Highlights

•	Neural	trajectories	in	the	hippocampus	exhib-
	ited gre	ater variabil	ity	durir	ng a working n	nemory
	(WM) t	ask compare	d to	thos	e in the entorhi	nal cor-
	tex and	amygdala re	gio	ns.		

• The distance of neural trajectories between encoding and retrieval states in the hippocampus was memory-load dependent during a WM task.

 Hippocampal neural trajectories fluctuated between the encoding and retrieval states in a taskdependent manner during both baseline and sharpwave ripple (SWR) periods.

• Hippocampal neural trajectories shifted from encoding to retrieval states during SWR period.

Hippocampal neural fluctuations between memory encoding and retrieval states during a working memory task in humans

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Abstract

Working memory (WM), eritical to various is fundamental to a plethora of cognitive functions, embodies but the intricate neural mechanisms which are not entirely understood. Notably, the role crucial to its operation are not fully comprehended. In particular, the roles of the hippocampus and sharp-wave ripple complexes (SWRs) eoordinated, rapidneuronal - rapid, synchronised neural events within the hippocampus - in WM tasks remains somewhat ambiguous, notwithstanding their confirmed involvement in __ are known to facilitate memory consolidation and retrieval. In our present research, we posit that multiunit activity patterns within the hippocampus operate synergistically, yet their contributions to WM tasks remain somewhat ambiguous. We propose that the coordinated activity patterns in the hippocampus work in unison with SWRs, consequently exhibiting distinctive displaying distinct dynamics during WM tasks. Our study engaged in a comprehensive involved an extensive analysis of a dataset derived obtained from intracranial electroencephalogram recordings from the medial temporal lobes lobe (MTL) of nine epileptic patients executing during an eight-second Sternberg task. We utilised Gaussian-process factor analysis was utilized to pinpoint to identify low-dimensional neural vectors representations, or 'trajectories,' within the MTL areas during the WM task. We discovered that the hippocampus showed the most pronounced variation in neural trajectories relative-found that the neural trajectory displayed the most substantial variations in the hippocampus compared to the entorhinal cortex and the amygdala. Intriguingly, amygdala. Moreover, we observed that the deviation in trajectories between the encoding and retrieval phases was seen to be dependent on memory load. Further Interestingly, hippocampal trajectories showed oscillatory behavior oscillated during the retrieval phase, indicating task-related transitions revealing task-dependent shifts between encoding and retrieval states, and embracing both which encompassed baseline and SWR episodesphases. These oscillations transitioned from encoding to retrieval states in correlation with the SWRs. Hence, these findings underscore the crucial consistent with the occurrence of SWRs. These findings underline the significant role of the hippocampus in tackling during the performance of WM tasks and propose an enticing hypothesis for future put forward a compelling hypothesis for further exploration: the functional state of the hippocampus undergoes a functional transition from encoding to retrieval during SWRs.

Keywords: working memory, WM, memory load, hippocampus, sharp-wave ripples, SWR, humans

Working memory (WM) serves a critical plays a crucial role in everyday life, with its neural foundations being an ongoing subject of studyand its neural underpinnings remain an area of ongoing

research. The hippocampus, particularly crucial to memoryfunction, remains central to this research notably integral to memory, continues to be a primary focus of this investigation [1] [2] [3] [4] [5] [6] [7] [8] [9]. Understanding Gaining insights into the role

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of the hippocampus in working memory is essential to advancing our comprehension vital to deepening our understanding of cognitive processes, thereby promoting hence fostering the progression of cognitive training and interventions.

Current evidence points toward a briefsuggests a transient, synchronized oscillation, known-referred to as sharp-wave ripple (SWR) [10], being associated is linked with several cognitive functions. These include, such as memory replay [11] [12] [13] [14] [15], memory consolidation [16] [17] [18] [19], memory recall [20] [21] [22], and neural plasticity [23] [24]. This suggests that SWR may play a crucial part in evidence indicates the likelihood that SWR could be a critical component of hippocampal processing, contributing to the performance of working memory working memory performance. However, studies research investigating the effects of SWRs on working memory are limited [25]and focus primarily on rodent models engaged remains sparse [25], and is largely limited to rodent models participating in navigation tasks, without clear delineation where the timing of memory acquisition and recall timing is not explicitly distinguished.

Recent studies have illustrated indicate that hippocampal neurons present exhibit low-dimensional representations during WM tasks. Specifically Notably, the firing patterns of place cells [26] [27] [28] [29] [30], located in the hippocampus, appear are observed to be encompassed within a dynamic, nonlinear threedimensional hyperbolic geometry in rodent models [31] . Additionally rodents [31]. Moreover, grid cells in the entorhinal cortex (EC)—the main route dominant pathway to the hippocampus [32] [33] [34]—display a displayed toroidal topology during exploration [35]. Regrettably, these studies are limited Unfortunately, these investigations are confined to spatial navigation tasks in rodents, affecting thus imposing limitations on the temporal resolution of WM tasks. The application applicability of these findings to human subjects and their extension generalization beyond navigation tasks are still unconfirmed remains to be established.

In light of these points, the present study seeks to corroborate Given these considerations, the current study aims to validate the hypothesis that hippocampal neurons portray unique exhibit distinctive representations in low-dimensional spaces, referred to designated as 'neural trajectory,' particularly during SWR periods

in WM tasks. To test this proposition, we used a dataset from during WM tasks, most prominently within SWR periods. To evaluate this claim, we employed a dataset of patients performing an eight-second Sternberg task with high temporal resolution (1 second s for fixation, 2 seconds s for encoding, 3 seconds s for maintenance, and 2 seconds s for retrieval) with a high temporal resolution, while their intracranial electroencephalography signals (iEEG) signals in within the medial temporal lobe (MTL) were being monitored [36]. To explore the investigate low-dimensional neural trajectories, we utilized the employed Gaussian-process factor analysis (GPFA), a recognized technique for examining method renowned for analyzing neural population dynamics [37].

