

Highlights

- Neural trajectories in the hippocampus exhibited greater variability during a working memory (WM) task compared to those in the entorhinal cortex and amygdala regions.
- The distance of neural trajectories between encoding and retrieval states in the hippocampus was memory-load dependent during a WM task.
- Hippocampal neural trajectories fluctuated between the encoding and retrieval states in a task-dependent manner during both baseline and sharp-wave ripple (SWR) periods.
- Hippocampal neural trajectories shifted from encoding to retrieval states during SWR period.

Hippocampal neural fluctuations between memory encoding and retrieval states during a working memory task in humans

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Abstract

Working memory (WM) plays a ~~critical role in various~~ pivotal role in multiple cognitive functions, ~~but the intricate neural mechanisms that support its operation remain elusive. Specifically, while yet the complex neural mechanisms supporting its operation continue to remain unclear.~~ In particular, despite the recognized roles of the hippocampus and sharp-wave ripple complexes (SWRs) – brief, synchronous neural ~~oseillation~~ oscillations observed in the hippocampus – ~~are recognized for their roles~~ in memory consolidation and retrieval, their ~~involvement in WM tasks has not yet been defined. Here we show~~ contribution to WM tasks remains undefined. We demonstrate that during a WM task, multiunit activity patterns in the hippocampus ~~display distinctive~~ exhibit unique dynamics, particularly during SWR periods. This study analyzed a dataset ~~derived~~ obtained from intracranial electroencephalogram recordings ~~conducted~~ performed in the medial temporal lobe (MTL) of nine ~~individuals with epilepsy~~ epilepsy patients during an eight-second Sternberg task. We ~~applied~~ employed Gaussian-process factor analysis to ~~determine~~ identify low-dimensional neural representations, ~~or referred to as~~ 'trajectories,' within the MTL regions ~~while performing~~ during the WM task. The results ~~revealed~~ depicted significant variations in ~~the hippocampus' neural trajectories compared~~ hippocampal neural trajectories as opposed to those in the entorhinal cortex and amygdala. ~~Additionally, the distance of the trajectory~~ Moreover, the trajectory distance between the encoding and retrieval phases was ~~dependent on memory load. Importantly~~ memory load-dependent. Notably, hippocampal trajectories during the retrieval phase ~~demonstrated fluctuations~~ showcased oscillations between encoding and retrieval ~~stages based on~~ states, contingent on the task type, particularly ~~showing~~ displaying a transient shift from encoding to retrieval states during SWRs. These findings ~~underline~~ emphasize the hippocampus's ~~essential function in performing~~ central role in executing WM tasks and ~~propose a hypothesis for future research~~ suggest a future research hypothesis: the functional state of the hippocampus ~~transition~~ transitions from encoding to retrieval during SWRs.

Keywords: working memory, memory load, hippocampus, sharp-wave ripples, humans

7 figures, 3 tables, 221 words for abstract, and 3073 words for main text

1. Introduction

Working memory (WM) significantly influences ~~everyday~~ daily life, and ~~the neural bases of this cognitive process~~ its neural bases continue to be ~~the subject of intensive research. One key~~ intensively researched. A primary focus of this research is the hippocampus, a structure integral to memory functions [1] [2] [3] [4] [5] [6] [7] [8] [9]. ~~A deeper~~ Deepening

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our understanding of the hippocampus's role in working memory is not only crucial for advancing our knowledge critical not only for knowledge advancement but also potentially for enhancing cognitive abilities cognitive abilities enhancement.

Current evidence suggests that a transient, synchronized oscillation, called known as sharp-wave ripple (SWR) [10], is associated with several cognitive functions. These include comprise memory replay [11] [12] [13] [14] [15], memory consolidation [16] [17] [18] [19], memory recall [20] [21] [22], and neural plasticity [23] [24]. These associations suggest that SWR may be a fundamental computational manifestation posit that SWR could be a core computational feature of hippocampal processing, contributing to working memory performance as well. However, research on the effects of SWRs SWR's effects on working memory is relatively scarce [25], and is predominantly limited sparse [25], being mainly restricted to rodent models engaged in navigation tasks, where the timing of with indefinable memory acquisition and recall is not clearly defined timing.

Recent studies have found research proposes that low-dimensional representations in the hippocampal neurons can explain WM task performances elucidate WM task performance. Specifically, the firing patterns of place cells [26] [27] [28] [29] [30], found in the hippocampus, have been identified display within a dynamic, nonlinear three-dimensional hyperbolic space in rats [31]. Additionally, grid cells in the entorhinal cortex (EC), which is the main pathway—a primary route to the hippocampus [32] [33] [34], exhibited—showed a toroidal geometry during exploration in rats [35]. However, these studies These studies, however, are limited by their focus emphasis on spatial navigation tasks in rodents, affecting which affect the temporal resolution of WM tasks. To illustrate For instance, the timing of when an animal acquires information is ambiguous in these settings information acquisition by an animal is unclear in these contexts. Therefore, the applicability generalizability of these findings to human subjects humans and tasks beyond navigation still requires confirmation verification.

Considering these factors, this study investigates explores the hypothesis that hippocampal neurons show exhibit unique 'neural trajectories' in low-dimensional spaces, particularly during SWR periods, in response

episodes, when responding to WM tasks. To test this hypothesis, we employed a We tested this hypothesis using a high-temporal-resolution dataset of patients performing an eight-second Sternberg task (1 s for fixation, 2 s for encoding, 3 s for maintenance, and 2 s for retrieval) with high temporal resolution. Intracranial electroencephalography (iEEG) signals within the The patients' medial temporal lobe (MTL) were recorded for these patients intracranial electroencephalography (iEEG) signals were recorded [36]. To examine analyze low-dimensional neural trajectories, we utilized employed Gaussian-process factor analysis (GPFA), an established method for analyzing a recognized method for examining neural population dynamics [37].

2. Methods

2.1. Dataset

The dataset used in this study, which is publicly available—This study utilized a publicly available dataset that comprises nine epilepsy patients performing a modified Sternberg task [36]. This task includes four phases: fixation (1s), encoding (2s), maintenance (3s), and retrieval (2s). During the encoding phase, participants were presented with a set of four, six, or eight alphabet letters. They were then tasked with determining Their task was to determine whether a probe letter displayed during the retrieval phase had previously appeared (the correct response for was previously presented (the accurate response in a Match IN task) or not (the correct response for accurate response for a Mismatch OUT task). Intracranial electroencephalography (iEEG) signals were captured collected with a 32 kHz sampling rate within a in the 0.5–5,000 Hz frequency range, using depth electrodes in targeting medial temporal lobe (MTL) regions: the anterior head of the left and right hippocampus (AHL and AHR), the posterior body of the hippocampus (PHL and PHR), the entorhinal cortex (ECL and ECR), and the amygdala (AL and AR), as depicted—illustrated in Figure 1A and Table 1. The iEEG signals were subsequently later downsampled to 2 kHz. Correlations between variables such as like set size and correct rate were examined (Figure ??S1). Multiunit spike timings were determined via identified using a spike sorting algorithm [38] using and the Combinato package (<https://github.com/jniediek/combinato>) (Figure 1C).

2.2. Calculation of neural trajectories using GPFA

Neural trajectories, also ~~referred to~~ known as 'factors', in the hippocampus, EC, and amygdala were ~~determined~~ calculated using GPFA [37] applied to the multiunit activity data for each session, ~~performed~~ implemented with the elephant package (<https://elephant.readthedocs.io/en/latest/reference/gpfa.html>). The bin size was set to 50 ms, without overlaps. Each factor was z-normalized across all sessions, ~~and after which~~ the Euclidean distance from the origin (O) was ~~then computed~~ computed. For each trajectory within a region such as AHL, geometric medians (g_F for fixation, g_E for encoding, g_M for maintenance, and g_R for retrieval phase) were calculated by determining the median coordinates of the trajectory during the four phases. ~~An optimal~~ Optimal GPFA dimensionality was ~~found to be established as~~ three using the elbow method obtained by examining the log-likelihood values ~~through via~~ a three-fold cross-validation approach (Figure 2B).

