

# Abstention for Noise-Robust Learning in Medical Image Segmentation

*presented by:*

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# Introduction

## What is Label Noise?

- Errors or inaccuracies in ground truth training labels.
- A pervasive problem in real-world datasets.

## Why is it Bad?

- Deep Neural Networks tend to memorize these errors.
- This leads to poor generalization and unreliable models.

## Amplified in Image Segmentation

- Segmentation demands pixel-perfect accuracy.
- This makes the annotation process uniquely tedious and error-prone, especially at object boundaries.

# Noise in Medical Segmentation

## The Annotation Bottleneck

- Acquiring clean labels is extremely difficult and expensive.
- Requires time from scarce, highly-trained medical experts.
- Subject to significant inter-observer variability (experts disagree).

## The High Stakes of Failure

- Medical segmentation is a critical, safety-sensitive task.
- Inaccurate models can directly impact patient diagnosis.
- Urgent need for models that are robust to noise.

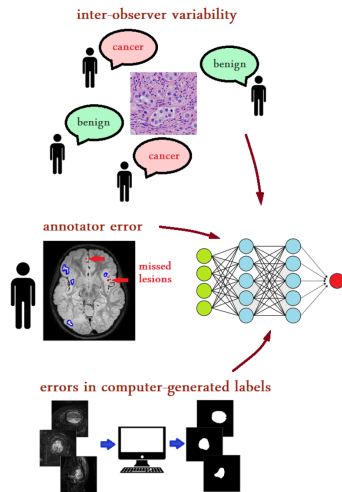


Figure: The primary sources of label noise in medical settings [3]

## Extensive research exists for mitigating label noise in classification tasks:

- Label Cleaning and Pre-processing.
- Robust Network Architectures.
- Data Re-weighting.
- Curriculum Learning and Knowledge Distillation.
- Noise-robust Loss Functions.

## Extensive research exists for mitigating label noise in classification tasks:

- Label Cleaning and Pre-processing.
- Robust Network Architectures.
- Data Re-weighting.
- Curriculum Learning and Knowledge Distillation.
- **Noise-robust Loss Functions.**
  - Relatively easy to implement.
  - Universal solutions.
  - Can be used alongside other methods.

- This critical area remains notably under-investigated for image segmentation.
  - Adapting existing methods to segmentation.
  - Developing new methods tailored for segmentation.
- Many existing methods are not directly suited for the spatial nature of segmentation noise and cannot be easily adapted.
- Developing new methods is complicated and requires significant research time and resources.

## Our Contributions:

- We address this research gap by adapting Abstention to segmentation.
- We improve and expand abstention beyond its current definition.



# Exploring Abstention

## The Mechanism

- Model can choose to *not* make a classification decision on ambiguous data.
- Adds an extra output unit ( $k + 1$ ) representing 'abstain' or 'ignore' class.
- The loss function is modified to reward abstention on uncertain samples.
- Higher abstention = lower loss = smaller contribution to the gradient.

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## The Benefits

- Avoids overfitting on noisy samples.
- Filters data during training with minimal computational overhead.
- No pre-processing required.
- Architecture (and potentially loss function) agnostic.

$$\mathcal{L}_{DAC}(x_j) = (1 - p_{k+1}) \left( - \sum_{i=1}^k t_i \log \frac{p_i}{1 - p_{k+1}} \right) + \alpha \log \frac{1}{1 - p_{k+1}}$$

- Modified CE
- Abstention probability  $p_{k+1}$ .
- Regularization term  $\left[ \alpha \log \frac{1}{1 - p_{k+1}} \right]$ .
- Incremental abstention penalty  $\alpha$ .
- $\alpha$  is initialized to a small value after a warm-up period.