1. Methods

1.1. Dataset

A public dataset [36] comprising experiments from publicly available dataset [36] was used, which consists of nine epilepsy patients was taken into consideration for this study. The patients were tasked with executing performing a modified Sternberg taskwhich included This task involves four phases: fixation (1s), encoding (2s), maintenance (3s), and retrieval (2s) [36]. During the encoding phase, participants were presented with exposed to four, six, or eight alphabet letters, known-referred to as the set size. Subsequently, they had to ascertain decide whether a probe letter revealed presented during the retrieval phase was displayed earlier (the suitable previously displayed (the correct choice for the Match IN task) or not (the suitable correct choice for the Mismatch OUT task). iEEG signals were registered via recorded at a sampling rate of 32 kHz, within a frequency spectrum range of 0.5-5,000 Hz, utilizing using depth electrodes implanted in the medial temporal lobe (MTL) regions: the anterior head of the left and the right hippocampus (AHL and AHR), the posterior body of the hippocampus (PHL and PHR), the entorhinal cortex (ECL and ECR), and the amygdala (AL and AR), as illustrated in Figure 1A and Table 1). The recorded. The iEEG signals were subsequently downsampled to a rate of 2 kHz. The interrelationship Correlations among variables such as set size and correct rate were explored investigated (Figure ??S1). The timings of multiunit spikes were identified using determined by a spike sorting algorithm [38] with using the Combinato package (https://github.com/jniediek/combinato)(Figure 1C).

1.2. Calculation of neural trajectories using GPFA

Neural trajectories, colloquially called also termed 'factors' (Figure 1D), in the hippocampus, EC, and amygdala (Figure 1D)were calculated utilizing GPFA [37], which was were computed using GPFA [37] applied to the multiunit activity data radiating from for each session. The computations were GPFA was performed with the elephant package (https://elephant.readthedocs.io/en/latest/reference/gpfa.html). The bin size was set at to 50 ms, with no overlaps. Each factor was znormalized across all sessions. The Euclidean distance from the origin (O) was subsequently then calculated (Figure 1E).

For each trajectory inside within a region, for exampleinstance, AHL, geometric medians (i.e., g_F for fixation, g_E for encoding, g_M for maintenance, and g_R for retrieval phase) were calculated by finding determined by calculating the median coordinates of the trajectory during the four phases (Figure 1D). An optimal dimensionality for GPFA was identified as three using the elbow method, which was derived by investigating the log-likelihood values through a three-fold cross-validation technique approach (Figure 2B).

1.3. Identifying SWR candidates from areas of the hippocampushippocampal regions

Potential SWR instances from events within the hippocampus were identified via an detected using a widely accepted method [39]. LFP signals from a given region of interest (ROI), such as AHL, were re-referenced by subtracting a calculated average an averaged signal from locations outside the ROI (e.g.e.g., AHR, PHL, PHR, ECL, ECR, AL, and AR) (see Figure 1A). The re-referenced LFP signals were further then filtered with a ripple-band filter (80–140 Hz) to detect identify SWR candidates (=SWR⁺ candidates) (see Figure 1B). SWR detection was carried out conducted using a published tool (https://github.com/Eden-Kramer-Lab/ripple_detection) [40], with the bandpass range adjusted to 80–140 Hz in line with human requirements for humans [21] [22], as

opposed to the conventional different from the original 150–250 Hz range typically applied to rodents.

Control events for SWR⁺ candidates, tagged labeled as SWR⁻ candidates, were identified by randomly shuffling the timestamps of SWR⁺ candidates randomly across all trials and subjects. The resultant resulting SWR⁺/SWR⁻ candidates underwent visual inspection (were then subjected to visual inspection, as shown in Figure 1).

1.4. Defining SWRs from alleged putative hippocampal CA1 regions

SWRs were distinguished from SWR candidates within likely in presumptive CA1 regions. Initially, these regions were designated defined as follows: SWR⁺/SWR⁻ candidates from in the hippocampus were mapped projected into a two-dimensional space based on the overlapping spike counts per unit using a supervised employing a supervised method using UMAP (Uniform Manifold Approximation and Projection) [41] (Figure 4A). Validation of the clustering was done Clustering validation was performed by computing the silhouette score [42] from the clustered samples (Table 2). Those areas Regions in the hippocampusscoring over, which scored above 0.6 on average across sessions (or the 75th percentile) were specified as likely (Figure 4B), were characterized as presumed CA1 regions, in turn, identifying five electrode positions across five participants from five patients (Table 3).

Those—SWR⁺/SWR⁻ candidates within—in the assumed CA1 regions were classified as SWR⁺/SWR⁻ and—had—, thus relinquishing their candidate statusrevoked. Log-normal distributions were observed in the—. The duration and ripple band peak amplitude of SWRs were observed to follow log-normal distributions (Figure 44C & E). Each SWR time period time period of SWR was partitioned relative to the time from the SWR center into pre- (at -800 to -300 ms from SWR center), mid- (at -250 to +250 ms), and post-post-SWR (at +300 to +800 ms) SWR-times.

1.5. Statistical evaluation

The Brunner–Munzel test and the Kruskal-Wallis test were performed using the SciPy package in Python [43]. A correlation analysis was executed Correlational analysis was performed by determining the rank of the

observed correlation coefficient in its associated setsize-shuffled surrogate using a custom Python script. The bootstrap test was conducted with implemented using an in-house Python script.