2.3. Identifying SWR candidates from hippocampal regions

Potential SWR events ~~within in~~ the hippocampus were ~~detected~~ identified using a widely ~~used~~ recognized method [39]. LFP signals from a region of interest (ROI) ~~like, such as~~ AHL, were re-referenced by ~~deducting the averaged~~ subtracting the average signal from locations outside the ROI (for instance, AHR, PHL, PHR, ECL, ECR, AL, and AR). The re-referenced LFP signals were then filtered with a ripple-band filter (80–140 Hz) to ~~determine~~ identify SWR candidates, ~~marked~~ denoted as SWR^+ candidates. SWR detection was ~~carried out~~ conducted using a published tool (https://github.com/Eden-Kramer-Lab/ripple_detection) [40], with the bandpass range adjusted to 80–140 Hz for humans [21] [22], ~~unlike contrasting with~~ the initial 150–250 Hz range typically applied to rodents. Control events for SWR^+ candidates, labeled as SWR^- candidates, were detected by randomly shuffling the timestamps of SWR^+ candidates across all trials and subjects. The resulting SWR^+/SWR^- candidates were ~~then~~ subsequently visually inspected.

2.4. Defining SWRs from putative hippocampal CA1 regions

Potential SWRs were ~~differentiated~~ distinguished from SWR candidates in ~~putative~~ presumptive CA1 (cornu Ammonis 1) regions. These regions were initially defined as follows: SWR^+/SWR^- candidates in the hippocampus were projected into a two-dimensional space based on overlapping spike counts per unit using a supervised ~~method~~ approach, UMAP (Uniform Manifold Approximation and Projection) [41]. Clustering validation was ~~performed~~ conducted by calculating the silhouette score [42] from clustered samples. Regions in the hippocampus, which scored ~~on average~~ above 0.6 ~~on average 0.6~~ across sessions (75th percentile), were identified as putative CA1 ~~regions~~ areas, resulting in the identification of five electrode positions from five patients. SWR^+/SWR^- candidates in these predetermined CA1 ~~regions were categorized~~ areas were classified as SWR^+/SWR^- , ~~and thus they no longer retained thereby~~ relinquishing their candidate status. The duration and ripple band peak amplitude of SWRs were found to follow log-normal distributions. Each ~~time period of SWR~~ was partitioned SWR period was segmented relative to the time from the SWR center into pre- (at –800 to –300 ms from the SWR center), mid- (at –250 to +250 ms), and post-SWR (at +300 to +800 ms) times.

2.5. Statistical evaluation

Both the Brunner–Munzel test and the Kruskal–Wallis test were ~~executed~~ administered using the SciPy package in Python [43]. Correlational analysis was ~~conducted~~ performed by determining the rank of the observed correlation coefficient within its associated set-size-shuffled surrogate using a customized Python script. The bootstrap test was ~~implemented~~ performed with an in-house Python script.

3. Results

3.1. iEEG recording and neural trajectory in MTL regions during a Sternberg task

Our analysis ~~employed~~ utilized a publicly accessible dataset [36], ~~which comprises~~ comprised of LFP signals (Figure 1A) from MTL regions (Table 1), recorded during the execution of a modified Sternberg task. ~~We~~

From these LFP signals, we extracted SWR⁺ candidates from LFP signals that were filtered in the 80–140 Hz ripple band (Figure 1B), originating in from all hippocampal regions (refer to the Methods section). Meanwhile, we defined SWR⁻ candidates, control events for SWR⁺ candidates, were defined at the same timestamps but distributed across different trials (Figure 1). The dataset also encompassed included multiunit spikes (Figure 1C), recognized via identified using a spike sorting algorithm [38]. Employing GPFA [37], we applied this Applying GPFA [37] to 50-ms windows of binned multiunit activity without overlap to determine, we determined the neural trajectories, or factors, of MTL regions by session and region (Figure 1D). We normalized each factor per session and region, for instance example, session #2 in AHL of subject #1. We 1, then calculated the Euclidean distance from the origin (O) (Figure 1E).

3.2. Hippocampal neural trajectory correlation with a Sternberg task

Figure 2A exhibits a displays the distribution of median neural trajectories, comprising which composed of 50 trials, within the three main factor spaces. Utilizing Using the elbow method, we established determined three as the optimal embedding dimension for the GPFA model as three (Figure 2B). The trajectory distance from the origin (O) — represented as $\|g_F\|$, $\|g_E\|$, $\|g_M\|$, and $\|g_R\|$ — in the hippocampus surpassed exceeded the corresponding distances in the EC and amygdala (Figure 2C & D).¹ Similarly, we computed

We also calculated the distances between the geometric medians of four phases, namely $\|g_{FGE}\|$, $\|g_{FGM}\|$, $\|g_{FGR}\|$, $\|g_{EGM}\|$, $\|g_{EGR}\|$, and $\|g_{MGR}\|$. The hippocampus showed exhibited larger distances between phases than those in compared to the EC and the amygdala.²

¹Hippocampus: Distance = 1.11 [1.01], median [IQR], $n = 195,681$ timepoints; EC: Distance = 0.94 [1.10], median [IQR], $n = 133,761$ timepoints; Amygdala: Distance = 0.78 [0.88], median [IQR], $n = 165,281$ timepoints.

²Hippocampus: Distance = 0.60 [0.70], median [IQR], $n = 8,772$ combinations; EC: Distance = 0.28 [0.52], median [IQR], $n = 5,017$ combinations ($p < 0.01$; Brunner–Munzel test); Amygdala: Distance = 0.24 [0.42], median [IQR], $n = 7,466$ combinations ($p < 0.01$; Brunner–Munzel test).

3.3. Memory-load-dependent neural trajectory distance between encoding and retrieval states in the hippocampus

Regarding memory load in the Sternberg task, we We observed a negative correlation between the correct rate of trials and the set size, which denotes indicating the number of letters to be encoded, during the Sternberg task (Figure 3A).³ Concomitantly, Simultaneously, we found a positive correlation was noted between the response time and set size (Figure 3B).⁴ Next, we discovered

Further, we identified a positive correlation between the set size and the trajectory distance separating the encoding and retrieval phases ($\log_{10}\|g_{EGR}\|$) (Figure 3C).⁵ However, distances between other phase combinations did not highlight show statistically significant correlations (Figures 3D and ??).

3.4. Detection of hippocampal SWR from putative CA1 regions

To enhance the precision of improve the accuracy of the recording sites and SWR detection, we approximated estimated the electrode placements in the CA1 regions of the hippocampus using distinguished distinctive multiunit spike patterns during SWR events. We embedded SWR⁺/SWR⁻ candidates from each session and hippocampal region were embedded in in a two-dimensional space using UMAP (Figure 4A).⁶ With Using the silhouette score as a quality metric for clustering clustering quality metric (Figure 4B and Table 2), recording sites demonstrating we identified recording sites that showed an average silhouette score

³Correct rate: set size four (0.99 ± 0.11 , mean \pm SD; $n = 333$ trials) vs. set size six (0.93 ± 0.26 ; $n = 278$ trials; $p < 0.001$, Brunner–Munzel test with Bonferroni correction) and set size eight (0.87 ± 0.34 ; $n = 275$ trials; $p < 0.05$; Brunner–Munzel test with Bonferroni correction). Generally, $p < 0.001$ for Kruskal–Wallis test; correlation coefficient = -0.20 , $p < 0.001$.

