

# Tianxing Li



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# Human Sensing Using Light

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# The Rise Of Light Sensing

IMU  
sensors



Radio  
antennas



Microphone



Cameras



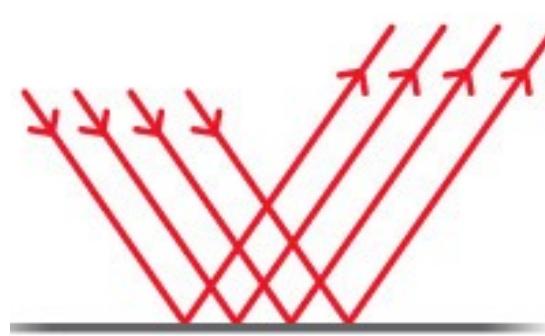


# Light As A Primary Modality For Fine-grained Human Sensing

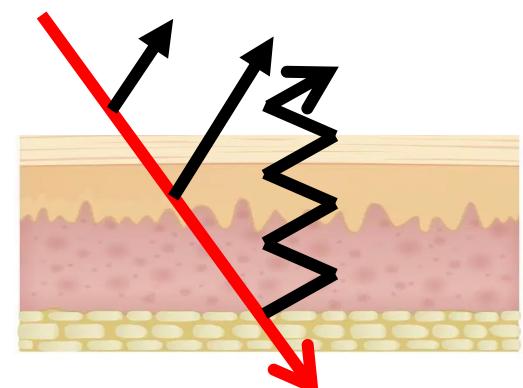
- Sense light intensity change caused by the human **blockage**, **reflection**, and **absorption** to infer fine-grained human behaviors and biomarkers.



Blockage



Reflection



Absorption



Biomechanical  
sensing



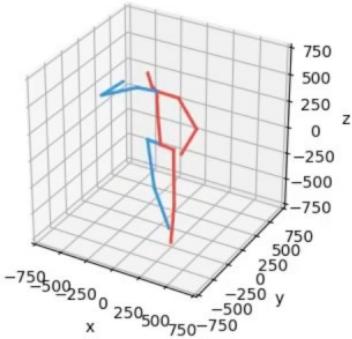
Biophysiological  
sensing



Biochemical  
sensing



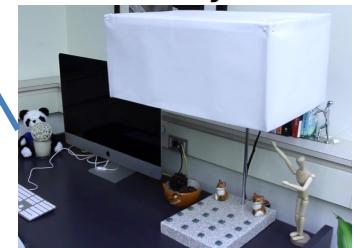
Skeleton pose  
reconstruction



MobiCom '15



MobiSys '16



UbiComp '17



Biomechanical  
sensing



Biophysiological  
sensing



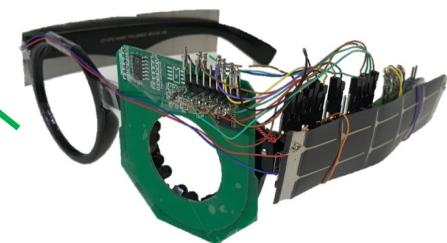
Biochemical  
sensing



Eye tracking



SenSys '17



MobiCom '18



Biomechanical  
sensing



Biophysiological  
sensing



Biochemical  
sensing



SenSys '20

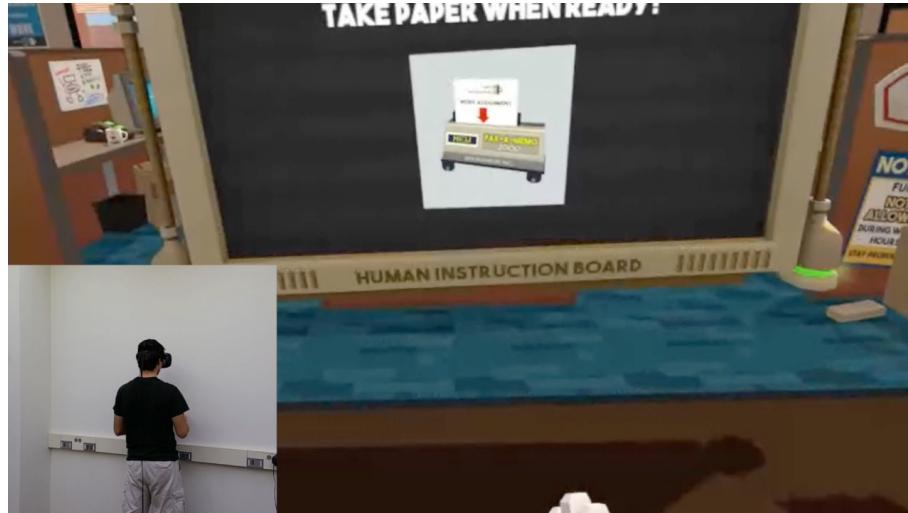
Noninvasive glucose monitoring



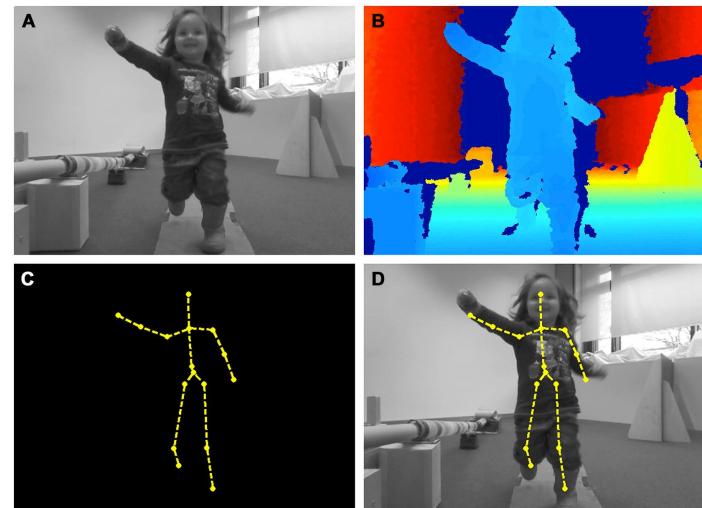
# Outline

- Introduction
- Biomechanical sensing: Skeleton pose reconstruction
- Biophysiological sensing: Battery-free eye tracking
- Biochemical sensing: Noninvasive glucose monitoring
- Conclusion & Future Work

# Skeleton Pose Reconstruction Applications



Human-computer interaction (HCI)

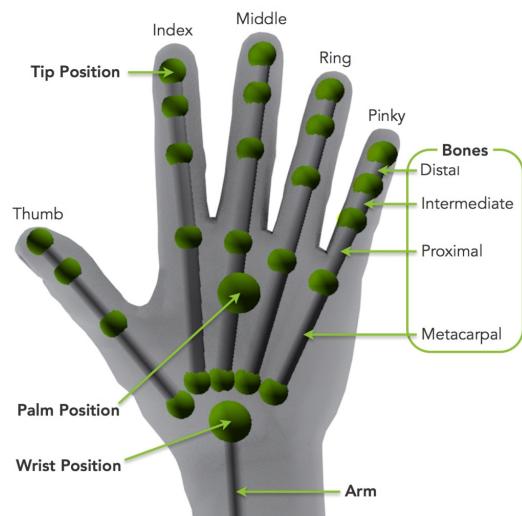
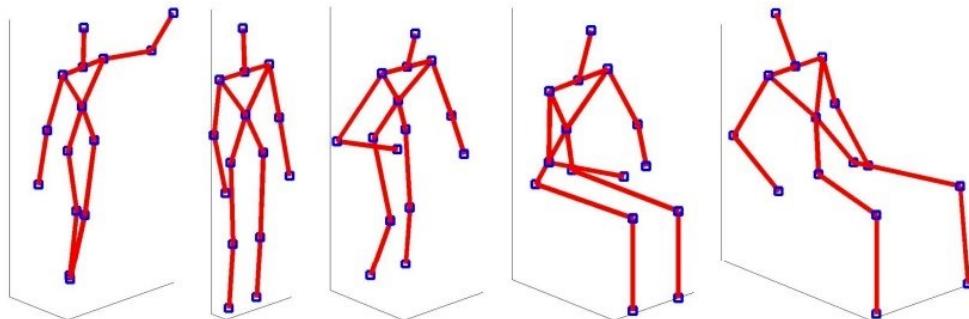


Health monitoring



# Skeleton Pose Reconstruction is Challenging

- Poses are complex
  - Whole-body pose has 26 degrees of freedom.
  - Hand pose has 23 degrees of freedom.





## Existing Skeleton Reconstruction Systems

LEAP  
MOTION



Leap Motion



Microsoft Kinect



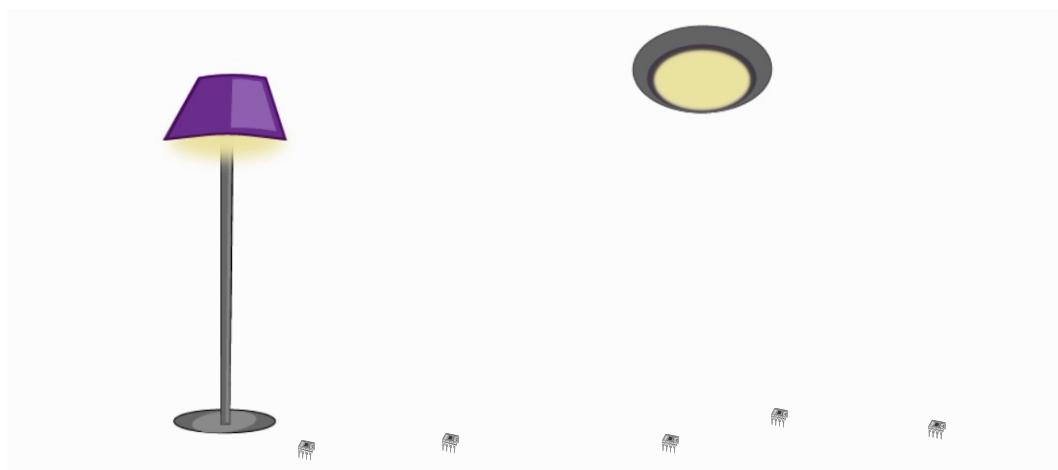
VICON

- :( Heavy computation overhead
- :( Privacy concern<sup>1</sup>
- :( Limited field of view (FoV)



## Solution: Light Blockage Sensing

- Replace cameras with distributed photodiodes
- Measure how body block light rays
- Aggregate light-blockage information to infer 3D poses



Photodiodes

# Design Challenges

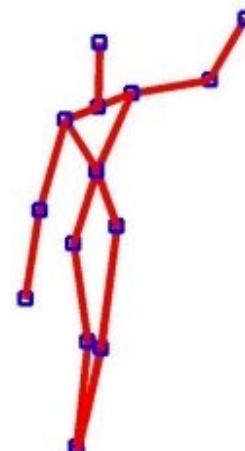
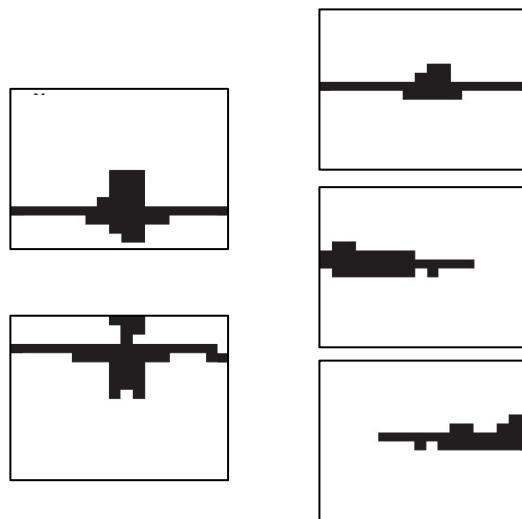
#1: Light interface with multiple light sources





# Design Challenges

## #2: 2D Low-resolution shadows



5 example shadows



## Design Challenges

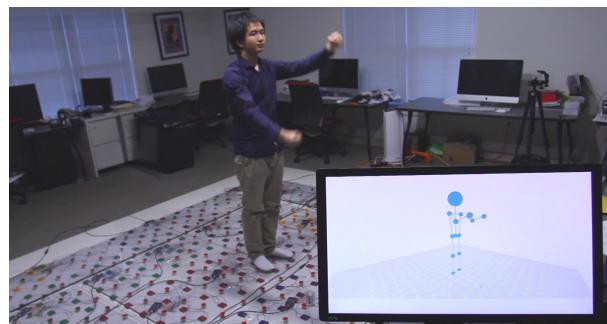
#3: Object blockage (furniture, other people, pets, etc.)





