
DinoV3–LSTM for Early-Stage Classification of Paroxysmal Atrial Fibrillation in ECGs Toward Prediction

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Abstract

1 Detecting precursors of paroxysmal atrial fibrillation in long-term ECGs is crucial
2 for timely intervention but remains difficult because precursor signals are subtle
3 and patient physiology varies widely. We present a streamlined framework that
4 adapts a distillation-based vision foundation model, DinoV3, to multi-channel
5 two-dimensional ECG encodings and combines it with an LSTM to form an
6 indicator model for precursor classification. We use three complementary 2D
7 representations—short-time Fourier transform, Gramian angular field, and progres-
8 sive moving-average transform—to capture time–frequency structure, temporal
9 relationships, and multiscale trends, respectively. Evaluated as a precursor clas-
10 sification study on public long-term ECG datasets, the DinoV3–LSTM pipeline
11 achieves competitive performance despite the absence of ECG-specific fine-tuning.
12 Finally, we outline two concrete next steps to move from precursor classification to
13 clinically useful prediction: ECG-domain fine-tuning with end-to-end optimiza-
14 tion, and rigorous lead-time and prospective validation to quantify true prediction
15 capability.

16 **1 Introduction**

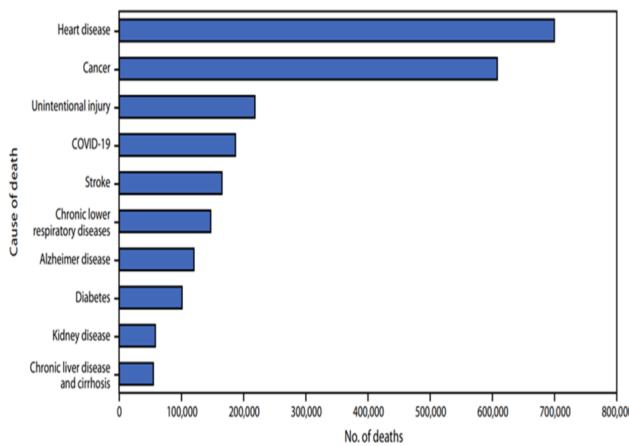


Figure 1: Global mortality statistics related to diseases

17 Cardiovascular diseases (CVDs) remain the leading cause of global mortality, a figure projected to
18 rise with the accelerating global aging population [1, 2]. Among these, cardiac arrhythmias represent

19 a significant and often life-threatening subclass. Paroxysmal atrial fibrillation (PAF), a common type
20 of irregular heart rhythm, is particularly dangerous as it can lead to severe complications such as
21 stroke, heart failure, and sudden cardiac death if not detected and managed promptly [3]. While
22 often asymptomatic, PAF can manifest as palpitations, shortness of breath, or dizziness, and its
23 transient nature makes timely diagnosis and intervention challenging. For patients with underlying
24 cardiac conditions or advanced heart failure, the sudden onset of PAF can be critically destabilizing,
25 necessitating proactive and early warning systems.

26 The advancement of artificial intelligence (AI), particularly in deep learning, has spurred numerous
27 research efforts in ECG-based arrhythmia classification, including PAF detection [4, 5]. These
28 studies have demonstrated impressive accuracy in identifying various arrhythmias from ECG signals.
29 However, a significant limitation of most existing AI-ECG approaches is their focus on classification,
30 determining the current cardiac state based on a contemporaneous ECG recording. While valuable
31 for diagnosis, this retrospective analysis falls short for patients where anticipation of an event is
32 paramount. For vulnerable individuals, such as those with advanced heart failure or other severe
33 cardiac comorbidities, a real-time predictive capability for impending PAF is not merely beneficial
34 but essential for enabling proactive medical intervention and preventing catastrophic outcomes.

35 In response to this critical need, a growing body of research has explored predictive models for
36 arrhythmias. These studies can generally be categorized into a few types: (1) **Feature-based**
37 **Predictive Models** that rely on hand-crafted features from heart rate variability (HRV) or P-wave
38 morphology extracted from preceding ECG segments, often utilizing machine learning classifiers like
39 SVM or decision trees [6, 7]. (2) **End-to-End Deep Learning Classification** approaches that use
40 neural networks to directly classify ECG segments into "normal" or "pre-AF" states within a fixed
41 temporal window before onset [8]. (3) More recently, **Self-Supervised Learning (SSL) enhanced**
42 **models** that leverage unlabeled ECG data to pre-train robust feature extractors. A notable example
43 is a recent study utilizing an MAE-based 1D-ViT [9] for feature extraction, followed by an LSTM
44 network for modeling state transitions and issuing early warnings for both PAF and ventricular
45 fibrillation (VF) [10]. This pipeline demonstrated strong performance.