# Deep Abstaining Classifier

$$\mathcal{L}_{DAC}(x_j) = (1 - p_{k+1}) \left( - \sum_{i=1}^k t_i \log \frac{p_i}{1 - p_{k+1}} \right) + \alpha \log \frac{1}{1 - p_{k+1}}$$

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**Algorithm 1**  $\alpha$  auto-tuning

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**Input:** total iter. ( $T$ ), current iter. ( $t$ ), total epochs ( $E$ ), abstention-free epochs ( $L$ ), current epoch ( $e$ ),  $\alpha$  init factor ( $\rho$ ), final  $\alpha$  ( $\alpha_{final}$ ), mini-batch cross-entropy over true classes ( $\mathcal{H}_c(P_{1...K}^M)$ )

$\alpha_{set} = False$

**for**  $t := 0$  to  $T$  **do**

**if**  $e < L$  **then**

$\beta = (1 - P_{k+1}^M) \mathcal{H}_c(P_{1...K}^M)$

**if**  $t = 0$  **then**

$\tilde{\beta} = \beta$  // initialize moving average

**end if**

$\tilde{\beta} \leftarrow (1 - \mu) \tilde{\beta} + \mu \beta$

**end if**

**if**  $e = L$  and **not**  $\alpha_{set}$  **then**

$\alpha := \tilde{\beta} / \rho$  // initialize  $\alpha$  at start of epoch  $L$

$\delta_\alpha := \frac{\alpha_{final} - \alpha}{E - L}$

$update_{epoch} = L$

$\alpha_{set} = True$

**end if**

**if**  $e > update_{epoch}$  **then**

$\alpha \leftarrow \alpha + \delta_\alpha$  // then update  $\alpha$  once every epoch

$update_{epoch} = e$

**end if**

**end for**

---

Figure: DAC's  $\alpha$  auto-tuning algorithm [5].

$$\mathcal{L}_{IDAC}(x_j) = (1 - p_{k+1}) \left( - \sum_{i=1}^k t_i \log \frac{p_i}{1 - p_{k+1}} \right) + \alpha(\tilde{\eta} - \hat{\eta})^2$$

- Extension of DAC.
- $\alpha$  is fixed during training.
- Uses noise estimation  $\tilde{\eta}$  to guide or 'inform' abstention  $\hat{\eta}$ .
- $\hat{\eta} = \sum_{l=1}^N \frac{p_{l,k+1}}{N}$ .

# Informed Deep Abstaining Classifier

$$\mathcal{L}_{IDAC}(x_j) = (1 - p_{k+1}) \left( - \sum_{i=1}^k t_i \log \frac{p_i}{1 - p_{k+1}} \right) + \alpha(\tilde{\eta} - \hat{\eta})^2$$

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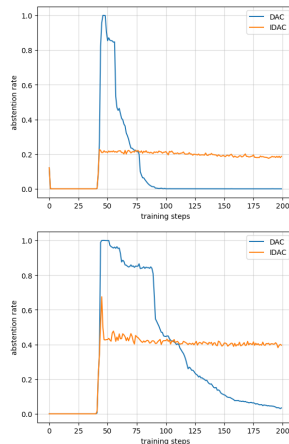


Figure: Abstention behaviour in DAC and IDAC at 10% (top) and 20% (bottom) label noise.

## Generalized Cross Entropy (GCE)

$$\mathcal{L}_{GCE}(x_j) = \frac{1 - f(x_j)^q}{q}$$



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## Symmetric Cross Entropy (SCE)

$$\mathcal{L}_{RCE}(x_j) = - \sum_{i=1}^k p_i \log(t_i)$$

$$\mathcal{L}_{SCE}(x_j) = \alpha \mathcal{L}_{CE}(x_j) + \beta \mathcal{L}_{RCE}(x_j)$$

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$$\mathcal{L}_{SCE}(x_j) = \alpha \mathcal{L}_{CE}(x_j) + \beta \mathcal{L}_{RCE}(x_j)$$