# Contributions in Skeleton Pose Reconstruction

## Whole-body poses

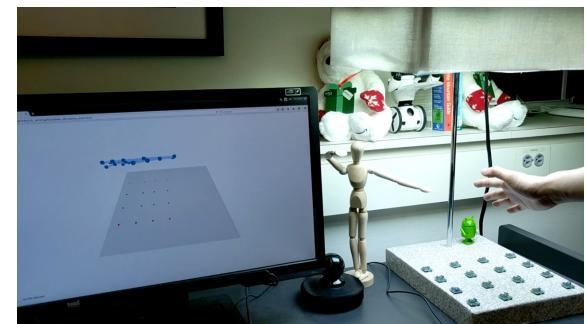


LiSense @ 60 Hz  
(MobiCom'15)



StarLight @ 40 Hz  
(MobiSys'16)

## Hand poses



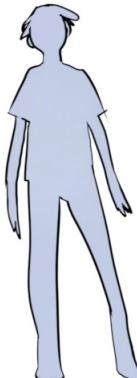
Aili @ 140 Hz  
(UbiComp'17)



# LiSense Overview

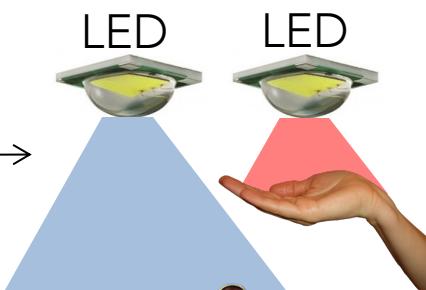
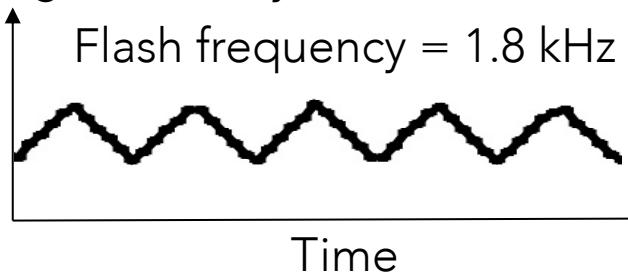
Challenge #1: Multiple light sources

Separate light rays via  
**light beacons**

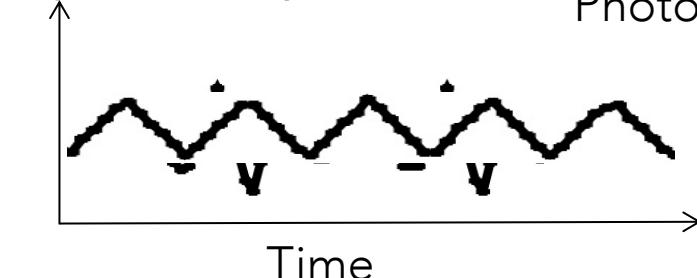


# Light Beacon Rationale

Light intensity



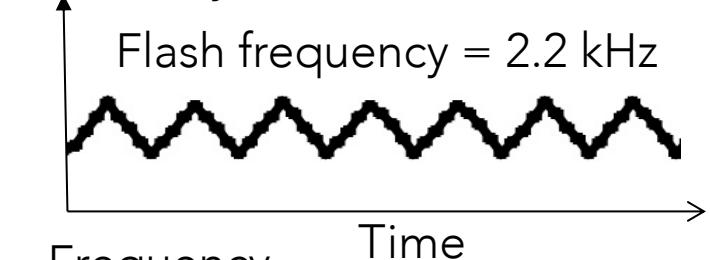
Light intensity



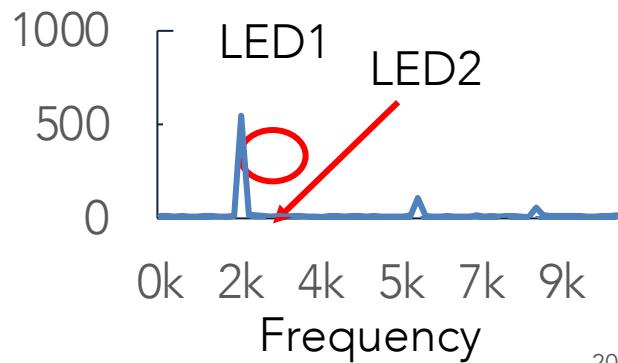
Photodiode

FFT

Light intensity



Frequency power

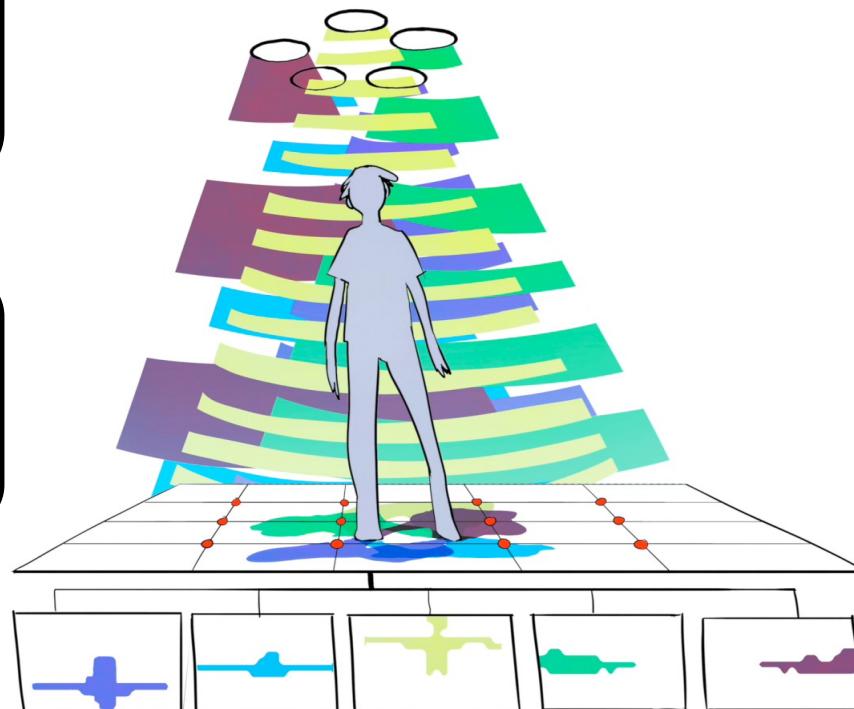




# LiSense Overview

Challenge #2:  
Reconstruct a 3D pose  
from 2D shadows

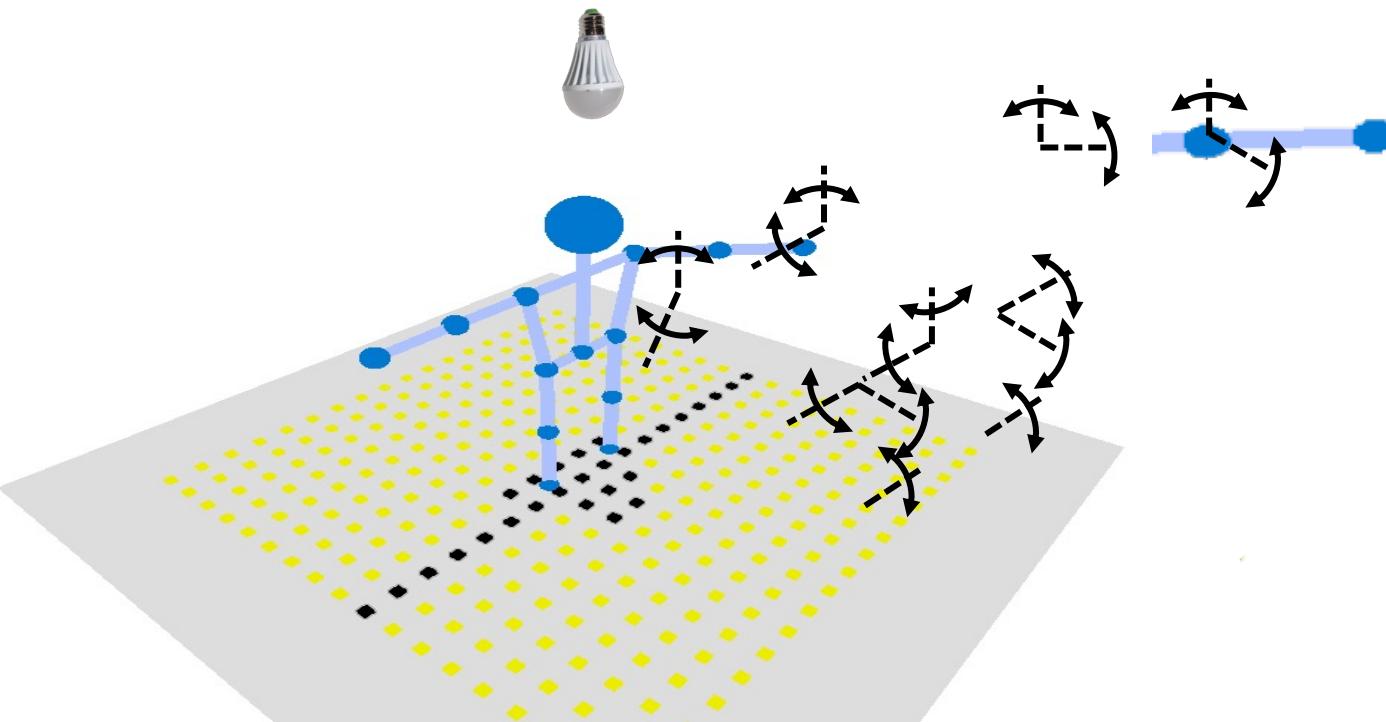
Seek a posture best  
fitting shadows cast in  
**multiple directions**





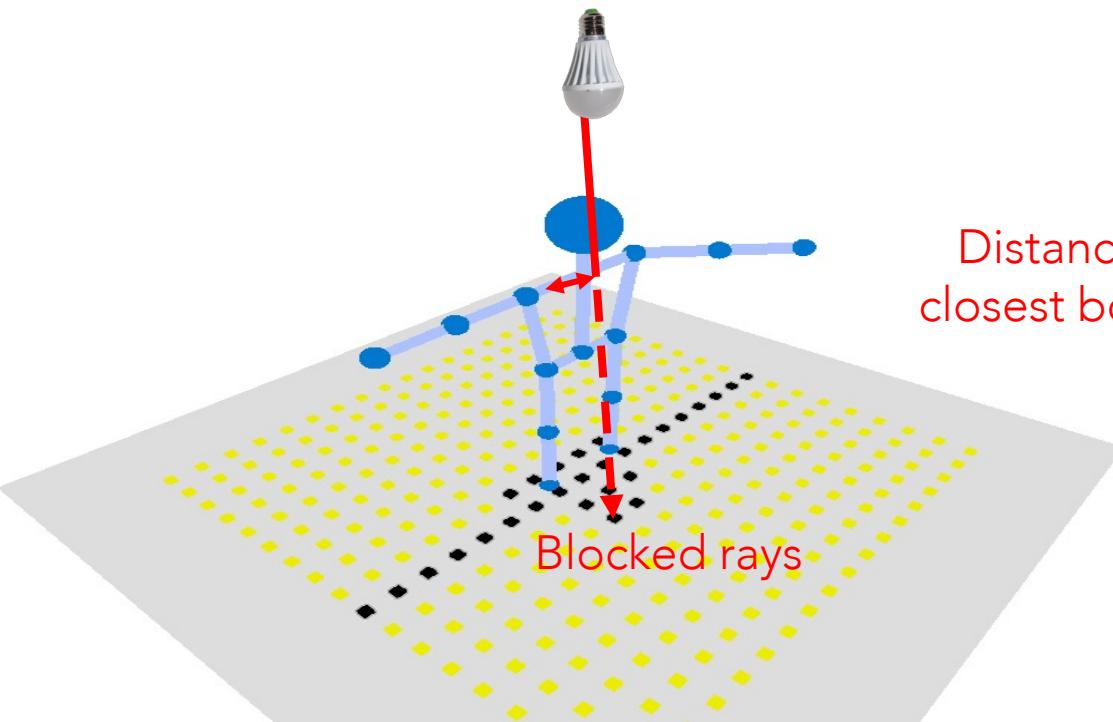
# Shadow-Based Inference

- Search for the skeleton best matching observed shadow maps



# Shadow-Based Inference

- Search for the skeleton best matching observed shadow maps



A candidate pose

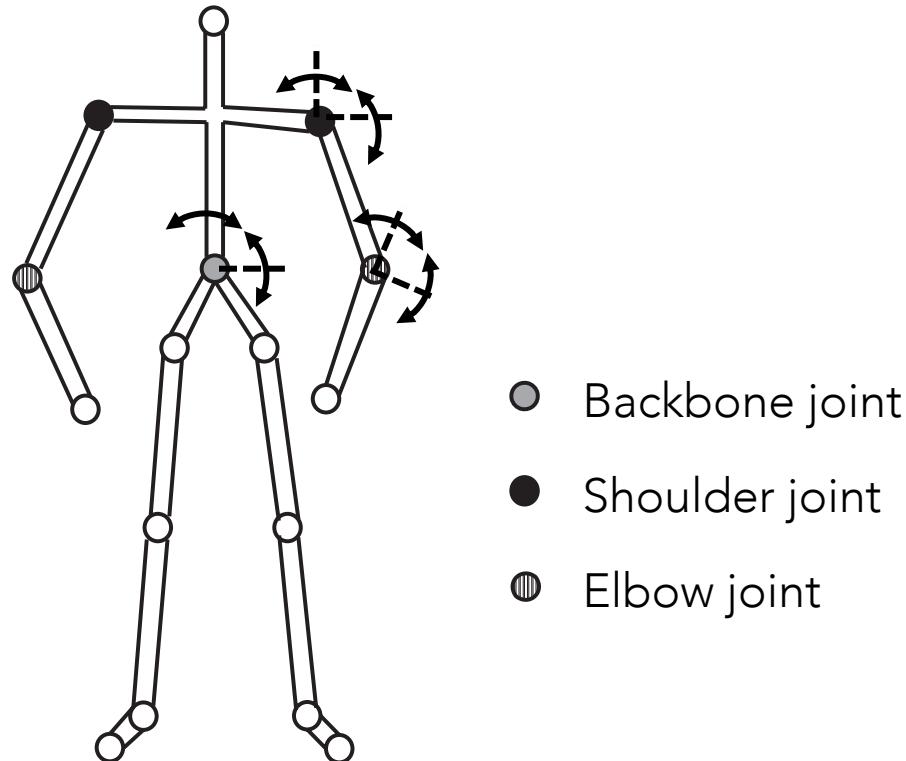
$$B^* = \operatorname{argmin}_{B^*} E(B)$$

