

Highlights

- Neural trajectories in the hippocampus exhibited greater variability during a working memory (WM) task compared to those in the entorhinal cortex and amygdala regions.
- The distance of neural trajectories between encoding and retrieval states in the hippocampus was memory-load dependent during a WM task.
- Hippocampal neural trajectories fluctuated between the encoding and retrieval states in a task-dependent manner during both baseline and sharp-wave ripple (SWR) periods.
- Hippocampal neural trajectories shifted from encoding to retrieval states during SWR period.

Hippocampal neural fluctuations between memory encoding and retrieval states during a working memory task in humans

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Abstract

Working memory (WM) ~~is integral to numerous cognitive functions, but the complex neural mechanisms essential for its operation are not entirely~~ serves as a critical cornerstone in a multitude of cognitive functions; yet, the elaborate neural mechanisms underpinning its functionality remain incompletely understood. Specifically, ~~the roles of while both~~ the hippocampus and sharp-wave ripple complexes (SWRs) ~~—rapid, synchronised neural events—~~ rapid, coordinated neural occurrences within the hippocampus ~~—are recognized to support—~~ are recognized for their roles in memory consolidation and retrieval. ~~However, their contributions to WM tasks remain somewhat unclear. We suggest that the coordinated activity patterns in the hippocampus collaborate, their involvement in WM tasks persists as somewhat equivocal. Our present research theorizes that the multiunit activity patterns within the hippocampus work synergistically with SWRs, displaying unique dynamics thereby demonstrating distinctive dynamism during WM tasks. Our investigation involved a comprehensive an in-depth analysis of a dataset acquired derived from intracranial electroencephalogram recordings acquired from the medial temporal lobe (MTL) of nine epileptic patients during individuals with epilepsy performing an eight-second Sternberg task. We use employed Gaussian-process factor analysis to identify discern low-dimensional neural representations, or 'trajectories,' within the MTL regions territories during the WM task. We discovered Our findings revealed that the neural trajectory showed exhibited the most significant variations in the hippocampus when compared to the entorhinal cortex and amygdala. Furthermore, we noticed that the discrepancy in trajectories Moreover, divergence in the trajectories identified between encoding and retrieval phases was dependent on memory load. Interestingly were memory load-dependent. Importantly, hippocampal trajectories oscillated during the retrieval phase, revealing displaying task-dependent shifts transitions between encoding and retrieval states, including inclusive of baseline and SWR phases episodes. These oscillations transitioned shifted from encoding to retrieval states congruent with the occurrence of SWRs. These in accordance with SWRs. Hence, these results highlight the substantial critical role of the hippocampus during WM tasks execution in performing WM tasks and propose a persuasive hypothesis for further examination: the hippocampus undergoes a functional transition subsequent investigation: the functional state of the hippocampus transitions from encoding to retrieval during SWRs.~~

Keywords: working memory, WM, memory load, hippocampus, sharp-wave ripples, SWR, humans

Working memory (WM) plays a crucial role in everyday life, and its neural underpinnings remain an area of ongoing research. The hippocampus, notably inte-

gral to memory, continues to be a primary focus of this investigation [1] [2] [3] [4] [5] [6] [7] [8] [9]. Gaining insights into the role of the hippocampus in working memory is vital to deepening our understanding of cognitive processes, hence fostering the progression of

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cognitive training and interventions.

Current evidence suggests a transient, synchronized oscillation, referred to as sharp-wave ripple (SWR) [10], is linked with several cognitive functions, such as memory replay [11] [12] [13] [14] [15], memory consolidation [16] [17] [18] [19], memory recall [20] [21] [22], and neural plasticity [23] [24]. This evidence indicates the likelihood that SWR could be a critical component of hippocampal processing, contributing to working memory performance. However, research investigating the effects of SWRs on working memory remains sparse [25], and is largely limited to rodent models participating in navigation tasks where the timing of memory acquisition and recall is not explicitly distinguished.

Recent studies indicate that hippocampal neurons exhibit low-dimensional representations during WM tasks. Notably, the firing patterns of place cells [26] [27] [28] [29] [30], located in the hippocampus, are observed to be encompassed within a dynamic, nonlinear three-dimensional hyperbolic geometry in rodents [31]. Moreover, grid cells in the entorhinal cortex (EC)—the dominant pathway to the hippocampus [32] [33] [34]—displayed toroidal topology during exploration [35]. Unfortunately, these investigations are confined to spatial navigation tasks in rodents, thus imposing limitations on the temporal resolution of WM tasks. The applicability of these findings to human subjects and their generalization beyond navigation tasks remains to be established.

Given these considerations, the current study aims to validate the hypothesis that hippocampal neurons exhibit distinctive representations in low-dimensional spaces, designated as ‘neural trajectory,’ during WM tasks, most prominently within SWR periods. To evaluate this claim, we employed a dataset of patients performing an eight-second Sternberg task with high temporal resolution (1 s for fixation, 2 s for encoding, 3 s for maintenance, and 2 s for retrieval), while their intracranial electroencephalography signals (iEEG) within the medial temporal lobe (MTL) were being monitored [36]. To investigate low-dimensional neural trajectories, we employed Gaussian-process factor analysis (GPFA), a method renowned for analyzing neural population dynamics [37].

1. Methods

1.1. Dataset

A publicly available dataset [36] was used, which consists of nine epilepsy patients performing a modified Sternberg task. This task involves four phases: fixation (1s), encoding (2s), maintenance (3s), and retrieval (2s) [36]. During the encoding phase, participants were exposed to four, six, or eight alphabet letters, referred to as the set size. Subsequently, they had to decide whether a probe letter presented during the retrieval phase was previously displayed (the correct choice for the Match IN task) or not (the correct choice for the Mismatch OUT task). iEEG signals were recorded at a sampling rate of 32 kHz, within a frequency range of 0.5–5,000 Hz, using depth electrodes implanted in the medial temporal lobe (MTL) regions: the anterior head of the left and the right hippocampus (AHL and AHR), the posterior body of the hippocampus (PHL and PHR), the entorhinal cortex (ECL and ECR), and the amygdala (AL and AR), as illustrated in Figure 4A and Table 1. The iEEG signals were subsequently downsampled to a rate of 2 kHz. Correlations among variables such as set size and correct rate were investigated (Figure ??S1). The timings of multiunit spikes were determined by a spike sorting algorithm [38] using the Combinato package (<https://github.com/jniediek/combinato>) (Figure 4C).

1.2. Calculation of neural trajectories using GPFA

Neural trajectories, also termed ‘factors’ (Figure 4D), in the hippocampus, EC, and amygdala (Figure 4D), were computed using GPFA [37] applied to the multiunit activity data for each session. GPFA was performed with the elephant package (<https://elephant.readthedocs.io/en/latest/reference/gpfa.html>). The bin size was set to 50 ms, with no overlaps. Each factor was z-normalized across all sessions. The Euclidean distance from the origin (O) was then calculated (Figure 4E).

For each trajectory within a region, for instance, AHL, *geometric medians* (i.e., g_F for fixation, g_E for encoding, g_M for maintenance, and g_R for retrieval phase) were determined by calculating the median coordinates of the trajectory during the four phases (Figure 4D). An optimal dimensionality for GPFA was identified as three

using the elbow method, which was derived by investigating the log-likelihood values through a three-fold cross-validation approach (Figure 2B).

1.3. Identifying SWR candidates from hippocampal regions

Potential SWR events within the hippocampus were detected using a widely accepted method [39]. LFP signals from a region of interest (ROI), such as AHL, were re-referenced by subtracting an averaged signal from locations outside the ROI (*e.g.*, AHR, PHL, PHR, ECL, ECR, AL, and AR) (see Figure 4A). The re-referenced LFP signals were then filtered with a ripple-band filter (80–140 Hz) to identify SWR candidates (=SWR⁺ candidates) (see Figure 4B). SWR detection was conducted using a published tool (https://github.com/Eden-Kramer-Lab/ripple_detection) [40], with the bandpass range adjusted to 80–140 Hz for humans [21] [22], different from the original 150–250 Hz range typically applied to rodents.

Control events for SWR⁺ candidates, labeled as SWR⁻ candidates, were identified by randomly shuffling the timestamps of SWR⁺ candidates across all trials and subjects. The resulting SWR⁺/SWR⁻ candidates were then subjected to visual inspection, as shown in Figure 4.

1.4. Defining SWRs from putative hippocampal CA1 regions

SWRs were distinguished from SWR candidates in presumptive CA1 regions. Initially, these regions were defined as follows: SWR⁺/SWR⁻ candidates in the hippocampus were projected into a two-dimensional space based on overlapping spike counts per unit employing a supervised method using UMAP (Uniform Manifold Approximation and Projection) [41] (Figure 4A). Clustering validation was performed by computing the silhouette score [42] from clustered samples (Table 2). Regions in the hippocampus, which scored above 0.6 on average across sessions (75th percentile) (Figure 4B), were characterized as presumed CA1 regions, identifying five electrode positions from five patients (Table 3).

SWR⁺/SWR⁻ candidates in the assumed CA1 regions were classified as SWR⁺/SWR⁻, thus relinquishing their candidate status. The duration and ripple band

peak amplitude of SWRs were observed to follow log-normal distributions (Figure 4C & E). Each time period of SWR was partitioned relative to the time from the SWR center into pre- (at -800 to -300 ms from SWR center), mid- (at -250 to +250 ms), and post-SWR (at +300 to +800 ms) times.

1.5. Statistical evaluation

The Brunner–Munzel test and the Kruskal–Wallis test were performed using the SciPy package in Python [43]. Correlational analysis was performed by determining the rank of the observed correlation coefficient in its associated set-size-shuffled surrogate using a custom Python script. The bootstrap test was implemented using an in-house Python script.

