Electrical Stimulation Optimization in Bioreactors for Tissue Engineering Applications

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Abstract. We review here the current research status on bioreactors for tissue engineering with cell electrical stimulation. Depending on the cell types, electrical stimulation has distinct objectives: 1) being employed both to mimic and enhance endogenous electricity measured in the natural regeneration of living organisms and 2) to mimic strain working conditions for contractible tissues (for instance muscle and cardiac tissues). Understanding the distinct parameters involved in electrical stimulation is crucial to optimize its application. The results presented in the literature and reviewed here reveal that the application of electrical stimulation can be essential for tissue engineering applications.

Introduction

Tissue Engineering is today seen as the ultimate solution in the treatment and replacement of lost or damaged tissues. Understanding the mechanisms underlying biological tissue differentiation, regeneration and growth is a timely goal. In particular, the proper identification of the relevant parameters involved and the respective possible optimization strategies for each tissue type is a common objective in this field of research. It has been established that the following conditions should generally be satisfied:

- i) an adequate mechanical laminar shear stress of the culture medium fluid that not only ensures nutrient and oxygen delivery but removal of cell activity byproducts as well [1,2];
- ii) an adequate low voltage and low intensity electrical stimulus that both mimics endogenous real organism conditions [3-5] and selectively enhances or inhibits cell regeneration. This type of stimulus evidently plays an essential role in artificial control of cellular differentiation [6], replication [7], growth [7, 8], maturation [9], adhesion and orientation [10].
- iii) for the particular case of muscular and cardiac tissues, electro-mechanical strain stimulation mimicking the biological strain working conditions (contraction and elongation). It should be noted that the electric impulses considered in this study should not be confused with the endogenous regenerated electric fields referred in point (i), instead they refer to the functional activation of muscle and cardiac tissues of biological organisms. The scaffolds for these tissue types are commonly denominated constructs (when requiring a cell culture for construction of the scaffold) being itself constituted by biological tissues. Typically the constructs mimic the elasticity of the final biological

- tissue [11-14]. Mechanical strain alone has also been considered for cartilaginous, blood vessel and ligament tissues;
- iv) the existence of a geometric adequate substrate that mimics the final desired shape and material properties. This is commonly solved by cultivating the tissue on a biodegradable scaffold which both in vitro and in vivo shapes the tissue to the intended biological shape [15-17]. Also the geometry of these scaffolds allow for medium perfusion ensuring adequate volumetric nutrient and oxygen delivery [18-20].

Regarding materials, numerous research have proposed using both natural and synthetic materials for the design and construction of tissues, including naturally occurring polymers, synthetic bioresorbable polymers or ceramics and biodegradable materials. Examples using polycaprolactone (PCL) matrix as reference, PCL reinforced with cellulose nanofibers (CNF) and PCL reinforced with CNF and hydroxyapatite nanoparticles have been developed and used by Morouço and collaborators (see [16]). Moreover, advances have been made in exploring the ideal geometries of scaffolds [21], mostly due to 3D printing methods that have been developed over the years such as fused deposition modelling, selective laser melting or selective laser sintering techniques [22, 23]. More recently, a 4D bioprinting technology that fabricates dynamic structures that improves cartilage and bone regeneration has also been proposed [22, 24].

Different types of stimulation have been used to benefit tissue regeneration applications over the years. Mechanical, electrical and magnetic stimulation have all been explored with promising results. However, numerical studies aiming to optimize the different stimulation parameters are critically needed focusing on the vast applications of tissue engineering. Early modelling studies performed by [25] for mechanical stimulation, by [26-28] and by [29] for electrical and magnetic stimulation have proven to be not only crucial for understanding the neurophysiological mechanics involved but have also helped to optimize the application of stimulation in different type of cells and models.

With the objective of optimizing in vitro tissue engineering for eventual in vivo chirurgical implantation in such a way that it is both economically viable and scalable to industrial levels, it is highly desirable to develop bioreactors that incorporate all the necessary conditions for tissue engineering. This review will therefore mainly focus on the research status of such bioreactors which already contemplate aforementioned culture conditions (i), (ii), (iii) and (iv); specifically we will address studies that deal with the application of electrical stimulation on a scaffold placed inside a bioreactor. Furthermore, this review aims to provide insight on the different parameters involved and suggest what future directions to take.

