

Time resolved electrophysiological brain imaging using MEG and EEG

Denis A. Engemann

denis.engemann@gmail.com



github: dengemann

twitter: dngman A small Twitter logo icon, featuring the blue bird silhouette.

slides by Denis Engemann and Alex Gramfort

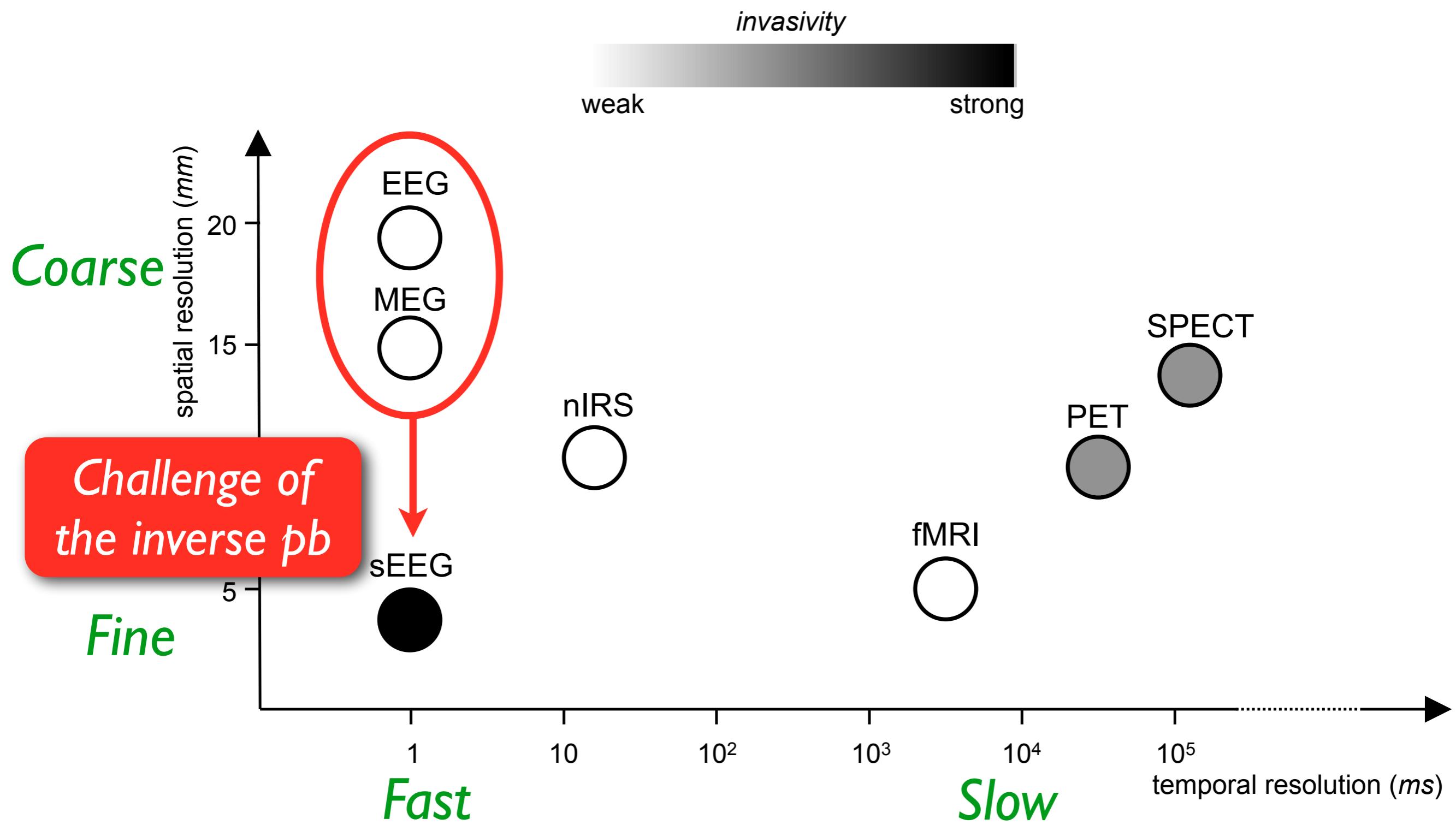
Bar Ilan- October 2015



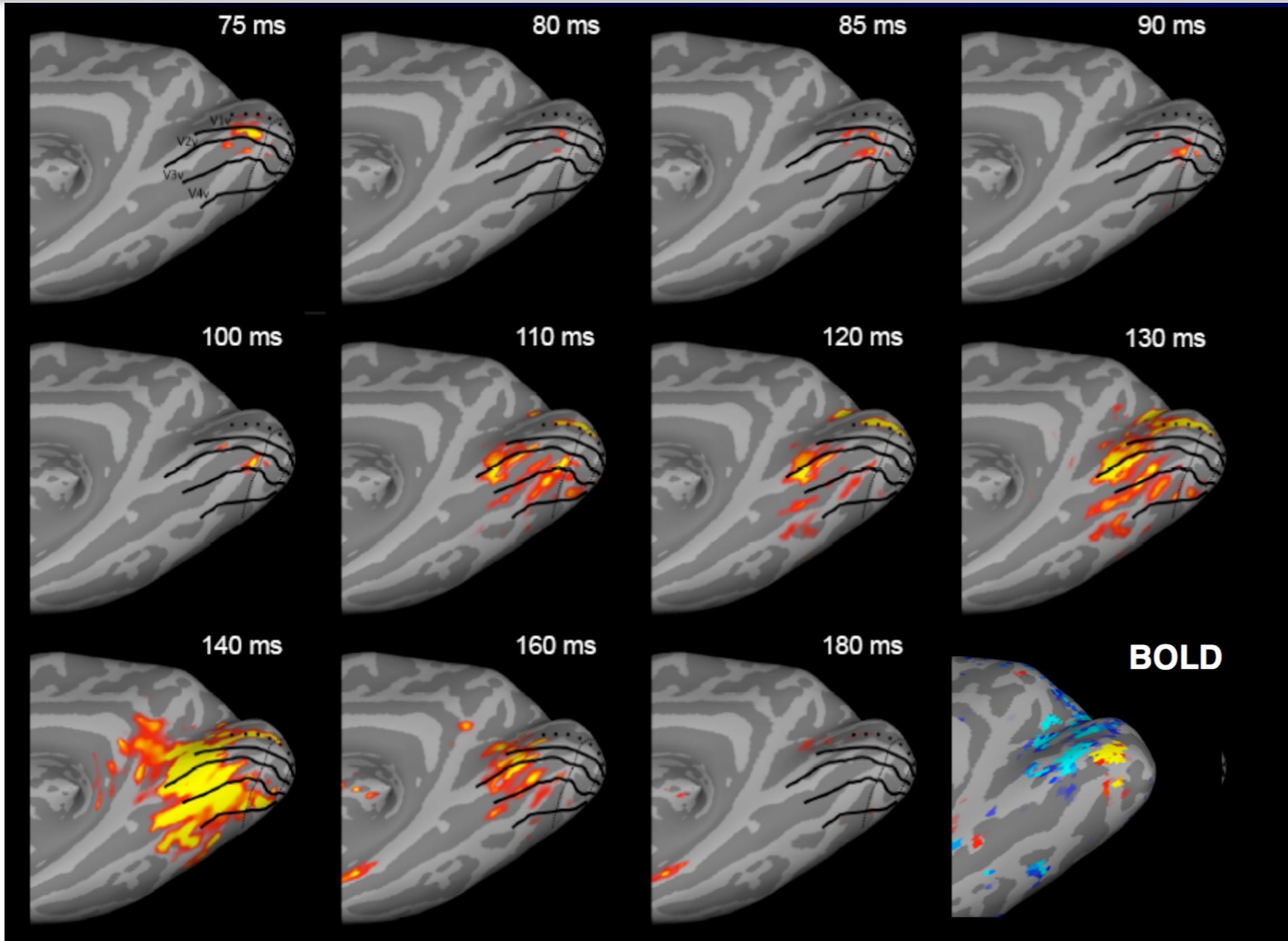
3 claims

- you should care about MEG and EEG
- The choice of your statistical model for source localization reflects hypotheses about brain sources
- The success of your source localization depends on domain knowledge and proper signal processing

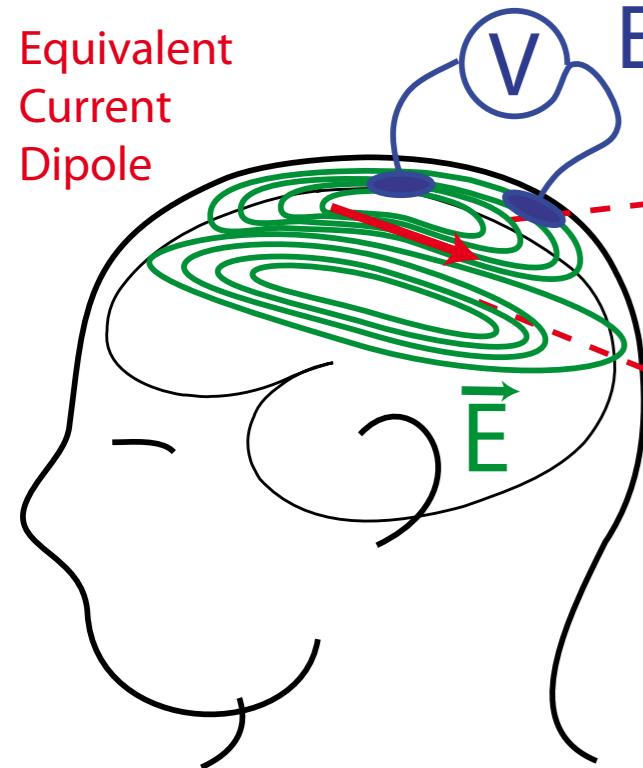
fast brain imaging methods



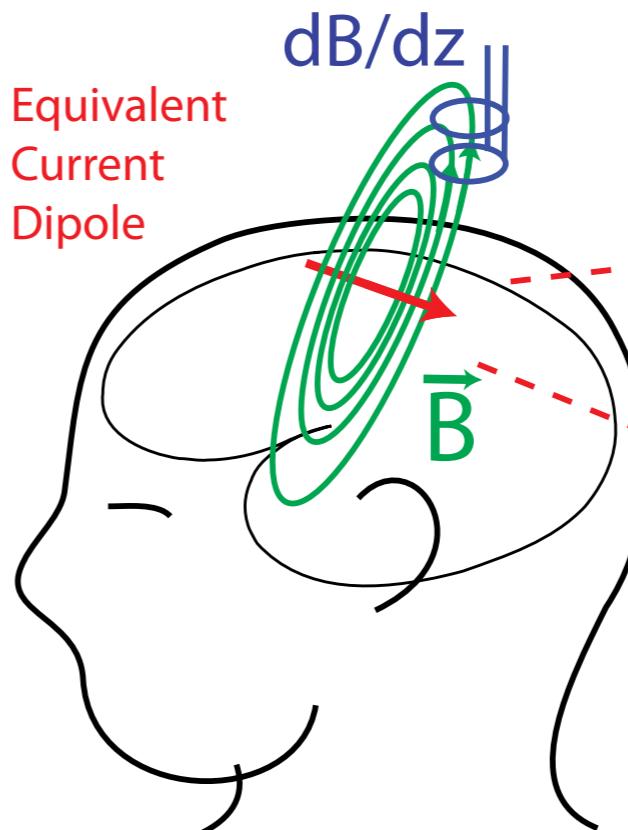
#temporal_resolution



yeah imaging!— sources?



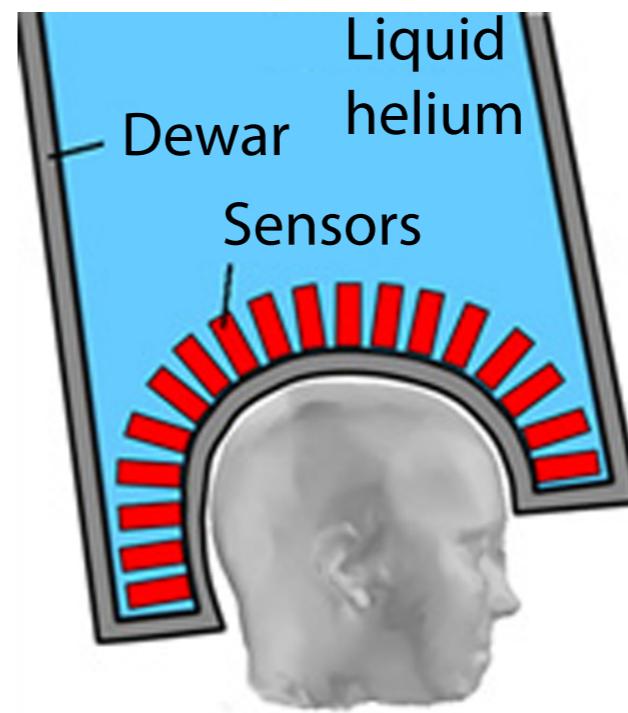
EEG recordings



MEG recordings



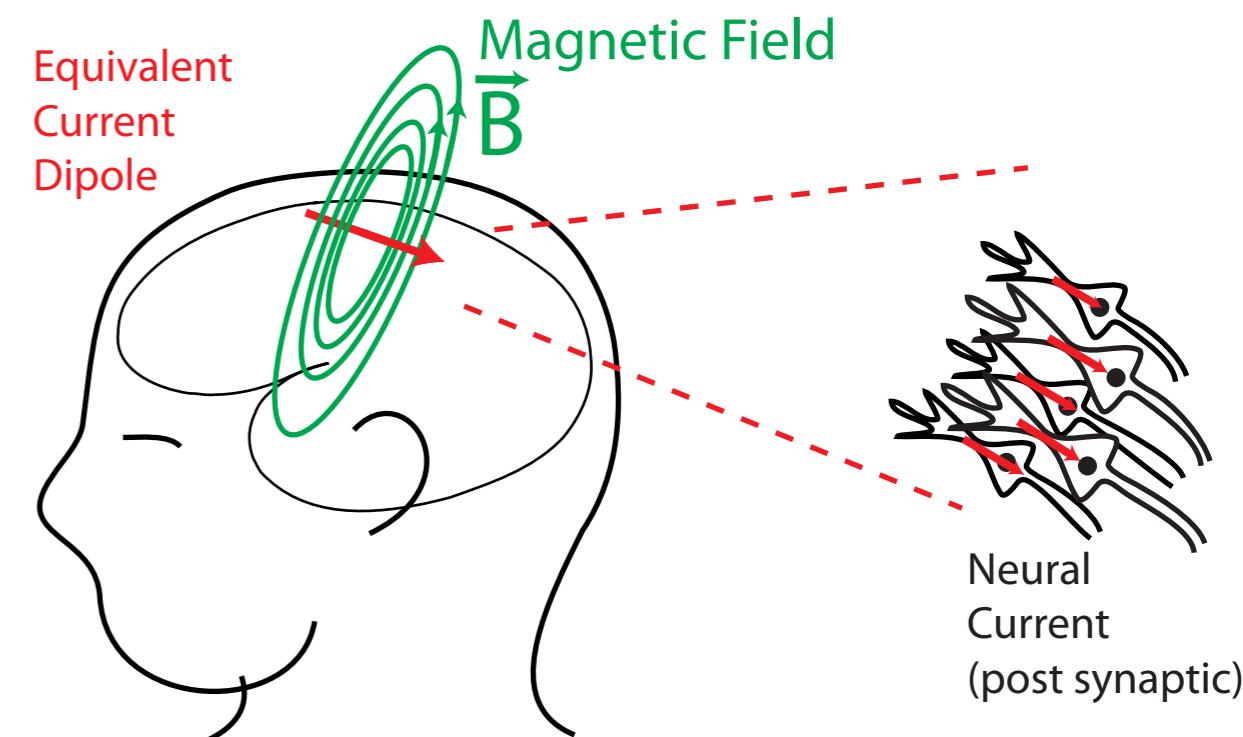
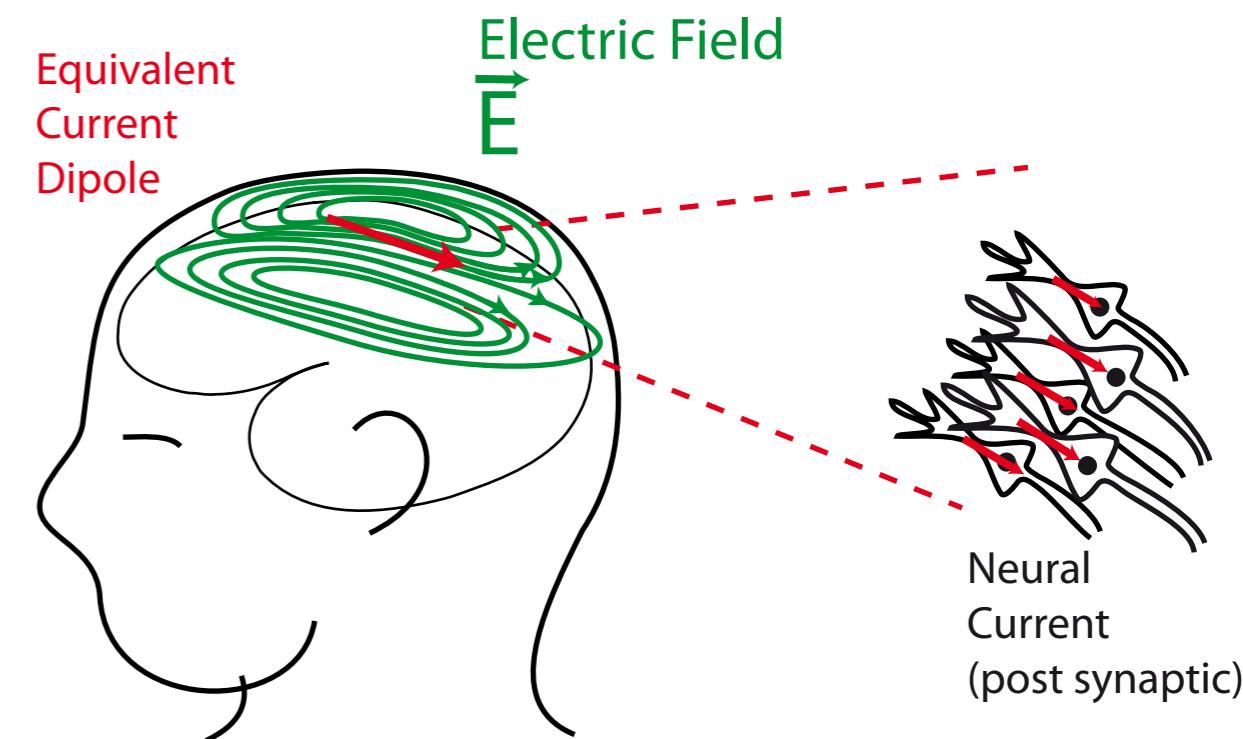
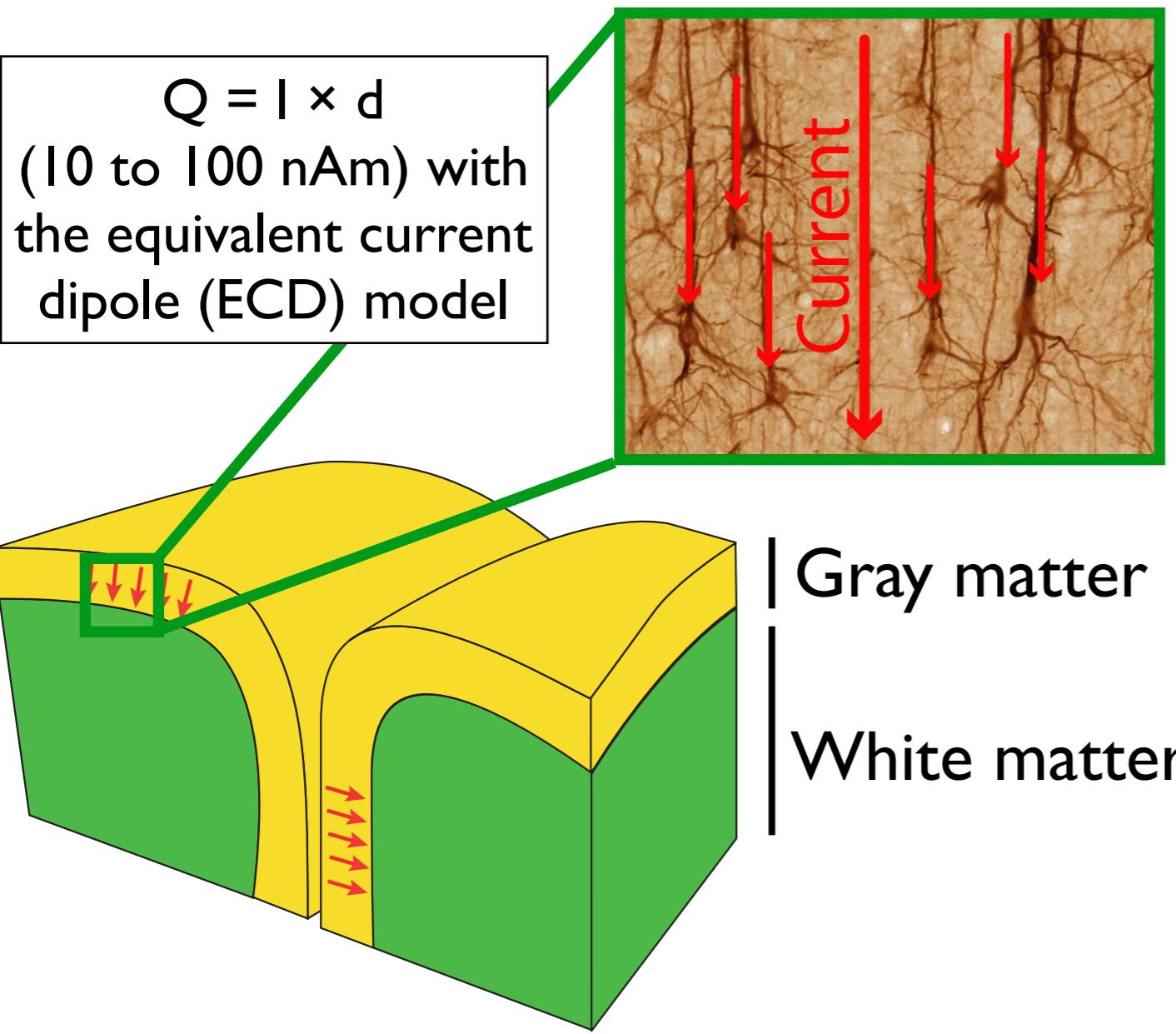
First EEG
recordings
in 1929
by H. Berger



Hôpital La Timone
Marseille, France

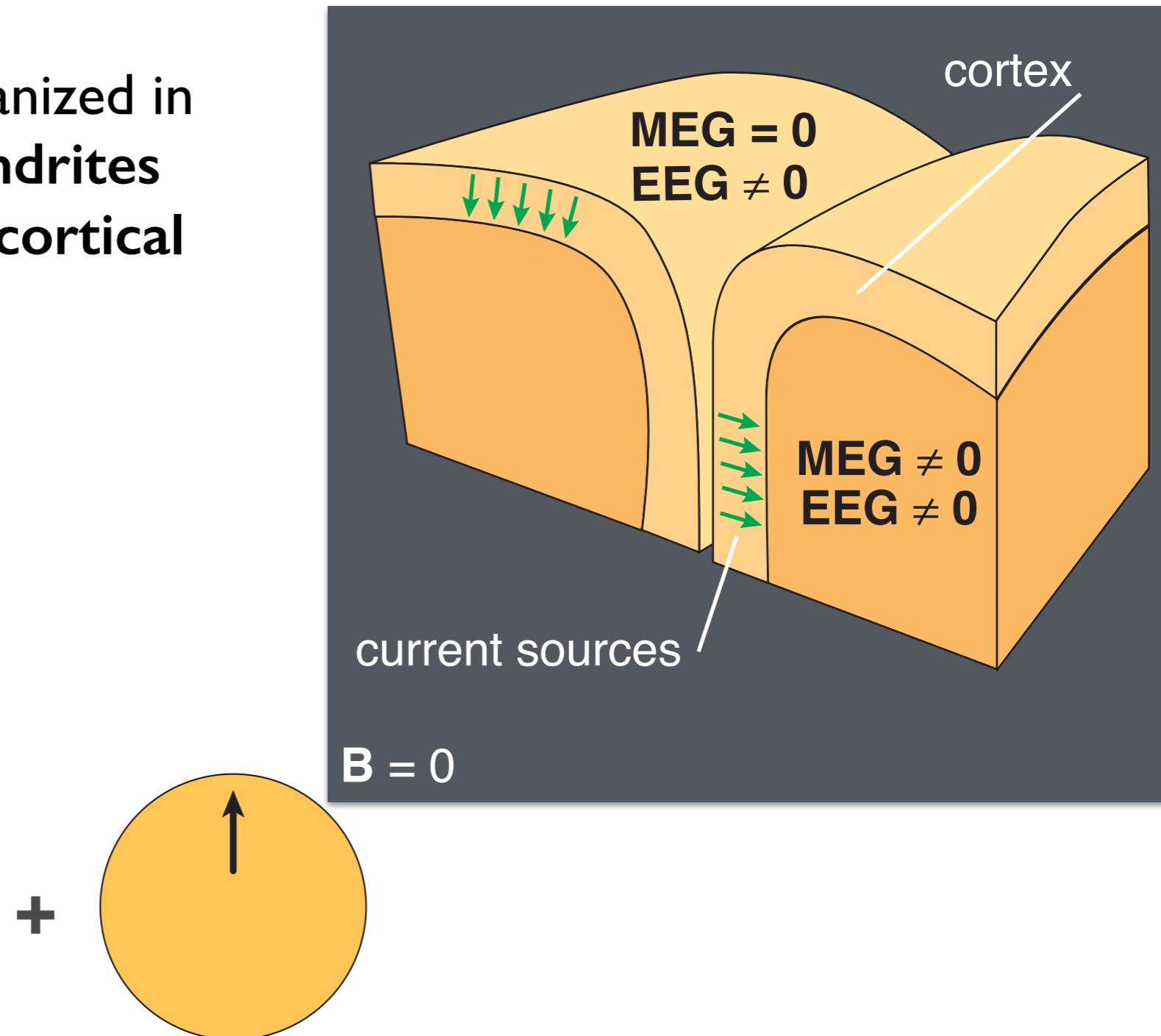
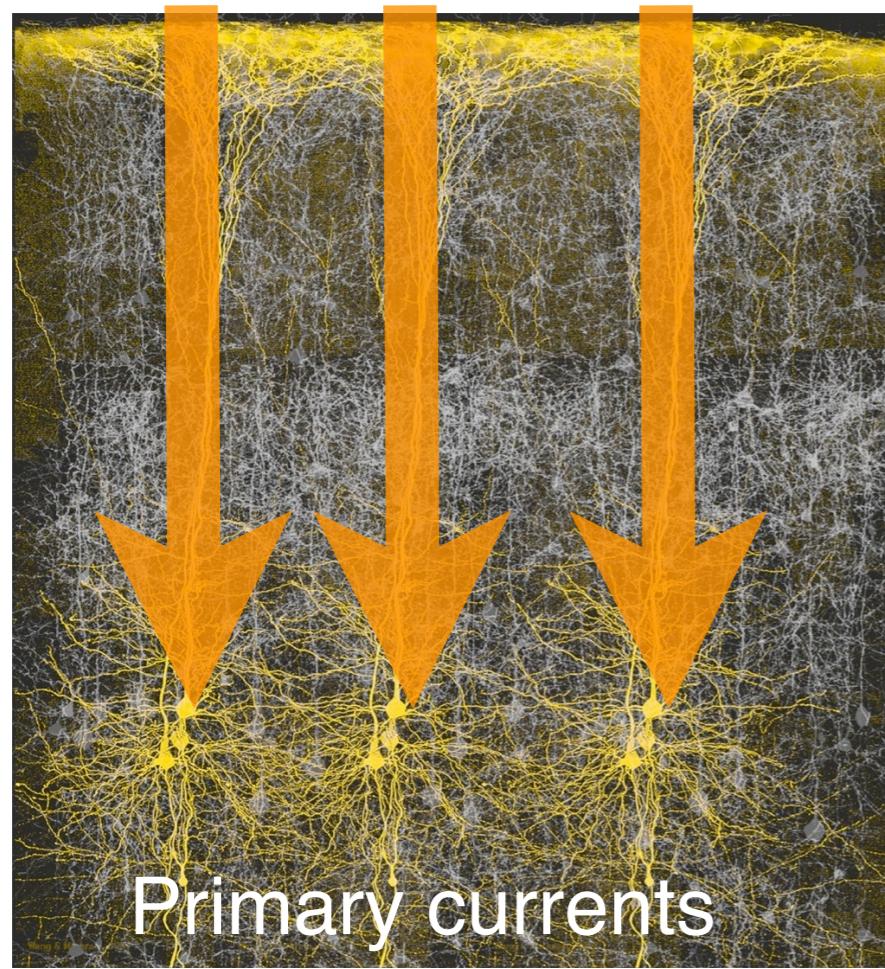
#sources #MEG #EEG