Distance between blocked rays and the closest body segment on a candidate pose

- Challenges:
  - No close-form solution
  - Large search area in high dimensional space

# Search for Pose Candidates E(B)

- Sequential search: prioritize the search order based on the body part size
- Fixed-step search: search from large to small movement magnitude



- Backbone joint
- Shoulder joint
- Elbow joint

# Experiment Settings

- 7 users
  - 169 cm – 190 cm
  - 60 kg – 80 kg
- Ground truth
  - Human labelling using three cameras





## Reconstruction Accuracy

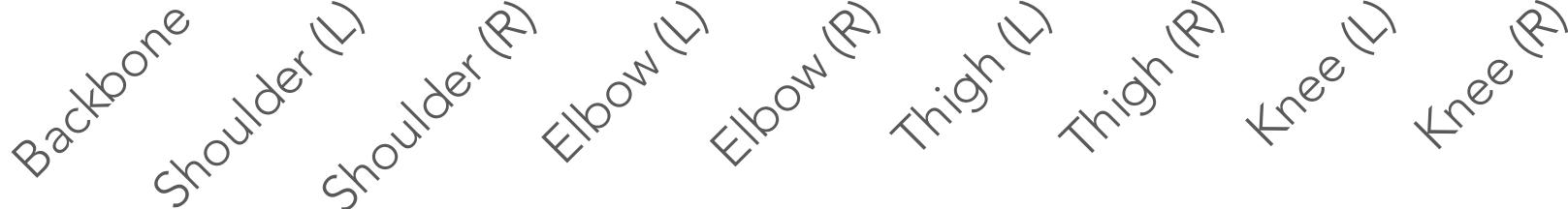
Angular error ( $^{\circ}$ )

25  
20

6 degrees

10 $^{\circ}$  mean angular error

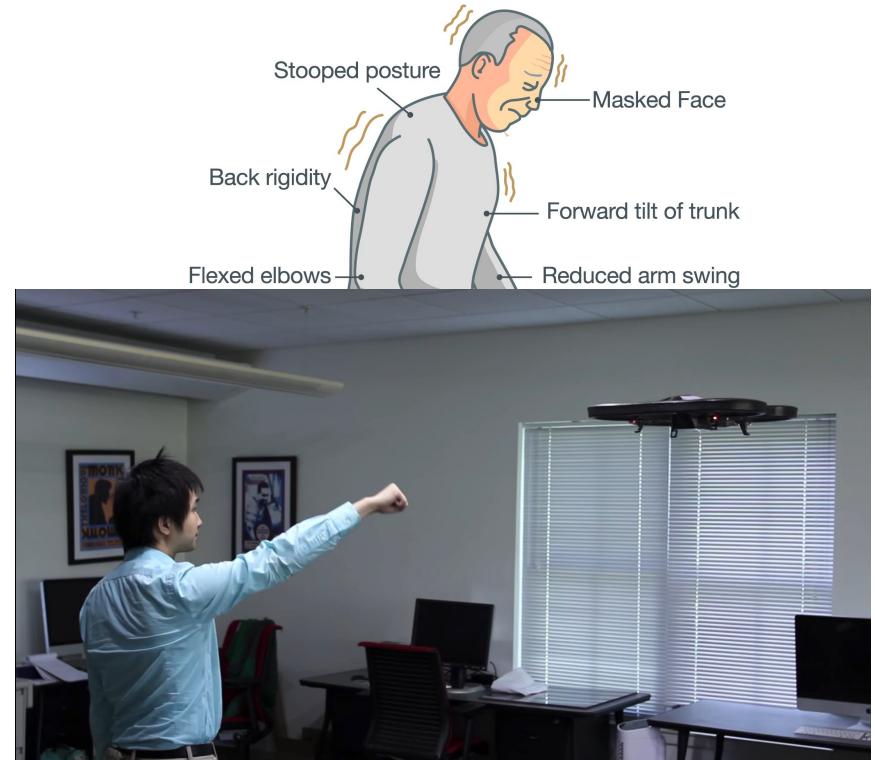
5  
0





# Potential Applications

- Health
  - Detect early symptoms of diseases (e.g., Parkinson's disease)
  - Help with stroke recovery
- HCI
  - Control robots with body movement
  - Virtual reality interaction
  - Translate sign language



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# Wearable Eye Tracking in VR/AR



New interactive input



Optimized Rendering

# Wearable Eye Tracking in Health



Fatigue detection



Detect early symptoms of diseases (e.g., ADHD)

# Existing Wearable Eye Trackers

- Camera-based
- ☹ High power consumption
- ⚡ Expensive

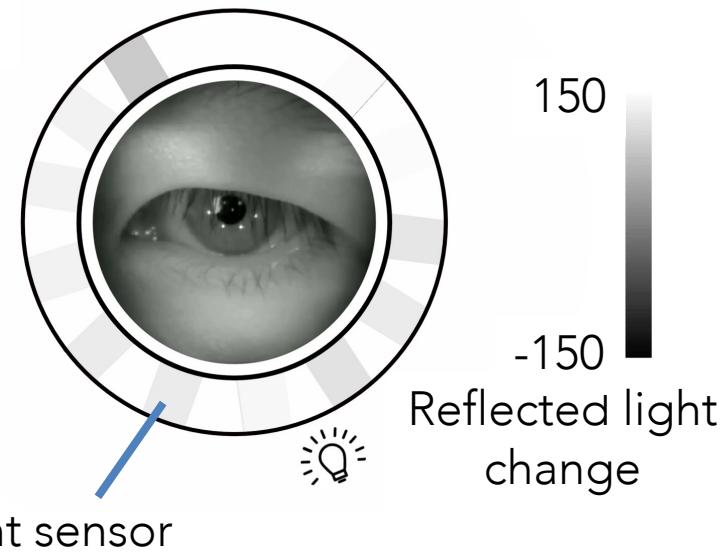
Can we design a low-power and low-cost eye tracker?



## My Approach

- Pupil's light absorption property
- Array of photodiodes to sample reflected light intensity change
- Benefits:
  - Low-cost
  - Low-power

