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Brain Tractography Registration with Nonrigid ICP

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ABSTRACT

The registration problem (also known as alignment, absolute orientation) is one of the outstanding and very basic problems in computer vision. In this problem, two or more datasets of points are given and the task is to optimally align them by estimating a best transformation (combination of translation, rotation and scaling). Due to its fundamental importance, it arises as a subtask in many different applications (e.g., object recognition, tracking, range data fusion, graphics, medical image alignment, robotics and structural bioinformatics etc [5]).

In This thesis we implement the method mentioned in [1], we show how to extend the ICP framework to nonrigid registration, while retaining the convergence properties of the original algorithm. The resulting optimal step nonrigid ICP framework allows the use of different regularisations, as long as they have an adjustable stiffness parameter. The registration loops over a series of decreasing stiffness weights, and incrementally deforms the template towards the target, recovering the whole range of global and local deformations. To find the optimal deformation for a given stiffness, optimal iterative closest point steps are used. Preliminary correspondences are estimated by a nearestpoint search. Then the optimal deformation of the template for these fixed correspondences and the active stiffness is calculated. Afterwards the process continues with new correspondences found by searching from the displaced template vertices. We present an algorithm using a locally affine regularisation which assigns an affine transformation to each vertex and minimises the difference in the transformation of neighbouring vertices. It is shown that for this regularisation the optimal deformation for fixed correspondences and fixed stiffness can be determined exactly and efficiently. The method succeeds for a wide range of initial conditions, and handles missing data robustly. It is compared qualitatively and quantitatively to other algorithms using synthetic examples and real world data [1].

INTRODUCTION



Figure 1: The Human Brain Fiber Pathway

1 BRAIN STRUCTURE (FIBER PATHWAYS)

Human brain which is our focus in this thesis, is the central organ of the human nervous system, it is made up of two main components, gray matter and white matter. Scientists have learned a lot about gray and white matter and the two halves of the brain through autopsies and imaging techniques and by studying diseases or conditions associated with brain damage.

The thesis focused on **White Matter** which is refers to areas of the central nervous system that are mainly made up of myelinated axons, also called tracts

or fiber pathways [6]. It is composed of bundles, which connect various gray matter areas of the brain to each other, and carry nerve impulses between neurons. Myelin acts as an insulator, which allows electrical signals to jump, rather than coursing through the axon, increasing the speed of transmission of all nerve signals [7].

Long thought to be passive tissue, white matter affects learning and brain functions, modulating the distribution of action potentials, acting as a relay and coordinating communication between different brain regions [8].

The Human Brain consists of these tracts bundles in left and right side:

- Anterior Thalamic Radiation (ATR)
- Corpus Callosum (CC)
- Genu of the Corpus Callosum (genu)
- Splenium of the Corpus Callosum (splenium)
- Body of Corpus Callosum (truncus)
- Body of Corpus Callosum (truncus)
- Cingulum (Cing)
- Corticospinal Tract (CST)
- Inferior Fronto-occipital Fasciculus (IFO)
- Inferior Longitudinal Fasciculus (ILF)
- Superior Longitudinal Fasciculus (SLF)
- Ventral Tegmental Area (VTA)

Thalamic Radiation (ATR) refers to fiber pathways that connect the anterior nuclear group of the thalamus and the midline nuclear group of the thalamus with the frontal lobe through the anterior thalamic peduncle, the anterior limb of the internal capsule and other parts of the cerebral white matter [9][10]. ATR abnormalities have a possible link with cognitive abnormalities and negative symptoms in schizophrenia[11].

Corpus Callosum (CC) is a wide, flat bundle of nerve fibers, located at the longitudinal fissure beneath the cortex, which acts as a link between the two hemispheres of the brain and facilitates communication between them. The term corpus callosum means 'tough body' in Latin. With approximately 200 - 250 million contralateral axonal projections to its credit, it is the largest among the various white matter structures in the central nervous system. The anterior portion of this structure is called 'genu', while the posterior structure is called 'splenium'. In between its anterior and posterior portions, lies the 'truncus' or its 'body'. Studies have revealed that the anterior of corpus callosum in left-handed people is eleven percent (100%) larger than that of right-handed people [12].

Genu of the Corpus Callosum (genu) refers to the rostral most portion of the corpus callosum. It is bounded caudally by the body of the corpus callosum and ventrocaudally by the rostrum of the corpus callosum [9].

Splenium of the Corpus Callosum (splenium) refers to the caudal most portion of the corpus callosum. It is bounded rostrally by the body of the corpus callosum [9]. It overlaps the tela chorioidea of the third ventricle and the mid-brain, and ends in a thick, convex, free border. A sagittal section of the splenium shows that the posterior end of the corpus callosum is acutely bent forward, the upper and lower parts being applied to each other [12].

Body of Corpus Callosum (truncus) refers to the portion of the corpus callosum located between the genu of the corpus callosum and the splenium of the corpus callosum. In a common parcellation, corpus callosum, it is divided into four parts: the rostral body of the corpus callosum, the anterior midbody of the corpus callosum, the posterior midbody of the corpus callosum and the isthmus of the corpus callosum [9]. **Cingulum (Cing)** refers to a fiber pathway that runs longitudinally in the cingulate white matter; it connects portions of the cingulate gyrus, the parietal lobe and the prefrontal cortex with the parahippocampal gyrus and adjacent structures of the temporal lobe. "All connectives entering and exiting the cingulate gyrus pass through the cingulum bundle". It is composed of the Cingulum ammonale and the Cingulum limitans [9].

Cingulum receives afferent fibers from the parts of the thalamus that are associated with the spinothalamic tract. This, in addition to the fact that the cingulum is a central structure in learning to correct mistakes, indicates that the cingulum is involved in appraisal of pain and reinforcement of behavior that reduces it [13]. The cingulum is described from various brain images as a C shaped structure within the brain that wraps around the frontal lobe to the temporal lobe right above the corpus callosum. It is located beneath the cingulate gyrus within the medial surface of the brain therefore encircling the entire brain. There are two primary parts of the cingulate cortex, as is typical with most brain structures. There is the posterior cingulate and anterior cingulate. The anterior is linked to emotion, especially apathy and depression. Here function and structure changes are related meaning any change within this structure would lead to a function change, particularly behavioral because of its function involving emotions. Damage to this area can have various effects on mental disorders and mental health. The posterior section is more related to cognitive functions. This can include attention, visual and spatial skills, working memory and general memory. Because of its location, the cingulum is very important to brain structure connectivity and the integration of information that it receives [14].