2. Results

2.1. iEEG recording and neural trajectory in MTL regions during a Sternberg task

We analyzed-leveraged a publicly available dataset for this study analysis [36]. This dataset consists of encompasses LFP signals (Figure 1A) from MTL regions (Table 1) obtained during a modified Sternberg task performance execution. We identified SWR⁺ candidates from LFP signals filtered through the 80-140 Hz ripple band (Figure 1B), originating across all hippocampal regions (refer to Methods). Correspondingly, SWR⁻ candidates were defined at the same timestampsbut shuffled between identical timestamps) but shuffled across different trials (Figure 1). dataset included multiunit spikes (Figure 1C) identified via a spike sorting algorithm [38]. Using By employing GPFA [37], and using the 50-ms binned multiunit activity with no overlaps, we determined the neural trajectories (or factors) of MTL regions per by session and region (Figure 1D). We normalized each factor by session and region, for instance, session #2 in AHL of subject #1. Subsequently, we calculated the Euclidean distance from the origin (O) (Figure 1E).

2.2. Correlation between hippocampal Hippocampal neural trajectory and correlation with a Sternberg taskperformance

Figure 2A shows illustrates the cloud of median neural trajectories of 50 trials within the three main factor spaces. We determined the optimal embedding dimension for the GPFA model to be three, using the elbow method (Figure 2B). The trajectory distance from the origin (O) (represented as $||g_F||$, $||g_E||$, $||g_M||$, and $||g_R||$) in the hippocampus was greater than the exceeded corresponding distances in the EC and amygdala (Figures 2C and D).

Similarly, we calculated computed the distances between the geometric medians of the four phases, namely $\|g_Fg_E\|$, $\|g_Fg_M\|$, $\|g_Fg_R\|$, $\|g_Eg_M\|$, $\|g_Eg_R\|$, and $\|g_Mg_R\|$. The results indicated that the hippocampus showed displayed larger distances between phases than both the EC and amygdala. ²

2.3. Memory load-dependence of load-dependent neural trajectory distance between encoding and retrieval states in the hippocampus

In the context terms of memory load in the Sternberg Stenberg task, we found-identified a negative correlation between the correct rate of trials and set size (the number of letters to encode) (Figure 3A).³ Similarly, we observed a positive correlation was observed between the response time and set size (Figure 3B).⁴.

Additionally, we observed Furthermore, we found a positive correlation between set size and the trajectory distance between the encoding and retrieval phases $(\log_{10}||g_Eg_R||)$ (Figure 3C).⁵. However, the distances between other combinations of phases did not show display statistically significant correlations (Figures 3D and S2).

2.4. Detection of hippocampal SWR from putative CA1 regions

To better localize For precision improvement in recording sites and improve SWR detection, we estimated the electrode position placements in the CA1 regions of the hippocampus using distinct multiunit

¹Hippocampus: Distance = 1.11 [1.01], median [IQR], n = 195,681 timepoints; EC: Distance = 0.94 [1.10], median [IQR], n = 133,761 timepoints; Amygdala: Distance = 0.78 [0.88], median [IQR], n = 165,281 timepoints.

 $^{^2}$ Hippocampus: Distance = 0.60 [0.70], median [IQR], n = 8,772 combinations; EC: Distance = 0.28 [0.52], median [IQR], n = 5,017 combinations (p < 0.01; Brunner–Munzel test); Amygdala: Distance = 0.24 [0.42], median [IQR], n = 7,466 combinations (p < 0.01; Brunner–Munzel test).

 $^{^3}$ Correct rate: set size four (0.99 ±0.11, mean ±SD; n = 333 trials) vs. set size six (0.93 ±0.26; n = 278 trials; p < 0.001, Brunner–Munzel test with Bonferroni correction) and set size eight (0.87 ±0.34; n = 275 trials; p < 0.05; Brunner–Munzel test with Bonferroni correction). Overall, p < 0.001 for Kruskal–Wallis test; correlation coefficient = -0.20, p < 0.001.

⁴Response time: set size four $(1.26 \pm 0.45 \text{ s}; n = 333 \text{ trials})$ vs. set size six $(1.53 \pm 0.91 \text{ s}; n = 278 \text{ trials})$ and set size eight $(1.66 \pm 0.80 \text{ s}; n = 275 \text{ trials})$. All comparisons p < 0.001, Brunner–Munzel test with Bonferroni correction; p < 0.001 for Kruskal–Wallis test; correlation coefficient = 0.22, p < 0.001

⁵Correlation between set size and $\log_{10}(\|\mathbf{g}_{\mathrm{E}}\mathbf{g}_{\mathrm{R}}\|)$: correlation coefficient = 0.05, p < 0.001. Specific values: $\|\mathbf{g}_{\mathrm{E}}\mathbf{g}_{\mathrm{R}}\| = 0.54$ [0.70] for set size four, n = 447; $\|\mathbf{g}_{\mathrm{E}}\mathbf{g}_{\mathrm{R}}\| = 0.58$ [0.66] for set size six, n = 381; $\|\mathbf{g}_{\mathrm{E}}\mathbf{g}_{\mathrm{R}}\| = 0.61$ [0.63] for set size eight, n = 395.

spike patterns during the SWR events. We embedded SWR+/SWR- candidates from each every session and hippocampal region were embedded in a two-dimensional space via using UMAP (Figure 4A). The quality of clustering was verified using. We used the silhouette score as a metric for quality of clustering (Figure 4B and Table 2). Recording sites vielding with an average silhouette score over exceeding 0.6 across all sessions were designated identified as putative CA1 regions. (Tables 2 and 3). We found identified five putative CA1 regions, out of which four weren't four of which were not labeled as seizure onset zones (Table 1).

We further labeled Subsequently, SWR+/SWR- candidates within these putative CA1 regions were labeled as SWR+ and SWR-, respectively⁸ (Table 3). Both SWR+ and SWR- exhibited equal durationthe same duration⁹ (Figure 4C) due to their definitions, and adopted followed a log-distribution. There was an increase We observed an augmentation in SWR+ incidence within the first during the initial 400 ms of the retrieval phase¹⁰ (Figure 4D). The peak ripple band amplitude of SWR+ was greater than that of outpaced SWR- and followed a log-normal distribution (Figure 4E).¹¹.

