

Module 12:

Model Building I

General Linear Model

A standard GLM can be written:

$$\mathbf{Y} = \mathbf{X}\boldsymbol{\beta} + \boldsymbol{\varepsilon} \quad \boldsymbol{\varepsilon} \sim N(\mathbf{0}, \mathbf{V})$$

where

$$\begin{bmatrix} Y_1 \\ Y_2 \\ \vdots \\ Y_n \end{bmatrix} = \begin{bmatrix} 1 & X_{11} & \cdots & X_{1p} \\ 1 & X_{21} & \cdots & X_{2p} \\ \vdots & \vdots & & \vdots \\ 1 & X_{np} & \cdots & X_{np} \end{bmatrix} \times \begin{bmatrix} \beta_0 \\ \beta_1 \\ \vdots \\ \beta_p \end{bmatrix} + \begin{bmatrix} \varepsilon_1 \\ \varepsilon_2 \\ \vdots \\ \varepsilon_n \end{bmatrix}$$

fMRI Data

Design matrix

Model parameters

Noise

V is the covariance matrix whose format depends on the noise model.

The quality of the model depends on our choice of X and V.

Model Building

- Proper construction of the design matrix is critical for effective use of the GLM.
- This process can be complicated by the following properties of the BOLD response:
 - It includes low-frequency noise and artifacts related to head movement and cardiopulmonary-induced brain movement.
 - The neural response shape may not be known.
 - The hemodynamic response varies in shape across the brain.

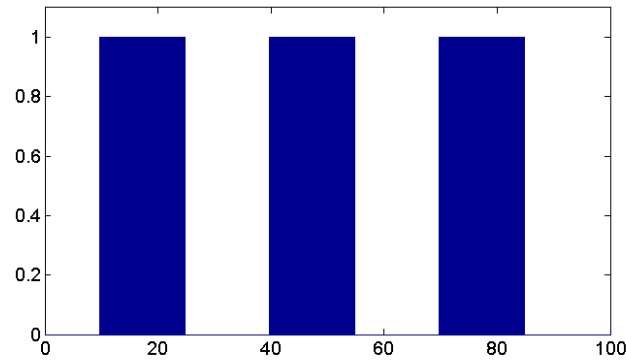
BOLD Response

- Predict the **shape** of the BOLD response to a given stimulus pattern. Assume the shape is known and the **amplitude** is unknown.
- The relationship between stimuli and the BOLD response is typically modeled using a **linear time invariant (LTI) system**.
- In an LTI system an **impulse** (i.e., neuronal activity) is convolved with an **impulse response function** (i.e., HRF).

