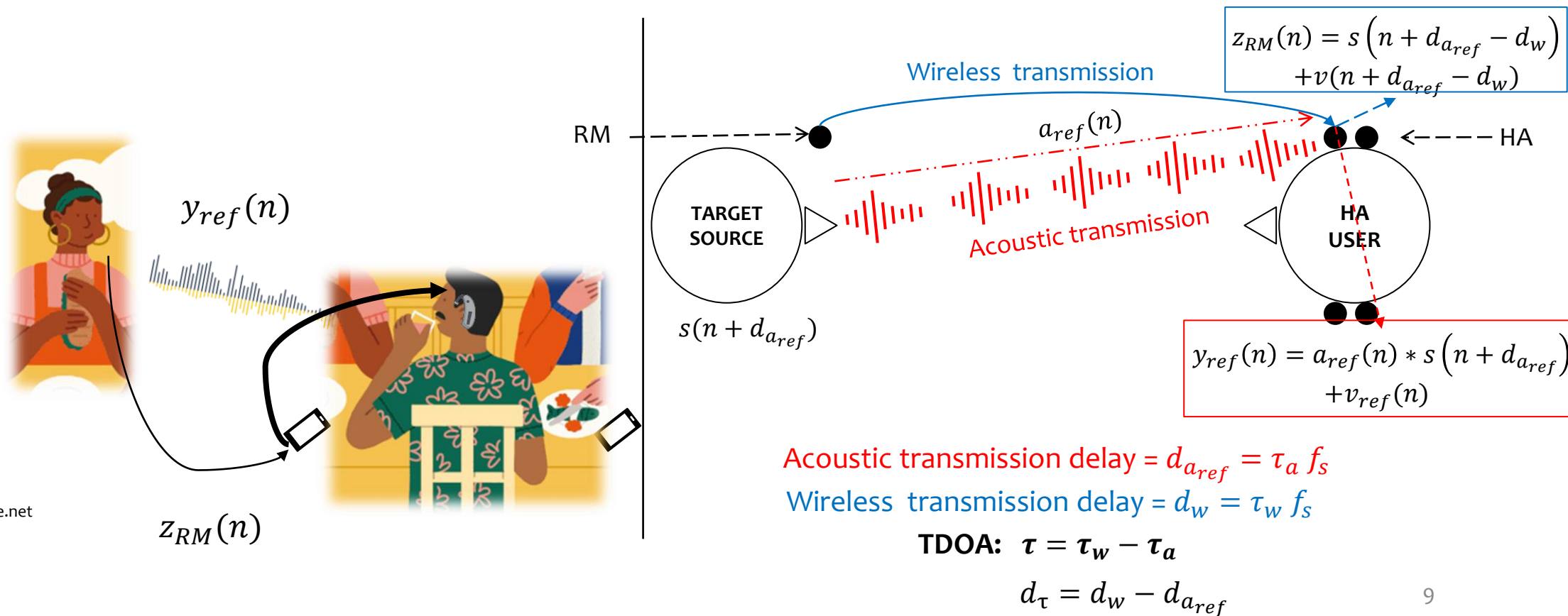


Introduction

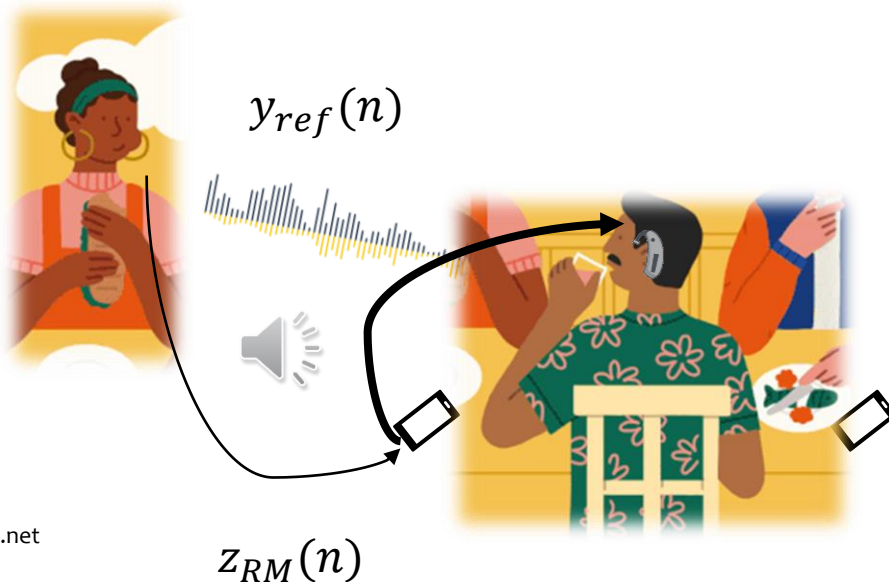
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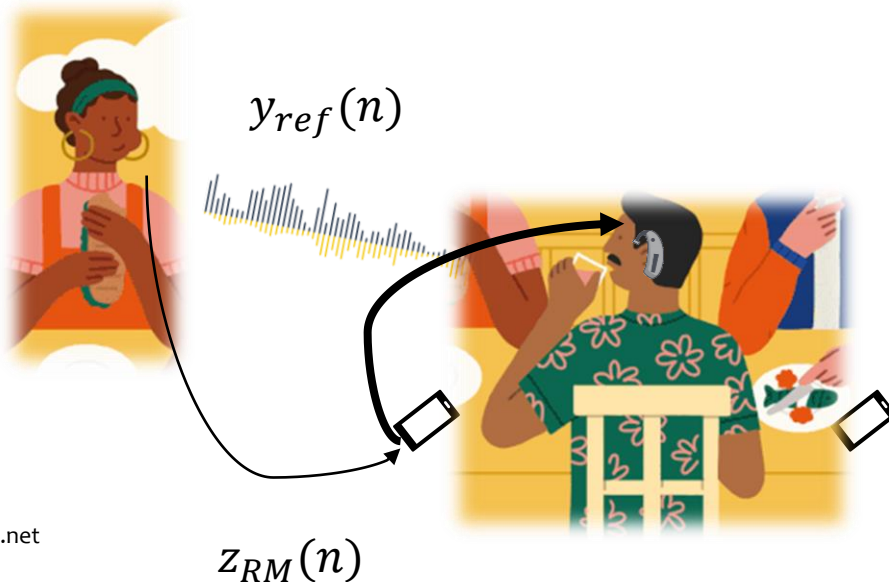
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Where  $\tau$  is the **time difference of arrival (TDOA)** between the airborne acoustic signal,  $y(n)$ , and the wirelessly transmitted signal,  $y(n - d_\tau)$ .