## Dice Loss (Dice Similarity Coefficient)

$$\mathcal{DSC}(x_j) = \frac{2 \sum_{i=1}^N p_i t_i}{\sum_{i=1}^N p_i + \sum_{i=1}^N t_i}$$

$$\mathcal{L}_{Dice}(x_j) = 1 - \mathcal{DSC}(x_j)$$

# Universal Abstention Framework

$$\mathcal{L}_{abstention}(x_j) = (1 - p_{k+1})\mathcal{L}_x(x_j) + \alpha \left| \log \frac{1 - \tilde{\eta}}{1 - p_{k+1}} \right| \quad (1)$$

$$\mathcal{L}_{abstention}(x_j) = (1 - p_{k+1})\mathcal{L}_x(x_j) + \alpha \left| \log \frac{1 - \tilde{\eta}}{1 - p_{k+1}} \right| \quad (1)$$

## Informed Regularization

- Combines DAC and IDAC.
- Allows for more freedom to abstain when noise level is high.
- Reduces overfitting in the final stages of training.
- Defaults back to DAC if  $\tilde{\eta}$  is unknown.

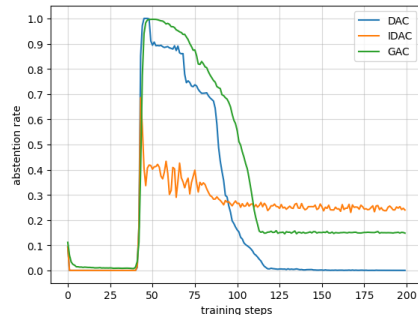


Figure: Abstention behaviour in DAC, IDAC, and GAC at 15% noise.

$$\alpha = \alpha_{final} * \left( \frac{e - L}{E - L} \right)^{\gamma} \quad (2)$$

current epoch  $e$ , total epochs  $E$ , warm-up epochs  $L$ .

- Replaces DAC's complicated auto-tuning algorithm with a simpler and more flexible calculation.
- $\gamma$  controls the rate of growth for  $\alpha$ .
- Higher  $\gamma \rightarrow$  smaller  $\alpha \rightarrow$  more abstention.
- Still allows for DAC's linear growth ( $\gamma = 1$ ).

# Power-law auto-tuning

$$\alpha = \alpha_{final} * \left( \frac{e - L}{E - L} \right)^{\gamma} \quad (2)$$

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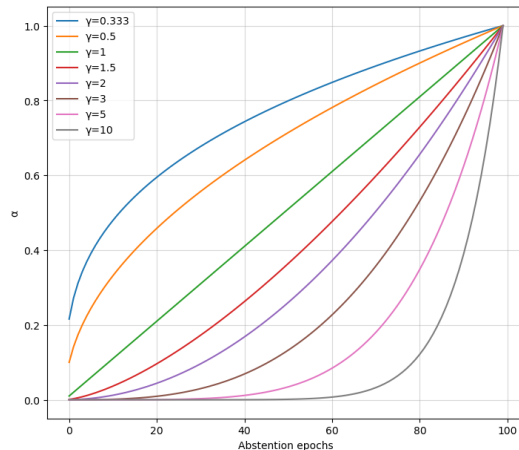


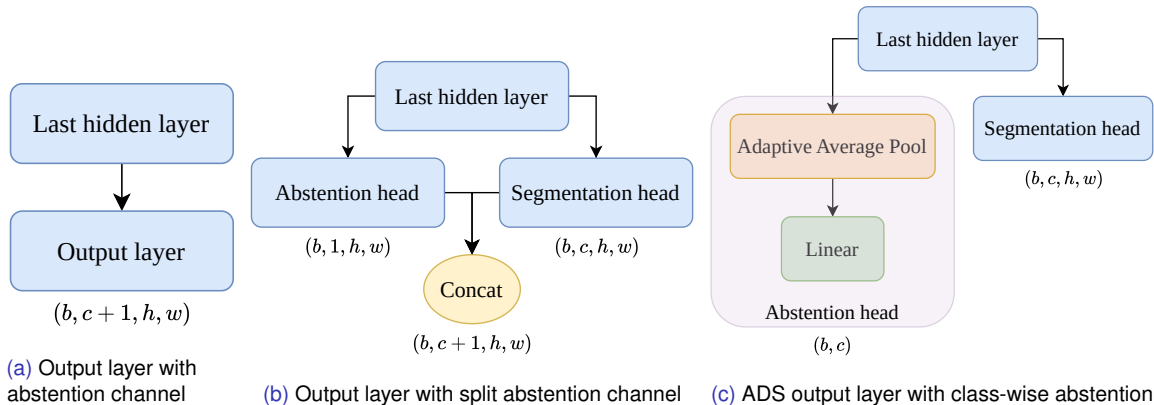
Figure: The effect of different values of  $\gamma$  on the growth of  $\alpha$  with  $\alpha_{final} = 1$ .