Methods

Information sources and literature search. Studies in English quantitatively assessing the application of electrical stimulation on a scaffold placed inside a bioreactor for tissue regeneration were identified by searching the Science Direct and PubMed electronic databases on November 12, 2017. The following search string was used to retrieve relevant publications: "("bioreactor" OR "dynamic cell culture") AND ("scaffold" OR "construct") AND ("regenerative medicine" OR "tissue engineering" OR "tissue regeneration") AND (stimuli OR stimulation) AND ("electric" OR "electrical")".

Selection and exclusion criteria. The publications retrieved by using the aforementioned search string were assessed for eligibility. Notably, for an article to be included in the qualitative analysis performed in this review, the following criteria had to be met: (1) published in English, (2) original research reports – e.g., reviews were excluded and (3) used electrical stimulation applied on cells placed on scaffolds inside bioreactors corresponding to cell culture conditions (ii) or (iii).

Additionally, the following exclusion criteria were considered: (1) case studies, (2) different types of stimulation that do not include electrical stimulation and (3) when cell culture was not directly studied.

Data extraction. Relevant data were extracted systematically from the selected articles and recorded on an extraction sheet (see Table 1). This procedure was pilot-tested independently by all the authors

to ensure that data extraction occurred consistently. The extraction sheet included several topics, notably information regarding cell preparation, characteristics of the scaffolds and bioreactors and the different parameters involved in stimulation.

Identification of articles. After all data were collected, all the authors were involved in the preliminary screening of the papers, which consisted of assessing their specific titles and abstracts for eligibility. Each article was assessed by two authors. Whenever disagreement occurred, the paper was not excluded without both authors reaching an agreement on the reason for exclusion. The full-text version of the remaining articles was then assessed. This second stage eligibility screening was performed by the same authors and used the same method except for the disagreements, which were solved by joint discussions of all the authors.

Results

Study Selection. The search strategy described above resulted in 66 results from Science Direct and 14 from PubMed. After discarding duplicate records, reviews and book chapters, 21 articles were assessed for eligibility on the basis of their titles, abstracts and keywords, with 9 being excluded from the review (see Figure 1). Out of the remaining 12, which had their full text analyzed; an additional 2 papers were also excluded-due to non-inclusion of either culture conditions (ii) and (iii). The process was repeated by analyzing the full-text of the remaining 10 articles [14, 30-36, [37,38]. The characteristics of these articles most relevant to this review were collected on an extraction sheet as described above (see Table 1).

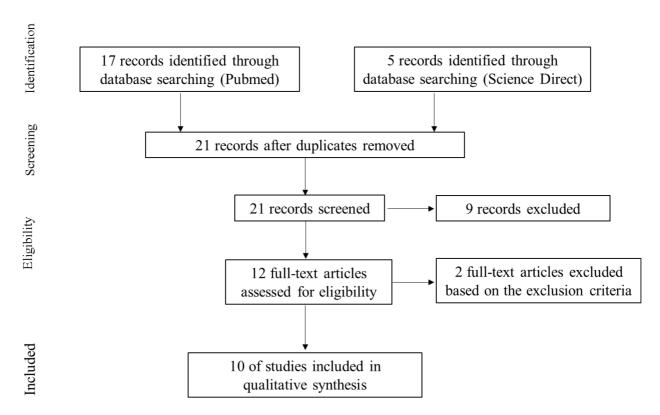


Figure 1. Flow chart diagram of the study selection process.

Characteristics of the studies. From the selected studies, [30, 37] correspond to tissue cultures applying low electrical current stimulation (ii) while the studies [14, 31-36, 38] correspond to electromechanical strain stimulation (iii).