Corticospinal Tract (CST) refers to a fiber pathway from the cerebral cortex to the spinal cord. Its fibers originate from pyramidal neurons of the precentral gyrus, and on their way to the spinal cord, they pass through parts of the cerebral white matter (including the posterior limb of the internal capsule),

the crus cerebri, the longitudinal pontine fibers, the pyramid of the medulla (where they are known as the pyramidal tract) and the pyramidal decussation. In the decussation, some fibers cross to the other side of the brainstem to form the lateral corticospinal tract. Those fibers that do not cross split to form the anterolateral corticospinal tract and the anterior corticospinal tract [9].

Fornix (Fornix) The fornix (Latin, "vault" or "arch") is a C-shaped bundle of fibers (axons) in the brain, and carries signals from the hippocampus to the hypothalamus. The fibres begin in the hippocampus on each side of the brain (where they are also known as the fimbria); the separate left and right sides are each called the crus of the fornix. The bundles of fibres come together in the midline of the brain, forming the body of the fornix. The inferior edge of the septum pellucidum (a membrane that separates the two lateral ventricles) is attached to the upper face of the fornix body. The body of the fornix travels anteriorly and divides again near the anterior commissure. The left and right parts separate, but there is also an anterior/posterior divergence. The posterior fibres (called the postcommissural fornix) of each side continue through the hypothalamus to the mammillary bodies; then to the anterior nuclei of thalamus, which project to the cingulate cortex. The anterior fibers (precommissural fornix) end at the septal nuclei and nucleus accumbens of each half of the brain [12].

While its exact function and importance in the physiology of the brain are still not entirely clear, it has been demonstrated that surgical transection – the cutting of the fornix along its body – can cause memory loss [15]. There is some debate over what type of memory is affected by this damage, but it has been found to most closely correlate with recall memory rather than recognition memory. This means that damage to the fornix can cause difficulty in recalling long-term information such as details of past events, but it has little effect on the ability to recognize objects or familiar situations [15].

Inferior Fronto-occipital Fasciculus (IFO) The occipitofrontal fasciculus passes backward from the frontal lobe, along the lateral border of the caudate nucleus, and on the medial aspect of the corona radiata; its fibers radiate in a fan-like manner and pass into the occipital and temporal lobes lateral to the posterior and inferior cornua [12].

Inferior Longitudinal Fasciculus (ILF) The inferior longitudinal fasciculus connects the temporal lobe and occipital lobe, running along the lateral walls of the inferior and posterior cornua of the lateral ventricle. The existence of this fasciculus independent from the occipitotemporal fasciculus has been questioned for the human being, such that it has been proposed that the term inferior longitudinal fasciculus be replaced by the term "occipitotemporal projection" [12].

Superior Longitudinal Fasciculus (SLF) refers to a fiber pathway in the cerebral white matter. It is composed of fibers that connect the cortex of the frontal lobe

with cortex of the occipital lobe and the temporal lobe. Some authors refer to the connection with the temporal lobe as the arcuate fasciculus [9].

is a pair of long bi-directional bundles of neurons connecting the front and the back of the cerebrum. Each association fiber bundle is lateral to the centrum ovale of a cerebral hemisphere and connects the frontal, occipital, parietal, and temporal lobes. The neurons pass from the frontal lobe through the operculum to the posterior end of the lateral sulcus where numerous neurons radiate into the occipital lobe and other neurons turn downward and forward around the putamen and radiate to anterior portions of the temporal lobe [12].

Ventral Tegmental Area (VTA) The VTA is one of the two major dopaminergic areas in the brain (the other being the substantia nigra). Although there is not a very clear anatomical separation between the VTA and substantia nigra, the areas do seem to differ slightly in where most of their neurons project to.

VTA is in the midbrain, situated adjacent to the substantia nigra. Although it contains several different types of neurons, it is primarily characterized by its dopaminergic neurons, which project from the VTA throughout the brain.

The VTA is considered an integral part of a network of structures, together known as the reward system, that are involved in reinforcing behavior.

The largest bundle of fibers leaving the substantia nigra, known as the nigrostriatal pathway, projects to the caudate and putamen (together known as the striatum). There are several major efferents that project from the VTA; two of the most prominent are the mesolimbic and mesocortical pathways, which travel to limbic and cortical areas, respectively.

The variation in the destination of their efferents leads to a divergence in the functions attributed to the VTA and substantia nigra. While the substantia nigra is primarily associated with movement, the VTA is thought to be involved with various cognitive and emotional processes. The functions associated with the VTA are diverse, but it is probably best known for the major role it seems to play in motivation, reward, and addiction [16].

When someone uses a drug of abuse, or attains some otherwise rewarding stimulus, dopamine levels typically rise in the nucleus accumbens, a structure found in the basal forebrain that is an important part of the reward system. The primary source of dopamine in the nucleus accumbens is neurons that project from the VTA and travel in the mesolimbic pathway. Thus, the VTA is also activated when one experiences something rewarding, and this integral role in the mediation of rewarding experiences has caused some to propose that activity in the VTA may be necessary to the development of addiction.

Dopamine is also important to normal cognition and so it is not surprising that the VTA has been implicated in the pathophysiology of disorders other than addiction. For example, dopaminergic neurons in the VTA have been proposed to play a role in schizophrenia, a disorder that is thought by some to be associated with high levels of dopamine. Alternatively, attention-deficit

hyperactivity disorder (ADHD) has been linked to low dopamine activity in the VTA. In truth, the dopaminergic projections from the VTA are so extensive that they are likely involved to some degree in a wide variety of normal and pathological behavior, but it is still not very clear exactly what role they play in most cognitive processes—both normal and disordered. It does seem clear, however, that due to the importance of dopamine signaling throughout the brain and the widespread dopaminergic projections of the VTA, the integrity of the VTA is crucial to proper brain function [16].

