## ORIGINAL ARTICLE: CYSTIC FIBROSIS-PEDIATRIC & ADULT





# The effects of high-frequency chest compression on end-tidal CO<sub>2</sub>

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#### Abstract

Introduction: High-frequency chest compression (HFCC) is used for airway clearance, but may have other effects. We sought to determine if HFCC provides augmented ventilation.

Methods: During treatment, capnometry was measured with the HFCC vest set to 6-20 Hz. End-tidal CO<sub>2</sub> (etCO<sub>2</sub>) was compared using generalized estimating equations.

Results: Twenty-four measurements were obtained from 15 subjects with mean age 15.2 ± 2.5 years and forced expiratory volume in one second (FEV<sub>1</sub>) % predicted 70 ± 23. EtCO<sub>2</sub> decreased with HFCC at 6 Hz when compared with baseline (P < .001), with small changes with increasing oscillation frequency. Change in etCO<sub>2</sub> was not predicted by FEV<sub>1</sub>, body mass index, age, or sex.

Conclusions: While HFCC has been shown to be a suitable method of airway clearance, investigators have failed to demonstrate differences between techniques. Assessment of these methodologies will become important as new airway clearance devices are proposed. Other outcome measures (besides FEV<sub>1</sub>) may be needed to assess effects of airway clearance, and we propose that physiologic measures might be one such measure which deserves further exploration.

#### **KEYWORDS**

capnometry, cystic fibrosis, high-frequency chest compression, ventilation

# 1 | INTRODUCTION

Cystic fibrosis (CF) is characterized by increased sputum viscosity, defective mucociliary clearance and airway obstruction. Airway clearance treatments including high-frequency chest compression (HFCC), are a mainstay of treatment of CF.<sup>2,3</sup> Comparisons between airway clearance methods are challenging.3 HFCC is the most popular choice for patients with CF in the U.S., although less common in other countries.4 We demonstrated that different HFCC frequencies have differing effects on volume and flow measured at the mouth.<sup>5</sup> We also observed increased changes in expiratory volumes with lower oscillation frequencies.<sup>5,6</sup> Thus we sought to determine if HFCC provides augmented ventilation (as assessed by

end-tidal CO2 [etCO2]) and whether the degree of ventilation is related to oscillation frequency or other patient factors.

#### 2 | METHODS

Patients with CF were recruited from the inpatient service at Children's Hospital of Pittsburgh if they were 6 to 21 years old, and admitted for pulmonary exacerbation. Subjects were excluded if they had pneumothorax, hypoxemia, or moderate/severe hemoptysis. Patients were offered the opportunity to repeat measurement in 7 days if they remained hospitalized. This study was conducted with the approval of the Institutional Review Board of the University of

Pittsburgh. Informed consent was obtained from the parents/patients before participation.

#### 2.1 | Capnometry

During a HFCC treatment, a sampling cannula was placed within the nostrils and connected to a digital capnometer (Capnostream™ 35, Medtronics, Boulder, CO). Patients were asked to close their mouth and take three to five normal (tidal) breaths through their nose, and etCO₂ was recorded. The HFCC vest (The Vest, Hill-Rom, Chicago, IL) was set to a pressure of 7 out of 10, and frequency of 6 Hz. After 1 minute of treatment, etCO₂ was re-measured and the HFCC treatment continued for four additional minutes. The device was paused, the patient was asked to cough three to four times, and an additional etCO₂ measurement was collected with the patient breathing through their nose to document recovery to baseline. This procedure was repeated with different HFCC frequencies (8, 10, 16, 18, and 20 Hz), with treatment at each frequency lasting 5 minutes. Capnography with a baseline etCO₂ of <30 mm Hg or an unstable tracing was excluded.

Subject characteristics were abstracted from the chart including age, sex, body mass index (BMI), and most recent spirometry results normalized according to GLI2012 equations.<sup>7</sup>

# 2.2 | Analysis

Differences in  $etCO_2$  and respiratory rate were compared with repeated measures analysis of variance with Tukey's multiple comparisons test, and generalized estimating equations using xtgee (STATA v15, StataCorp LLC, College Station, TX), adjusting for age, sex, BMI, forced expiratory volume in one second (FEV<sub>1</sub>), and respiratory rate.

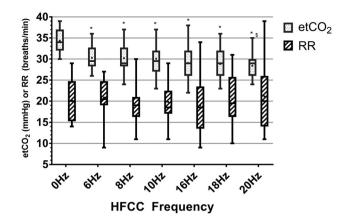
#### 3 | RESULTS

### 3.1 | Subjects

Twenty subjects with CF were recruited, 15 (5 M/10 F) of whom produced usable capnography. Subjects had a mean  $\pm$  standard deviation (range) age of  $15.2 \pm 2.54$  (10.8-19.8) years, BMI of  $50 \pm 27$  (0.98-90.6) percentile, and FEV<sub>1</sub> of  $70 \pm 23$  (29-112) percent-of-predicted.