1. Short TDOAs lead to comb-filtering effect [1].  
1–10 ms
2. Long TDOAs lead to echoes [1].  
>10 ms

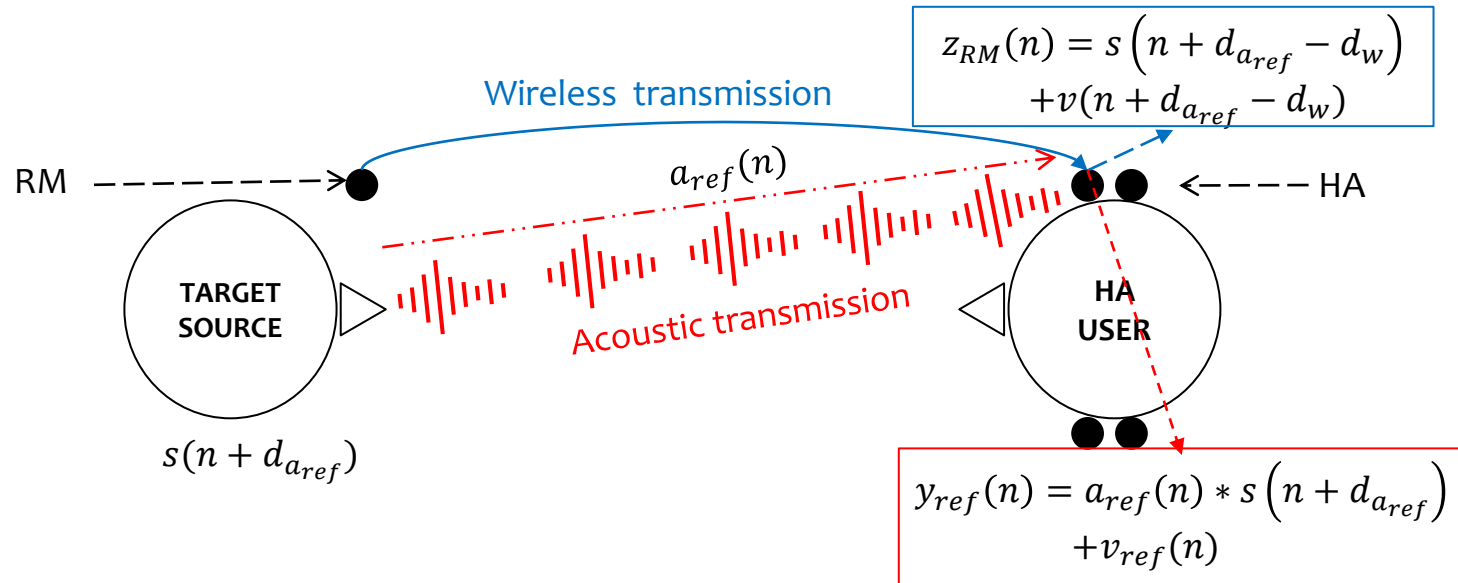


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1. TDOA,  $\tau$ , can be positive i.e.,  $\tau \geq 0$  or negative i.e.,  $\tau < 0$ .
  - a) But for  $\tau < 0$ , the RM signal can be stored in a buffer.
  - b)  $0 \leq \tau \leq 10 \text{ ms}$ , to avoid undesirable perceptual audio effects [2].
2. Direct RM signal playback can be detrimental in the presence of TDOAs.

**Use a combination of HA microphone and RM signals !**

## Signal Model



Acoustic transmission delay =  $d_{a_{ref}} = \tau_a f_s$

Wireless transmission delay =  $d_w = \tau_w f_s$

TDOA:  $\tau = \tau_w - \tau_a$

**Signals available for processing :**

**From the HA microphones:**

$$y_{ref}(n) = x_{ref}(n) + v_{ref}(n)$$