2. Results

2.1. iEEG recording and neural trajectory in MTL regions during a Sternberg task

We leveraged a publicly available dataset for this analysis [36]. This dataset encompasses LFP signals (Figure 1A) from MTL regions (Table 1) during a modified Sternberg task execution. We identified SWR⁺ candidates from LFP signals filtered through the 80–140 Hz ripple band (Figure 1B), originating across all hippocampal regions (refer to Methods). Correspondingly, SWR⁻ candidates were defined at identical timestamps) but shuffled across different trials (Figure 1). The dataset included multiunit spikes (Figure 1C) identified via a spike sorting algorithm [38]. By employing GPFA [37], and using the 50-ms binned multiunit activity with no overlaps, we determined the neural trajectories (or factors) of MTL regions by session and region (Figure 1D). We normalized each factor by session and region for instance, session #2 in AHL of subject #1. Subsequently, we calculated the Euclidean distance from the origin (*O*) (Figure 1E).

2.2. Hippocampal neural trajectory correlation with a Sternberg task

Figure 2A illustrates the cloud of median neural trajectories of 50 trials within the three main factor spaces. We determined the optimal embedding dimension for the GPFA model to be three, using the elbow method (Figure 2B). The trajectory distance from the origin (*O*)

(represented as $\|g_F\|$, $\|g_E\|$, $\|g_M\|$, and $\|g_R\|$) in the hippocampus exceeded corresponding distances in the EC and amygdala (Figures 2C and D).¹

Similarly, we computed the distances between the geometric medians of four phases, namely $\|g_{FGE}\|$, $\|g_{FGM}\|$, $\|g_{FGR}\|$, $\|g_{EGM}\|$, $\|g_{EGR}\|$, and $\|g_{MGR}\|$. The results indicated that the hippocampus displayed larger distances between phases than both the EC and amygdala.²

2.3. Memory load-dependent neural trajectory distance between encoding and retrieval states in the hippocampus

In terms of memory load in the Stenberg task, we identified a negative correlation between the correct rate of trials and set size (the number of letters to encode) (Figure 3A).³ Similarly, a positive correlation was observed between the response time and set size (Figure 3B).⁴

Furthermore, we found a positive correlation between set size and the trajectory distance between the encoding and retrieval phases ($\log_{10}\|g_{EGR}\|$) (Figure 3C).⁵ However, distances between other combinations of phases did not display statistically significant correlations (Figures 3D and S2).

¹Hippocampus: Distance = 1.11 [1.01], median [IQR], $n = 195,681$ timepoints; EC: Distance = 0.94 [1.10], median [IQR], $n = 133,761$ timepoints; Amygdala: Distance = 0.78 [0.88], median [IQR], $n = 165,281$ timepoints.

²Hippocampus: Distance = 0.60 [0.70], median [IQR], $n = 8,772$ combinations; EC: Distance = 0.28 [0.52], median [IQR], $n = 5,017$ combinations ($p < 0.01$; Brunner–Munzel test); Amygdala: Distance = 0.24 [0.42], median [IQR], $n = 7,466$ combinations ($p < 0.01$; Brunner–Munzel test).

³Correct rate: set size four (0.99 ± 0.11 , mean \pm SD; $n = 333$ trials) vs. set size six (0.93 ± 0.26 ; $n = 278$ trials; $p < 0.001$, Brunner–Munzel test with Bonferroni correction) and set size eight (0.87 ± 0.34 ; $n = 275$ trials; $p < 0.05$; Brunner–Munzel test with Bonferroni correction). Overall, $p < 0.001$ for Kruskal–Wallis test; correlation coefficient = -0.20, $p < 0.001$.

⁴Response time: set size four (1.26 ± 0.45 s; $n = 333$ trials) vs. set size six (1.53 ± 0.91 s; $n = 278$ trials) and set size eight (1.66 ± 0.80 s; $n = 275$ trials). All comparisons $p < 0.001$, Brunner–Munzel test with Bonferroni correction; $p < 0.001$ for Kruskal–Wallis test; correlation coefficient = 0.22, $p < 0.001$.

⁵Correlation between set size and $\log_{10}(\|g_{EGR}\|)$: correlation coefficient = 0.05, $p < 0.001$. Specific values: $\|g_{EGR}\| = 0.54$ [0.70] for set size four, $n = 447$; $\|g_{EGR}\| = 0.58$ [0.66] for set size six, $n = 381$; $\|g_{EGR}\| = 0.61$ [0.63] for set size eight, $n = 395$.

2.4. Detection of hippocampal SWR from putative CA1 regions

For precision improvement in recording sites and SWR detection, we estimated the electrode placements in the CA1 regions of the hippocampus using distinct multiunit spike patterns during the SWR events. SWR^+ / SWR^- candidates from every session and hippocampal region were embedded in a two-dimensional space using UMAP (Figure 4A).⁶ We used the silhouette score as a metric for quality of clustering (Figure 4B and Table 2). Recording sites with an average silhouette score exceeding 0.6 across all sessions were identified as putative CA1 regions.⁷ (Tables 2 and 3). We identified five putative CA1 regions, four of which were not labeled as seizure onset zones (Table 1).

Subsequently, SWR^+ / SWR^- candidates within these putative CA1 regions were labeled as SWR^+ and SWR^- , respectively⁸ (Table 3). Both SWR^+ and SWR^- exhibited the same duration⁹ (Figure 4C) due to their definitions, and followed a log-distribution. We observed an augmentation in SWR^+ incidence during the initial 400 ms of the retrieval phase¹⁰ (Figure 4D). The peak ripple band amplitude of SWR^+ outpaced SWR^- and followed a log-normal distribution (Figure 4E).¹¹

2.5. Transient changes in hippocampal neural trajectory during SWR

We computed the distance of the trajectory from the origin (O) during SWR events in both the encoding and retrieval phases (Figure 5A). Observing the increase in distance during SWR as shown in Figure 5A, we differentiated each SWR into three stages: pre-, mid-, and post-SWR. Therefore, the distances from O during those SWR periods are identified as $\|pre-eSWR^+\|$, $\|mid-eSWR^+\|$ among others.

⁶Consider the AHL in session #1 of subject #1, for illustration purposes.

⁷The identified regions were: AHL of subject #1, AHR of subject #3, PHL of subject #4, AHL of subject #6, and AHR of subject #9.

⁸These definitions led to equal counts for both categories: SWR^+ ($n = 1,170$) and SWR^- ($n = 1,170$).

⁹These definitions led to equal durations for both categories: SWR^+ (93.0 [65.4] ms) and SWR^- (93.0 [65.4] ms).

¹⁰ SWR^+ increased against the bootstrap sample; 95th percentile = 0.42 [Hz]; $p < 0.05$.

¹¹ SWR^+ (3.05 [0.85] SD of baseline, median [IQR]; $n = 1,170$) vs. SWR^- (2.37 [0.33] SD of baseline, median [IQR]; $n = 1,170$; $p < 0.001$; Brunner–Munzel test).

$\|\text{mid-eSWR}^+\|^{12}$ was greater than $\|\text{pre-eSWR}^+\|^{13}$, and $\|\text{mid-rSWR}^+\|^{14}$ was larger than $\|\text{pre-rSWR}^+\|$ in both Match IN and Mismatch OUT tasks.¹⁵

2.6. Visualization of hippocampal neural trajectory during SWR in two-dimensional spaces

Following our observations of neural trajectory 'jumping' during SWR (Figure 5), we visualized the three-dimensional trajectories of pre-, mid-, and post-SWR events during the encoding and retrieval phases (Figure 6), the distance between which was found to be memory-load dependent (Figure 3).

To provide two-dimensional visualization, we linearly aligned peri-SWR trajectories by assigning \mathbf{g}_E at the origin (0, 0) and \mathbf{g}_R at $(\|\mathbf{g}_{EGR}\|, 0)$. Post this, we rotated these aligned trajectories around the \mathbf{g}_{EGR} axis (the x-axis). Thus, the distances from the origin in the original three-dimensional spaces are preserved in the two-dimensional equivalent.

The scatter plot within these two-dimensional spaces reveals characteristic distributions of peri-SWR trajectories based on phases and task types. For instance, one can observe that the magnitude of $\|\text{mid-eSWR}^+\|$ surpasses that of $\|\text{pre-eSWR}^+\|$ (Figure 6B), consistent with our earlier findings (Figure 5).

2.7. Fluctuations of hippocampal neural trajectories between encoding and retrieval states

Next, we examined trajectory *directions* in relation to $\overrightarrow{\mathbf{g}_{EGR}}$. The directions of SWRs were defined by the neural trajectory at -250 ms and +250 ms from their center, i.e., $\overrightarrow{\text{eSWR}^+}$.

We calculated the density of $\overrightarrow{\text{eSWR}^+} \cdot \overrightarrow{\mathbf{g}_{EGR}}$, $\overrightarrow{\text{rSWR}^-} \cdot \overrightarrow{\mathbf{g}_{EGR}}$, and $\overrightarrow{\text{eSWR}^-} \cdot \overrightarrow{\mathbf{g}_{EGR}}$ (Figures 7A–D). $\overrightarrow{\text{rSWR}^-} \cdot \overrightarrow{\mathbf{g}_{EGR}}$ displayed a biphasic distribution.

By taking the difference between the distribution of $\overrightarrow{\text{rSWR}^+} \cdot \overrightarrow{\mathbf{g}_{EGR}}$ (Figures 7A and B) and that of $\overrightarrow{\text{rSWR}^-} \cdot \overrightarrow{\mathbf{g}_{EGR}}$ (Figures 7C and D), we computed the contributions of SWR (Figures 7E and F), which revealed a shift

in the direction of $\overrightarrow{\mathbf{g}_{EGR}}$ (Figures 7E and F: *red rectangles*).

Moreover, exclusively in the Mismatch OUT task, $\overrightarrow{\text{eSWR}^+} \cdot \overrightarrow{\mathbf{g}_{EGR}}$ was less than $\overrightarrow{\text{eSWR}^-} \cdot \overrightarrow{\mathbf{g}_{EGR}}$ (baseline periods) (Figure 7F: *pink circles*). In simpler terms, eSWR and rSWR pointed in the opposite direction only in the Mismatch OUT task but not in the Match IN task (Figure 7E: *pink circles*).