Pupil dilation





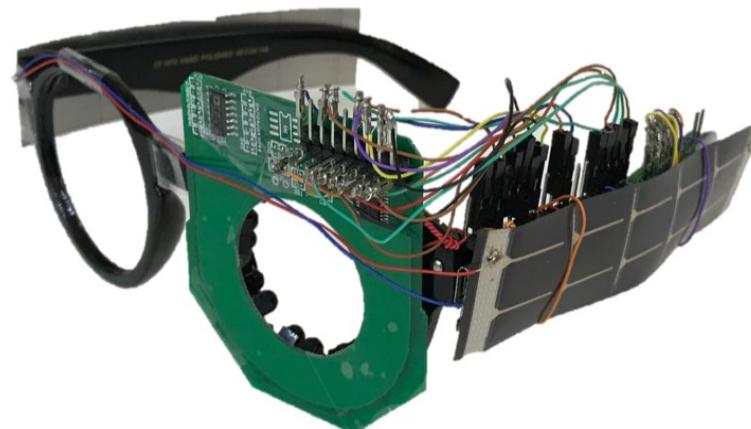
# Contributions in Eye Tracking

VR headset



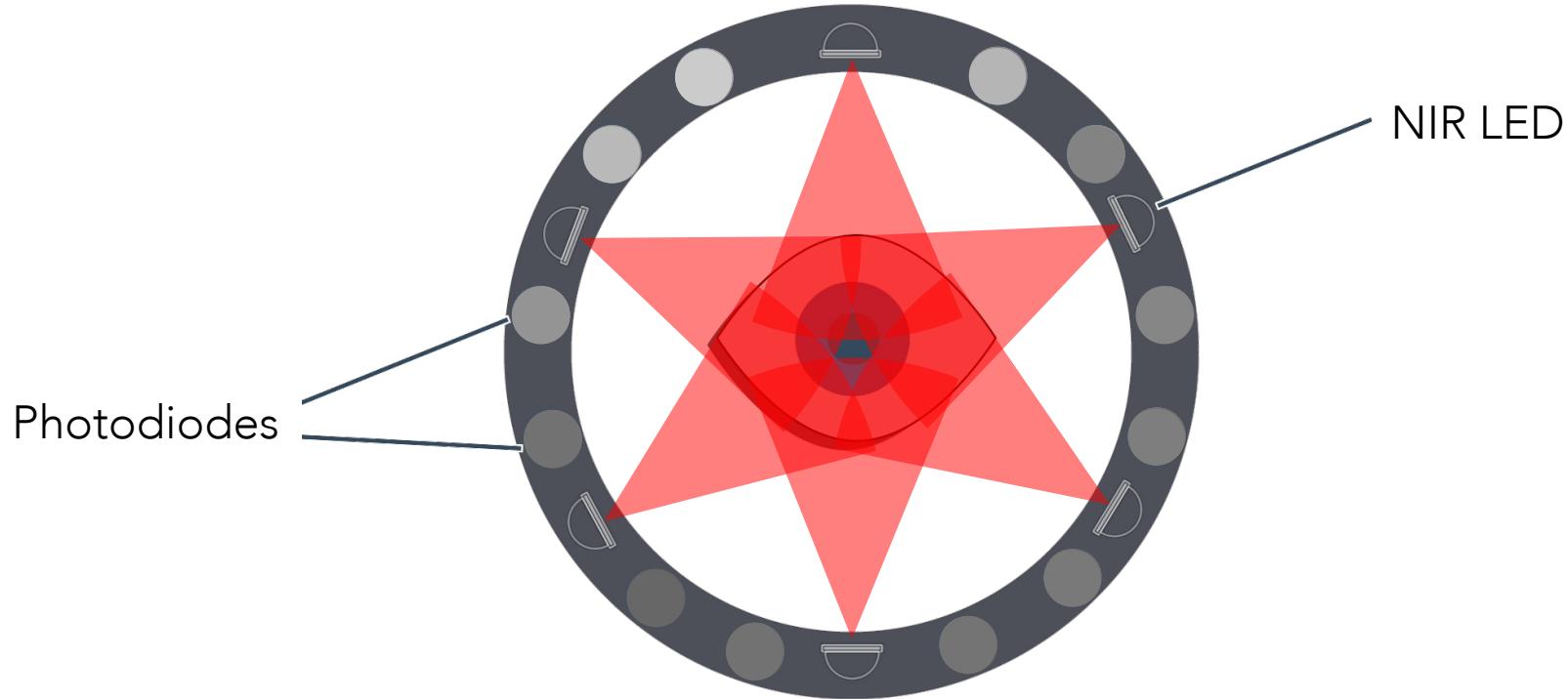
SenSys'17

Regular/AR glasses



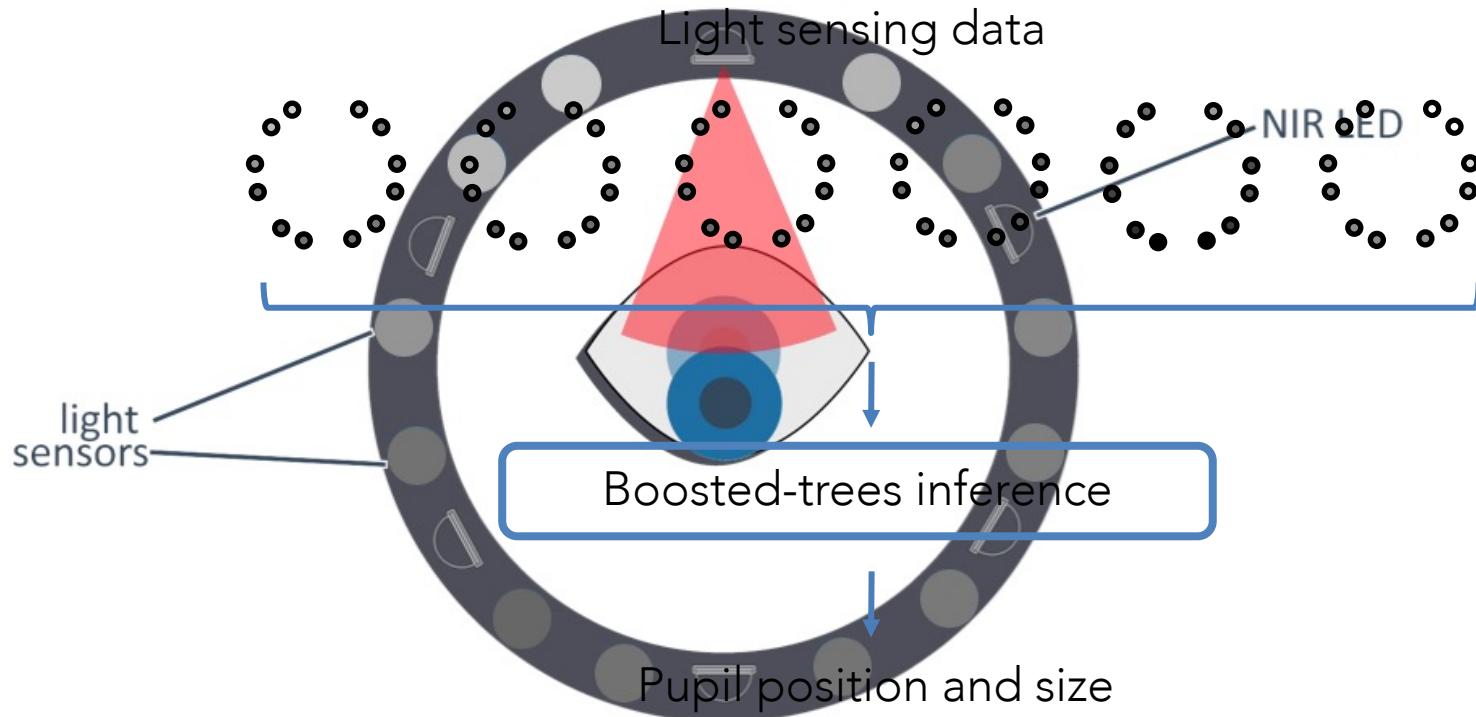
MobiCom'18

# Sensing with Multiple NIR LEDs

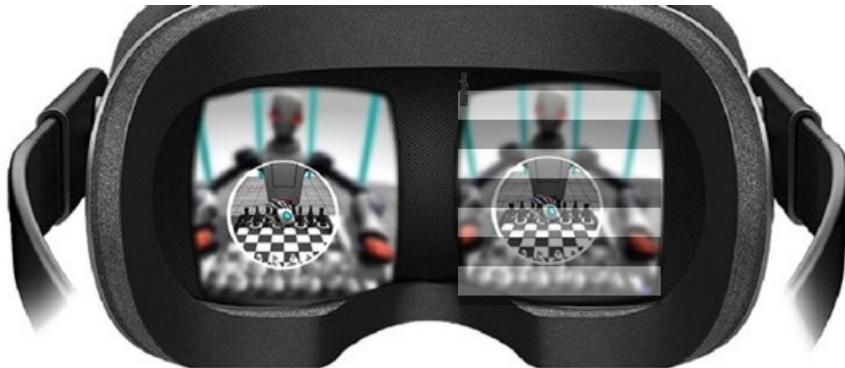




# Sensing with Multiple NIR LEDs



# High Tracking Rate is Essential!



VR  
 $> 90 \text{ Hz}$



Health  
 $> 120 \text{ Hz}$



# Predictability of Eye Movements

- Characteristics of four types of eye movement



Fixation

Predictable



Smooth pursuit

Predictable



Blink

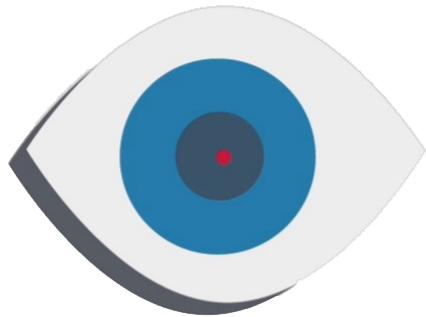
Pupil covered



Saccade

Unpredictable

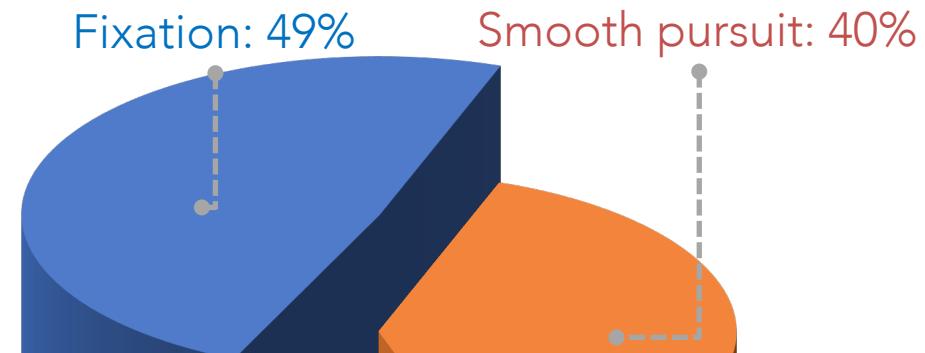
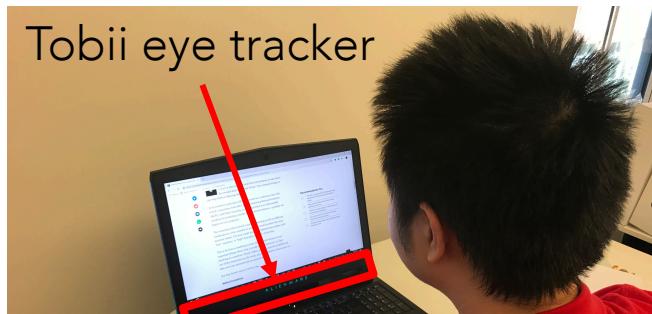
# Pupil Movement is Jerky...



Saccadic movement occupies a small portion!

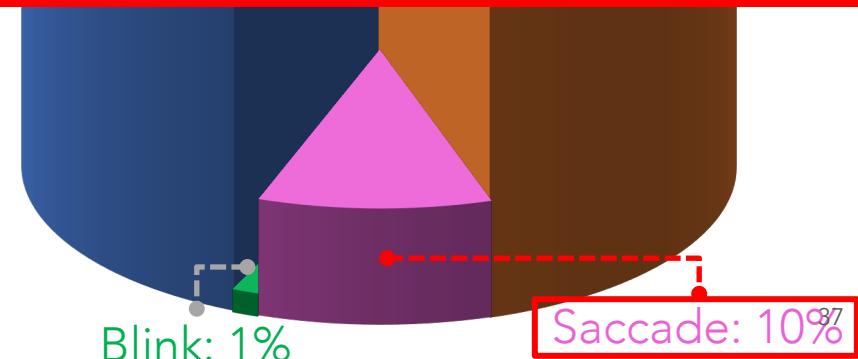


# User Study on Eye Movement Patterns



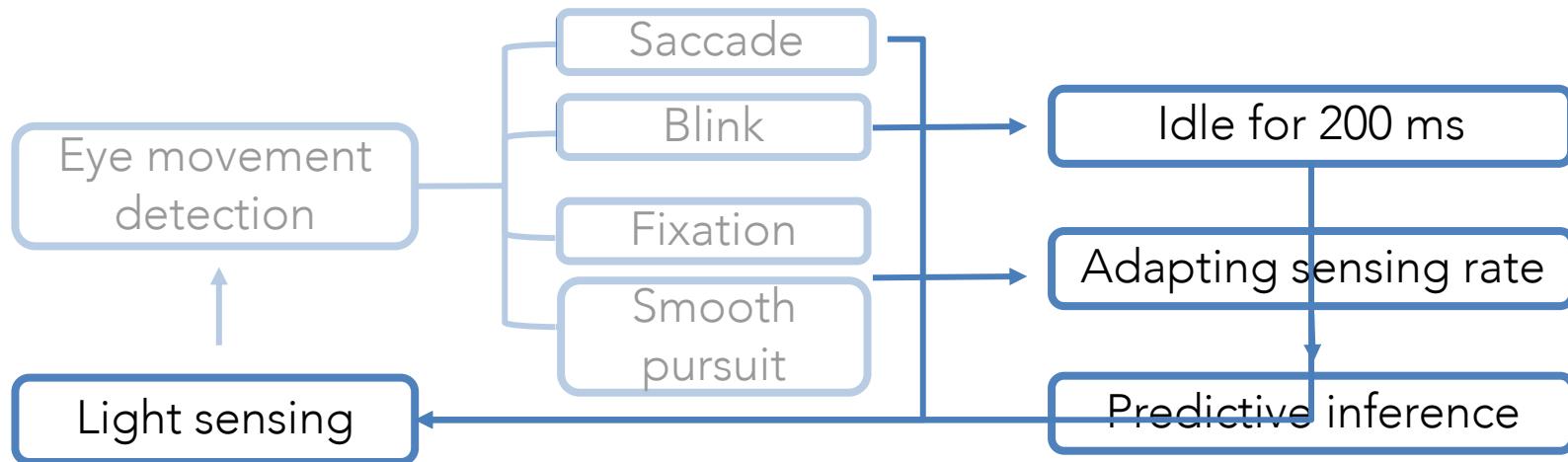
Most eye movements are predictable

- 10 x 
- 5 activities: slow reading, fast reading, watching videos, playing games, in conversation

