

Highlights

- Neural trajectories in the hippocampus exhibited greater variability during a working memory (WM) task compared to those in the entorhinal cortex and amygdala regions.
- The distance of neural trajectories between encoding and retrieval states in the hippocampus was memory-load dependent during a WM task.
- Hippocampal neural trajectories fluctuated between the encoding and retrieval states in a task-dependent manner during both baseline and sharp-wave ripple (SWR) periods.
- Hippocampal neural trajectories shifted from encoding to retrieval states during SWR period.

Hippocampal neural fluctuations between memory encoding and retrieval states during a working memory task in humans: Encoding-to-retrieval shift during sharp-wave ripples

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Abstract

Working memory (WM) is crucial to various cognitive functions, yet its neural mechanisms remain largely elusive. Emerging interest focuses on the roles of the hippocampus and sharp-wave-ripple ~~sharp wave-ripple~~ complexes (SWRs) – transient, synchronous neural events in the hippocampus – in memory consolidation and retrieval, however, their relationship to WM tasks remains ambiguous. Recent studies propose that multiunit activity patterns in the hippocampus may operate concurrently with SWRs, exhibiting distinct dynamics during WM tasks. We performed an analysis of an electroencephalogram dataset from the medial temporal lobe (MTL) ~~nine epilepsy patients in~~ nine patients with epilepsy during an eight-second Sternberg task. Low-dimensional neural representations, or 'trajectories', within the MTL were extracted using Gaussian-process factor analysis as the WM task ~~– was performed~~. The results show that significant differences in neural trajectories exist in the hippocampus compared to the entorhinal cortex and amygdala. Additionally, the divergence in trajectories between the encoding and retrieval phases ~~on memory load~~, appears to be memory load-dependent. Interestingly, hippocampal trajectories fluctuate during the retrieval phase, indicating task-dependent shifts between encoding and retrieval states ~~– occurring during both~~ base-line and SWR events. These shifts from encoding to retrieval states are synchronized with the presence of SWRs, highlighting the critical function of the hippocampus in WM tasks ~~and a new~~. This finding suggests a novel hypothesis: the hippocampus modulates its functional state from encoding to retrieval ~~during in the event of~~ SWRs.

Keywords: working memory, WM, memory load, hippocampus, sharp-wave ripples, SWR, humans

1. Introduction

Working memory (WM) plays a ~~crucial role in~~ everyday life, yet its underlying neural mechanisms remain to be fully elucidated critical role in our daily activities, but the neural mechanisms underlying it are not completely understood. Particularly, the function of the hippocampus, a vital brain region contributing to memory, commands key brain region involved in memory, warrants ongoing investigation [1, 2, 3, 4, 5, 6, 7, 8, 9]. ~~Gaining insight into the role~~ Enhancing

our understanding of the hippocampus's role in working memory ~~fosters a deeper understanding of cognitive processes and facilitates can lead to deeper insights into cognitive processes, thereby promoting~~ the development of cognitive training strategies and interventions.

~~Transient and synchronous oscillations, referred to as sharp~~ Sharp wave ripples (SWR), ~~are known to be associated with various transient and synchronous oscillations generated by the hippocampus, are associated with key~~ cognitive functions, including memory replay [10, 11, 12, 13], memory consolidation [14, 15, 16, 17], memory recall [18, 19, 20], and

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neural plasticity [21, 22]. ~~Therefore, SWR might constitute a fundamental aspect of processing in the hippocampus and contribute to~~ Consequently, SWRs could be critical to hippocampal processing and influence working memory performance. However, studies ~~investigating the effects examining the influence~~ of SWRs on working memory ~~remain scarce [23], and are predominantly limited to rodent models using navigation tasks, in which the exact timings of memory acquisition and recall are not distinguished.~~ are scarce [23] and primarily center on rodent models utilizing navigation tasks. Such research has not clearly differentiated between the specific timing of memory recall and acquisition.

