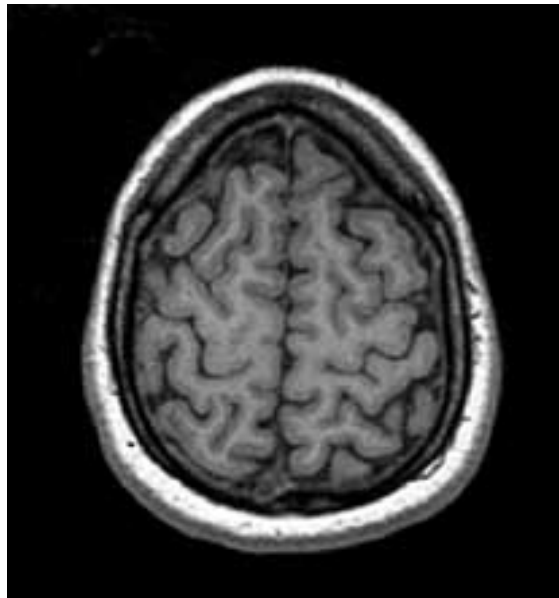


Module 5:

fMRI Signal & Noise

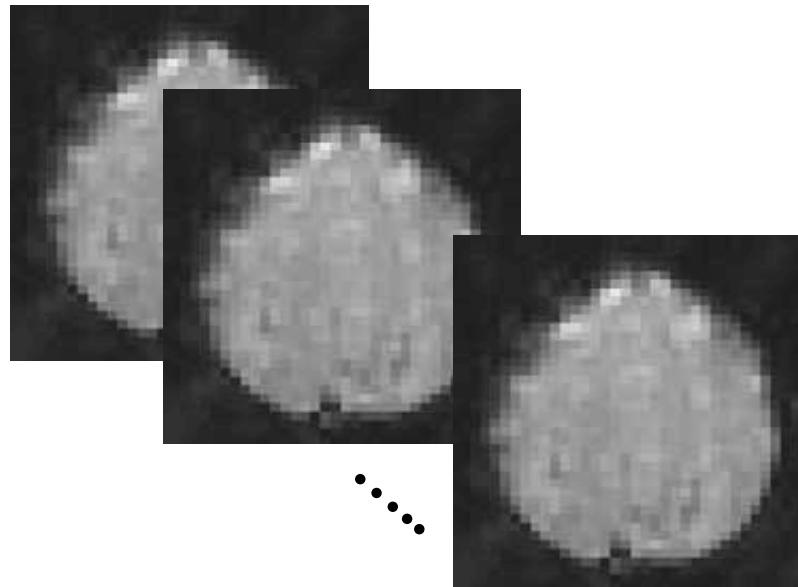
MRI

- MRI studies brain anatomy.
 - Structural (T1) images
 - High spatial resolution
 - Can distinguish different types of tissue