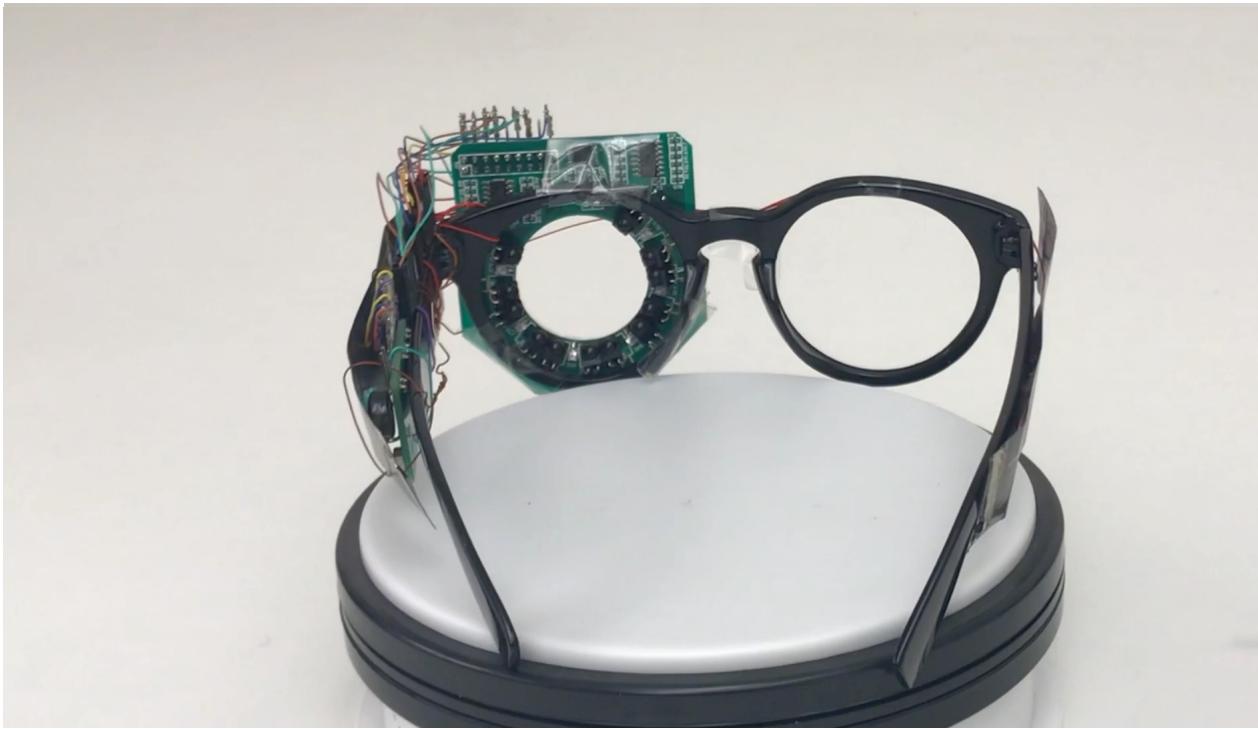




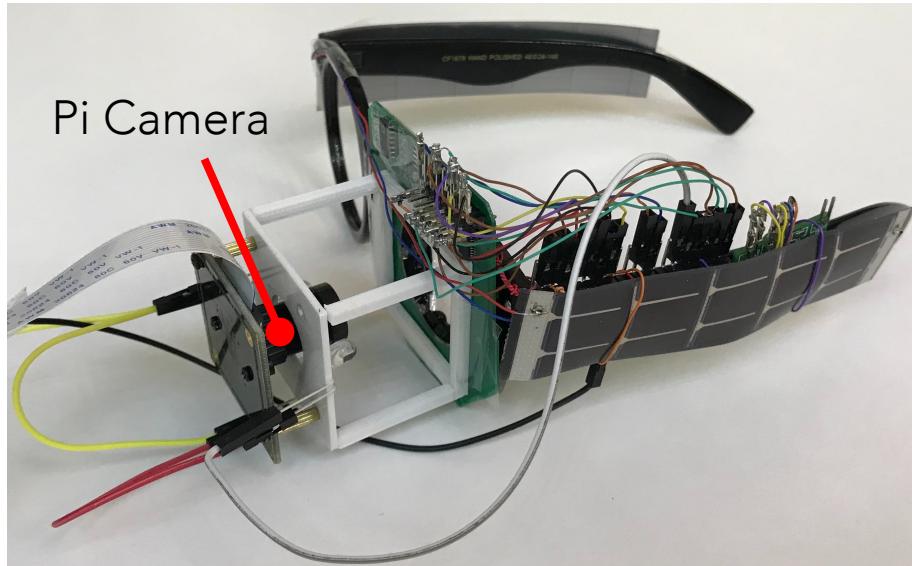
# Adaptation Based On Eye Movement



# Prototype



# Experiment Setups



Pupil Lab API + human label

- 22 x



	# of users
Eye color	Black
Skin color	Blue
	Green
	White
	Yellow
	Black

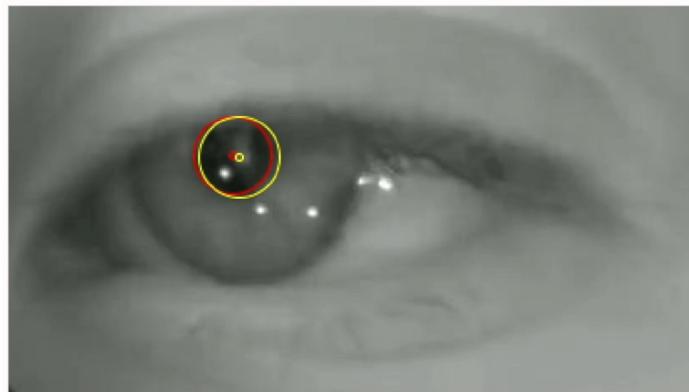
- 5-min training data
- 5 activities (10 mins each)
  - slow reading
  - fast reading
  - watching videos
  - playing games
  - conversation



## Tracking Accuracy

- Pupil position error
  - 0.8-mm mean error
  - Only 0.4 mm larger than the most accurate camera-based wearable eye tracker
- Pupil diameter error
  - 0.3-mm mean error

Eye Tracking Performance: Slow Reading



● Ground truth      ● Our system



# Energy Analysis

Avg. power consumption:  $395 \mu\text{W}$  < Avg. harvested power:  $450 \mu\text{W}$



■ Power Consumption



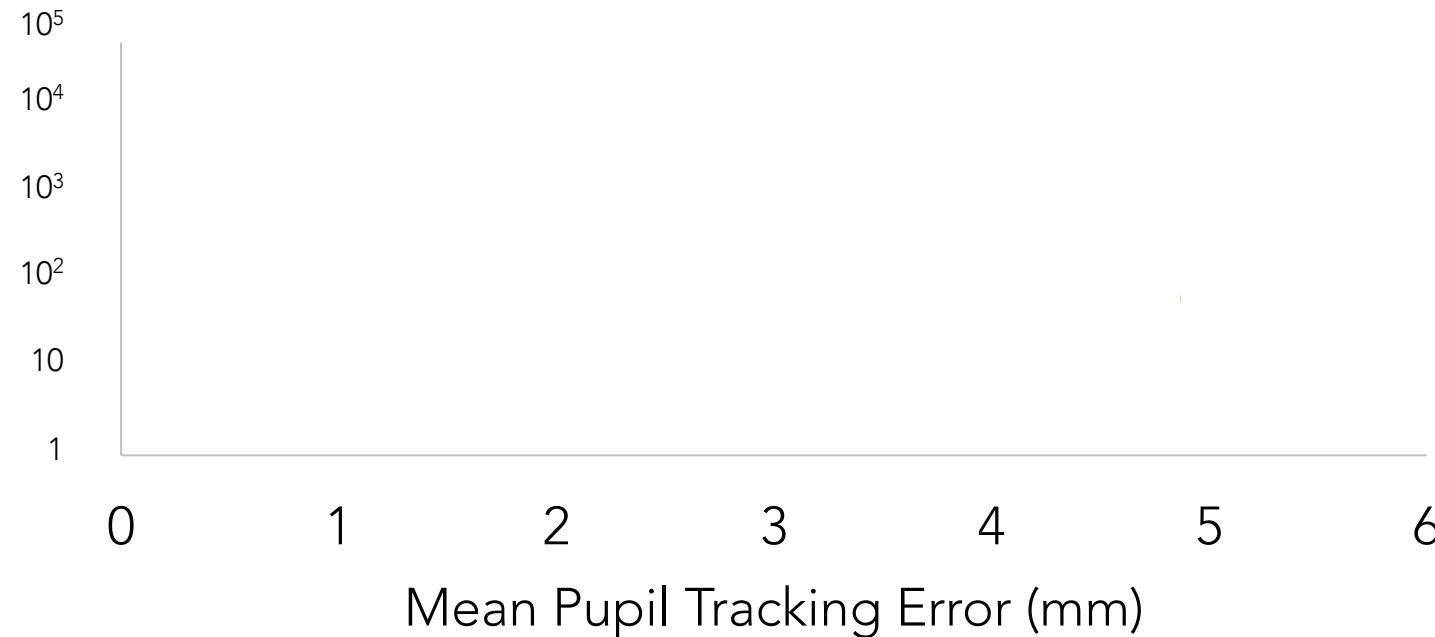
■ Power Consumption





# Our System vs. Existing Eye Trackers

Energy consumption ( $\mu\text{J}$ ) per  
gaze tracking inference





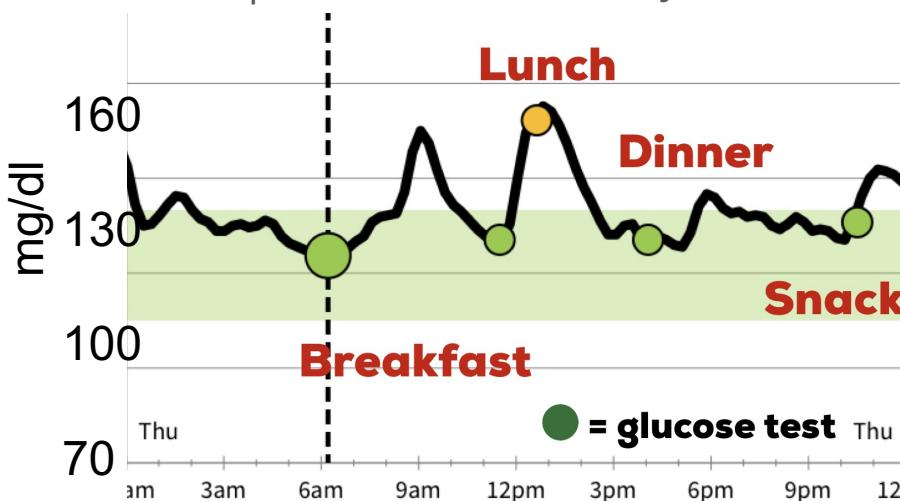
# Outline

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- Biomechanical sensing: Skeleton pose reconstruction
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# The Importance Of Glucose Monitoring

- 30+ million Americans have diabetes
- Glucose monitoring can manage diabetes conditions
  - Require > 3 times a day



- Normal: 70-140 mg/dl
- High: > 140 mg/dl
- Low: < 70 mg/dl

## Existing Method #1: Finger Pricking

😢 Painful, invasive



## Existing method #2: Continuous Glucose Monitoring (CGM)

⌚ Invasive needle



# Existing Noninvasive Glucose Monitoring

- :( Skin irritation
- :( Environmental factors



# Optical Noninvasive Glucose Monitoring

- Light absorption

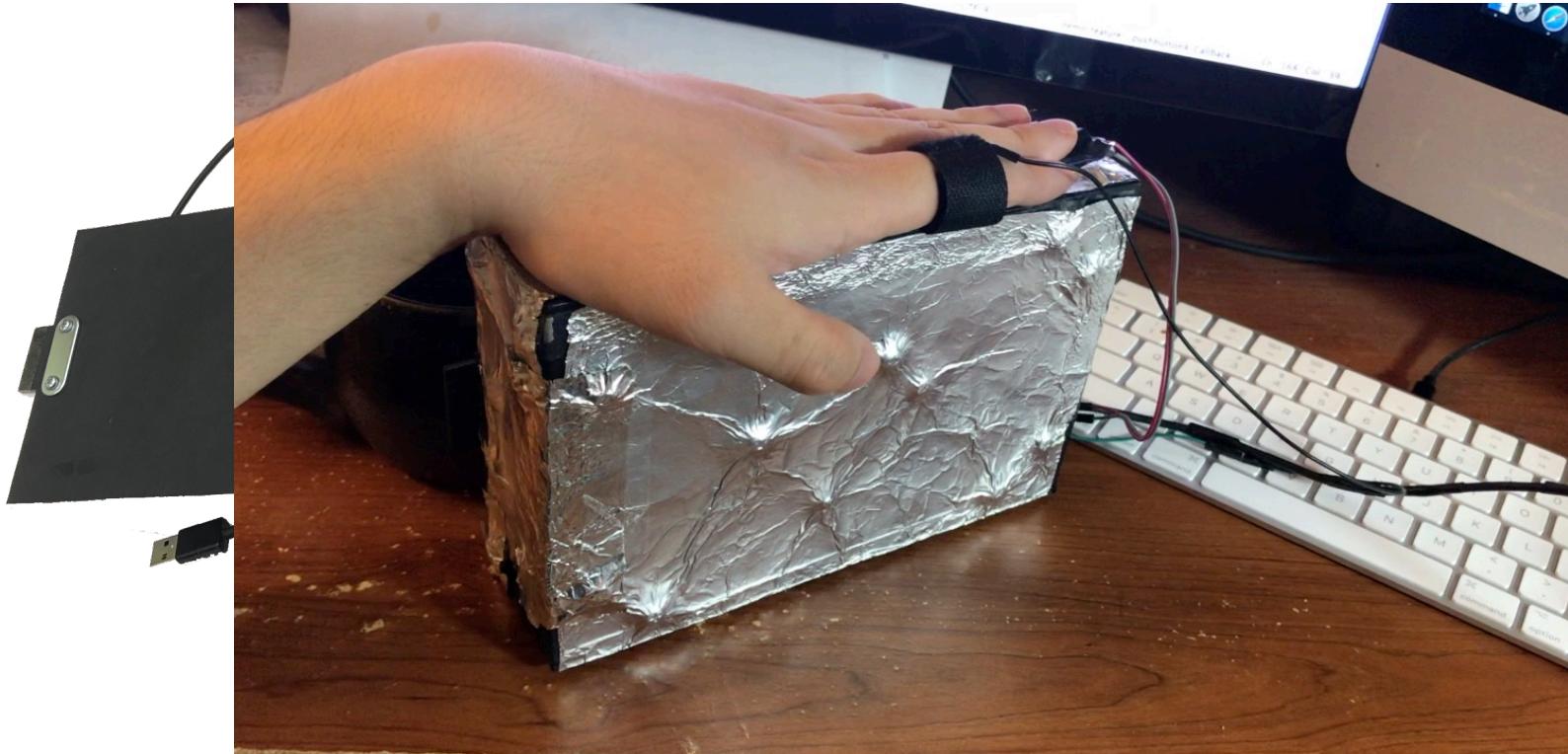


We need a noninvasive, accurate, and low-cost glucose monitoring system!