Large cortical pyramidal cells organized in macro-assemblies with their **dendrites** normally oriented to the local cortical surface

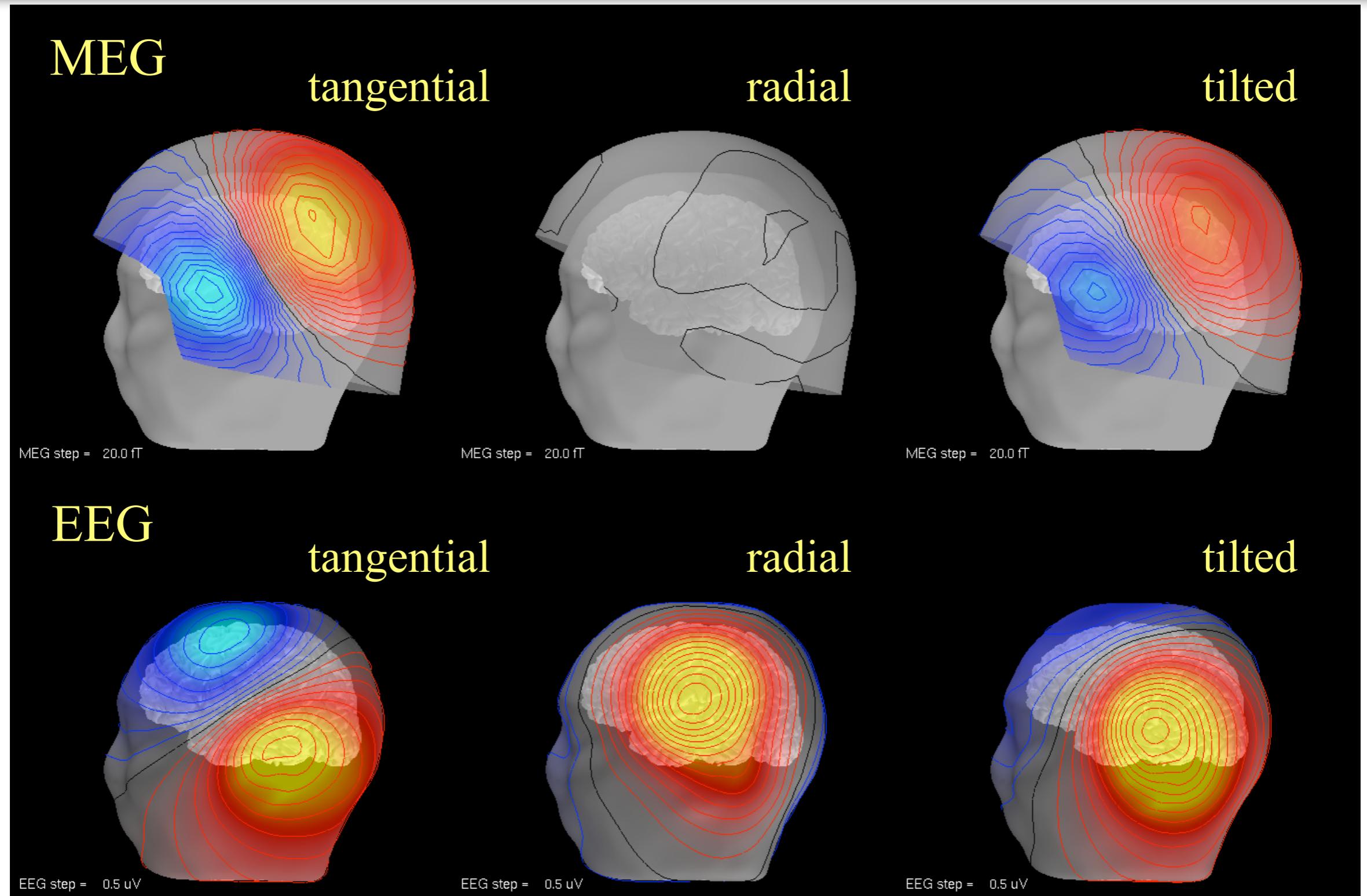


MEG+EEG are complementary

Large cortical pyramidal cells organized in macro-assemblies with their **dendrites** normally oriented to the local cortical surface

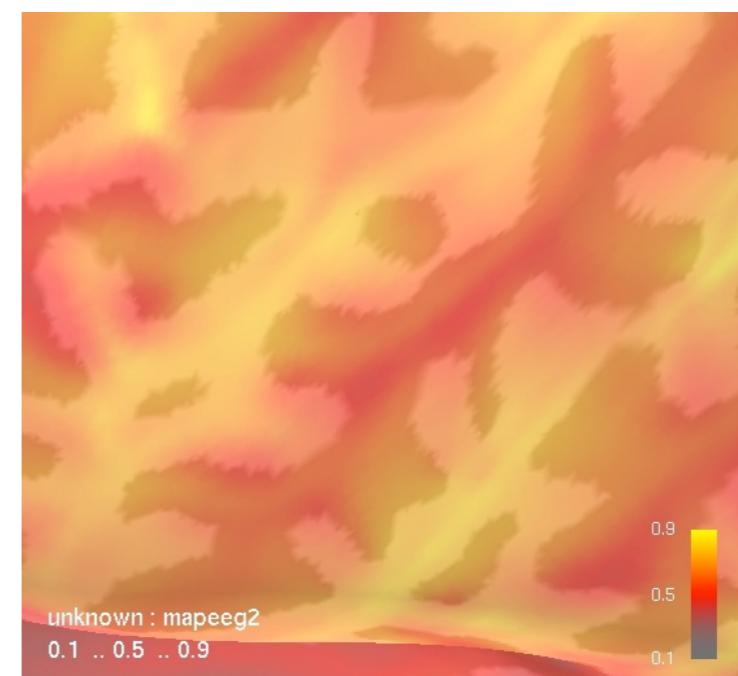
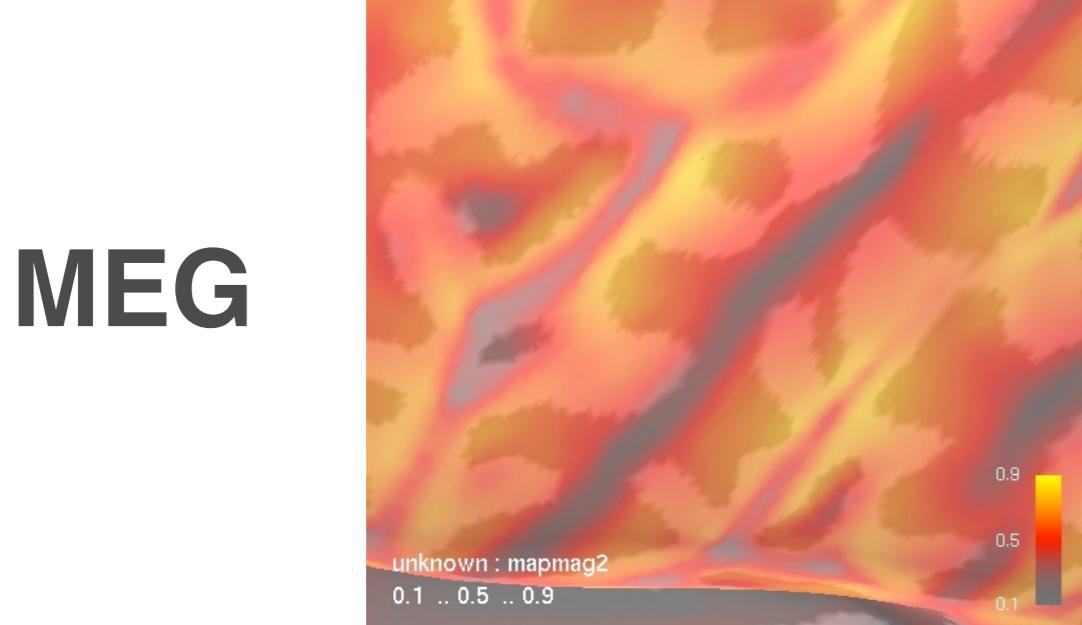
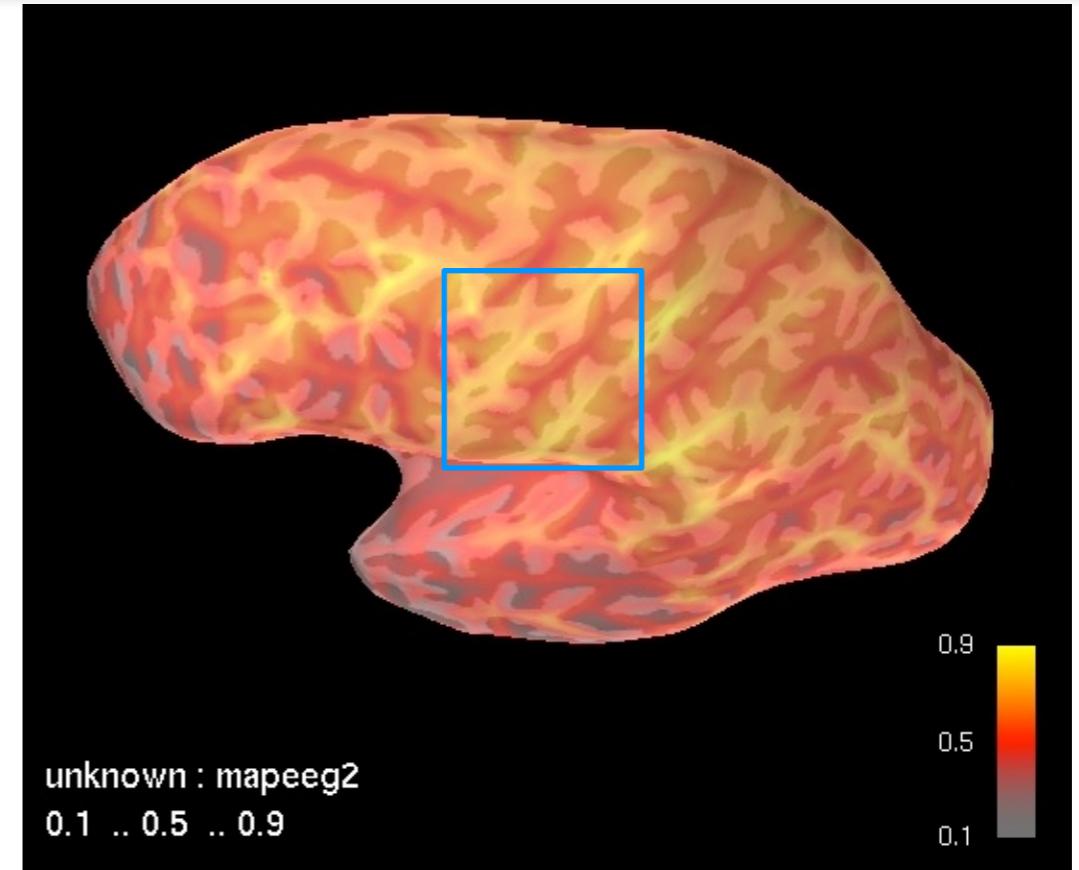
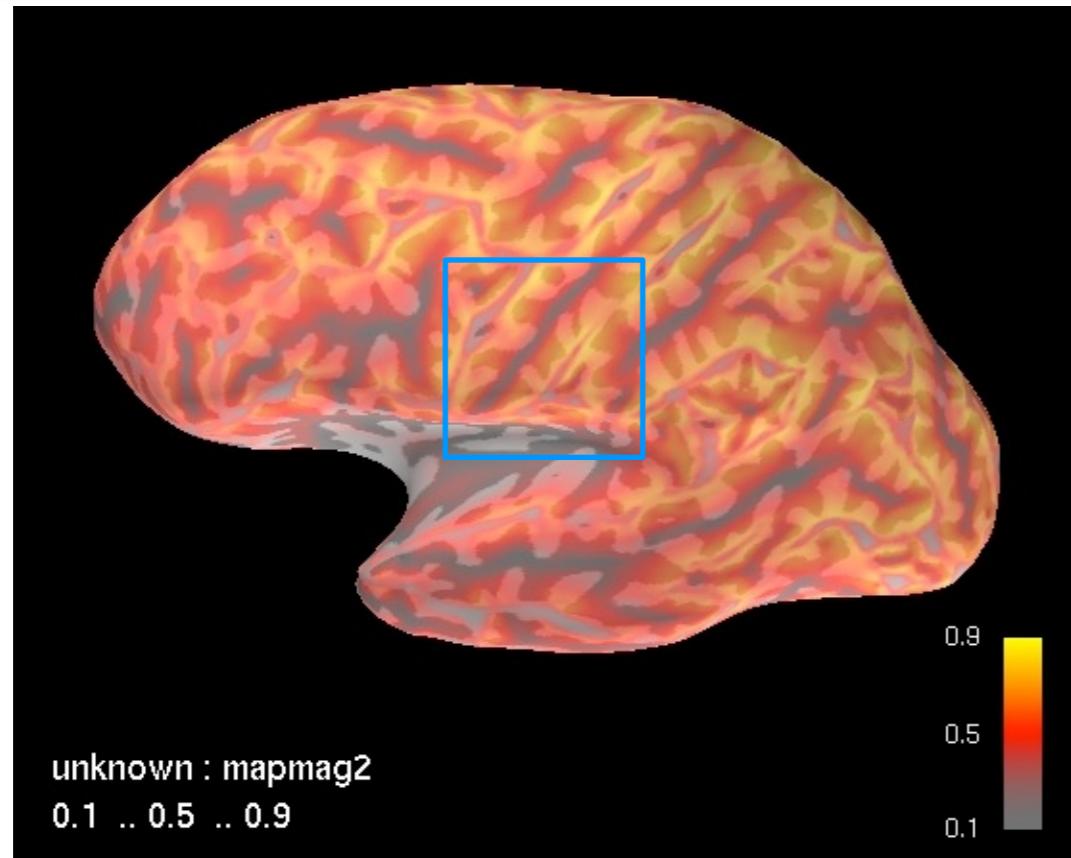


MEG+EEG are complementary



MEG has only one prototypical field pattern

MEG+EEG are complementary

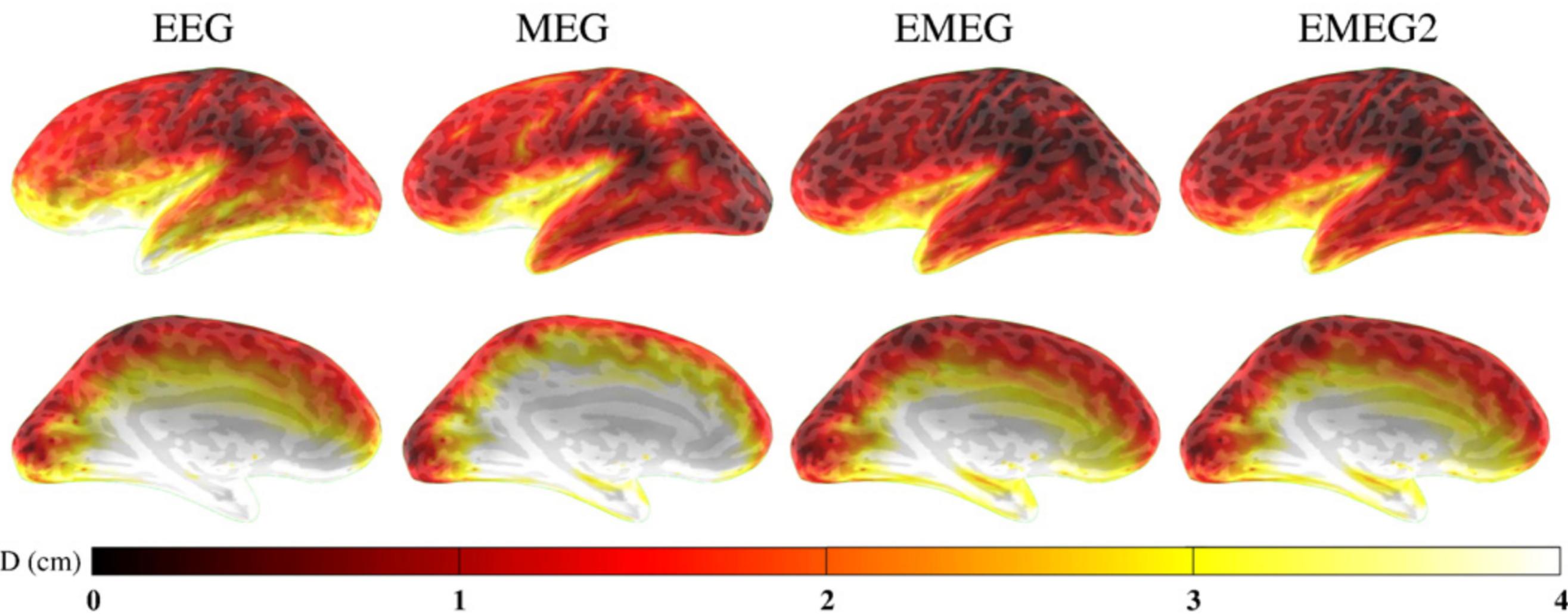


MEG

EEG

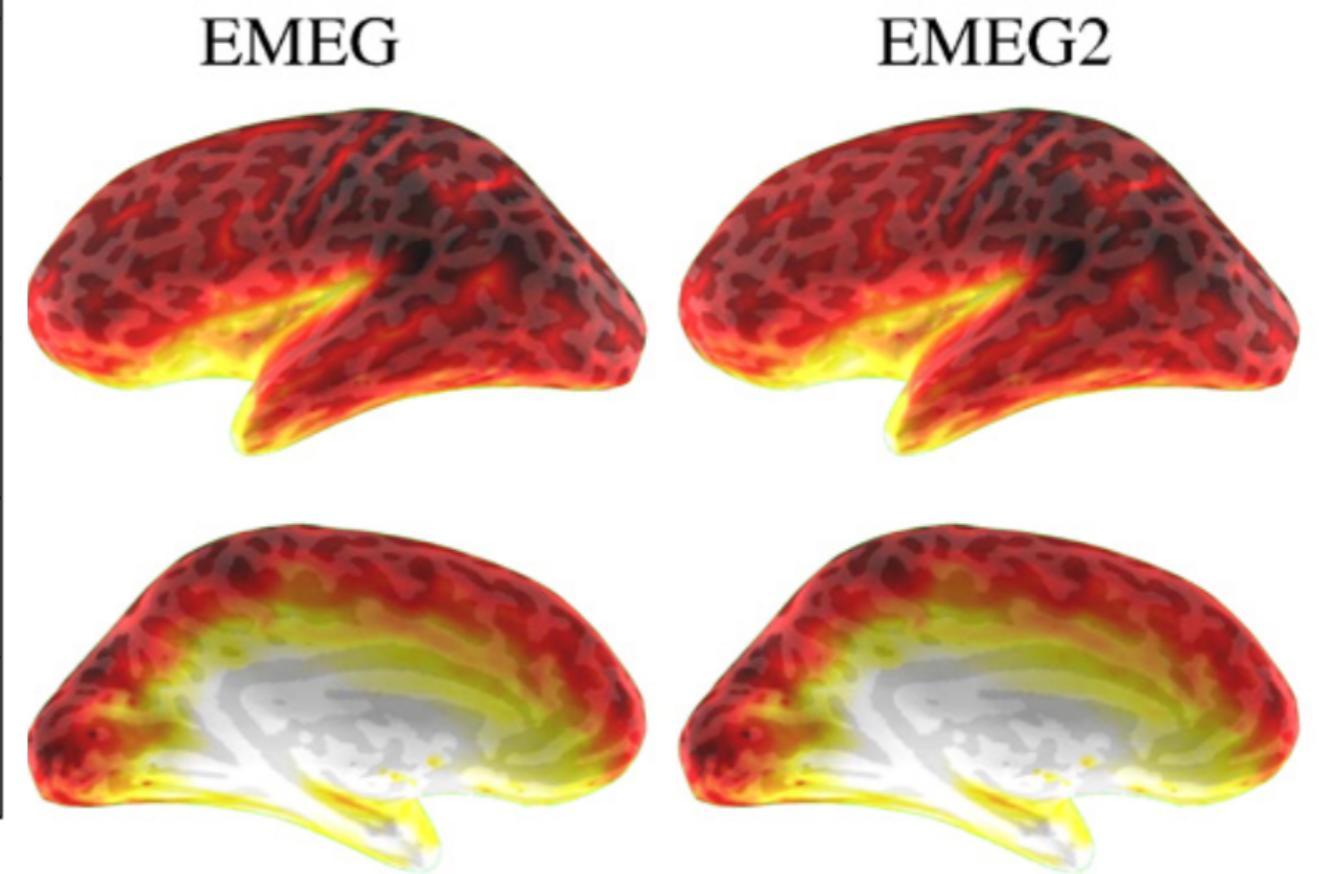
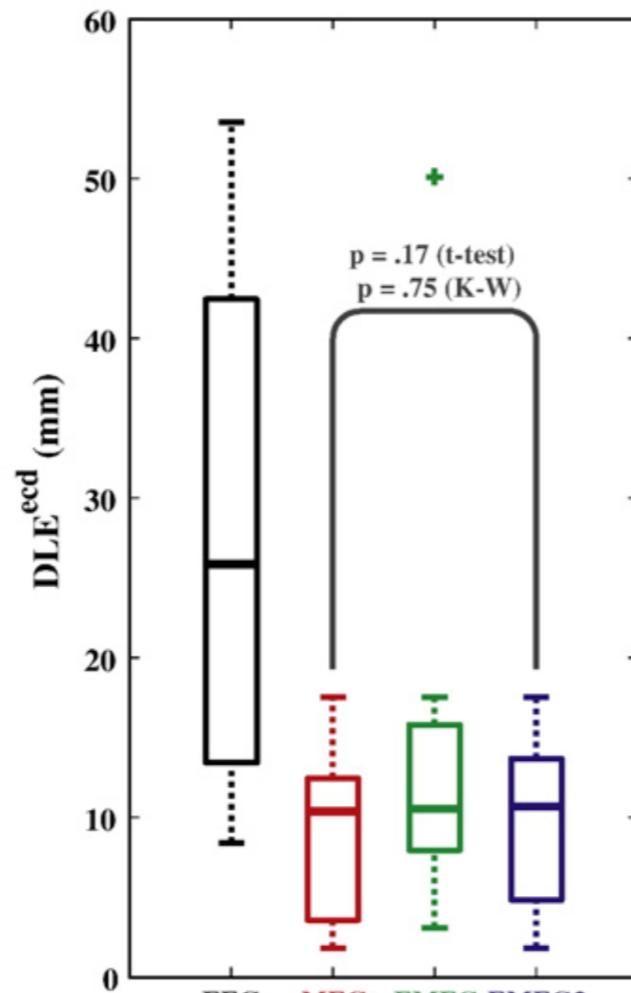
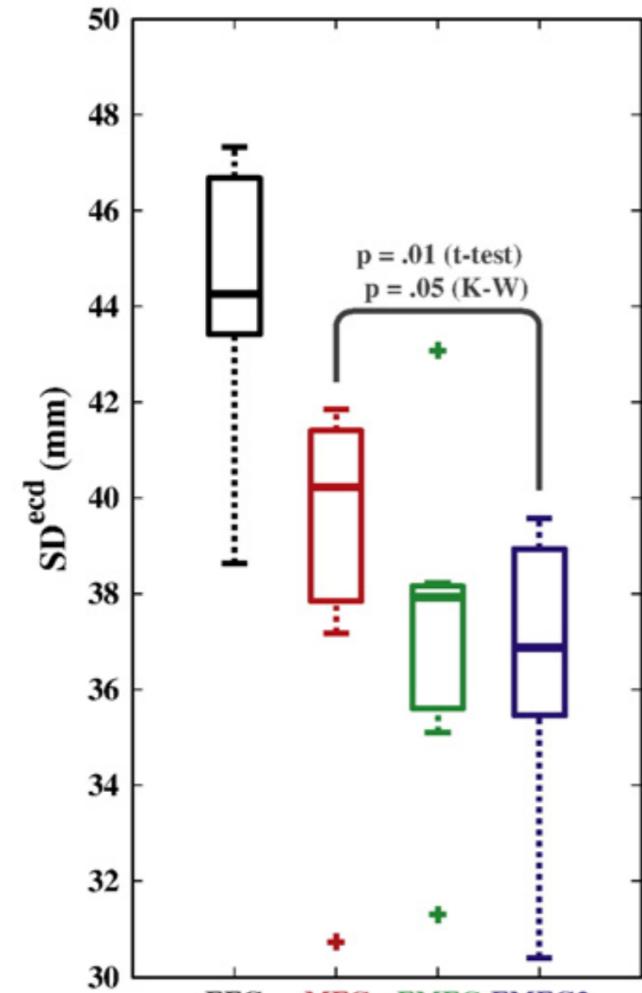
sensitivity across cortical regions