- **Generalized Abstaining Classifier (GAC):** GCE + Abstention
- **Symmetric Abstaining Classifier (SAC):** SCE + Abstention
- **Abstaining Dice Segmenter (ADS):** Dice + Abstention



- **Generalized Abstaining Classifier (GAC):** GCE + Abstention
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  - needs to adapt Abstention to Dice's class-wise nature.

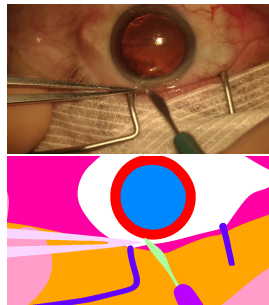
# ADS Class-wise Abstention



**Figure:** Transforming the output layer of an abstaining model from pixel-wise to class-wise abstention.

# Experiments

- 4,670 high-quality annotated images from cataract surgery.
- Dense annotations.
- Has 3 variants for number of classes.
- We used the first variant (8 classes).
- Normalized and resized to 480x256.



**Figure:** Example image frame (top) and semantic segmentation labels (bottom) from the CaDIS Dataset [2].

# Datasets: DSAD

- 13,195 laparoscopic annotated images.
- Binary segmentations for 11 anatomical structures.
- 1,430 stomach images used for multi-organ segmentation (7 organs).
- Sparse annotations ( $\approx 82\%$  background).
- Normalized and resized to 480x384.

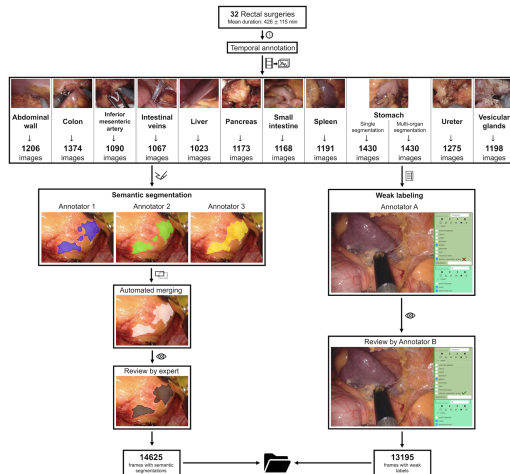


Figure: Overview of the data acquisition and validation process of DSAD [1].

- Morphological operations: Erosion and Dilation.
- Random label flipping.
- 5 noise level for each dataset.
- CaDIS: 5-25%.
- DSAD: 3-15%.



Figure: Two examples of Erosion and Dilation. Correct segmentation boundaries in red [6].

- Most commonly used segmentation architecture.
- Designed for medical image segmentation.
- encoder captures context and decoder enables precise localization.
- Skip connections bridge the two paths.
- Used with pretrained ResNet-50 backbone.

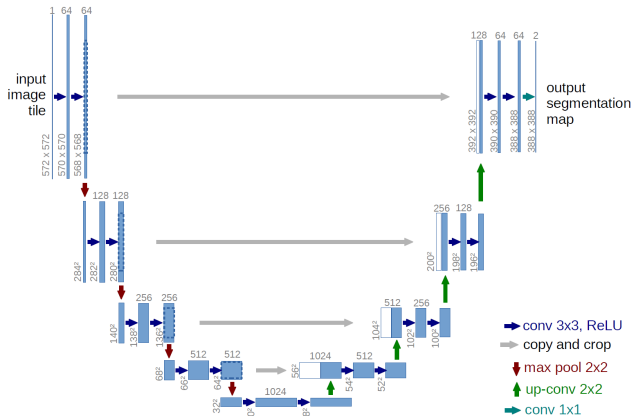


Figure: The U-Net architecture [4].