Conclusions	Actived enhead in vico oil profression.	Smukenous perkision and semination of the semina	The bookgrabbility of the protogram between the protogram between the rapid translation of the organization with the at 2.6 y/cm.	Further duckers would be medical to studies where it decision electrical effects and effects and addressed.	In strict, the synergatic simulation state to everlate and only for the quality of cardas construct development cardas construct development but also for patients by reclaring the waiting from in future clinical scenarios.		The results include that decision that decision in mechanical decision in mechanical simulation about improved habit force on similar force assumption of simulation. Were mechanical simulation having a salationally greater final cell country in the sessue.		The research will provide some experiments from from the form future such in one plantization future such in one behaviors.	Only using saddled med debeds diffusion and addless of the second of these diffusion and diffusion and diffus
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	Geommetry Cylindrical.	isk with porosity of 78%.	Peratelippade for length with microgroose (25 x 50 ym). x (00 ym).	Paraleippdic springes (8 mm 4 (10 mm 4 1.5 mm) with microchannels for perfusion similation.	Square sloces (20 mm x 20 mm).	Paralelpipedic dices.	Clinzical	Daks.	Disks (deposited in controllips).	bedangler stape (10 mm e Am for anadisous caffed, cylerical stape O mm 30 mm) for sponge on stape sides for reactor culture.
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Cells	Outre	High glucos Dubeccrós modified Bagiés medum (DARM) suptemend with 10% Bagla borne serun (#BS).	ign-glacose DMEM 4.5 91, glacose, 4mM L- glubranne, 10% Feal Bown Serun, 10mM HEPES Buffer, and 100 rishmL pericilin and 100 pgimL steptomycin.	high-glucose DMEM + 10% Files I, We HelberS. and 1% penicilin (10,000 Unif-leagedomycin (10,000 µg/ml).	L-DMEM, 10% RBS, cardea myocyte growth supplement (Science) Research Lefter abrilding and 100 July penicilin and 100 July mategolomycin.	Juleocos moffled Eagle movement (DARA), Gaton 22201 - 10% least borne serum (FBS) + 1% pen l,étrep.	Dubeco's modified Eagle's medium, 10% hores serum, 2% least hories serum, 1% sericlin-steptomycin, M e-aminocaproto ast 2 mg/mt, insudin, and ascorbic acid, 50 mg/mt.	Pemount (ThermoFisher Scientific) medum.	high-gluose Dubecons and olded age medium [CMAI] (hydron, Ur. IGAI, 10% leist bone serun (nietagon, CA. IGAI, and 100 unstern, periodin 100 gym. Bespoonwall (hydron, Ur. IGAI) supdemented with 26 mmAI. HEPES (Sigma, MO, USA).	Merinan essential medium medium despetițiel production aupplemented with 10% FBS) (Altana Biologicale, PES) (Altana Biologicale, 2 mM Lgubarmer, 100 un'iskmi pericilin and 100 mg/ml streptomycin.
	Type of Cals Human meserchymal stromal cells (MASCs).	Cardac cells from 1-2d ay old moratal Sprague-Dawler ats.	2-day oid neonstal Sprague Dawley rat hearts (cardiomycoyles/file colasts and cardiomycoyles).	Cardos fissus 2 daty obl Sprague regiment of in the to Davidy risk cardos in viol.	Cardia cels from Lavis rat (meserch ymal stem cells).	Human atrial floods at floods colis floods at cells floods exeriment on adult rat entricular myccytes).	Carden cels from 2. to 3-day obt meanstal Sprague-Dawley rask (Cardomyocytes).	Thisliss anterior muscle from a mouse.	Rat adpose tissue- derived stromal cells (stem cells.)	Unrestricted som also human stem cells. (stem cells).
Application	Bone is sue graft (in vitro to in vivo).	Engineerd carlise tissue (in vitro).	Implantable contractile cardac tissue (in vivo).	Cardac Bsale engineering (in viro). in viro).	Gardar tis sue engineering (in vitro).	Cardac niche: myoozedun, ordomyooytes, fabrolässis, erodnielal cells (in vitro) n	Cardiac tissue bioreactor (in vitro).	Ugaments, tendons, and skdetal mus des tissue engineering (in vilro).	Stem cell alignment and modiffy (in vitro).	(in stock) Upparent regeneration (in stock). (in stock) (in stock
	References [30]	[81]	[32]	<u> </u>	[86]	[35, 39]	<u>8</u>	[14]	[38, 41]	[37, 40]