46 Despite these advances, the MAE-LSTM pipeline, while effective, presents a key limitation. It
47 typically involves a decoupled training process in which the feature extractor (MAE-based 1D-ViT)
48 and the temporal warning model (LSTM) are trained separately. In many cases, the pre-trained
49 encoder's weights are frozen or only partially adapted during downstream supervised fine-tuning.
50 This separation can restrict task-specific discriminability, as the features learned from a generic
51 masking task may not be optimally tuned for capturing the subtle, evolving patterns of pre-arrhythmic
52 states.

53 To address this limitation, we propose a novel end-to-end AF early warning framework that replaces
54 the MAE-based feature extraction module with DinoV3, a state-of-the-art self-supervised learning
55 backbone. We adapt DinoV3 to process 2D ECG patch representations (PMAT [11], STFT, GAF)
56 and integrate it seamlessly with an LSTM warning head, enabling joint optimization across the entire
57 pipeline. This end-to-end approach allows DinoV3 to refine its representation learning directly for
58 the early detection of precursor electrophysiological changes, while also benefiting from the strong
59 general priors inherited from its self-supervised pre-training.

60 It is noteworthy that, in our current study, DinoV3 was employed without additional fine-tuning on
61 large-scale ECG datasets. As a result, its performance is slightly lower than the best-reported MAE-
62 LSTM pipeline. Nonetheless, achieving comparable early warning accuracy without domain-specific
63 fine-tuning underscores DinoV3's potential as a powerful backbone for arrhythmia prediction. We
64 hypothesize that further fine-tuning and fully end-to-end optimization will unlock superior predictive
65 performance. Moreover, DinoV3's attention mechanisms provide interpretable patch-level saliency
66 maps, offering clinicians valuable insights into which ECG segments drive the early warning. This
67 work thus lays the foundation for more accurate, interpretable, and clinically actionable AF early
68 warning systems.

69 2 Related Work

70 This section reviews existing research pertinent to AF prediction and early warning systems, high-
71 lighting the progression from traditional methods to advanced deep learning and foundation models,
72 ultimately setting the stage for our proposed DinoV3-based end-to-end framework.

73 **2.1 AF Prediction and Early Warning Research**

74 Early and accurate prediction of AF is paramount for improving patient outcomes and preventing
75 severe complications such as stroke and heart failure [3]. Historically, AF prediction has largely relied
76 on manual feature engineering from electrocardiogram (ECG) signals, combined with conventional
77 machine learning classifiers.

78 **Traditional ECG Features and Shallow Models.** Classical approaches to AF prediction predomi-
79 nantly utilized hand-crafted features extracted from ECG recordings. These included various heart
80 rate variability (HRV) metrics, which quantify beat-to-beat variations in heart rate, and morphological
81 features such as P-wave duration, QRS complex characteristics, and T-wave abnormalities [6, 7].
82 Machine learning models like Support Vector Machines (SVMs), Logistic Regression, and XGBoost
83 were then employed to classify these features as indicative of impending AF. While these methods
84 offer a degree of interpretability and have shown promise in certain contexts, they suffer from signifi-
85 cant limitations. Their performance is highly sensitive to the accuracy of fiducial point detection (e.g.,
86 P-wave onset/offset), which can be challenging in noisy or atypical ECG recordings. Furthermore,
87 these models often require relatively long ECG windows (e.g., 5 minutes or more of R-R intervals) to
88 extract stable and reliable features, which can delay timely warnings [12].

89 **Deep Learning for AF Classification and Prediction.** The advent of deep learning has revo-
90 lutionized ECG analysis by enabling automatic feature extraction and classification directly from
91 raw or minimally preprocessed signals [4, 5]. Convolutional Neural Networks (CNNs) have proven
92 highly effective for learning complex spatio-temporal patterns in ECG data, achieving expert-level
93 performance in arrhythmia detection and classification [13]. Recurrent Neural Networks (RNNs),
94 particularly Long Short-Term Memory (LSTM) networks, are well-suited for modeling the sequen-
95 tial nature of ECG data, capturing temporal dependencies crucial for predicting future events [14].
96 However, many early deep learning methods primarily focused on classification of the current state
97 rather than prediction of future events. While valuable for diagnosis, this approach often falls short
98 in providing the necessary lead time for proactive intervention, especially for patients requiring
99 continuous monitoring for paroxysmal events.