2 REGISTRATION

The registration problem (also known as alignment, absolute orientation) is one of the outstanding and very basic problems in computer vision. In this problem, two or more datasets of points are given and the task is to optimally align them by estimating a best transformation (combination of translation, rotation and scaling). Due to its fundamental importance, it arises as a subtask in many different applications (e.g., object recognition, tracking, range data fusion, graphics, medical image alignment, robotics and structural bioinformatics ... etc) [5].

2.1 *Iterative closest point (ICP)*

ICP, which is an algorithm employed to minimize the distance between two or more points clouds, is one of the widely used algorithms in aligning three dimensional models given an initial guess of the rigid body transformation required [17]. In ICP (in our case) one points cloud (vertex cloud), the reference, or target, is kept fixed, while the other one, the source, is transformed to best match the reference. The algorithm iteratively revises the transformation (combination of translation, rotation and scaling) needed to minimize a distance from the source to the reference points cloud.

3 PCA TRANSFORMATION

PCA is mathematically defined as an orthogonal linear transformation that transforms the data to a new coordinate system such that the greatest variance by some projection of the data comes to lie on the first coordinate (called the first principal component), the second greatest variance on the second coordinate, and so on [18]. PCA is used in the code as a preliminary step, so that the template and target are aligned as much as possible before the registration can begin.

4 LEAST SQUARES (LSQR)

LSQR is iterative method for solving $Ax = b$ and $\min ||Ax - b||^2$, where the matrix A is large and sparse. The method is based on the bidiagonalization procedure of Golub and Kahan. It is analytically equivalent to the standard method of conjugate gradients, but possesses more favorable numerical properties [19]. It is used in this thesis to solve the cost function which we will discuss in the next chapter in details.

METHOD

1 THE ICP FRAMEWORK

The main subject of this thesis is demonstrating how the ICP framework can be extended to nonrigid registration, whilst retaining the convergence properties of the original algorithm. The principle idea is the application of the work presented in [1]. The resulting optimal step nonrigid ICP framework allows for the use of different regularisations, as long as they have an adjustable stiffness parameter. The registration loops over a series of decreasing stiffness weights and incrementally deforms the template towards the target, recovering the whole range of global and local deformations. To find the optimal deformation for a given stiffness, optimal iterative closest point steps are used. Preliminary correspondences are estimated by a nearest point search. Subsequently, the optimal deformation of the template for these fixed correspondences and the active stiffness is calculated. Afterwards, the process continues with new correspondences found by searching from the displaced template vertices. We present an algorithm using a locally affine regularisation which assigns an affine transformation to each vertex and minimises the difference in the transformation of neighbouring vertices. It is shown that for this regularisation, the optimal deformation for fixed correspondences and fixed stiffness can be determined exactly and efficiently. The method is successful for a wide range of initial conditions, and handles missing data robustly. Furthermore, it is compared qualitatively and quantitatively to other algorithms using synthetic examples and real world data.

As has been defined in the introduction, vertex registration is a problem in which two or more datasets of points are given and the task is to optimally align them by estimating a best transformation. In our case, we use a dense registration method to find a mapping from each point in the template onto the target while sparse methods find correspondence only for selected feature points. This is done by deforming the template, locally moving it closer in each iteration to the target in order to wrap them together with respect to stiffness. ICP moves the template S towards the target T step by step. In each iteration, it minimizes the difference between the template S and the target, T as illustrated in figure {2}, to reach the minimal value by solving the main equation (1):

$$||Ax - b||^2 \quad (1)$$

In equation (1) x is a list of X_i , each X_i is a 3×4 affine matrix which uses homogeneous coordinates $[x, y, z, 1]$ in 3D Euclidean space. By stacking X_i together we get $4n \times 3$ matrix x as shown in equation (2):

$$X = [X_1, X_2, \dots, X_n]^T \quad (2)$$

If we were to simply solve the equation (1) by assigning A as the template and b as the target, we will get exactly $Ax = b$, which means the difference between them is zero. That leads to the deforming of A and a complete loss of its shape, therefore, we need to add the stiffness part to the equation that will prevent this deformation by keeping the vertices originally as close to each other as possible which we will later explain in this chapter.

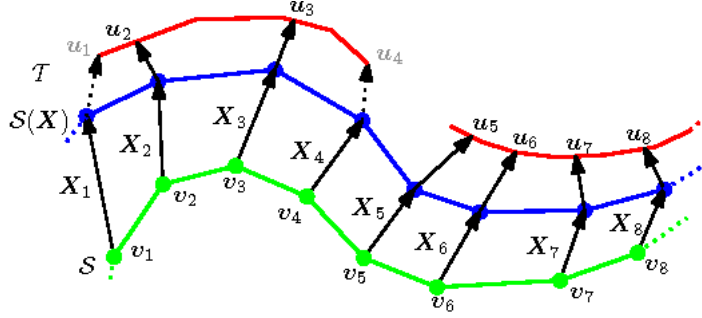


Figure 2: The template graph S (green) is deformed by locally affine transformations (X_i) onto the target graph T (red). The algorithm determines closest points (u_i) for each displaced source vertex ($X_i v_i$) and finds the optimal deformation for the stiffness used in this iteration. This is repeated until a stable state is found. The process then continues with a lower stiffness. Due to the stiffness constraint the vertices do not move directly towards the target graph, but may move parallel along it. The correspondences u_1 and u_4 are dropped as they lie on the border of the target [1].