Types of cell tissues. As for the cell types considered in each of the selected references, six studies deal with cardiac tissue engineering [31-36, 38], one with bone tissue engineering [30], one with muscle/ligament/tendon tissue engineering [14] and two with stem cell tissue engineering, [38]. Regarding the objective of generic cell differentiation, Dodel and his collaborators (see [37]) explicitly show that differentiation into ligament tissue requires electrical stimulation. In all these studies, it has been shown experimentally that the electrical stimulation and electro-mechanic stimulation is beneficial to the cell culture with respect to the control cultures without any electrical or mechanical stimulation. The interpretation is therefore common among all these studies, the stimuli mimic the natural organism conditions of tissues. In particular the cardiac tissue is naturally strain stimulated in living organisms as well as muscle, ligament and tendon tissues. We highlight the study [36] where electric strain, mechanical strain and both electro-mechanical stimulations are compared for cardiac tissue with the conclusion that electro-mechanical strain with electric stimulation when delayed with respect to the mechanical stimulation is the more beneficial stimuli for cell health. Not surprisingly this is indeed the stimulation that more closely resembles the working conditions of cardiac tissue in living organisms.

Scaffold Characteristics. The scaffolds employed in the reactors are commonly made out of a mixture of both non-biological and biological cell tissues (synthesized and/or natural). The biological components range from generic components as collagen [30, 33], chitosan [37, 38], collagen-chitosan hydrogels [32, 38], poly(glycerol sebacate) [31] and poly(l-lactic acid) [38] to specific tissues adequate as substrate for each target cell culture. These tissues range from fresh pig hearts [34] (cardiac), human umbilical vein endothelial cells [35] (cardiac), rat hearts [33, 36] (cardiac) to adipose-derived stem/stromal cells [14] (ligament differentiation). The non-biological components for the scaffolds are commonly polymers as discussed in the introduction.

Synthetic scaffolds were employed in [30-32, 37]. When required to have a cell culture for the construction of the scaffolds, these are typically denominated as constructs [33-36, 14, 38]. The fabrication process employed includes cell culture after mixture/deposition in the base substrate [33-36, 38] and electrospinning [14, 37].

The specific shape of the scaffolds depend on the application: [31-35] considered parallelipipedic / square slices, [36, 37] considered cylindrical, and finally [14, 38, 37] considered disk shaped scaffolds.

Bioreactor. Each bioreactor has distinct objectives while in [31, 34-36, 14, 38] cell culture was studied strictly in vitro, in [32] cell culture was studied strictly in vivo, in [30, 33] the goal was to study the viability and optimization of the transfer of in vitro cell culture to living organisms. In particular [30] suggest a bioreactor that enhances cell proliferation in vivo and in [33] it is shown that mechanical perfusion and electrical stimulation in vitro prior to transference of cell cultures to living organisms improves cell survival rate in vivo.

The geometry of the reactors considered in the selected studies is typically either cylindrical [30-32, 36] or parallelipipedic [33-35, 14, 38, 37] (see [39] for detailed description of [35]). When considering mechanical strain stimulation, servo actuators are typically employed [34-36, 14]. As for the electrical electrodes, composition involves either -gold [30] (wire of diameter 300um forming a pattern of 12mm by 3mm), carbon [31-33, 35, 36] (rods with diameter ranging from 0.5mm to 5mm), silver [34] (wire of 75µm diameter), stainless steel [38, 37] (rods of diameter 1.4mm, described in [40]) and salt bridges [38] (square agar bridges, the actual electrode is a carbon rod, described in [41]). It is relevant to note that the direct insertion of electrodes in the culture medium may induce ionization depending on the specific value of the voltage and current intensity. As this is undesirable for the cell culture, one possible solution is to consider salt bridges between the actual culture medium and independent recipients where the actual electrodes are immersed (see for instance [5] and references therein), being [38] the only selected bioreactor study that actually employed salt bridges. Typically for electro-mechanical strain stimulation the electrodes are in direct contact with the culture

medium (through the reactor wells when present) [30-33, 35-37] or in direct contact with the cells/scaffold [34, 14].