100 **Pathway Modeling and Early Warning Frameworks.** To overcome the limitations of static
101 classification, more recent research has shifted towards pathway modeling or state-evolution mod-
102 eling. This paradigm frames the early warning task as monitoring the continuous progression of
103 cardiac states: from a normal state (S_0), through a precursor state (S_1) characterized by subtle
104 electrophysiological changes, to an eventual event state (S_2) like AF onset [15, 16]. Systems built
105 on this concept typically combine powerful feature encoders with recurrent models (like LSTMs)
106 to track these transitions over time. For instance, a recent work successfully utilized a Masked
107 Autoencoder (MAE)-based 1D Vision Transformer (ViT) as a feature extractor, paired with an LSTM
108 for modeling temporal evolution. This pipeline achieved remarkable performance in both PAF and
109 VF early warning tasks, delivering clinically relevant lead times while maintaining high accuracy
110 [15]. This approach optimized a combined metric (e.g., a harmonic metric, HM) that balances
111 accuracy and lead time, demonstrating the feasibility of effective early warning systems. However, a
112 common practice in such SSL-enhanced frameworks is that the pre-trained encoder's weights are
113 often fixed or only lightly fine-tuned during the subsequent warning training phase. This decoupling
114 can potentially hinder the optimal specialization of the feature extractor for the nuanced demands of
115 precursor detection, leaving some discriminative power untapped.

116 **2.2 Foundation Models and Self-Supervised Learning for ECG**

117 The concept of foundation models, trained on broad data at scale and adaptable to a wide range of
118 downstream tasks, has gained significant traction across various AI domains [17]. Self-Supervised
119 Learning (SSL) plays a crucial role in developing these models by enabling them to learn powerful,
120 general-purpose representations from unlabeled data, thereby addressing the data scarcity and labeling
121 challenges prevalent in medical fields such as ECG analysis [18].

122 **Self-Supervised Learning Strategies in ECG.** Common SSL strategies applied to ECG include:

123 • **Generative Models:** Methods like Masked Autoencoders (MAE) learn to reconstruct
124 masked or corrupted portions of the input signal. This forces the model to capture meaningful
125 underlying data structures [19]. For example, MAE-based pretraining on large ECG corpora
126 using 1D-ViT encoders has demonstrably improved downstream arrhythmia classification
127 performance [9].

128 • **Contrastive Learning:** Approaches such as SimCLR [20], CPC [21], and BYOL [22] learn
129 representations by maximizing the similarity between different augmented views of the
130 same data sample while minimizing similarity with other samples. These methods have also
131 been successfully applied to learn robust features from ECG data [23].

132 Despite their effectiveness, a common challenge for these SSL methods, especially when integrated
133 into multi-stage pipelines, is that the pre-trained feature extractors are often treated as fixed compo-
134 nents after initial pre-training. This limits their ability to fully adapt to the specific nuances of the
135 downstream task during supervised fine-tuning, potentially restricting their optimal discriminative
136 power for subtle precursor detection.

137 **Distillation-based Foundation Models.** More recently, distillation-based self-supervised learning,
138 exemplified by models like DINO [24], DINOV2 [25], and its latest iteration, DinoV3[26], has shown
139 immense promise. These models learn rich, dense, and highly transferable features from unlabeled
140 data through a teacher-student knowledge distillation framework. Unlike generative or contrastive
141 approaches, DINO-style models inherently produce robust attention maps and learn powerful rep-
142 resentations without relying on explicit masking strategies or complex data augmentations. This
143 paradigm offers a compelling direction for developing general-purpose encoders that can be more
144 seamlessly integrated and adapted within end-to-end learning frameworks, such as for the complex
145 task of ECG-based AF early warning.

146 3 Method

147 This section details our proposed end-to-end early warning framework for paroxysmal atrial fibrilla-
148 tion (PAF) using a DinoV3-based feature extractor. We outline the overall architecture, describe the
149 datasets utilized for training and evaluation, explain the model’s structure.