MEG+EEG are complementary



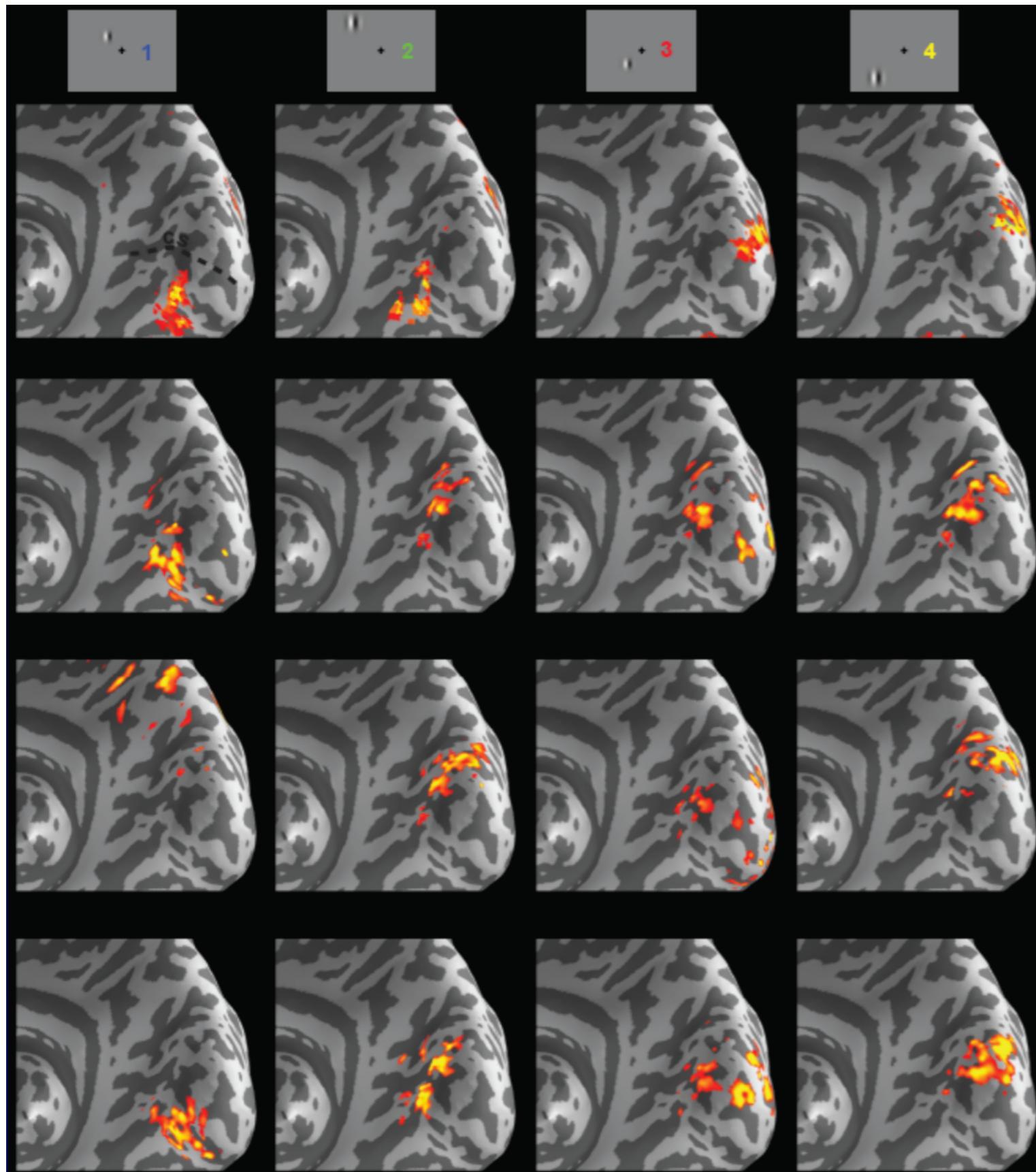
spatial dispersion of combined MEG+EEG

MEG+EEG are complementary



spatial dispersion of combined MEG+EEG

MEG+EEG map better on BOLD



fMRI

MEG

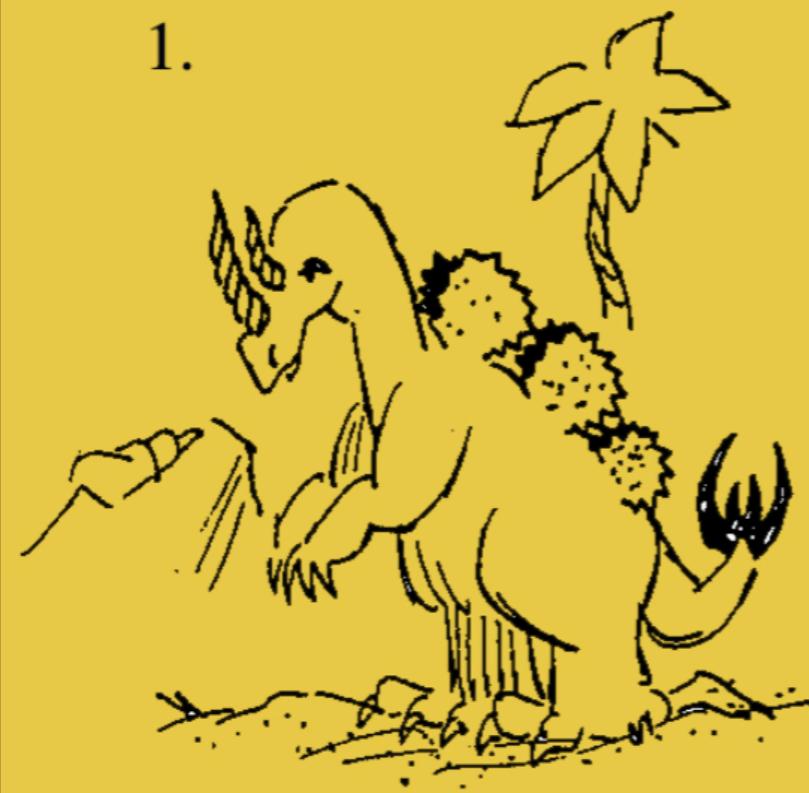
EEG

MEEG

MEG, EEG and statistics

Basic concepts, notations, modeling strategies

1.



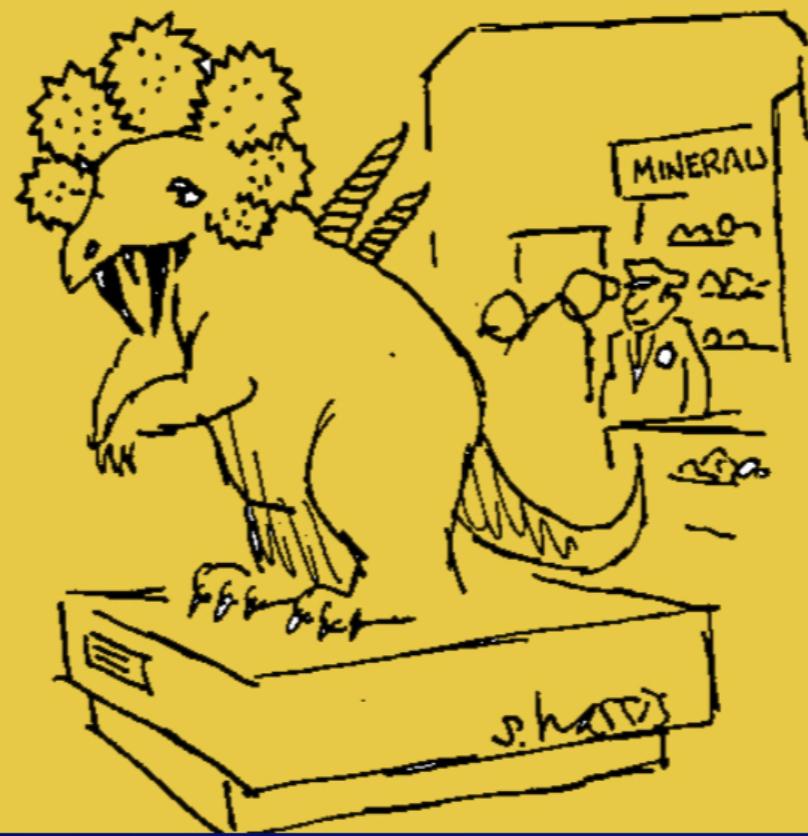
2.



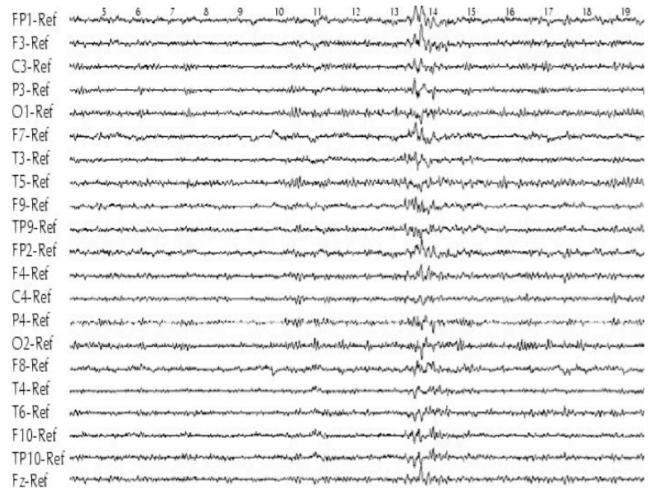
3.



4.



inverse and forward problems



can be solved

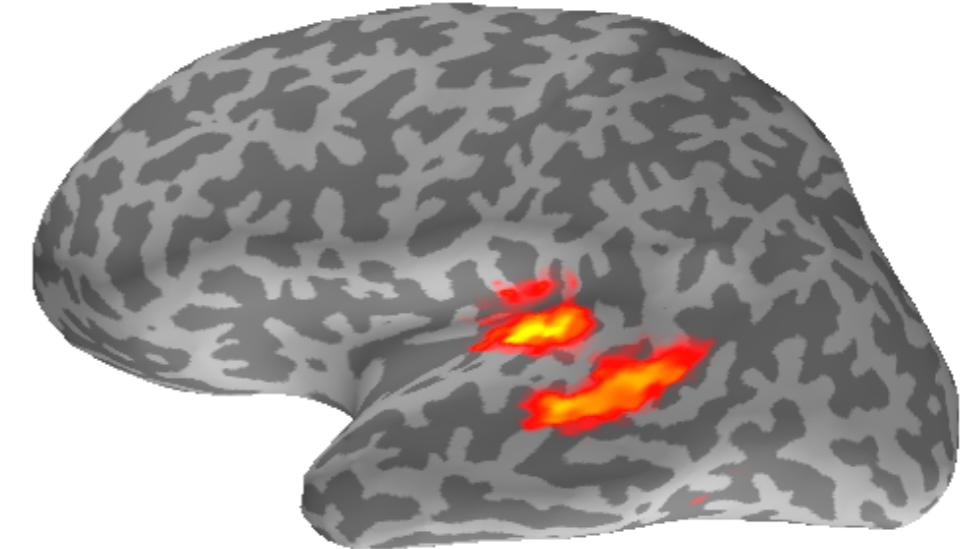
O.T! R.V. ATOME? ~~if~~ $\int S \cdot dS$ was done in the most general form in 1867. I have now lagged & & γ from T & T' and have the numerical value of $\int S \cdot dS$ in 6 lines. Thus verifying T + T' value of $\int S \cdot dS$ $\int S \cdot dS$
Your plan seems indept of T + T' or at me. Publish!
I am busy applying the physical necessities of scientific life.
Wilson II ServoScope Cambridge. Proves have
goofed in as grooves, corrugated plates, gratings
~~EEG~~ $\int S \cdot dS$. I can have time for criticism they
~~EEG~~ $\int S \cdot dS$. $\int S \cdot dS = \frac{8\pi a}{2i+1} \frac{L+i}{2L} \frac{1}{L-i}$
except when S=0 when $\int S \cdot dS = \frac{6\pi a^2}{2i+1}$
Hence $\int_{-1}^{+1} (J_i^{(G)})^2 d\mu = \frac{2}{2i+1} \frac{2^{2i} L-i}{L+i}$ without exception
you do $\frac{2}{2i+1}$

MEG/EEG

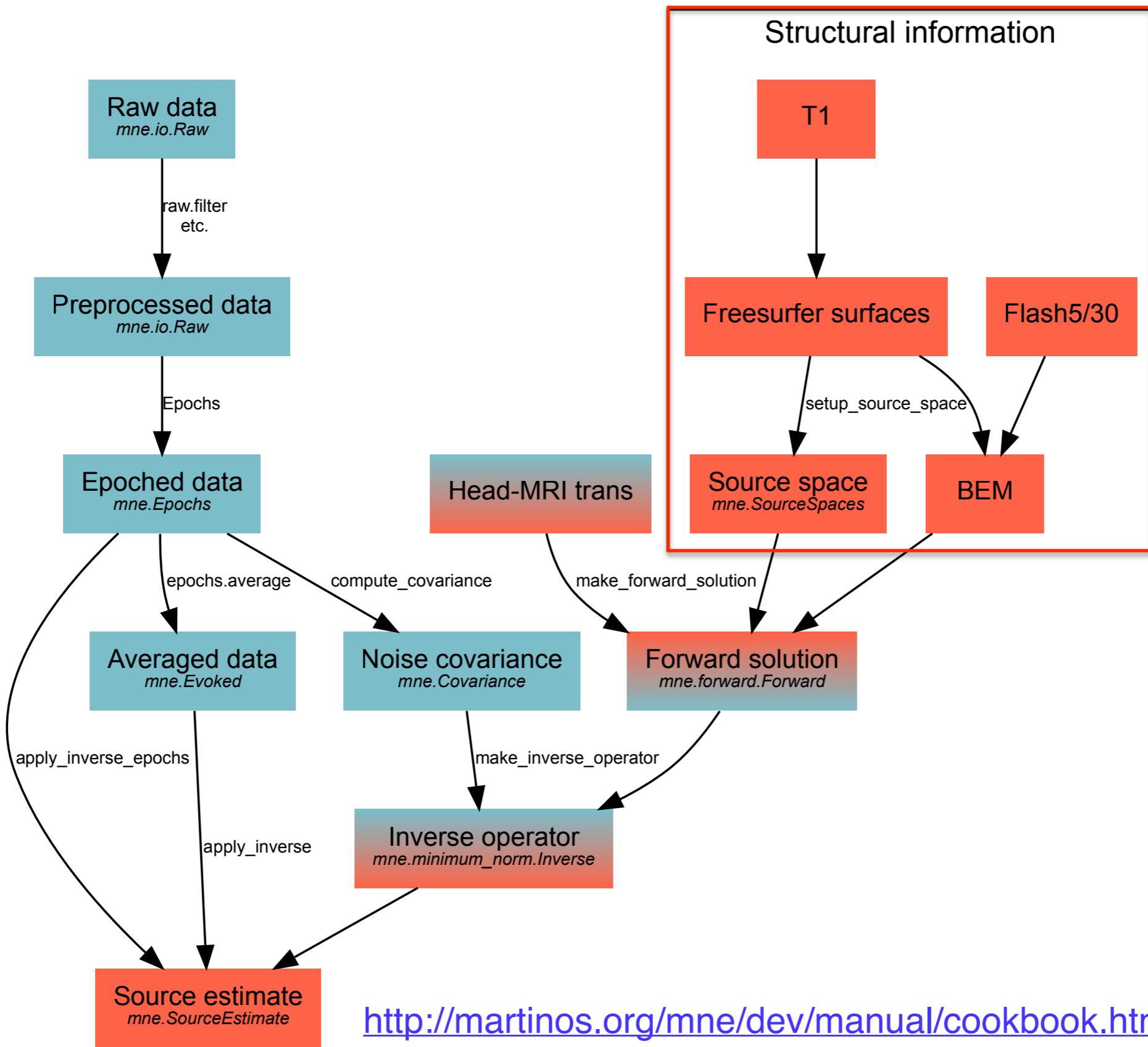
equivalent currents



ill-posed:
can only be
approximated



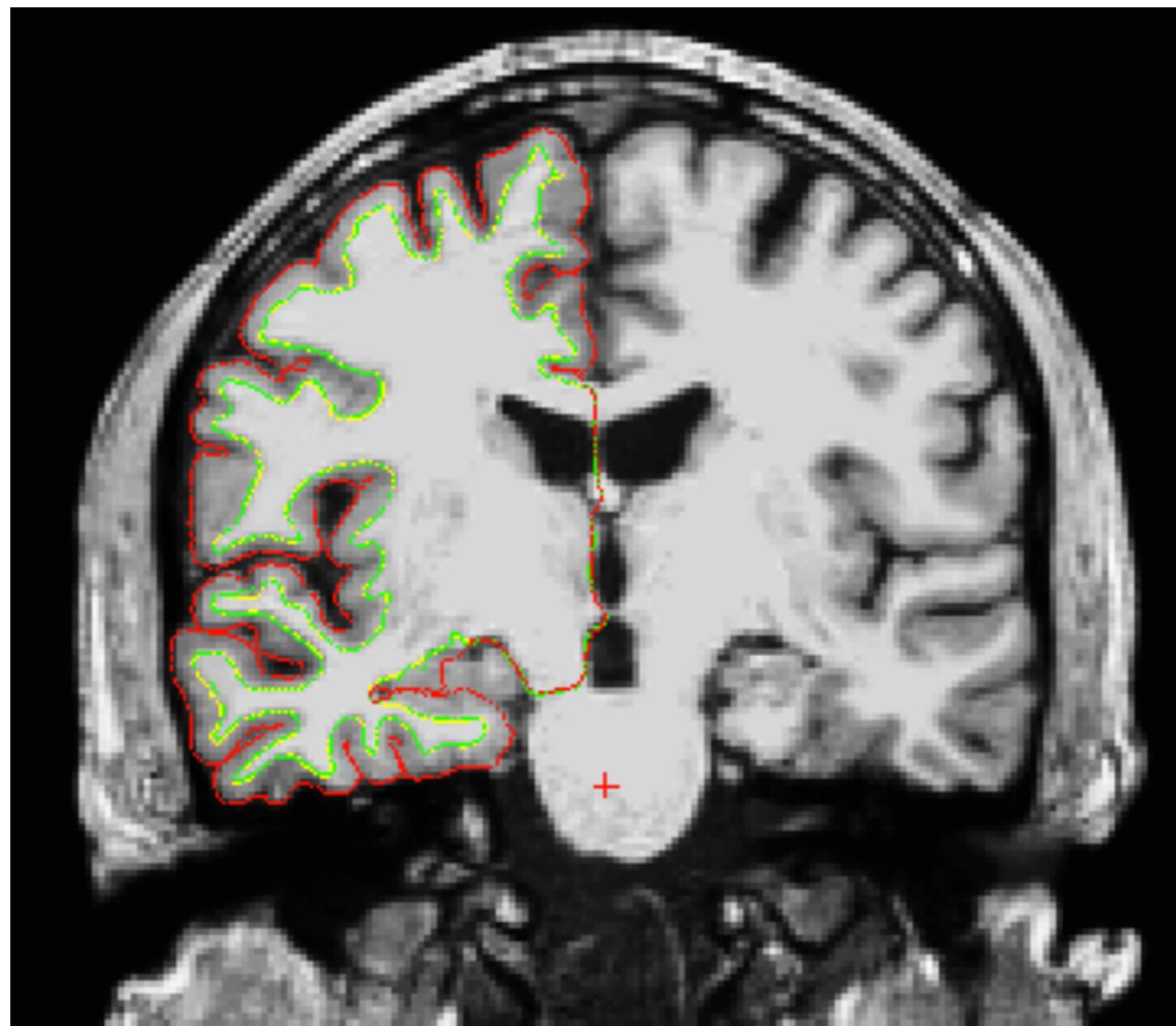
inverse modeling workflow



Freesurfer recon-all

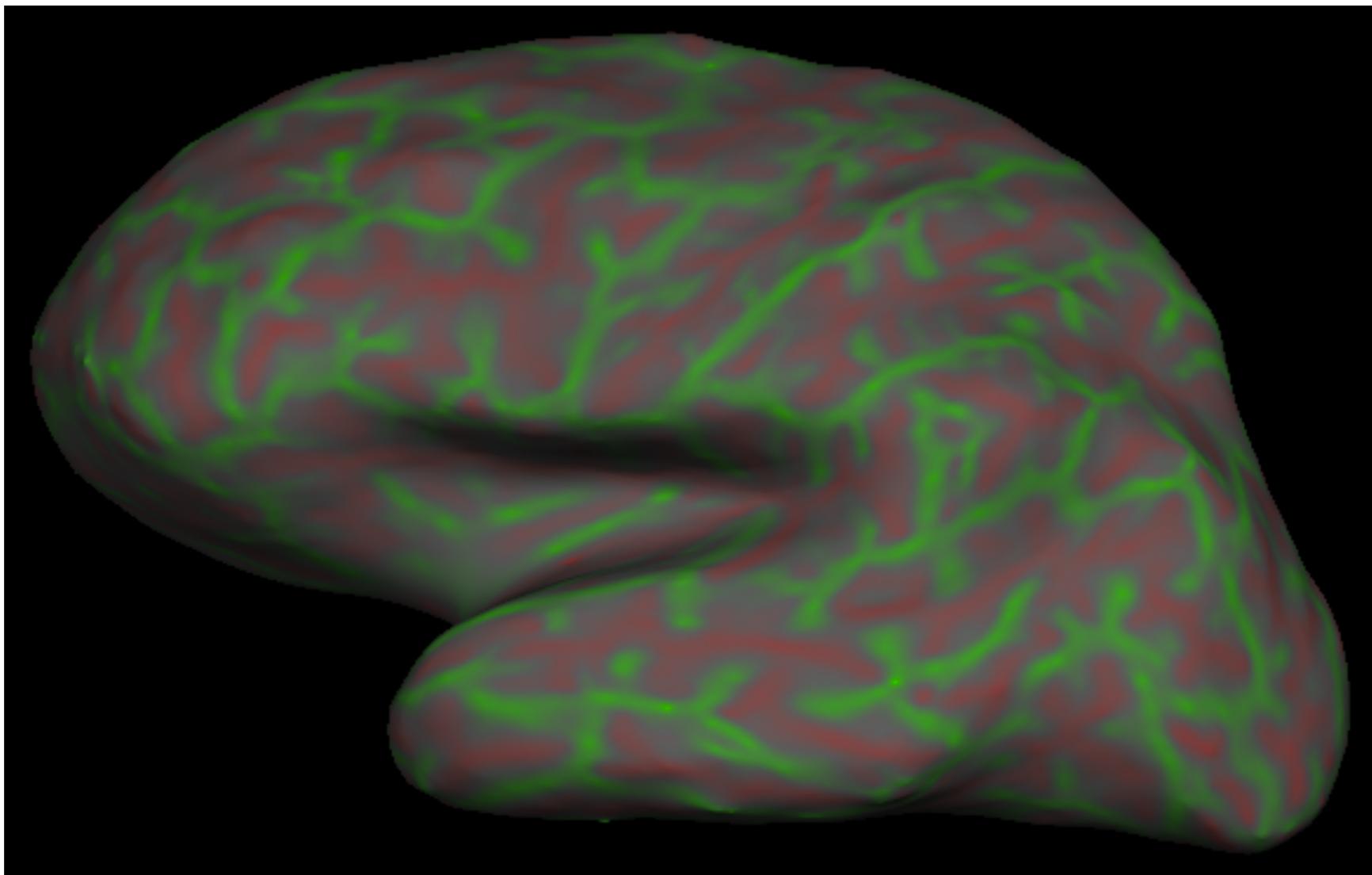
check segmentation with:

```
$ tkmedit ${SUBJECT} T1.mgz -surface rh.white
```



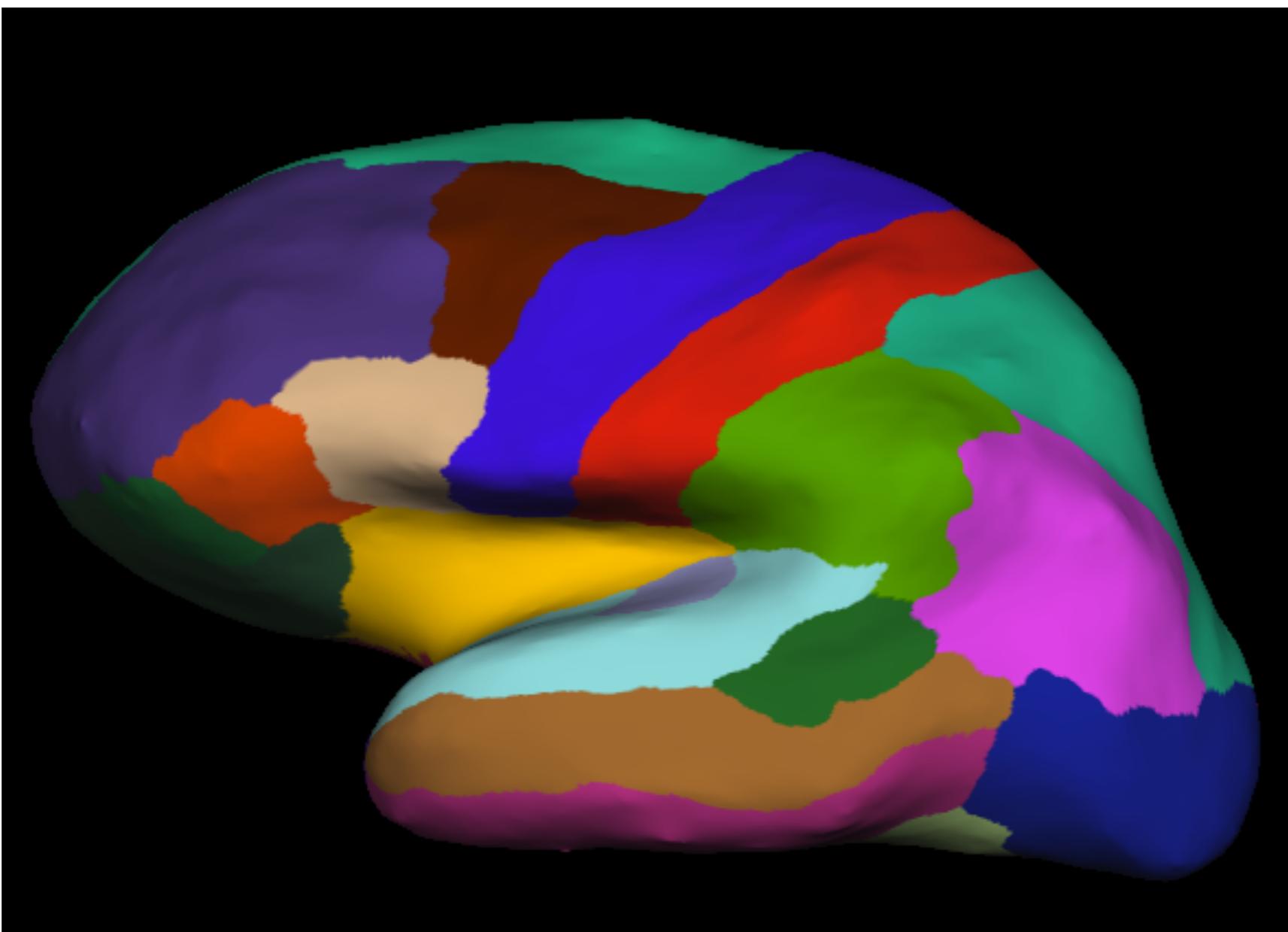
recon all — surfaces

```
$ tksurfer sample lh inflated -curv
```