2.5. Transient changes in hippocampal neural trajectories trajectory during SWRevents

We ealeulated computed the distance of the trajectory from the origin (O) during SWR events in both the encoding and retrieval phases (Figure 5A). Observing an the increase in distance during SWR as shown in Figure 5A, we elassified differentiated each SWR into three stages: pre-, mid-, and post-SWR. Consequently Therefore, the distances from O during these SWR stages are denoted those SWR periods are identified as ||pre-eSWR+||, ||mid-eSWR+|| among others.

The ||mid-eSWR⁺||¹² was larger greater than ||pre-eSWR⁺||¹³, and ||mid-rSWR⁺||¹⁴ was bigger larger than ||pre-rSWR⁺|| in both Match IN and Mismatch OUT tasks.¹⁵.

2.6. Visualization of hippocampal neural trajectories trajectory during SWR in two-dimensional spaces

Following our observations on of neural trajectory 'jumping' during a SWR event SWR (Figure 5), we visualized the three-dimensional trajectories of pre-, mid-, and post-SWR events during the encoding and retrieval phases (Figure 6), the distance between which was found to depend on memory load be memory-load dependent (Figure 3).

To enable provide two-dimensional visualization, we linearly aligned peri-SWR trajectories by assigning g_E at the origin (0, 0) and g_R at $(\|g_Eg_R\|, 0)$. We then Post this, we rotated these aligned trajectories around the g_Eg_R axis (the x-axis). This method ensured that Thus, the distances from the origin in the original three-dimensional spaces were are preserved in the two-dimensional counterparts equivalent.

The scatter plot within these two-dimensional spaces illustrate reveals characteristic distributions of peri-SWR trajectories based on the phases and types of task. One can observe, for example, phases and task types. For instance, one can observe that the magnitude of ||mid-eSWR⁺|| surpasses that of ||pre-eSWR⁺|| (Figure 6B), which is consistent with our earlier findings (Figure 5).

2.7. Directionality Fluctuations of hippocampal neural trajectories between encoding and retrieval states

We then investigated the Next, we examined trajectory directions of the trajectories in relation to $\overline{g_Eg_R}$. The directions of SWRs were defined by the neural trajectory at -250 ms and +250 ms from their center, namely i.e., \overline{eSWR}^+ .

⁶Consider the AHL in session #1 of subject #1, for illustration purposes.

⁷The designated identified regions were: AHL of subject #1, AHR of subject #3, PHL of subject #4, AHL of subject #6, and AHR of subject #9.

⁸These definitions resulted in led to equal counts for both categories: SWR^+ (n = 1,170) and SWR^- (n = 1,170).

⁹These definitions resulted in led to equal durations for both categories: SWR⁺ (93.0 [65.4] ms) and SWR⁻ (93.0 [65.4] ms).

¹⁰The occurrence of SWR⁺ increased against the bootstrap sample; 95th percentile = 0.42 [Hz]; p < 0.05.

¹¹SWR⁺ (3.05 [0.85] SD of baseline, median [IQR]; n = 1,170) vs. SWR⁻ (2.37 [0.33] SD of baseline, median [IQR]; n = 1,170; p < 0.001; Brunner–Munzel test).

 $^{^{12}}$ 1.25 [1.30], median [IQR], n = 1,281, in Match IN task; 1.12 [1.35], median [IQR], n = 1,163, in Mismatch OUT task

¹³1.08 [1.07], median [IQR], n = 1,149, in Match IN task; 0.90 [1.12], median [IQR], n = 1,088, in Mismatch OUT task

 $^{^{14}1.32}$ [1.24], median [IQR], n = 935, in Match IN task; 1.15 [1.26], median [IQR], n = 891, in Mismatch OUT task

 $^{^{15}1.19}$ [0.96], median [IQR], n = 673, in Match IN task; 0.94 [0.88], median [IQR], n = 664, in Mismatch OUT task

We calculated the density of $\overrightarrow{eSWR} \cdot \overrightarrow{g_Eg_R}$, $\overrightarrow{rSWR} \cdot \overrightarrow{g_Eg_R}$, and $\overrightarrow{eSWR} \cdot \overrightarrow{rSWR}$ (Figures 7A–D). The rSWR \cdot $\overrightarrow{g_Eg_R}$ demonstrated displayed a biphasic distribution.

By comparing taking the difference between the distribution of $\overrightarrow{rSWR}^{\perp} \cdot \overrightarrow{g_Eg_R}$ (Figures 7A and B) with and that of $\overrightarrow{rSWR}^{\perp} \cdot \overrightarrow{g_Eg_R}$ (Figures 7C and D), we computed the contributions of SWR (Figures 7E and F), which indicated revealed a shift in the direction of $\overrightarrow{g_Eg_R}$ (Figures 7E and F: red rectangles).

Furthermore, and only Moreover, exclusively in the Mismatch OUT task, eSWR⁺ · rSWR⁺ was less than eSWR⁻ · rSWR⁻ (baseline periods) (Figure 7F: pink circles). Put simply In simpler terms, eSWR and rSWR pointed in opposite directions the opposite direction only in the Mismatch OUT task but not in the Match IN task (Figure 7E: pink circles).

3. Discussion

4. Discussion

This study posits that hippocampal neurons generate distinct trajectories hypothesized that within lowdimensional spaces during a working memory (WM) task in humans, specifically hippocampal neurons form unique trajectories, particularly during sharp-wave ripple (SWR) periods. Initially, the multiunit spikes in the medial temporal lobe (MTL) regions were projected onto three-dimensional spaces during a Sternberg task using Gaussian Process Factor Analysis (GPFA) (Figure 1D-E and Figure 2A). The trajectory distance distance of the trajectory across WM phases (||g_Fg_E||, $\|g_F g_M\|$, $\|g_F g_R\|$, $\|g_E g_M\|$, $\|g_E g_R\|$, and $\|g_M g_R\|$) was markedly notably larger in the hippocampus than in the EC and amygdala (Figure 2E), which implies indicating dynamic neural activity in the hippocampus during the WM task. Additionally Further, in the hippocampus, the trajectory distance between the encoding and retrieval phases (||g_Eg_E||) was found to positively correlate exhibited a positive correlation with memory load (Figure 3C-D), denoting reflecting WM processing. The hippocampal neural trajectory momentarily increased was found to increase transiently during SWRs (Figure 5). Eventually Finally, the hippocampal neural trajectory alternated switched between encoding and retrieval states, progressing specifically moving from encoding to retrieval during SWR events (Figure 7). Such discoveries not only interpret varying aspects These findings not only explain various facets of hippocampal neural activity during a WM task in humans, but also offer fresh new insights into how SWRs help alter influence the switch in neural states.