2 SETUP DATA

The method presented in [1] deals with graph representations of the data $S = (V, E)$ where S , V and E are assigned to graph, vertices and edges, respectively. As described in the introduction, our data contains human brain fiber bundles (pathways) saved in a *ply* data format, as shown in the simplified figure {3}. The *ply* format consists of three parts; the first, uppermost part is the header of the file which contains the file description (i.e. format, comment, etc) and the major components of the header element parts which describe how many elements each part has. In the sample in figure {3}, there are 69283 vertices in x, y, z and 603 fibers. The second part of the *ply* files contains vertices in 3D Euclidean coordinate space while the last part of the *ply* file represents the end

index of each fiber. As the method in [1] require the template to be in graph format, we develop a tool to read *ply* files into a numpy array of arrays which can subsequently be used as a graph. To be able to use *numpy ndarray* as a graph, we put each tract in a separate array with respect to the link between points (Edges E). To do so, we put each point linked together next to each other, and then wrap all the tracts belonging to the same bundle (i.e ATR, CC, genu, splenium, etc) in a new *numpy ndarray*.

```
ply
format ascii 1.0
comment DTI Tractography, produced by fiber-track
element vertices 69283
property float x
property float y
property float z
element fiber 603
property int endindex
end_header
-4.71338558197 -19.9100589752 4.76097154617
-4.73113059998 -19.3581771851 4.68979740143
-4.72901630402 -18.8120174408 4.5764541626
-4.79067516327 -18.2503032684 4.52395439148
.....
152
299
364
494
637
767
```

Figure 3: Simplified *ply* file sample

3 PREPARATION STEPS

After we read the data in graph format, we must align the template graph to the target graph as closely as possible. In order to do so, we use *Principal Components Analysis (PCA)*. Before applying PCA, we scale the template graph and the target graph to a $[0, 1]$ scale to match each other. This is done by subtracting all points from the minimum value in the graph and then dividing them by the maximum value in the graph. Next, we apply PCA and use $[-1, 1]^3$ cube combination and measure the distance between each point in the template graph to the closest point in the target graph $\sum ||v_i - v_j||_F^2$ where $v_i \in S, v_j \in T$ eight times to select the combination with the minimum distance as is illustrated in table {1}.

1	2	3	4	5	6	7	8
(x,y,z)	(x,y,-z)	(x,-y,z)	(x,-y,-z)	(-x,-y,z)	(-x,y,-z)	(-x,y,z)	(-x,-y,-z)

Table 1: $[-1, 1]^3$ cube combination

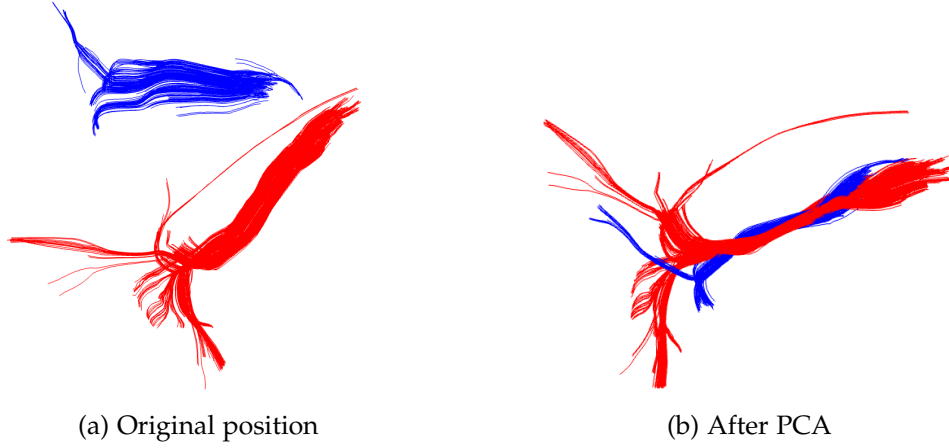


Figure 4: PCA alignment

4 DISTANCE MEASUREMENT

In all process in our code we use K-D tree (or k-dimensional) to measure the euclidean distance between the points, either on PCA transformation, ICP or any where we measure the distance.

4.1 The K-D tree

The K-D tree is a space-partitioning data structure (binary tree) for organizing points, every leaf node is a k-dimensional point. Every non-leaf node can be thought of as implicitly generating a splitting hyperplane that divides the space into two parts, known as half-spaces. Points to the left of this hyperplane are represented by the left subtree of that node and points to the right of the hyperplane are represented by the right subtree. The hyperplane direction is chosen in the following way: every node in the tree is associated with one of the k dimensions, with the hyperplane perpendicular to that dimension's axis. So, for example, if for a particular split the "x" axis is chosen, all points in the subtree with a smaller "x" value than the node will appear in the left subtree and all points with larger "x" value will be in the right subtree. In such a case, the hyperplane would be set by the x-value of the point, and its normal would be the unit x-axis [20].

5 FINDING THE AFFINE TRANSFORMATION

After we prepare our data, we refer back to [1] and determine how we need to build the cost function. As we are going to explain, it consists of three parts: distance term, stiffness term and landmark term.

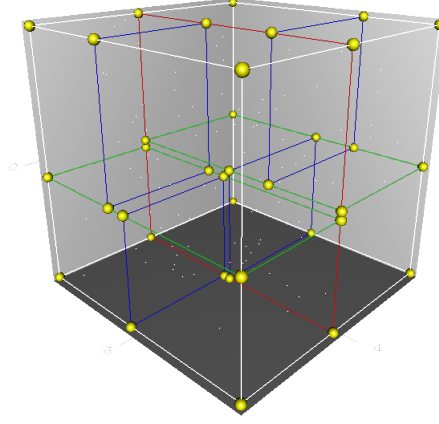


Figure 5: A 3-dimensional k-d tree. The first split (the red vertical plane) cuts the root cell (white) into two subcells, each of which is then split (by the green horizontal planes) into two subcells. Finally, four cells are split (by the four blue vertical planes) into two subcells. Since there is no more splitting, the final eight are called leaf cells [2].