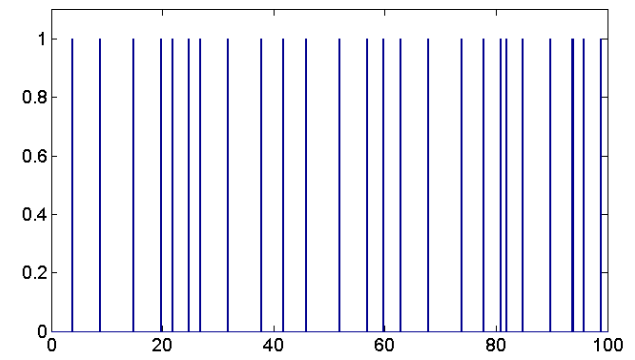
Convolution Examples

Experimental
Stimulus Function

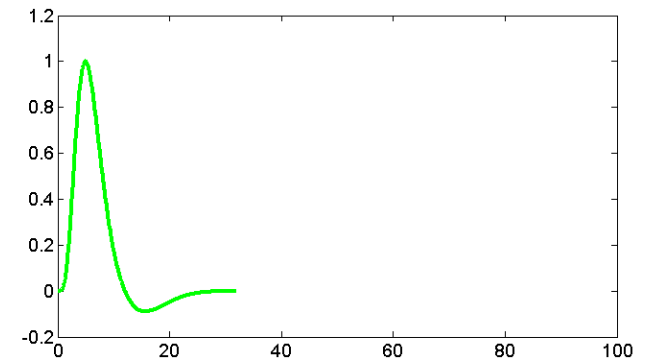
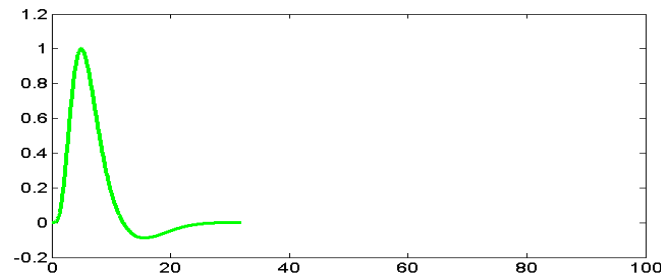
Block Design



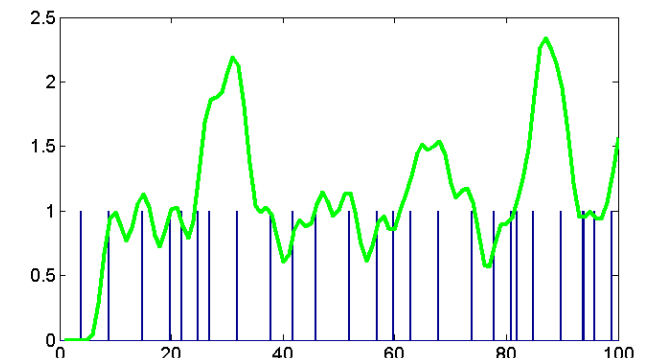
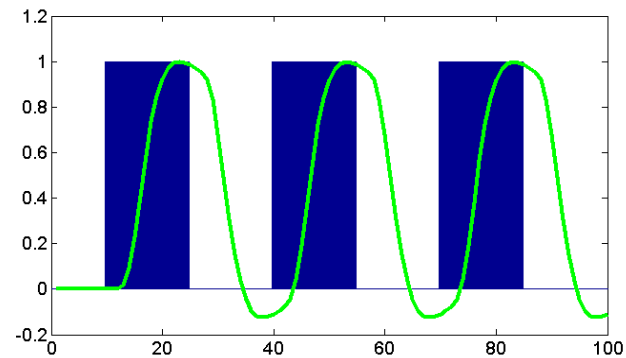
Event-Related



Hemodynamic
Response
Function



Predicted
Response

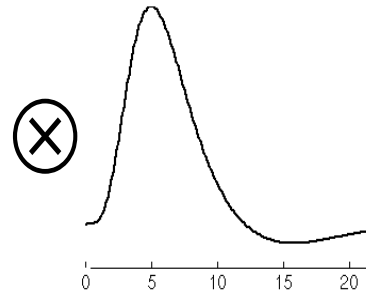


Multiple Conditions

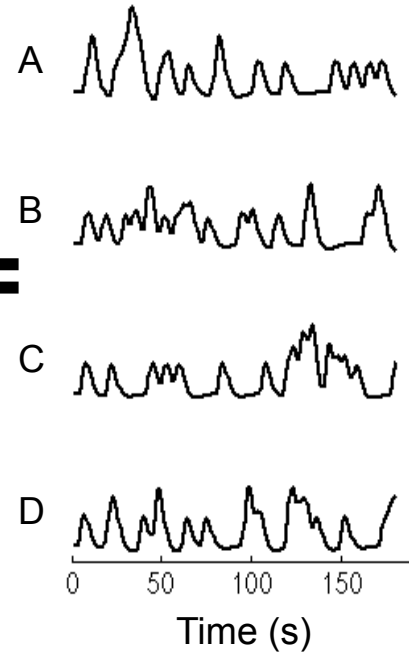
Indicator functions
(Onsets)