Our findings show We found that the distance of hippocampal the neural trajectory across the phases ; even after was greater in the hippocampus compared to that in the EC and amygdala, even when considering the distance from O in these regions $\frac{1}{2}$ surpassed that in the EC and amygdala (Figure 2C-E). This reaffirms the participation supports the involvement of the hippocampus in the WM task, coinciding with prior assertions aligning with previous reports of hippocampal persistent firing during the maintenance phase [3] [4] [5] [6]. However, when applying we applied GPFA to multiunit activity during a 1second level resolution of the WM task, we noticed observed that the neural trajectory in low-dimensional space demonstrated showed a memory-load dependence between dependency between the encoding and retrieval phases, denoted symbolized as $\|g_E g_R\|$ (Figure 3). This supports the association between the hippocampus and These findings corroborate the association of the hippocampus with WM processing.

Our analysis focused on was confined to putative CA1 regions (Figure 4), which is supported by various contributions was bolstered by several factors. This specific concentration arises from well-established observations where SWRs coincide with spike clusters focus stems from established observations that SWRs synchronize with spike bursts of interneurons and pyramidal neurons [44] [45] [46] [47], potentially within a 50 μ m radius of the recording site [48]. increase in the instances of SWRs was identified We further identified an increased incidence of SWRs during the first 0-400 ms of the retrieval phase (Figure 4D). This observation aligns with earlier reports of increased SWR occurrence before finding harmonizes with previous reports of heightened SWR occurrence preceding spontaneous verbal recall [21] [22], reinforcing our findings supporting our results under a triggered retrieval condition. The observed log-normal distributions of both SWR length-duration and ripple band peak amplitude observed in this study (Figure 4C & E) concur with the field's consensus [39]. Consequently, confining recordings is in accordance with the consensus in this field [39]. As a result, our decision to restrict recording sites to putative CA1 regions likely improved contributed to enhancing the accuracy of SWR detection. However, the observed increase in trajectory distance from O during SWRs (Figure 5) may be skewed higher might have been skewed towards higher values due to channel selection. Nevertheless However, this potential bias does not significantly undermine our primary conclusions substantially challenge our primary findings.

Interestingly, during the retrieval phase, trajectory directions alternated the trajectory directions oscillated between encoding and retrieval states both during during both baseline and SWR periods (Figure 7C & D). Furthermore Moreover, the balance of this oscillation transitioned shifted from encoding to retrieval state during SWR episodes events (Figure 7 E & F). These outcomes align with preceding reports regarding results are consistent with previous reports on the role of SWRs SWR in memory retrieval [21] [22]. Our findings suggest a novel understandingwhere highlight a new understanding, suggesting that SWRs occur when the hippocampal representation transitions from encoding to retrieval states, thereby revealing unexplored. Therefore, these results reveal novel aspects of hippocampal representations, such as including (i) neuronal oscillation between encoding and retrieval phases states during a WM task, and (ii) SWR functioning as a catalyst serving as a trigger for changing neural states.

MoreoverFurthermore, our study identified uncovered WM-task type-specific differences between encoding- and retrieval-SWRs (Figure 7E-F)specific to WM-task types. Notably, counter opposing movements of encoding-SWR (eSWR) and retrieval-SWR (rSWR) were not seen observed in the Match IN task but were evident apparent in the Mismatch OUT task. These observations can be explained by the memory engram theory can explain these observations [49]. The [49]. Particularly, the Match In task, for instance, presented participants with previous letters, whereas provided participants with previously presented letters, contrastingly, the Mismatch OUT task introduced a new letter absent not present in the encoding phase. These interpretations highlight the vital underscore the significant role of SWR in human cognitive processes.

In conclusion, this the present investigation demon-

strated that during a WM task, hippocampal activity oscillates between encoding and retrieval states uniquely transitioning during a WM task and uniquely transitions from encoding to retrieval during SWR eventsincidents. These findings offer valuable insights provide meaningful insight into the neural substrates and workings counterparts and functionality of working memory within in the hippocampus.

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Contributors

Y.W. and T.Y. conceptualized the study; Y.W. performed the data analysis; Y.W. and T.Y. wrote the original draft; and all authors reviewed the final manuscript.

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Declaration of Interests

The authors declare that they have no competing interests.

Data and code availability

The data is available on G-Node (https://doi.gin.g-node.org/10.12751/g-node.d76994/).

The source code is available on GitHub (https://github.com/yanagisawa-lab/hippocampal-neural-fluctuation-during-a-WM-task-in-humans).

Inclusion and Diversity Statement

We support inclusive, diverse, and equitable conduct of research.

Declaration of Generative AI in Scientific Writing

The authors employed ChatGPT, provided by OpenAI, for enhancing the manuscript's English language quality. After incorporating the suggested improvements, the authors meticulously revised the content. Ultimate responsibility for the final content of this publication rests entirely with the authors.