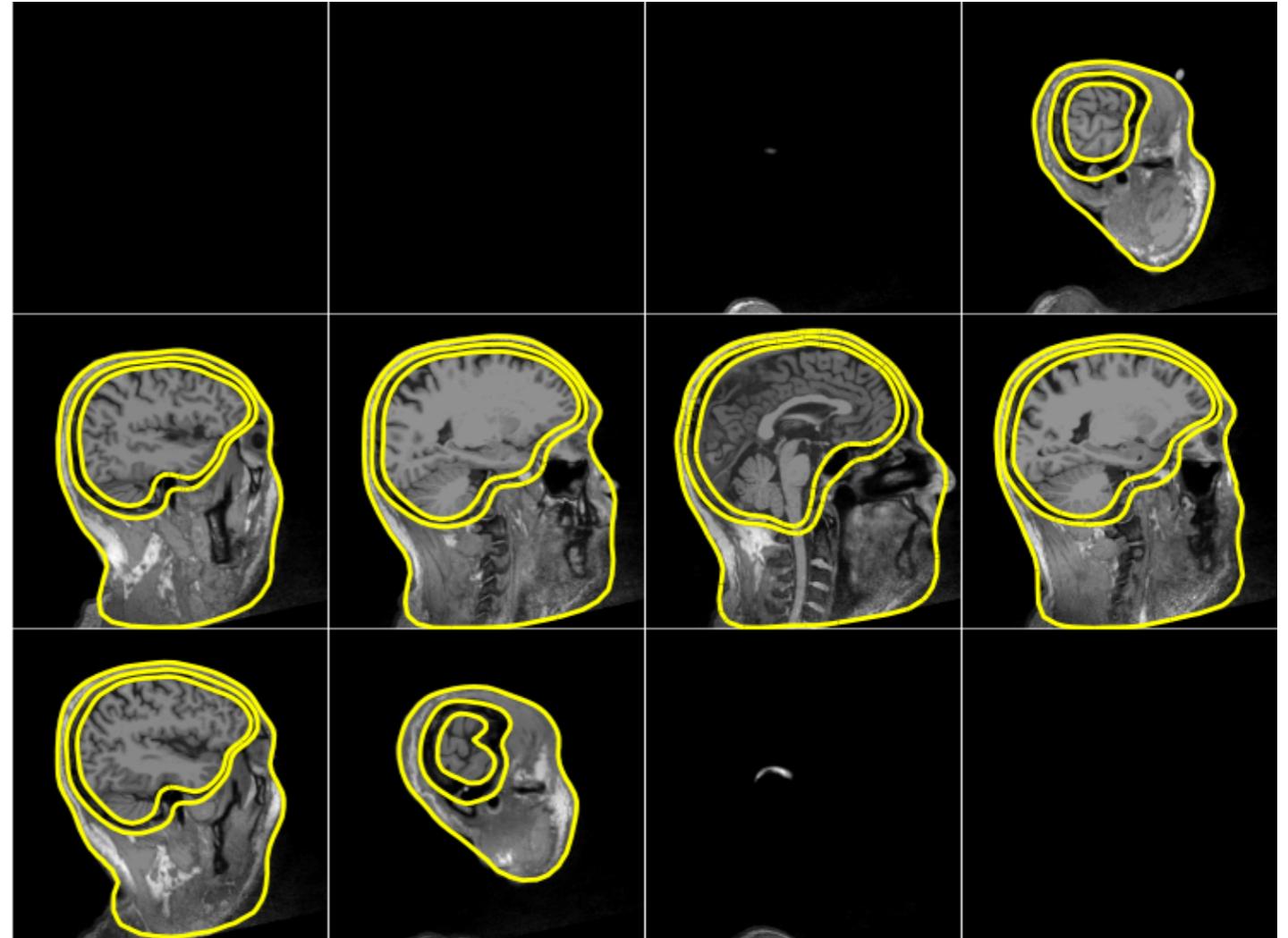
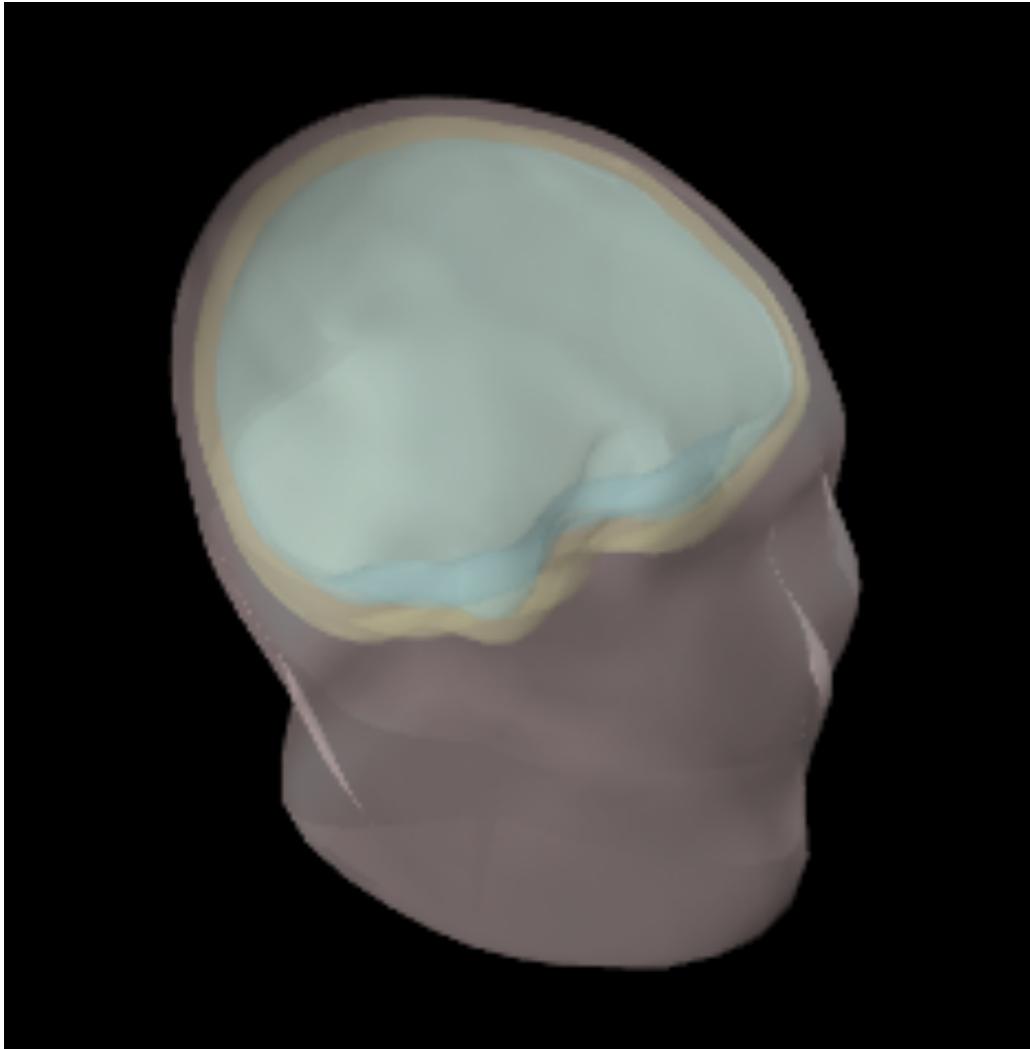


recon all — labels

```
$ tksurfer sample lh inflated -annotation aparc
```



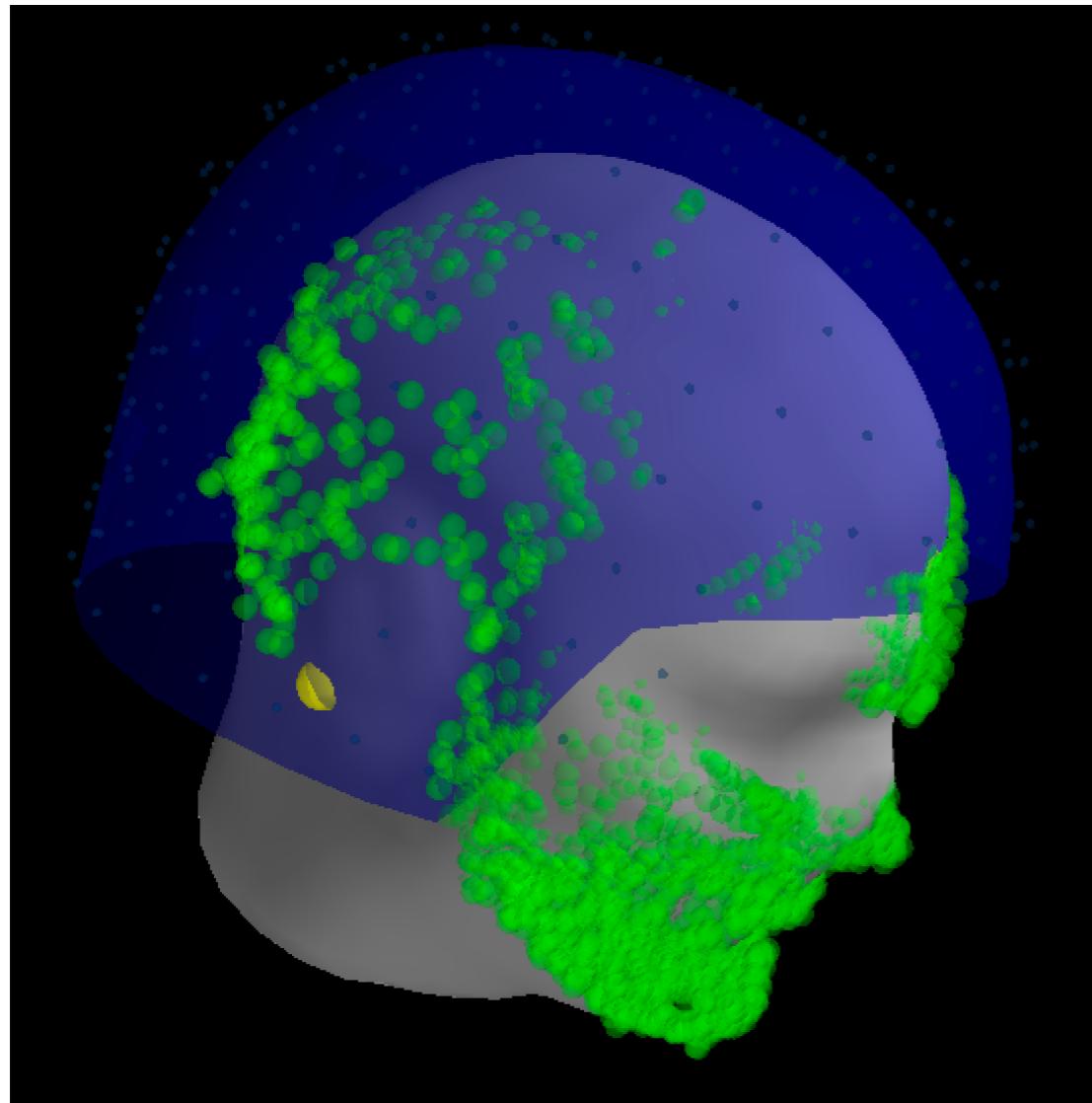
BEM surfaces



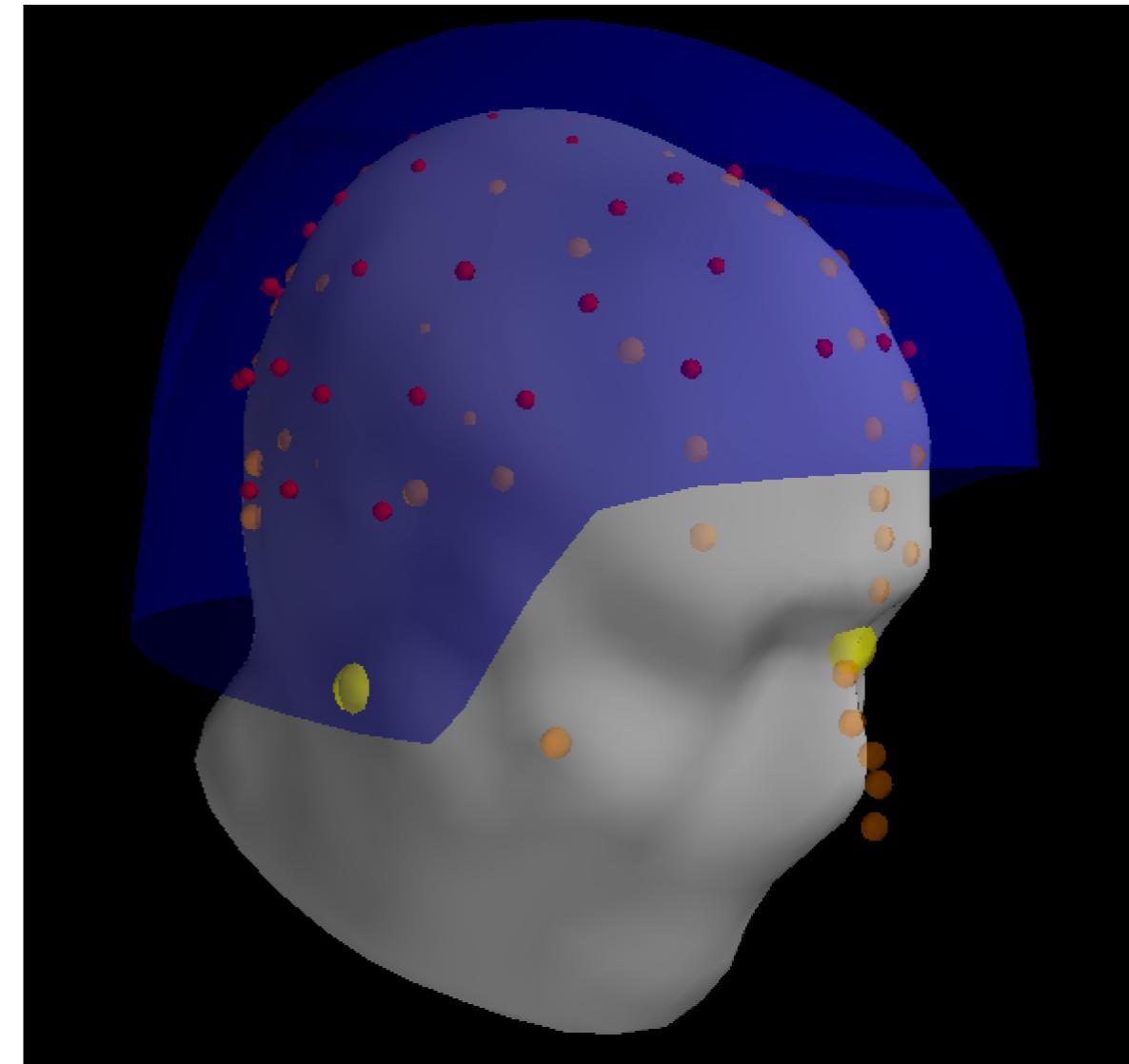
For EEG: 3 layer boundary element model (BEM):

- I) brain 2) skull 3) head

MEG (and EEG?) Coregistration

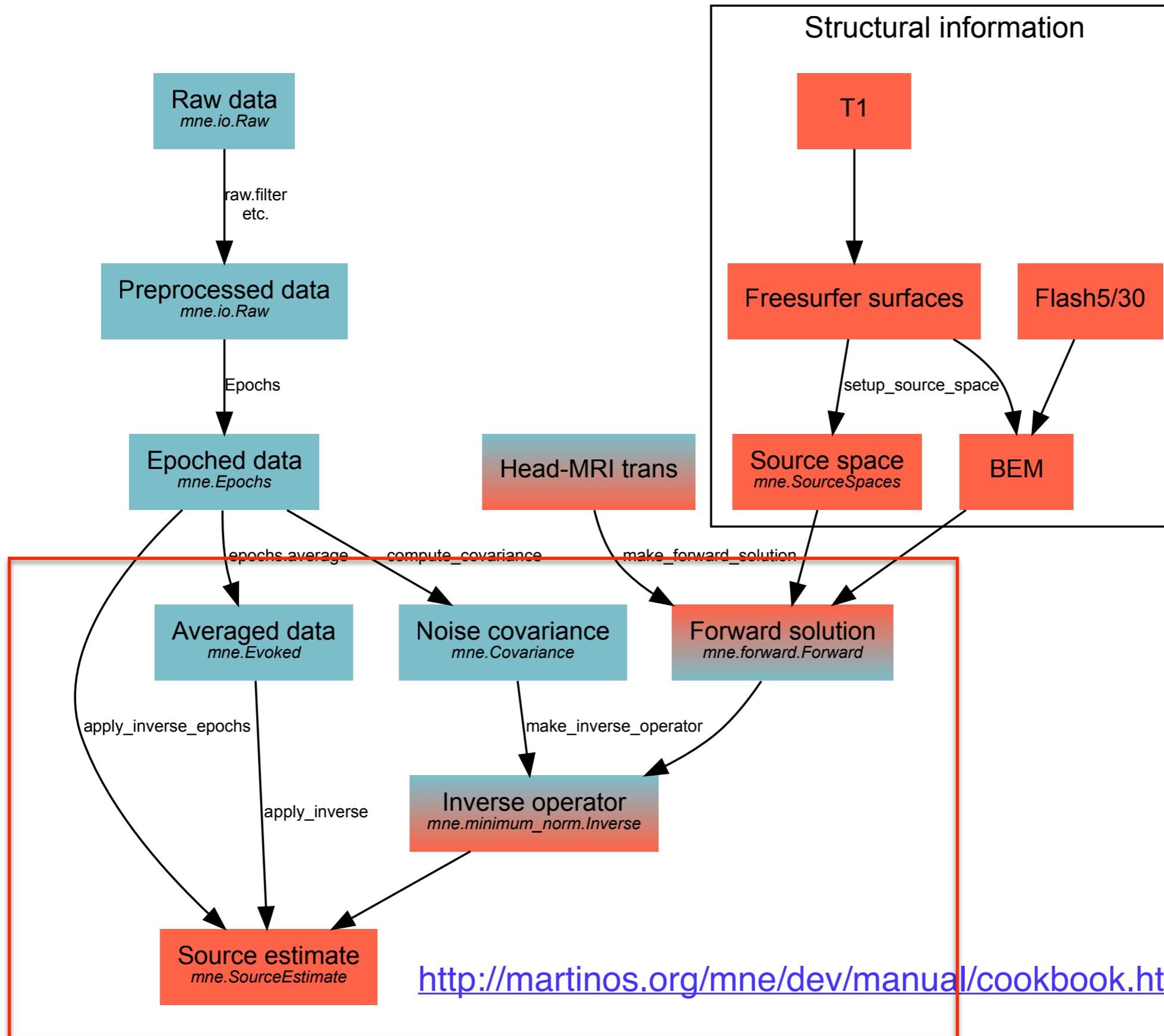


MEG + headshape points



MEG + EEG electrodes + fiducials

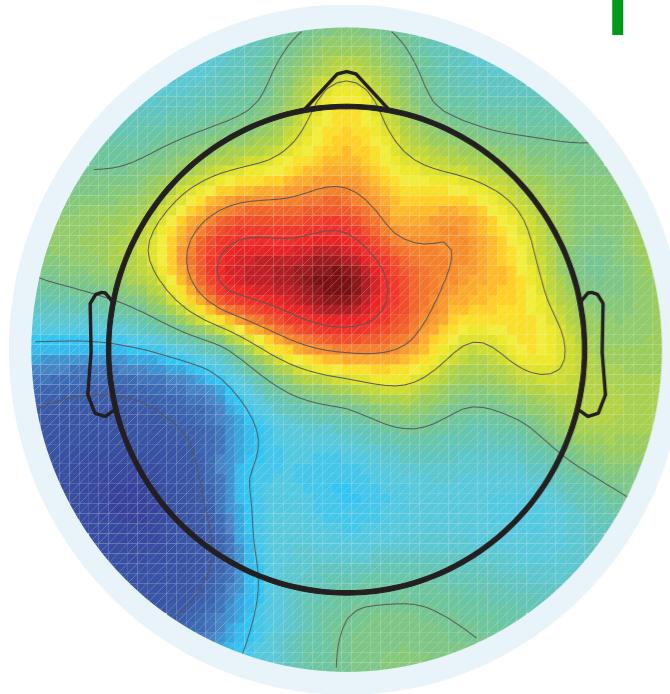
inverse modeling workflow



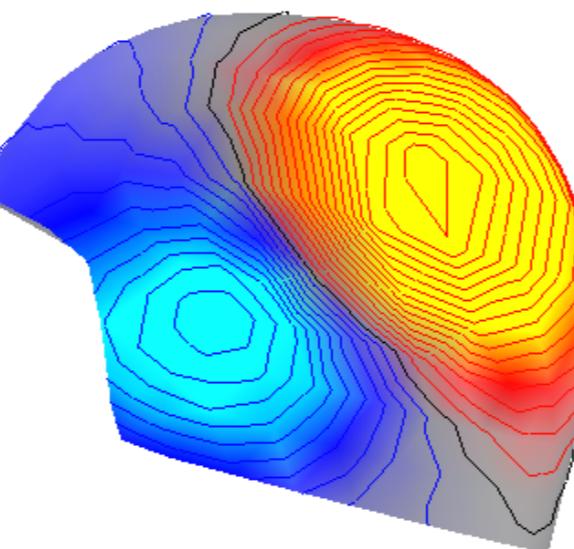
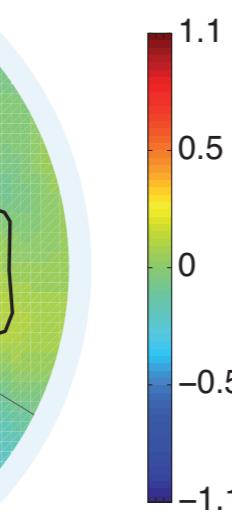
M/EEG Measurements: Notation

$$M = \begin{bmatrix} & \\ & \textcolor{red}{\boxed{\text{MEG}}} \\ & \end{bmatrix} \in \mathbb{R}^{d_m \times d_t}$$

MEG
and/or
EEG

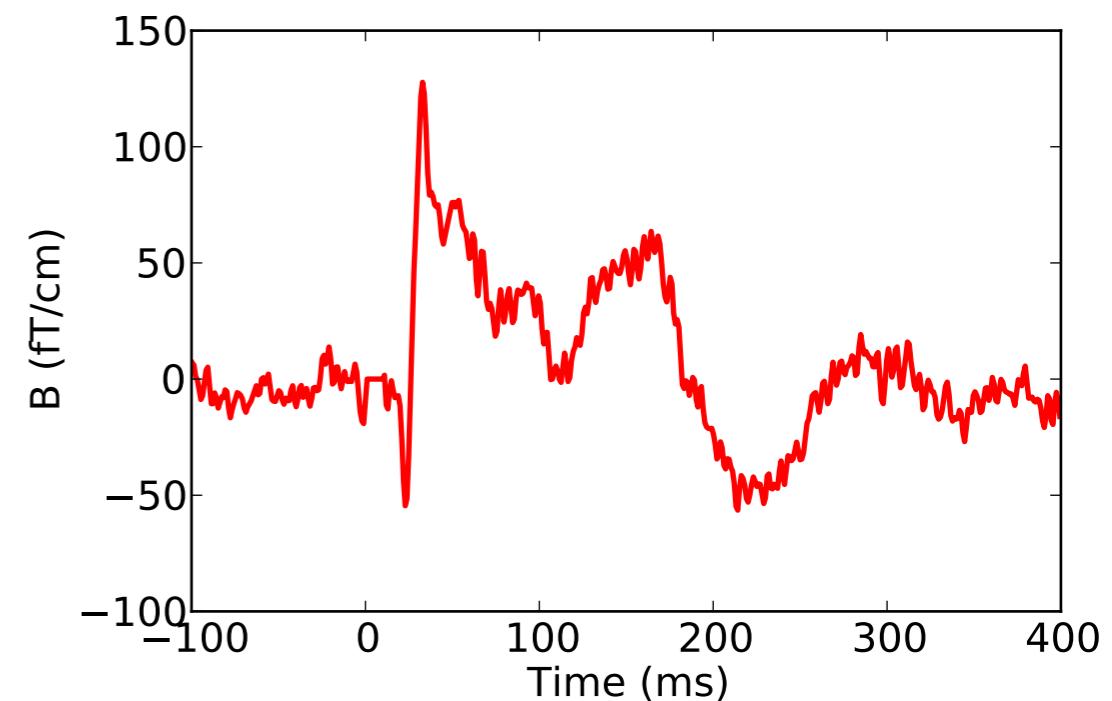


2D topography



3D topography

d_m : Nb of sensors
 d_t : Nb of time points



I row = I time series
on I sensor

L2 a.k.a. Minimum Norm Estimates (MNE)

$$\phi(\mathbf{X}) = \|\mathbf{WX}\|_F^2 = \sum_{i,j} w_i^2 x_{ij}^2 = \|\mathbf{X}\|_{\Sigma,2}^2$$

$\mathbf{W}^2 = \Sigma$ *source covariance*

Leads to a **closed form solution** (matrix multiplication):

$$\hat{\mathbf{X}} = \mathbf{R}\mathbf{G}^t (\mathbf{G}\mathbf{R}\mathbf{G}^t + \mathbf{C})^{-1} \mathbf{Y}$$

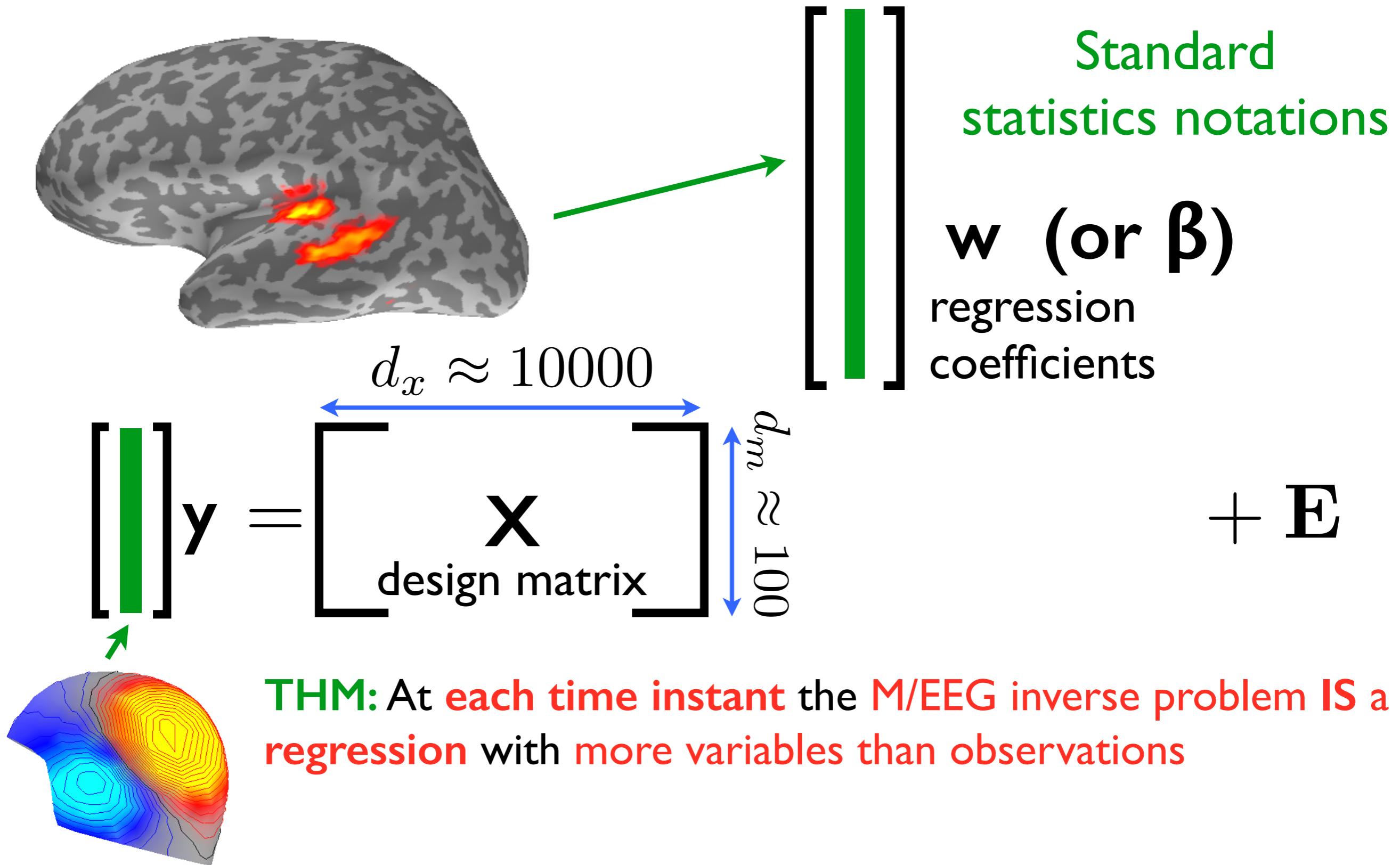
[Tikhonov et al. 77, Wang et al. 92, Hämäläinen et al. 94]