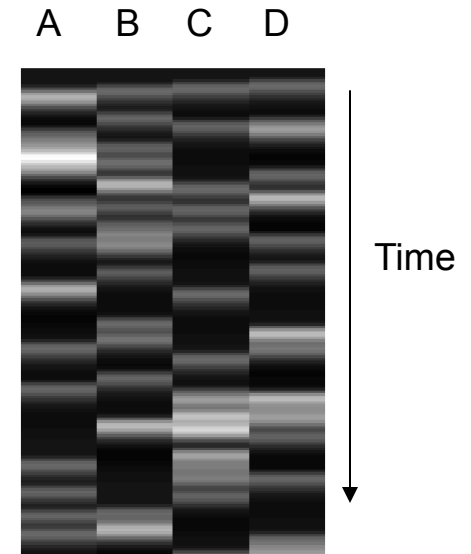
Assumed HRF
(Basis function)



Design Matrix (X^T)



Design Matrix (X)



Assumptions:

Assume neural activity
function is correct

Assume HRF
is correct

Assume LTI
system

HRF Models

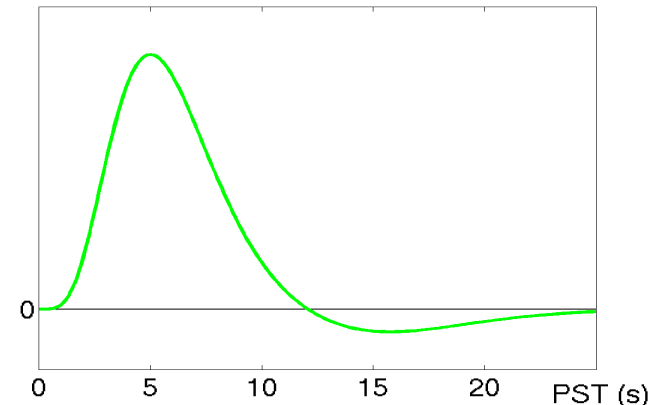
- Often a fixed canonical HRF is used to model the response to neuronal activity

- Linear combination of 2 gamma functions.

- Optimal if correct.

- If wrong, leads to bias and power loss.

- Unlikely that the same HRF is valid for all voxels.
- True response may be faster/slower
- True response may have smaller/bigger undershoot

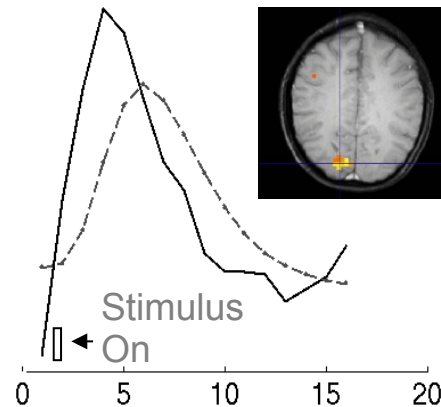


Problems

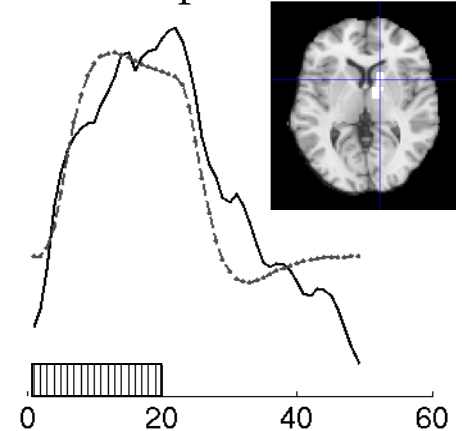
The HRF shape depends both on the vasculature and the time course of neural activity.

Assuming a fixed HRF is usually not appropriate.