150 3.1 Overview of the Proposed Framework

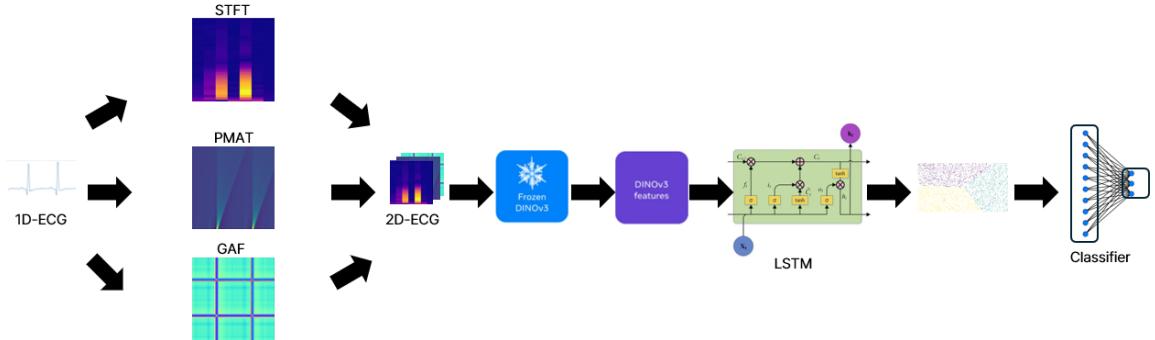


Figure 2: Overall Structure

151 Our goal is to evaluate whether a vision Foundation Model pre-trained on large-scale image data
152 (DinoV3) can provide robust, transferable representations for ECG state classification without ECG-
153 specific pretraining. The system is organized in two functional blocks for the current study: (1)
154 **Feature extraction** via a DinoV3 backbone adapted to 2D ECG patch representations (PMAT, STFT,
155 GAF), and (2) **Indicator (classification) head** — a temporal model (LSTM) and classifier that maps
156 sequences of extracted features to one of three ECG states (S0: normal, S1: precursor, S2: event).
157 While the overall architecture is designed to support future end-to-end fine-tuning and prospective
158 prediction, here we experimentally isolate and evaluate the classification-stage performance.

159 **3.2 Datasets**

160 We used publicly available long-term ECG datasets that are widely used in AF research to ensure
161 reproducibility and comparability.

- 162 • **PAF 2001 Dataset[27]:** This database was created for the Computers in Cardiology Chal-
163 lenge 2001 to facilitate the development of automated methods for predicting paroxysmal
164 atrial fibrillation (PAF). It comprises a learning set and a test set, each containing 50 record
165 sets from different subjects. Each record set includes two 30-minute, two-channel ECG
166 recordings. Notably, for subjects with PAF, one 30-minute record immediately precedes a
167 PAF episode, while the other is distant from any PAF activity. This structure is critical for
168 training models to distinguish between pre-PAF states and normal rhythm. The dataset also
169 includes corresponding 5-minute continuation records for verification and QRS annotations.
- 170 • **MIT-BIH Normal Sinus Rhythm (NSR) Database[28]:** This database consists of 18
171 long-term ECG recordings from subjects referred to Boston’s Beth Israel Hospital, who
172 were found to have no significant arrhythmias. It includes recordings from 5 men (aged 26
173 to 45) and 13 women (aged 20 to 50). This dataset provides valuable healthy control data,
174 essential for robustly training the model to recognize and distinguish normal cardiac activity
175 from pre-arrhythmic states.
- 176 • **IRIDIA-AF Database[29]:** This dataset comprises 167 Holter monitoring records from
177 152 patients with paroxysmal AF, collected from an outpatient cardiology clinic in Belgium
178 between 2006 and 2017. Records vary in length from 19 to 95 hours, divided into 24-
179 hour files, and are sampled at 200 Hz. All AF episodes were manually annotated and
180 reviewed by an expert cardiologist and a specialist cardiac nurse. This extensive and expertly
181 annotated dataset offers a rich resource for training and validating models for AF detection
182 and prediction, particularly in real-world long-term monitoring scenarios.

183 These datasets were preprocessed consistently (normalization, 128Hz resampling, noise reduction
184 filter) to produce training and evaluation sets for the indicator (classification) task.

185 **3.3 Model Structure**

186 Our early warning framework is designed with three main components that collaboratively extract
187 discriminative ECG features and capture states.

- 188 • **DinoV3-based Feature Extractor:** To enhance representation learning, we replace the
189 original MAE-based 1D Vision Transformer with DinoV3 as the backbone. Raw 1D ECG
190 signals are converted into multi-channel 2D representations using Progressive Moving Average
191 Transform (PMAT), Short-Time Fourier Transform (STFT), and Gramian Angular Field
192 (GAF). These representations are fed into DinoV3, a self-supervised vision transformer
193 pre-trained on large-scale image datasets. DinoV3 provides robust high-level semantic fea-
194 tures and interpretable attention maps, enabling the detection of subtle electrophysiological
195 variations related to arrhythmia onset.
- 196 • **LSTM-based Classification indicator Model:** An LSTM network processes the sequential
197 state indicators to model the temporal evolution of ECG states. By capturing long-range
198 dependencies, the LSTM effectively learns the progression pathway from stable rhythm (S0),
199 through precursor states (S1), to arrhythmic events (S2). This enables accurate classification
200 for impending arrhythmias.

201 This Two-state annotation is used solely to train and evaluate the classification (indicator) model in
202 this study; moving from accurate indicator classification to reliable prospective event prediction is
203 left to future work.

204 **3.4 ECG State Annotation**

205 Accurate labeling of sequential segments is critical for training the indicator model. We adopt a
206 sliding-window scheme with a 10-second window and 5-second stride; labels are assigned based on
207 the window endpoint relative to the annotated event onset T_{onset} .

- 208 • **Normal State (S0):** segments whose window endpoint lies more than 20 minutes before
 209 T_{onset} . These segments are considered to represent stable, baseline rhythm.
- 210 • **Precursor State (S1):** segments whose window endpoint falls within the 20-minute interval
 211 immediately preceding T_{onset} . These segments may contain subtle alterations that precede
 212 the AF episode.
- 213 • **Event State (S2):** segments whose window endpoint is at or after T_{onset} and which contain
 214 the arrhythmic event.

