

## Highlights

- Neural trajectories in the hippocampus exhibited greater variability during a working memory (WM) task compared to those in the entorhinal cortex and amygdala regions.
- The distance of neural trajectories between encoding and retrieval states in the hippocampus was memory-load dependent during a WM task.
- Hippocampal neural trajectories fluctuated between the encoding and retrieval states in a task-dependent manner during both baseline and sharp-wave ripple (SWR) periods.
- Hippocampal neural trajectories shifted from encoding to retrieval states during SWR period.

# Hippocampal neural fluctuations between memory encoding and retrieval states during a working memory task in humans

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## Abstract

The ~~working~~ Working memory (WM), ~~a cornerstone of many critical to various~~ cognitive functions, ~~holds complex neural mechanisms that are not yet embodies intricate neural mechanisms which are not~~ entirely understood. Specifically, ~~the involvement~~ Notably, the role of the hippocampus and sharp-wave ripple complexes (SWRs) – ~~rapid, coincident neural coordinated, rapid neuronal~~ events within the hippocampus – in WM tasks remains somewhat ~~uncertain, despite their established roles ambiguous, notwithstanding their confirmed involvement~~ in memory consolidation and retrieval. In our ~~current present~~ research, we ~~propose posit~~ that multiunit activity patterns within the hippocampus ~~interact operate~~ synergistically with SWRs, ~~thereby displaying unique consequently exhibiting distinctive~~ dynamics during WM tasks. ~~This study involved an extensive~~ Our study engaged in a comprehensive analysis of a dataset ~~obtained derived~~ from intracranial electroencephalogram recordings from the medial temporal ~~lobe lobes~~ (MTL) of nine ~~patients with epilepsy, while performing epileptic patients executing~~ an eight-second Sternberg task. Gaussian-process factor analysis was ~~employed to identify utilized to pinpoint~~ low-dimensional neural ~~representations vectors~~, or 'trajectories,' within the MTL during the WM task. We ~~found discovered~~ that the hippocampus ~~exhibited the most significant variations showed the most pronounced variation~~ in neural trajectories ~~compared relative~~ to the entorhinal cortex and the amygdala. ~~Interestingly, the divergence~~ Intriguingly, the deviation in trajectories between the encoding and retrieval phases was ~~memory load dependent. More specifically seen to be dependent on memory load. Further,~~ hippocampal trajectories ~~oscillated showed oscillatory behavior~~ during the retrieval phase, ~~revealing task dependent indicating task related~~ transitions between encoding and retrieval states, ~~encapsulating and embracing both~~ baseline and SWR episodes. These oscillations ~~moved transitioned~~ from encoding to retrieval states ~~correlating in correlation~~ with the SWRs. ~~Therefore Hence,~~ these findings ~~emphasize the essential underscore the crucial~~ role of the hippocampus in ~~performing tackling~~ WM tasks and ~~suggest a compelling premise for further investigation propose an enticing hypothesis for future exploration:~~ the functional state of the hippocampus ~~transitions switches~~ from encoding to retrieval during SWRs.

**Keywords:** working memory, WM, memory load, hippocampus, sharp-wave ripples, SWR, humans

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Working memory (WM) ~~plays a crucial serves~~ a critical role in everyday life, ~~and its neural underpinnings remain an area of ongoing research with its neural foundations being an ongoing subject of study.~~ The hippocampus, ~~notably integral to memory~~

~~, continues to be a primary focus of this investigation particularly crucial to memory function, remains central to this research~~ [1] [2] [3] [4] [5] [6] [7] [8] [9]. ~~Gaining insights into Understanding~~ the role of the hippocampus in working memory is ~~vital to deepening our understanding essential to advancing our~~

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comprehension of cognitive processes, hence fostering the progression of thereby promoting cognitive training and interventions.

Current evidence suggests a transient points toward a brief, synchronized oscillation, referred to known as sharp-wave ripple (SWR) [10], is linked being associated with several cognitive functions, such as. These include memory replay [11] [12] [13] [14] [15], memory consolidation [16] [17] [18] [19], memory recall [20] [21] [22], and neural plasticity [23] [24]. This evidence indicates the likelihood that SWR could be a critical component of suggests that SWR may play a crucial part in hippocampal processing, contributing to working memory performance the performance of working memory. However, research studies investigating the effects of SWRs on working memory remains sparse [25], and is largely limited to rodent models participating are limited [25] and focus primarily on rodent models engaged in navigation tasks where the timing, without clear delineation of memory acquisition and recall is not explicitly distinguished timing.

Recent studies indicate have illustrated that hippocampal neurons exhibit present low-dimensional representations during WM tasks. Notably Specifically, the firing patterns of place cells [26] [27] [28] [29] [30], located in the hippocampus, are observed to be encompassed appear within a dynamic, nonlinear three-dimensional hyperbolic geometry in rodents [31]. Moreover rodent models [31]. Additionally, grid cells in the entorhinal cortex (EC)—the dominant pathway main route to the hippocampus [32] [33] [34]—displayed display a toroidal topology during exploration [35]. Unfortunately, these investigations are confined. Regrettably, these studies are limited to spatial navigation tasks in rodents, thus imposing limitations on affecting the temporal resolution of WM tasks. The applicability application of these findings to human subjects and their generalization extension beyond navigation tasks remains to be established are still unconfirmed.

Given these considerations, the current study aims to validate. In light of these points, the present study seeks to corroborate the hypothesis that hippocampal neurons exhibit distinctive portray unique representations in low-dimensional spaces, designated referred to as 'neural trajectory,' during WM tasks, most prominently within SWR periods. To evaluate this claim, we

employed a dataset of particularly during SWR periods in WM tasks. To test this proposition, we used a dataset from patients performing an eight-second Sternberg task with high temporal resolution (1 s second for fixation, 2 s seconds for encoding, 3 s seconds for maintenance, and 2 s seconds for retrieval) with a high temporal resolution, while their intracranial electroencephalography signals (iEEG) within signals in the medial temporal lobe (MTL) were being monitored [36]. To investigate explore the low-dimensional neural trajectories, we employed utilized the Gaussian-process factor analysis (GPFA), a method renowned for analyzing recognized technique for examining neural population dynamics [37].

## 1. Methods

### 1.1. Dataset

A publicly available dataset [36] was used, which consists of public dataset [36] comprising experiments from nine epilepsy patients performing was taken into consideration for this study. The patients were tasked with executing a modified Sternberg task. This task involves which included four phases: fixation (1s), encoding (2s), maintenance (3s), and retrieval (2s) [36]. During the encoding phase, participants were exposed to presented with four, six, or eight alphabet letters, referred to known as the set size. Subsequently, they had to decide ascertain whether a probe letter presented revealed during the retrieval phase was previously displayed (the correct displayed earlier (the suitable choice for the Match IN task) or not (the correct suitable choice for the Mismatch OUT task). iEEG signals were recorded at registered via a sampling rate of 32 kHz, within a frequency range spectrum of 0.5–5,000 Hz, using utilizing depth electrodes implanted in the medial temporal lobe (MTL) regions: the anterior head of the left and the right hippocampus (AHL and AHR), the posterior body of the hippocampus (PHL and PHR), the entorhinal cortex (ECL and ECR), and the amygdala (AL and AR), as illustrated in (Figure 1A and Table 1: The). The recorded iEEG signals were subsequently downsampled to a rate of 2 kHz. Correlations The interrelationship among variables such as set size and correct rate were investigated explored (Figure ??S1). The timings of multiunit spikes were determined by identified using a spike sorting algorithm [38] using

with the Combinato package (<https://github.com/jniediek/combinato>) (Figure 1C).

### 1.2. Calculation of neural trajectories using GPFA

Neural trajectories, ~~also termed colloquially called~~ 'factors' (Figure 1D), in the hippocampus, EC, and amygdala (Figure 1D) ~~, were computed using GPFA [37] were calculated utilizing GPFA [37], which was applied to the multiunit activity data for radiating from each session. GPFA was The computations were performed with the elephant package (<https://elephant.readthedocs.io/en/latest/reference/gpfa.html>). The bin size was set to at 50 ms, with no overlaps. Each factor was z-normalized across all sessions. The Euclidean distance from the origin ( $O$ ) was then subsequently calculated (Figure 1E).~~

For each trajectory ~~within inside~~ a region, for ~~instance example~~, AHL, ~~geometric medians (i.e.,  $g_F$  for fixation,  $g_E$  for encoding,  $g_M$  for maintenance, and  $g_R$  for retrieval phase) were determined by calculating calculated by finding~~ the median coordinates of the trajectory during the four phases (Figure 1D). An optimal dimensionality for GPFA was identified as three using the elbow method, which was derived by investigating the log-likelihood values through a three-fold cross-validation ~~approach technique~~ (Figure 2B).