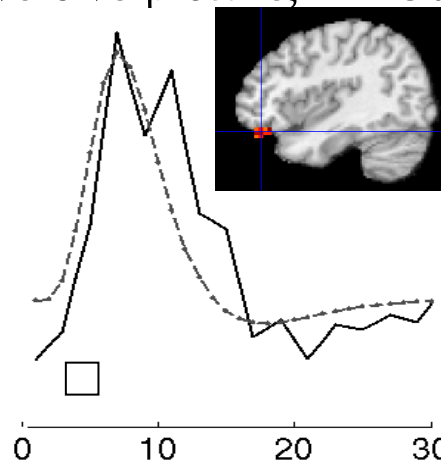
Checkerboard, $n = 10$



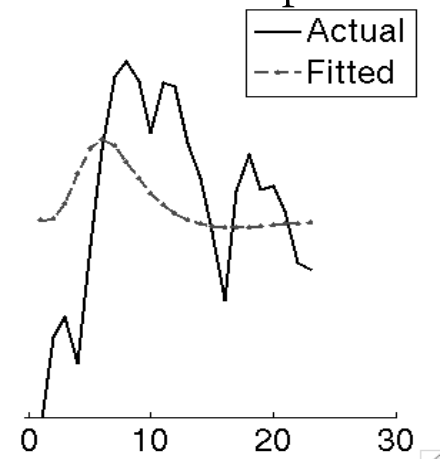
Thermal pain, $n = 23$



Aversive picture, $n = 30$



Aversive anticipation



Temporal Basis Functions

- To allow for different types of HRFs in different brain regions, it is typically better to use **temporal basis functions**.
- A linear combination of functions can be used to account for delays and dispersions in the HRF.
 - The stimulus function is convolved with each of the basis functions to give a set of regressors.
 - The parameter estimates give the coefficients that determine the combination of basis functions that best models the HRF for the trial type and voxel in question.

Temporal Basis Functions

- In an LTI system the BOLD response is modeled

$$x(t) = (s * h)(t)$$

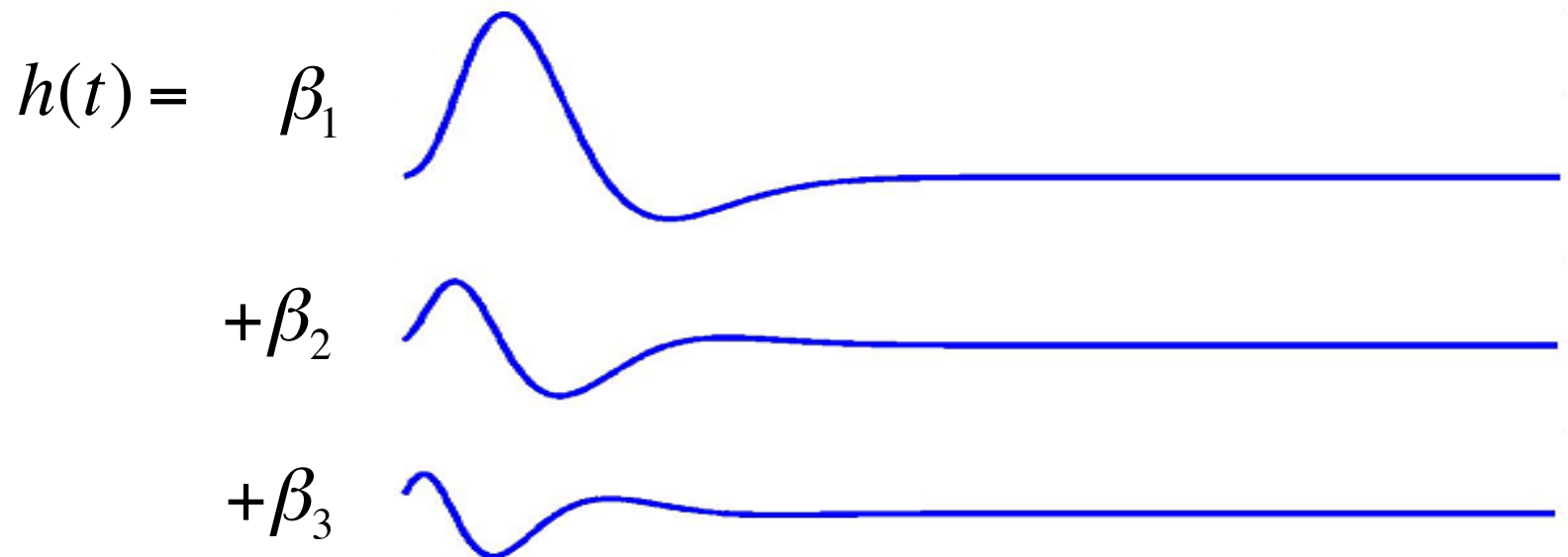
where $s(t)$ is a stimulus function and $h(t)$ the HRF.