⁴Response time: set size four (1.26 ± 0.45 s; $n = 333$ trials) vs. set size six (1.53 ± 0.91 s; $n = 278$ trials) and set size eight (1.66 ± 0.80 s; $n = 275$ trials). All comparisons $p < 0.001$, Brunner–Munzel test with Bonferroni correction; $p < 0.001$ for Kruskal–Wallis test; correlation coefficient = 0.22 , $p < 0.001$.

⁵Correlation between set size and $\log_{10}(\|g_{EGR}\|)$: correlation coefficient = 0.05 , $p < 0.001$. Specific values: $\|g_{EGR}\| = 0.54$ [0.70] for set size four, $n = 447$; $\|g_{EGR}\| = 0.58$ [0.66] for set size six, $n = 381$; $\|g_{EGR}\| = 0.61$ [0.63] for set size eight, $n = 395$.

⁶Consider the AHL in session #1 of subject #1 as a case in point an example.

exceeding 0.6 across all sessions ~~were identified~~ as putative CA1 regions.⁷ (Tables 2 and 3). ~~We From these, we~~ identified five putative CA1 regions, four of which were not ~~indicated identified~~ as seizure onset zones (Table 1). ~~Subsequently,~~

~~We labeled~~ SWR⁺/SWR⁻ candidates ~~within from~~ these putative CA1 regions ~~were labeled~~ as SWR⁺ and SWR⁻, respectively⁸ (Table 3). Both SWR⁺ and SWR⁻ ~~manifested identical durations~~⁹, due to their definitions ~~and,~~ ~~presented equivalent durations~~⁹. They followed a log-normal distribution (Figure 4C). ~~During An increase in SWR⁺ incidence was detected during the initial 400 ms of the retrieval phase,~~ ~~an increase in SWR⁺ incidence was found~~¹⁰ (Figure 4D). The peak ripple band amplitude of SWR⁺ ~~surpassed was higher than~~ that of SWR⁻ ~~and followed,~~ ~~following~~ a log-normal distribution (Figure 4E).¹¹.

3.5. Transient changes in hippocampal neural trajectory during SWR

We ~~assessed examined~~ the 'distance' of the neural trajectory from the origin (*O*) during SWR events in both encoding and retrieval phases (Figure 5A). ~~Observing the Upon observing an~~ increase in distance during SWR, as ~~illustrated shown~~ in Figure 5A, we categorized each SWR into three stages: pre-, mid-, and post-SWR. ~~Hence Thus,~~ the distances from *O* during ~~those such~~ SWR intervals are ~~identified represented~~ as $\|\text{pre-eSWR}^+\|$, $\|\text{mid-eSWR}^+\|$, and others. ~~As a result~~ ~~Consequently,~~ $\|\text{mid-eSWR}^+\|$ ¹² exceeded $\|\text{pre-eSWR}^+\|$ ¹³, and $\|\text{mid-rSWR}^+\|$ ¹⁴ was larger

⁷The identified regions were the AHL of subject #1, AHR of subject #3, PHL of subject #4, AHL of subject #6, and AHR of subject #9.

⁸These definitions ~~produced resulted in~~ equal counts for both categories: SWR⁺ ($n = 1,170$) and SWR⁻ ($n = 1,170$).

⁹~~These definitions result in equal durations for both categories: SWR⁺ (93.0 65.4ms) and SWR⁻ (93.0 65.4ms):~~

⁹~~These definitions resulted in equal durations for both categories: SWR⁺ (93.0 [65.4] ms) and SWR⁻ (93.0 [65.4] ms).~~

¹⁰SWR⁺ increased against the bootstrap sample; 95th percentile = 0.42 [Hz]; $p < 0.05$.

¹¹SWR⁺ (3.05 [0.85] SD of baseline, median [IQR]; $n = 1,170$) vs. SWR⁻ (2.37 [0.33] SD of baseline, median [IQR]; $n = 1,170$; $p < 0.001$; Brunner-Munzel test).

¹²1.25 [1.30], median [IQR], $n = 1,281$ in Match IN task; 1.12 [1.35], median [IQR], $n = 1,163$ in Mismatch OUT task

¹³1.08 [1.07], median [IQR], $n = 1,149$ in Match IN task; 0.90 [1.12], median [IQR], $n = 1,088$ in Mismatch OUT task

¹⁴1.32 [1.24], median [IQR], $n = 935$ in Match IN task; 1.15 [1.26], median [IQR], $n = 891$ in Mismatch OUT task

than $\|\text{pre-rSWR}^+\|$ in both the Match IN and Mismatch OUT tasks.¹⁵.

3.6. Visualization of hippocampal neural trajectory during SWR in two-dimensional spaces

~~Having observed neural trajectory Observing~~ 'jumping' ~~of the neural trajectory~~ during SWR (Figure 5), we visualized ~~the~~ three-dimensional trajectories of pre-, mid-, and post-SWR events during the encoding and retrieval phases (Figure 6). The distance between these was found to be memory-load dependent (Figure 3). ~~To provide~~

~~To provide a~~ two-dimensional visualization, we linearly aligned peri-SWR trajectories by setting \vec{g}_E at the origin (0, 0) and \vec{g}_R at ($\|\vec{g}_{ER}\|$, 0). ~~Subsequently, we We then~~ rotated these aligned trajectories around the \vec{g}_{ER} axis (the x axis), ensuring ~~that the the~~ ~~preservation of~~ distances from the origin in ~~the~~ original three-dimensional spaces and angles from \vec{g}_{ER} ~~are retained in the in~~ two-dimensional equivalent. ~~Scatter plot visualization of neural trajectories within these correlates.~~

In two-dimensional spaces, ~~scatter plot visualization~~ revealed distinct distributions of peri-SWR trajectories based on phases and task types. ~~A notable example of this is the observation that For instance,~~ the magnitude of $\|\text{mid-eSWR}^+\|$ ~~exceeds that of exceeded~~ $\|\text{pre-eSWR}^+\|$ (Figure 6B), ~~which is as~~ consistent with our previous ~~observations findings~~ (Figure 5).

3.7. Fluctuations of hippocampal neural trajectories between encoding and retrieval states

~~Subsequently Next,~~ we investigated the 'direction' of the trajectory in relation to \vec{g}_{ER} , ~~which was~~ found to be dependent on memory load (Figure 3). ~~The We~~ ~~defined the~~ directions of the SWRs ~~were determined~~ by the neural trajectory at -250 ms and +250 ms from their center, ~~denoted labeled~~ as, for example, eSWR^+ . We ~~calculated computed~~ the cosine similarities between \vec{g}_{ER} , eSWR^+ , and rSWR^+ ~~in during~~ both SWR (SWR⁺) ~~and baseline periods (SWR⁻) (Figure 7A – D).~~ $\text{rSWR}^+ \cdot \vec{g}_{ER}$ ~~exhibited manifested~~ a biphasic distribution. By computing the difference between the distribution of $\text{rSWR}^+ \cdot \vec{g}_{ER}$ (Figure 7A & B) and that

¹⁵1.19 [0.96], median [IQR], $n = 673$ in Match IN task; 0.94 [0.88], median [IQR], $n = 664$ in Mismatch OUT task

of $\overrightarrow{rSWR^-} \cdot \overrightarrow{g_{EGR}}$ (Figure 7C & D), ~~we were able to determine it was possible to discern~~ the contributions of SWR (Figure 7E & F), ~~which~~. This analysis indicated a shift in the direction of $\overrightarrow{g_{EGR}}$ (Figure 7E & F: red rectangles). Furthermore

Moreover, $\overrightarrow{eSWR^+} \cdot \overrightarrow{rSWR^+}$ was less than $\overrightarrow{eSWR^-} \cdot \overrightarrow{rSWR^-}$ strictly in the Mismatch OUT task (Figure 7F: pink circles). ~~In other words~~ Therefore, ~~eSWR and rSWR pointed in the opposite direction opposite directions~~ exclusively in Mismatch OUT task but ~~not didn't do so in~~ Match IN task (Figure 7E: pink circles).