# Experimental Setup

- Optimized hyperparameters with U-Net for highest noise level for each dataset.
- Trained for 50 epochs.
- AdamW with  $\text{lr}=0.003$ .
- $\text{lr}$  divided by 5 every 10 epochs.
- A single NVIDIA A100 80GB GPU.

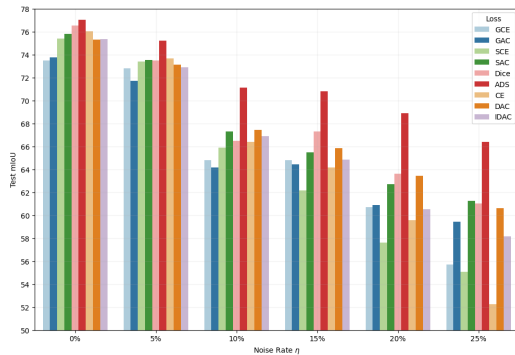
Loss	CaDIS	DSAD
DAC	$\alpha_{final} = 1$ $L = 10$	$\alpha_{final} = 2$ $L = 18$
IDAC	$\alpha = 1$ $L = 10$	$\alpha = 1$ $L = 10$
GCE	$q=0.5$	$q=0.1$
GAC	$\alpha_{final} = 3$ $L = 10$ $\gamma = 3$	$\alpha_{final} = 2$ $L = 15$ $\gamma = 2$
SCE	$\alpha = 1$ $\beta = 1$	$\alpha = 0.5$ $\beta = 1$
SAC	$\alpha_{final} = 1$ $L = 10$ $\gamma = 1.5$	$\alpha_{final} = 1$ $L = 20$ $\gamma = 3$
ADS	$\alpha_{final} = 1$ $L = 10$ $\gamma = 3$ $w = 16$	$\alpha_{final} = 4$ $L = 10$ $\gamma = 1.5$ $w = 16$