- Model the HRF as a linear combination of **temporal basis functions**, $f_i(t)$, such that

$$h(t) = \sum \beta_i f_i(t)$$

Temporal Basis Functions

$$h(t) = \sum \beta_i f_i(t)$$



Temporal Basis Functions

- The BOLD response can be rewritten:

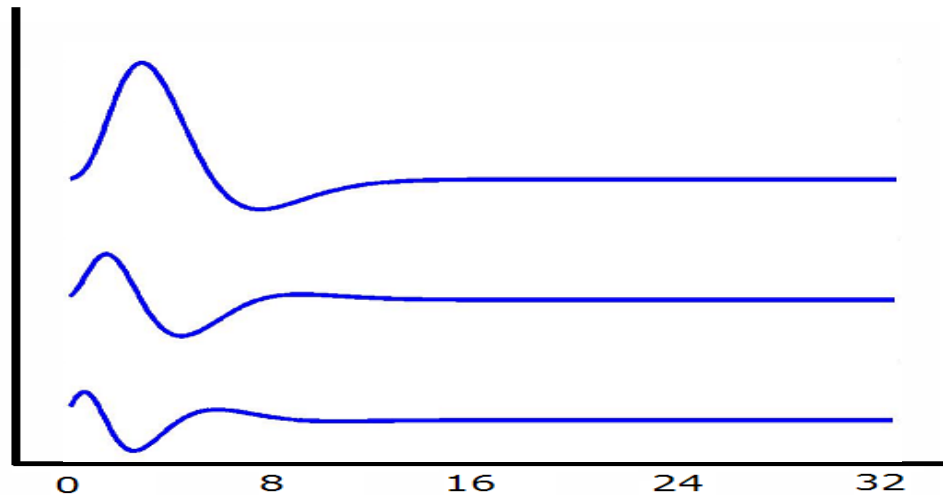
$$x(t) = \sum \beta_i (s * f_i)(t)$$

- In the GLM framework the convolution of the stimulus function with each basis function makes up a separate column of the design matrix.
- Each corresponding β_i describes the weight of that component.

Temporal Basis Functions

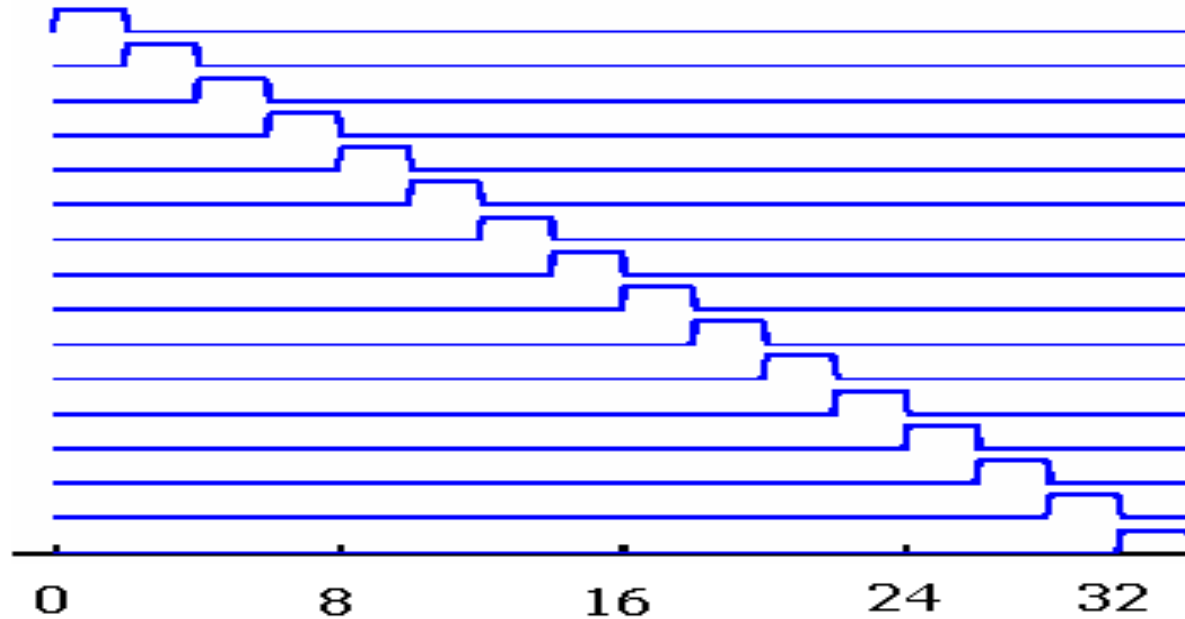
- Typically-used models vary in the degree they make *a priori* assumptions about the shape of the response.
- In the most extreme case, the shape of the HRF is fixed and only the amplitude is allowed to vary.
- By contrast, a *finite impulse response* (FIR) basis set, contains one free parameter for every time-point following stimulation for every cognitive event type.