#### 3.2 | Capnometry data

A total of 24 measurements were gathered from the 15 subjects. No complications occurred during testing. Changes in etCO<sub>2</sub> and respiratory rate with varied oscillation frequencies are depicted in Figure 1. All frequencies had lower etCO<sub>2</sub> compared with vest off (P<.0001), and etCO<sub>2</sub> at 20 Hz was lower than at 6, 8, and 10 Hz (P<.05). After adjusting for patient age, sex, BMI, baseline FEV<sub>1</sub>, and respiratory rate, modeled etCO<sub>2</sub> decreased significantly with application of HFCC at 6 Hz when compared with baseline (-4 mm



**FIGURE 1** EtCO<sub>2</sub> (dotted bars, mm Hg) and respiratory rate (hatched bars, breaths per minute) measured during a treatment with high-frequency chest compression at a variety of oscillation frequencies from 6 to 20 Hz. Median values represented by horizontal bar, mean values by X. EtCO<sub>2</sub> at each frequency was lower (P < .05, \*) than with vest off (0 Hz), and etCO<sub>2</sub> at 20 Hz was lower (P < .05) than at 0, 6, 8, and 10 Hz (\$). EtCO<sub>2</sub>, end-tidal CO<sub>2</sub>; HFCC, high-frequency chest compression

Hg at 6 Hz vs baseline, P < .0001). Increasing frequencies produced a significant but very small slope in etCO<sub>2</sub> (-2 mm Hg at 20 Hz vs 6 Hz). Change in etCO<sub>2</sub> was not associated with baseline FEV<sub>1</sub>, BMI, age or sex. Respiratory rate was associated with lower etCO<sub>2</sub> (-0.12 mm Hg per breath/minute, P = .022), but there were no differences in rate between baseline and any frequencies (P = .57).

#### 4 | DISCUSSION

The main finding of our study is that HFCC results in augmented ventilation as assessed by a lower etCO<sub>2</sub>. HFCC is a suitable method of airway clearance and sputum production in patients with CF similar to conventional physiotherapy,<sup>8</sup> but most investigators have failed to demonstrate significant differences between HFCC and positive expiratory pressure devices for treatment of CF.<sup>4</sup>

Interestingly, we found that all frequencies lowered  $etCO_2$  compared with "vest off", but a relatively small difference in  $etCO_2$  between frequencies. This was not predicted based on prior observations<sup>5,6</sup> that lower frequencies tended to result in greater changes in exhaled volume and higher frequencies tended to result in greater changes in airflow rate. Subjects in the current study were experiencing an acute exacerbation of their obstructive lung disease, while patients in the other studies were studied when well, and this could contribute to this finding.

Al-Saady analyzed external high-frequency oscillation (EHFO) and  $CO_2$  in 20 healthy adult subjects and five adult subjects with respiratory failure wearing a cuirass ventilator.  $EtCO_2$  was measured in healthy subjects, and arterial  $pCO_2$  in subjects with respiratory failure at oscillation frequencies ranging from 1 to 5 Hz. EHFO significantly decreased  $etCO_2$  or  $PaCO_2$  at all frequencies, maximally from 38 to 27 mm Hg. In patients with respiratory failure, EHFO was

shown to increase  $PaO_2$  and decrease  $PaCO_2$ . Is it difficult to relate their findings to ours, as their study differed in the patient population, use of arterial  $pCO_2$ , the methods of chest wall oscillation (cuirass vs inflatable vest), and the oscillation frequencies (much lower than ours).

Studies of airway clearance techniques have often used spirometry outcome measures. As  $\mathsf{FEV}_1$  tends to change relatively slowly, studies to detect differences in airway clearance methodologies using this outcome would require a large sample size or a prolonged follow-up period. Additionally, some studies may use markers, such as sputum weight, which may be unfeasible in a pediatric population. Rigorous assessments of these methodologies may be increasingly important as new devices,  $^{10-12}$  including portable devices lacking clinical evidence, are proposed for patient use.

Other outcome measures might be used to assess effects of airway clearance. These include imaging techniques (eg, He-MRI, He-MRI, 14 nuclear medicine clearance scans 15) or other pulmonary function measures (eg, multiple breath washout 16,17). We propose that physiologic measures, such as changes in ventilation that we observed may also allow for comparisons between airway clearance methods.

There are several limitations with this study. First, our sample size was relatively small. Although we attempted to allow  $etCO_2$  to return to baseline, we cannot exclude a degree of carryover effect between oscillation frequencies, the order of which was not randomized. Other factors, such as the coughing maneuvers may also have contributed to changes in  $etCO_2$ . Additionally,  $etCO_2$  may underestimate blood  $pCO_2$  due to leak around the cannula, although there is no reason for such leak to be consistently higher after the baseline  $etCO_2$  measurement.

In summary, HFCC mildly increases minute ventilation in patients with CF. The clinical implications of this observation, and its potential use to compare devices, deserve further exploration.

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