- ⌚ Expensive and bulky
- ⌚ Lacking clinical evaluations



## Prototype In Use



5 cm



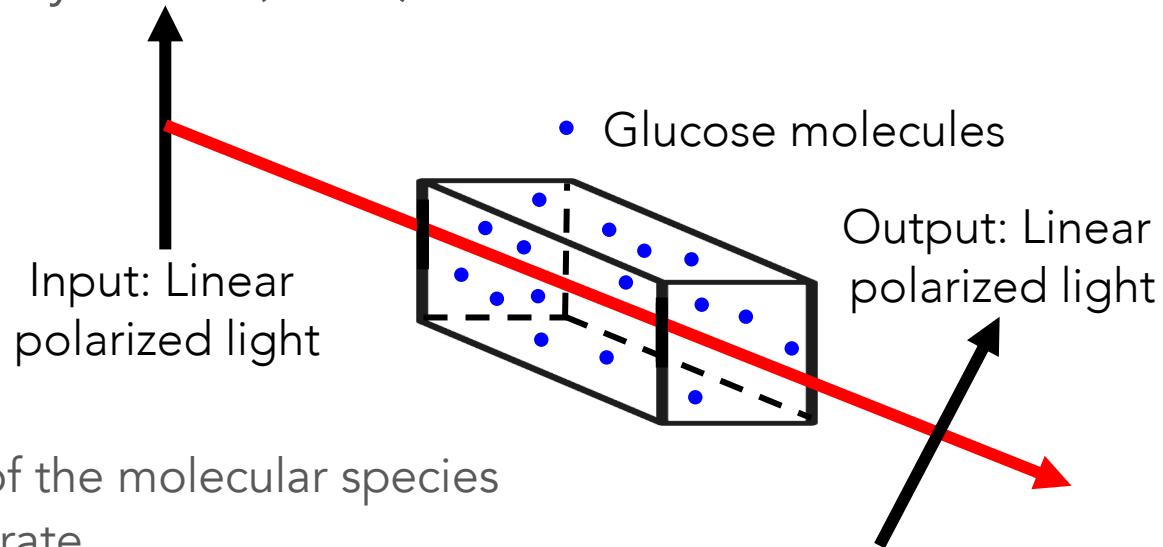
## Rationale

- Glucose is an optically active (chiral) molecule

Difficult to compute in vivo

$$\alpha = R(\lambda, T) \cdot C \cdot L$$

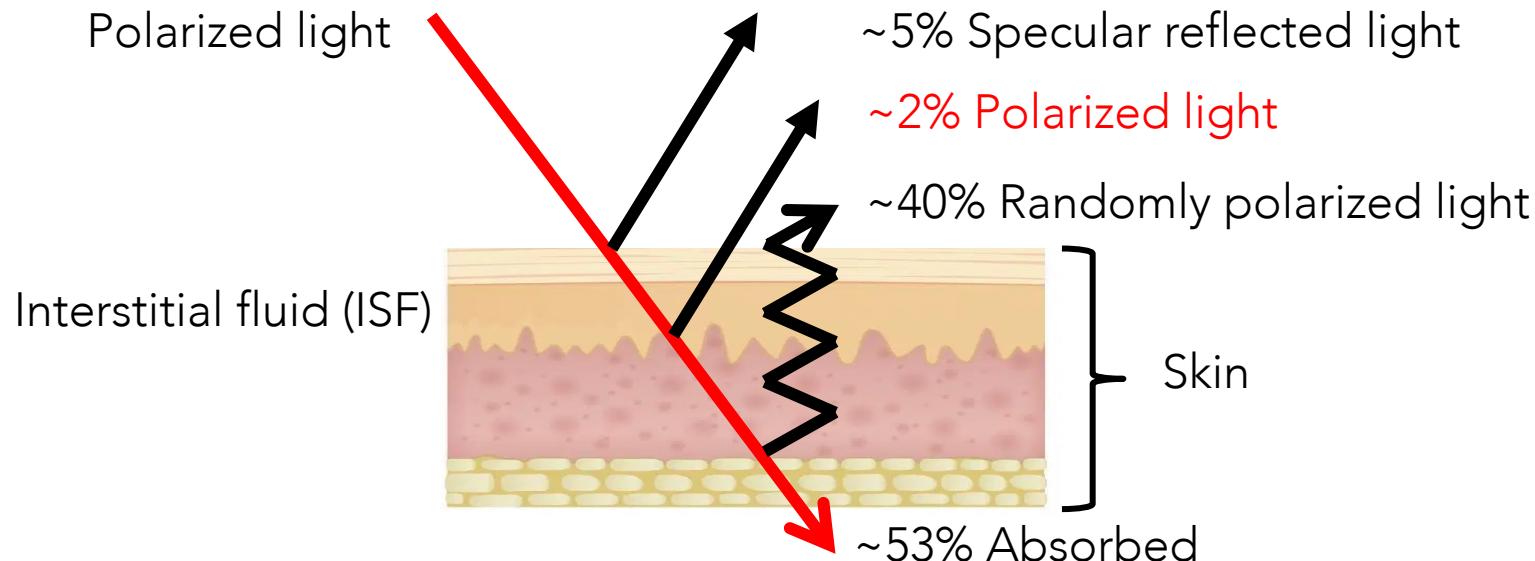
- $\alpha$ : Optical rotation
- R: Rotatory power of the molecular species
- C: Glucose concentrate
- L: Optical path





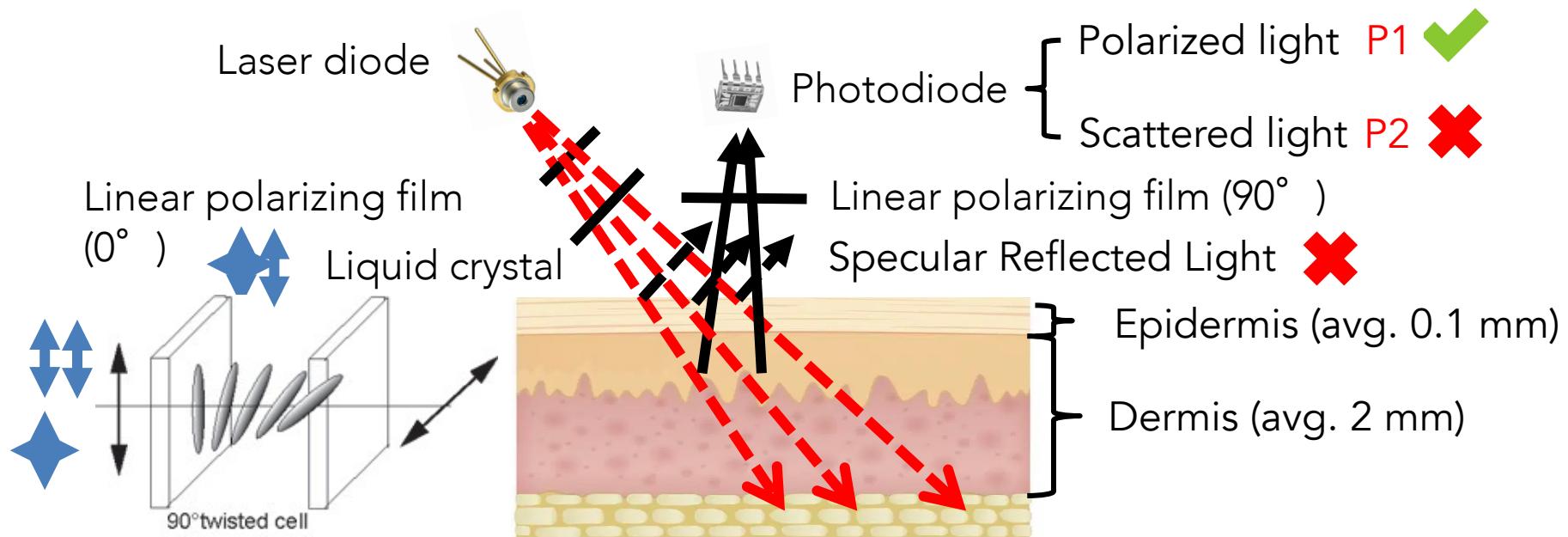
## Challenges

- #1: Skin scattering





# Sensing Changes In Light Polarization





# Experiment Setup

Liner polarizing film ( $0^\circ$ )

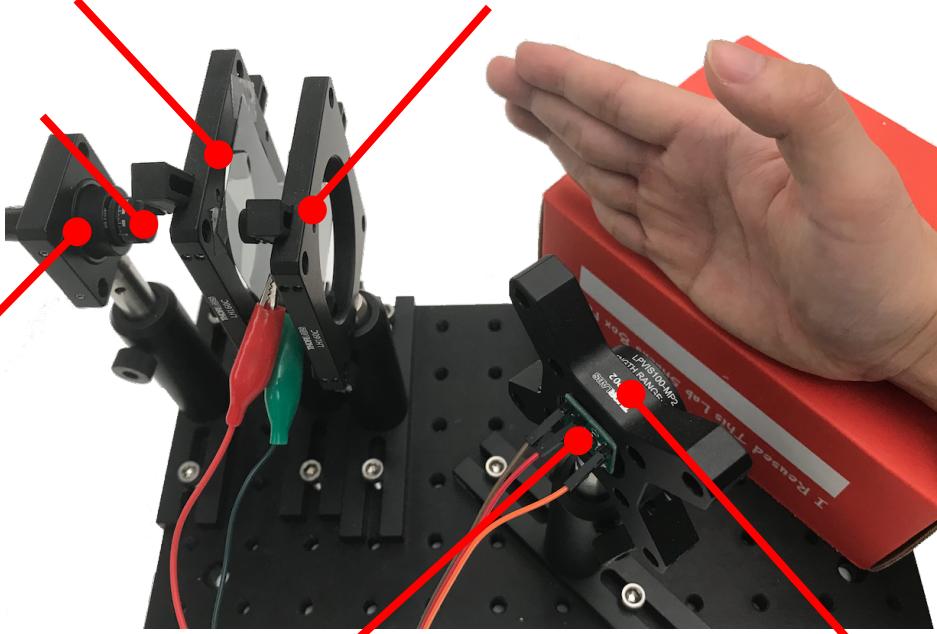
Diffuser

Red laser diode

Liquid crystal

Photodiod

Liner polarizing film ( $90^\circ$ )





