

# 3D Arterial Segmentation via Single 2D Projections and Depth Supervision in Contrast-Enhanced CT Images

## Supplementary Material

Table 1: **Data augmentation and input preprocessing during training.** The input volume  $V$  is pre-cropped to  $(300, 300, 150)$  around the ostia of the superior mesenteric artery.

| Transformation        | Parameters                                      | Probability |
|-----------------------|---|-------------|
| Rescale               | $[0, 1]$  | $p = 1$     |
| Gaussian blur         | $\sigma \in [0, 2]$                             | $p = 0.75$  |
| Gamma change          | $\lambda \in [-3, 3]$                           | $p = 0.75$  |
|                       | scaling $s \in [0.8, 0.2]$                      | $p = 0.9$   |
| Affine transformation | rotations of up to $15^\circ$                   | $p = 0.9$   |
|                       | translation of up to $(30, 30, 3)$ in each axis | $p = 0.9$   |
| Crop volume           | from $(300, 300, 150)$ to $(256, 256, 128)$     | $p = 1$     |

Table 2: **Processing operations for different stages of our pipeline:** rib extraction, maximum intensity projection of the input, and postprocessing of the depth maps. •  $M_{y_1|y_2} \in \mathbb{R}^{300 \times 300 \times 150}$  denotes a cropping mask  $M(x, y, z) = 1$  if  $y < y_1$  or  $y > (300 - y_2)$ , else 0. •  $V * C_a \leq b$  denotes a convolution operation of a volume  $V$  with a cube of size  $a$ , followed by a thresholding operation at threshold  $b$  and re-binarization.

| Stage          | Operation   | Parameters  |
|----------------|---|---|
| Rib extraction | threshold and binarize                                | $V < 300 \rightarrow 0, \quad V \geq 300 \rightarrow 1$                   |
|                | connected components (CCs)                            | connectivity of 6 (no diagonal pixels)                                    |
|                | mask out  | CCs smaller than 100000 pixels  |
|                | mask out  | CCs $c$ where $\exists(x, y, z) \in c$ such that $M_{80 30}(x, y, z) = 0$ |
|                | binary dilation                                       | structuring element: cube of size 5                                       |
| Input MIP      | apply mask  | ribs, vertebrae, $M_{80 100}$   |
|                | clip volume   | $[150, 255]$  |
|                | crop volume   | $(256, 256, 128)$   |
|                | rotate: Euler angles $(\alpha_x, \alpha_y, \alpha_z)$ | $(0, 0, 0)$ , $(-90, 0, 0)$ or $(0, 0, -90)$                              |
|                | resample  | $(256, 256, 128)$   |
|                | rescale   | $[150, 255] \rightarrow [0, 255]$   |
| Depth map      | maximum intensity projection                          | y axis  |
|                | compute depth map                                     | intensity fluctuation $th = 0.1$<br>(Step 3 of depth map generation)      |
|                | remove disconnected pixels                            | $D * C_3 \leq 1$  |
|                | remove very sparse areas                              | $D * C_{11} \leq 9$   |

Table 3: **Ablation experiment on training with fixed viewpoints (VPs)**. We train models using 2D projections on **fixed** viewpoints (same for each training sample). The 3 viewpoints considered are: coronal projection  $\rightarrow c$ , axial projection  $\rightarrow a$ , sagittal projection  $\rightarrow s$ . Each experiment is averaged over 5 cross-validation folds in accordance with our experimental design.

| # VPs | Viewpoints | Dice              | Precision         | Recall           | Skeleton Recall  | MSD             |
|-------|------------|-------------------|-------------------|------------------|------------------|-----------------|
| 3     | $c, a, s$  | $90.78 \pm 1.30$  | $90.66 \pm 1.30$  | $91.18 \pm 3.08$ | $81.77 \pm 2.13$ | $1.16 \pm 0.13$ |
| 2     | $c, a$     | $88.97 \pm 1.11$  | $85.26 \pm 1.72$  | $93.43 \pm 1.35$ | $83.78 \pm 2.15$ | $1.22 \pm 0.09$ |
|       | $a, s$     | $91.01 \pm 0.65$  | $90.20 \pm 2.70$  | $92.14 \pm 2.09$ | $81.56 \pm 2.91$ | $1.13 \pm 0.05$ |
|       | $c, s$     | $90.68 \pm 0.44$  | $89.03 \pm 0.95$  | $92.64 \pm 0.96$ | $81.20 \pm 1.16$ | $1.07 \pm 0.03$ |
|       | avg        | $90.22 \pm 1.19$  | $88.16 \pm 2.86$  | $92.74 \pm 1.63$ | $82.18 \pm 2.47$ | $1.14 \pm 0.09$ |
| 1     | $c$        | $77.59 \pm 1.91$  | $68.15 \pm 2.76$  | $91.17 \pm 3.04$ | $79.89 \pm 1.69$ | $2.18 \pm 0.21$ |
|       | $a$        | $32.82 \pm 23.33$ | $24.61 \pm 23.13$ | $92.44 \pm 3.45$ | $80.73 \pm 2.39$ | $4.38 \pm 5.17$ |
|       | $s$        | $71.86 \pm 3.62$  | $58.66 \pm 4.99$  | $93.94 \pm 1.91$ | $82.94 \pm 1.91$ | $2.32 \pm 0.27$ |
|       | avg        | $60.76 \pm 24.14$ | $50.47 \pm 23.21$ | $92.52 \pm 3.09$ | $81.19 \pm 2.39$ | $2.96 \pm 3.15$ |

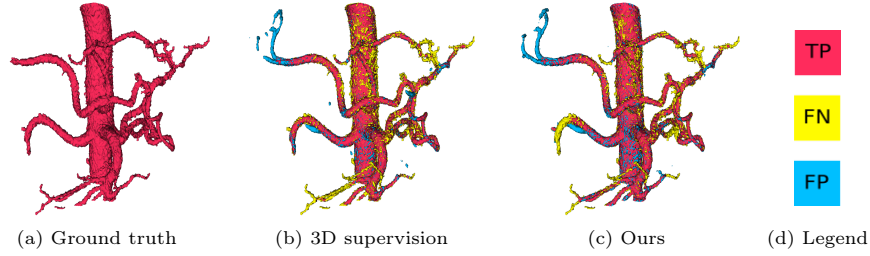


Fig. 1: **Qualitative results**. 3D rendering of the predicted segmentation of one of our models (c) compared to a model trained using full 3D supervision (b).

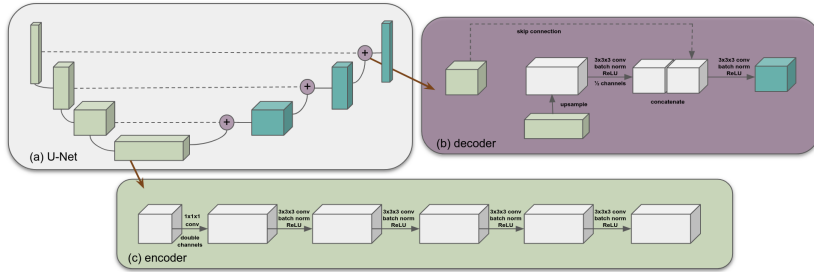


Fig. 2: **Network architecture** Our U-Net has 4 layers. Between each encoder layer we perform a  $2\times$  max pooling operation and double the output channels. The number of output channels at each layer are: 16, 32, 64, 128.