5.1 The original cost function:

As we mention above, the cost function as it shown in equation (3) consists of three terms, each of which represent different concepts: the distance term, stiffness term and landmark term. The distance term represents the distance between the template graph S and target graph T which has to be as minimal as possible (i.e., which must be minimized). The stiffness term regularizes the template graph to prevents it from being exactly the target graph. The final term is the landmark term which gives the initial case for the template graph.

$$E(X) = E_d(X) + \alpha E_s(X) + \beta E_t(X) \quad (3)$$

Let us illustrate the first term, **the distance term**. As we mention before it is euclidean distance between points in template graph S and points in target graph T , which can be written as represented in equation (4), this distance has to be minimized as much as possible to align template graph S to target graph T with respect to the original shape of template graph S as much as possible, that means we need to make sure (by using stiffness term, which we will discuss later in this section) that all points which close to each other stay as possible as they are.

$$E_d(X) = \sum_{v_i \in V} w_i \text{dist}^2(T, X_i v_i) \quad (4)$$

In equation (4), v_i represent the vertices V in the template graph S in homogeneous coordinate $v_i = [x, y, z, 1]^T$, as we mentioned before, to be able to multiply them with affine matrices X_i which are 3×4 matrices including transformation part which illustrated in equation (1). The distance between each vertex $v_i \in V$ in the template graph S and it is closest vertex $u_i \in U$ in target graph T noted

with $dist^2(T, X_i v_i)$, and $w \in [0, 1]$ is weight which is *one* if the correspondence for this vertex v_i is found in the target graph S , and *zero* if not. This concept will let each vertex v_i in the template graph T moves toward its correspondence vertex u_i in the target graph T if it found, otherwise, it moves with its neighbors because of the stiffness. Simply we use distance threshold as parameter to distinguish correspondances.

Now we come to the second term, **the stiffness term**, which regularizes the shape deformation, represented in equation (5):

$$E_s(X) = \sum_{i,j \in E} ||(X_i - X_j)G||_F^2 \quad (5)$$

Regularizing the deformation occurs by penalising the weighted difference of the transformations of neighbouring vertices under the Frobenius norm $||.||_F$ using a weighting matrix $G := diag(1, 1, 1, \gamma)$. γ can be used to weight differences in the rotational and skew part of the deformation against the translational part of the deformation as it mentioned in [1]. The value of parameter γ depends on the units of the data, and on the type of deformation that shall be expressed. In our case we choose it to be one because we already scaled our data into the $[-1, 1]^3$ cube.

As it mentioned in [1] and in this thesis as well we use twelve parameters per vertex in 3×4 shape. This will allow us to write the cost function as a quadratic function which can be solved directly.

The Frobenius norm in equation (5) defined for matrix A as demonstrated in equation (6):

$$||A||_F = \sqrt{\sum_{i=1}^m \sum_{j=1}^n |a_{ij}|^2} \quad (6)$$

By applying this equation we keep the vertices, which linked together (there is an edge between them, they are in the same tract) or neighbors, close to each other.

The α parameter in equation (3) is a constant that manages the effect of the stiffness term, when it is high the neighbor vertices stay close to each other and vice versa, when it is low, more deformation can occur.

The final part of equation (3) is **Stiffness term** which demonstrated in bellow in equation (7):

$$E_l(X) = \sum_{(v_i, l) \in L} ||(X_i v_i - l)||^2 \quad (7)$$

Refer back to [1], it mention that landmark uses for initialization and guidance of the registration. Given a set of landmarks $L = \{(v_{i1}, l_1), (v_{i2}, l_2), \dots, (v_{il}, l_l)\}$

mapping template graph S vertices V_i into the target graph T vertices U_i , the landmark weight β in equation (3) is used to fade out the importance of the potentially noisy landmarks towards the end of the registration process.

The registration can be found even without landmarks. Without landmarks the cost function has global minima where the template is collapsed onto a point on the target surface, but the local minimum corresponding to the correct registration can be found for a wide range of initial conditions.

In our case, we use PCA transformation as initial step to align two graphs, therefore, we omit the landmark term later on from our cost function, this consider to be a first optimization to the cost function due to reduction of calculation effort and time the landmark term in our code.

Let us go deeper to illustrate the cost function more, and put the graphs in matrices that suit our cost function to ease implementation of the method.

Distance term in equation (3) and (4) become:

$$\begin{aligned} \bar{E}_d(X) &= \sum_{v_i \in V} w_i \|X_i v_i - u_i\|^2 \\ &= \left\| (W \otimes I_3) \begin{pmatrix} X_1 & & \\ & \ddots & \\ & & X_n \end{pmatrix} \begin{bmatrix} v_1 \\ \vdots \\ v_n \end{bmatrix} - \begin{bmatrix} u_1 \\ \vdots \\ u_n \end{bmatrix} \right\|^2 \end{aligned} \quad (8)$$

where $W = \text{diag}(w_1, \dots, w_n)$ is corresponded weight in diagonal matrix multiplied by Kronecker product \otimes to I_3 identity matrix, X is diagonal matrix of X_i that we need to solve multiplied by V which is vertices of template graph S subtracted by the (corresponded) vertices U of the target graph T .

the **Kronecker product**, denoted by \otimes , is an operation on two matrices of arbitrary size resulting in a block matrix. It is a generalization of the outer product (which is denoted by the same symbol) from vectors to matrices, and gives the matrix of the tensor product with respect to a standard choice of basis [21].

For instance, If A is an $m \times n$ matrix and B is a $p \times q$ matrix, then the Kronecker product $A \otimes B$ is the $mp \times nq$ block matrix:

$$A \otimes B = \begin{bmatrix} a_{11}B & \dots & a_{1n}B \\ \vdots & \ddots & \vdots \\ a_{m1}B & \dots & a_{mn}B \end{bmatrix}$$

So, the result of $W \otimes I_3$ is $3n \times 3n$ matrix, where X matrix has size $3n \times 4n$, V has $4n \times 1$ shape and U has shape $3n \times 1$.

We continue reform the equation to be differentiated easily by putting it into canonical form. We swap the position of X and the V matrices. For V matrix

we define a sparse matrix D which contains the the vertices $v_i \in V$ in diagonal position as demonstrated below:

$$D = \begin{bmatrix} v_1^T & & & \\ & v_2^T & & \\ & & \ddots & \\ & & & v_n^T \end{bmatrix} \quad (9)$$

The new format of the equation become:

$$\bar{E}_d(X) = ||W(DX - U)||_F^2 \quad (10)$$

Where the matrix W has size $n \times n$, the matrix D has size $n \times 4n$ (vertices v_i are in homogeneous coordinates $[x, y, z, 1]^T$), X has size $4n \times 3$, and U doesn't change with shape $n \times 3$ (vertices u_i are in 3D coordinate).