3. Discussion

4. Discussion

This study hypothesized that within low-dimensional spaces during a working memory (WM) task in humans, hippocampal neurons form unique trajectories, particularly during sharp-wave ripple (SWR) periods. Initially, the multiunit spikes in medial temporal lobe (MTL) regions were projected onto three-dimensional spaces during a Sternberg task using Gaussian Process Factor Analysis (GPFA) (Figure 4D–E and Figure 2A). The distance of the trajectory across WM phases ($\|\mathbf{g}_{FGE}\|$, $\|\mathbf{g}_{FGM}\|$, $\|\mathbf{g}_{FGR}\|$, $\|\mathbf{g}_{EGM}\|$, $\|\mathbf{g}_{EGR}\|$, and $\|\mathbf{g}_{MGR}\|$) was notably larger in the hippocampus than in the EC and amygdala (Figure 2E), indicating dynamic neural activity in the hippocampus during the WM task. Further, in the hippocampus, the trajectory distance between the encoding and retrieval phases ($\|\mathbf{g}_{FGE}\|$) exhibited a positive correlation with memory load (Figure 3C–D), reflecting WM processing. The hippocampal neural trajectory was found to increase transiently during SWRs (Figure 4). Finally, the hippocampal neural trajectory switched between encoding and retrieval states, moving from encoding to retrieval during SWR events (Figure 7). These findings not only explain various facets of hippocampal neural activity during a WM task in humans but also offer new insights into how SWRs influence the switch in neural states.

We found that the distance of the neural trajectory across the phases was greater in the hippocampus compared to that in the EC and amygdala, even when considering the distance from O in these regions (Figure 2C–E). This supports the involvement of the hippocampus in the WM task, aligning with previous reports of hippocampal persistent firing during the maintenance phase [3] [4] [5] [6]. However, when we applied GPFA to multiunit activity during a 1-second level resolution of the WM task, we observed that the neural

¹²1.25 [1.30], median [IQR], $n = 1,281$, in Match IN task; 1.12 [1.35], median [IQR], $n = 1,163$, in Mismatch OUT task

¹³1.08 [1.07], median [IQR], $n = 1,149$, in Match IN task; 0.90 [1.12], median [IQR], $n = 1,088$, in Mismatch OUT task

¹⁴1.32 [1.24], median [IQR], $n = 935$, in Match IN task; 1.15 [1.26], median [IQR], $n = 891$, in Mismatch OUT task

¹⁵1.19 [0.96], median [IQR], $n = 673$, in Match IN task; 0.94 [0.88], median [IQR], $n = 664$, in Mismatch OUT task

trajectory in low-dimensional space showed a memory-load dependency between the encoding and retrieval phases, symbolized as $\|g_{\text{EGR}}\|$ (Figure 3). These findings corroborate the association of the hippocampus with WM processing.

Our analysis was confined to putative CA1 regions (Figure 4), which was bolstered by several factors. This specific focus stems from established observations that SWRs synchronize with spike bursts of interneurons and pyramidal neurons [44] [45] [46] [47], potentially within a 50 μm radius of the recording site [48]. We further identified an increased incidence of SWRs during the first 0–400 ms of the retrieval phase (Figure 4D). This finding harmonizes with previous reports of heightened SWR occurrence preceding spontaneous verbal recall [21] [22], supporting our results under a triggered retrieval condition. The observed log-normal distributions of both SWR duration and ripple band peak amplitude in this study (Figure 4C & E) is in accordance with the consensus in this field [39]. As a result, our decision to restrict recording sites to putative CA1 regions likely contributed to enhancing the accuracy of SWR detection. However, the increase in trajectory distance from *O* during SWRs (Figure 4) might have been skewed towards higher values due to channel selection. However, this potential bias does not substantially challenge our primary findings.

Interestingly, during the retrieval phase, the trajectory directions oscillated between encoding and retrieval states during both baseline and SWR periods (Figure 7C & D). Moreover, the balance of this oscillation shifted from encoding to retrieval state during SWR events (Figure 7E & F). These results are consistent with previous reports on the role of SWR in memory retrieval [21] [22]. Our findings highlight a new understanding, suggesting that SWRs occur when the hippocampal representation transitions from encoding to retrieval states. Therefore, these results reveal novel aspects of hippocampal representations, including (i) neuronal oscillation between encoding and retrieval states during a WM task and (ii) SWR serving as a trigger for changing neural states.

Furthermore, our study uncovered WM-task type-specific differences between encoding- and retrieval-SWRs (Figure 7E–F). Notably, opposing movements of encoding-SWR (eSWR) and retrieval-SWR (rSWR) were not observed in the Match IN task but were appar-

ent in the Mismatch OUT task. These observations can be explained by the memory engram theory [49]. Particularly, the Match IN task provided participants with previously presented letters, contrastingly, the Mismatch OUT task introduced a new letter not present in the encoding phase. These interpretations underscore the significant role of SWR in human cognitive processes.

In conclusion, the present investigation demonstrated that hippocampal activity oscillates between encoding and retrieval states during a WM task and uniquely transitions from encoding to retrieval during SWR incidents. These findings provide meaningful insight into the neural counterparts and functionality of working memory in the hippocampus.

References

- [1] W. B. Scoville, B. Milner, LOSS OF RECENT MEMORY AFTER BILATERAL HIPPOCAMPAL LESIONS, *Journal of Neurology, Neurosurgery, and Psychiatry* 20 (1) (1957) 11–21. URL <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC497229/>
- [2] L. R. Squire, The Legacy of Patient H.M. for Neuroscience, *Neuron* 61 (1) (2009) 6–9. doi:10.1016/j.neuron.2008.12.023. URL <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC2649674/>
- [3] E. Boran, T. Fedele, P. Klaver, P. Hifiker, L. Stieglitz, T. Grunwald, J. Sarnthein, Persistent hippocampal neural firing and hippocampal-cortical coupling predict verbal working memory load, *Science Advances* 5 (3) (2019) eaav3687. doi:10.1126/sciadv.aav3687. URL <https://www.science.org/doi/10.1126/sciadv.aav3687>
- [4] J. Kamiński, S. Sullivan, J. M. Chung, I. B. Ross, A. N. Mamelak, U. Rutishauser, Persistently active neurons in human medial frontal and medial temporal lobe support working memory, *Nature Neuroscience* 20 (4) (2017) 590–601, number: 4 Publisher: Nature Publishing Group. doi:10.1038/nn.4509. URL <https://www.nature.com/articles/nn.4509>
- [5] S. Kornblith, R. Q. Quiroga, C. Koch, I. Fried, F. Mormann, Persistent Single-Neuron Activity during Working Memory in the Human Medial Temporal Lobe, *Current Biology* 27 (7) (2017) 1026–1032, publisher: Elsevier. doi:10.1016/j.cub.2017.02.013. URL [https://www.cell.com/current-biology/abstract/S0960-9822\(17\)30149-5](https://www.cell.com/current-biology/abstract/S0960-9822(17)30149-5)
- [6] M. C. M. Faraut, A. A. Carlson, S. Sullivan, O. Tudusciuc, I. Ross, C. M. Reed, J. M. Chung, A. N. Mamelak, U. Rutishauser, Dataset of human medial temporal lobe single neuron activity during declarative memory encoding and recognition, *Scientific Data* 5 (1) (2018) 180010, number: 1 Publisher: Nature Publishing Group. doi:10.1038/sdata.2018.10. URL <https://www.nature.com/articles/sdata201810>

