

# **MEDICAL SENSORS**

PROJECT REPORT

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## **PET/CT Image Denoising and Segmentation based on a Multi Observation and Multi Scale Markov Tree Model**

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October 29, 2016

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## **Chapter 1**

# **Introduction**

## **Chapter 2**

# **Literature Review**

## **2.1 HMT**

I am with Minh the bitch.

## 2.2 2D DISCRETE WAVELET TRANSFORM

### 2.2.1 Overview

A wavelet is a wave-like oscillation with an amplitude that begins at zero, increases, and then decreases back to zero. It can typically be visualized as a "brief oscillation" like one recorded by a seismograph or heart monitor [1]. As a mathematical tool, wavelets can be used to extract information from many different kinds of data, including – but certainly not limited to – audio signals and images [2].

In numerical analysis and functional analysis, a Discrete Wavelet Transform (DWT) is any wavelet transform for which the wavelets are discretely sampled. As with other wavelet transforms, a key advantage it has over Fourier Transform (FT) is temporal resolution: it captures both frequency and location information (location in time) [3].

In signal processing, wavelets make it possible to recover weak signals from noise. This has proven useful especially in the processing of X-ray and magnetic-resonance images in medical applications. Images processed in this way can be "cleaned up" without blurring or muddling the details [4].

### 2.2.2 Definition

In 2-Dimensional dyadic multiresolution, a wavelet orthonormal basis in  $L^2(\mathbb{R}^2)$  is built up from (tensor) products involving:

- A scale function  $\varphi$  associated to a multiresolution  $\{V_j\}_{j \in \mathbb{Z}}$  of  $L^2(\mathbb{R})$
- An orthonormal wavelet  $\psi \in L^2(\mathbb{R})$  to define a complete orthonormal system, for the Hilbert space  $L^2(\mathbb{R})$  of square integrable functions.

The orthonormal wavelet  $\psi$  is constructed as the family of functions:

$$\psi_{jn}^k(x) = 2^{\frac{j}{2}} \psi^k\left(2^j x_1 - n_1, 2^j x_2 - n_2\right) \quad (2.1)$$

for integers  $j, k \in \mathbb{Z}$ .

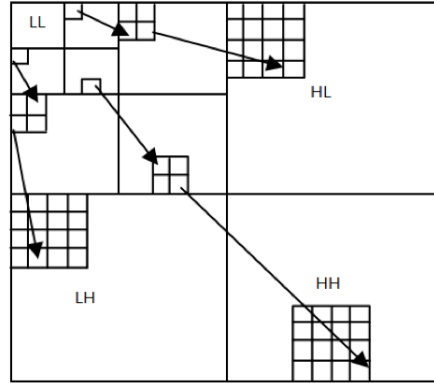
For this purpose, one defines three wavelets:

$$\psi^1(x_1, x_2) = \varphi(x_1)\psi(x_2) \quad (2.2a)$$

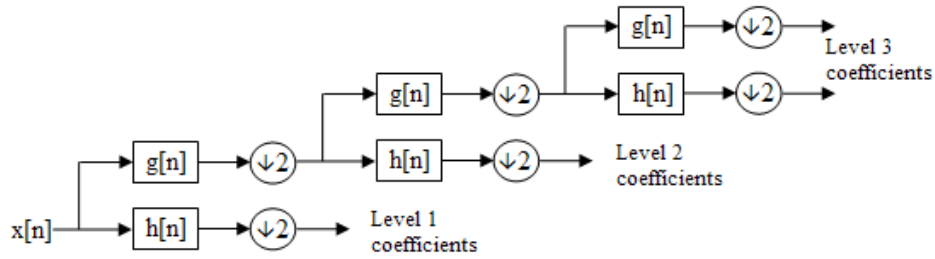
$$\psi^2(x_1, x_2) = \psi(x_1)\varphi(x_2) \quad (2.2b)$$

$$\psi^3(x_1, x_2) = \varphi(x_1)\varphi(x_2) \quad (2.2c)$$

In the case of the discrete wavelet transform, the mother wavelet is shifted and scaled by powers of



**Figure 2.1:** Wavelet coefficients arrangement



**Figure 2.2:** A 3 level filter bank

two:

$$\psi_{j,k}(t) = \frac{1}{\sqrt{2^j}} \psi\left(\frac{t - k2^j}{2^j}\right) \quad (2.3)$$

where  $j$  is the scale parameter and  $k$  is the shift parameter, both which are integers.

Recall that the wavelet coefficient  $\gamma$  of a signal  $x(t)$  is the projection of  $x(t)$  onto a wavelet, and let  $x(t)$  be a signal of length  $2^N$ . In the case of a child wavelet in the discrete family above:

$$\gamma_{jk} = \int_{-\infty}^{\infty} x(t) \frac{1}{\sqrt{2^j}} \psi\left(\frac{t - k2^j}{2^j}\right) dt \quad (2.4)$$

This decomposition, which can be seen in Figure 2.1 [5], is repeated to further increase the frequency resolution and the approximation coefficients decomposed with high and low pass filters and then down-sampled. This is represented as a binary tree with nodes representing a sub-space with a different time-frequency localisation. The tree is known as a filter bank, see Figure 2.2.

## **2.3 CONTOURLET TRANSFORM**



## **2.4 PET IMAGE DENOISING**

## **2.5 PET/CT IMAGE SEGMENTATION**

## **Chapter 3**

# **Implementation**

## **Chapter 4**

# **Result and Discussion**

## **Chapter 5**

## **Conclusion**

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I want to cite this paper [5]

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