We continue to reform **the stiffness term** which penalises differences between the transformation matrices (affine matrices) X assigned to neighboring vertices. The simplified form of stiffness term will be:

$$E_s(X) = ||(M \otimes G)X||_F^2 \quad (11)$$

where M is node-arc incidence matrix which defined for directed graph. The number of rows in this matrix equal the number of nodes (vertices) and the number of columns equal the number of arcs (edges) on the graph and the values has to be *zeros, ones and/or minus ones*. the value will be *zero* if the edge on this column not connected to the vertex on this row where the value lie, otherwise the value has to be either 1 or -1 , it will be 1 if the edge direction coming to the vertex and -1 otherwise, it is illustrated in the figure {6}, the matrix M has size $e \times n$ where e and n are the number of edges and vertices respectively. $G = \text{diag}(1, 1, 1, y)$ is diagonal matrix and the result of $M \otimes G$ is a matrix with size $4e \times 4n$.

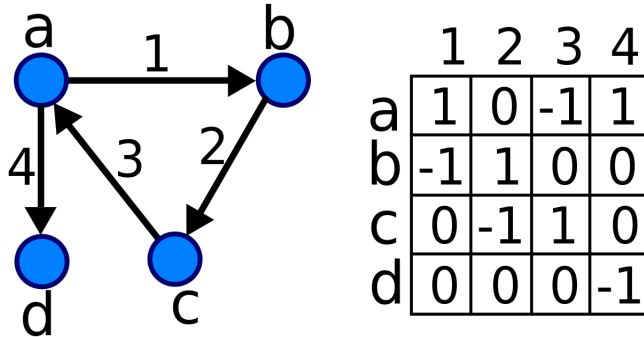


Figure 6: Oriented graph with corresponding incidence matrix [3]

Final term is **the landmark term** needs to be reformed as well, we reform it similar to distance term. We only consider those vertices from D (D from the

distance term (8)) are landmarks in a new matrix called D_L , and vertices from U (which are vertices from target graph T) are corresponded to those landmarks and put them in a new matrix called $U_L = [l_1, l_1, \dots, l_l]^T$.

The final shape of the cost function is quadratic function as shown below:

$$\bar{E}(X) = \left\| \begin{bmatrix} \alpha M \otimes G \\ WD \\ \beta D_L \end{bmatrix} X - \begin{bmatrix} 0 \\ WU \\ U_L \end{bmatrix} \right\|^2 = \|AX - B\|_F^2 \quad (12)$$

The current form of the function can be minimized by setting its derivative to zero and solve it as linear equation. The minimum value of $\bar{E}(X)$ is when $X = (A^T A)^{-1} A^T B$. Even the A is a sparse matrix and most of its values are zeros, it is still large matrix and it takes the most time of solving the equation. To solve this problem, we will remove the landmark term as mentioned before, because we already have the initial step by applying PCA, after we omit the landmark term the function will look like this:

$$\bar{E}(X) = \left\| \begin{bmatrix} \alpha M \otimes G \\ WD \end{bmatrix} X - \begin{bmatrix} 0 \\ WU \end{bmatrix} \right\|^2 = \|AX - B\|_F^2 \quad (13)$$

6 APPLYING THE TRANSFORMATIONS

Let us review the principal of affine transformation briefly. If we have a point $[x, y, 1]$ in homogeneous coordinate in 2D euclidean space and we want to move this point three unit through the X axis, $[x, y, 1]^T a = [x + 3, y, 1]^T$, in this case a is called affine matrix.

$$\begin{bmatrix} x \\ y \\ 1 \end{bmatrix} \begin{bmatrix} 1 & 0 & 3 \\ 0 & 1 & 0 \\ 0 & 0 & 1 \end{bmatrix} = \begin{bmatrix} x + 3 \\ y \\ 1 \end{bmatrix}$$

The example mentioned above is only for translation, we have still some other moves (i.e. sheer, rotation and scale) as demonstrated in figure {7} for 2D shape.

We have shown that how 2D transformation occurs, and the same applies to 3D as illustrated below:

$$\begin{bmatrix} \hat{x} \\ \hat{y} \\ \hat{z} \\ 1 \end{bmatrix} \begin{bmatrix} a & b & c & e \\ f & g & h & i \\ j & k & l & m \\ 0 & 0 & 0 & 1 \end{bmatrix} = \begin{bmatrix} x \\ y \\ z \\ 1 \end{bmatrix}$$

