## Multi-label classification for CT brain images

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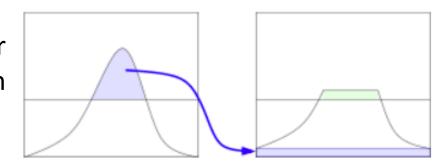
#### **Data augmentation**

#### **Dataset Splitting**

• We split the patients in the dataset into training and validation parts with the ratio 9:1

#### **Contrast Limited Adaptive Histogram Equalization (CLAHE)**

- CLAHE limiting the slope of the cumulative distribution function (CDF), which is equivalent to limiting the amplitude of the histogram.
- If the bins in the histogram exceed the upper limit of contrast, the pixels in the histogram will be evenly dispersed into other bins.



#### Other data augmentation method

- In this project, we also use several common augmentation techniques to avoid training data overfitting
- For instance, flip, rotation, scale and color jittering
- During training and testing, the image data has been resized to 224x224

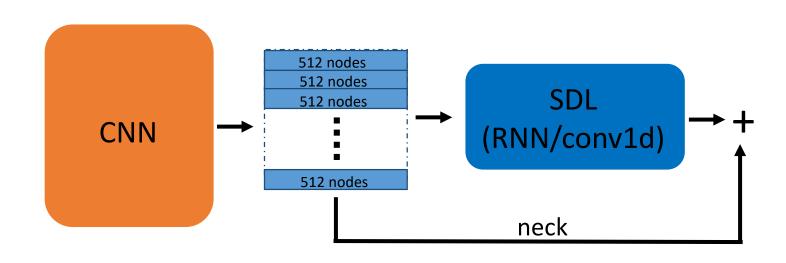
#### **Architecture**

#### **CNN** backbone

- We use ResNET18 and VGG16 for feature extraction and generates an Nx512 feature matrix
- Due to the limitations of GPU hardware we use VGG16 for the following study

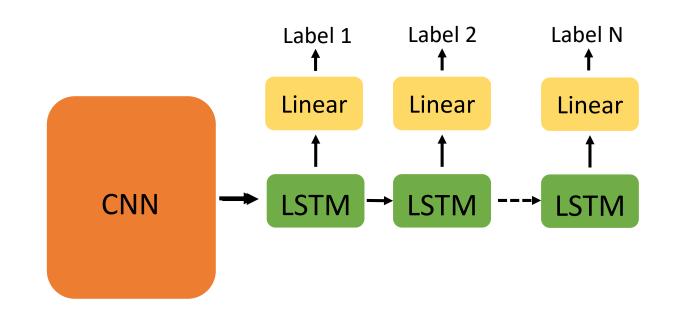
#### Slice dependencies learning (SDL)

- Intuitively, the relationship between different slices within one patient should be considered
- Here we use RNN/1dconv to learn the dependencies between slices
- We combine CNN output feature as the input of RNN
- Furthermore, we use a "neck", a method that adds RNN output and CNN output to reduce the vanishing gradient problem.

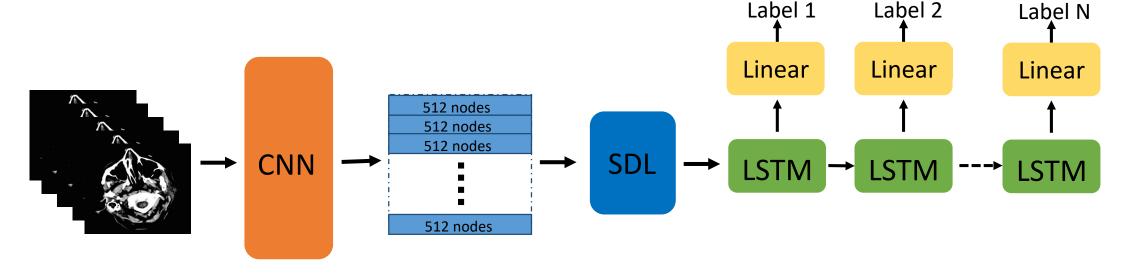


#### Multi-label classification prediction (LRNN)

- In this part, we further considered the correlation between different trauma or disease
- We use binary decoder RNN to do the final multi-label classification
- This model runs 5 time-steps, each time producing a single scalar which is the score for one particular class, or produce a feature matrix construct by each class
- The CNN feature act as an initial state of LSTM and the input is set to zero



# Framework Label 1 Label 2 Linear Lin



#### **Training**

#### **Asymmetric loss function**

- To deal with imbalance data, positive samples is much more important than the negative one.
- ASL is a variation of Binary Cross-Entropy and Focal Loss

$$\begin{array}{l} L = -yL_+ - (1-y)L_- \\ \begin{cases} L_+ = (1-p)^{\gamma+} + \log(p) \\ L_- = p^{\gamma-} - \log(1-p) \end{array} & \text{Y: ground-truth label} \\ \begin{array}{l} \text{L+ / L-: the positive and negative loss parts} \\ \gamma : \text{focusing parameter} \\ \end{cases}$$

- ASL as separate focusing parameters r+/r-.
- By setting r->r+ it's easy to emphasize positive samples.

#### **Pretrain CNN backbone**

- To reduce training time and increase performance, we pretrain CNN with CT image in the dataset using simple CNN architecture and VGG16 + linear layer with parameters below
  - ➤ Input size = 224\*224
  - batch size = 16
  - ➤ learning rate = 10<sup>-4</sup>
  - > optimizer = Adam

#### **CNN + RNN training**

- We use the pretrained VGG16 to set the initial value of the feature extractor in the final model. Using parameters:
  - ➤ Input size = 224
  - batch size = not fixed (separate by patients)
  - ➤ learning rate = 10<sup>-5</sup>
  - optimizer = Adam
- We use early stopping technique to choose the best model base on the F2 score, not the accuracy

#### **Experiment result**

Model	F2 score (valid)	F2 score (kaggle)
VGG16	0.712	0.721
VGG16 + LRNN	0.720	0.750
VGG16 + SDL(GRU)	0.745	0.768
VGG16 + SDL(1Dconv)	0.747	0.750
VGG16 + SDL(GRU) + LRNN	0.765	0.773
VGG16 + SDL(1Dconv) + LRNN	0.757	0.774
VGG16 + LRNN + SDL(GRU)	0.766	0.783