Remarks:

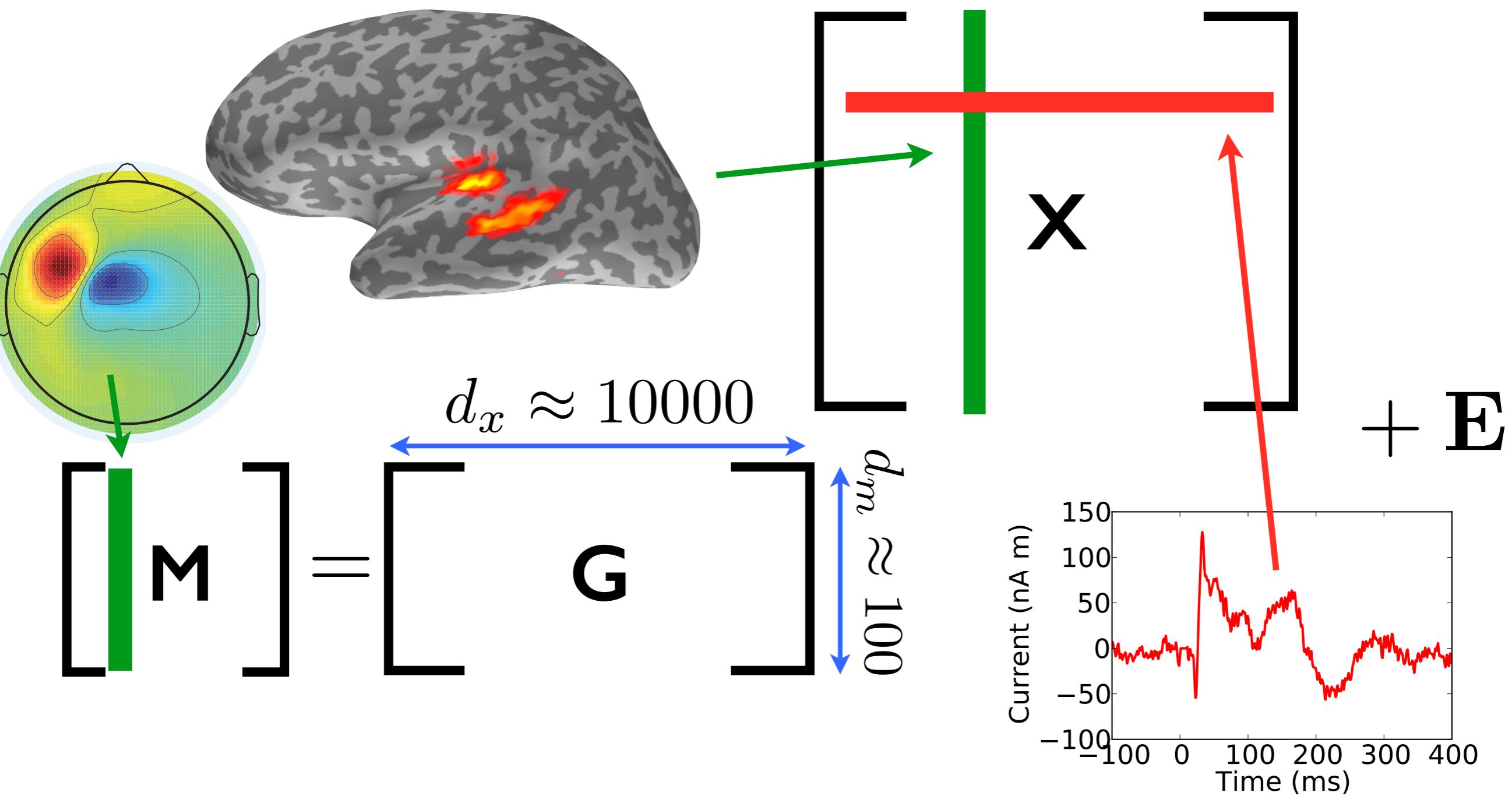
- **Really fast** to compute (SVD of \mathbf{G}), hence very much used in the field.
- In practice, it's **much more complicated** (whitening data, correcting artifacts, channels with different SNRs, setting λ based on SNR, loose orientation, SNR varies with time...)

THM: A lot of domain knowledge to make it work²⁴

$y = Xw + E$: An ill-posed problem

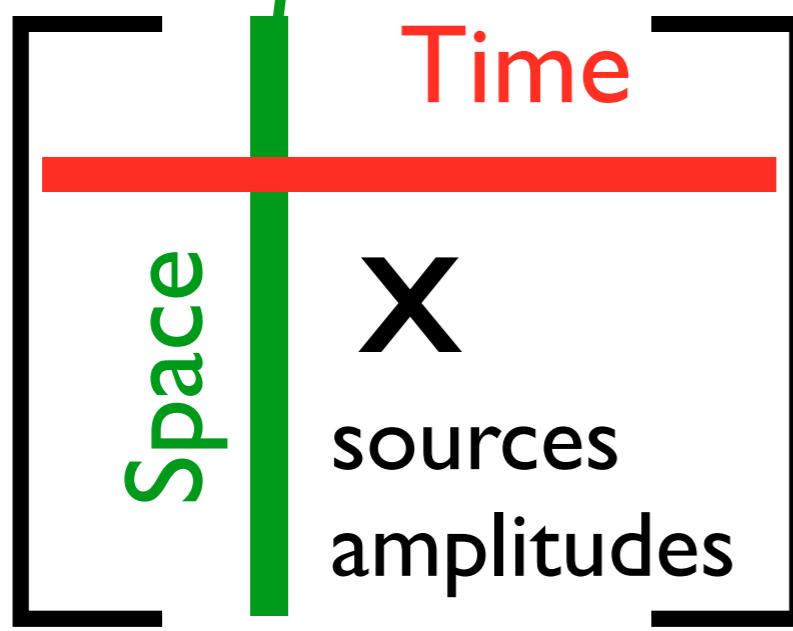
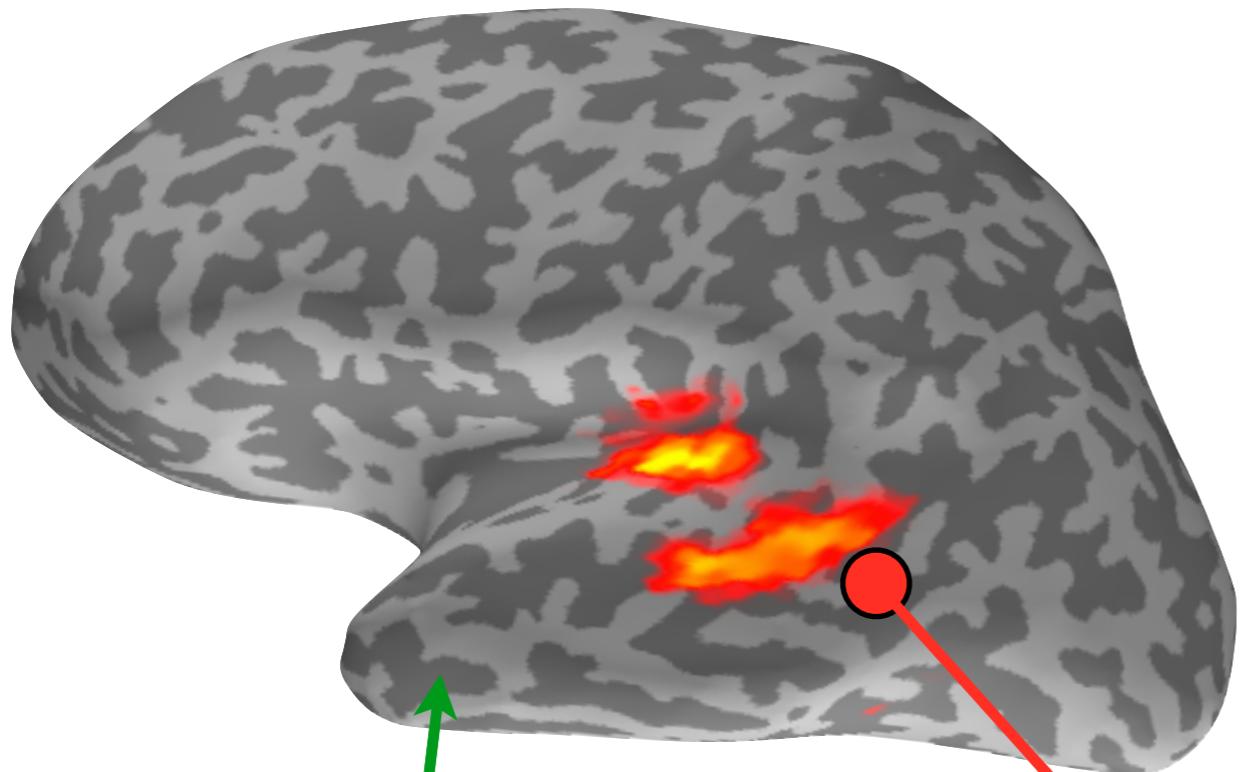


Basic distributed model: $M = GX + E$



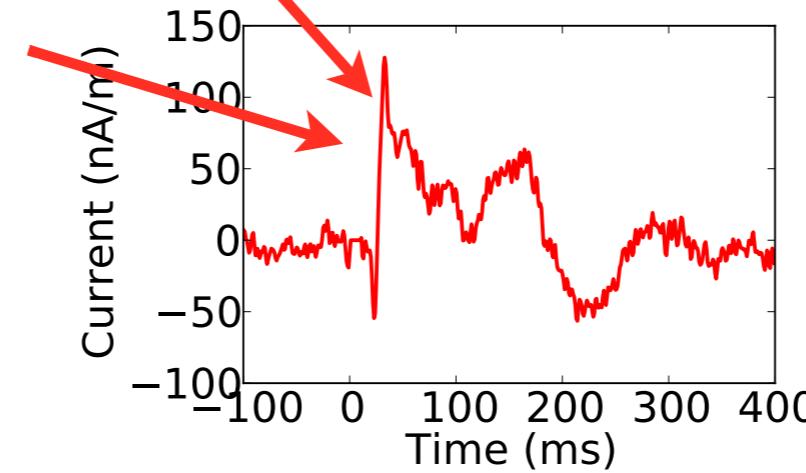
Linear problem with more unknowns than the number of equations: it's ill-posed => Regularize

Distributed model



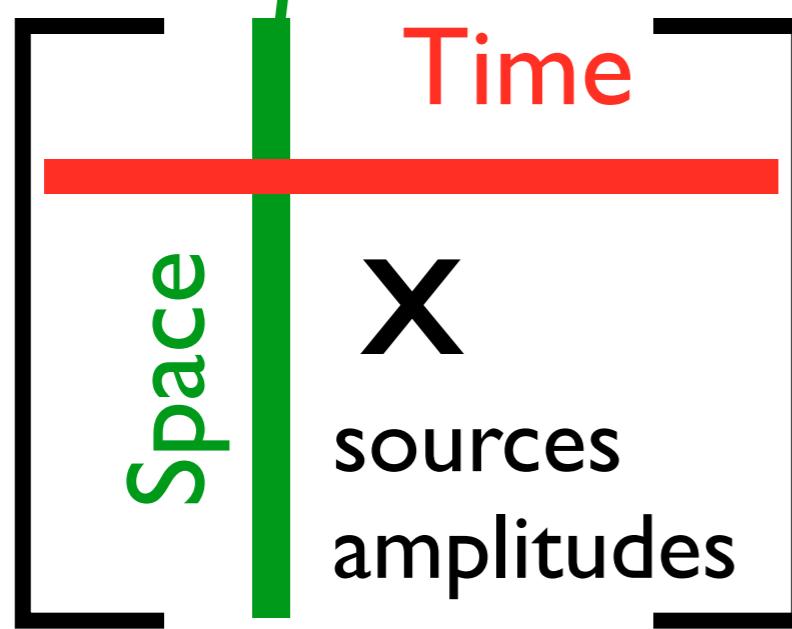
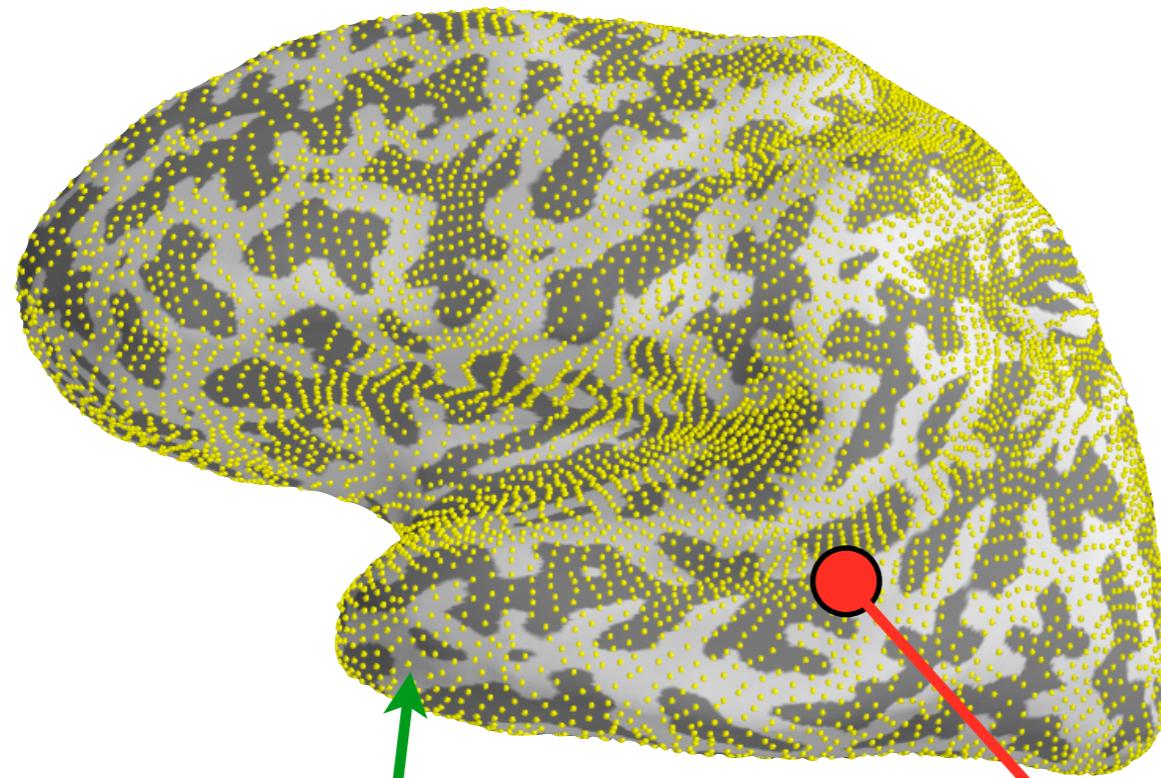
Scalar field defined over time

Position 5000 candidate
sources over each
hemisphere
(e.g. every 5mm)



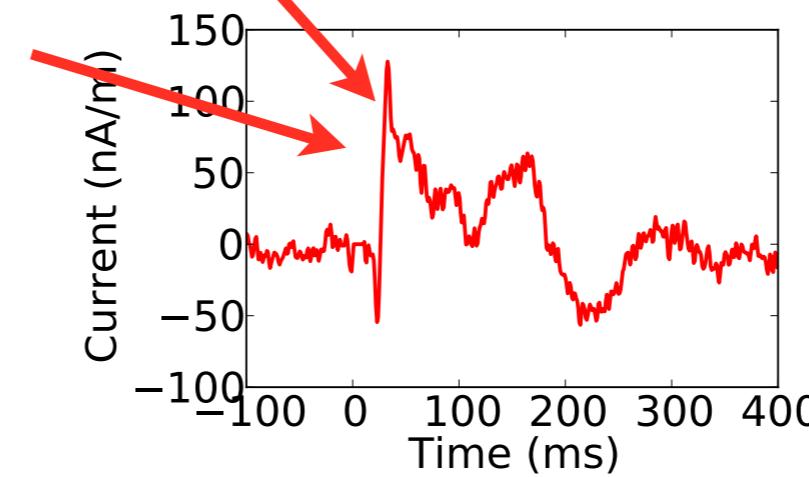
[Dale and Sereno 93]

Distributed model



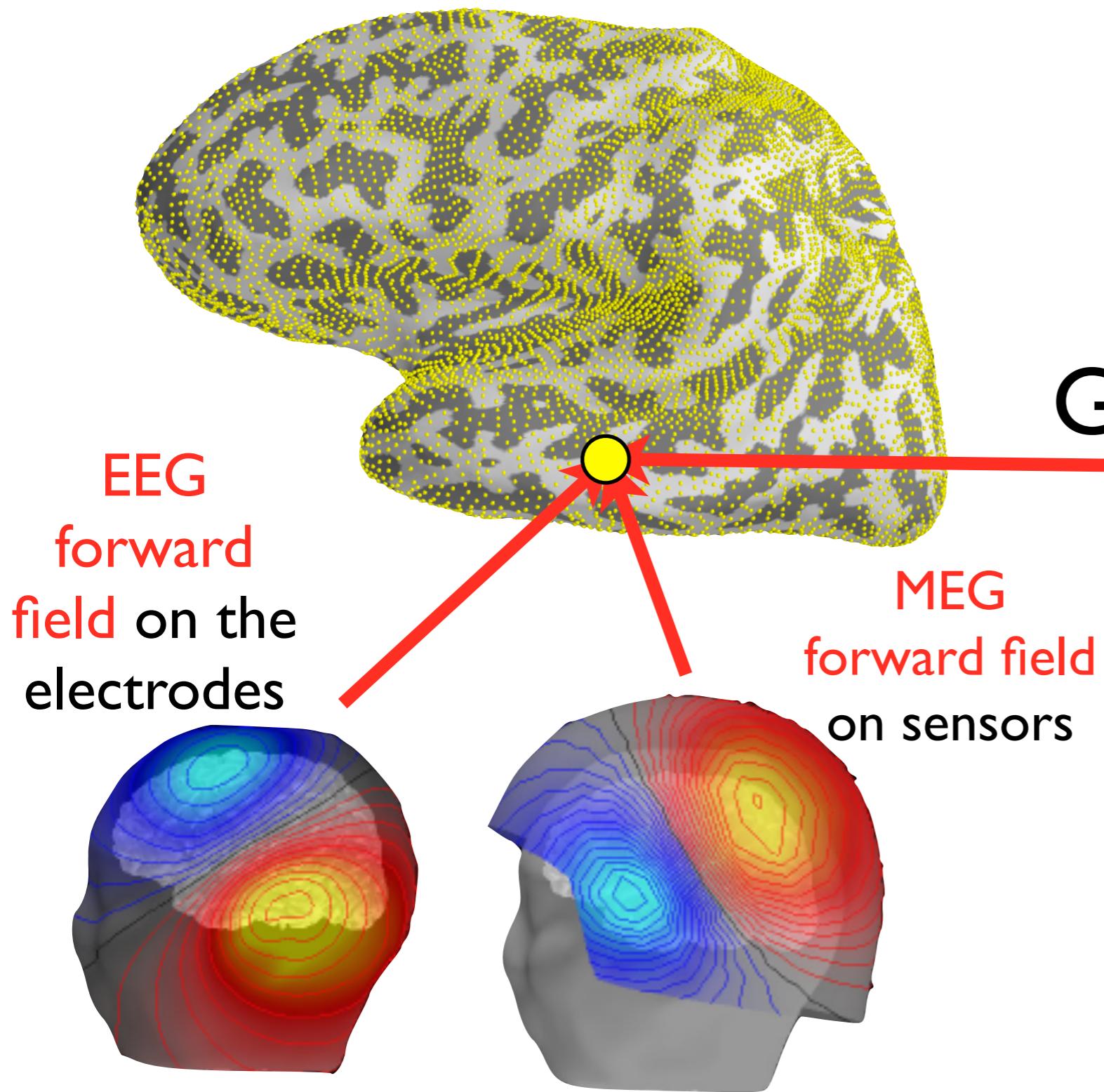
Scalar field defined over time

Position 5000 candidate sources over each hemisphere
(e.g. every 5mm)



[Dale and Sereno 93]

Distributed model

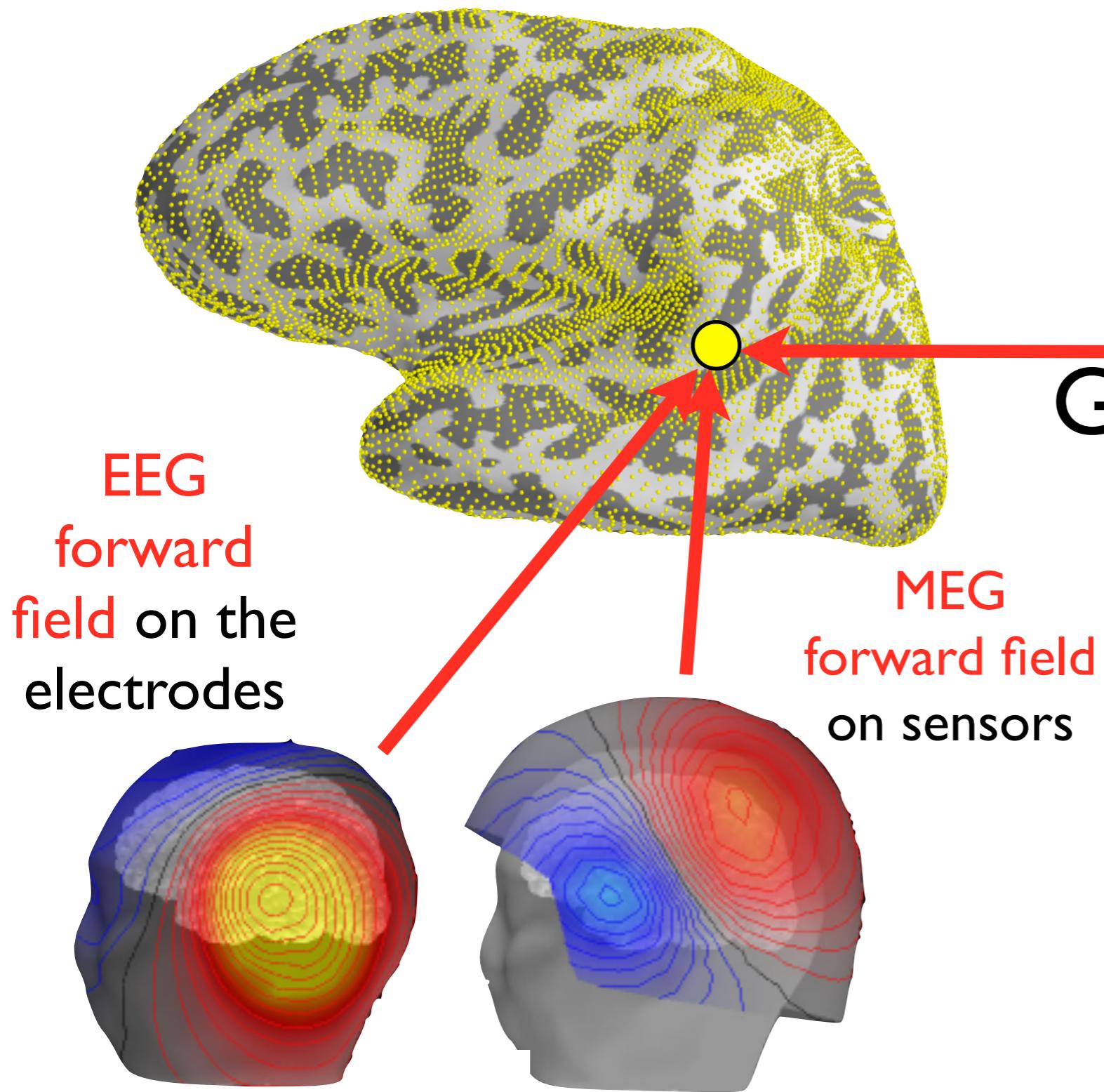


one column = Forward field of one dipole

$$G = \begin{bmatrix} \text{---} & | & \text{---} \\ G_{\text{EEG}} & | & G_{\text{MEG}} \\ \text{---} & | & \text{---} \end{bmatrix}$$