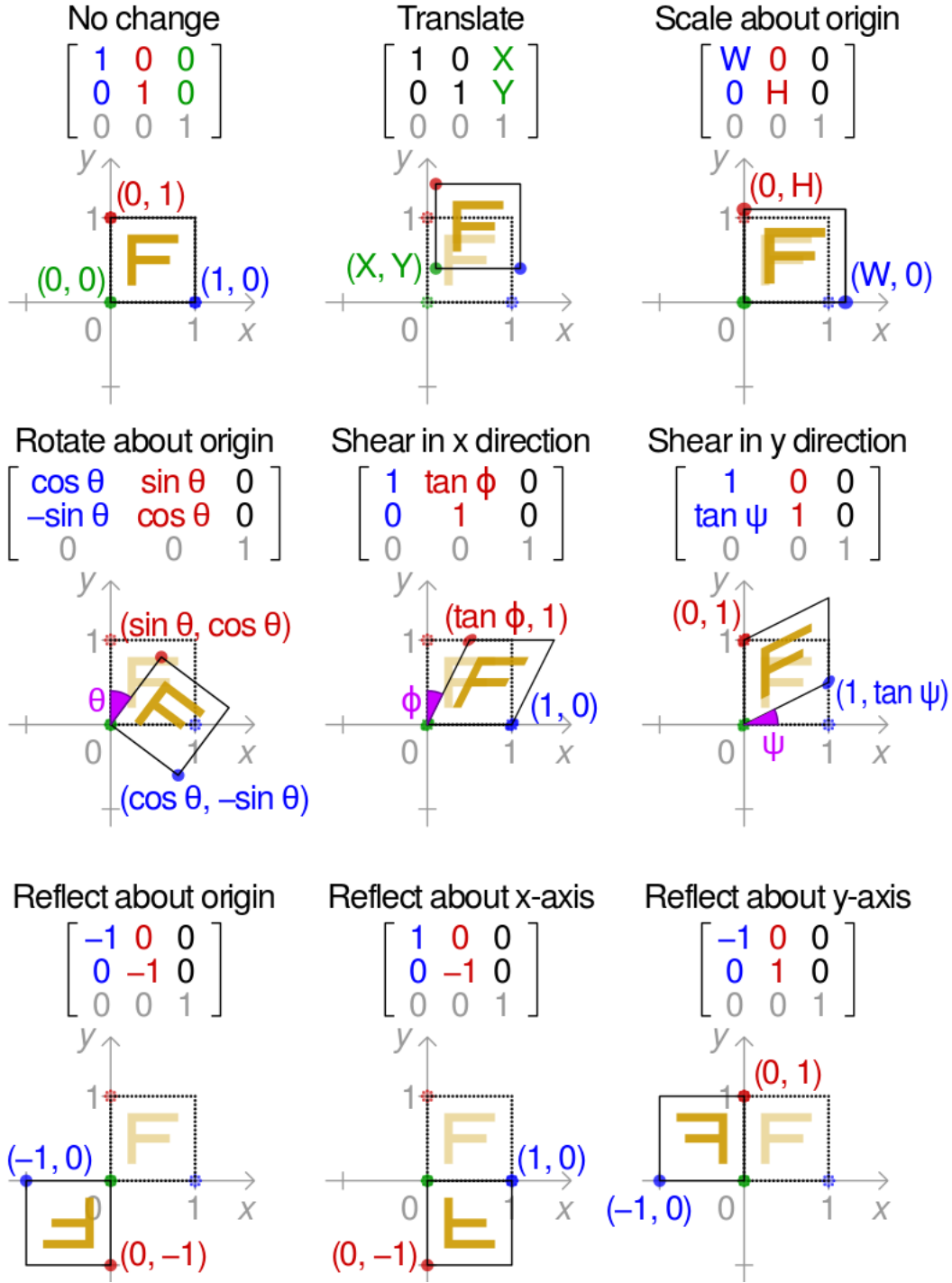


Figure 7: 2D affine transformation matrices [4]

But this is still on point, if we have more points like our case, the equation above become:

$$\begin{bmatrix} \hat{x}_1 & \hat{x}_2 & \dots & \hat{x}_n \\ \hat{y}_1 & \hat{y}_2 & \dots & \hat{y}_n \\ \hat{z}_1 & \hat{z}_2 & \dots & \hat{z}_n \\ 1 & 1 & \dots & 1 \end{bmatrix} \begin{bmatrix} a & b & c & e \\ f & g & h & i \\ j & k & l & m \\ 0 & 0 & 0 & 1 \end{bmatrix} = \begin{bmatrix} x_1 & x_2 & \dots & x_n \\ y_1 & y_2 & \dots & y_n \\ z_1 & z_2 & \dots & z_n \\ 1 & 1 & \dots & 1 \end{bmatrix}$$

7 NONRIGID OPTIMAL ICP ALGORITHMS

As we mentioned in the introduction, *Iterative Closest Point (ICP)* is an algorithm employed to minimize the distance between two or more points clouds, to achieve this goal, we use *Sparse Least Squares algorithm (LSQR)* which is iterative method for solving $Ax = b$ and $\min ||Ax - b||^2$, where the matrix A is large and sparse (as in our case). The method is based on the bidiagonalization procedure of Golub and Kahan. It is analytically equivalent to the standard method of conjugate gradients, but possesses more favorable numerical properties [19].

We will demonstrait the idea of using *lsqr* to solve our cost function in the next chapter implementation.

IMPLEMENTATION

To implement the method we have discussed before, we wrote the code in *Python Programming Language* and *Spyder* version 3 and *Integrated Development Environment (IDE)* are used.

As we mentioned before, our data is in *ply* format as shown in figure {3}, to read this format we wrote our own method using *plyfile* library due to special case of our data which has different arrangement files. The method we wrote return data in *numpy ndarray* structure where each array tract is putted in an array and all tracts belong to the same bundle were putted together with respect to the sequences of the neighboring vertices.

Then we apply PCA transformation (*sklearn.decomposition* library) to the data and generate histogram (*matplotlib.pyplot* library) for distances between each vertex in the template graph S and its closet vertex in target graph T , before and after PCA transformation to compare the distance difference, because in some cases where the two graphs (template and target) are already in the best alignment before ICP, PCA transformation increase the distance between them as we will show in the result chapter. If the distance between two graphs is increased we drop the PCA transformation step. For distance measurement we use *K-D tree* from *scikit learn*.

We continue to build variables as shown in equation (13), to do so, we use histograms generated in the previous step to determine the threshold for the maximum distance we need to consider for W in the **distance term** for cost function, if the value is equal or below the threshold $w_i = 1$, otherwise $w_i = 0$. Then we build W as diagonal sparse matrix using *scipy.sparse* library. Then we continue using the same library (*scipy.sparse*) to build D sparse matrix and calculate WD and WU .

Now we have the **distance term** of the cost function, we need to build the **stiffness term**, we use the same library (*scipy.sparse*) to build M sparse matrix and G diagonal sparse matrix and calculate Kronecker product ($M \otimes G$).

The final step of building the cost function is to vertically stack MG and WD to have A , and vertically stack zero sparse matrix and WU to have B as require $\|Ax - b\|_F^2$.

The last step is solving the cost function $\|Ax - b\|_F^2$ by using *LSQR* from *scipy.sparse.linalg* library. As mentioned in the *scipy.sparse.linalg.lsqr* documentation [22], b in equation $Ax - b$ must be a vector, and as b in our case is a matrix size $n \times 3$, we use matrices fundamental concept to solve this problem as we use *lsqr* three times for each column and horizontally stack the result to get the affine matrices combination.