215 These states are meticulously annotated to serve as ground truth for training the LSTM-based indicator
 216 model, enabling it to recognize and classify the ECG state of individual segments. In the future, the
 217 warning model utilizes these classifications to identify the critical transition pathways from S0 to S1
 218 and ultimately to S2.

219 4 Experiments

220 This section presents the experimental setup and results for evaluating the classification performance
 221 of the DinoV3-based indicator model. Our primary goal is to demonstrate the effectiveness of using
 222 DinoV3 as the feature extractor.

223 4.1 Evaluation of Indicator Model Classification Performance

224 We compare the DinoV3-based indicator model against representative baselines, including classical
 225 deep ECG classifiers and recent SSL-enhanced pipelines adapted to ECG.

Model	Acc	Spe	Sen	F1
FCN _{wang} [30]	0.6124	0.7567	0.5944	0.5673
ConvNeXt[31]	0.4967	0.6667	0.3333	0.2212
ViT1D[32]	0.5325	0.7169	0.3968	0.1541
Trs[9]	0.5900	0.7561	0.6416	0.6208
DinoV3 (Proposed)	0.5950	0.7479	0.5368	0.5489

Table 1: Comparison of classification performance by changing feature extractor

226 Table 1 illustrates the classification performance for the paroxysmal Atrial fibrillation event (PAF).
 227 When trained for classification, the DinoV3-based indicator model achieves competitive results across
 228 all metrics (Acc, Spe, Sen, MCC, F1) compared to other baselines, including traditional ECG classi-
 229 fication models and contrastive learning models. This demonstrates that DinoV3 exhibits enhanced
 230 capabilities in extracting discriminative features for ECG state recognition even without the ECG
 231 dataset fine tuning, thereby establishing a robust foundation for the subsequent warning model.
 232 These results suggest that DinoV3’s powerful feature extraction abilities can effectively contribute to
 233 detecting various ECG abnormalities.

234 5 Discussion and Limitations

235 In this study we evaluated the utility of a publicly available Foundation Model (DinoV3) — pretrained
 236 on large-scale image data and applied *without* ECG-specific pretraining — as a feature extractor
 237 for an ECG-state **classification** (indicator) model targeting paroxysmal atrial fibrillation (PAF). Our
 238 principal finding is that DinoV3-derived representations, when applied to 2D ECG patch transforms
 239 (PMAT, STFT, GAF) and coupled with a temporal classification head (LSTM), yield competitive
 240 indicator-stage performance (Table 1). This result highlights notable cross-domain transferability:
 241 visual representations learned at scale retain structure that can be exploited for biological time-series
 242 classification, at least at the upstream classification (indicator) level.

243 Crucially, we reiterate that the present work focuses on the **classification/indicator stage** — i.e.,
 244 recognizing and distinguishing ECG segments that are normal (S0), precursor (S1), or event (S2).
 245 We did not perform prospective time-to-event prediction experiments in this manuscript. Translating
 246 accurate indicator classification into reliable early-warning or prediction requires additional modeling

247 choices (e.g., explicit temporal forecasting, survival analysis, calibration over time) and rigorous
248 temporal validation; these steps are outside the scope of the current paper and are discussed below as
249 future directions.

250 Despite promising indicator-stage results, there are important limitations:

- 251 • **No ECG-specific pretraining in main experiments.** The DinoV3 backbone was used
252 primarily in its publicly released image-pretrained form. While this allowed us to probe
253 cross-domain transferability, we expect that ECG-specific pretraining and/or systematic
254 fine-tuning would further improve discriminative power for precursor patterns.
- 255 • **Classification vs. predictive utility.** Strong performance on S0/S1/S2 classification does
256 not automatically imply robust prospective prediction of PAF onset. Predictive performance
257 must be evaluated under temporal holdout schemes that respect event timing, and with
258 metrics appropriate for forecasting (e.g., lead-time distribution, time-dependent AUROC,
259 calibration of predicted risk).
- 260 • **Dataset diversity and generalization.** Public long-term ECG datasets with high-quality,
261 temporally precise annotations for precursor intervals are limited. Broader external val-
262 idation across multiple cohorts, devices, and recording conditions is necessary to assess
263 generalizability and to avoid dataset-specific biases.
- 264 • **Clinical validation and interpretability.** Although DinoV3 attention maps provide patch-
265 level saliency that may aid interpretability, these visualizations require formal evaluation by
266 clinicians to determine clinical relevance and to avoid misleading explanations. Human-in-
267 the-loop validation and prospective pilot studies are needed before clinical deployment.