G is the gain matrix obtained by concatenation of the forward fields

Distributed model

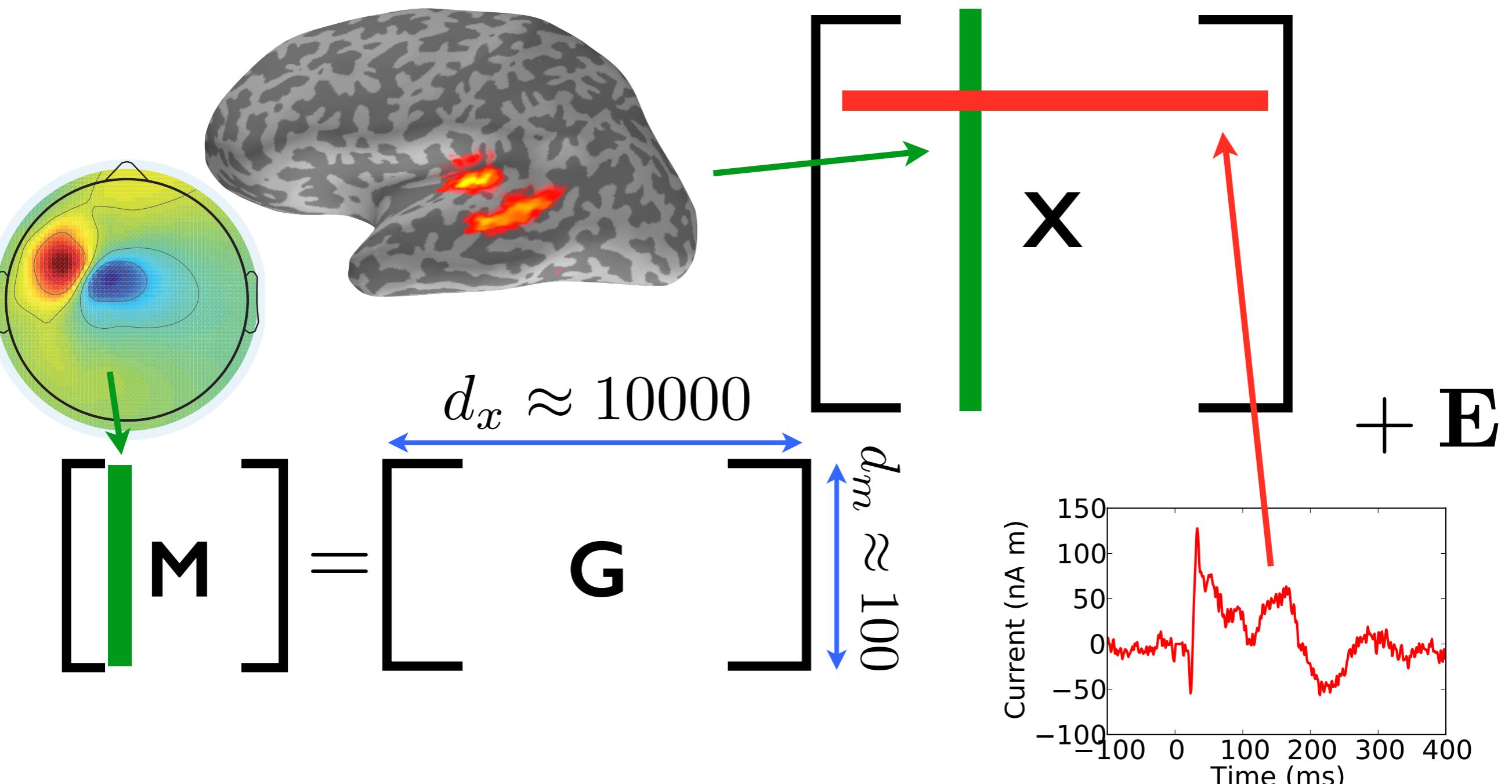


one column = Forward field of one dipole

$$G = \begin{bmatrix} G_{EEG} \\ G_{MEG} \end{bmatrix}$$

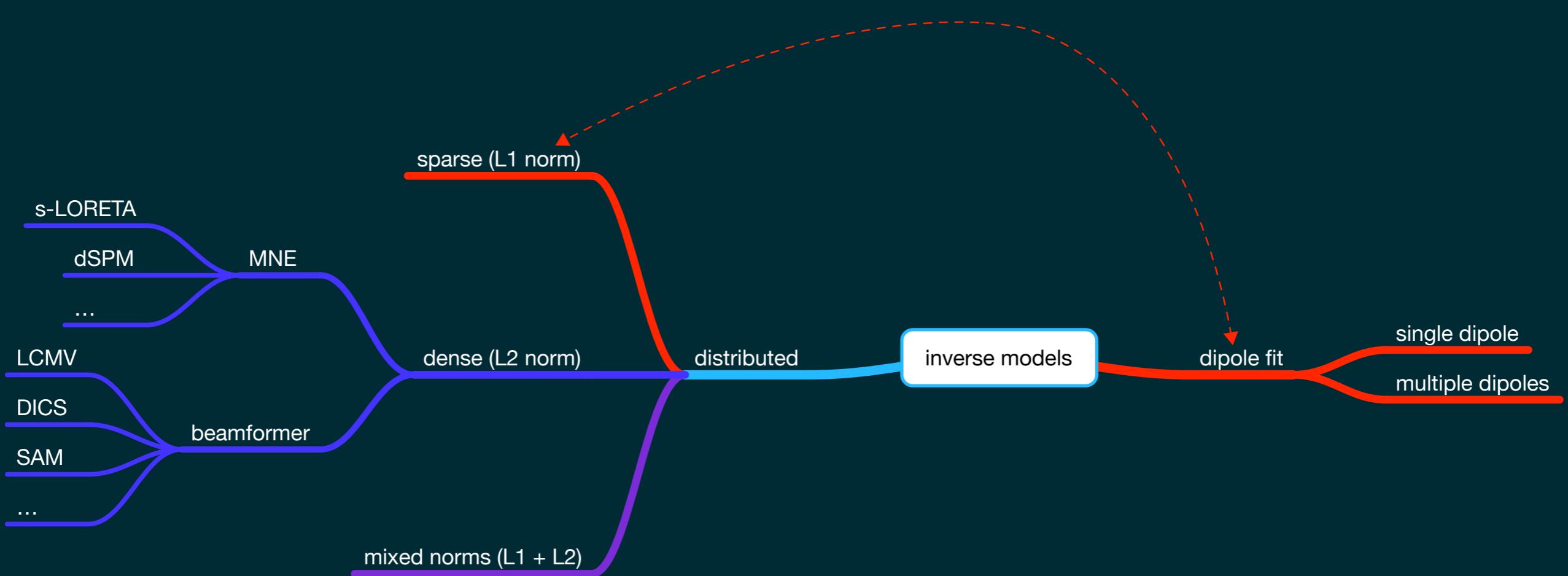
G is the gain matrix obtained by concatenation of the forward fields

$M = GX + E$: An ill-posed problem



Linear problem with more unknowns than the number of equations: it's ill-posed => Regularize

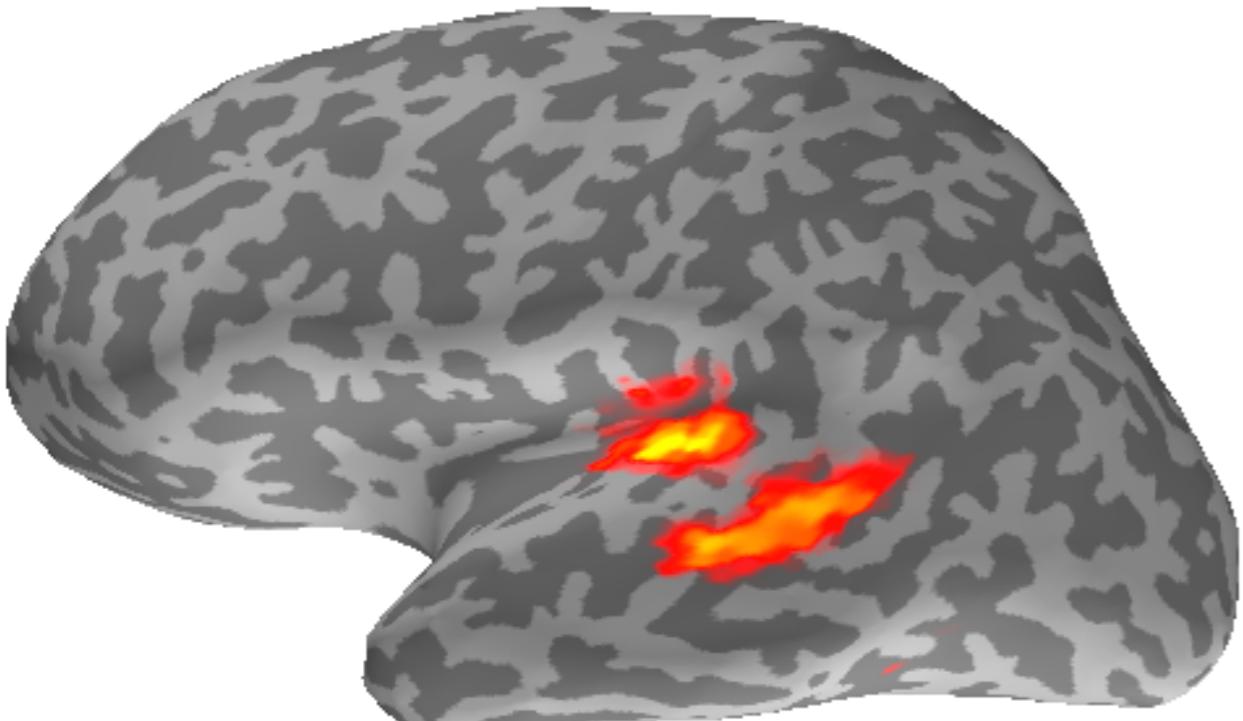
What's my model?



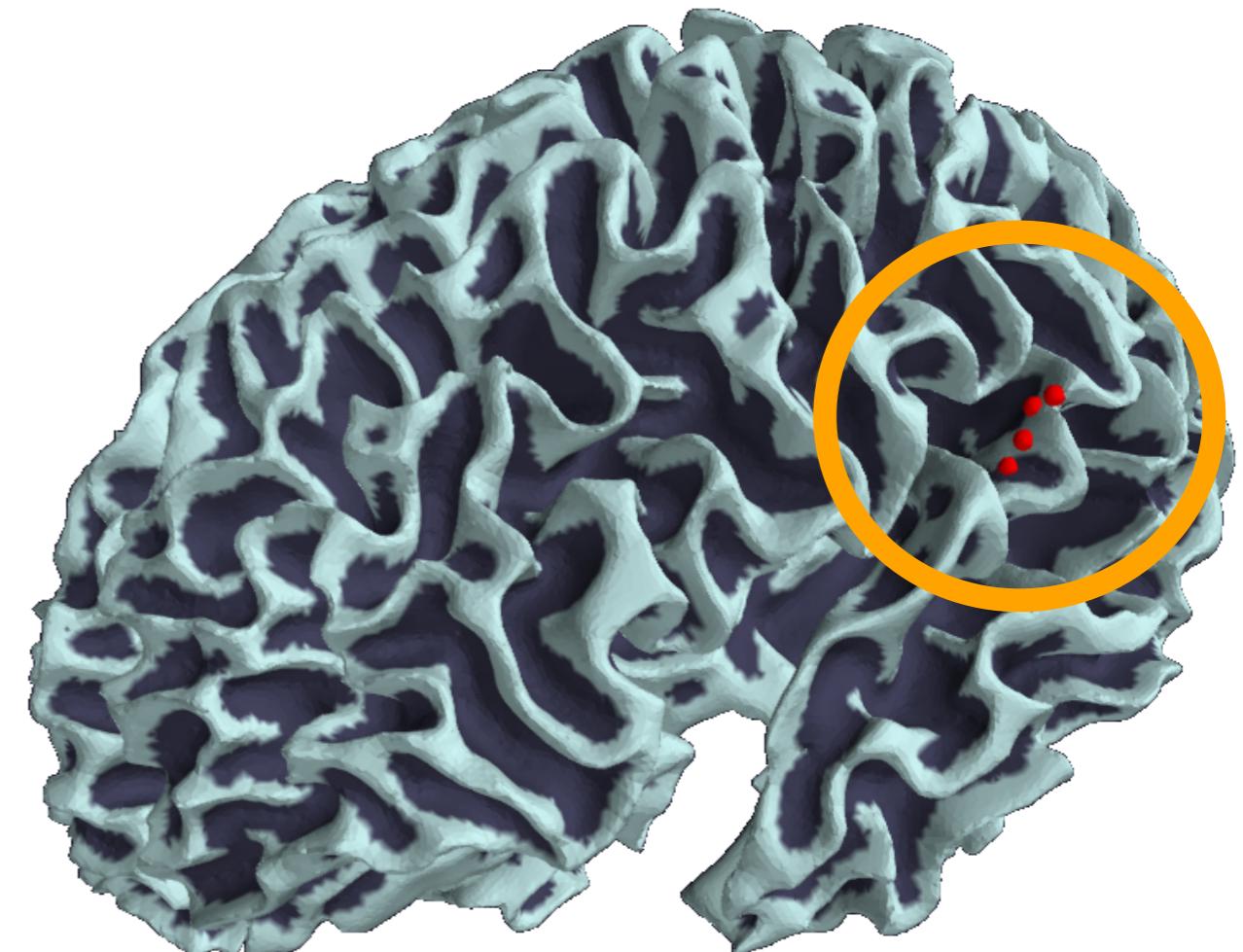
LI vs L2 norms on combined M/EEG data

Activation in left-auditory cortex

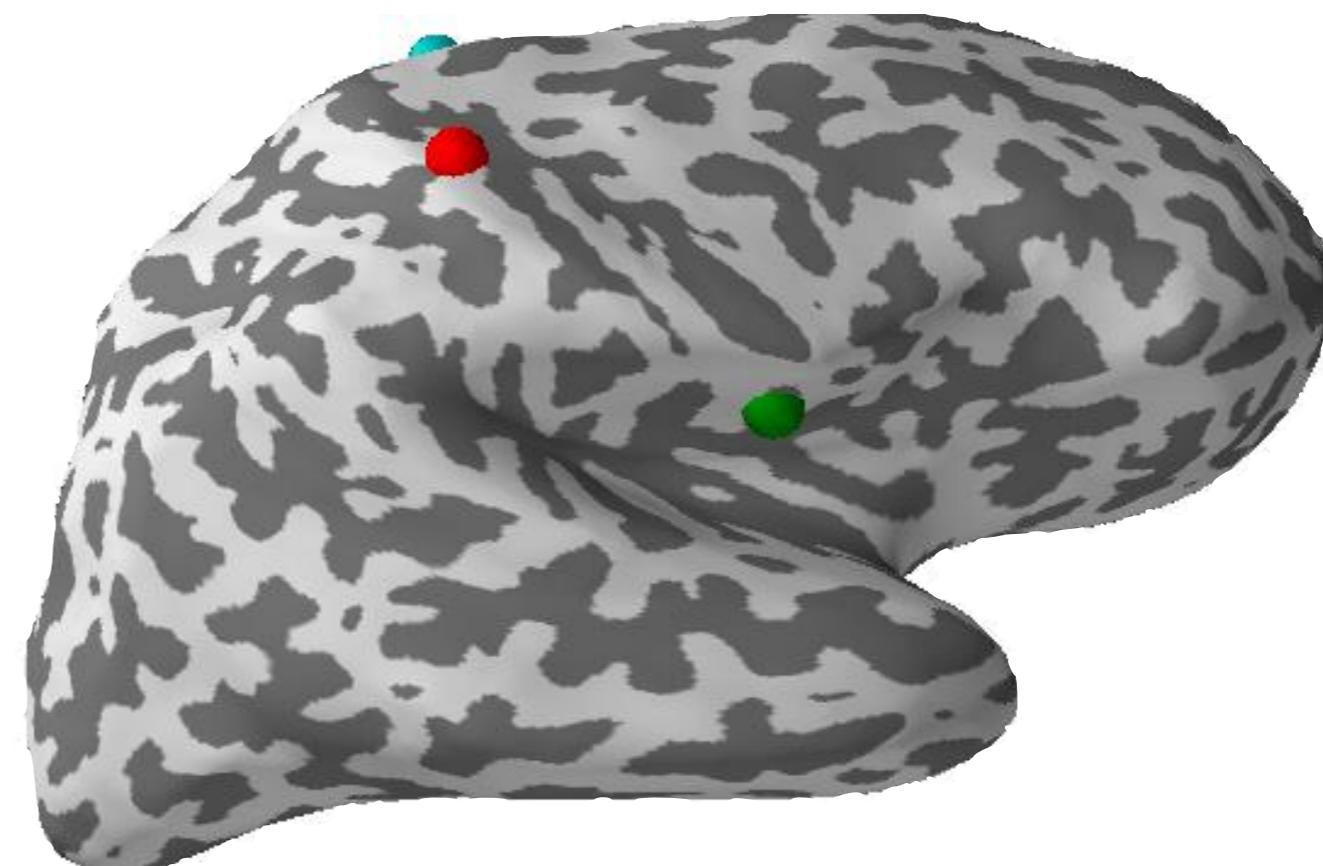
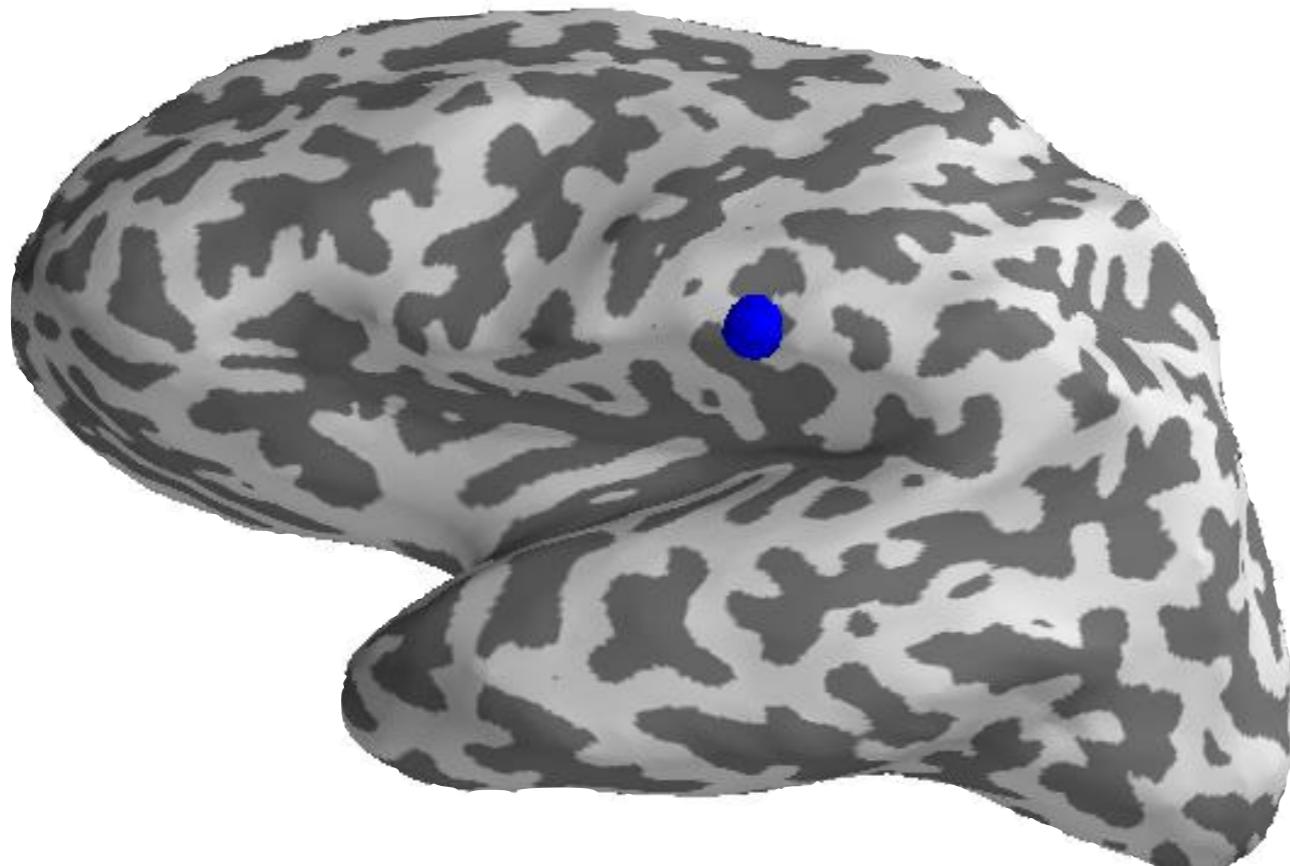
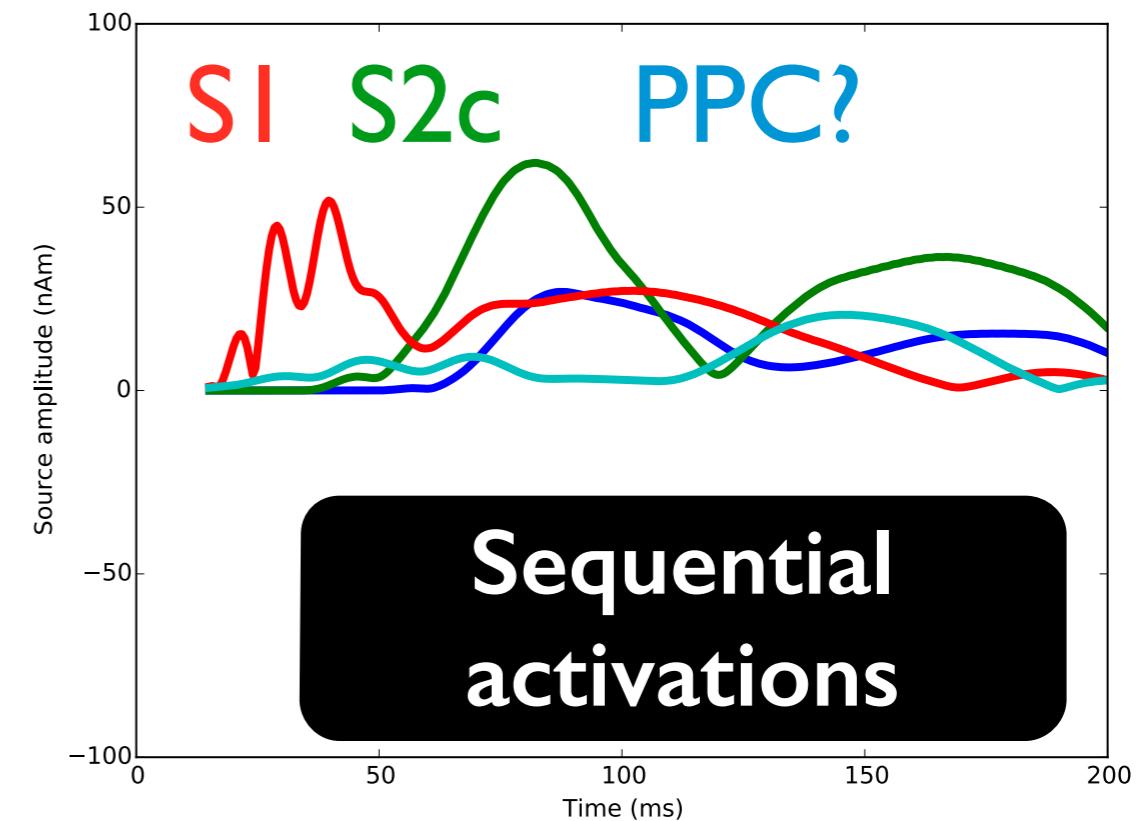
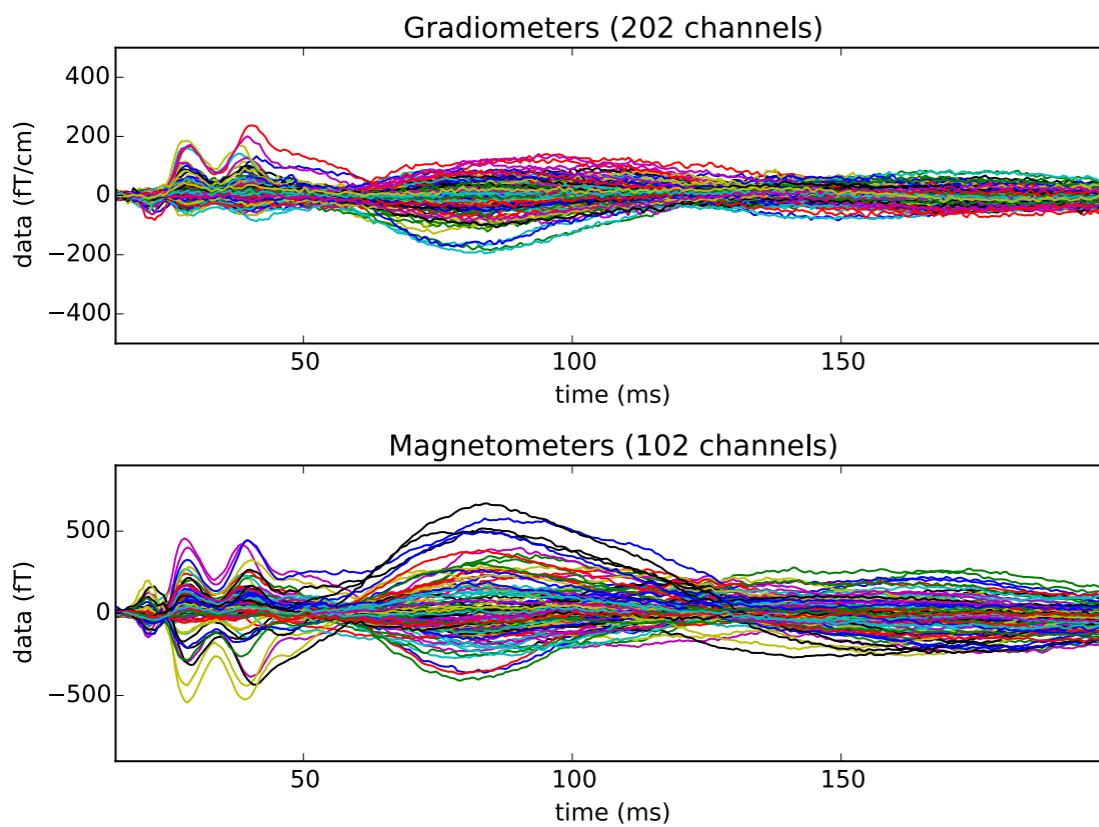
L2 result (thresholded)



LI result



$L^1,2$ mixed norm on MEG data



Inverse problem framework

Penalized (variational) formulation (with whitened data):

$$\mathbf{X}^* = \arg \min_{\mathbf{X}} \|\mathbf{M} - \mathbf{G}\mathbf{X}\|_F^2 + \lambda \phi(\mathbf{X}), \lambda > 0$$

Data fit **Regularization**

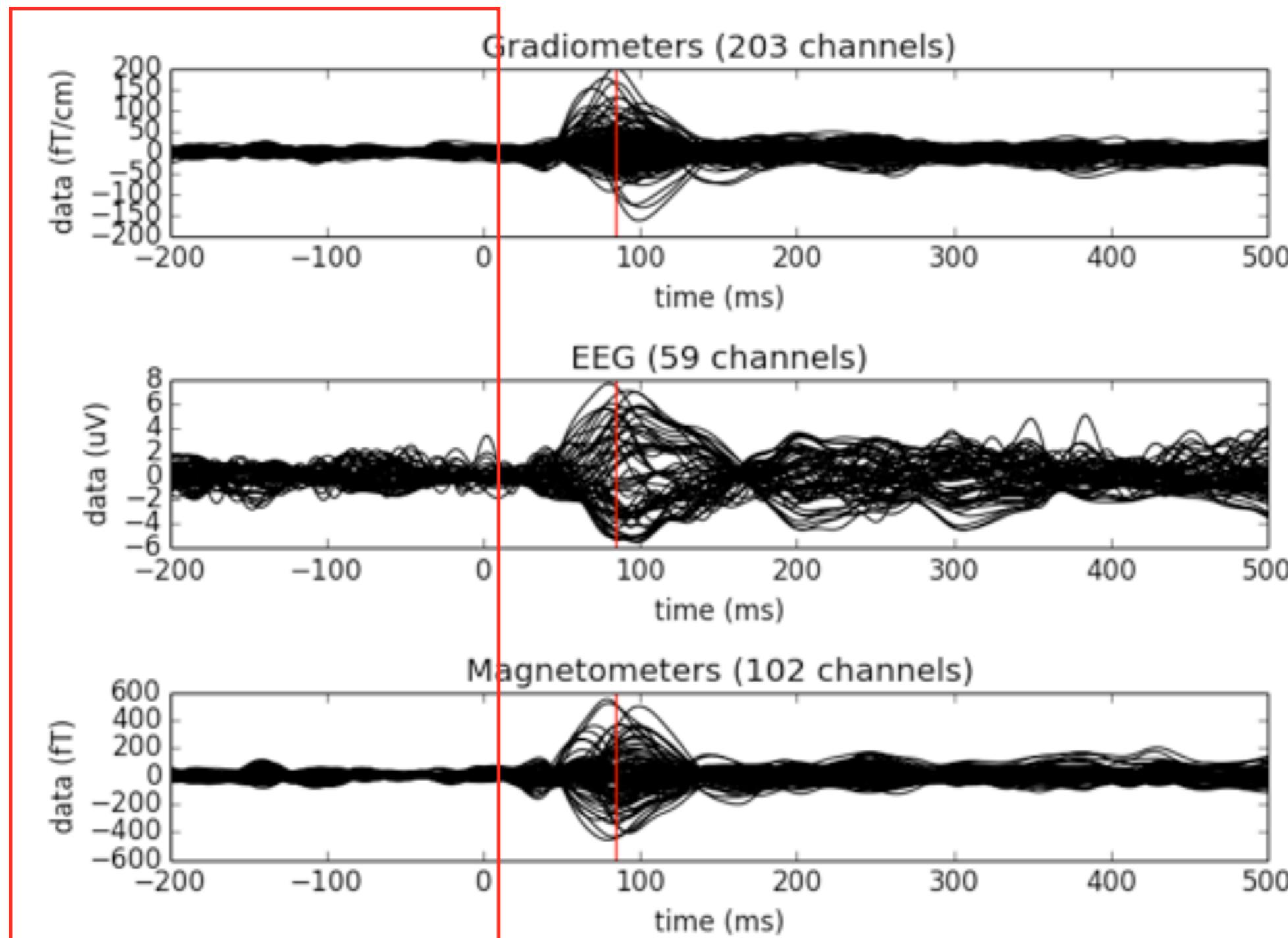
λ : Trade-off between the **data fit** and the **regularization**

where $\|\mathbf{A}\|_F^2 = \text{tr}(\mathbf{A}^T \mathbf{A})$

How do you whiten data?