$$\underline{y}_{HA}(n) = [y_1(n) \quad \dots \quad y_M(n)]^T$$

**From the RMs (received at the HA unit):**

$$y_{RM}(n) = \hat{a}_{ref}(n) * z_{RM}(n)$$

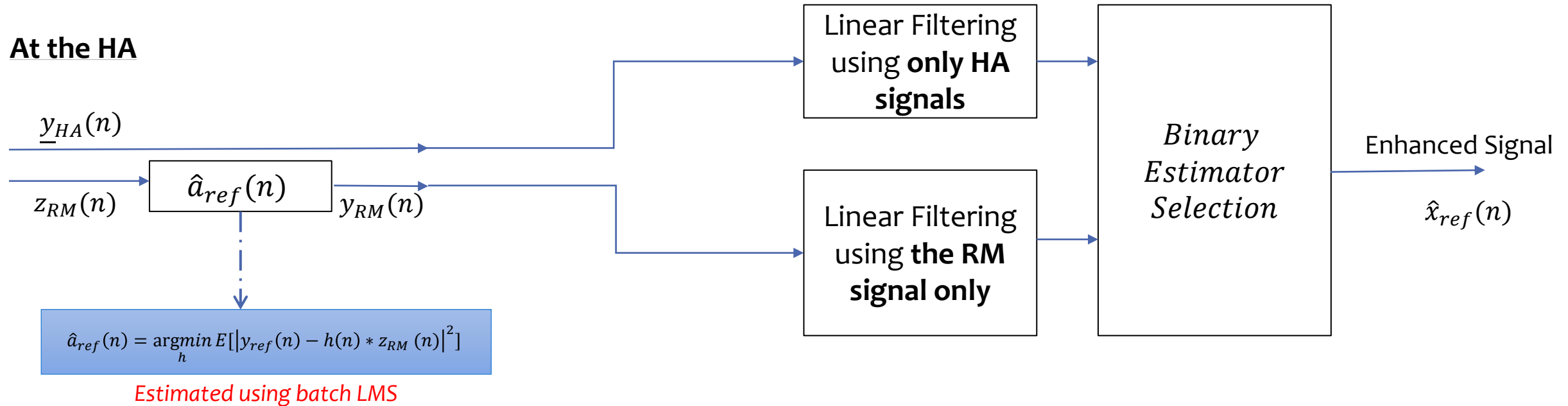
**Now, TDOA  $\{y_{ref}(n), y_{RM}(n)\}$ :  $\tau = \tau_w$**

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# Binary Estimator Selection Algorithm



# Signal Model

**Signals available for processing (in STFT domain):**

**From the HA microphones:**

$$\underline{y}_{HA}(k, l) = \begin{bmatrix} Y_{HA,1}(k, l) \\ Y_{HA,2}(k, l) \\ \vdots \\ Y_{HA,M}(k, l) \end{bmatrix} \in \mathbb{C}^{M \times 1}$$

**From the RMs (received at the HA unit):**

$$\underline{y}_{RM}(k, l) = \begin{bmatrix} Y_{RM}(k, l) \\ Y_{RM}(k, l-1) \\ \vdots \\ Y_{RM}(k, l-L+1) \end{bmatrix} \in \mathbb{C}^{L \times 1}$$

$Y_{HA,m}(k, l)$  – STFT coefficient of the  $m^{th}$  noisy HA microphone signal,  $y_m(n)$ .