4. Discussion

This study ~~hypothesizes that in low-dimensional spaces during a WM posits that during a working memory (WM)~~ task in humans, hippocampal neurons form ~~unique trajectories, primarily during SWR distinct trajectories in low-dimensional spaces, particularly during sharp-wave ripples (SWR) periods.~~ Initially, multiunit spikes in the ~~MTL—medial temporal lobe (MTL)~~ regions were projected onto three-dimensional spaces during a Sternberg task, using Gaussian-process factor analysis (GPFA) (Figure 1D–E & Figure 2A). The ~~trajectory—distances—distances of the trajectories~~ across WM phases ($\|g_{FGE}\|$, $\|g_{FGM}\|$, $\|g_{FGR}\|$, $\|g_{EGM}\|$, $\|g_{EGR}\|$, and $\|g_{MGR}\|$) were significantly larger in the hippocampus ~~compared to the EC than in the entorhinal cortex (EC)~~ and amygdala (Figure 2E), indicating dynamic ~~and responsive~~ neural activity in the hippocampus during the WM task. ~~Also, in—In addition,~~ within the hippocampus, the ~~trajectory distance—distance of the trajectory~~ between the encoding and retrieval phases ($\|g_{FGE}\|$) ~~correlated positively showed a positive correlation~~ with memory load (Figure 3C–D), ~~reflecting which reflects~~ WM processing. The hippocampal neural trajectory ~~transiently expanded during SWRs briefly expanded during SWR events~~ (Figure 5) ~~—Lastly, the hippocampal neural trajectory—and~~ alternated between encoding and retrieval states, transitioning from ~~encoding—to retrieval—the encoding to the retrieval state~~ during SWR events (Figure 7). These findings ~~explain aspects of—provide insights into~~ hippocampal neural activity during a WM task in humans and ~~offer new insights into SWRs as a state-switching element propose SWRs as crucial to the shift~~ in hippocampal neural states.

The ~~distance of the neural trajectory across the phases was significantly trajectory distance across phases was~~ substantially longer in the hippocampus ~~compared to than in~~ the EC and amygdala, even ~~when considering the distance—considering distances~~ from O in these regions (Figure 2C–E). This ~~establishes the involvement reinforces the role~~ of the hippocampus in the WM task; ~~corroborating previous studies indicating hippocampal persistent—consistent with earlier studies showing persistent hippocampal~~ firing during the task's maintenance phase [3] [4] [5] [6]. ~~However, in the present study, applying—Applying~~ GPFA to multiunit activity ~~during a—at one-second level resolution of resolution during~~ the WM task ~~revealed, this study found~~ that the neural trajectory in low-dimensional space ~~presented—exhibited~~ a memory-load dependency between the encoding and retrieval phases, ~~denoted represented~~ as $\|g_{EGR}\|$ (Figure 3). These ~~findings support the association of the hippocampus results support the hippocampus's association~~ with WM processing.

Our analysis ~~focused on—targeted~~ putative CA1 regions (Figure 4), ~~is a decision~~ supported by several factors. This specific focus ~~results from established stems from existing~~ observations that SWRs synchronize with interneuron and ~~pyramidal—pyramid~~ neuron spike bursts [44] [45] [46] [47], potentially within a 50 μm radius of the recording site [48]. ~~Furthermore, we identified an increased—Moreover, an elevated~~ incidence of SWRs ~~was identified~~ during the first 0–400 ms of the retrieval phase (Figure 4D). ~~This finding aligns, aligning~~ with previous reports of ~~heightened SWR occurrence preceding—increased SWR occurrence before~~ spontaneous verbal recall [21] [22], ~~supporting which supports~~ our results under a triggered retrieval condition. The observed log-normal distributions of both SWR duration and ripple band peak amplitude ~~in this study~~ (Figure 4C & E) ~~coincide—agree~~ with the current consensus in this field [39]. ~~Consequently, our decision to limit scientific domain [39]. Therefore, restricting~~ recording sites to putative CA1 regions likely ~~contributed to improving improved~~ the precision, or true positive rate, of SWR detection. ~~Although—However,~~ the trajectory distance increase from O during SWRs (Figure 5) ~~might—may~~ be artificially inflated towards higher values due to channel selection, ~~this~~. This potential bias does not ~~substantially challenge our main findings significantly affect our main~~

conclusions.

Interestingly, ~~during the retrieval phase, trajectory directions alternated the trajectory directions oscillated~~ between encoding and retrieval states during both baseline and SWR periods in a task-dependent manner ~~during the retrieval phase~~ (Figure 7C & D). ~~Additionally~~In addition, the balance of this fluctuation transitioned from ~~encoding to the encoding to the~~ retrieval state during SWR events (Figure 7E & F). These results align with ~~previous studies on the role of SWR~~earlier studies on SWR's role in memory retrieval [21] [22]. Our findings suggest that: (i) neuronal oscillation between encoding and retrieval states occurs during a WM task, and (ii) SWR events ~~serve as indicators of the transition in hippocampal neural states indicate the transition~~ from encoding to retrieval ~~states~~ during a WM task.

~~Moreover~~Furthermore, our study ~~noted differences specific to the observed WM-task type between encoding—type-specific differences between encoding-SWRs (eSWR) and retrieval-SWRs (rSWR)~~ (Figure 7E–F). Notably, opposing movements of ~~encoding-SWR (eSWR) and retrieval-SWR (rSWR)~~eSWR and rSWR were not observed in ~~the~~ Match IN task but were apparent in ~~the~~ Mismatch OUT task. ~~Memory—This observation could be attributed to memory engram theory [49] might explain these observations: Match In task presented. The Match IN task presented the~~ participants with previously shown letters, while ~~the~~ Mismatch OUT task introduced a new letter ~~absent that was not present~~ in the encoding phase. This ~~explanation underscores the significant suggests the essential~~ role of SWR in human cognitive processes.

In conclusion, this study ~~illustrates shows~~ that during a WM task in humans, hippocampal activity ~~fluctuate transitions~~ between encoding and retrieval states, ~~uniquely transitioning specifically shifting~~ from encoding to retrieval during SWR events. These findings offer novel insights into the neural correlates and functionality of working memory within the hippocampus.

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Contributors

Y.W. and T.Y. conceptualized the study; Y.W. performed the data analysis; Y.W. and T.Y. wrote the original draft; and all authors reviewed the final manuscript.

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Declaration of Interests

The authors declare that they have no competing interests.

Data and code availability

The data is available on G-Node (<https://doi.gin.g-node.org/10.12751/g-node.d76994/>).
The source code is available on GitHub (<https://github.com/yanagisawa-lab/hippocampal-neural-fluctuation-during-a-WM-task-in-humans>).

Inclusion and Diversity Statement

We support inclusive, diverse, and equitable conduct of research.

Declaration of Generative AI in Scientific Writing

The authors employed ChatGPT, provided by OpenAI, for enhancing the manuscript's English language quality. After incorporating the suggested improvements, the authors meticulously revised the content. Ultimate responsibility for the final content of this publication rests entirely with the authors.