Inverse models require
appropriate
preprocessing

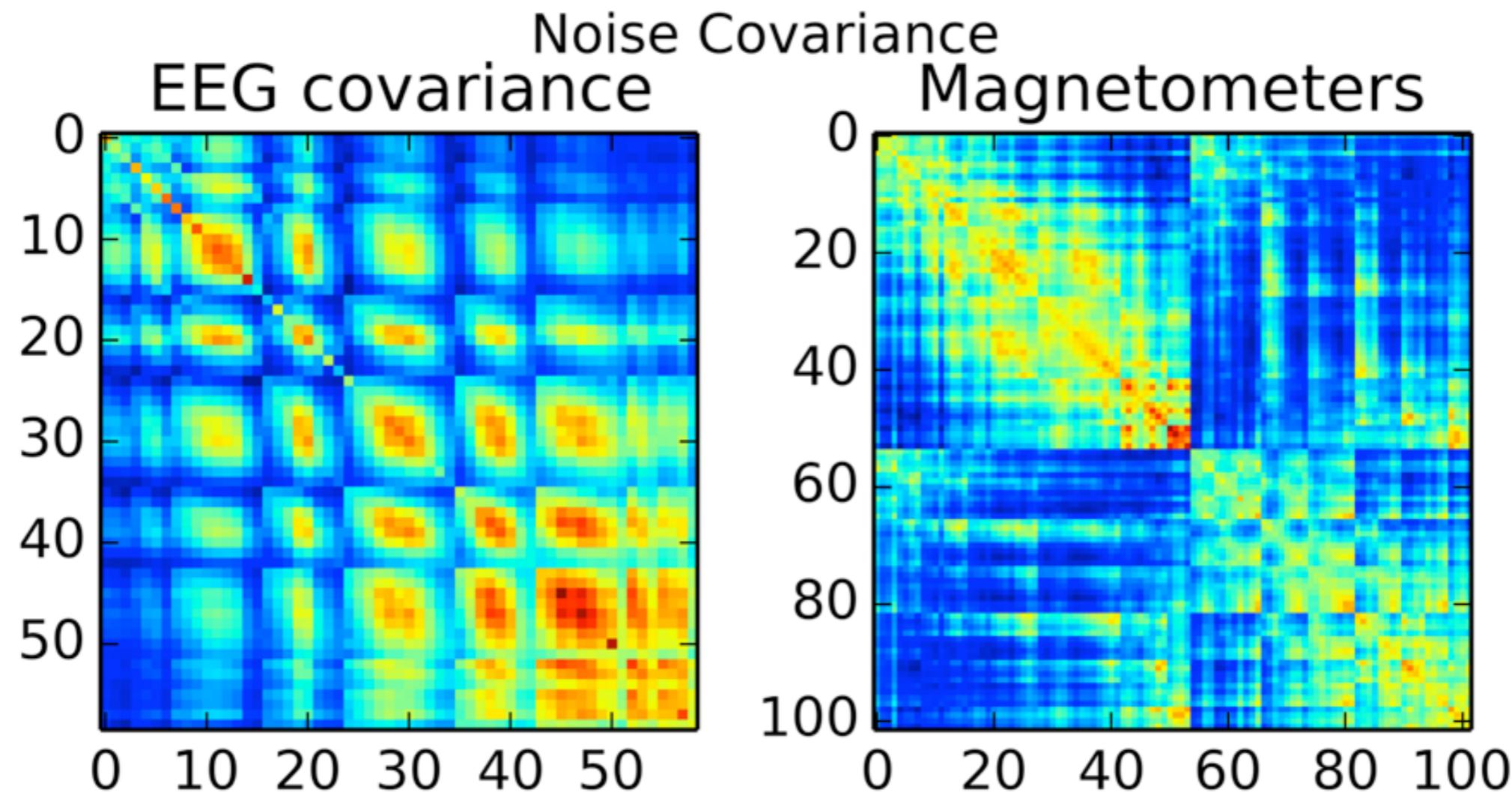
Challenge: M/EEG fusion



Baseline

Data from different sensors have
to be put on the same scale.

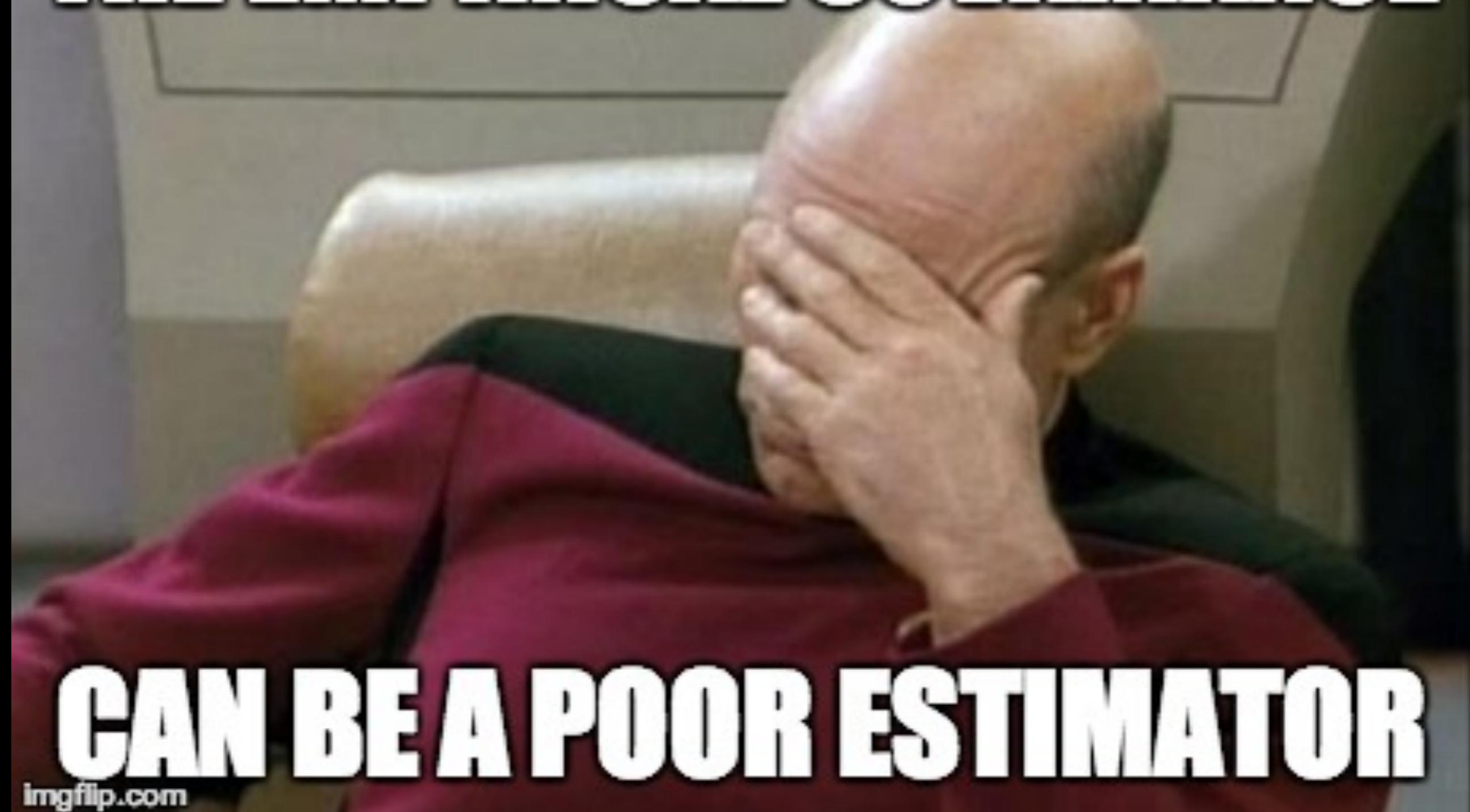
Challenge: M/EEG fusion



$$C = \frac{1}{T} MM^t$$

With whitened data the covariance would be diagonal

THE EMPIRICAL COVARIANCE



CAN BE A POOR ESTIMATOR

Model selection: Log-likelihood

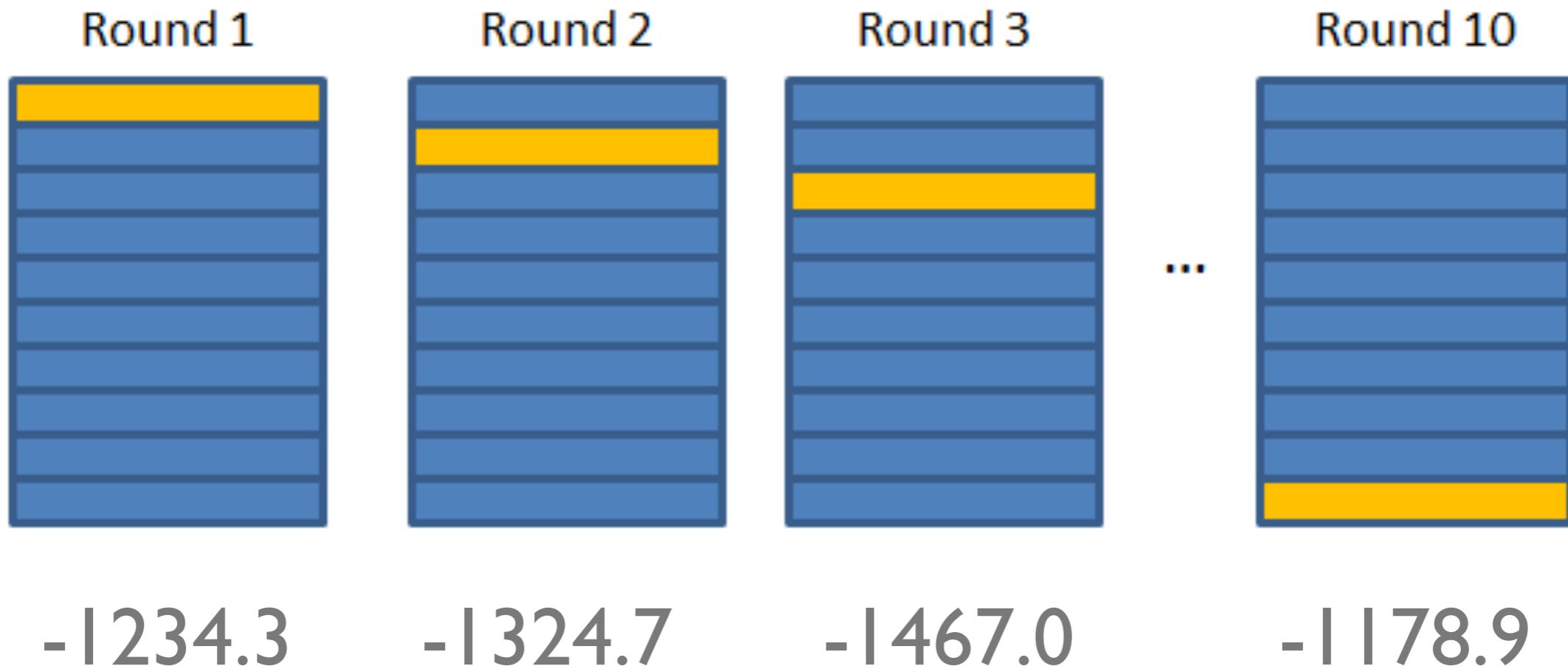
Given my model \mathbf{C} how likely are unseen data \mathbf{Y} ?

$$\mathcal{L}(Y|C) = -\frac{1}{2T} \text{Trace}(YY^t C^{-1}) - \frac{1}{2} \log((2\pi)^N \det(C))$$

Higher log likelihood = better \mathbf{C} & better whitening

Cross-validation

-  Validation Set
-  Training Set



average log likelihood and select the best model

We compared 5 strategies:

1. Hand-set (REG)

$$C' = C + \alpha I, \quad \alpha > 0$$

simple, fast

2. Ledoit-Wolf (LW)

$$C_{LW} = (1 - \alpha)C + \alpha\mu I \quad \mu = \text{mean}(\text{diag}(C))$$

3. Cross-validated shrinkage (SC)

$$C_{SC} = (1 - \alpha_{CV})C + \alpha_{CV}\mu I$$

4. Probabilistic PCA (PPCA)

$$C_{PPCA} = HH^t + \sigma^2 I_N$$

5. Factor Analysis (FA)

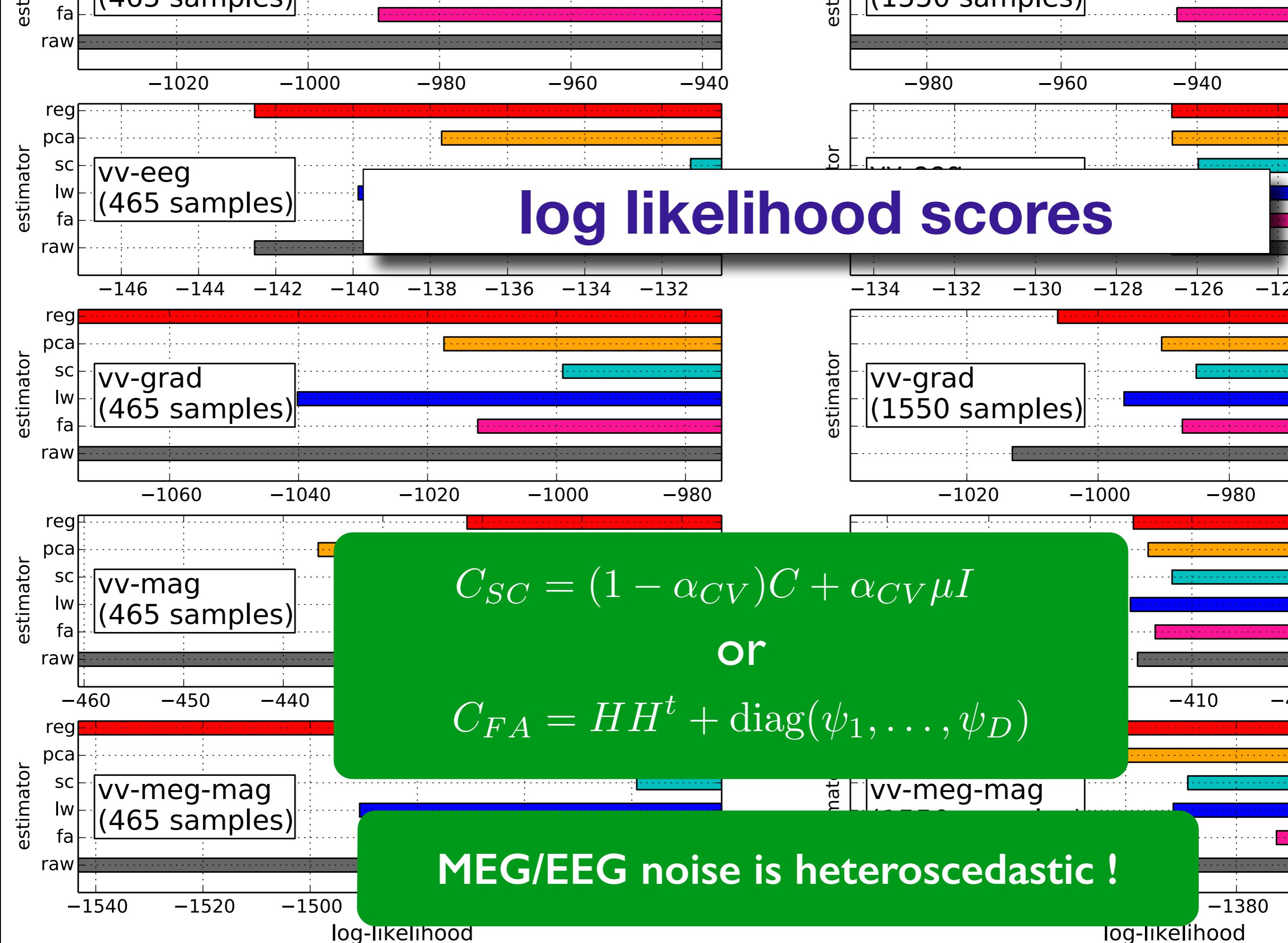
$$C_{FA} = HH^t + \text{diag}(\psi_1, \dots, \psi_D)$$

complex, slow

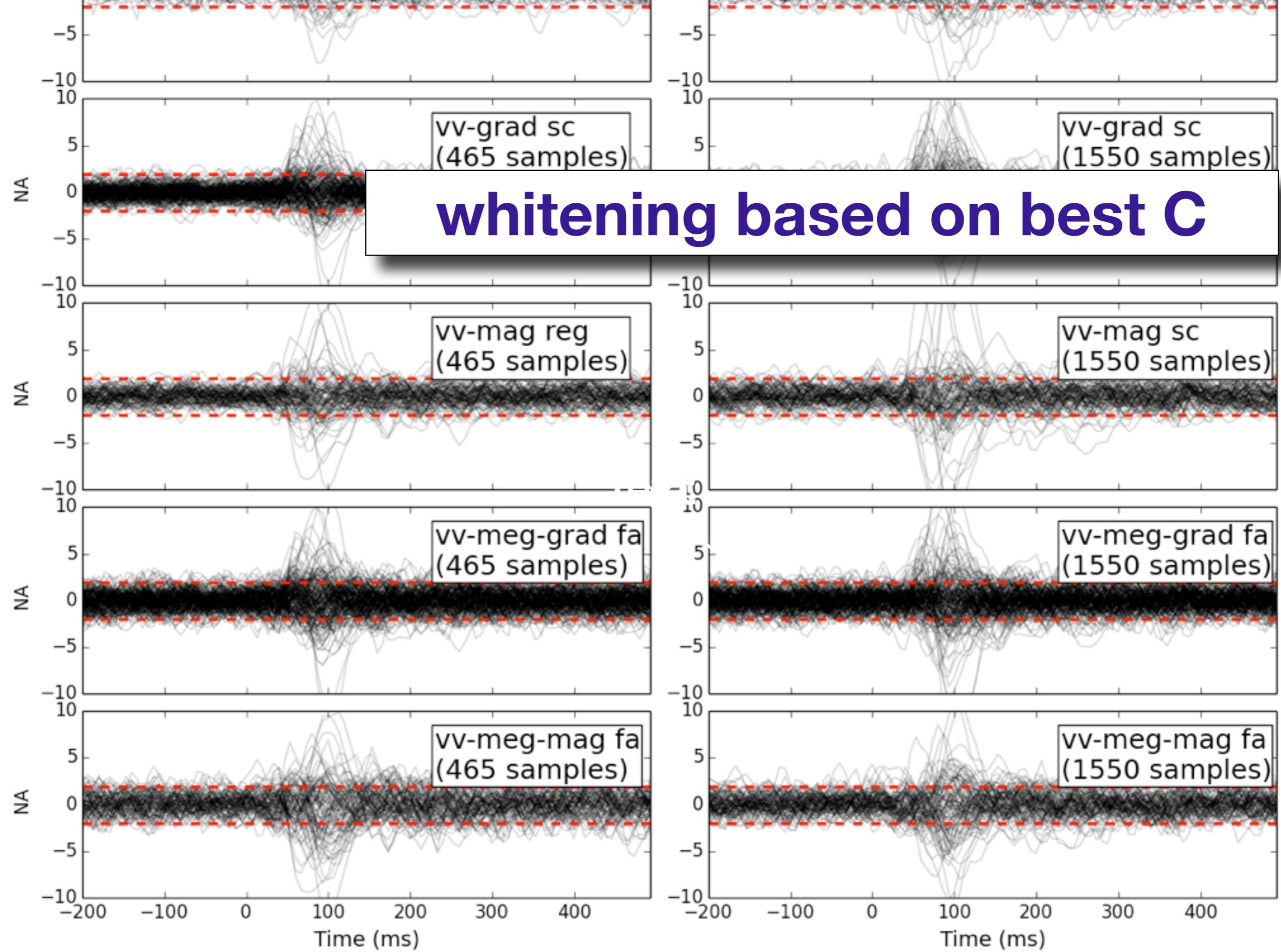


MEG and EEG data

key	dataset and channel type
bt1-mag	4D Magnes 3600 WH magnetometers
ctf-mag	CTF-275 axial gradiometers
vv-eeg	VectorView EEG electrodes
vv-grad	VectorView planar gradiometers
vv-mag	VectorView magnetometers
vv-meg-grad	VectorView planar gradiometers, combined estimation
vv-meg-mag	VectorView magnetometers, combined estimation



whitening based on best C

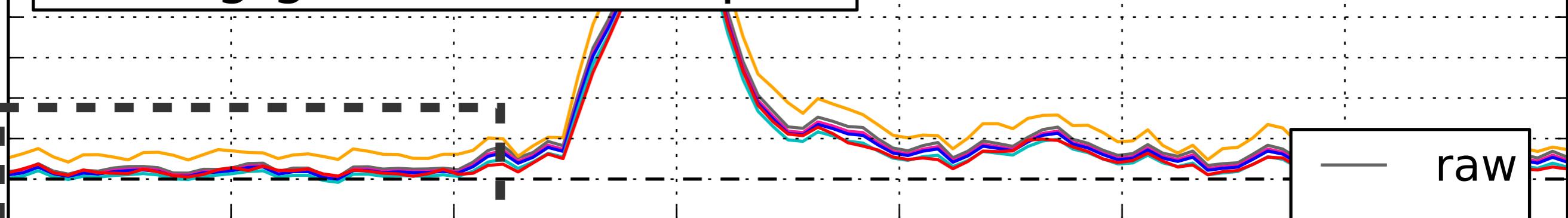


vv-mag (1550 samples)

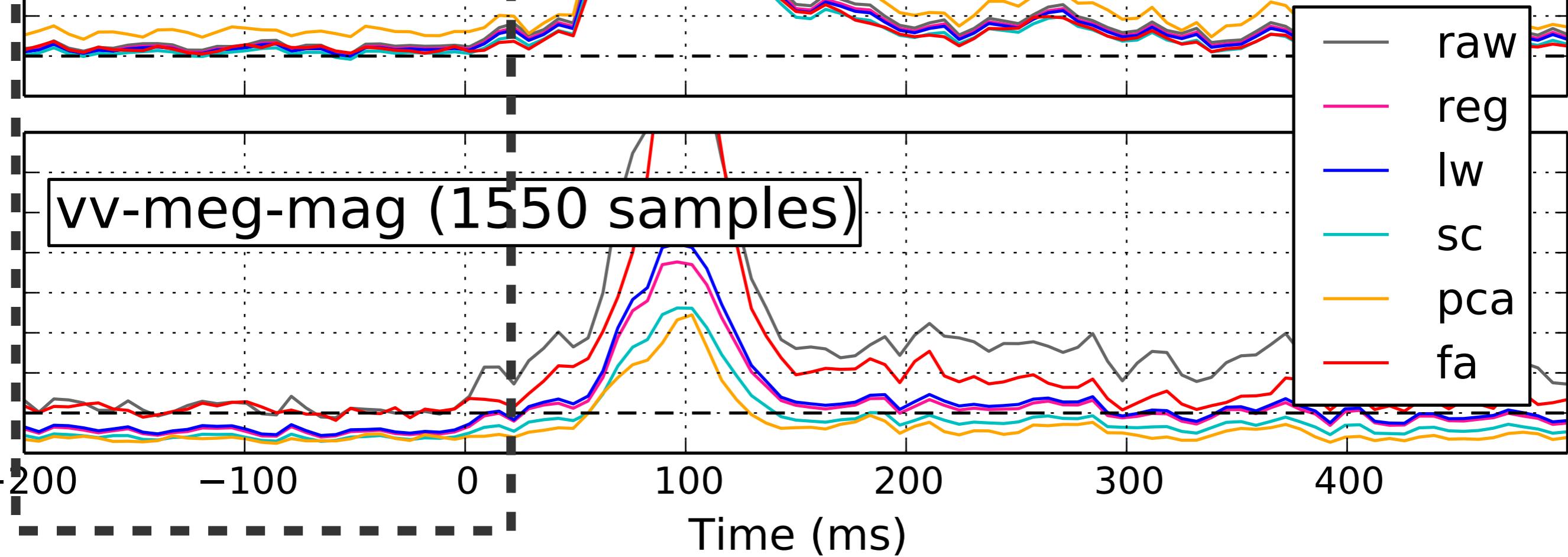
whitened Global Field Power (χ^2)



vv-meg-grad (1550 samples)



vv-meg-mag (1550 samples)





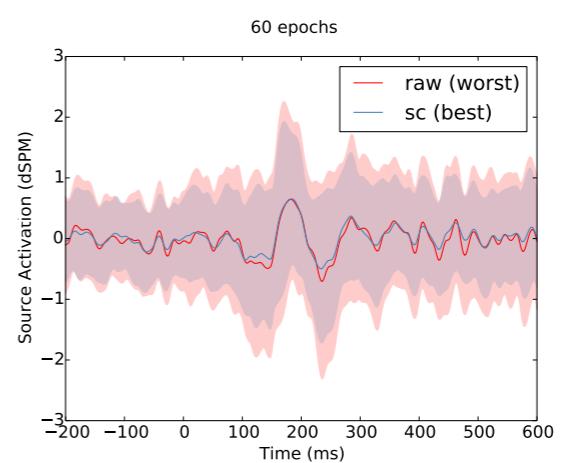
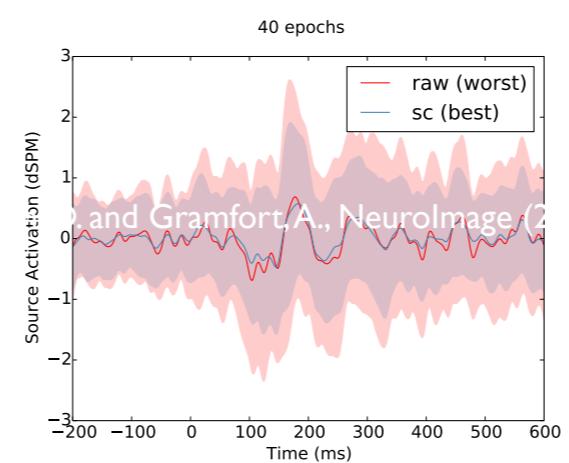
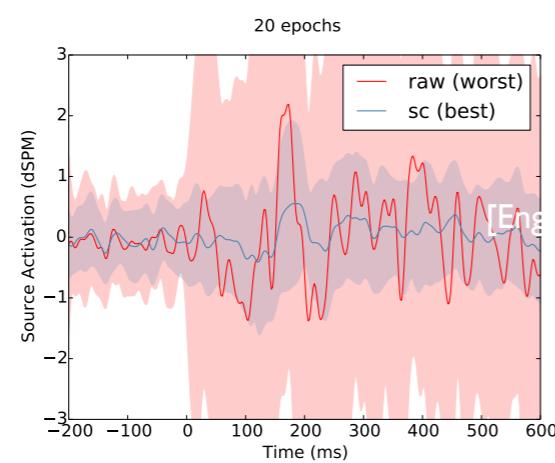
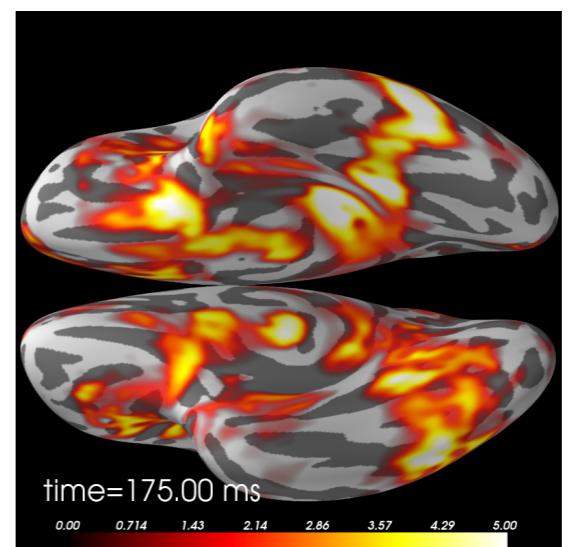
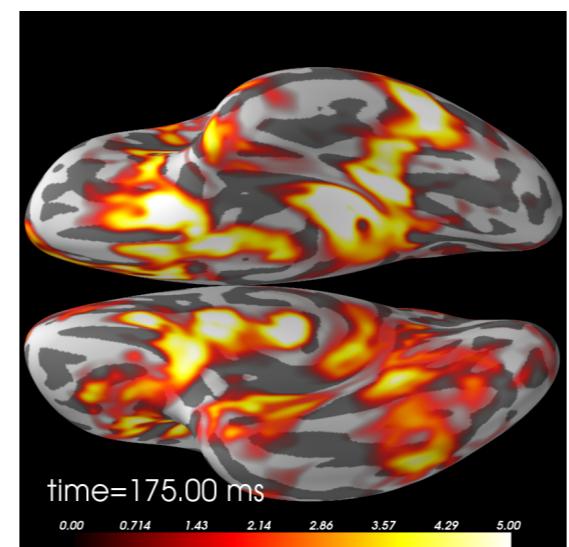
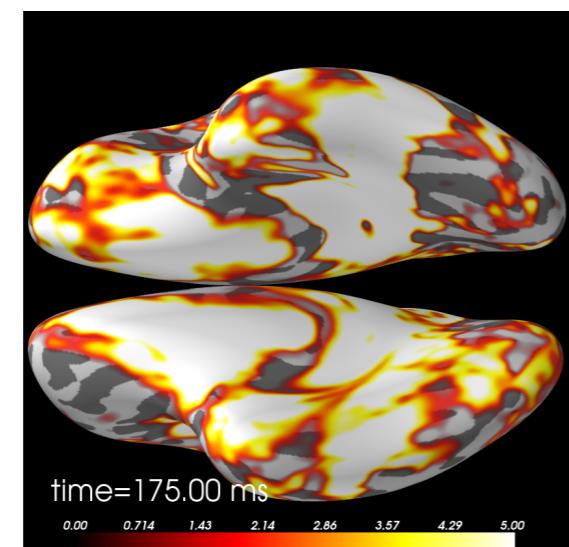
Should we care?