- [7] A. A. Borders, C. Ranganath, A. P. Yonelinas, The hippocampus supports high-precision binding in visual working memory, *Hippocampus* 32 (3) (2022) 217–230. doi:10.1002/hipo.23401.
- [8] J. Li, D. Cao, S. Yu, X. Xiao, L. Imbach, L. Stieglitz, J. Sarnthein, T. Jiang, Functional specialization and interaction in the amygdala-hippocampus circuit during working memory processing, *Nature Communications* 14 (1) (2023) 2921, number: 1 Publisher: Nature Publishing Group. doi:10.1038/s41467-023-38571-w. URL <https://www.nature.com/articles/s41467-023-38571-w>
- [9] V. Dimakopoulos, P. Mégevand, L. H. Stieglitz, L. Imbach, J. Sarnthein, Information flows from hippocampus to auditory cortex during replay of verbal working memory items, *eLife* 11 (2022) e78677, publisher: eLife Sciences Publications, Ltd. doi:10.7554/eLife.78677. URL <https://doi.org/10.7554/eLife.78677>
- [10] G. Buzsáki, Hippocampal sharp wave-ripple: A cognitive biomarker for episodic memory and planning, *Hippocampus* 25 (10) (2015) 1073–1188, eprint: <https://onlinelibrary.wiley.com/doi/pdf/10.1002/hipo.22488>. doi:<https://doi.org/10.1002/hipo.22488>. URL <https://onlinelibrary.wiley.com/doi/abs/10.1002/hipo.22488>
- [11] M. A. Wilson, B. L. McNaughton, Reactivation of hippocampal ensemble memories during sleep, *Science* (New York, N.Y.) 265 (5172) (1994) 676–679. doi:10.1126/science.8036517.
- [12] Z. Nádasdy, H. Hirase, A. Czurkó, J. Csicsvari, G. Buzsáki, Replay and Time Compression of Recurring Spike Sequences in the Hippocampus, *Journal of Neuroscience* 19 (21) (1999) 9497–9507, publisher: Society for Neuroscience Section: ARTICLE. doi:10.1523/JNEUROSCI.19-21-09497.1999. URL <https://www.jneurosci.org/content/19/21/9497>
- [13] A. K. Lee, M. A. Wilson, Memory of sequential experience in the hippocampus during slow wave sleep, *Neuron* 36 (6) (2002) 1183–1194. doi:10.1016/s0896-6273(02)01096-6.
- [14] K. Diba, G. Buzsáki, Forward and reverse hippocampal place-cell sequences during ripples, *Nature Neuroscience* 10 (10) (2007) 1241–1242, number: 10 Publisher: Nature Publishing Group. doi:10.1038/nn1961. URL <https://www.nature.com/articles/nn1961>
- [15] T. J. Davidson, F. Kloosterman, M. A. Wilson, Hippocampal replay of extended experience, *Neuron* 63 (4) (2009) 497–507. doi:10.1016/j.neuron.2009.07.027.
- [16] G. Girardeau, K. Benchenane, S. I. Wiener, G. Buzsáki, M. B. Zugaro, Selective suppression of hippocampal ripples impairs spatial memory, *Nature Neuroscience* 12 (10) (2009) 1222–1223. doi:10.1038/nn.2384. URL <http://www.nature.com/articles/nn.2384>
- [17] V. Ego-Stengel, M. A. Wilson, Disruption of ripple-associated hippocampal activity during rest impairs spatial learning in the rat, *Hippocampus* 20 (1) (2010) 1–10. doi:10.1002/hipo.20707.
- [18] A. Fernández-Ruiz, A. Oliva, E. Fermino de Oliveira, F. Rocha-Almeida, D. Tingley, G. Buzsáki, Long-duration hippocampal sharp wave ripples improve memory, *Science* (New York, N.Y.) 364 (6445) (2019) 1082–1086. doi:10.1126/science.aax0758. URL <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC6693581/>
- [19] J. Kim, A. Joshi, L. Frank, K. Ganguly, Cortical–hippocampal coupling during manifold exploration in motor cortex, *Nature* (2022) 1–8 Publisher: Nature Publishing Group. doi:10.1038/s41586-022-05533-z. URL <https://www.nature.com/articles/s41586-022-05533-z>
- [20] C.-T. Wu, D. Haggerty, C. Kemere, D. Ji, Hippocampal awake replay in fear memory retrieval, *Nature Neuroscience* 20 (4) (2017) 571–580. doi:10.1038/nn.4507.
- [21] Y. Norman, E. M. Yeagle, S. Khuvis, M. Harel, A. D. Mehta, R. Malach, Hippocampal sharp-wave ripples linked to visual episodic recollection in humans, *Science* 365 (6454) (2019) eaax1030. doi:10.1126/science.aax1030. URL <https://www.sciencemag.org/lookup/doi/10.1126/science.aax1030>
- [22] Y. Norman, O. Raccach, S. Liu, J. Parvizi, R. Malach, Hippocampal ripples and their coordinated dialogue with the default mode network during recent and remote recollection, *Neuron* 109 (17) (2021) 2767–2780.e5, publisher: Elsevier. doi:10.1016/j.neuron.2021.06.020. URL [https://www.cell.com/neuron/abstract/S0896-6273\(21\)00461-X](https://www.cell.com/neuron/abstract/S0896-6273(21)00461-X)
- [23] C. J. Behrens, L. P. van den Boom, L. de Hoz, A. Friedman, U. Heinemann, Induction of sharp wave–ripple complexes in vitro and reorganization of hippocampal networks, *Nature Neuroscience* 8 (11) (2005) 1560–1567, number: 11 Publisher: Nature Publishing Group. doi:10.1038/nn1571. URL <https://www.nature.com/articles/nn1571>
- [24] H. Norimoto, K. Makino, M. Gao, Y. Shikano, K. Okamoto, T. Ishikawa, T. Sasaki, H. Hioki, S. Fujisawa, Y. Ikegaya, Hippocampal ripples down-regulate synapses, *Science* (New York, N.Y.) 359 (6383) (2018) 1524–1527. doi:10.1126/science.aao0702.
- [25] S. P. Jadhav, C. Kemere, P. W. German, L. M. Frank, Awake Hippocampal Sharp-Wave Ripples Support Spatial Memory, *Science* 336 (6087) (2012) 1454–1458, publisher: American Association for the Advancement of Science. doi:10.1126/science.1217230. URL <https://www.science.org/doi/abs/10.1126/science.1217230>
- [26] J. O’Keefe, J. Dostrovsky, The hippocampus as a spatial map: Preliminary evidence from unit activity in the freely-moving rat, *Brain Research* 34 (1971) 171–175, place: Netherlands Publisher: Elsevier Science. doi:10.1016/0006-8993(71)90358-1.
- [27] J. O’Keefe, Place units in the hippocampus of the freely moving rat, *Experimental Neurology* 51 (1) (1976) 78–109. doi:10.1016/0014-4886(76)90055-8. URL <https://www.sciencedirect.com/science/article/pii/0014488676900558>
- [28] A. D. Ekstrom, M. J. Kahana, J. B. Caplan, T. A. Fields, E. A. Isham, E. L. Newman, I. Fried, Cellular networks underlying human spatial navigation, *Nature* 425 (6954) (2003) 184–188, number: 6954 Publisher: Nature Publishing Group. doi:10.1038/nature01964.

- URL <https://www.nature.com/articles/nature01964>
- [29] K. B. Kjelstrup, T. Solstad, V. H. Brun, T. Hafting, S. Leutgeb, M. P. Witter, E. I. Moser, M.-B. Moser, Finite Scale of Spatial Representation in the Hippocampus, *Science* 321 (5885) (2008) 140–143, publisher: American Association for the Advancement of Science. doi:10.1126/science.1157086. URL <https://www.science.org/doi/abs/10.1126/science.1157086>
- [30] C. D. Harvey, F. Collman, D. A. Dombeck, D. W. Tank, Intracellular dynamics of hippocampal place cells during virtual navigation, *Nature* 461 (7266) (2009) 941–946, number: 7266 Publisher: Nature Publishing Group. doi:10.1038/nature08499. URL <https://www.nature.com/articles/nature08499>
- [31] H. Zhang, P. D. Rich, A. K. Lee, T. O. Sharpee, Hippocampal spatial representations exhibit a hyperbolic geometry that expands with experience, *Nature Neuroscience* (Dec. 2022). doi:10.1038/s41593-022-01212-4. URL <https://www.nature.com/articles/s41593-022-01212-4>
- [32] P. A. Naber, F. H. Lopes da Silva, M. P. Witter, Reciprocal connections between the entorhinal cortex and hippocampal fields CA1 and the subiculum are in register with the projections from CA1 to the subiculum, *Hippocampus* 11 (2) (2001) 99–104, eprint: <https://onlinelibrary.wiley.com/doi/pdf/10.1002/hipo.1028>. doi:10.1002/hipo.1028. URL <https://onlinelibrary.wiley.com/doi/abs/10.1002/hipo.1028>
- [33] N. M. van Strien, N. L. M. Cappaert, M. P. Witter, The anatomy of memory: an interactive overview of the parahippocampal–hippocampal network, *Nature Reviews Neuroscience* 10 (4) (2009) 272–282, number: 4 Publisher: Nature Publishing Group. doi:10.1038/nrn2614. URL <https://www.nature.com/articles/nrn2614>
- [34] B. A. Strange, M. P. Witter, E. S. Lein, E. I. Moser, Functional organization of the hippocampal longitudinal axis, *Nature Reviews Neuroscience* 15 (10) (2014) 655–669, number: 10 Publisher: Nature Publishing Group. doi:10.1038/nrn3785. URL <https://www.nature.com/articles/nrn3785>
- [35] R. J. Gardner, E. Hermansen, M. Pachitariu, Y. Burak, N. A. Baas, B. A. Dunn, M.-B. Moser, E. I. Moser, Toroidal topology of population activity in grid cells, *Nature* 602 (7895) (2022) 123–128, number: 7895 Publisher: Nature Publishing Group. doi:10.1038/s41586-021-04268-7. URL <https://www.nature.com/articles/s41586-021-04268-7>
- [36] E. Boran, T. Fedele, A. Steiner, P. Hilfiker, L. Stieglitz, T. Grunwald, J. Sarnthein, Dataset of human medial temporal lobe neurons, scalp and intracranial EEG during a verbal working memory task, *Scientific Data* 7 (1) (2020) 30, number: 1 Publisher: Nature Publishing Group. doi:10.1038/s41597-020-0364-3. URL <https://www.nature.com/articles/s41597-020-0364-3>
- [37] B. M. Yu, J. P. Cunningham, G. Santhanam, S. I. Ryu, K. V. Shenoy, M. Sahani, Gaussian-Process Factor Analysis for Low-Dimensional Single-Trial Analysis of Neural Population Activity, *Journal of Neurophysiology* 102 (1) (2009) 614–635. doi:10.1152/jn.90941.2008. URL <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC2712272/>
- [38] J. Niediek, J. Boström, C. E. Elger, F. Mormann, Reliable Analysis of Single-Unit Recordings from the Human Brain under Noisy Conditions: Tracking Neurons over Hours, *PLOS ONE* 11 (12) (2016) e0166598, publisher: Public Library of Science. doi:10.1371/journal.pone.0166598. URL <https://journals.plos.org/plosone/article?id=10.1371/journal.pone.0166598>
- [39] A. A. Liu, S. Henin, S. Abbaspour, A. Bragin, E. A. Buffalo, J. S. Farrell, D. J. Foster, L. M. Frank, T. Gedankien, J. Gotman, J. A. Guidera, K. L. Hoffman, J. Jacobs, M. J. Kahana, L. Li, Z. Liao, J. J. Lin, A. Losonczy, R. Malach, M. A. van der Meer, K. McClain, B. L. McNaughton, Y. Norman, A. Navas-Olive, L. M. de la Prida, J. W. Rueckemann, J. J. Sakon, I. Skelin, I. Soltesz, B. P. Staresina, S. A. Weiss, M. A. Wilson, K. A. Zaghoul, M. Zugaro, G. Buzsáki, A consensus statement on detection of hippocampal sharp wave ripples and differentiation from other fast oscillations, *Nature Communications* 13 (1) (2022) 6000, number: 1 Publisher: Nature Publishing Group. doi:10.1038/s41467-022-33536-x. URL <https://www.nature.com/articles/s41467-022-33536-x>
- [40] K. Kay, M. Sosa, J. E. Chung, M. P. Karlsson, M. C. Larkin, L. M. Frank, A hippocampal network for spatial coding during immobility and sleep, *Nature* 531 (7593) (2016) 185–190. doi:10.1038/nature17144.
- [41] L. McInnes, J. Healy, N. Saul, L. Großberger, UMAP: Uniform Manifold Approximation and Projection, *Journal of Open Source Software* 3 (29) (2018) 861. doi:10.21105/joss.00861. URL <https://joss.theoj.org/papers/10.21105/joss.00861>
- [42] P. J. Rousseeuw, Silhouettes: A graphical aid to the interpretation and validation of cluster analysis, *Journal of Computational and Applied Mathematics* 20 (1987) 53–65. doi:10.1016/0377-0427(87)90125-7. URL <https://www.sciencedirect.com/science/article/pii/0377042787901257>
- [43] P. Virtanen, R. Gommers, T. E. Oliphant, M. Haberland, T. Reddy, D. Cournapeau, E. Burovski, P. Peterson, W. Weckesser, J. Bright, S. J. van der Walt, M. Brett, J. Wilson, K. J. Millman, N. Mayorov, A. R. J. Nelson, E. Jones, R. Kern, E. Larson, C. J. Carey, Polat, Y. Feng, E. W. Moore, J. VanderPlas, D. Laxalde, J. Perktold, R. Cimrman, I. Henriksen, E. A. Quintero, C. R. Harris, A. M. Archibald, A. H. Ribeiro, F. Pedregosa, P. van Mulbregt, SciPy 1.0 Contributors, SciPy 1.0: fundamental algorithms for scientific computing in Python, *Nature Methods* 17 (2020) 261–272, aDS Bibcode: 2020NatMe..17..261V. doi:10.1038/s41592-019-0686-2. URL <https://ui.adsabs.harvard.edu/abs/2020NatMe..17..261V>
- [44] G. Buzsáki, Two-stage model of memory trace formation: a role for "noisy" brain states, *Neuroscience* 31 (3) (1989) 551–570. doi:10.1016/0306-4522(89)90423-5.
- [45] M. L. V. Quyen, A. Bragin, R. Staba, B. Crépon, C. L. Wilson, J. Engel, Cell Type-Specific Firing during Ripple Oscillations in the Hippocampal Formation of Humans, *Jour-*