Canonical HRF + Derivatives



Including the derivatives allows for a shift in **delay** and **dispersion**.

Finite Impulse Response



The model estimates an HRF of arbitrary shape for each event type in each voxel of the brain

Basis sets

Single HRF

Model

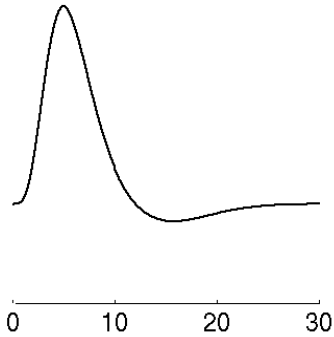
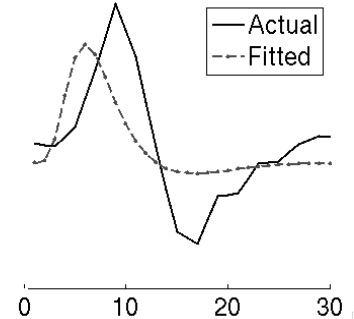


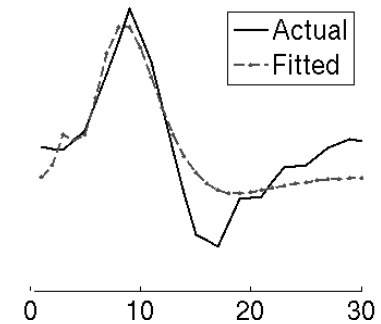
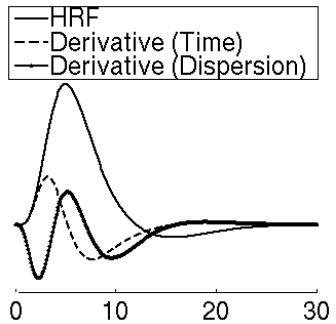
Image of predictors



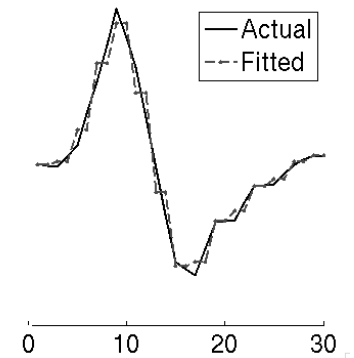
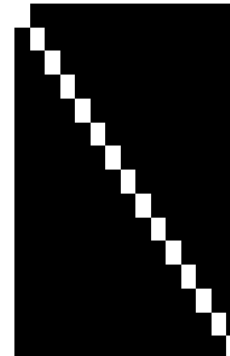
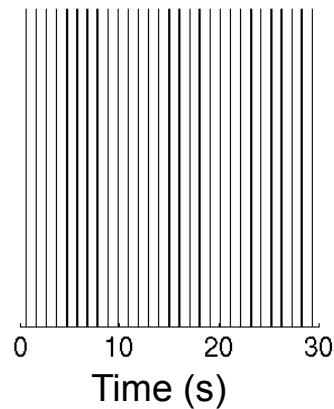
Data & Fitted