### 1.3. Identifying SWR candidates from ~~hippocampal regions areas of the hippocampus~~

Potential SWR ~~events instances from~~ within the hippocampus were ~~detected using a widely identified via an~~ accepted method [39]. LFP signals from a ~~given~~ region of interest (ROI), such as AHL, were re-referenced by subtracting ~~an averaged a calculated average~~ signal from locations outside the ROI (~~e.g.e.g.~~, AHR, PHL, PHR, ECL, ECR, AL, and AR) (see Figure 1A). The re-referenced LFP signals were ~~then~~ further filtered with a ripple-band filter (80–140 Hz) to ~~identify detect~~ SWR candidates (=SWR<sup>+</sup> candidates) (see Figure 1B). SWR detection was ~~conducted carried out~~ using a published tool ([https://github.com/Eden-Kramer-Lab/ripple\\_detection](https://github.com/Eden-Kramer-Lab/ripple_detection)) [40], with the bandpass range adjusted to 80–140 Hz ~~for humans in line with human requirements [21] [22], different from the original as opposed to the conventional~~ 150–250 Hz range typically applied to rodents.

Control events for SWR<sup>+</sup> candidates, ~~labeled tagged~~ as SWR<sup>-</sup> candidates, were identified by ~~randomly shuffling the timestamps of SWR<sup>+</sup> candidates randomly~~ across all trials and subjects. The ~~resulting resultant~~ SWR<sup>+</sup>/SWR<sup>-</sup> candidates ~~were then subjected to visual inspection, as shown in underwent visual inspection~~ (Figure 1).

### 1.4. Defining SWRs from ~~putative alleged~~ hippocampal CA1 regions

SWRs were distinguished from SWR candidates ~~in presumptive within likely~~ CA1 regions. Initially, these regions were ~~defined designated~~ as follows: SWR<sup>+</sup>/SWR<sup>-</sup> candidates ~~in from~~ the hippocampus were ~~projected mapped~~ into a two-dimensional space based on ~~the~~ overlapping spike counts per unit ~~employing a supervised method using using a supervised~~ UMAP (Uniform Manifold Approximation and Projection) [41] (Figure 4A). ~~Clustering validation was performed Validation of the clustering was done~~ by computing the silhouette score [42] from ~~the~~ clustered samples (Table 2). ~~Regions Those areas~~ in the hippocampus ~~, which scored above scoring over~~ 0.6 on average across sessions (~~or the~~ 75th percentile) (Figure 4B), ~~were characterized as presumed were specified as likely~~ CA1 regions, ~~in turn,~~ identifying five electrode positions ~~from five patients across five participants~~ (Table 3).

~~Those~~ SWR<sup>+</sup>/SWR<sup>-</sup> candidates ~~in within~~ the assumed CA1 regions were classified as SWR<sup>+</sup>/SWR<sup>-</sup> ~~; thus relinquishing and had~~ their candidate status ~~. The revoked. Log-normal distributions were observed in the duration and ripple band peak amplitude of SWRs were observed to follow log-normal distributions (Figure 44C & E). Each time period of SWR SWR time period was partitioned relative to the time from the SWR center into pre- (at -800 to -300 ms from SWR center), mid- (at -250 to +250 ms), and post-SWR post- (at +300 to +800 ms) SWR times.~~

### 1.5. Statistical evaluation

The Brunner–Munzel test and the Kruskal–Wallis test were performed using the SciPy package in Python [43]. ~~Correlational analysis was performed A correlation analysis was executed~~ by determining the rank of the ~~observed~~ correlation coefficient in its associated set-size-shuffled surrogate using a custom Python script.

The bootstrap test was ~~implemented using~~ conducted with an in-house Python script.

## 2. Results

### 2.1. iEEG recording and neural trajectory in MTL regions during a Sternberg task

We ~~leveraged-analyzed~~ a publicly available dataset for this ~~analysis-study~~ [36]. This dataset ~~encompasses~~ consists of LFP signals (Figure 1A) from MTL regions (Table 1) obtained during a modified Sternberg task execution performance. We identified SWR<sup>+</sup> candidates from LFP signals filtered through the 80–140 Hz ripple band (Figure 1B) ~~,-originating-~~ across all hippocampal regions (refer to Methods). Correspondingly, SWR<sup>-</sup> candidates were defined at identical timestamps ~~-)but-shuffled-across-the-same-timestamps-but-shuffled-between~~ different trials (Figure 1). The dataset included multiunit spikes (Figure 1C) identified via a spike sorting algorithm [38]. ~~By-employing-Using~~ GPFA [37], and ~~using-the~~ 50-ms binned multiunit activity ~~with-no~~ without overlaps, we determined the neural trajectories (or factors) of MTL regions ~~by-per~~ session and region (Figure 1D). We normalized each factor by session and region, for instance, session #2 in AHL of subject #1. Subsequently, we calculated the Euclidean distance from the origin (*O*) (Figure 1E).

### 2.2. ~~Hippocampal-Correlation between hippocampal neural trajectory correlation-with-a-and~~ Sternberg task performance

Figure 2A ~~illustrates-shows~~ the cloud of median neural trajectories of 50 trials within the three main factor spaces. We determined the optimal embedding dimension for the GPFA model to be three, using the elbow method (Figure 2B). The trajectory distance from the origin (*O*) (represented as  $\|g_F\|$ ,  $\|g_E\|$ ,  $\|g_M\|$ , and  $\|g_R\|$ ) in the hippocampus ~~exceeded-was greater than the~~ corresponding distances in the EC and amygdala (Figures 2C and D).<sup>1</sup>

Similarly, we ~~computed-calculated~~ the distances between the geometric medians of the four phases, namely

<sup>1</sup>Hippocampus: Distance = 1.11 [1.01], median [IQR],  $n = 195,681$  timepoints; EC: Distance = 0.94 [1.10], median [IQR],  $n = 133,761$  timepoints; Amygdala: Distance = 0.78 [0.88], median [IQR],  $n = 165,281$  timepoints.

$\|g_Fg_E\|$ ,  $\|g_Fg_M\|$ ,  $\|g_Fg_R\|$ ,  $\|g_Eg_M\|$ ,  $\|g_Eg_R\|$ , and  $\|g_Mg_R\|$ . The results indicated that the hippocampus ~~displayed~~ showed larger distances between phases than both the EC and amygdala.<sup>2</sup>

### 2.3. Memory ~~load-dependent-load-dependence of~~ neural trajectory distance between encoding and retrieval states in the hippocampus

In ~~terms-the context~~ of memory load in the ~~Stenberg~~ Sternberg task, we ~~identified-found~~ a negative correlation between the correct rate of trials and set size (the number of letters to encode) (Figure 3A).<sup>3</sup> Similarly, we observed a positive correlation ~~was-observed~~ between the response time and set size (Figure 3B).<sup>4</sup>

~~Furthermore,-we-found~~ Additionally, we observed a positive correlation between set size and the trajectory distance between the encoding and retrieval phases ( $\log_{10}\|g_{EGR}\|$ ) (Figure 3C).<sup>5</sup> However, the distances between other combinations of phases did not ~~display~~ statistically-show significant correlations (Figures 3D and S2).

### 2.4. Detection of hippocampal SWR from putative CA1 regions

~~For-precision-improvement-in-To~~ better localize recording sites and improve SWR detection, we estimated the electrode ~~placements-position~~ in the CA1 regions of the hippocampus using distinct multiunit spike patterns during ~~the~~ SWR events. We embedded SWR<sup>+</sup>/SWR<sup>-</sup> candidates from ~~every-each~~ session

<sup>2</sup>Hippocampus: Distance = 0.60 [0.70], median [IQR],  $n = 8,772$  combinations; EC: Distance = 0.28 [0.52], median [IQR],  $n = 5,017$  combinations ( $p < 0.01$ ; Brunner–Munzel test); Amygdala: Distance = 0.24 [0.42], median [IQR],  $n = 7,466$  combinations ( $p < 0.01$ ; Brunner–Munzel test).