Tables

Subject ID	# of sessions	AHL	AHR	PHL	PHR	ECL	ECR	AL	AR	SOZ
1	4	✓	n.a.	✓	✓	✓	n.a.	✓	n.a.	AHR & LR
2	7	✓	✓	✓	✓	✓	✓	✓	✓	AHR & PHR
3	3	✓	✓	✓	✓	✓	✓	✓	n.a.	AHL & PHL
4	2	✓	✓	✓	✓	✓	✓	✓	✓	AHL & AHR & PHL & PHR
5	3	✓	n.a.	n.a.	✓	n.a.	n.a.	✓	n.a.	DRR
6	6	✓	✓	✓	✓	✓	✓	✓	✓	AHL & PHL & ECL & AL
7	4	✓	✓	✓	✓	✓	✓	✓	✓	AHR & PHR
8	5	✓	✓	✓	✓	✓	✓	✓	✓	ECR
9	2	✓	✓	✓	✓	✓	✓	✓	✓	ECR & AR

Table 1 – Electrode Distribution within the Dataset

This figure denotes the placements of electrodes and seizure onset zones. Regions marked with ✓ were included in the dataset, while those imprinted with n.a. were absent. The abbreviations used are as follows: AHL, left hippocampal head; AHR, right hippocampal head; PHL, left hippocampal body; PHR, right hippocampal body; ECL, left entorhinal cortex; ECR, right entorhinal cortex; AL, left amygdala; AR, right amygdala; SOZ represents the seizure onset zone.

Subject	AHL	AHR	PHL	PHR
1	0.60 ± 0.14	n.a.	n.a.	0.1 ± 0
2	0.21 ± 0.16	0.17 ± 0.21	0.18 ± 0.22	0.20 ± 0.15
3	0.40 ± 0.42	0.83 ± 0.12	n.a.	n.a.
4	0.10 ± 0.00	0.10 ± 0.00	0.90 ± 0.00	0.10 ± 0.14
5	n.a.	n.a.	n.a.	n.a.
6	0.63 ± 0.06	n.a.	n.a.	0.27 ± 0.06
7	0.10 ± 0.00	0.35 ± 0.35	0.37 ± 0.47	0.10 ± 0.00
8	0.13 ± 0.10	n.a.	0.28 ± 0.49	n.a.
9	n.a.	0.85 ± 0.07	0.15 ± 0.07	n.a.

Table 2 – Silhouette score of UMAP clustering for SWR⁺ candidates and SWR⁻ candidates

The silhouette scores (mean ±SD across sessions per subject) for UMAP clustering of SWR⁺ candidates and SWR⁻ candidates are based on their respective multiunit spike patterns (Figure 4A). The mean scores were 0.205 and the standard deviation was 0.285, calculated for the interquartile range (IQR; Figure 4B).

Subject ID	# of sessions	# of trials	ROI	# of SWRs	SWR incidence [Hz]
#1	2	100	AHL	274	0.34
#3	2	97	AHR	325	0.42
#4	2	99	PHL	202	0.26
#6	2	100	AHL	297	0.37
#9	2	97	AHR	72	0.09
Total = 10		Total = 493		Total = 1170	0.30 ± 0.13 (mean ± SD)

Table 3 – Summary of Detected SWR Events

The table provides statistics of presumptive CA1 regions and SWR events. Only the initial two sessions (sessions 1 and 2) from each subject were included in our analysis to reduce sampling bias.

Figures

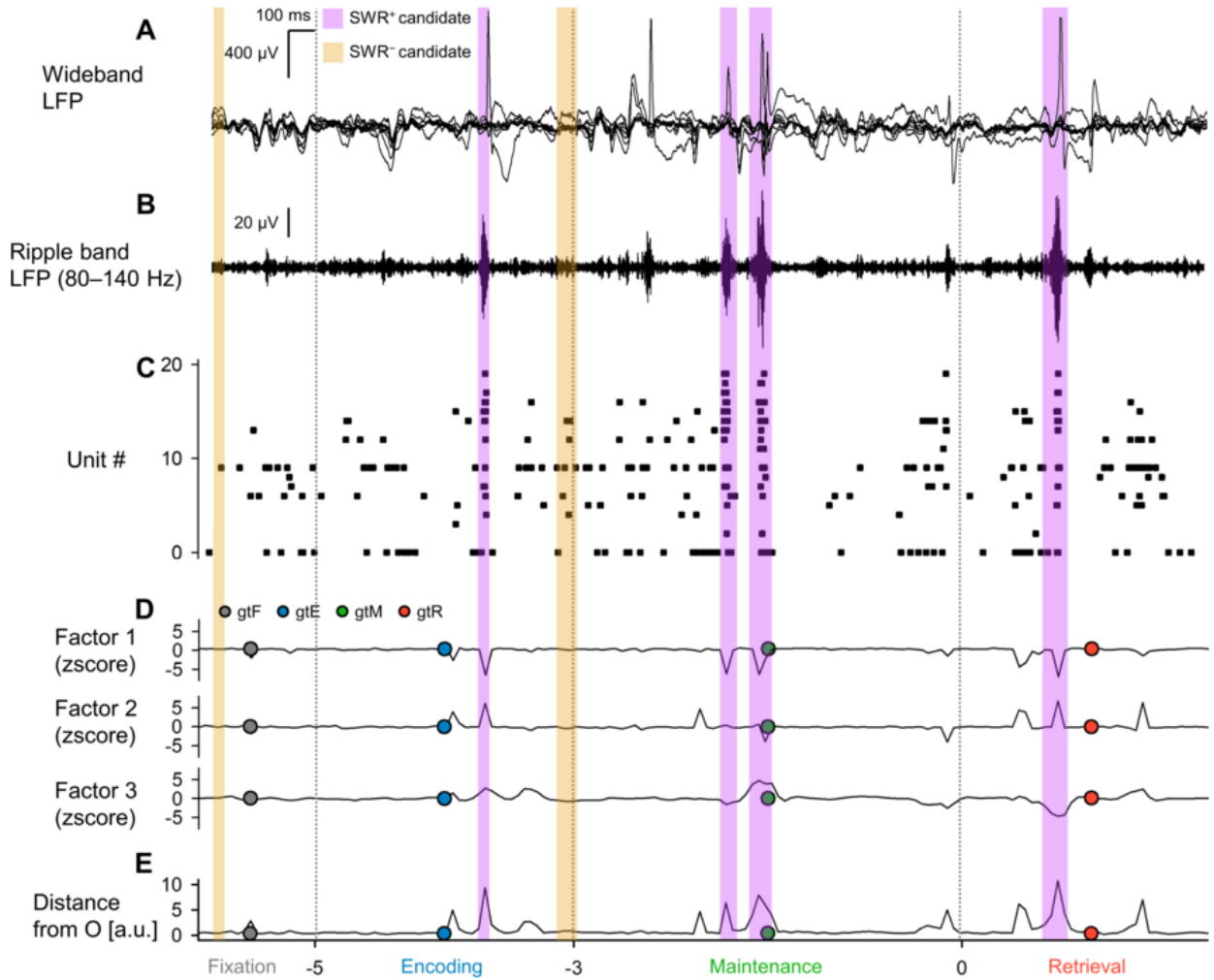


Figure 1 – Local Field Potentials (LFP), Multiunit Activity, and Neural Trajectories in the Hippocampus During a Modified Sternberg Task

A. Representative wideband LFP signals for intracranial EEG recording from the left hippocampal head are presented. This recording took place while the subject performed a modified Sternberg working memory task. Task stages included fixation (1 s, gray), encoding (2 s, blue), maintenance (3 s, green), and retrieval (2 s, red). **B.** Displays the associated ripple band LFP traces. Note purple and yellow rectangles, which denote the timings for SWR⁺ candidates and SWR⁻ candidates, respectively (the latter serving as control events for SWR⁺). **C.** A raster plot illustrates multiunit spikes from the LFP traces. These spikes have been sorted using a spike algorithm [38]. **D.** Shows neural trajectories computed by GPFA[37] based on spike counts per unit with 50-ms bins. The geometric median of each phase is marked by dot circles. **E.** Indicates the distance of the neural trajectory from the origin point *O*.