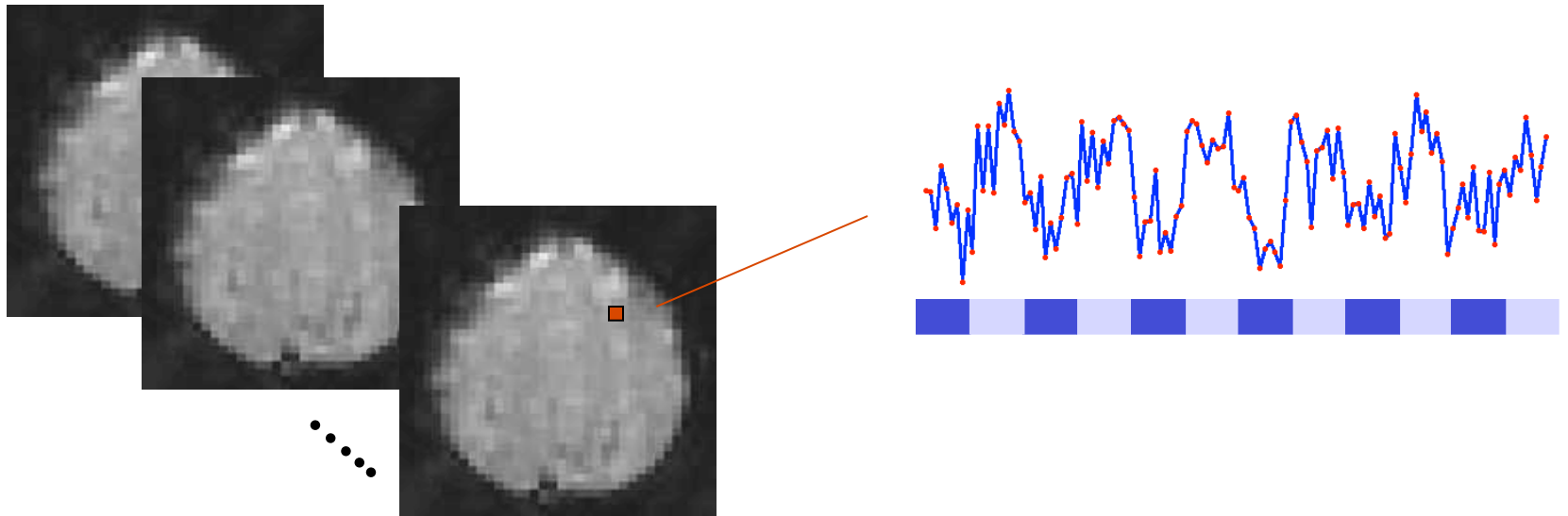
fMRI

- fMRI studies brain function.
 - Functional (T2*) images
 - Lower spatial resolution/ Higher temporal resolution
 - Relate changes in signal to experimental manipulation



Functional MRI

- An fMRI experiment consists of a sequence of individual MR images, where one can study oxygenation changes in the brain across time.



BOLD fMRI

- The most common approach towards fMRI uses the **Blood Oxygenation Level Dependent** (BOLD) contrast.
- It allows us to measure the ratio of oxygenated to deoxygenated hemoglobin in the blood.
- It doesn't measure neuronal activity directly, instead it measures the metabolic demands (**oxygen consumption**) of active neurons.

BOLD Contrast

- Hemoglobin exists in two different states each with different magnetic properties producing different local magnetic fields. (Pauling 1936)
 - Oxyhemoglobin is **diamagnetic**.
 - Deoxyhemoglobin is **paramagnetic**.
- BOLD fMRI takes advantage of the difference in $T2^*$ between oxygenated and deoxygenated hemoglobin.
 - Deoxyhemoglobin suppresses the MR signal.
 - As the concentration of deoxyhemoglobin **decreases** the fMRI signal **increases**.

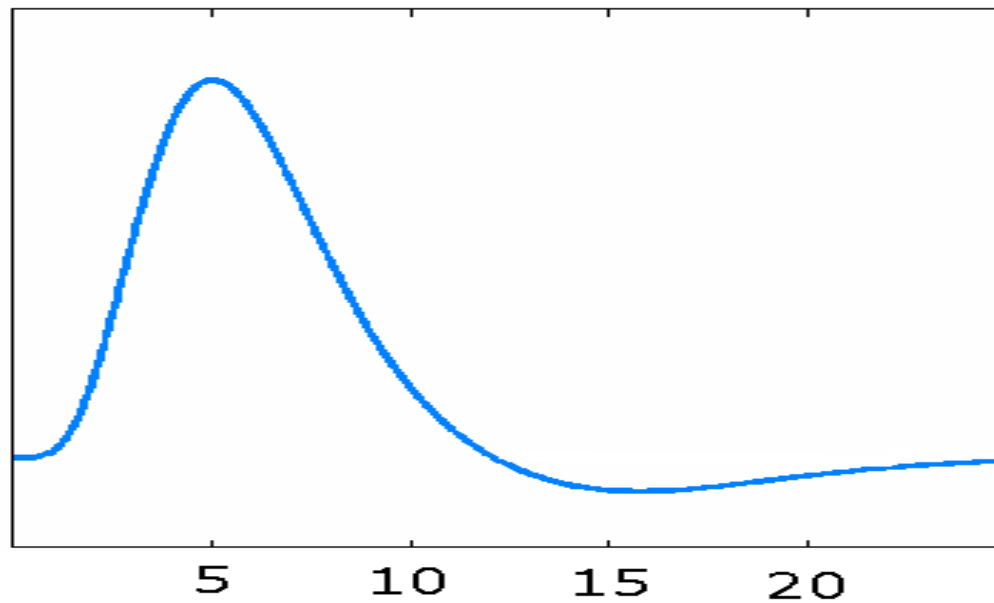
BOLD Signal

- The change in the MR signal triggered by instantaneous neuronal activity is known as the **hemodynamic response function**.
- As neural activity increases, so does metabolic demand for oxygen and nutrients.
- As oxygen is extracted from the blood, the hemoglobin becomes paramagnetic which creates distortions in the magnet field that cause a $T2^*$ decrease (i.e. a faster decay of the signal).