268 Based on the above, we identify concrete next steps to bridge the gap between the present indicator-
269 stage findings and clinically useful predictive systems:

- 270 1. **ECG-specific fine-tuning and ablation studies:** systematically fine-tune DinoV3 on large
271 ECG corpora, compare frozen vs. partially fine-tuned vs. fully end-to-end settings, and
272 report corresponding gains in indicator and (eventually) prediction metrics.
- 273 2. **Temporal/predictive modeling:** extend the pipeline to explicit time-to-event or sequence-
274 forecasting models and evaluate under temporally strict validation (e.g., by-record or by-
275 patient splits, prospective simulation).
- 276 3. **External and prospective validation:** test on heterogeneous external datasets and, where
277 possible, conduct prospective pilot evaluations to measure real-world utility, false alarm
278 rates, and clinician acceptance.
- 279 4. **Clinician-centered interpretability studies:** present attention/saliency maps and decision
280 traces to expert cardiologists for qualitative and quantitative assessment.
- 281 5. **Robustness and calibration:** evaluate model calibration over lead time and implement
282 uncertainty-aware decision thresholds suitable for clinical workflows.

283 Taken together, the current results establish a promising proof-of-concept: Foundation Models can
284 serve as effective upstream feature extractors for the *classification* stage in AF early-warning pipelines,
285 but additional work (fine-tuning, temporal prediction modeling, and clinical validation) is required to
286 realize reliable prospective warning systems.

287 6 Conclusion

288 We investigated the feasibility of using a vision Foundation Model (DinoV3) as a feature extractor
289 for an ECG-state classification (indicator) model relevant to paroxysmal atrial fibrillation (PAF).
290 By converting ECG signals into 2D patch-based representations and coupling DinoV3 embeddings
291 with a temporal LSTM classifier, we demonstrated competitive indicator-stage performance despite
292 using DinoV3 without ECG-specific pretraining. These findings indicate meaningful cross-domain
293 transferability and position Foundation Models as a viable starting point for building upstream
294 components of AF early-warning systems.

295 It is important to emphasize the scope of this work: the experiments target the **classification**
296 (**indicator**) stage that precedes prospective prediction. We do not claim to have developed a validated

297 predictive early-warning system in this manuscript. Rather, our contribution is to show that (1)
298 Foundation Models can yield useful representations for ECG-state discrimination without domain-
299 specific pretraining, and (2) these representations provide a strong foundation for subsequent work
300 on fine-tuning, end-to-end optimization, and time-to-event prediction.

301 Future work will prioritize systematic ECG fine-tuning of the backbone, extension to explicit predic-
302 tive modeling with temporally rigorous evaluation, comprehensive external validation, and clinician-
303 in-the-loop interpretability studies. Addressing these steps is essential to translate the present
304 proof-of-concept into clinically actionable early-warning tools that improve patient outcomes.

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388 **Agents4Science AI Involvement Checklist**

389 This checklist is designed to allow you to explain the role of AI in your research. This is important for
390 understanding broadly how researchers use AI and how this impacts the quality and characteristics
391 of the research. **Do not remove the checklist! Papers not including the checklist will be desk**
392 **rejected.** You will give a score for each of the categories that define the role of AI in each part of the
393 scientific process. The scores are as follows:

- 394 • **[A] Human-generated:** Humans generated 95% or more of the research, with AI being of
395 minimal involvement.
396 • **[B] Mostly human, assisted by AI:** The research was a collaboration between humans and
397 AI models, but humans produced the majority (>50%) of the research.
398 • **[C] Mostly AI, assisted by human:** The research task was a collaboration between humans
399 and AI models, but AI produced the majority (>50%) of the research.
400 • **[D] AI-generated:** AI performed over 95% of the research. This may involve minimal
401 human involvement, such as prompting or high-level guidance during the research process,
402 but the majority of the ideas and work came from the AI.

403 These categories leave room for interpretation, so we ask that the authors also include a brief
404 explanation elaborating on how AI was involved in the tasks for each category. Please keep your
405 explanation to less than 150 words.

406 **IMPORTANT,** please:

- 407 • **Delete this instruction block, but keep the section heading “Agents4Science AI Involve-**
408 **ment Checklist”,**
409 • **Keep the checklist subsection headings, questions/answers and guidelines below.**
410 • **Do not modify the questions and only use the provided macros for your answers.**

411 1. **Hypothesis development:** Hypothesis development includes the process by which you
412 came to explore this research topic and research question. This can involve the background
413 research performed by either researchers or by AI. This can also involve whether the idea
414 was proposed by researchers or by AI.

415 Answer: **[TODO]** [B]

416 Explanation: **[TODO]** AI informed trend analysis, but the research direction and core ideas
417 were proposed by the researcher

418 2. **Experimental design and implementation:** This category includes design of experiments
419 that are used to test the hypotheses, coding and implementation of computational methods,
420 and the execution of these experiments.