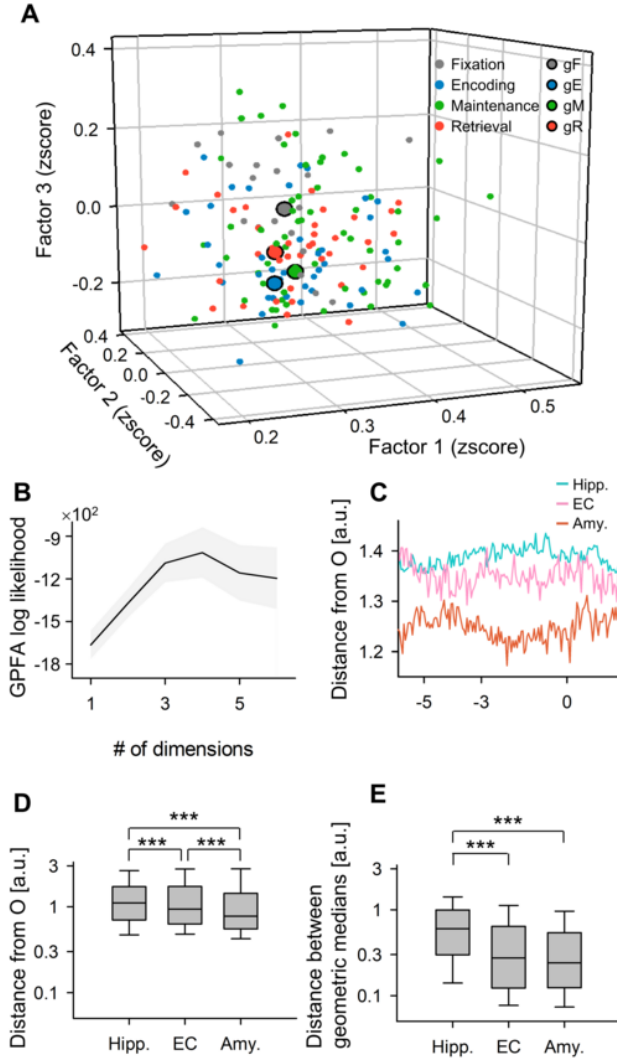


Figure 2 – State-Dependent Trajectories of Hippocampal Neurons

A. Neural trajectories are depicted as a point cloud within the first three-dimensional factors derived from GPFA [37]. The smaller dots represent 50-ms neural trajectory bins, and the larger dots with *black* edges denote the geometric medians for each phase in the Sternberg working memory task: fixation ($\|g_F\|$, *gray*), encoding ($\|g_E\|$, *blue*), maintenance ($\|g_M\|$, *green*), and retrieval ($\|g_R\|$, *red*). **B.** The figure presents the log-likelihood of the GPFA models versus the number of dimensions used to embed multiunit spikes found in the medial temporal lobe (MTL) regions. Specifically, the elbow method identified three as the optimal dimension. **C.** This panel displays the distance of the neural trajectories from the origin (O) for the hippocampus (Hipp.), entorhinal cortex (EC), and amygdala (Amy.), plotted against the time elapsed from the probe onset. **D.** The trajectory distance from O within the MTL regions is shown. The hippocampus has the greatest distance, followed by the EC and the Amygdala. **E.** The box plot illustrates inter-phase trajectory distances within the MTL regions.

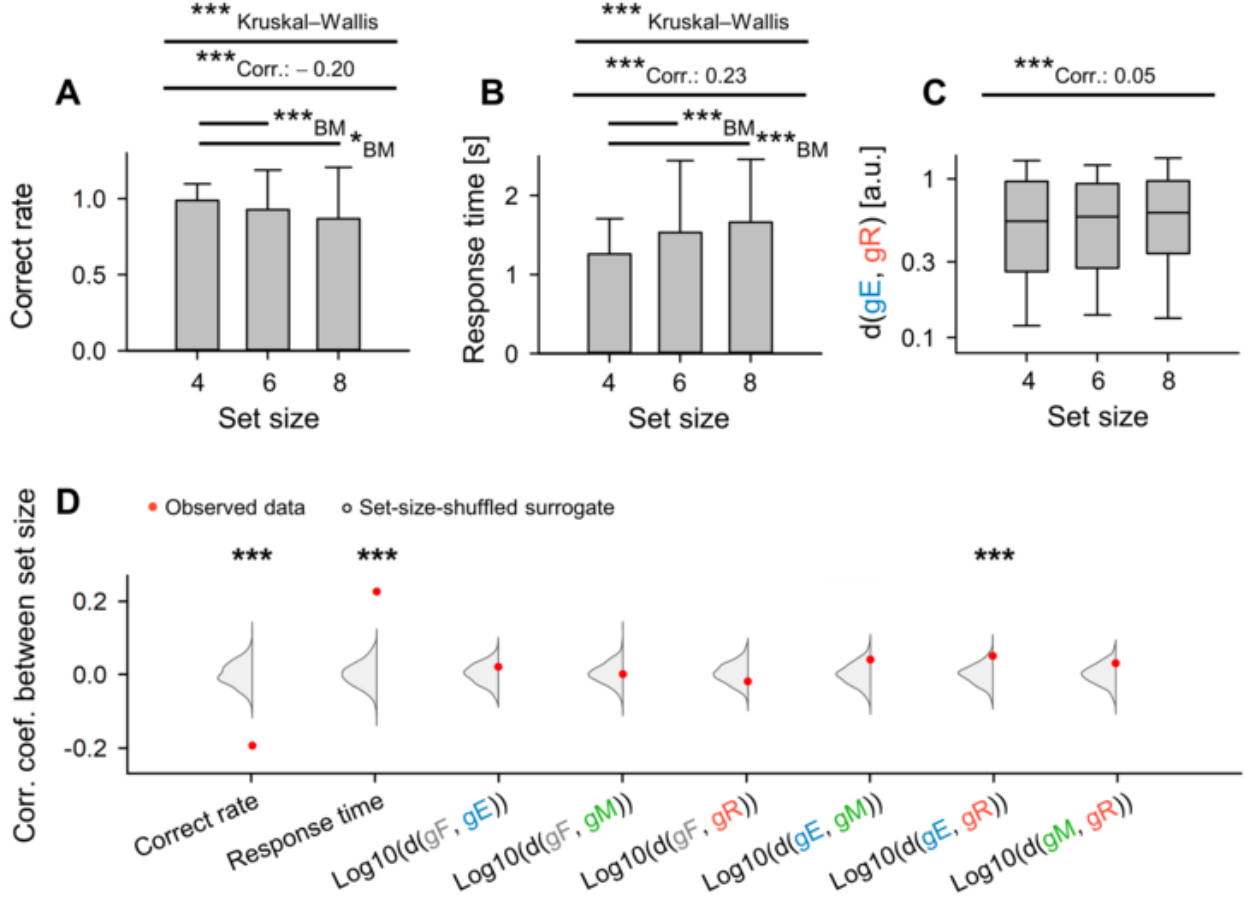


Figure 3 – Relationship between Trajectory Distance and Memory Load: States of Encoding and Retrieval in the Hippocampus

A. Demonstrates the relationship between set size (number of letters to be encoded) and accuracy in the working memory task (coefficient = -0.20 , $***p < 0.001$). **B.** Displays the correlation between set size and response time (coefficient = 0.23 , $***p < 0.001$). **C.** Exhibits the influence of set size on the inter-phase distances between the encoding and retrieval phases ($\|g_E g_R\|$) (correlation coefficient = 0.05 , $***p < 0.001$). **D.** Indicates experimental observations of correlations between set size and the following parameters: accuracy, response time, $\log_{10} \|g_F g_E\|$, $\log_{10} \|g_F g_M\|$, $\log_{10} \|g_F g_R\|$, $\log_{10} \|g_E g_M\|$, $\log_{10} \|g_E g_R\|$, and $\log_{10} \|g_M g_R\|$ represented by *red* dots. The *gray* kernel density plots illustrate the corresponding shuffled surrogate with set size ($n = 1,000$) ($***ps < 0.001$).