<sup>3</sup>Correct rate: set size four ( $0.99 \pm 0.11$ , mean  $\pm$ SD;  $n = 333$  trials) vs. set size six ( $0.93 \pm 0.26$ ;  $n = 278$  trials;  $p < 0.001$ , Brunner–Munzel test with Bonferroni correction) and set size eight ( $0.87 \pm 0.34$ ;  $n = 275$  trials;  $p < 0.05$ ; Brunner–Munzel test with Bonferroni correction). Overall,  $p < 0.001$  for Kruskal–Wallis test; correlation coefficient =  $-0.20$ ,  $p < 0.001$ .

<sup>4</sup>Response time: set size four ( $1.26 \pm 0.45$  s;  $n = 333$  trials) vs. set size six ( $1.53 \pm 0.91$  s;  $n = 278$  trials) and set size eight ( $1.66 \pm 0.80$  s;  $n = 275$  trials). All comparisons  $p < 0.001$ , Brunner–Munzel test with Bonferroni correction;  $p < 0.001$  for Kruskal–Wallis test; correlation coefficient =  $0.22$ ,  $p < 0.001$ .

<sup>5</sup>Correlation between set size and  $\log_{10}(\|g_{EGR}\|)$ : correlation coefficient =  $0.05$ ,  $p < 0.001$ . Specific values:  $\|g_{EGR}\| = 0.54$  [0.70] for set size four,  $n = 447$ ;  $\|g_{EGR}\| = 0.58$  [0.66] for set size six,  $n = 381$ ;  $\|g_{EGR}\| = 0.61$  [0.63] for set size eight,  $n = 395$ .



and hippocampal region ~~were embedded~~ in a two-dimensional space ~~using via~~ UMAP (Figure 4A).<sup>6</sup> ~~We used~~ The quality of clustering was verified using the silhouette score as a metric ~~for quality of clustering~~ (Figure 4B and Table 2). Recording sites ~~with yielding~~ an average silhouette score ~~exceeding over~~ 0.6 across all sessions were ~~identified designated~~ as putative CA1 regions.<sup>7</sup> (Tables 2 and 3). We ~~identified found~~ five putative CA1 regions, ~~four of which were not out of which~~ ~~four weren't~~ labeled as seizure onset zones (Table 1).

~~Subsequently, We further labeled~~ SWR<sup>+</sup>/SWR<sup>-</sup> candidates within these putative CA1 regions ~~were labeled~~ as SWR<sup>+</sup> and SWR<sup>-</sup>, respectively<sup>8</sup> (Table 3). Both SWR<sup>+</sup> and SWR<sup>-</sup> exhibited ~~the same duration equal~~ duration<sup>9</sup> (Figure 4C) due to their definitions, and ~~followed adopted~~ a log-distribution. ~~We observed an augmentation~~ There was an increase in SWR<sup>+</sup> incidence during the initial ~~within the first~~ 400 ms of the retrieval phase<sup>10</sup> (Figure 4D). The peak ripple band amplitude of SWR<sup>+</sup> ~~outpaced was greater than that of~~ SWR<sup>-</sup> and followed a log-normal distribution (Figure 4E).<sup>11</sup>

## 2.5. Transient changes in hippocampal neural trajectory trajectories during SWR events

We ~~computed calculated~~ the distance of the trajectory from the origin (*O*) during SWR events in both the encoding and retrieval phases (Figure 5A). Observing ~~the an~~ increase in distance during SWR as shown in Figure 5A, we ~~differentiated classified~~ each SWR into three stages: pre-, mid-, and post-SWR. ~~Therefore Consequently~~, the distances from *O* during those SWR periods are identified these SWR stages are denoted as  $\|\text{pre-eSWR}^+\|$ ,  $\|\text{mid-eSWR}^+\|$  among others.

The  $\|\text{mid-eSWR}^+\|$ <sup>12</sup> was ~~greater larger~~ than

<sup>6</sup>Consider the AHL in session #1 of subject #1, for illustration purposes.

<sup>7</sup>The ~~identified designated~~ regions were: AHL of subject #1, AHR of subject #3, PHL of subject #4, AHL of subject #6, and AHR of subject #9.

<sup>8</sup>These definitions ~~led to resulted in~~ equal counts for both categories: SWR<sup>+</sup> ( $n = 1,170$ ) and SWR<sup>-</sup> ( $n = 1,170$ ).

<sup>9</sup>These definitions ~~led to resulted in~~ equal durations for both categories: SWR<sup>+</sup> (93.0 [65.4] ms) and SWR<sup>-</sup> (93.0 [65.4] ms).

<sup>10</sup>The occurrence of SWR<sup>+</sup> increased against the bootstrap sample; 95th percentile = 0.42 [Hz];  $p < 0.05$ .

<sup>11</sup>SWR<sup>+</sup> (3.05 [0.85] SD of baseline, median [IQR];  $n = 1,170$ ) vs. SWR<sup>-</sup> (2.37 [0.33] SD of baseline, median [IQR];  $n = 1,170$ ;  $p < 0.001$ ; Brunner-Munzel test).

<sup>12</sup>1.25 [1.30], median [IQR],  $n = 1,281$ , in Match IN task; 1.12 [1.35], median [IQR],  $n = 1,163$ , in Mismatch OUT task

$\|\text{pre-eSWR}^+\|$ <sup>13</sup>, and  $\|\text{mid-rSWR}^+\|$ <sup>14</sup> was ~~larger bigger~~ than  $\|\text{pre-rSWR}^+\|$  in both Match IN and Mismatch OUT tasks.<sup>15</sup>

## 2.6. Visualization of hippocampal neural trajectory trajectories during SWR in two-dimensional spaces

Following our observations ~~of on~~ neural trajectory 'jumping' during SWR a SWR event (Figure 5), we visualized the three-dimensional trajectories of pre-, mid-, and post-SWR events during the encoding and retrieval phases (Figure 6), the distance between which was found to ~~be memory-load dependent depend on~~ memory load (Figure 3).

To ~~provide enable~~ two-dimensional visualization, we linearly aligned peri-SWR trajectories by assigning  $\mathbf{g}_E$  at the origin (0, 0) and  $\mathbf{g}_R$  at ( $\|\mathbf{g}_{EGR}\|$ , 0). ~~Post this, we~~ We then rotated these aligned trajectories around the  $\mathbf{g}_{EGR}$  axis (the x-axis). ~~Thus, This method ensured that~~ the distances from the origin in the original three-dimensional spaces ~~are were~~ preserved in the two-dimensional ~~equivalent counterparts~~.

The scatter plot within these two-dimensional spaces ~~reveals illustrate~~ characteristic distributions of peri-SWR trajectories based on ~~phases and task types~~. ~~For instance, one can observe the phases and types of task.~~ One can observe, for example, that the magnitude of  $\|\text{mid-eSWR}^+\|$  surpasses that of  $\|\text{pre-eSWR}^+\|$  (Figure 6B), ~~which is~~ consistent with our earlier findings (Figure 5).

## 2.7. Fluctuations Directionality of hippocampal neural trajectories between encoding and retrieval states

~~Next, we examined trajectory~~ We then investigated the directions of the trajectories in relation to  $\overrightarrow{\mathbf{g}_{EGR}}$ . The directions of SWRs were defined by the neural trajectory at -250 ms and +250 ms from their center, ~~i.e., namely~~  $\overrightarrow{\mathbf{eSWR}^+}$ .

We calculated the density of  $\overrightarrow{\mathbf{eSWR}^+} \cdot \overrightarrow{\mathbf{g}_{EGR}}$ ,  $\overrightarrow{\mathbf{rSWR}^-} \cdot \overrightarrow{\mathbf{g}_{EGR}}$ , and  $\overrightarrow{\mathbf{eSWR}^-} \cdot \overrightarrow{\mathbf{rSWR}^-}$  (Figures 7A-D). ~~The~~  $\overrightarrow{\mathbf{rSWR}^-}$ .