BOLD Signal

- An over-compensation in blood flow dilutes the concentration of deoxyhemoglobin and tips the balance towards oxyhemoglobin.
 - This leads to a peak in BOLD signal about 4-6 s following activation.
- After reaching its peak, the BOLD signal decreases to an amplitude below baseline level.
 - This poststimulus undershoot is due to a combination of reduced blood flow and increased blood volume.

HRF



The strongest signal appears 5-6 seconds after activation.

HRF Properties

- Magnitude of signal changes is quite small
 - 0.1 to 5%
 - Hard to see in individual images
- Response is delayed and quite slow
 - Extracting temporal information is tricky, but possible
 - Even short events have a rather long response
- Exact shape of the response has been shown to vary across subjects and regions.

Interpretation

- How well does BOLD signal reflect increases in neural firing?
- The BOLD signal corresponds relatively closely to the local electrical field potential surrounding a group of cells, which is likely to reflect changes in post-synaptic activity, under many conditions.
- Demonstrations have shown that high-field BOLD activity closely tracks the position of neural firing and local field potentials.

LTI System

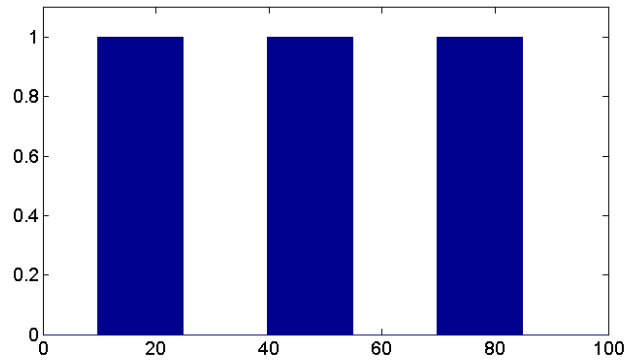
- The relationship between stimuli and the BOLD response is often modeled using a **linear time invariant (LTI) system**.
 - Here the neuronal activity acts as the **input** or **impulse** and the HRF acts as the **impulse response function**.
- In this framework the signal at time t , $x(t)$, is modeled as the convolution of a stimulus function $v(t)$ and the hemodynamic response $h(t)$, that is,