Tables

Subject ID	of sessions	AHL	AHR	PHL	PHR	ECL	ECR	AL	AR	SOZ
1	4	O	X	О	О	O	х	О	х	"AHR, LR"
2	7	0	o	0	0	0	0	o	o	"AHR, PHR"
3	3	0	0	0	0	0	0	o	x	"AHL, PHL"
4	2	o	o	o	o	0	o	o	o	"AHL, AHR, PHL, PHR"
5	3	0	X	X	0	X	X	o	X	DRR
6	6	o	o	o	o	o	o	o	o	"AHL, PHL, ECL, AL"
7	4	0	0	0	0	0	0	0	o	"AHR, PHR"
8	5	o	o	o	o	o	O	o	o	ECR
9	2	o	o	o	o	o	o	0	0	"ECR, AR"

 $Table\ 1 - \underline{Electrode\ Distribution\ within\ the\ Dataset} \quad Distribution\ of\ Electrodes\ within\ the\ Dataset$

The This figure outlines represents the electrode placements and the seizure onset zones. Areas labelled Regions designated with "o" are included were available in the dataset, while whereas those indicated by marked with "x" (navy) are absentwere not present. Denoted abbreviations Abbreviations include: AHL, left hippocampal head; AHR, right hippocampal head; PHL, left hippocampal body; PHR, right hippocampal body; ECL, left entorhinal cortex; ECR, right entorhinal cortex; AL, left amygdala; AR, right amygdala; and SOZ refers to symbolizes the seizure onset zone.

Subject	AHL	AHR	PHL	PHR	
1	0.60 ± 0.14	n.a.	n.a.	0.1 ± 0	
2	0.21 ± 0.16	0.17 ± 0.21	0.18 ± 0.22	0.20 ± 0.15	
3	0.40 ± 0.42	0.83 ± 0.12	n.a.	n.a.	
4	0.10 ± 0.00	0.10 ± 0.00	0.90 ± 0.00	0.10 ± 0.14	
5	n.a.	n.a.	n.a.	n.a.	
6	0.63 ± 0.06	n.a.	n.a.	0.27 ± 0.06	
7	0.10 ± 0.00	0.35 ± 0.35	0.37 ± 0.47	0.10 ± 0.00	
8	0.13 ± 0.10	n.a.	0.28 ± 0.49	n.a.	
9	n.a.	0.85 ± 0.07	0.15 ± 0.07	n.a.	

Table 2 – Silhouette scores of UMAP clustering for SWR^+ candidates and SWR^- candidates Silhouette score of UMAP clustering for SWR^+ candidates and SWR^- candidates

The silhouette scores (mean \pm SD across sessions per subject) pertaining to for UMAP clustering of SWR+ candidates and SWR candidates are calculated and presented in (Figure 4A. These calculations are) were calculated based on their corresponding multiunit spike patterns , where the (mean values observed are were 0.205 with a standard deviation of [0.285. The-], median and interquartile range are also presented (see [IQR]; Figure 4B).

Subject ID	of sessions	of trials	ROI	of SWRs	SWR incidence [Hz]
1	2	100	AHL	274	0.34
3	2	97	AHR	325	0.42
4	2	99	PHL	202	0.26
6	2	100	AHL	297	0.37
9	2	97	AHR	72	0.09
Total = 10	Total = 493	"Total = 1,170"	$0.30 \pm 0.13 \text{ (mean } \pm \text{SD)}$		

Table 3 – Accounting for Specific SWR Events Accounting for Defined SWR Events

The table compiles collates statistics related to assumed of putative CA1 regions and SWR events. To minimize sampling bias, only Only the initial first two sessions (sessions 1 and 2) from each subject were utilized considered to minimize sampling bias.

Figures

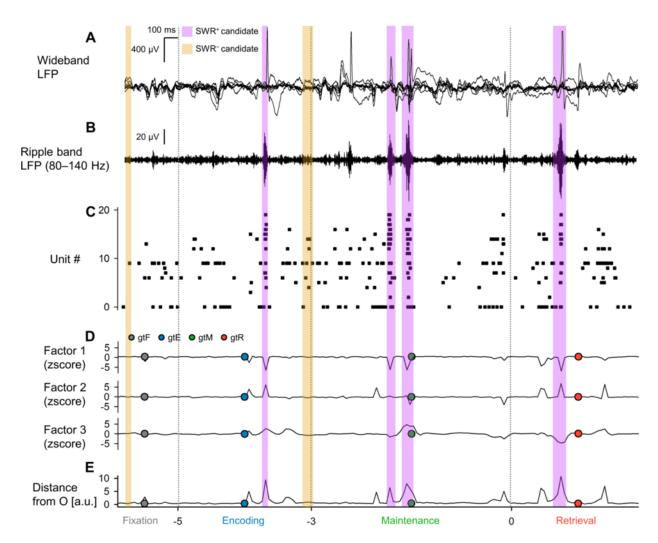


Figure 1 – Local Field Potentials (LFP), Multiunit Activity, and Neural Trajectories in the Hippocampus During a Modified Sternberg Task

A. These traces show representative wideband LFP intracranial EEG (iEEG) signals recorded from the left hippocampal head. The subject performed a modified Sternberg working memory task, which includes fixation (1 s, gray), encoding (2 s, blue), maintenance (3 s, green), and retrieval (2 s, red). **B.** We then present the corresponding ripple band LFP traces. **C.** The raster plot depicts multiunit spikes taken from the LFP traces, sorted using a spike algorithm [38]. **D.** Subsequently, we illustrate the neural trajectories, which are calculated by GPFA on spike counts per unit with 50-ms bins. Each phase's geometric median is marked by the dot circles. **E.** The trajectory's distance from the origin **O** is portrayed, with purple and yellow rectangles indicating the timings for SWR⁺ candidates and SWR⁻ candidates (considered as controls for SWR⁺), respectively.