<sup>13</sup>1.08 [1.07], median [IQR],  $n = 1,149$ , in Match IN task; 0.90 [1.12], median [IQR],  $n = 1,088$ , in Mismatch OUT task

<sup>14</sup>1.32 [1.24], median [IQR],  $n = 935$ , in Match IN task; 1.15 [1.26], median [IQR],  $n = 891$ , in Mismatch OUT task

<sup>15</sup>1.19 [0.96], median [IQR],  $n = 673$ , in Match IN task; 0.94 [0.88], median [IQR],  $n = 664$ , in Mismatch OUT task

$\vec{g}_{\text{EGR}}$  displayed demonstrated a biphasic distribution.

By taking the difference between comparing the distribution of  $\vec{r}\text{SWR}^+ \cdot \vec{g}_{\text{EGR}}$  (Figures 7A and B) and with that of  $\vec{r}\text{SWR}^- \cdot \vec{g}_{\text{EGR}}$  (Figures 7C and D), we computed the contributions of SWR (Figures 7E and F), which revealed indicated a shift in the direction of  $\vec{g}_{\text{EGR}}$  (Figures 7E and F: red rectangles).

Moreover, exclusively Furthermore, and only in the Mismatch OUT task,  $\vec{e}\text{SWR}^+ \cdot \vec{r}\text{SWR}^+$  was less than  $\vec{e}\text{SWR}^- \cdot \vec{r}\text{SWR}^-$  (baseline periods) (Figure 7F: pink circles). In simpler terms Put simply,  $\vec{e}\text{SWR}$  and  $\vec{r}\text{SWR}$  pointed in the opposite direction opposite directions only in the Mismatch OUT task but not in the Match IN task (Figure 7E: pink circles).

### 3. Discussion

### 4. Discussion

This study hypothesized that posits that hippocampal neurons generate distinct trajectories within low-dimensional spaces during a working memory (WM) task in humans, hippocampal neurons form unique trajectories, particularly specifically during sharp-wave ripple (SWR) periods. Initially, the multiunit spikes in the medial temporal lobe (MTL) regions were projected onto three-dimensional spaces during a Sternberg task using Gaussian Process Factor Analysis (GPFA) (Figure 1D–E and Figure 2A). The distance of the trajectory trajectory distance across WM phases ( $\|\vec{g}_{\text{FGE}}\|$ ,  $\|\vec{g}_{\text{FGM}}\|$ ,  $\|\vec{g}_{\text{FGR}}\|$ ,  $\|\vec{g}_{\text{EGM}}\|$ ,  $\|\vec{g}_{\text{EGR}}\|$ , and  $\|\vec{g}_{\text{MGR}}\|$ ) was notably markedly larger in the hippocampus than in the EC and amygdala (Figure 2E), indicating which implies dynamic neural activity in the hippocampus during the WM task. Further Additionally, in the hippocampus, the trajectory distance between the encoding and retrieval phases ( $\|\vec{g}_{\text{FGE}}\|$ ) exhibited a positive correlation was found to positively correlate with memory load (Figure 3C–D), reflecting denoting WM processing. The hippocampal neural trajectory was found to increase transiently momentarily increased during SWRs (Figure 5). Finally Eventually, the hippocampal neural trajectory switched alternated between encoding and retrieval states, moving progressing specifically from encoding to retrieval during SWR events (Figure 7). These findings not only explain various facets Such

discoveries not only interpret varying aspects of hippocampal neural activity during a WM task in humans, but also offer new fresh insights into how SWRs influence the switch in help alter neural states.

We found Our findings show that the distance of the hippocampal neural trajectory across the phases was greater in the hippocampus compared to that in the EC and amygdala, even when, even after considering the distance from  $O$  in these regions, surpassed that in the EC and amygdala (Figure 2C–E). This supports the involvement reaffirms the participation of the hippocampus in the WM task, aligning with previous reports coinciding with prior assertions of hippocampal persistent firing during the maintenance phase [3] [4] [5] [6]. However, when we applied applying GPFA to multiunit activity during a 1-second level resolution of the WM task, we observed noticed that the neural trajectory in low-dimensional space showed demonstrated a memory-load dependency between the dependence between encoding and retrieval phases, symbolized denoted as  $\|\vec{g}_{\text{EGR}}\|$  (Figure 3). These findings corroborate the association of the hippocampus with This supports the association between the hippocampus and WM processing.

Our analysis was confined to focused on putative CA1 regions (Figure 4), which was bolstered by several factors is supported by various contributions. This specific focus stems from established observations that SWRs synchronize with spike bursts concentration arises from well-established observations where SWRs coincide with spike clusters of interneurons and pyramidal neurons [44] [45] [46] [47], potentially within a 50  $\mu\text{m}$  radius of the recording site [48]. We further identified an increased incidence of SWRs An increase in the instances of SWRs was identified during the first 0–400 ms of the retrieval phase (Figure 4D). This finding harmonizes with previous reports of heightened SWR occurrence preceding observation aligns with earlier reports of increased SWR occurrence before spontaneous verbal recall [21] [22], supporting our results reinforcing our findings under a triggered retrieval condition. The observed log-normal distributions of both SWR duration length and ripple band peak amplitude observed in this study (Figure 4C & E) is in accordance with the consensus in this field [39]. As a result, our decision to restrict recording sites concur with the field's consensus [39]. Consequently, confining

recordings to putative CA1 regions likely contributed to enhancing improved the accuracy of SWR detection. However, the observed increase in trajectory distance from *O* during SWRs (Figure 5) might have been skewed towards higher values may be skewed higher due to channel selection. However/Nevertheless, this potential bias does not substantially challenge our primary findings/significantly undermine our primary conclusions.

Interestingly, during the retrieval phase, the trajectory directions oscillated trajectory directions alternated between encoding and retrieval states during both both during baseline and SWR periods (Figure 7C & D). Moreover/Furthermore, the balance of this oscillation shifted/transitioned from encoding to retrieval state during SWR events/episodes (Figure 7 E & F). These results are consistent with previous reports on outcomes align with preceding reports regarding the role of SWR SWRs in memory retrieval [21] [22]. Our findings highlight a new understanding, suggesting that suggest a novel understanding where SWRs occur when the hippocampal representation transitions from encoding to retrieval states. Therefore, these results reveal novel, thereby revealing unexplored aspects of hippocampal representations, including such as (i) neuronal oscillation between encoding and retrieval states/phases during a WM task, and (ii) SWR serving as a trigger functioning as a catalyst for changing neural states.

Furthermore/Moreover, our study uncovered WM-task type-specific identified differences between encoding- and retrieval-SWRs (Figure 7E–F) specific to WM-task types. Notably, opposing counter movements of encoding-SWR (eSWR) and retrieval-SWR (rSWR) were not observed-seen in the Match IN task but were apparent-evident in the Mismatch OUT task. These observations can be explained by the The memory engram theory [49]. Particularly, the can explain these observations [49]. The Match In task provided participants with previously presented letters, contrastingly, for instance, presented participants with previous letters, whereas the Mismatch OUT task introduced a new letter not-present absent in the encoding phase. These interpretations underscore the significant highlight the vital role of SWR in human cognitive processes.

In conclusion, the present this investigation demonstrated that during a WM task, hippocampal ac-

tivity oscillates between encoding and retrieval states during a WM task and uniquely transitions, uniquely transitioning from encoding to retrieval during SWR incidents/events. These findings provide meaningful insight offer valuable insights into the neural counterparts and functionality substrates and workings of working memory in within the hippocampus.

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## Contributors

Y.W. and T.Y. conceptualized the study; Y.W. performed the data analysis; Y.W. and T.Y. wrote the original draft; and all authors reviewed the final manuscript.

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## Declaration of Interests

The authors declare that they have no competing interests.

## Data and code availability

The data is available on G-Node (<https://doi.gin.g-node.org/10.12751/g-node.d76994/>). The source code is available on GitHub (<https://github.com/yanagisawa-lab/hippocampal-neural-fluctuation-during-a-WM-task-in-humans>).

## Inclusion and Diversity Statement

We support inclusive, diverse, and equitable conduct of research.

## Declaration of Generative AI in Scientific Writing

The authors employed ChatGPT, provided by OpenAI, for enhancing the manuscript’s English language quality. After incorporating the suggested improvements, the authors meticulously revised the content. Ultimate responsibility for the final content of this publication rests entirely with the authors.