421 Answer: **[TODO]** [C]

422 Explanation: **[TODO]** Researcher designs experiments; AI handles coding and execution,
423 with researcher refining errors or logic gaps.

424 3. **Analysis of data and interpretation of results:** This category encompasses any process to
425 organize and process data for the experiments in the paper. It also includes interpretations of
426 the results of the study.

427 Answer: **[TODO]** [C]

428 Explanation: **[TODO]** Researcher designs experiments; AI handles coding and execution,
429 with researcher refining errors or logic gaps.

430 4. **Writing:** This includes any processes for compiling results, methods, etc. into the final
431 paper form. This can involve not only writing of the main text but also figure-making,
432 improving layout of the manuscript, and formulation of narrative.

433 Answer: **[TODO]** [D]

434 Explanation: **[TODO]** AI drafted the overall framework; I manually revised the logical flow
435 and experimental-result interpretations to correct overinterpretation.

- 436 5. **Observed AI Limitations:** What limitations have you found when using AI as a partner or
437 lead author?
438 Description: [TODO] AI often risks overinterpretation in experiments and lacks creativity
439 in topic selection, yet proves useful when merging diverse fields.

440 **Agents4Science Paper Checklist**

441 **1. Claims**

442 Question: Do the main claims made in the abstract and introduction accurately reflect the
443 paper's contributions and scope?

444 Answer: [Yes]

445 Justification: [TODO]That's generally correct.

446 Guidelines:

- 447 • The answer NA means that the abstract and introduction do not include the claims
448 made in the paper.
- 449 • The abstract and/or introduction should clearly state the claims made, including the
450 contributions made in the paper and important assumptions and limitations. A No or
451 NA answer to this question will not be perceived well by the reviewers.
- 452 • The claims made should match theoretical and experimental results, and reflect how
453 much the results can be expected to generalize to other settings.
- 454 • It is fine to include aspirational goals as motivation as long as it is clear that these goals
455 are not attained by the paper.

456 **2. Limitations**

457 Question: Does the paper discuss the limitations of the work performed by the authors?

458 Answer: [Yes]

459 Justification: [TODO]The discussion mentions future directions but does not address
460 limitations related to AI itself, such as computational efficiency.

461 Guidelines:

- 462 • The answer NA means that the paper has no limitation while the answer No means that
463 the paper has limitations, but those are not discussed in the paper.
- 464 • The authors are encouraged to create a separate "Limitations" section in their paper.
- 465 • The paper should point out any strong assumptions and how robust the results are to
466 violations of these assumptions (e.g., independence assumptions, noiseless settings,
467 model well-specification, asymptotic approximations only holding locally). The authors
468 should reflect on how these assumptions might be violated in practice and what the
469 implications would be.
- 470 • The authors should reflect on the scope of the claims made, e.g., if the approach was
471 only tested on a few datasets or with a few runs. In general, empirical results often
472 depend on implicit assumptions, which should be articulated.
- 473 • The authors should reflect on the factors that influence the performance of the approach.
474 For example, a facial recognition algorithm may perform poorly when image resolution
475 is low or images are taken in low lighting.
- 476 • The authors should discuss the computational efficiency of the proposed algorithms
477 and how they scale with dataset size.
- 478 • If applicable, the authors should discuss possible limitations of their approach to
479 address problems of privacy and fairness.
- 480 • While the authors might fear that complete honesty about limitations might be used by
481 reviewers as grounds for rejection, a worse outcome might be that reviewers discover
482 limitations that aren't acknowledged in the paper. Reviewers will be specifically
483 instructed to not penalize honesty concerning limitations.

484 **3. Theory assumptions and proofs**

485 Question: For each theoretical result, does the paper provide the full set of assumptions and
486 a complete (and correct) proof?

487 Answer: [NA]

488 Justification: [TODO]It does not contain any theoretical assumptions. Therefore, the answer
489 is marked as NA.

490 Guidelines:

- 491 • The answer NA means that the paper does not include theoretical results.
 492 • All the theorems, formulas, and proofs in the paper should be numbered and cross-
 493 referenced.
 494 • All assumptions should be clearly stated or referenced in the statement of any theorems.
 495 • The proofs can either appear in the main paper or the supplemental material, but if
 496 they appear in the supplemental material, the authors are encouraged to provide a short
 497 proof sketch to provide intuition.

498 **4. Experimental result reproducibility**

499 Question: Does the paper fully disclose all the information needed to reproduce the main ex-
 500 perimental results of the paper to the extent that it affects the main claims and/or conclusions
 501 of the paper (regardless of whether the code and data are provided or not)?

502 Answer: [Yes]

503 Justification: [TODO]This is entirely feasible simply because we used publicly available
 504 models, data and weights.