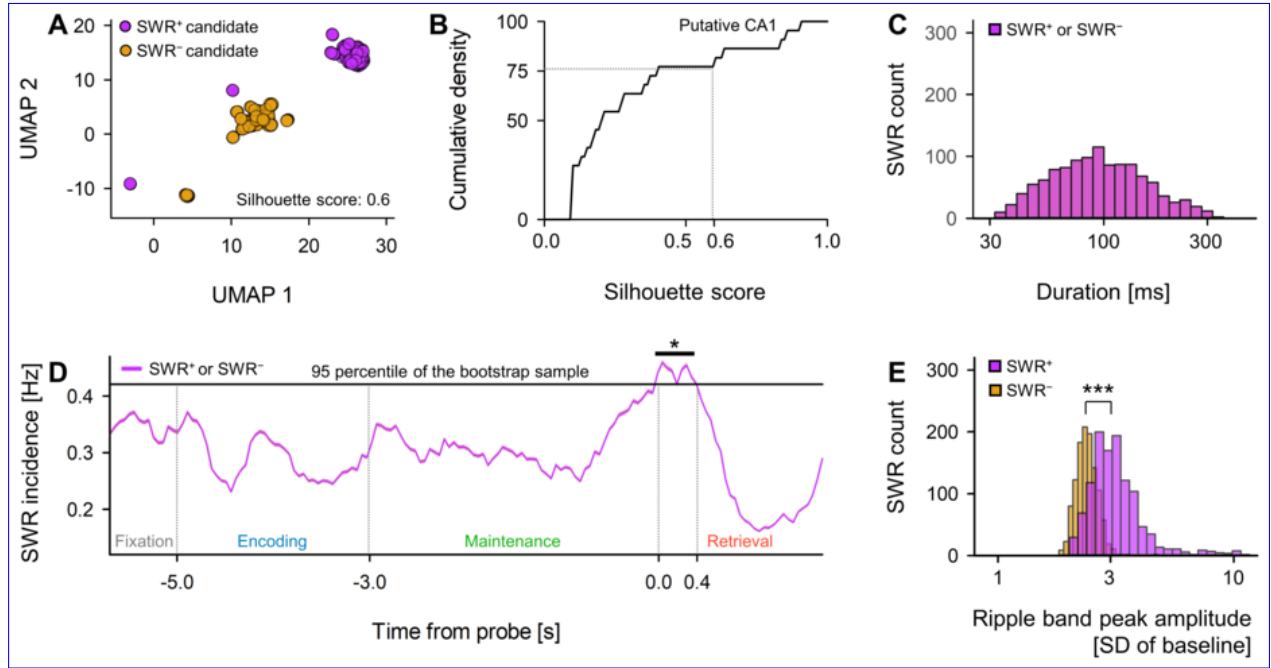
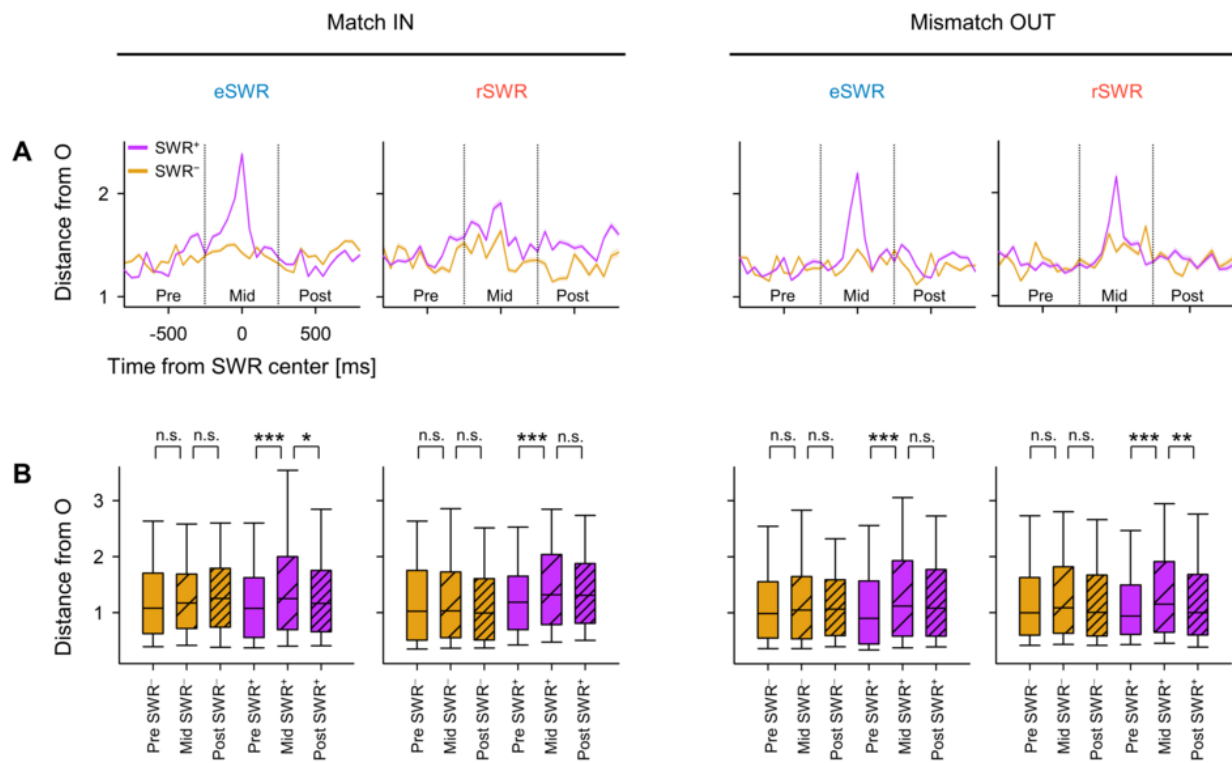


Figure 4 – Detection of SWRs in Presumptive CA1 Regions Detection of SWRs in Putative CA1 Regions

A. Two-dimensional UMAP [41] projection displays multi-unit spikes during SWR⁺ candidates (*purple*) and SWR⁻ candidates (*yellow*). **B.** A cumulative density plot indicates silhouette scores, reflecting UMAP clustering quality (see Table 2). Hippocampal regions with silhouette scores exceeding 0.60 (equivalent to the 75th percentile) are identified as putative CA1 regions. SWR⁺ and SWR⁻ candidates, which were recorded from these regions, are classified as SWR⁺ and SWR⁻ respectively ($n = 1,170$). **C.** Identical distributions of durations are presented for SWR⁺ (*purple*) and SWR⁻ (*yellow*), based on their definitions (93.0 [65.4] ms, median [IQR]). **D.** SWR incidence for both SWR⁺ (*purple*) and SWR⁻ (*yellow*), relative to the probe's timing, is illustrated as a mean \pm 95% confidence interval. However, intervals may not be visibly apparent due to their confined ranges, be aware that a significant SWR incidence increase was detected during the initial 400 ms of the retrieval phase (0.421 [Hz], $*p < 0.05$, bootstrap test). **E.** Distributions of ripple band peak amplitudes for SWR⁻ (*yellow*; 2.37 [0.33] SD of baseline, median [IQR]) and SWR⁺ (*purple*; 3.05 [0.85] SD of baseline, median [IQR]) are manifested ($***p < 0.001$, the Brunner–Munzel test).