- nal of Neuroscience 28 (24) (2008) 6104–6110, publisher: Society for Neuroscience Section: Brief Communications. doi:10.1523/JNEUROSCI.0437-08.2008. URL <https://www.jneurosci.org/content/28/24/6104>
- [46] S. Royer, B. V. Zemelman, A. Losonczy, J. Kim, F. Chance, J. C. Magee, G. Buzsáki, Control of timing, rate and bursts of hippocampal place cells by dendritic and somatic inhibition, *Nature Neuroscience* 15 (5) (2012) 769–775, number: 5 Publisher: Nature Publishing Group. doi:10.1038/nn.3077. URL <https://www.nature.com/articles/nn.3077>
- [47] N. Hájos, M. R. Karlócai, B. Németh, I. Ulbert, H. Monyer, G. Szabó, F. Erdélyi, T. F. Freund, A. I. Gulyás, Input-output features of anatomically identified CA3 neurons during hippocampal sharp wave/ripple oscillation in vitro, *The Journal of Neuroscience: The Official Journal of the Society for Neuroscience* 33 (28) (2013) 11677–11691. doi:10.1523/JNEUROSCI.5729-12.2013.
- [48] E. W. Schomburg, C. A. Anastassiou, G. Buzsáki, C. Koch, The Spiking Component of Oscillatory Extracellular Potentials in the Rat Hippocampus, *The Journal of Neuroscience* 32 (34) (2012) 11798–11811. doi:10.1523/JNEUROSCI.0656-12.2012. URL <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC3459239/>
- [49] X. Liu, S. Ramirez, P. T. Pang, C. B. Puryear, A. Govindarajan, K. Deisseroth, S. Tonegawa, Optogenetic stimulation of a hippocampal engram activates fear memory recall, *Nature* 484 (7394) (2012) 381–385, number: 7394 Publisher: Nature Publishing Group. doi:10.1038/nature11028. URL <https://www.nature.com/articles/nature11028>
- [50] M. K. van Vugt, A. Schulze-Bonhage, B. Litt, A. Brandt, M. J. Kahana, Hippocampal Gamma Oscillations Increase with Memory Load, *The Journal of Neuroscience* 30 (7) (2010) 2694–2699. doi:10.1523/JNEUROSCI.0567-09.2010. URL <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC2835496/>
- [51] K. Nader, Memory traces unbound, *Trends in Neurosciences* 26 (2) (2003) 65–72. doi:10.1016/S0166-2236(02)00042-5. URL <https://www.sciencedirect.com/science/article/pii/S0166223602000425>

Contributors

Y.W. and T.Y. conceptualized the study; Y.W. performed the data analysis; Y.W. and T.Y. wrote the original draft; and all authors reviewed the final manuscript.

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Declaration of Interests

The authors declare that they have no competing interests.

Data and code availability

The data is available on G-Node (<https://doi.gin.g-node.org/10.12751/g-node.d76994/>). The source code is available on GitHub (<https://github.com/yanagisawa-lab/hippocampal-neural-fluctuation-during-a-WM-task-in-hum>)

Inclusion and Diversity Statement

We support inclusive, diverse, and equitable conduct of research.

Declaration of Generative AI in Scientific Writing

The authors employed ChatGPT, provided by OpenAI, for enhancing the manuscript’s English language quality. After incorporating the suggested improvements, the authors meticulously revised the content. Ultimate responsibility for the final content of this publication rests entirely with the authors.

Tables

Subject ID	of sessions	AHL	AHR	PHL	PHR	ECL	ECR	AL	AR	SOZ
1	4	o	x	o	o	o	x	o	x	"AHR, LR"
2	7	o	o	o	o	o	o	o	o	"AHR, PHR"
3	3	o	o	o	o	o	o	o	x	"AHL, PHL"
4	2	o	o	o	o	o	o	o	o	"AHL, AHR, PHL, PHR"
5	3	o	x	x	o	x	x	o	x	DRR
6	6	o	o	o	o	o	o	o	o	"AHL, PHL, ECL, AL"
7	4	o	o	o	o	o	o	o	o	"AHR, PHR"
8	5	o	o	o	o	o	o	o	o	ECR
9	2	o	o	o	o	o	o	o	o	"ECR, AR"

Table 1 – Distribution of Electrodes within the Dataset

This figure represents the electrode placements and the seizure onset zones. Regions designated with "o" were available in the dataset, whereas those marked with "x" (*navy*) were not present. Abbreviations include: AHL, left hippocampal head; AHR, right hippocampal head; PHL, left hippocampal body; PHR, right hippocampal body; ECL, left entorhinal cortex; ECR, right entorhinal cortex; AL, left amygdala; AR, right amygdala; and SOZ symbolizes the seizure onset zone.

Subject	AHL	AHR	PHL	PHR
1	0.60 ± 0.14	n.a.	n.a.	0.1 ± 0
2	0.21 ± 0.16	0.17 ± 0.21	0.18 ± 0.22	0.20 ± 0.15
3	0.40 ± 0.42	0.83 ± 0.12	n.a.	n.a.
4	0.10 ± 0.00	0.10 ± 0.00	0.90 ± 0.00	0.10 ± 0.14
5	n.a.	n.a.	n.a.	n.a.
6	0.63 ± 0.06	n.a.	n.a.	0.27 ± 0.06
7	0.10 ± 0.00	0.35 ± 0.35	0.37 ± 0.47	0.10 ± 0.00
8	0.13 ± 0.10	n.a.	0.28 ± 0.49	n.a.
9	n.a.	0.85 ± 0.07	0.15 ± 0.07	n.a.

Table 2 – Silhouette score of UMAP clustering for SWR^+ candidates and SWR^- candidates

The silhouette scores (mean \pm SD across sessions per subject) for UMAP clustering of SWR^+ candidates and SWR^- candidates (Figure 4A) were calculated based on their corresponding multiunit spike patterns (mean values were 0.205 [0.285], median [IQR]; Figure 4B).

Subject ID	of sessions	of trials	ROI	of SWRs	SWR incidence [Hz]
1	2	100	AHL	274	0.34
3	2	97	AHR	325	0.42
4	2	99	PHL	202	0.26
6	2	100	AHL	297	0.37
9	2	97	AHR	72	0.09
Total = 10	Total = 493	"Total = 1,170"	0.30 ± 0.13 (mean ± SD)		

Table 3 – Accounting for Defined SWR Events

The table collates statistics of putative CA1 regions and SWR events. Only the first two sessions (sessions 1 and 2) from each subject were considered to minimize sampling bias.