Finally for visualization we customize functions from *open3d* library to view brain bundles due to special case of our data.

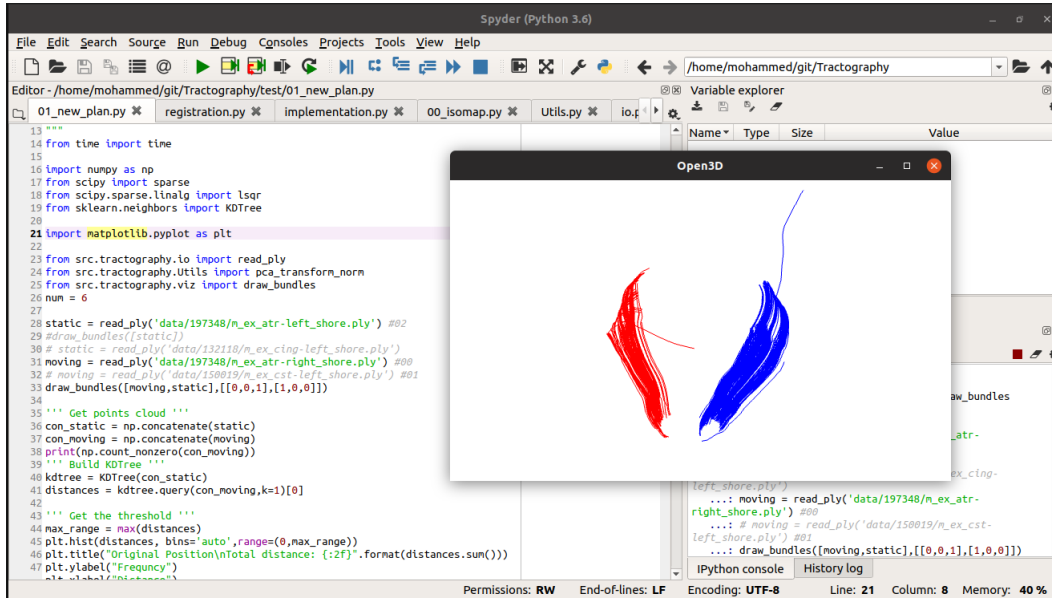


Figure 8: IDE and visualization tool

RESULT

CONCLUSION

BIBLIOGRAPHY

- [1] Brian Amberg, Sami Romdhani, and Thomas Vetter. Optimal step nonrigid icp algorithms for surface registration. In *Computer Vision and Pattern Recognition, 2007. CVPR'07. IEEE Conference on*, pages 1–8. IEEE, 2007.
- [2] Wikipedia, the free encyclopedia. 3d tree, February 2006. [Online; accessed Feb 9, 2019].
- [3] Wikipedia, the free encyclopedia. Oriented graph with corresponding incidence matrix, 2010. [Online; accessed Feb 9, 2019].
- [4] Wikipedia, the free encyclopedia. 2d affine transformation matrices, 2016. [Online; accessed Feb 10, 2019].
- [5] Hongdong Li and Richard Hartley. The 3d-3d registration problem revisited. In *2007 IEEE 11th International Conference on Computer Vision*. IEEE, 2007.
- [6] Hal Blumenfeld. *Neuroanatomy through Clinical Cases*. Oxford University Press, 2010.
- [7] Stephen B. Klein. *Biological Psychology*. Worth Publishers, 2008.
- [8] R. Douglas Fields. White matter matters. *Scientific American*, 298(3):54–61, mar 2008.
- [9] University of Washington. Braininfo. <http://braininfo.rprc.washington.edu>, 1994.
- [10] Sabine E. Grimm, Nigel Armstrong, Bram L. T. Ramaekers, Xavier Pouwels, Shona Lang, Svenja Petersohn, Rob Riemsma, Gillian Worthy, Lisa Stirk, Janine Ross, Jos Kleijnen, and Manuela A. Joore. Nivolumab for treating metastatic or unresectable urothelial cancer: An evidence review group perspective of a NICE single technology appraisal. *PharmacoEconomics*, oct 2018.
- [11] Daniel Mamah, Thomas E. Conturo, Michael P. Harms, Erbil Akbudak, Lei Wang, Amanda R. McMichael, Mokhtar H. Gado, Deanna M. Barch, and John G. Csernansky. Anterior thalamic radiation integrity in schizophrenia: A diffusion-tensor imaging study. *Psychiatry Research: Neuroimaging*, 183(2):144 – 150, 2010.
- [12] Pr Denis Ducreux. Connectopedia knowledge database. <http://www.fmritools.com/kdb/index.html>, 2015.
- [13] Per Brodal. *The Central Nervous System*. OXFORD UNIV PR, 2016.

- [14] Jared Tanner. An overview of and introduction to the cingulum, 2010.
- [15] Henry Gray. *Anatomy of the Human Body*. Philadelphia : Lea & Febiger, 1918.
- [16] Peter W. Kalivas. Neurotransmitter regulation of dopamine neurons in the ventral tegmental area. *Brain Research Reviews*, 18(1):75–113, jan 1993.
- [17] Zhengyou Zhang. Iterative point matching for registration of free-form curves and surfaces. *International Journal of Computer Vision*, 13(2):119–152, oct 1994.
- [18] I.T. Jolliffe. *Principal Component Analysis (Springer Series in Statistics)*. Springer, 2002.
- [19] Christopher C Paige and Michael A Saunders. Lsqr: An algorithm for sparse linear equations and sparse least squares. *ACM Transactions on Mathematical Software (TOMS)*, 8(1):43–71, 1982.
- [20] Jon Louis Bentley. Multidimensional binary search trees used for associative searching. *Communications of the ACM*, 18(9):509–517, 1975.
- [21] Wikipedia contributors. Kronecker product, February 2019. [Online; accessed 9-February-2019].
- [22] Eric Jones, Travis Oliphant, Pearu Peterson, et al. SciPy: Open source scientific tools for Python, 2001. [Online; accessed February 11th, 2019].