$Y_{RM}(k, l)$  – STFT coefficient of the noisy RM signal received at the HA,  $y_{RM}(n)$ .

$\underline{y}_{HA}(k, l)$  – multi-channel HA STFT coefficient vector.

$\underline{y}_{RM}(k, l)$  – multi-frame RM STFT coefficient vector.

$M$  – number of HA microphones

$L$  – number of past-frames .

# Signal Model

*Signals available for processing (in STFT domain):*

**From the HA microphones:**

$$\underline{\mathbf{y}}_{HA}(k, l) = \begin{bmatrix} Y_{HA,1}(k, l) \\ Y_{HA,2}(k, l - 1) \\ \vdots \\ Y_{HA,M}(k, l - L + 1) \end{bmatrix} \in \mathbb{C}^{M \times 1}$$

**From the RMs (received at the HA unit):**

$$\underline{\mathbf{y}}_{RM}(k, l) = \begin{bmatrix} Y_{RM}(k, l) \\ Y_{RM}(k, l - 1) \\ \vdots \\ Y_{RM}(k, l - L + 1) \end{bmatrix} \in \mathbb{C}^{L \times 1}$$

Rank-1 Multi-channel Wiener Filter[3]:

$$\underline{\mathbf{w}}_{MWF} = \underset{\mathbf{w}}{\operatorname{argmin}} E[||\underline{\mathbf{w}}^H \underline{\mathbf{y}}_{HA} - X_{ref}||^2]$$

$$\hat{X}_{MWF} = \underline{\mathbf{w}}_{MWF}^H \underline{\mathbf{y}}_{HA}$$

Single Channel Multi-Frame Wiener Filter [4], [5]:

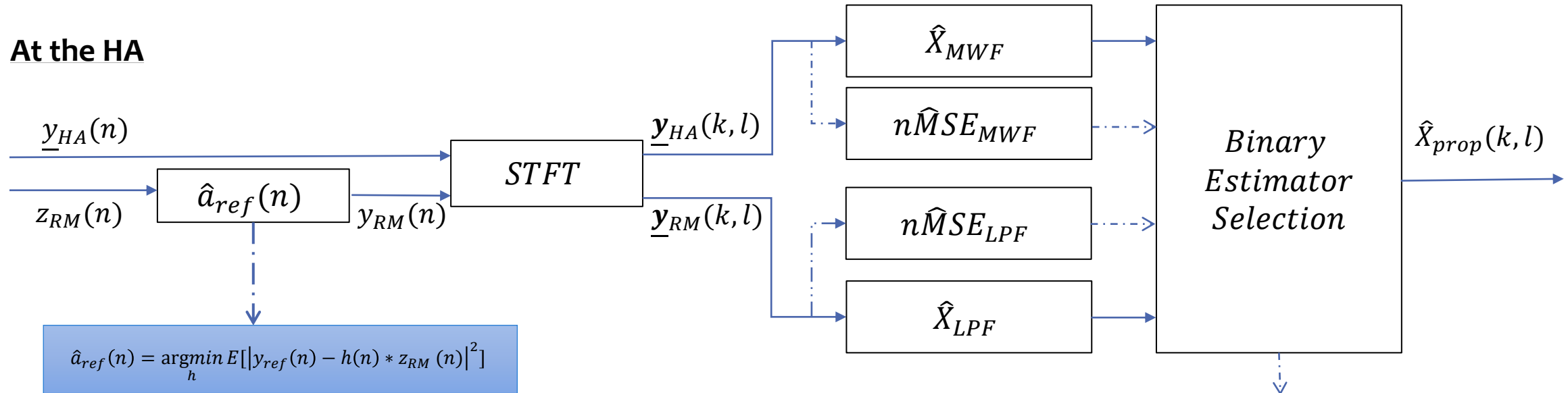
$$\underline{\mathbf{w}}_{LPF} = \underset{\mathbf{w}}{\operatorname{argmin}} E[||\underline{\mathbf{w}}^H \underline{\mathbf{y}}_{RM} - X_{ref}||^2]$$

$$\hat{X}_{LPF} = \underline{\mathbf{w}}_{LPF}^H \underline{\mathbf{y}}_{RM}$$



# Binary Estimator Selection Algorithm

**At the HA**



$$\hat{a}_{ref}(n) = \underset{h}{\operatorname{argmin}} E[|y_{ref}(n) - h(n) * z_{RM}(n)|^2]$$