Figures

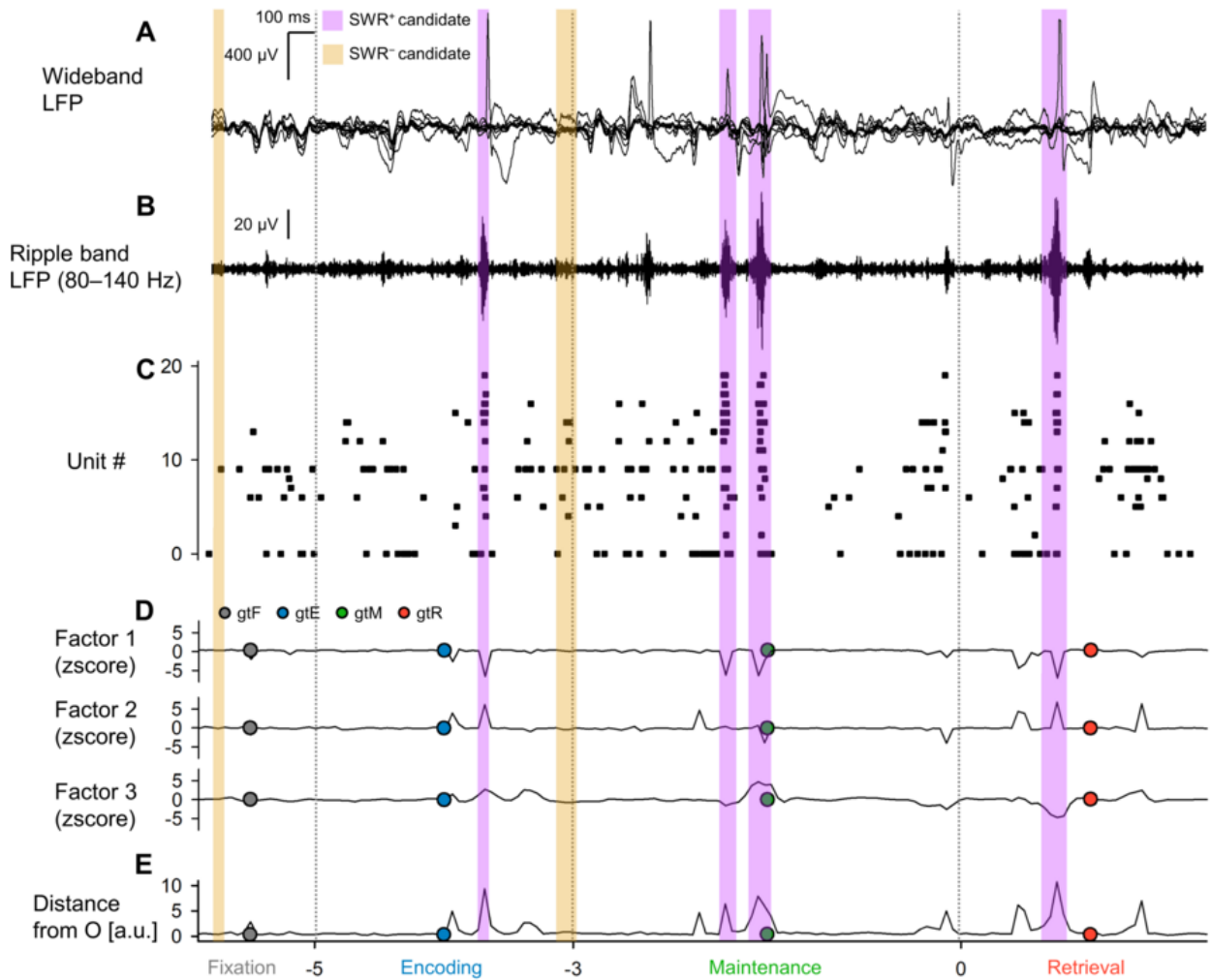


Figure 1 – Local Field Potentials (LFP), Multiunit Activity, and Neural Trajectories in the Hippocampus During a Modified Sternberg Task Local Field Potential (LFP), Multiunit Activity, and Neural Trajectory of the Hippocampus during a Modified Sternberg Task [8? , 9]

A. These traces show representative wideband LFP-intracranial EEG (iEEG) signals recorded from the left hippocampal head. The subject performed a modified Sternberg working memory task, which includes fixation (This segment presents representative wideband LFP traces from iEEG signals, observed in the left hippocampal head throughout the completion of a modified Sternberg working memory task. The task involves fixation (1 s, s, gray); encoding (encoding (2 s, s, blue), maintenance (maintenance (3 s, s, green), and retrieval (retrieval (2 s, s, red).) [8? , 9]. B. We then present the corresponding ripple band LFP traces. The corresponding ripple band LFP traces are depicted here [48, 23, 24]. C. The raster plot depicts multiunit spikes taken from the LFP traces, sorted using a spike algorithm [38]. The raster plot of multiunit spikes, derived from the LFP traces utilizing a spike sorting algorithm, is illustrated here [38]. D. Subsequently, we illustrate the neural trajectories, which are calculated by GPFA on spike counts per unit with This part represents the neural trajectory, established by the GPFA, computed from the spike counts per unit within 50-ms bins. Each phase's geometric median is marked by the dot circles. bins [37]. The dotted circles represent the geometric median coordinates for each phase. E. The trajectory's distance from the origin The distance from the trajectory to the point O is portrayed, with is demonstrated here. It is notable that the purple and yellow rectangles indicating the timings for SWR rectangles denote the timings for SWR⁺ candidates and SWR⁻ candidates and SWR⁻ candidates (considered as controls for SWR⁺ candidates, respectively, functioning as controls for SWR⁺), respectively. [50, 1, 40, 51, 11, 12, 13].



Figure 2 – State-Dependent Trajectories of Hippocampal Neurons State-dependent Hippocampal Neural Trajectory

A. Neural trajectories—This figure presents the neural trajectory within the initial three-dimensional factors first three dimensions, derived from the using Gaussian Process Factor Analysis (GPFA) are displayed. The Each smaller dots correspond to dot signifies the coordinates of a 50-ms neural trajectory bins, while the larger dots with indicated in black edges signify represent the geometric medians for respective stages of successive phases in the Sternberg working memory task. The phases include fixation (*gray*), encoding (*blue*), maintenance (*green*), and retrieval (*red*) [37]. B. The figure conveys graph shows the log-likelihood of the GPFA models versus compared to the count number of dimensions used to embed multiunit employed for embedding multi-unit spikes found in the within medial temporal lobe (MTL) territories regions. In specific, Notably, the elbow method pinpointed the optimal dimension dimensionality was found to be three, based on the elbow method [43]. C. This panel illustrates section delineates the distance of between the neural trajectories from trajectory and the origin (*O*) for the hippocampus (Hipp.), entorhinal cortex (EC), and amygdala (Amy.), against the and plots it over time elapsed from since the probe onset of the probe [36]. D. The distance of subsequent graph underscores the trajectory's distance from *O* within across MTL regions is displayed. The with the hippocampus shows registering the farthest most extensive distance, followed by the EC and the Amygdala [18]. E. The plot represents final depiction signifies the inter-phase trajectory distances within the MTL regions [39]. Abbreviations:

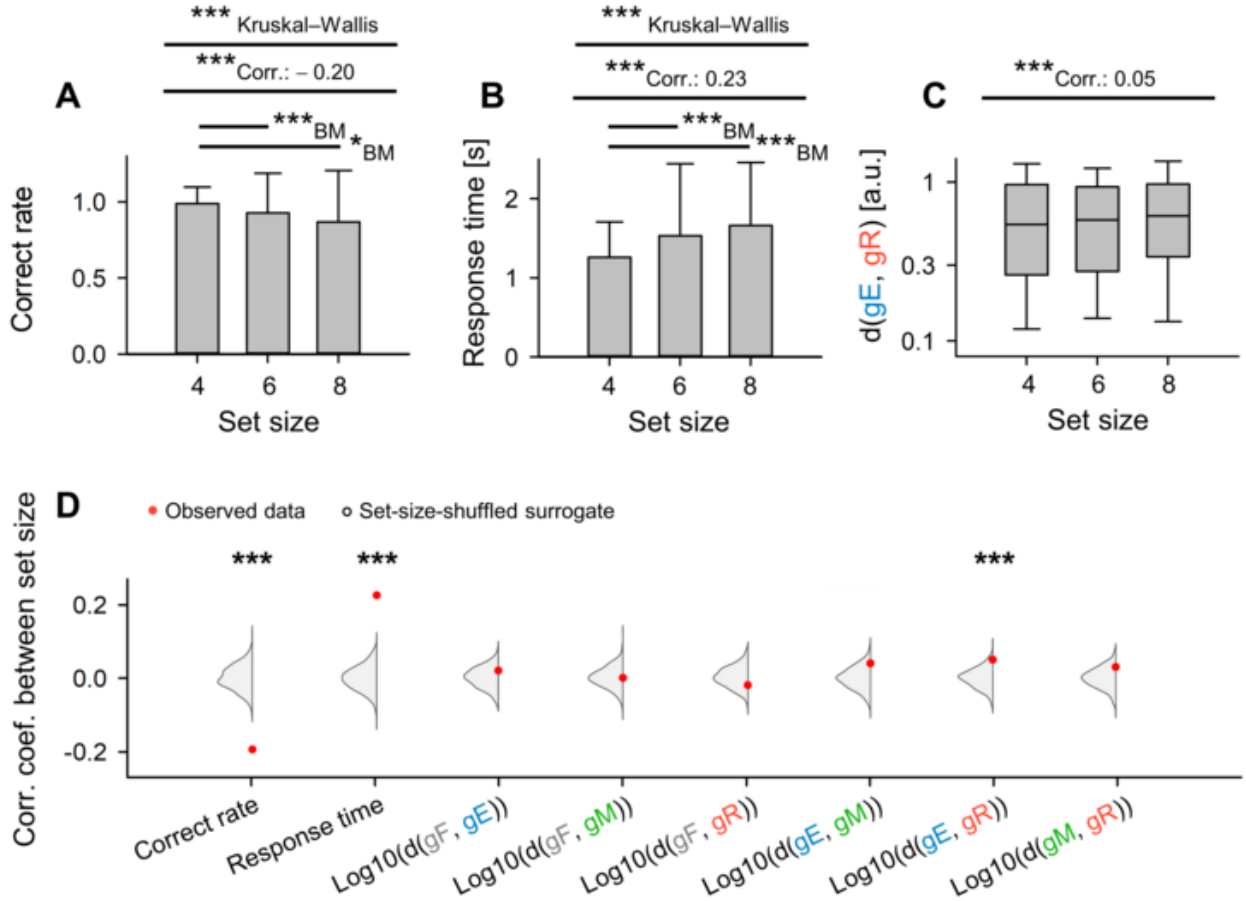


Figure 3 – Dependency of Trajectory Distance on Memory Load: Encoding and Retrieval States in Hippocampus
Dependence of Trajectory Distance on Memory Load Between Encoding and Retrieval States in the Hippocampus