Stimulation. Studies included in this review show that different stimulation parameters seem to play a key role on cell differentiation, regeneration and growth. Scaffold stiffness (Young's modulus) and electric resistivity: Laminar shear stress and perfusion mimicking the volumetric biological vascular systems. Also important is understanding the adhesion of cell cultures and its biodegradability. The geometry and topology of the scaffold is also crucial in the optimization of stimuli application [21, 23]. We highlight the two different types of stimulation that are mostly used and the main parameters involved:

- i) Mechanical stimulation: amplitude, frequency and pulse shape, periodicity on/off during culture time and synchronization with respect to electrical stimulation were the main parameters involved;
- ii) Electrical stimulation: electrodes characteristics like shape, dimensions and spacing between electrodes varied according to the different applications studied [30-33, 35-38]. Additionally, electric voltage and intensity, frequency and pulse shape, periodicity on/off during culture time and synchronization with respect to mechanical stimulation (when present) are parameters that have been shown to influence the results of electrical stimulation [32, 38].

Discussion

In this review paper we report in detail the influence of applying electrical stimulation on cells placed on a scaffold inside a bioreactor. Most of the papers in the literature to-date have used only mechanical stimulation. However, recently, some studies have shown the advantage of using different types of stimulation, such as, electrical or magnetic either in isolation or in combination [29, 42-44]. In order to understand the neurophysiology of the underlying mechanics, an in-depth study of all stimulation parameters involved should be performed. Initially our plan was to consider both numerical and experimental studies. However after searching on Science Direct and PubMed for relevant papers that address an updated string (the original string with addition of the keywords: simulation, numerical and modelling), we did not find any paper addressing the use of computational simulation to optimize the stimulation parameters. Therefore we decided to focus only on the experimental results. Here, we are mainly interested in understanding which type of parameters have been used for the different tissue engineering applications and possible optimizations on designs, protocols and stimulation parameters that may increase cell differentiation, growth, proliferation and survival rate. It was also possible to conclude that different electrode characteristics were considered empirically for the different applications, for instance, either they were emerged in the medium orthogonally to the scaffold or horizontally aligned with the scaffold. Additionally, electric voltage and intensity, frequency and pulse shape, periodicity on/off during culture time and synchronization with respect to mechanical stimulation (when present) are parameters that have been shown to influence the results of electrical stimulation [32, 38].

Once the relevance and optimization of the physical parameters for each stimulus is experimentally measured, numerical simulations can significantly reduce experimental time and costs [44]. In particular the optimal topologies and configurations of bioreactors can be investigated by numerical simulations prior to new experimental setups. For instance, Pereira et al., show numerically the importance of choosing the adequate mechanical stimuli parameters to improve shear stress value and fluid flow on the scaffold. Further, other numerical studies have investigated the influence of mechanical stimulation on the growth and distribution of cells on scaffolds and tissue differentiation [45-48].

Additionally, the developed bioscaffolds are usually tested and studied in vivo, presenting a significant expensive option thereby necessitating the development of numerical approaches. Therefore computational studies are of paramount importance to optimize the direct digital

manufacturing of scaffolds that can be produced using different geometries, geometry gradients, topologies and also different materials.

Finally, we note that the low number of bioreactor studies including (i), (iii) and (ii) or (iv) reflects both the complexity and multidisciplinary nature of the research field as distinct conditions are required for each organic tissue and the multitude of scaffold materials and respective construction process. It is relevant to note that no studies including both regenerative electrical stimulation and electro-mechanic strain stimulation have been found, it is however expected that further enhancement for contractible tissues may be expected by considering both these stimulations.

Conclusions

Only few studies were found that focus on the application of electrical stimulation on cells placed on a scaffold inside a bioreactor. The results are promising when using an electrical stimuli and also when combining it with mechanical stimulation. An increase in cell proliferation and density was observed as well as an enhancement in tissue morphology. Additionally, further studies must be performed where stimuli responsive scaffolds are used enabling a better cell proliferation, differentiation or tissue growth. This can be achieved through the combination of different types of stimuli to optimize both the response of the intelligent scaffold and cells behavior. Numerical studies can play here a key role to optimize all the stimulation parameters involved and predict cell response which can lead to a reduction of experimental time and costs.

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