20 epochs

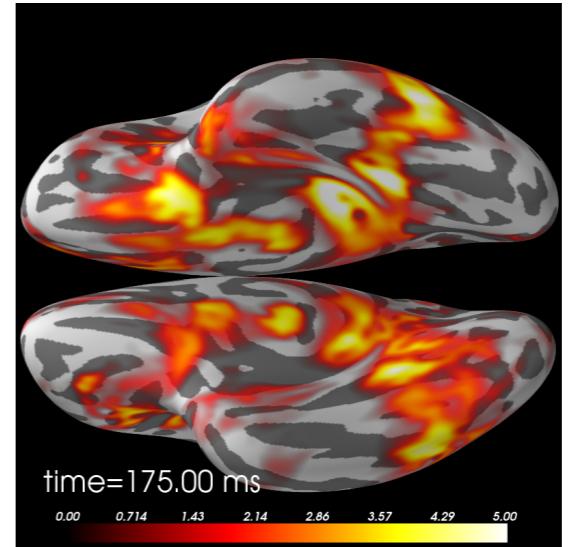
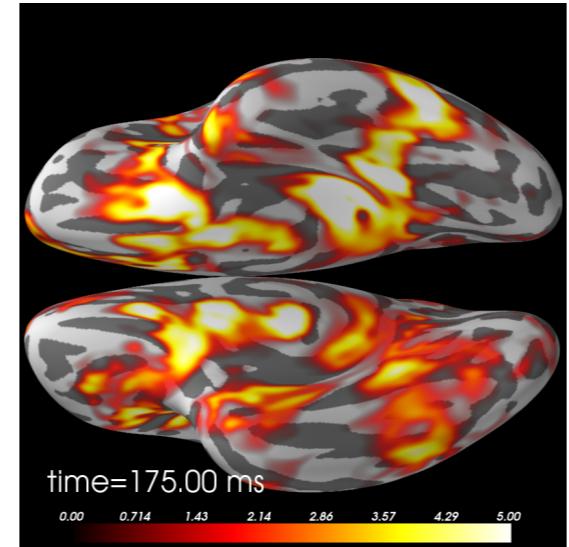
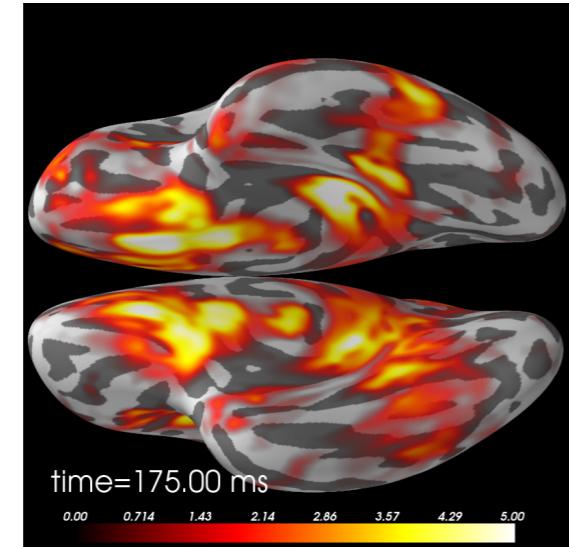
40 epochs

60 epochs

worst



best

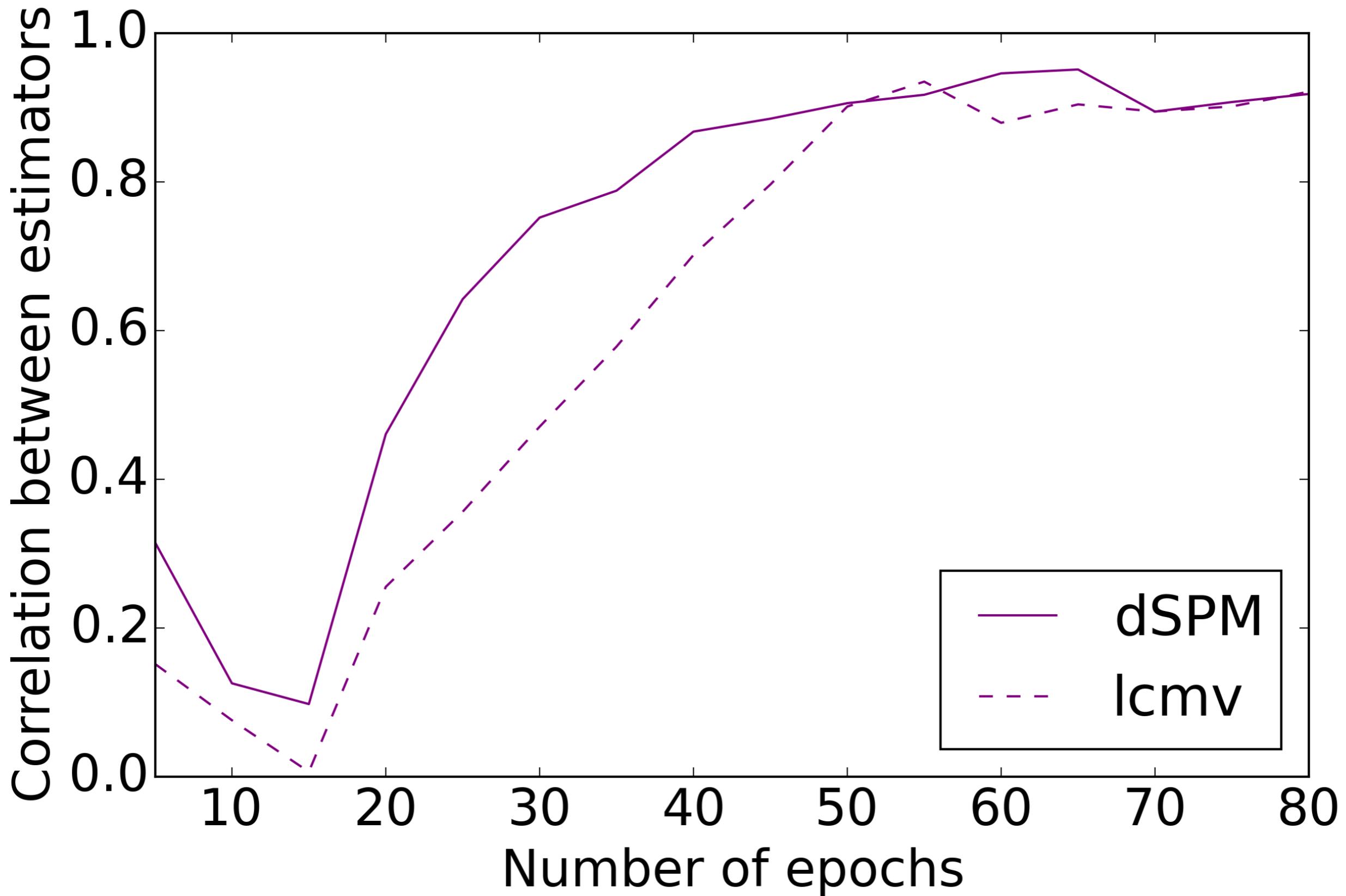


faces > scrambled SPM faces dataset

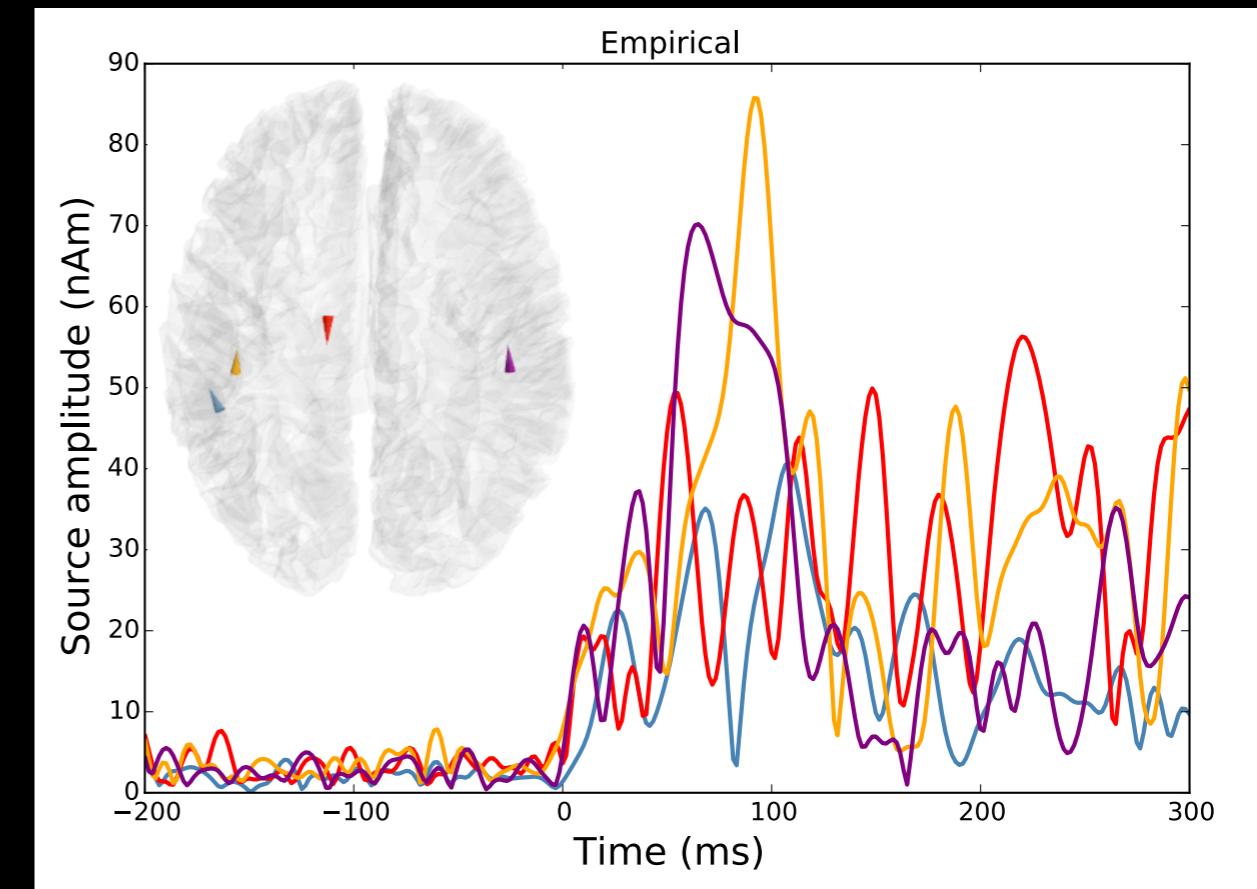
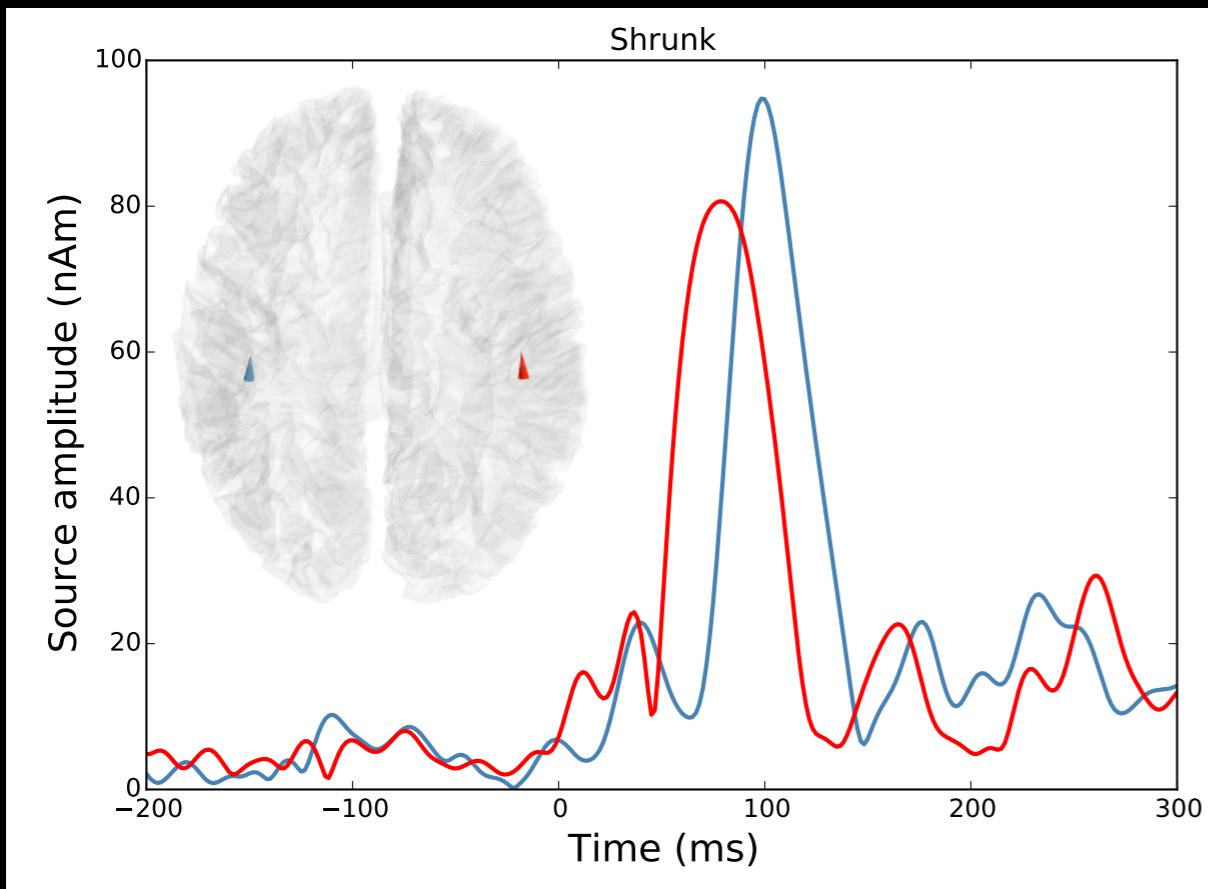
Engemann, D. and Gramfort, A., NeuroImage (2015)

std

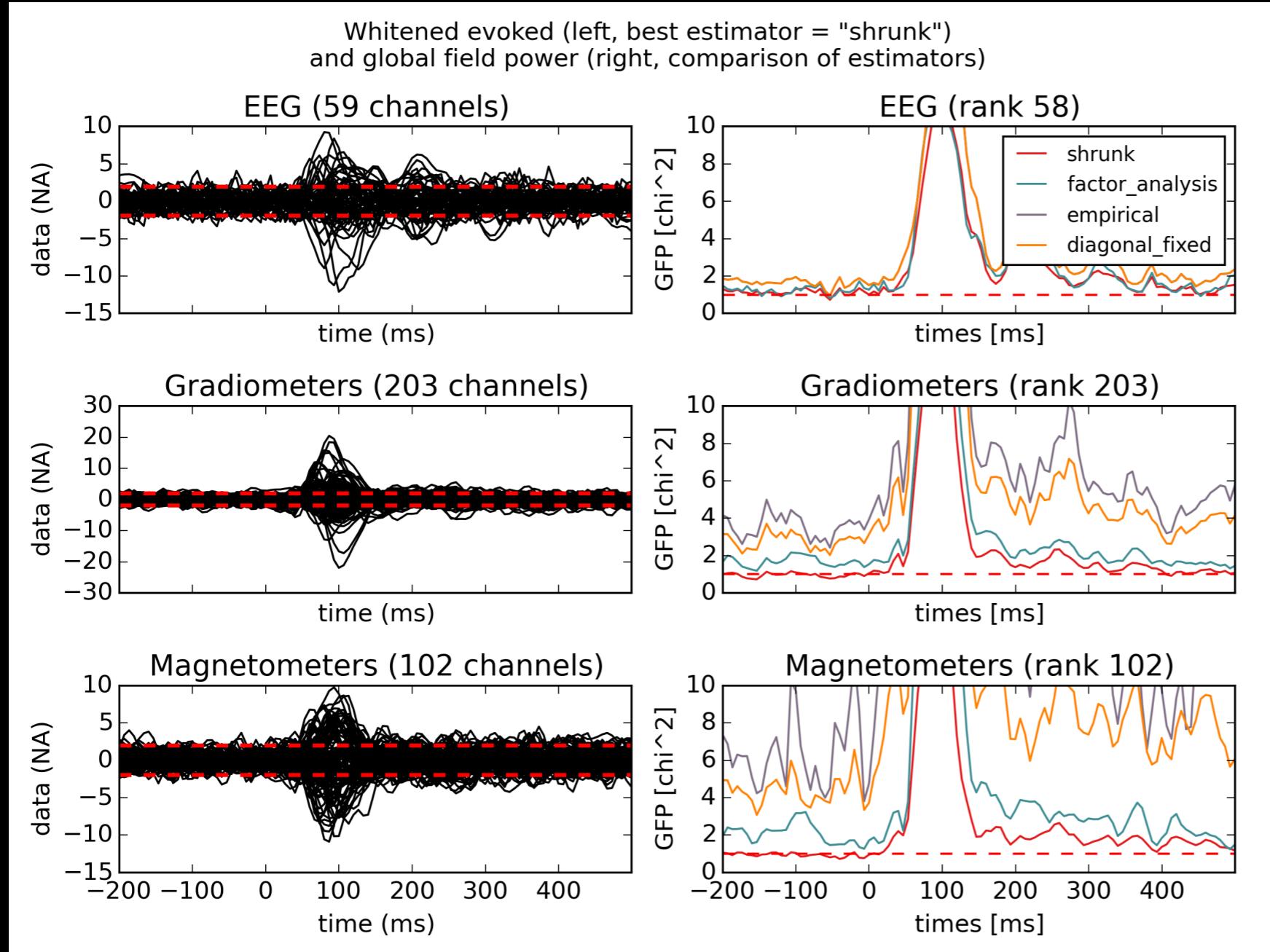
correlation between bad and good source estimates



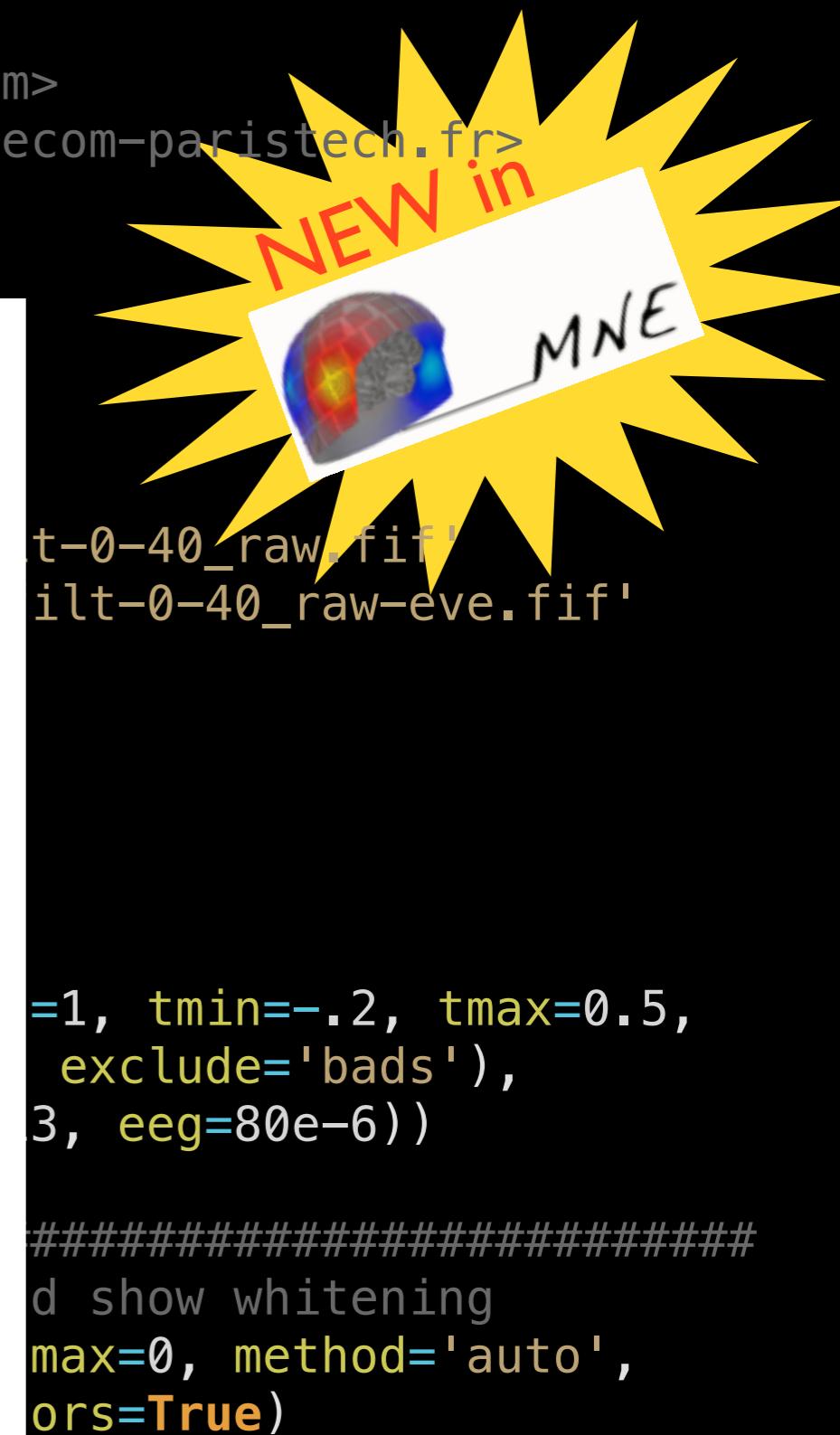
sparse solvers and covariance



```
# Authors: Denis A. Engemann <denis.engemann@gmail.com>
#          Alexandre Gramfort <alexandre.gramfort@telecom-paristech.fr>
#
# License: BSD (3-clause)
```



```
evoked = epochs.average()
evoked.plot() # plot evoked response
evoked.plot_white(noise_covs) # compare estimators
```



```
# Authors: Denis A. Engemann <denis.engemann@gmail.com>
#          Alexandre Gramfort <alexandre.gramfort@telecom-paristech.fr>
#
# License: BSD (3-clause)

import mne

data_path = mne.datasets.sample.data_path()
raw_fname = data_path + '/MEG/sample/sample_audvis_filt-0-40_raw.fif'
event_fname = data_path + '/MEG/sample/sample_audvis_filt-0-40_raw-eve.fif'

raw = mne.io.Raw(raw_fname, preload=True)
raw.info['bads'] += ['MEG 2443']
raw.filter(1, 30)

epochs = mne.Epochs(
    raw, events=mne.read_events(event_fname), event_id=1, tmin=-.2, tmax=0.5,
    picks=mne.pick_types(raw.info, meg=True, eeg=True, exclude='bads'),
    baseline=None, reject=dict(mag=4e-12, grad=4000e-13, eeg=80e-6))

#####
# Compute covariance using automated regularization and show whitening
noise_covs = mne.cov.compute_covariance(epochs[:20], tmax=0, method='auto',
                                         return_estimators=True)

evoked = epochs.average()
evoked.plot() # plot evoked response
evoked.plot_white(noise_covs) # compare estimators
```



3 claims

- you should care about MEG and EEG
- The choice of your statistical model for source localization reflects hypotheses about brain sources
- The success of your source localization depends on domain knowledge and proper signal processing