Estimated using batch LMS

$$\hat{X}_{prop}(k, l) = \hat{G} \cdot \hat{X}_{MWF}(k, l) + (1 - \hat{G}) \cdot \hat{X}_{LPF}(k, l)$$

$$\hat{G}(k, l) = \begin{cases} 1, & \frac{nMSE_{MWF}(k, l)}{nMSE_{LPF}(k, l)} < 1 \\ 0, & \text{otherwise} \end{cases}$$

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### Simulation Parameters:

1. **Speech signal:** CSTR VCTK corpus [6] .
2. **HAHRIR:** Monaural Left ( $M=2$ ), anechoic hearing aid head-related impulse responses from [7].
3. **Noisy Types:** isotropic SSN, cafeteria noise recordings [7].
4. **SNR at the HA :** 0 dB.
5. **SNR at the RM:** 20 dB.
6. **TDOAs :** 0-40 ms.
7. **Performance metrics:** ESTOI (speech intelligibility), MSE (speech quality).

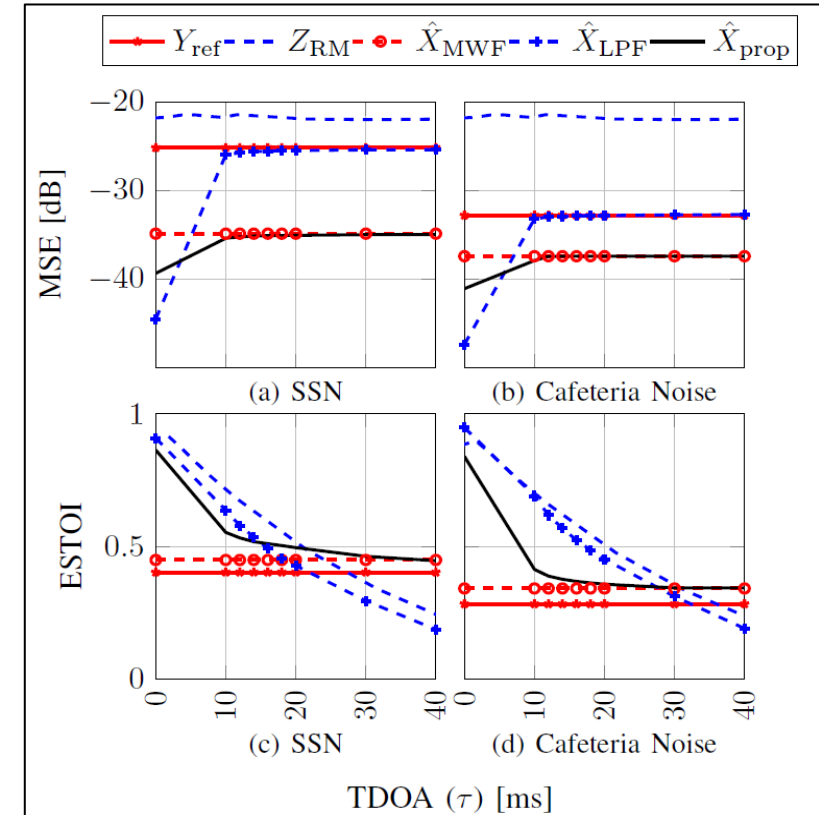


Figure 1 :Performance in terms of (a), (b) MSE and (c), (d) ESTOI for different TDOAs ( $\tau$ ), for SSN and Cafeteria Noise at 0 dB SNR.

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# Audio Examples

## Speech enhancement using binary estimator selection applied to hearing aids with a remote microphone

The demos consist of monoaural left signals for different noise and SNRs, headphones are recommended for listening.

- The monaural left signals are generated using measured HRIRs from the Kayser Database [3]
- The speech signals are taken from the VCTK Corpus [2]

This page was generated using **trackswitch.js** in [1].

### Isotropic Speech Shaped Noise



Source: [https://vsathyapriyan.github.io/bes\\_complex/](https://vsathyapriyan.github.io/bes_complex/)

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# Conclusion

- Remote microphone signal introduces **undesirable perceptual effects for  $\tau > 10$  ms**.
- Binary estimator selection (BES) algorithm **uses both the HA and RM signals**, in the presence of a TDOA.
- Binary estimator selection (BES) algorithm, **chooses between** an MMSE filter on the HA microphone signals, **MWF** and an MMSE filter on the RM signals, **LPF**, in the presence of TDOAs.
- The **BES algorithm provides a benefit in estimated speech intelligibility for  $0 \leq \tau \leq 30$  ms**, over the MWF, that uses only the HA microphone signals.

# References

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Questions?



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