## Tables

Subject ID	of sessions	AHL	AHR	PHL	PHR	ECL	ECR	AL	AR	SOZ
1	4	o	x	o	o	o	x	o	x	"AHR, LR"
2	7	o	o	o	o	o	o	o	o	"AHR, PHR"
3	3	o	o	o	o	o	o	o	x	"AHL, PHL"
4	2	o	o	o	o	o	o	o	o	"AHL, AHR, PHL, PHR"
5	3	o	x	x	o	x	x	o	x	DRR
6	6	o	o	o	o	o	o	o	o	"AHL, PHL, ECL, AL"
7	4	o	o	o	o	o	o	o	o	"AHR, PHR"
8	5	o	o	o	o	o	o	o	o	ECR
9	2	o	o	o	o	o	o	o	o	"ECR, AR"

**Table 1 – Distribution of Electrodes within the Dataset** Electrode Distribution within the Dataset

~~This~~ The figure ~~represents the outlines~~ electrode placements and ~~the~~ seizure onset zones. ~~Regions designated~~ Areas labelled with "o" ~~were available~~ are included in the dataset, ~~whereas~~ while those ~~marked with~~ indicated by "x" (navy) ~~were not present~~ are absent. ~~Abbreviations include~~ Denoted abbreviations: AHL, left hippocampal head; AHR, right hippocampal head; PHL, left hippocampal body; PHR, right hippocampal body; ECL, left entorhinal cortex; ECR, right entorhinal cortex; AL, left amygdala; AR, right amygdala; ~~and~~ SOZ symbolizes refers to the seizure onset zone.



Subject	AHL	AHR	PHL	PHR
1	0.60 ± 0.14	n.a.	n.a.	0.1 ± 0
2	0.21 ± 0.16	0.17 ± 0.21	0.18 ± 0.22	0.20 ± 0.15
3	0.40 ± 0.42	0.83 ± 0.12	n.a.	n.a.
4	0.10 ± 0.00	0.10 ± 0.00	0.90 ± 0.00	0.10 ± 0.14
5	n.a.	n.a.	n.a.	n.a.
6	0.63 ± 0.06	n.a.	n.a.	0.27 ± 0.06
7	0.10 ± 0.00	0.35 ± 0.35	0.37 ± 0.47	0.10 ± 0.00
8	0.13 ± 0.10	n.a.	0.28 ± 0.49	n.a.
9	n.a.	0.85 ± 0.07	0.15 ± 0.07	n.a.

**Table 2 – ~~Silhouette score of UMAP clustering for  $SWR^+$  candidates and  $SWR^-$  candidates~~ Silhouette scores of UMAP clustering for  $SWR^+$  candidates and  $SWR^-$  candidates**

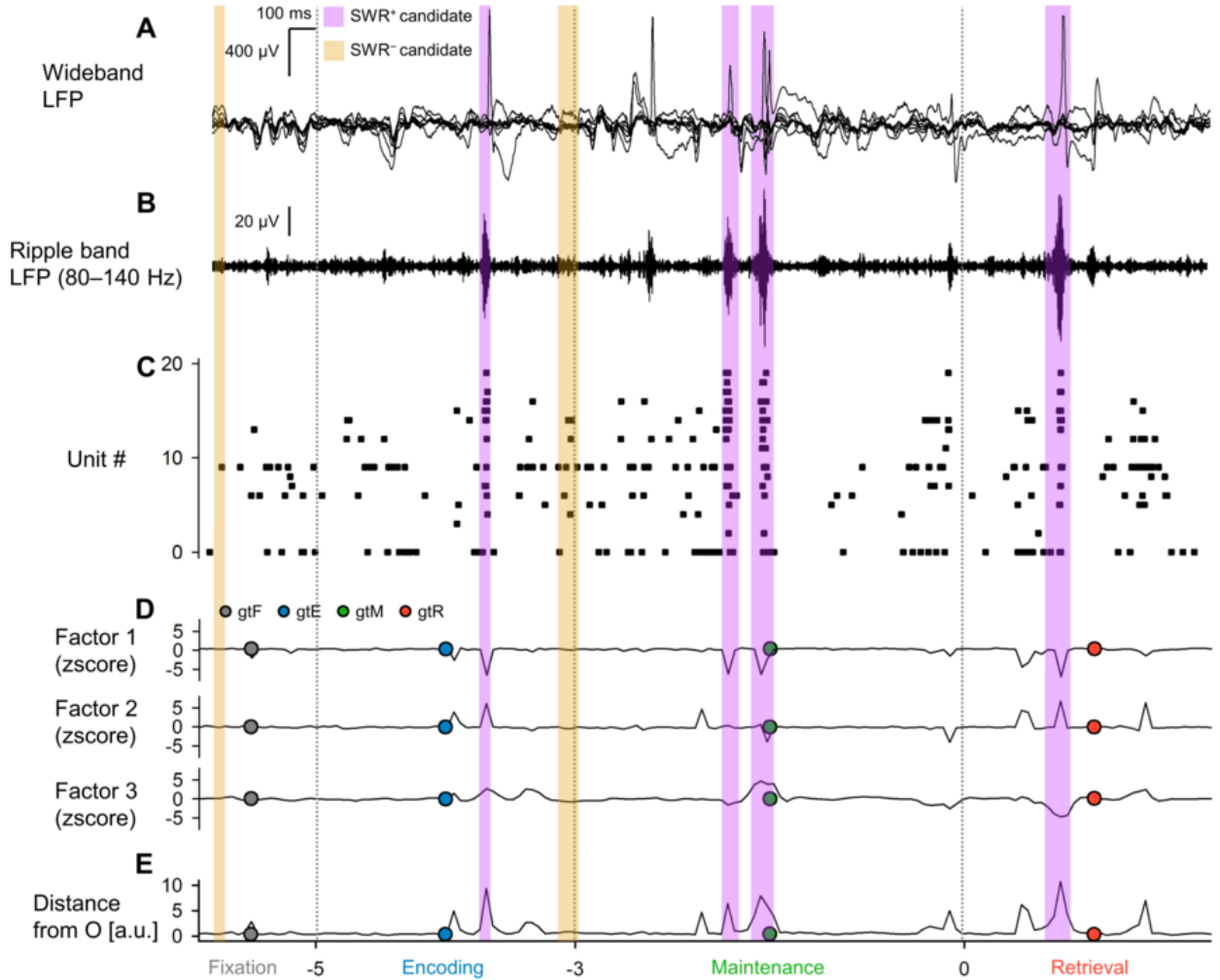
The silhouette scores (mean ± SD across sessions per subject) ~~for pertaining to~~ UMAP clustering of  $SWR^+$  candidates and  $SWR^-$  candidates ~~are calculated and presented in Figure 4A) were calculated.~~ These calculations are based on their corresponding multiunit spike patterns, ~~where the mean values were observed are 0.205 with a standard deviation of 0.285.~~ The median ~~IQR~~ and interquartile range are also presented (see Figure 4B).

Subject ID	of sessions	of trials	ROI	of SWRs	SWR incidence [Hz]
1	2	100	AHL	274	0.34
3	2	97	AHR	325	0.42
4	2	99	PHL	202	0.26
6	2	100	AHL	297	0.37
9	2	97	AHR	72	0.09
Total = 10	Total = 493	"Total = 1,170"	0.30 ± 0.13 (mean ± SD)		