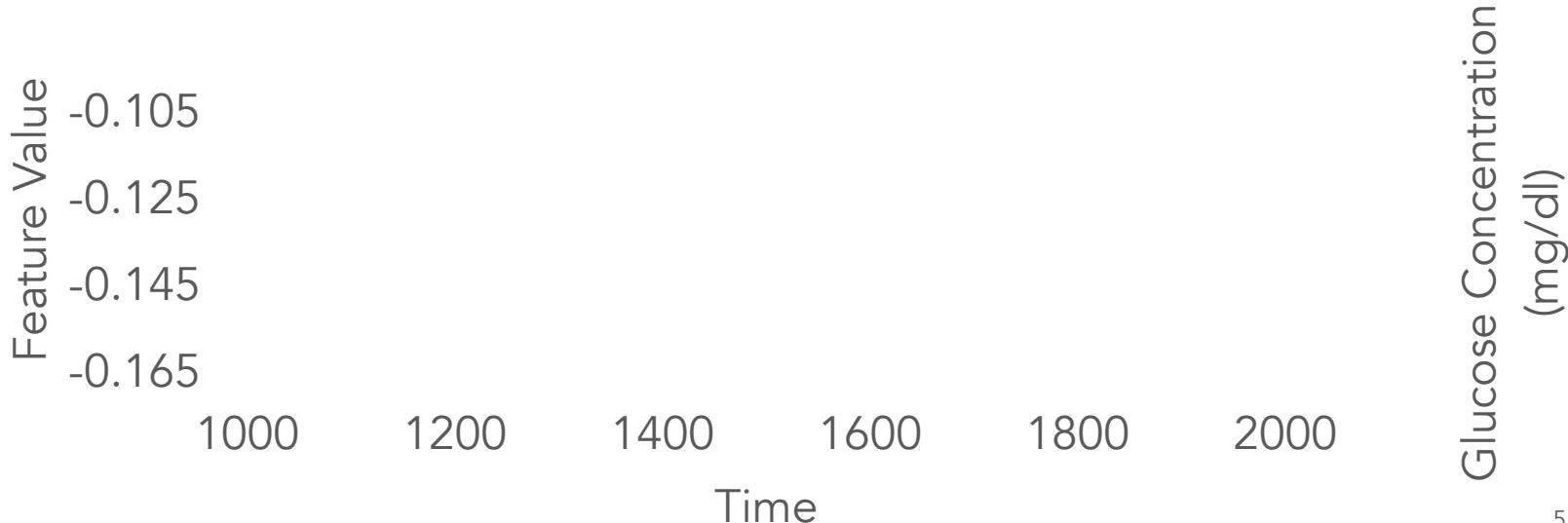
## Results

$$I_{per} = P1 + 0.5 \times P2$$

$$I_{par} = 0.5 \times P2$$

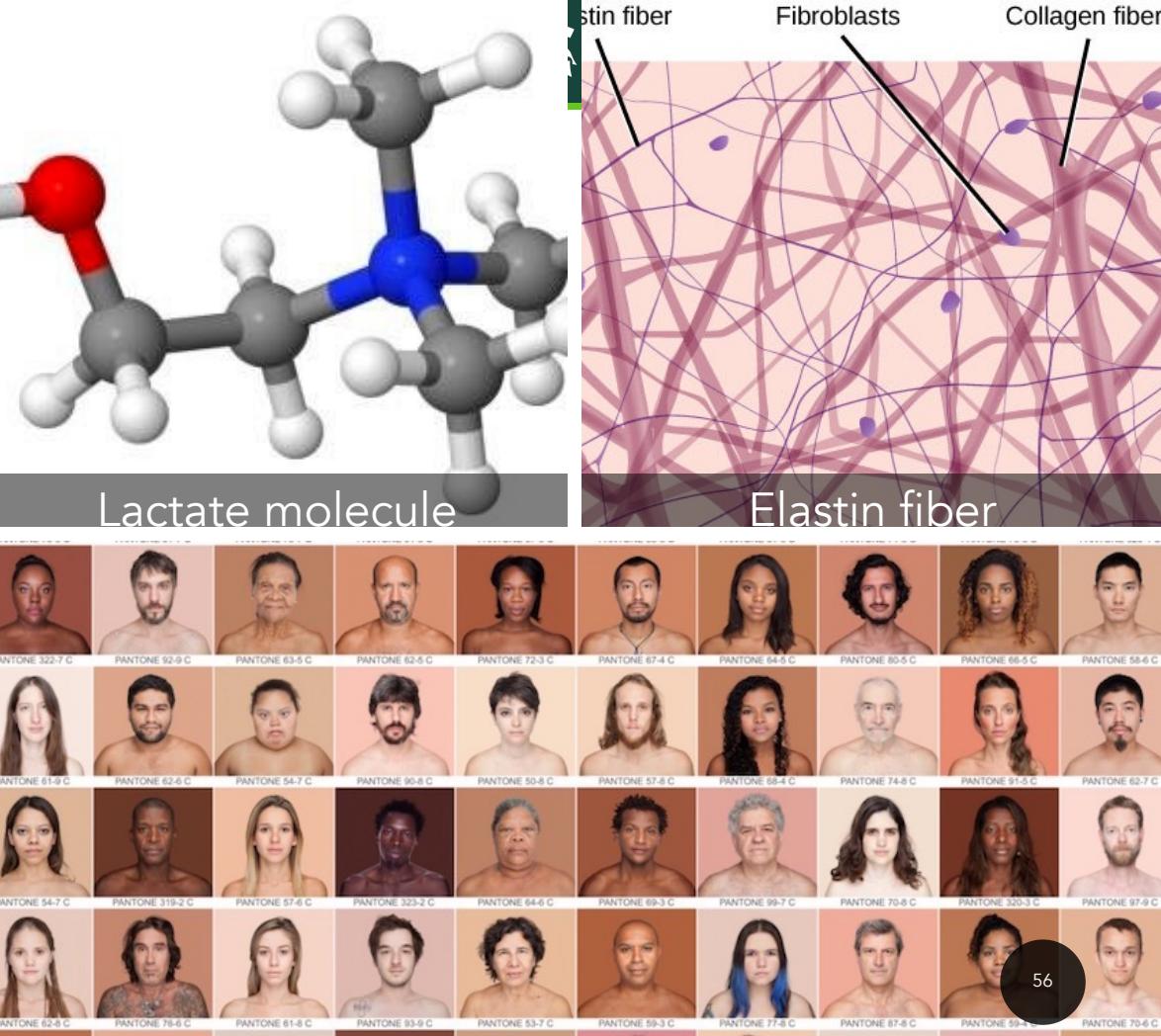
$$R = 0.86, p < 0.05$$

$$\text{Feature value} = I_{per} - I_{par}$$



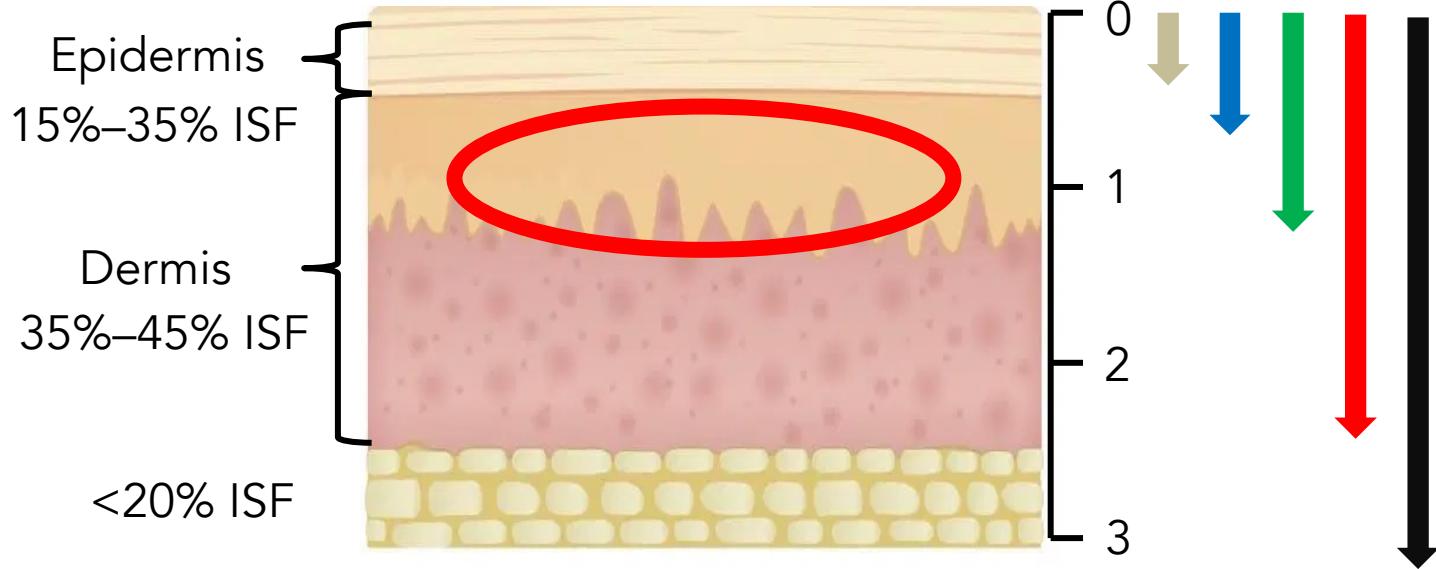
# Challenges

- #1: Skin scattering
- #2: Confound factors
- #3: User diversity





## Multiple Wavelengths & Intensity Levels

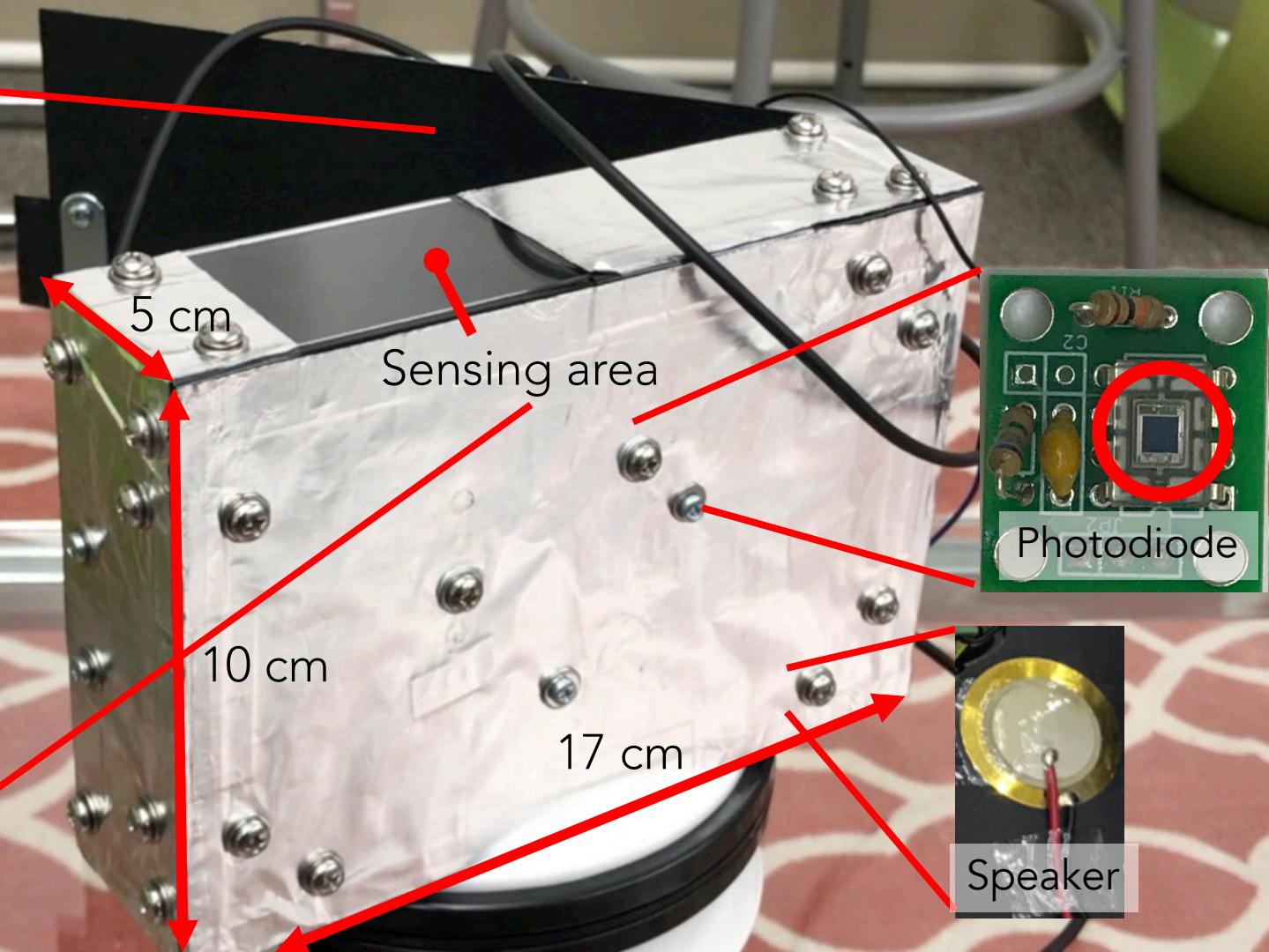
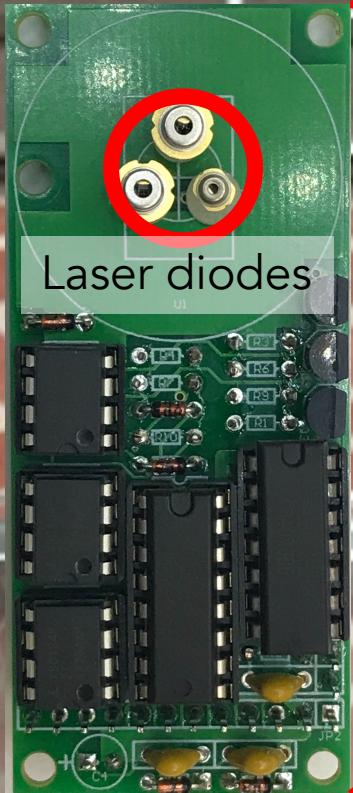




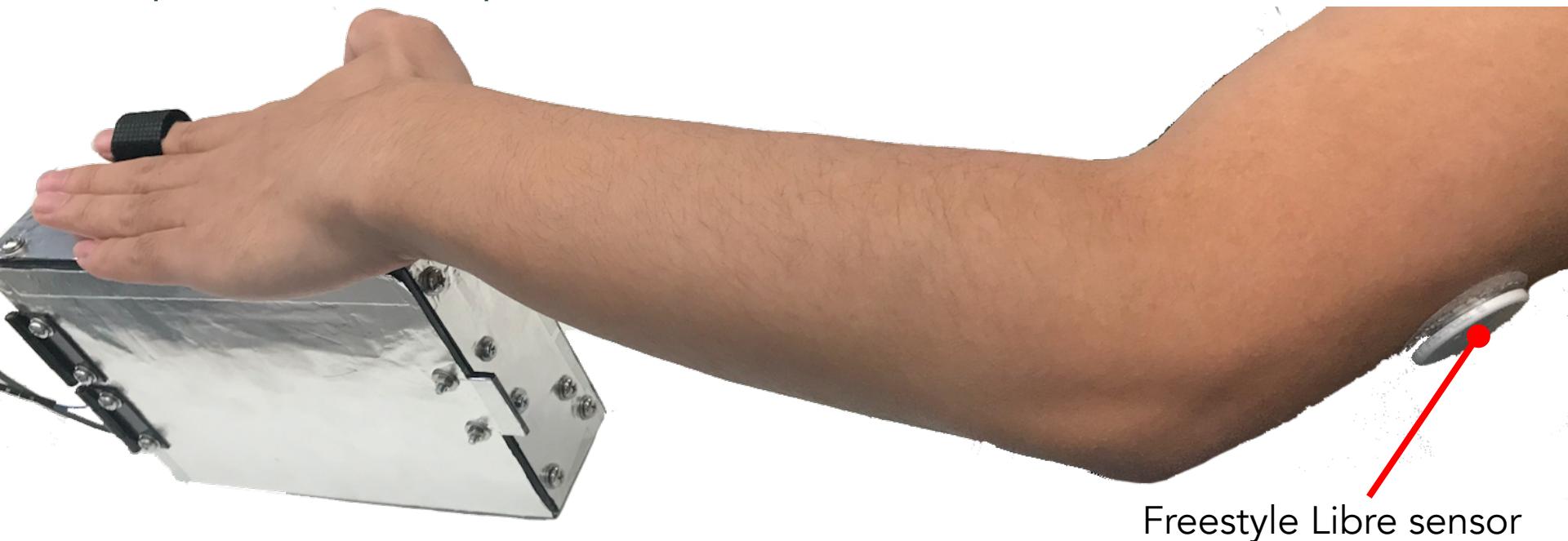
# Results

- RGB lights with 7 intensity levels (21 features)