$$x(t) = (v * h)(t)$$

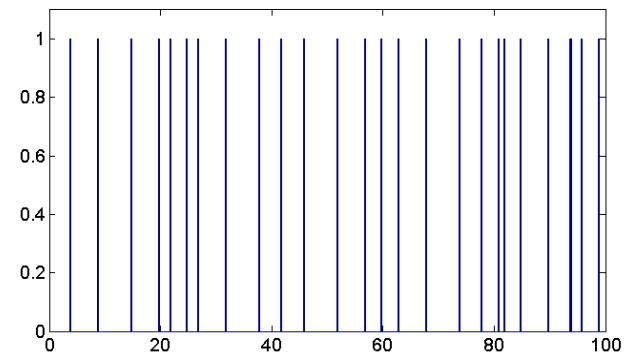
Convolution Examples

Experimental
Stimulus Function

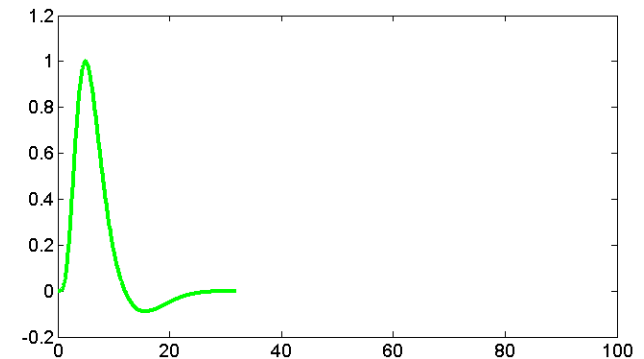
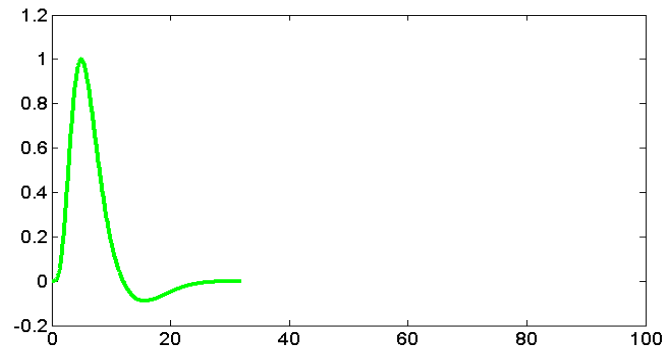
Block Design



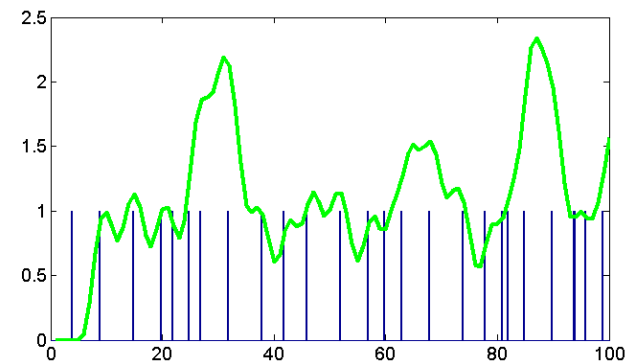
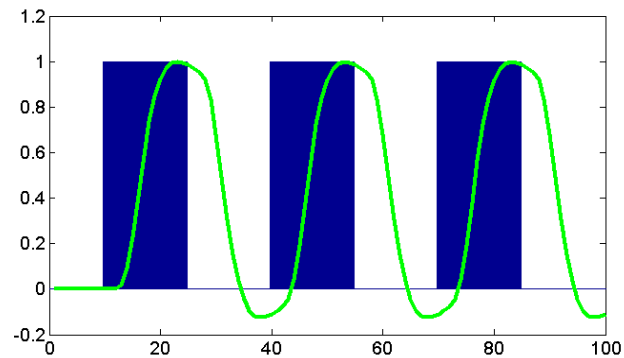
Event-Related



Hemodynamic
Response
Function



Predicted
Response



Non-linearity

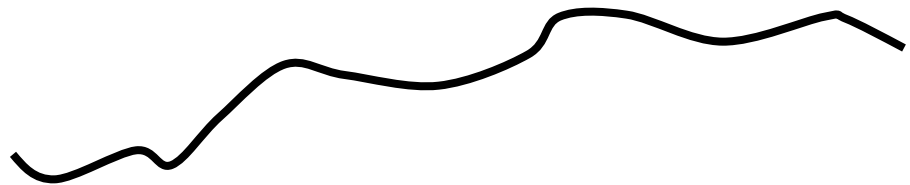
- Studies have shown that the BOLD response is roughly linear, with some departures from linearity.
- There is some evidence of **refractory effects**, which are reductions in amplitude of a response as a function of inter-stimulus intervals.
- There is evidence of non-linearity if the stimulus are spaced closer than 5-6 s apart.

fMRI Noise

- The measured fMRI signal is corrupted by random noise and various nuisance components that arise due to hardware reasons and the subjects themselves.
- Sources of noise:
 - Thermal motion of free electrons in the system.
 - Patient movement during the experiment.
 - Physiological effects, such as the subject's heartbeat and respiration.
 - Low frequency signal drift.

Drift

- Slow changes in voxel intensity over time (low-frequency noise) is present in the fMRI signal.
- Scanner instabilities and not motion or physiological noise may be the main cause of the drift, as drift has been seen in cadavers.
- We need to include drift parameters in our future models.