**Table 3 – ~~Accounting for Defined SWR Events~~ Accounting for Specific SWR Events**

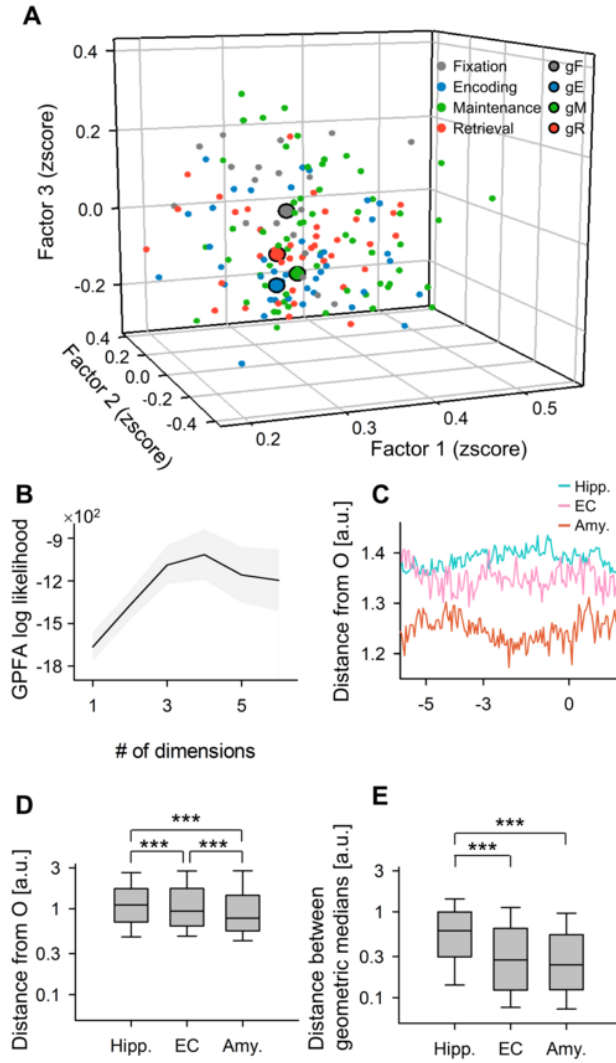
The table ~~collates~~ compiles statistics ~~of putative-related to assumed~~ CA1 regions and SWR events. ~~Only~~ To minimize sampling bias, only the ~~first initial~~ two sessions (sessions 1 and 2) from each subject were ~~considered to minimize sampling bias~~ utilized.

## Figures



**Figure 1 – Local Field Potentials (LFP), Multiunit Activity, and Neural Trajectories in the Hippocampus During a Modified Sternberg Task**

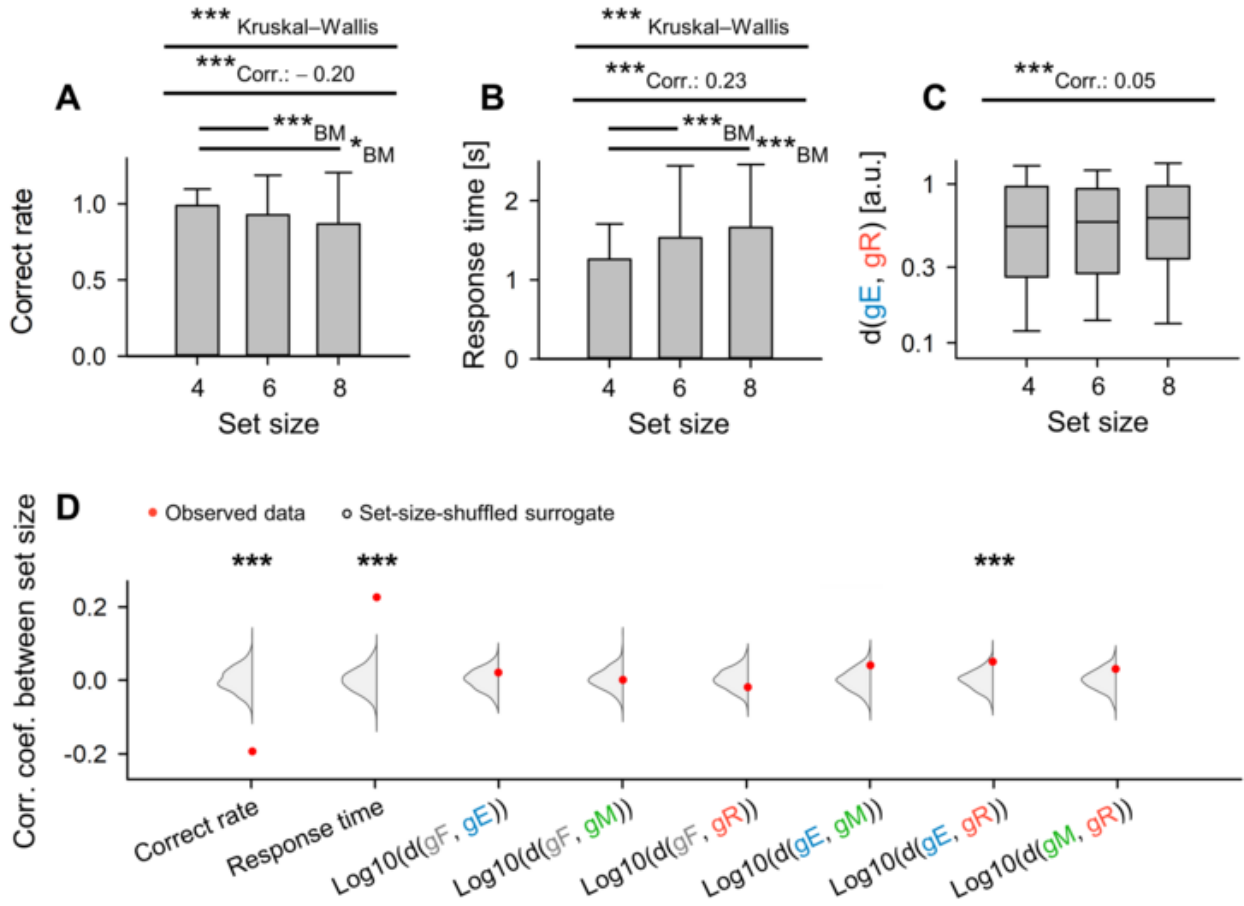
**A.** These traces show representative wideband LFP intracranial EEG (iEEG) signals recorded from the left hippocampal head. The subject performed a modified Sternberg working memory task, which includes fixation (1 s, gray), encoding (2 s, blue), maintenance (3 s, green), and retrieval (2 s, red). **B.** We then present the corresponding ripple band LFP traces. **C.** The raster plot depicts multiunit spikes taken from the LFP traces, sorted using a spike algorithm [38]. **D.** Subsequently, we illustrate the neural trajectories, which are calculated by GPFA on spike counts per unit with 50-ms bins. Each phase's geometric median is marked by the dot circles. **E.** The trajectory's distance from the origin *O* is portrayed, with purple and yellow rectangles indicating the timings for SWR<sup>+</sup> candidates and SWR<sup>-</sup> candidates (considered as controls for SWR<sup>+</sup>), respectively.



**Figure 2 – State-Dependent Trajectories of Hippocampal Neurons**

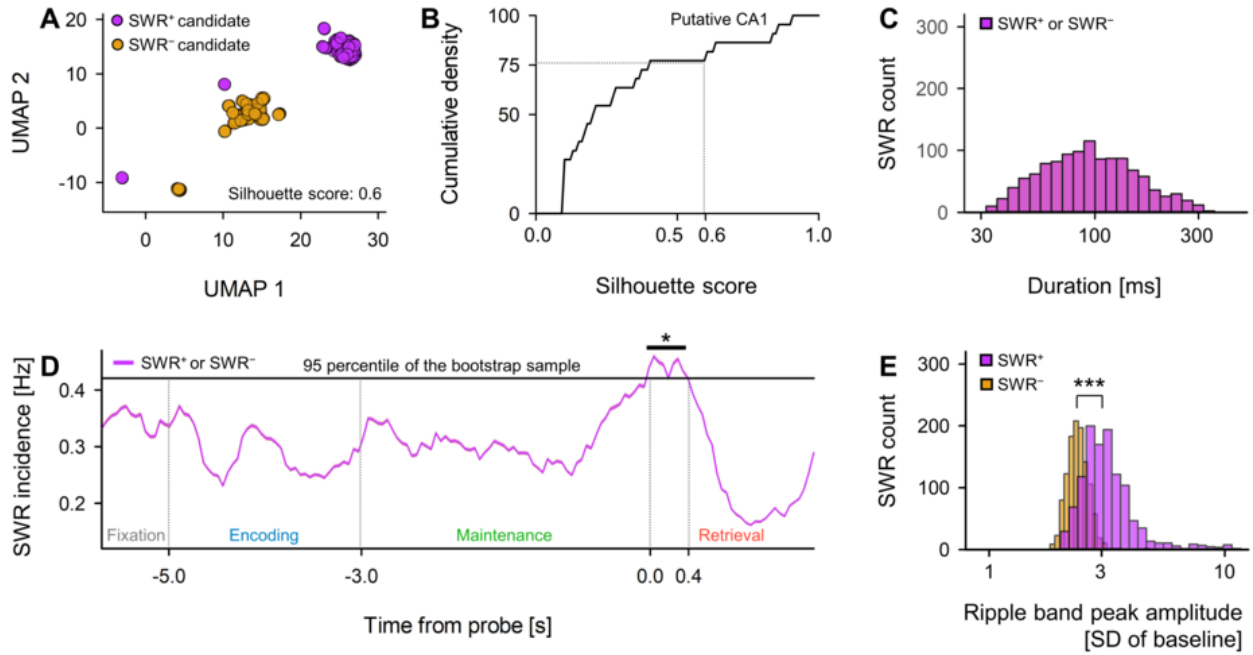
**A.** Neural trajectories within the initial three-dimensional factors derived from the Gaussian Process Factor Analysis (GPFA) are displayed. The smaller dots correspond to coordinates of 50-ms neural trajectory bins, while the larger dots with *black* edges signify the geometric medians for respective stages in the Sternberg working memory task: fixation (*gray*), encoding (*blue*), maintenance (*green*), and retrieval (*red*). **B.** The figure conveys the log-likelihood of the GPFA models versus the count of dimensions used to embed multiunit spikes found in the medial temporal lobe (MTL) territories. In specific, the elbow method pinpointed the optimal dimension to be three. **C.** This panel illustrates the distance of the neural trajectories from the origin (*O*) for the hippocampus (Hipp.), entorhinal cortex (EC), and amygdala (Amy.), against the time elapsed from the probe onset. **D.** The distance of the trajectory from *O* within MTL regions is displayed. The hippocampus shows the farthest distance, followed by the EC and the Amygdala. **E.** The plot represents inter-phase trajectory distances within the MTL regions. Abbreviations:





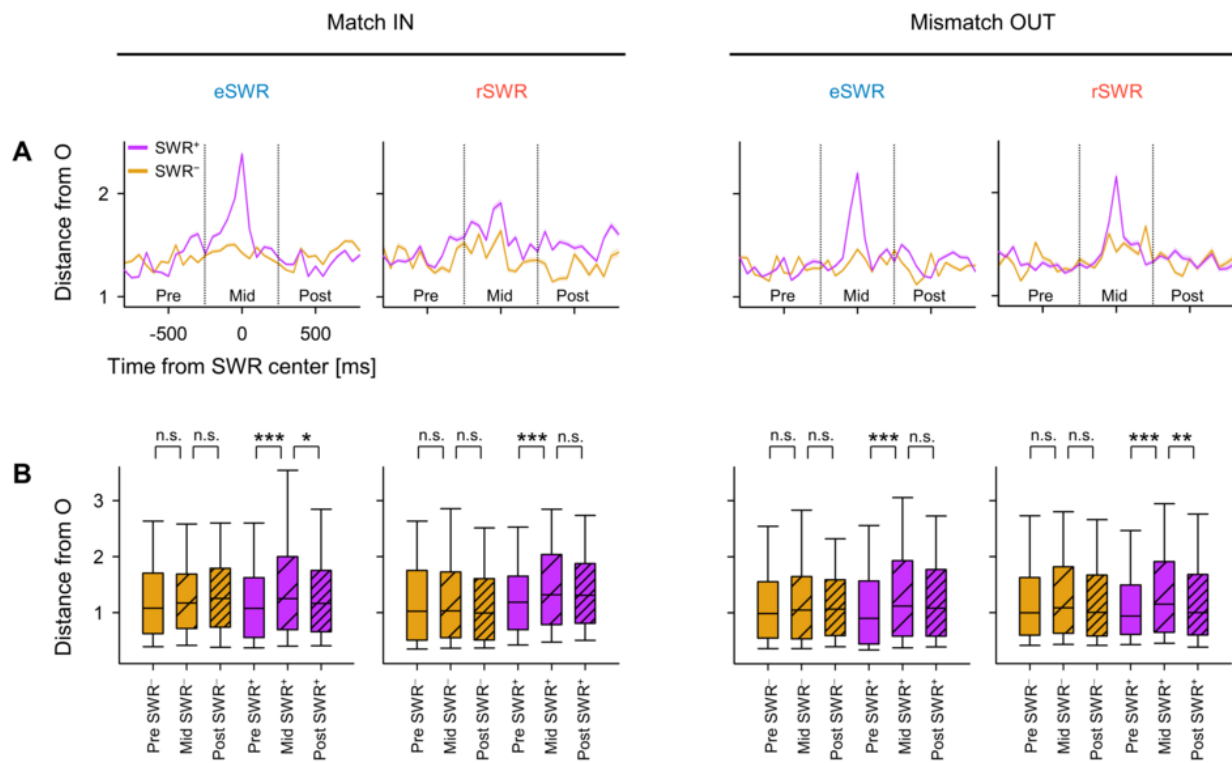
**Figure 3 – Dependency of Trajectory Distance on Memory Load: Encoding and Retrieval States in Hippocampus**

**A.** The relationship between set size (number of letters that need to be encoded) and correct rate in the working memory task (coefficient = -0.20, \*\*\* $p < 0.001$ ). **B.** The correlation between set size and response time (coefficient = 0.23, \*\*\* $p < 0.001$ ). **C.** The impact of set size on the inter-phase distances between the encoding and retrieval phases ( $\|g_{EgR}\|$ ) (correlation coefficient = 0.05). **D.** Red dots represent experimental observations of correlations between set size and the following parameters: correct rate, response time,  $\log_{10} \|g_{FgE}\|$ ,  $\log_{10} \|g_{FgM}\|$ ,  $\log_{10} \|g_{FgR}\|$ ,  $\log_{10} \|g_{EgM}\|$ ,  $\log_{10} \|g_{EgR}\|$ , and  $\log_{10} \|g_{MgR}\|$ . The gray kernel density plot illustrates the corresponding set-size-shuffled surrogate ( $n = 1,000$ ) (\*\*\* $ps < 0.001$ ).



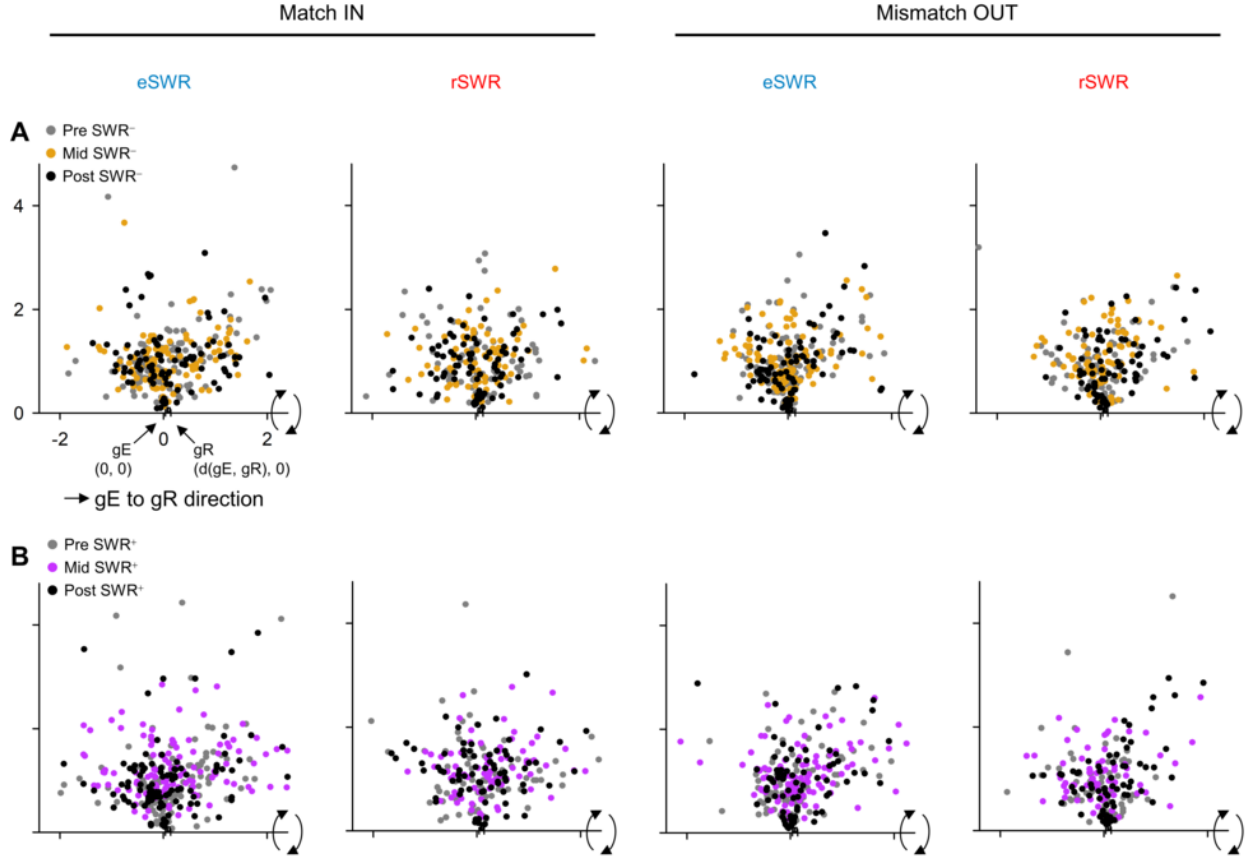
**Figure 4 – Detection of SWRs in Presumptive CA1 Regions**