ID	Age	Gender	Race	R	
				Single W&I	Multi W&I
1	31	M	Asian	0.86	0.86
2	23	M	Asian	0.64	0.83
3	18	M	Asian	0.6	0.78
4	24	M	Asian	0.63	0.81
5	23	F	Asian	0.65	0.74
6	23	M	White	0.71	0.75
7	25	M	African American	0.46	0.78
8	24	M	American Indian	0.51	0.74
9	33	F	Asian	0.48	0.75



## Experiment Setup

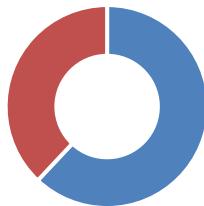




## Study Participants

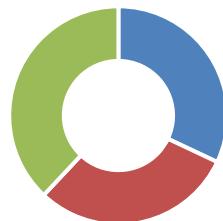
- 50 participants (41 patients and 9 healthy people)

Gender



■ Male ■ Female

Age



■ 18-30 ■ 30-50  
■ >50

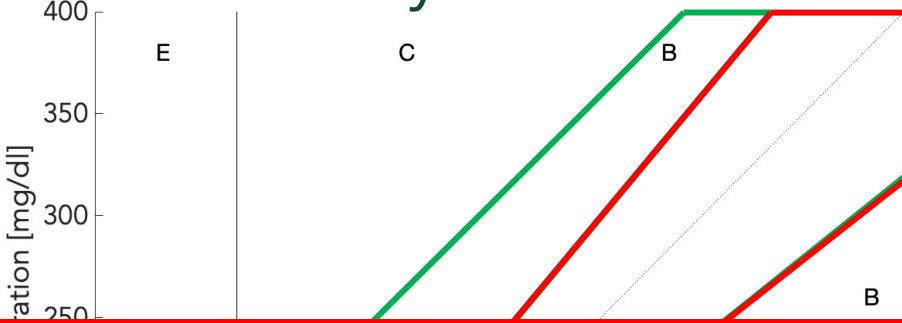
Race



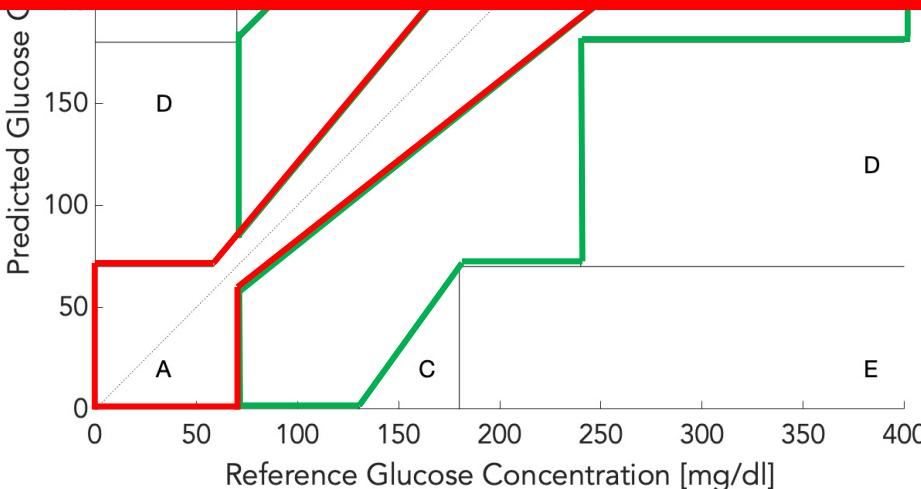
■ Asian  
■ American Indian  
■ African American  
■ Hispanic or Latino  
■ Native Hawaiian  
■ White



# Clarke Error Grid Analysis



89% of the results are within zone A





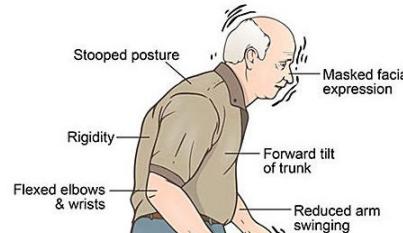
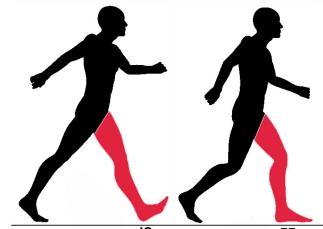
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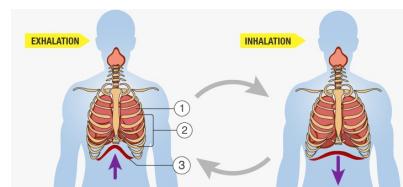


# Future Direction: Human Sensing In The Light

Biomechanical sensing



Biophysiological sensing

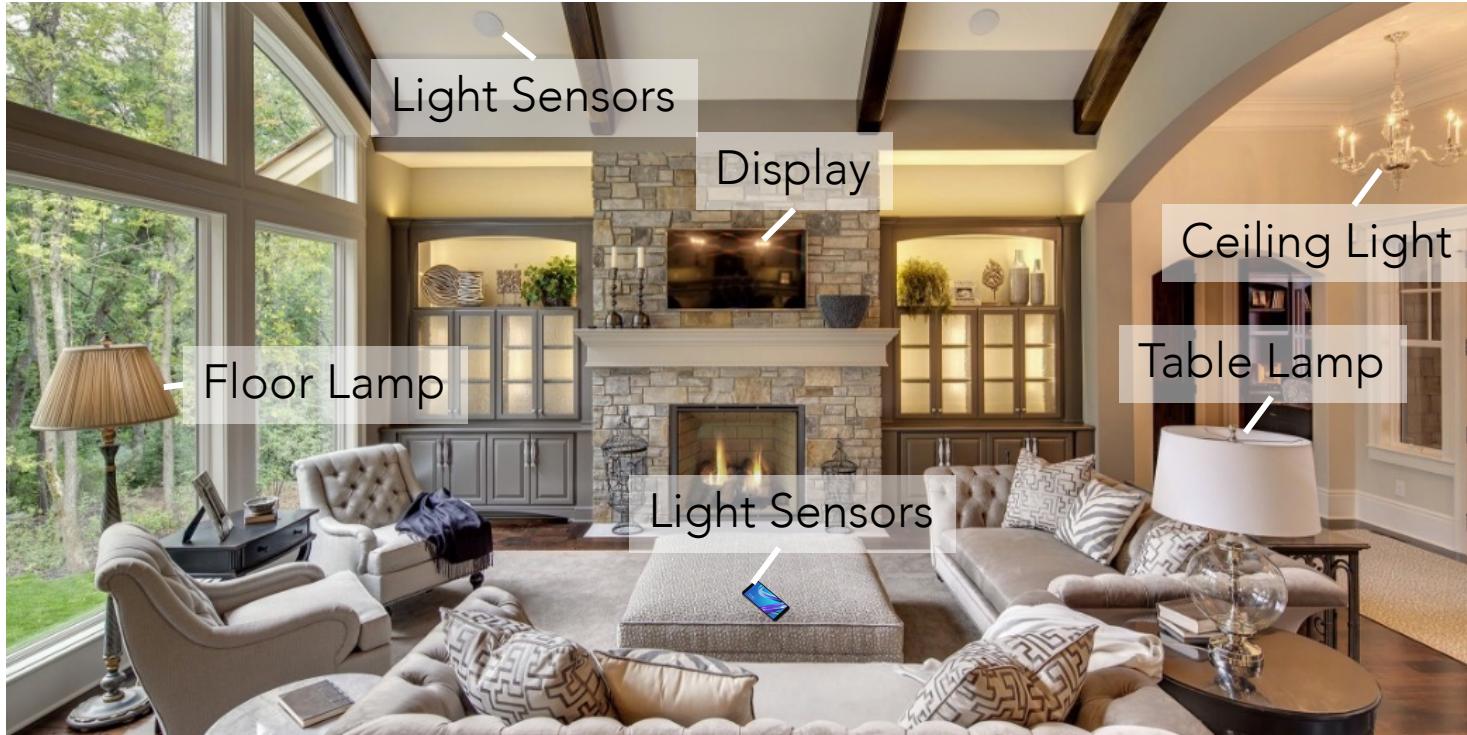


Biochemical sensing



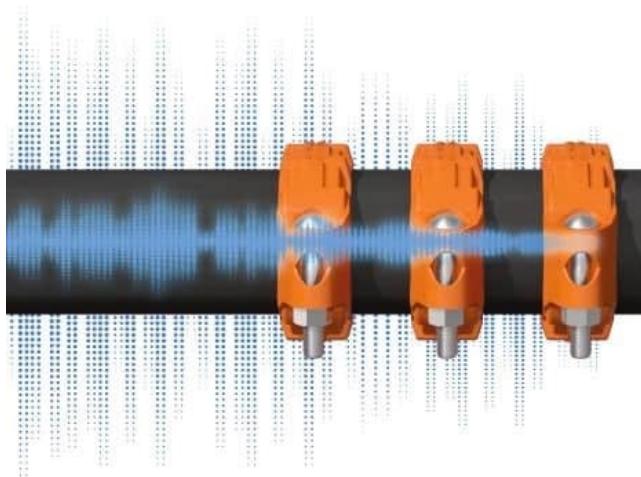


## Future Direction: Emerging Privacy and Security Risks

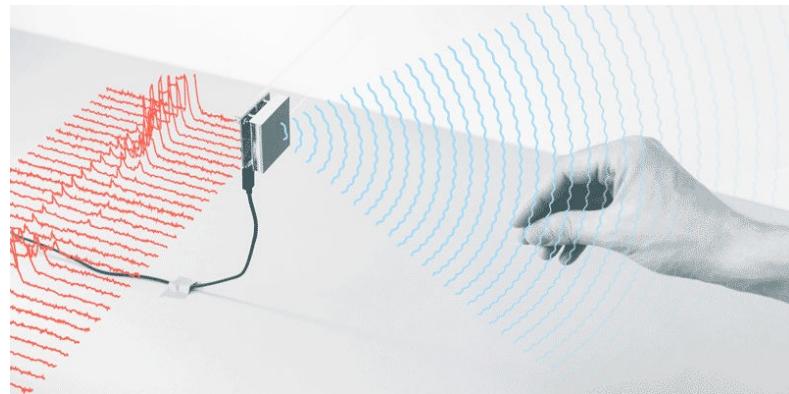




## Future Direction: Light + Other Emerging Modality For Human Sensing



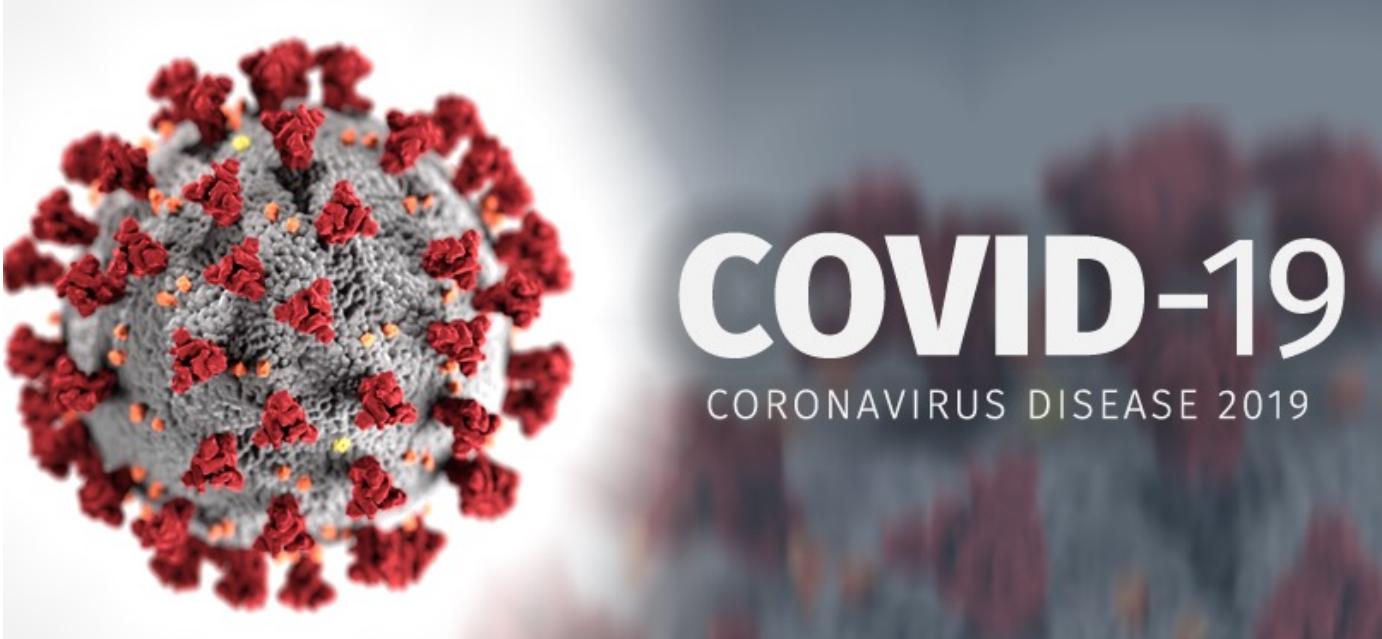
Vibration/Acoustic sensing



Mm-wave sensing



## Current projects





# Human Sensing Using Light

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