HRF + derivatives



Finite Impulse Response (FIR)

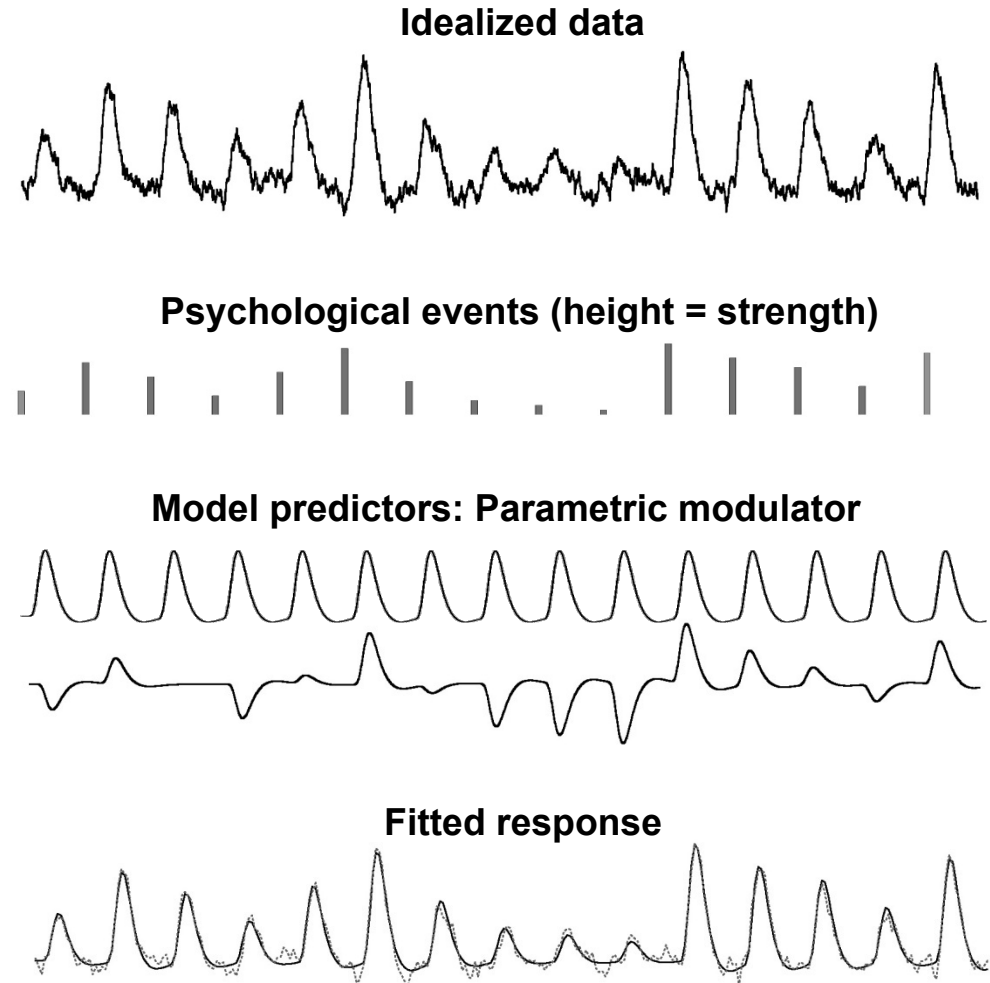


Parametric Modulation

- Often a stimulus can be parametrically varied across repetitions, and it is thought that this may be reflected in the strength of the neuronal response.
- In these types of situations the **parametric modulation** can be modeled by including an additional regressor in the design matrix that accounts for the possible variation in neural response.

Parametric Modulators

Parametric modulators are often used to model trial-to-trial variation in a psychological process.



End of Module



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