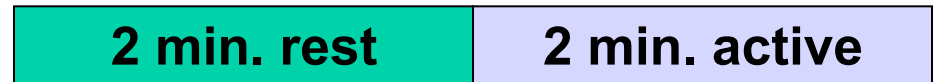


Issues

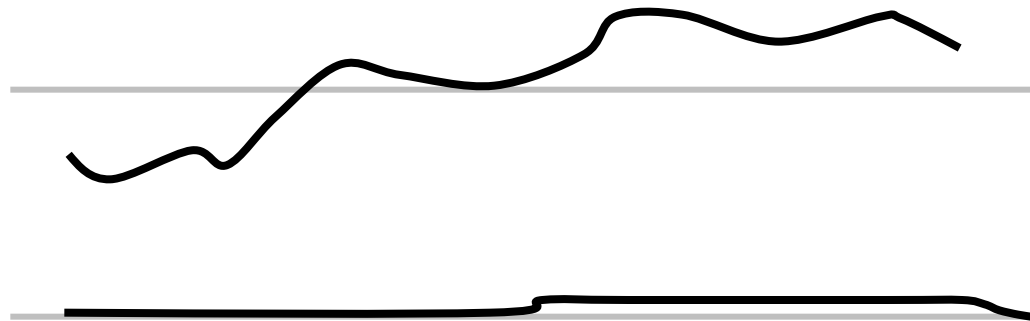
- Drift can have serious consequences:
 - Experimental conditions that vary slowly may be confused with drift.
 - Experimental designs should use high frequencies (more rapid alternations of stimulus on/off states).

- Bad Design:

**Typical Drift
Pattern & Magnitude**



**Typical Signal
Magnitude**



... you'll never detect this signal, due to the drift

Motion

- Subject motion during the experiment can also give rise to serious problems.
- Typically motion correction is performed in the pre-processing stages of the analysis.
- However, 'spin-history' artifacts may remain that cannot be removed.
 - This is caused by through-plane motion.
 - Attempts to account for it are often made in the modeling stage.

Physiological Noise

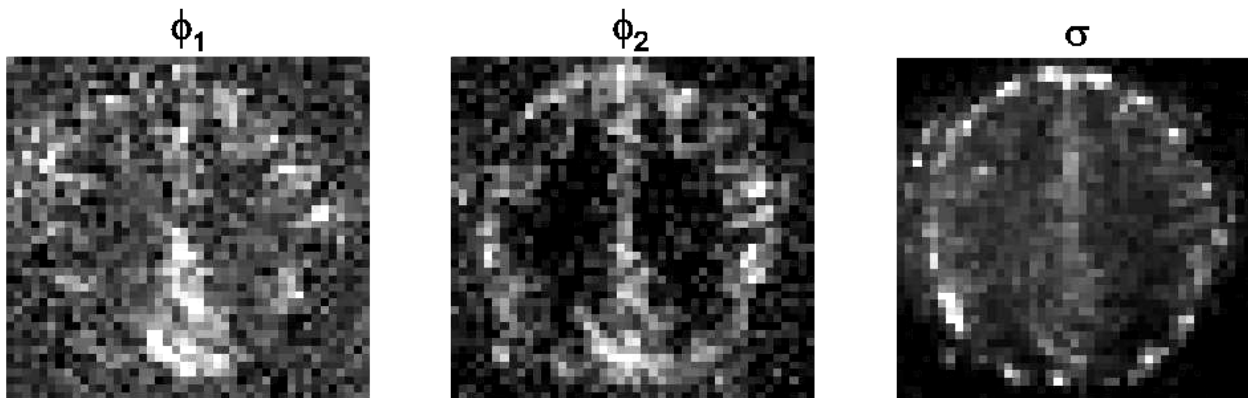
- Respiration and heart beat give rise to high-frequency noise.
- It can potentially be modeled, but if the TR is too low there will be problems with aliasing.
- For standard TR values ($\sim 2\text{s}$) this type of noise is difficult to remove and is often left in the data giving rise to temporal autocorrelations.

fMRI Noise

- Some noise components can be removed prior to analysis, while others need to be included as components in subsequent models.
- However, it is difficult to remove or model all sources of noise and therefore significant autocorrelation will be present in the signal.
- In fMRI we typically use autoregressive (AR) or autoregressive moving-average (ARMA) processes to model the correlation.

Spatio-temporal Behavior

- The spatiotemporal behavior of these noise processes is complex.



Spatial maps of the model parameters from an AR(2) model estimated for each voxel's noise data.

End of Module



@fMRIstats