**Table:** The hyperparameters used in our experiments.

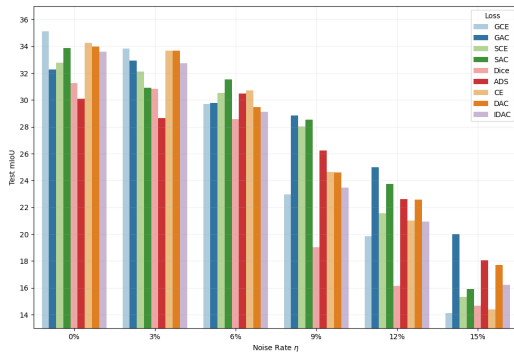


# Evaluations

# Results



(a) CaDIS



(b) DSAD

**Figure:** Test mIoU (%) scores of a U-Net model trained on CaDIS (a) and DSAD (b) at 5 different noise levels.

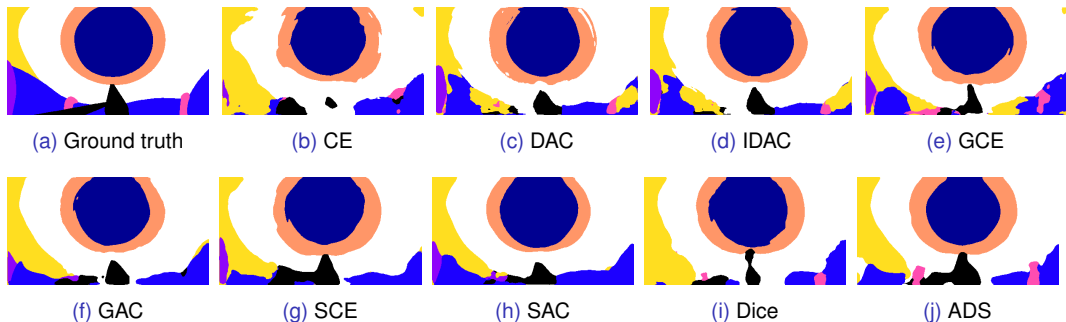
# U-Net Performance

Dataset	Noise rate $\eta$ (%)	Loss function								
		CE	DAC	IDAC	GCE	GAC	SCE	SAC	Dice	ADS
CaDIS	0	<b>76.02±0.70</b>	75.29±0.79	75.36±0.73	73.49±3.27	<b>73.76±2.80</b>	75.38±0.75	<b>75.83±0.62</b>	76.52±0.47	<b>77.04±0.37</b>
	5	<b>73.67±1.03</b>	73.14±0.46	72.89±0.41	<b>72.83±1.11</b>	71.73±2.79	73.41±0.71	<b>73.51±1.59</b>	73.48±0.28	<b>75.22±0.85</b>
	10	66.39±0.17	<b>67.43±0.49</b>	66.92±0.49	<b>64.82±0.86</b>	64.16±2.57	65.92±0.91	<b>67.29±1.65</b>	66.51±0.61	<b>71.12±0.55</b>
	15	64.15±2.47	<b>65.85±1.05</b>	64.87±0.91	<b>64.81±0.46</b>	64.44±2.70	62.16±1.99	<b>65.48±2.11</b>	67.31±0.73	<b>70.80±1.08</b>
	20	59.56±1.21	<b>63.42±0.87</b>	60.54±2.27	60.73±1.41	<b>60.91±1.64</b>	57.62±4.22	<b>62.70±0.31</b>	63.64±0.82	<b>68.88±0.49</b>
	25	52.27±1.70	<b>60.63±2.73</b>	58.19±4.77	55.71±1.30	<b>59.46±0.76</b>	55.08±0.93	<b>61.27±1.22</b>	61.04±1.41	<b>66.39±0.67</b>
DSAD	0	<b>34.25±2.50</b>	34.01±0.96	33.60±0.72	<b>35.14±1.65</b>	32.26±0.53	32.78±1.19	<b>33.86±1.83</b>	<b>31.28±0.87</b>	30.09±1.10
	3	<b>33.69±1.85</b>	33.67±2.01	32.76±2.03	<b>33.84±2.56</b>	32.94±2.23	<b>32.11±1.09</b>	30.90±2.76	<b>30.83±4.78</b>	28.64±2.76
	6	<b>30.70±2.47</b>	29.47±1.97	29.11±2.10	29.69±1.96	<b>29.78±4.27</b>	30.51±2.16	<b>31.55±2.43</b>	28.56±1.00	<b>30.48±3.61</b>
	9	<b>24.65±2.90</b>	24.58±2.61	23.47±2.48	22.95±2.93	<b>28.84±4.17</b>	28.02±2.37	<b>28.55±1.29</b>	19.04±1.92	<b>26.23±2.05</b>
	12	21.00±3.15	<b>22.59±4.35</b>	20.94±1.86	19.84±2.89	<b>25.00±4.13</b>	21.57±0.67	<b>23.73±0.68</b>	16.15±1.49	<b>22.63±0.51</b>
	15	14.41±2.59	<b>17.69±3.97</b>	16.24±1.45	14.12±2.91	<b>20.01±2.56</b>	15.31±0.75	<b>15.91±3.53</b>	14.65±1.50	<b>18.05±1.63</b>

**Table:** Average test mIoU (%) and standard deviation (5 runs) of a U-Net model trained on CaDIS and DSAD datasets with various rate of label noise, comparing five abstaining loss functions [DAC, IDAC, GAC, SAC, ADS] against their non-abstaining baselines [CE, GCE, SCE, Dice]. Best results in each bracket are in **bold**.