A. The relationship—A significant correlation has been documented between the set size (the number of letters that need to be encoded/encode) and correct-the correctness rate in the working-memory-WM task (coefficient = -0.20, *** $p < 0.001$) [50, 8, 7]. B. The—A notable correlation exists between set size and response time (coefficient = 0.230, 23, *** $p < 0.001$) [9]. C. The impact of—There is a correlation between set size on-and the inter-phase distances between the encoding and retrieval phases ($\|g_{EgR}\| \|g_{EgR}\|$), but it's less significant (correlation coefficient = 0.05) [8]. D. Red dots represent experimental observations of-express the observed correlations between set size and the following stated parameters: correct rate, response time, $\log_{10} \|g_{FgE}\| \|g_{FgE}\|$, $\log_{10} \|g_{FgM}\| \|g_{FgM}\|$, $\log_{10} \|g_{FgR}\| \|g_{FgR}\|$, $\log_{10} \|g_{EgM}\| \|g_{EgM}\|$, $\log_{10} \|g_{EgR}\| \|g_{EgR}\|$, and $\log_{10} \|g_{MgR}\| \|g_{MgR}\|$. The gray kernel density plot illustrates the corresponding set-size-shuffled-surrogate-randomized set-size measurements ($n = 1,000$) (** $p < 0.001$) [24, 47].

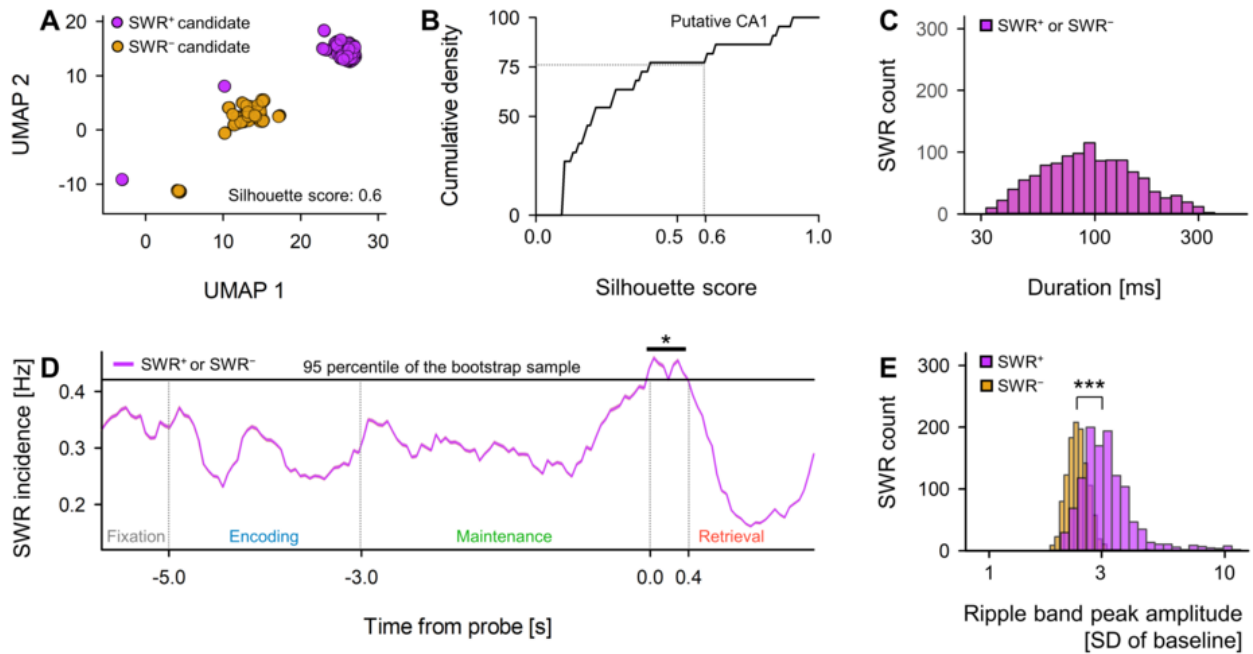


Figure 4 – Detection of SWRs in Presumptive CA1 Regions- Detection of SWRs in Presumed CA1 Regions

A. **Two-dimensional UMAP** (A two-dimensional Uniform Manifold Approximation and Projection (UMAP) [41] projection of multiunit multi-unit spikes during SWR⁺ candidates potential SWRs (purple) and SWR⁻ candidates non-SWRs (yellow) periods is given [41]. B. **Cumulative** The cumulative density plot shows of silhouette scores, indicative measuring the quality of UMAP clustering quality, for across diverse hippocampal regions, is shown (see refer to Table 2 for reference). Note Regions that hippocampal regions with attained a silhouette scores greater than score above 0.60 (equivalent corresponding to the 75th percentile) were, are identified as possible probable CA1 regions areas. SWR⁺ and SWR⁻ candidates recorded from Within these speculative potential CA1 regions, the SWR and non-SWR periods were respectively classified categorized as SWR⁺ SWRs and SWR⁻ non-SWRs ($n = 1,170$) [42]. C. The identical distributions of durations are presented for SWR⁺ both SWRs (purple) and SWR⁻ non-SWRs (yellow) are depicted, owing to based on their respective definitions (93.0 [65.4] ms, median [IQR]) [16][22]. D. **SWR incidence** for both SWR⁺ An illustration of the frequency of SWRs (purple) and SWR⁻ non-SWRs (yellow) obtained relative to over time from the probe's timing is illustrated as a start of stimulation, represented by mean value \pm 95% confidence interval is given. However, as the intervals may not It should be visible noted that due to their narrow range close intervals, note that visual differentiation can be difficult. Additionally, there was a significant discernible increase in SWR incidence was detected frequency during the initial 400 ms of the retrieval phase (0.421 [Hz], * $p < 0.05$, bootstrap test) [10][17][18]. E. **The distributions** Distributions of ripple band peak amplitudes for SWR⁻ non-SWRs (yellow; 2.37 [0.33] times the standard deviation (SD) of the baseline, median [IQR]) and SWR⁺ SWRs (purple; 3.05 [0.85] times the SD of the baseline, median [IQR]) are delineated exhibited. Considerable differences were observed (***) $p < 0.001$, by the Brunner–Munzel test) [21][14][39].

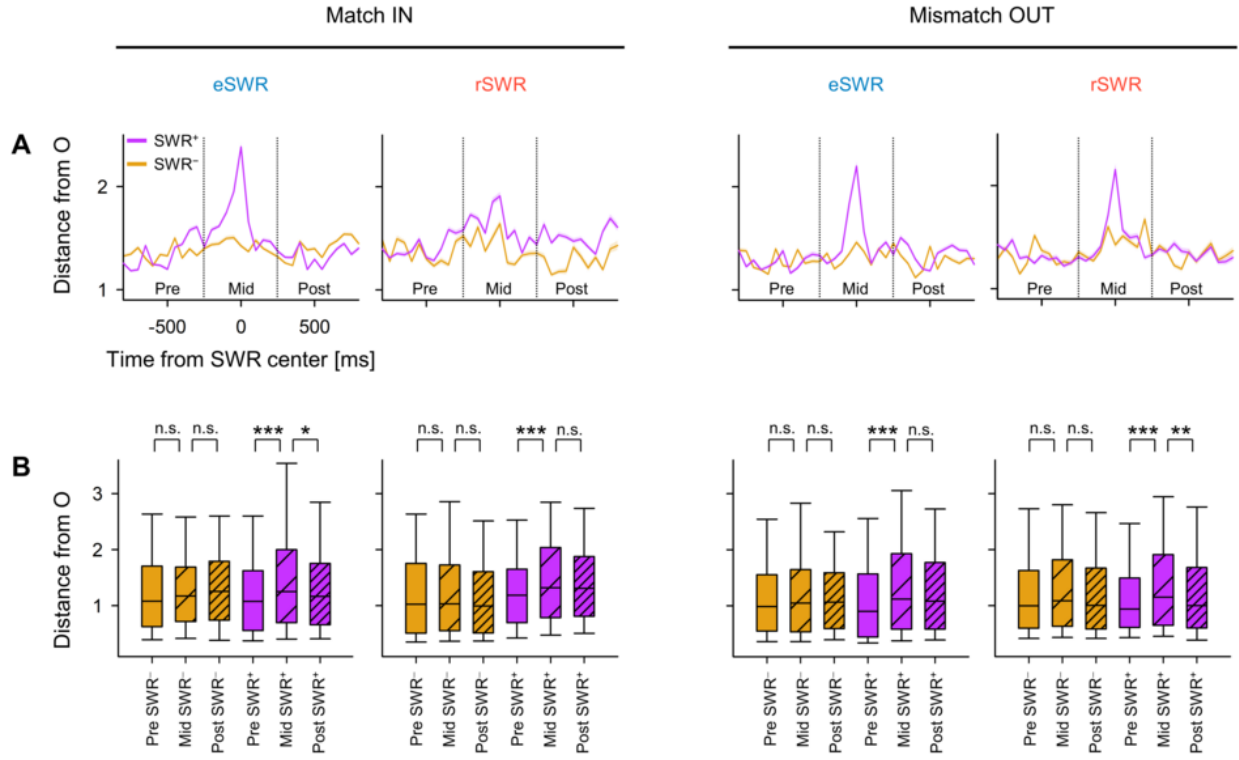
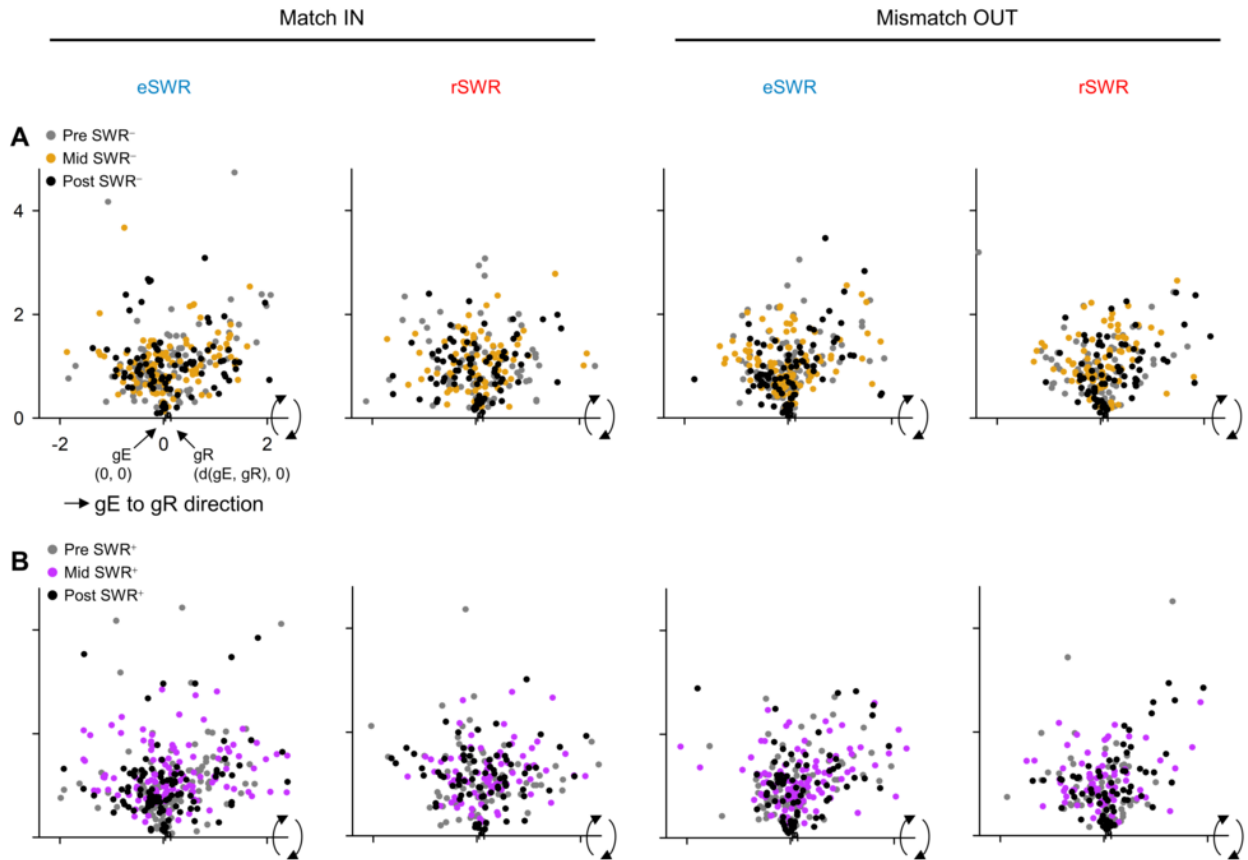