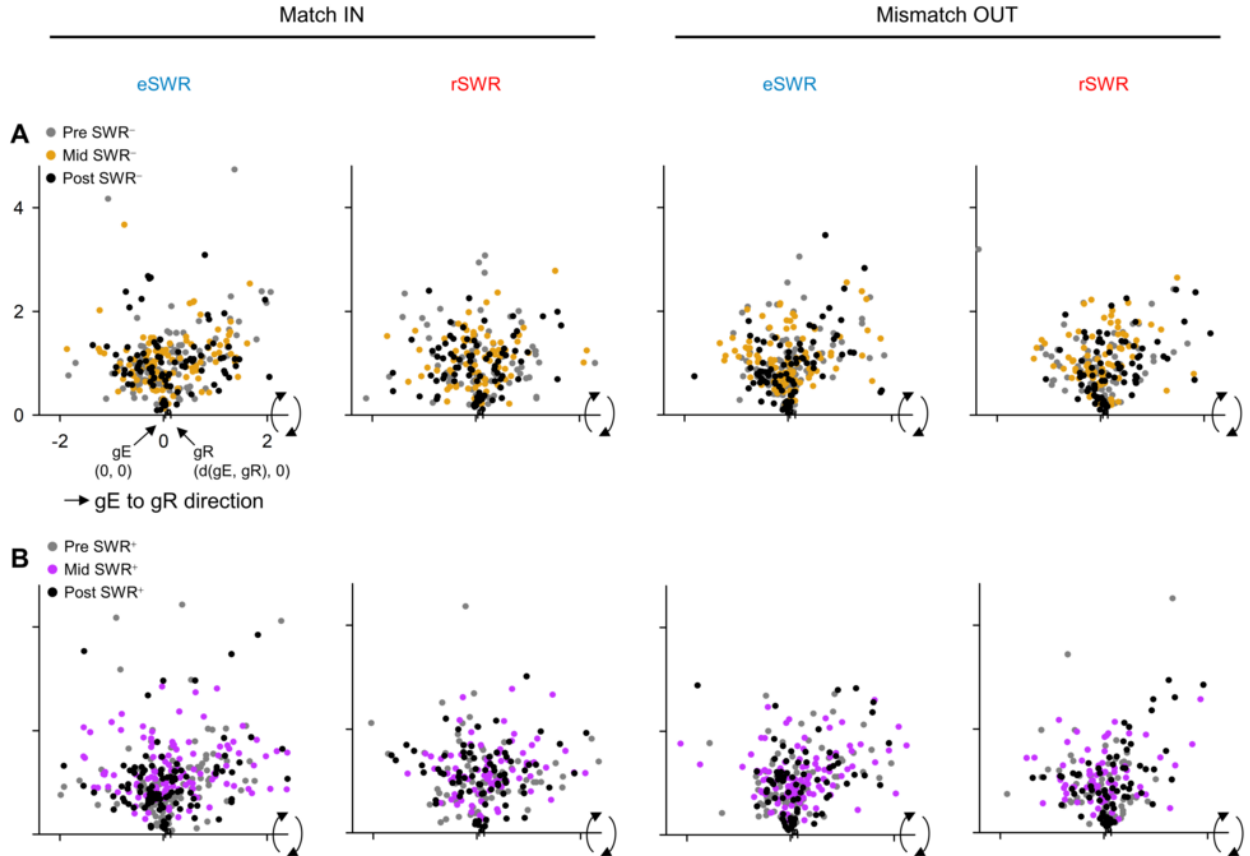


Figure 6 – Visualization of Neural Trajectories during SWR in Two-Dimensional Spaces

The panels depict hippocampal neural trajectories during SWR projected onto two-dimensional spaces. **A.** Shows the hippocampal neural trajectories as point clouds during pre-SWR⁻ (gray), mid-SWR⁻ (yellow), and post-SWR⁻ (black). **B.** Conveys the equivalent for SWR⁺ rather than SWR⁻. The projection was executed as follows: First, a linear transformation placed g_E at the origin $O(0,0)$, and g_R at $(\|g_E g_R\|, 0)$. The point cloud was subsequently rotated around the $g_E g_R$ axis (similar to the x axis) for adaptation to two-dimensional spaces. Thus, within these two-dimensional spaces, the distances from point O and the angles for the $g_E g_R$ axis are retained as in the original three-dimensional spaces created by GPFA. Abbreviations: SWR denotes sharp-wave ripple events; eSWR refers to SWR during the encoding phase; rSWR signals SWR during the retrieval phase; SWR⁺, characterizes an SWR event; SWR⁻ signifies control events for SWR⁺; pre-SWR, mid-SWR, or post-SWR, represent the time intervals from -800 to -250 ms, from -250 to +250 ms, or from +250 to +800 ms from the center of the SWR.

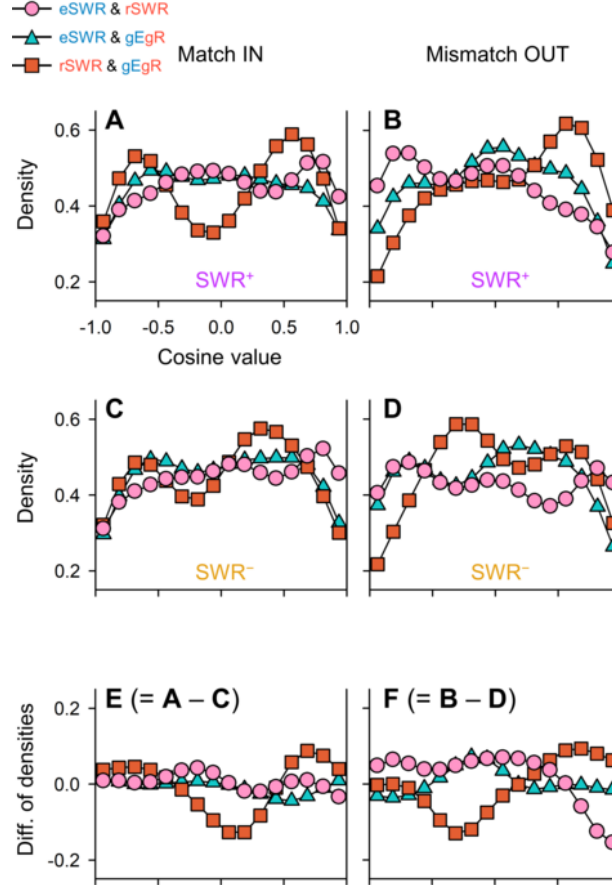


Figure 7 – Neural Trajectories Direction during SWRs Based on Encoding and Retrieval States

A–B Shows the kernel density estimation distributions of $\overrightarrow{eSWR^+} \cdot \overrightarrow{rSWR^+}$ (depicted as pink circles), $\overrightarrow{eSWR^+} \cdot \overrightarrow{gEgR}$ (blue triangles), and $\overrightarrow{rSWR^+} \cdot \overrightarrow{gEgR}$ (red rectangles) in the Match In (A) and Mismatch OUT tasks (B). **C–D** Illustrates the corresponding distributions of SWR^- instead of those of SWR^+ in A and B. **E–F** Renders the differences in the distributions of SWR^+ and SWR^- , detailing the SWR components ($E = C - A$, $F = D - B$). The biphasic distributions of $\overrightarrow{rSWR^+} \cdot \overrightarrow{gEgR}$ indicates fluctuations between the encoding and retrieval states during the Sternberg task. Also, contradicting directionality between $\overrightarrow{eSWR^+}$ and $\overrightarrow{rSWR^+}$ was observed (pink circles) not in the Match IN task (E), but in Mismatch OUT task (F). Lastly, transition from the retrieval to encoding states are apparent in the SWR components in both Match IN and Mismatch OUT tasks (red rectangles in E–F).