505 Guidelines:

- 506 • The answer NA means that the paper does not include experiments.
 507 • If the paper includes experiments, a No answer to this question will not be perceived
 508 well by the reviewers: Making the paper reproducible is important.
 509 • If the contribution is a dataset and/or model, the authors should describe the steps taken
 510 to make their results reproducible or verifiable.
 511 • We recognize that reproducibility may be tricky in some cases, in which case authors
 512 are welcome to describe the particular way they provide for reproducibility. In the case
 513 of closed-source models, it may be that access to the model is limited in some way
 514 (e.g., to registered users), but it should be possible for other researchers to have some
 515 path to reproducing or verifying the results.

516 **5. Open access to data and code**

517 Question: Does the paper provide open access to the data and code, with sufficient instruc-
 518 tions to faithfully reproduce the main experimental results, as described in supplemental
 519 material?

520 Answer: [Yes]

521 Justification: [TODO]This is entirely feasible simply because we used publicly available
 522 models, data and weights.

523 Guidelines:

- 524 • The answer NA means that paper does not include experiments requiring code.
 525 • Please see the Agents4Science code and data submission guidelines on the conference
 526 website for more details.
 527 • While we encourage the release of code and data, we understand that this might not be
 528 possible, so “No” is an acceptable answer. Papers cannot be rejected simply for not
 529 including code, unless this is central to the contribution (e.g., for a new open-source
 530 benchmark).
 531 • The instructions should contain the exact command and environment needed to run to
 532 reproduce the results.
 533 • At submission time, to preserve anonymity, the authors should release anonymized
 534 versions (if applicable).

535 **6. Experimental setting/details**

536 Question: Does the paper specify all the training and test details (e.g., data splits, hyper-
 537 parameters, how they were chosen, type of optimizer, etc.) necessary to understand the
 538 results?

539 Answer: [Yes]

540 Justification: [TODO]The training procedure follows the same details as in Reference 9,
 541 making it fully implementable.

542 Guidelines:

- 543 • The answer NA means that the paper does not include experiments.
544 • The experimental setting should be presented in the core of the paper to a level of detail
545 that is necessary to appreciate the results and make sense of them.
546 • The full details can be provided either with the code, in appendix, or as supplemental
547 material.

548 **7. Experiment statistical significance**

549 Question: Does the paper report error bars suitably and correctly defined or other appropriate
550 information about the statistical significance of the experiments?

551 Answer: [No]

552 Justification: [TODO]This paper focuses solely on the results of the Foundation Model and
553 does not discuss those details.

554 Guidelines:

- 555 • The answer NA means that the paper does not include experiments.
556 • The authors should answer "Yes" if the results are accompanied by error bars, confi-
557 dence intervals, or statistical significance tests, at least for the experiments that support
558 the main claims of the paper.
559 • The factors of variability that the error bars are capturing should be clearly stated
560 (for example, train/test split, initialization, or overall run with given experimental
561 conditions).

562 **8. Experiments compute resources**

563 Question: For each experiment, does the paper provide sufficient information on the com-
564 puter resources (type of compute workers, memory, time of execution) needed to reproduce
565 the experiments?

566 Answer: [No]

567 Justification: [TODO]Reference 9 occupies about 1–2 GB of VRAM, and since Dino's
568 model size is adjustable, we deemed it unnecessary to specify.

569 Guidelines:

- 570 • The answer NA means that the paper does not include experiments.
571 • The paper should indicate the type of compute workers CPU or GPU, internal cluster,
572 or cloud provider, including relevant memory and storage.
573 • The paper should provide the amount of compute required for each of the individual
574 experimental runs as well as estimate the total compute.

575 **9. Code of ethics**

576 Question: Does the research conducted in the paper conform, in every respect, with the
577 Agents4Science Code of Ethics (see conference website)?

578 Answer: [Yes]

579 Justification: [TODO]Yes

580 Guidelines:

- 581 • The answer NA means that the authors have not reviewed the Agents4Science Code of
582 Ethics.
583 • If the authors answer No, they should explain the special circumstances that require a
584 deviation from the Code of Ethics.

585 **10. Broader impacts**

586 Question: Does the paper discuss both potential positive societal impacts and negative
587 societal impacts of the work performed?

588 Answer: [No]

589 Justification: [TODO]The paper only presents an optimistic outlook, suggesting that a future
590 prediction model could be developed and applied meaningfully in clinical practice.

591 Guidelines:

- 592 • The answer NA means that there is no societal impact of the work performed.
593 • If the authors answer NA or No, they should explain why their work has no societal
594 impact or why the paper does not address societal impact.
595 • Examples of negative societal impacts include potential malicious or unintended uses
596 (e.g., disinformation, generating fake profiles, surveillance), fairness considerations,
597 privacy considerations, and security considerations.
598 • If there are negative societal impacts, the authors could also discuss possible mitigation
599 strategies.