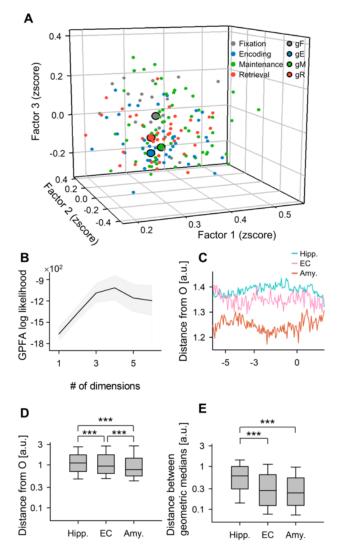


Figure 2 – State-Dependent Trajectories of Hippocampal Neurons

A. Neural trajectories within the initial three-dimensional factors derived from the Gaussian Process Factor Analysis (GPFA) are displayed. The smaller dots correspond to coordinates of 50-ms neural trajectory bins, while the larger dots with black edges signify the geometric medians for respective stages in the Sternberg working memory task: fixation (gray), encoding (blue), maintenance (green), and retrieval (red). B. The figure conveys the log-likelihood of the GPFA models versus the count of dimensions used to embed multiunit spikes found in the medial temporal lobe (MTL) territories. In specific, the elbow method pinpointed the optimal dimension to be three. C. This panel illustrates the distance of the neural trajectories from the origin (O) for the hippocampus (Hipp.), entorhinal cortex (EC), and amygdala (Amy.), against the time elapsed from the probe onset. D. The distance of the trajectory from O within MTL regions is displayed. The hippocampus shows the farthest distance, followed by the EC and the Amygdala. E. The plot represents inter-phase trajectory distances within the MTL regions. Abbreviations:

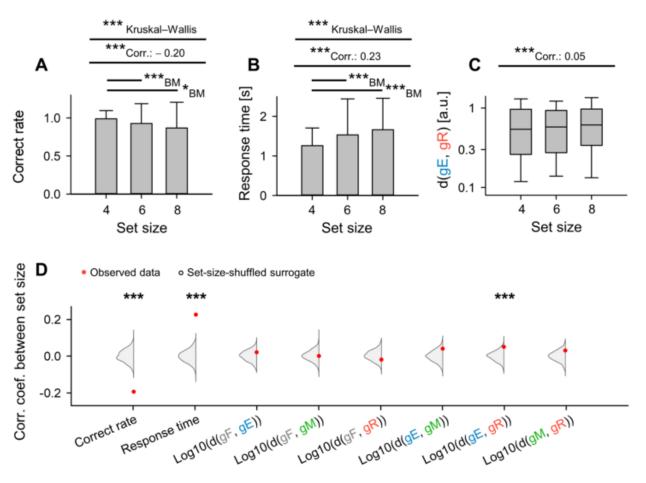


Figure 3 - Dependency of Trajectory Distance on Memory Load: Encoding and Retrieval States in Hippocampus

A. The relationship between set size (number of letters that need to be encoded) and correct rate in the working memory task (coefficient = -0.20, ***p < 0.001). **B.** The correlation between set size and response time (coefficient = 0.23, ***p < 0.001). **C.** The impact of set size on the inter-phase distances between the encoding and retrieval phases ($\|g_Eg_R\|$) (correlation coefficient = 0.05). **D.** Red dots represent experimental observations of correlations between set size and the following parameters: correct rate, response time, $\log_{10} \|g_Fg_E\|$, $\log_{10} \|g_Fg_R\|$, $\log_{10} \|g_Fg_R\|$, $\log_{10} \|g_Eg_R\|$, $\log_{10} \|g_Eg_R\|$, and $\log_{10} \|g_Mg_R\|$. The gray kernel density plot illustrates the corresponding set-size-shuffled surrogate (n = 1,000) (***ps < 0.001).

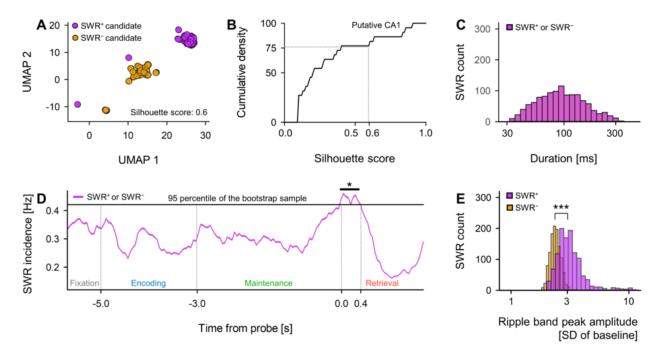


Figure 4 – Detection of SWRs in Presumptive CA1 Regions

A. Two-dimensional UMAP (Uniform Manifold Approximation and Projection) [41] projection of multiunit spikes during SWR⁺ candidates (*purple*) and SWR⁻ candidates (*yellow*). B. Cumulative density plot shows silhouette scores, indicative of UMAP clustering quality, for hippocampal regions (see Table 2 for reference). Note that hippocampal regions with silhouette scores greater than 0.60 (equivalent to the 75th percentile) were identified as possible CA1 regions. SWR⁺ and SWR⁻ candidates recorded from these speculative CA1 regions were respectively classified as SWR⁺ and SWR⁻ (*ns* = 1,170). C. The identical distributions of durations are presented for SWR⁺ (*purple*) and SWR⁻ (*yellow*), owing to their definitions (93.0 [65.4] ms, median [IQR]). D. SWR incidence for both SWR⁺ (*purple*) and SWR⁻ (*yellow*) obtained relative to the probe's timing is illustrated as a mean ±95% confidence interval. However, as the intervals may not be visible due to their narrow range, note that a significant increase in SWR incidence was detected during the initial 400 ms of the retrieval phase (0.421 [Hz], *p < 0.05, bootstrap test). E. The distributions of ripple band peak amplitudes for SWR⁻ (*yellow*; 2.37 [0.33] SD of baseline, median [IQR]) and SWR⁺ (*purple*; 3.05 [0.85] SD of baseline, median [IQR]) are delineated (***p < 0.001, the Brunner–Munzel test).