**A.** Two-dimensional UMAP (Uniform Manifold Approximation and Projection) [41] projection of multiunit spikes during SWR<sup>+</sup> candidates (purple) and SWR<sup>-</sup> candidates (yellow). **B.** Cumulative density plot shows silhouette scores, indicative of UMAP clustering quality, for hippocampal regions (see Table 2 for reference). Note that hippocampal regions with silhouette scores greater than 0.60 (equivalent to the 75<sup>th</sup> percentile) were identified as possible CA1 regions. SWR<sup>+</sup> and SWR<sup>-</sup> candidates recorded from these speculative CA1 regions were respectively classified as SWR<sup>+</sup> and SWR<sup>-</sup> ( $n_s = 1,170$ ). **C.** The identical distributions of durations are presented for SWR<sup>+</sup> (purple) and SWR<sup>-</sup> (yellow), owing to their definitions (93.0 [65.4] ms, median [IQR]). **D.** SWR incidence for both SWR<sup>+</sup> (purple) and SWR<sup>-</sup> (yellow) obtained relative to the probe's timing is illustrated as a mean  $\pm$  95% confidence interval. However, as the intervals may not be visible due to their narrow range, note that a significant increase in SWR incidence was detected during the initial 400 ms of the retrieval phase (0.421 [Hz],  $*p < 0.05$ , bootstrap test). **E.** The distributions of ripple band peak amplitudes for SWR<sup>-</sup> (yellow; 2.37 [0.33] SD of baseline, median [IQR]) and SWR<sup>+</sup> (purple; 3.05 [0.85] SD of baseline, median [IQR]) are delineated ( $***p < 0.001$ , the Brunner–Munzel test).



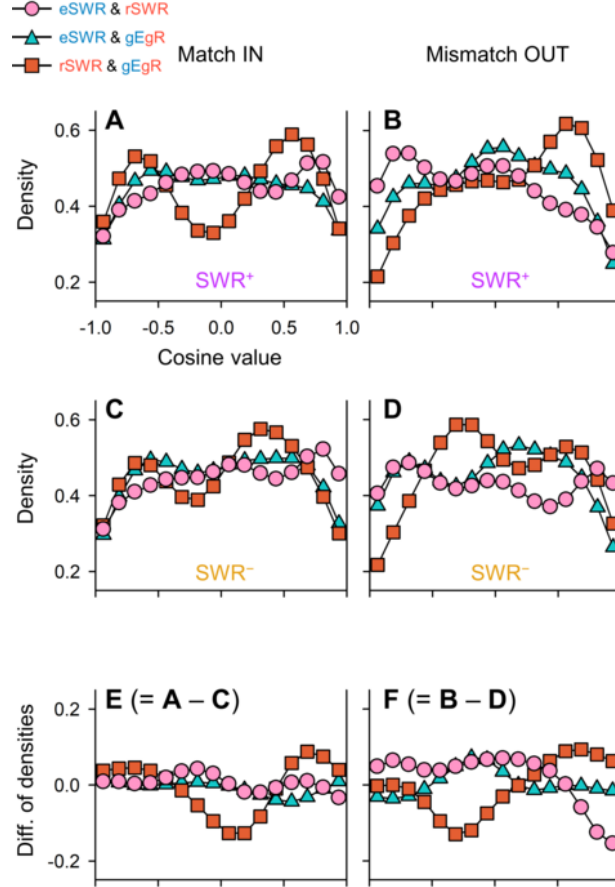
**Figure 5 – Transient Alterations in Neural Trajectory During SWR Events**

**A.** Displayed is the distance from origin (*O*) of the peri-sharp-wave-ripple trajectory (mean  $\pm$ 95% confidence interval). The intervals may not be apparent due to their slender ranges. **B.** Shown is the distance from the origin (*O*) during pre-, mid-, and post-SWR periods (\* $p < 0.05$ , \*\* $p < 0.01$ , \*\*\* $p < 0.001$ ; assessed using the Brunner–Munzel test). Abbreviations: SWR, sharp-wave ripple events; eSWR, SWR during the encoding phase; rSWR, SWR while in the retrieval phase; SWR<sup>+</sup>, positive SWR event; SWR<sup>-</sup>, control events for SWR<sup>+</sup>; pre-, mid-, or post-SWR denote the time intervals from  $-800$  to  $-250$  ms, from  $-250$  to  $+250$  ms, or from  $+250$  to  $+800$  ms, all relative to the center of the SWR.



**Figure 6 – Visualization of Neural Trajectories during SWR in Two-Dimensional Spaces**

The panels display hippocampal neural trajectories during SWR as projected onto two-dimensional spaces. **A.** Indicates hippocampal neural trajectories pre-SWR<sup>-</sup> (gray), mid-SWR<sup>-</sup> (yellow), and post-SWR<sup>-</sup> (black). **B.** Represents the equivalents for SWR<sup>+</sup> as opposed to SWR<sup>-</sup>. The  $\|g_E g_R\|$  varied among sessions. The projection was applied in the following manner: First, a linear transformation positioned  $g_E$  at the origin  $O$  (0,0), and  $g_R$  at  $(\|g_E g_R\|, 0)$ . The point cloud was then rotated around the  $g_E g_R$  axis (equivalent to the x axis) for fitting into two-dimensional spaces. Therefore, within these two-dimensional spaces, both the distances from  $O$  and the angles preserved the original makeup of the  $g_E g_R$  axis from the original three-dimensional spaces. Abbreviations: SWR signifies sharp-wave ripple events; eSWR denotes SWR during the encoding phase; rSWR indicates SWR during the retrieval phase; SWR<sup>+</sup>, marks an SWR event; SWR<sup>-</sup> refers to control events for SWR<sup>+</sup>; pre-SWR, mid-SWR, or post-SWR, reference the time intervals from -800 to -250 ms, from -250 to +250 ms, or from +250 to +800 ms from the center of SWR.



**Figure 7 – Directions of Neural Trajectories during SWRs Based on Encoding and Retrieval States**

**A–B** Kernel density estimation (KDE) distributions of  $\overrightarrow{eSWR^+} \cdot \overrightarrow{rSWR^+}$  (pink circles),  $\overrightarrow{eSWR^+} \cdot \overrightarrow{gEgR}$  (blue triangles), and  $\overrightarrow{rSWR^+} \cdot \overrightarrow{gEgR}$  (red rectangles) in Match In (A) and Mismatch OUT tasks (B). **C–D** Present the corresponding distributions of  $SWR^-$  instead of those of  $SWR^+$  in A and B. **E–F** Depict the differences in the distributions of  $SWR^+$  and  $SWR^-$ , illuminating the SWR components ( $E = C - A$ ;  $F = D - B$ ). Note the biphasic distributions of  $\overrightarrow{rSWR^+} \cdot \overrightarrow{gEgR}$ , suggesting fluctuations between the encoding and retrieval states during the Sternberg task. Moreover, inverse directionality between  $\overrightarrow{eSWR^+}$  and  $\overrightarrow{rSWR^+}$  was observed (pink circles) in the Mismatch OUT task, but not in the Match IN task **E–F**). Finally, shifts from the retrieval to encoding states were evident in the SWR components in both the Match IN and Mismatch OUT tasks (red rectangles in E and F).