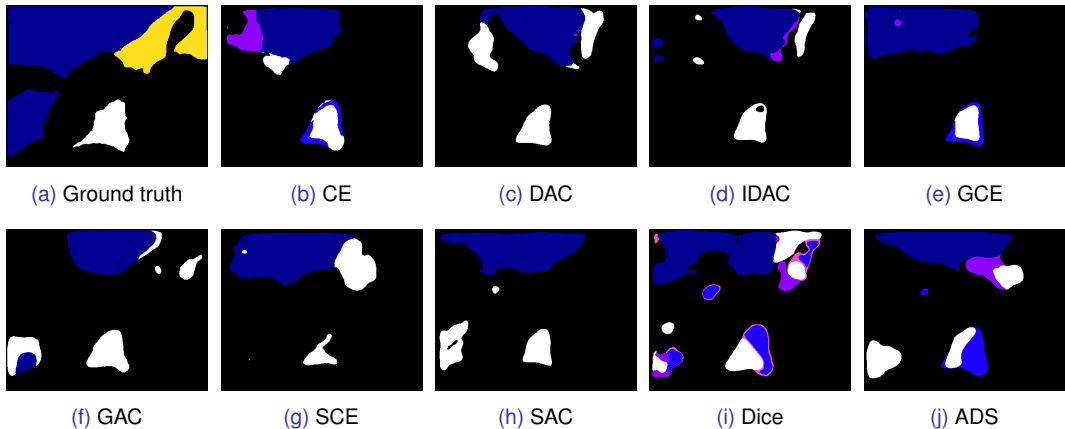
Dataset	Loss function								
	CE	DAC	IDAC	GCE	GAC	SCE	SAC	Dice	ADS
CaDIS	56.02±1.30	<b>57.02±0.81</b>	56.29±1.05	55.56±2.08	<b>58.08±1.43</b>	58.37±0.53	<b>59.77±1.17</b>	59.55±1.66	<b>61.84±2.23</b>
DSAD	<b>16.73±2.34</b>	15.90±3.19	16.20±1.37	16.26±1.37	<b>19.01±1.69</b>	12.74±2.03	<b>14.03±3.53</b>	12.46±0.86	<b>17.16±2.02</b>

**Table:** Average test mIoU (%) and standard deviation (5 runs) of a DeepLabV3+ model trained on CaDIS and DSAD datasets at 25% and 15% label noise, respectively. Best results in each bracket are in **bold**.



**Figure:** Visualisation of a sample clean ground truth from CaDIS and the segmentation predictions of a U-Net model trained with each loss function at 25% noise.

# Visualizations



**Figure:** Visualisation of a sample clean ground truth from DSAD and the segmentation predictions of a U-Net model trained with each loss function at 15% noise.

# Conclusions

- Adapted abstention for Medical Image Segmentation.
- Enhanced abstention with Informed regularization and flexible  $\alpha$ -tuning.
- Integration with different and distinct loss functions.
- Empirical proof: Abstention boosts robustness across losses, datasets, and architectures.
- Abstention is a modular and easy-to-use extension for robust learning in medical imaging.



- **Dynamic Noise Estimation:** Develop methods to learn the noise rate directly from the data.
- **Real-World Noise Validation:** Test on clinical datasets with naturally occurring, unsimulated noise.
- **Abstention as an Uncertainty Metric:** Use the model's abstention signal to flag difficult cases for expert review, creating a human-in-the-loop system.

A decorative header consisting of three vertical bars: a blue bar on the left, a grey bar in the middle, and a yellow bar on the right.

Thank You

- [1] Matthias Carstens et al. “The Dresden Surgical Anatomy Dataset for Abdominal Organ Segmentation in Surgical Data Science”. In: *Sci Data* 10.1 (Jan. 2023), p. 3. ISSN: 2052-4463. DOI: [10.1038/s41597-022-01719-2](https://doi.org/10.1038/s41597-022-01719-2).
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