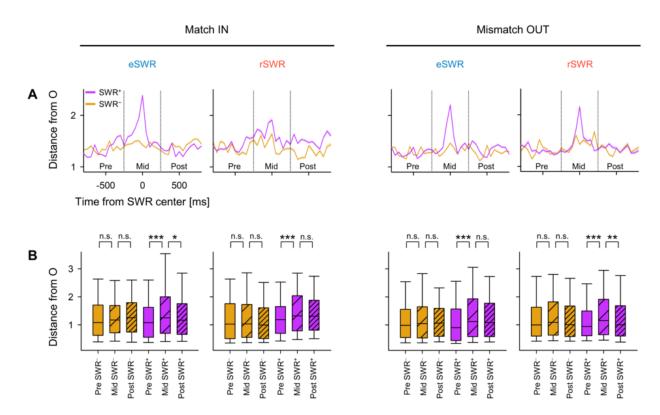
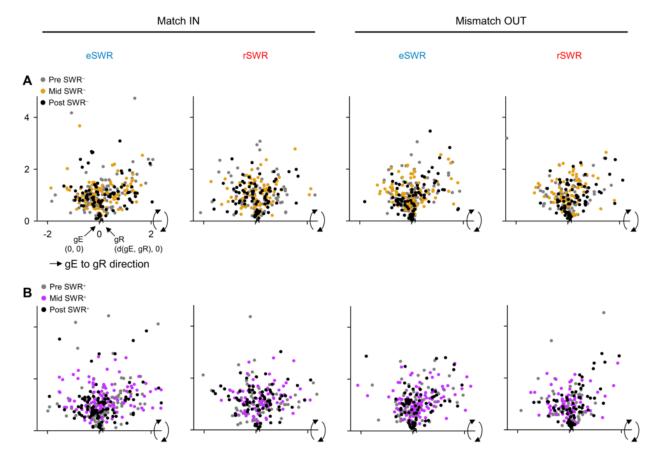


Figure 5 - Transient Alterations in Neural Trajectory During SWR Events

A. Displayed is the distance from origin (O) of the peri-sharp-wave-ripple trajectory (mean $\pm 95\%$ confidence interval). The intervals may not be apparent due to their slender ranges. **B.** Shown is the distance from the origin (O) during pre-, mid-, and post-SWR periods (*p < 0.05, **p < 0.01, ***p < 0.001; assessed using the Brunner–Munzel test). Abbreviations: SWR, sharp-wave ripple events; eSWR, SWR during the encoding phase; rSWR, SWR while in the retrieval phase; SWR⁺, positive SWR event; SWR⁻, control events for SWR⁺; pre-, mid-, or post-SWR denote the time intervals from -800 to -250 ms, from -250 to +250 ms, or from +250 to +800 ms, all relative to the center of the SWR.



 $Figure\ 6-\ Visualization\ of\ Neural\ Trajectories\ during\ SWR\ in\ Two-Dimensional\ Spaces$

The panels display hippocampal neural trajectories during SWR as projected onto two-dimensional spaces. *A.* Indicates hippocampal neural trajectories pre-SWR⁻ (gray), mid-SWR⁻ (yellow), and post-SWR⁻ (black). *B.* Represents the equivalents for SWR⁺ as opposed to SWR⁻. The $\|g_Eg_R\|$ varied among sessions. The projection was applied in the following manner: First, a linear transformation positioned g_E at the origin O (0,0), and g_R at ($\|g_Eg_R\|$, 0). The point cloud was then rotated around the g_Eg_R axis (equivalent to the x axis) for fitting into two-dimensional spaces. Therefore, within these two-dimensional spaces, both the distances from O and the angles preserved the original makeup of the g_Eg_R axis from the original three-dimensional spaces. Abbreviations: SWR signifies sharp-wave ripple events; eSWR denotes SWR during the encoding phase; rSWR indicates SWR during the retrieval phase; SWR⁺, marks an SWR event; SWR⁻ refers to control events for SWR⁺; pre-SWR, mid-SWR, or post-SWR, reference the time intervals from -800 to -250 ms, from -250 to +250 ms, or from +250 to +800 ms from the center of SWR.

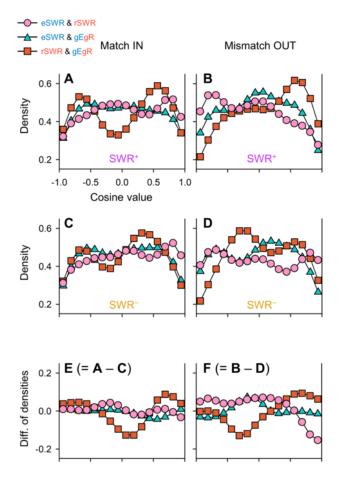


Figure 7 – Directions of Neural Trajectories during SWRs Based on Encoding and Retrieval States

A-B Kernel density estimation (KDE) distributions of $\overrightarrow{eSWR^+} \cdot \overrightarrow{rSWR^+}$ ($pink\ circles$), $\overrightarrow{eSWR^+} \cdot \overrightarrow{g_Eg_R}$ ($blue\ triangles$), and $\overrightarrow{rSWR^+} \cdot \overrightarrow{g_Eg_R}$ ($red\ rectangles$) in Match In (A) and Mismatch OUT tasks (B). C-D Present the corresponding distributions of SWR $^-$ instead of those of SWR $^+$ in A and B. E-F Depict the differences in the distributions of SWR $^+$ and SWR $^-$, illuminating the SWR components (E = C - A; F = D - B). Note the biphasic distributions of $\overrightarrow{rSWR^+} \cdot \overrightarrow{g_Eg_R}$, suggesting fluctuations between the encoding and retrieval states during the Sternberg task. Moreover, inverse directionality between $\overrightarrow{eSWR^+}$ and $\overrightarrow{rSWR^+}$ was observed ($pink\ circles$) in the Mismatch OUT task, but not in the Match IN task E-F). Finally, shifts from the retrieval to encoding states were evident in the SWR components in both the Match IN and Mismatch OUT tasks ($red\ rectangles$ in E and F).