Figure 5 – Transient Alterations in Neural Trajectory During SWR Events Transient Changes in Neural Trajectory During SWR

A. Displayed is the distance from origin (Depicts the average distance from the origin (O) of the) of the peri-sharp-wave-ripple trajectory (mean (SWR) trajectory, alongside a 95% confidence interval). The intervals may not be apparent due to their slender ranges. % confidence interval, which may not be evident due to its limited range [16, 21, 10]. **B.** Shown is the distance from the origin (Demonstrates the distance from the origin (O) during) throughout pre-, mid-, and, and post-SWR periods (intervals (* $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$; assessed using the; according to the Brunner–Munzel test). Abbreviations: SWR, test [3]). The defined terms are: SWR, sharp-wave ripple events; eSWR, SWR during the encoding phase; rSWR, SWR while in the retrieval phase; SWR⁺, positive SWR event; SWR⁻, an SWR event; SWR⁻, control events for SWR, the control events aligned with SWR⁺; pre-, mid-, or, or post-SWR denote the time intervals from, the time segments from –800 to –250 ms, from ms, from –250 to +250 ms, or from ms, and from +250 to +800 ms, all relative to the center of the SWR, ms, respectively, each relative to the SWR center.



The panels display hippocampal neural trajectories during Sharp-Wave Ripple (SWR) events in a two-dimensional space context. **A.** Indicates hippocampal neural trajectories pre-SWR⁻ of the pre- (gray), mid-SWR⁻ mid- (yellow), and post-SWR⁻ (black) phases of an SWR event [10]. **B.** Represents the equivalents for The trajectories that correspond with SWR⁺ as opposed to conditions are presented, contrasting with the SWR⁻ backdrop [18]. The Variations in the magnitude of $\|g_{EGR}\|$ varied among are evident across sessions [39]. The projection was applied in the following manner protocol is outlined as follows: First initially, a linear transformation positioned g_E was located at the origin O (0,0), and g_R at $(\|g_{EGR}\|, 0)$, realized through linear transformation [19]. The Subsequently, rotation of the point cloud was then rotated around the g_{EGR} axis (equivalent to the x-axis) for fitting into was conducted to accommodate a two-dimensional space space [37]. Therefore, within these two-dimensional spaces As a result, both the distances from O and the angles preserved the original makeup of relative to the g_{EGR} axis from the remained consistent with their original three-dimensional space configuration [41]. Abbreviations Key terms used in this context: SWR signifies sharp-wave ripple pertains to Sharp-Wave Ripple events; eSWR denotes means SWR during the encoding phase; rSWR indicates signifies SWR during the retrieval phase; SWR⁺, marks defines an SWR event; SWR⁻ refers to represents the control events event for SWR⁺; pre-SWR, mid-SWR, or and post-SWR, reference the indicate time intervals from -800 to -250 ms, from -250 to +250 ms, or and from +250 to +800 ms from the center of an SWR event, respectively [31].

The panels display hippocampal neural trajectories during Sharp-Wave Ripple (SWR) events in a two-dimensional space context. **A.** Indicates hippocampal neural trajectories pre-SWR⁻ of the pre- (gray), mid-SWR⁻ mid- (yellow), and post-SWR⁻ (black) phases of an SWR event [10]. **B.** Represents the equivalents for The trajectories that correspond with SWR⁺ as opposed to conditions are presented, contrasting with the SWR⁻ backdrop [18]. The Variations in the magnitude of $\|g_{EGR}\|$ varied among are evident across sessions [39]. The projection was applied

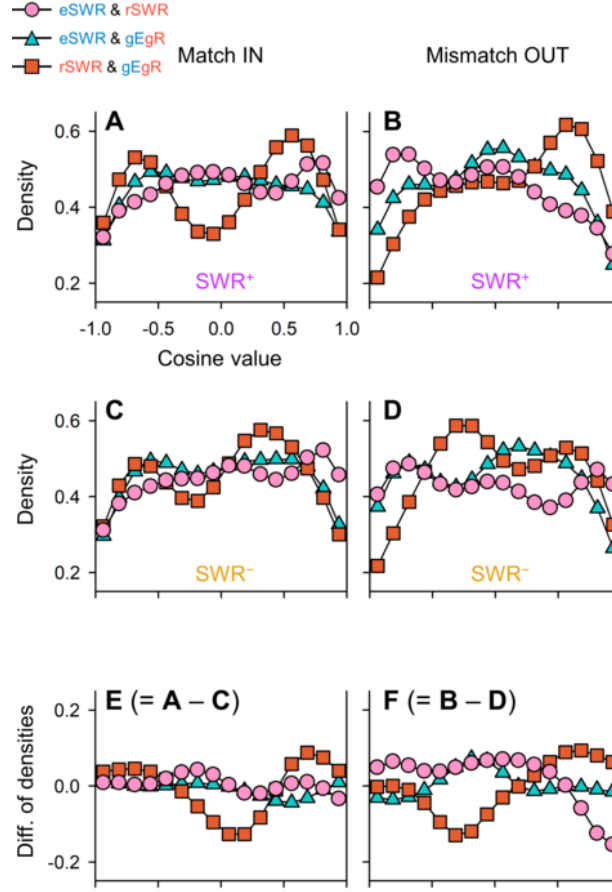


Figure 7 – Directions of Neural Trajectories during SWRs Based on Encoding and Retrieval States- Directionality of Neural Trajectories in SWR Based on Encoding and Retrieval States

A–B Depicted are the Kernel density estimation (KDE) distributions of $\overrightarrow{eSWR^+} \cdot \overrightarrow{rSWR^+}$ (pink circles), $\overrightarrow{eSWR^+} \cdot \overrightarrow{gEGR}$ (blue triangles), and $\overrightarrow{rSWR^+} \cdot \overrightarrow{gEGR}$ (red rectangles) in Match IN (A) and Mismatch OUT tasks (B) [8]. C–D Present the corresponding Similar distributions of for these tasks where SWR⁻ instead of those of replaces SWR⁺ in A and B have been presented [9]. E–F Depict the differences in Distinctions between the distributions of SWR⁺ and SWR⁻; illuminating highlight the SWR components ($E = C - A$; $F = D - B$). Note, where the biphasic distributions of $\overrightarrow{rSWR^-} \cdot \overrightarrow{gEGR}$, suggesting fluctuations indicate neural oscillations between the encoding and retrieval states during the Sternberg task [7]. Moreover Contrarily, the Mismatch OUT task showed an inverse directionality relationship between $\overrightarrow{eSWR^+}$ and $\overrightarrow{rSWR^+}$ was observed (pink circles) in the Mismatch OUT task, but a finding not observed in the Match IN task (E–F) [32, 33]. Finally Lastly, shifts transitions from the retrieval to encoding states were evident in for the SWR components were apparent in both the Match IN and Mismatch OUT tasks (red rectangles in E and F–F) [38, 48].