~~Further~~ Moreover, it has been ~~discovered found~~ that hippocampal neurons ~~exhibit present~~ low-dimensional representations during WM tasks. ~~For instance, the The~~ firing patterns of place cells [24, 25, 26, 27, 28, 29] in the hippocampus ~~are embedded within, for instance,~~ align with a dynamic, nonlinear three-dimensional hyperbolic geometry in rodents [30]. ~~Moreover Similarly,~~ grid cells in the entorhinal cortex (EC) ~~the primary gateway the main entry point~~ to the hippocampus [31, 32, 33] ~~displayed display~~ a toroidal topology during exploration [34]. ~~Nevertheless, these experiments are again constrained~~ However, these studies primarily relate to spatial navigation tasks in rodents, ~~limited in and provide limited~~ temporal resolution for WM tasks. Additionally, it ~~has yet to be investigated whether these findings can be generalized to humans and is still uncertain whether these results apply to humans or to~~ tasks beyond navigation.

In light of these considerations, this study ~~explores tests~~ the hypothesis that hippocampal neurons ~~exhibit distinct representations in demonstrate distinct~~ low-dimensional spaces ~~as a 'neural trajectory' representations, or 'neural trajectories',~~ during WM tasks, ~~with a particular emphasis on specifically during~~ SWR periods. To ~~test this hypothesis, we utilized investigate this, we used~~ a dataset of patients performing an eight-second Sternberg task (with high temporal resolution: 1 s for fixation, 2 s for encoding, 3 s for maintenance, and 2 s for retrieval) while their intracranial electroencephalography signals (iEEG) in the medial temporal lobe (MTL) were ~~being recorded~~ [35]. We ~~employed implemented~~ Gaussian-process factor analysis (GPFA) ~~based on multiunit activities on~~

multichannel unit activity to explore low-dimensional neural trajectories, a ~~known tool for analyzing proven method to analyze~~ neural population dynamics [36].
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2. Methods

2.1. Dataset

We ~~utilized a A~~ publicly accessible dataset [35] ~~wherein was utilized [35], which included~~ nine epilepsy patients ~~performed performing~~ a modified Sternberg task comprising the ~~following subsequent~~ four phases: fixation (1 s), encoding (2 s), maintenance (3 s), and retrieval (2 s) [35]. During the encoding phase, participants were ~~presented with shown~~ sets of four, six, or eight alphabetical letters, ~~which we refer to denoted herein~~ as the set size. ~~Subsequently, participants task was to determine~~ During the retrieval phase, participants were required to ascertain whether a probe letter ~~presented during the retrieval phase~~ had been previously ~~displayed shown~~ (the correct choice for the Match IN task) or not (the correct choice for the Mismatch OUT task). Intracranial EEG (iEEG) signals were ~~captured collected~~ using depth electrodes implanted within the medial temporal lobe (MTL) regions: ~~the~~ left and right hippocampal head (AHL and AHR), ~~hippocampal~~ body (PHL and PHR), entorhinal cortex (ECL and ECR), and amygdala (AL and AR). These signals were recorded at a sampling rate of 32 kHz and within ~~the a~~ frequency range of 0.5–5,000 Hz (Figure 4A and Table 1). The iEEG signals were then resampled at a rate of 2 kHz. ~~We uncovered correlations between the~~ Correlations between experimental variables such as set size and accuracy rate ~~were uncovered~~ (Figure ??S1). ~~The times Times~~ of multiunit spikes were estimated using a spike sorting algorithm [37] from the Combinato package (<https://github.com/jniediek/combinato>) (Figure 4C).

2.2. Calculation of neural trajectories using GPFA

To ~~derive extract~~ the neural trajectories (referred to as factors; Figure 4D) within the hippocampus, entorhinal cortex (EC), and amygdala, we ~~used employed~~ GPFA [36] on multiunit activity data for each session (Figure 4D). ~~We implemented GPFA GPFA was implemented~~ using the elephant package (<https://elephant.readthedocs.io/en/>

latest/reference/gpfa.html). ~~We configured the bin size~~ The bin size was configured as 50 ms, with no overlaps. Each factor was z-normalized across all sessions. ~~We calculated the~~ The Euclidean distance from the origin (O) ~~using was calculated based on~~ these trajectories (Figure 4E).

Within each trajectory for a region such as AHL, ~~we calculated the~~ geometric medians (i.e., g_F for fixation, g_E for encoding, g_M for maintenance, and g_R for retrieval phase) were calculated by establishing the median coordinates of the trajectory during the four phases (Figure 4D). ~~We defined the~~ The optimal dimensionality for GPFA ~~as was defined to be~~ three, as determined via using the elbow method ~~using via~~ log-likelihood values in a three-fold cross-validation approach (Figure 2B).

2.3. Defining SWR candidates from hippocampal regions

~~To pinpoint potential SWR events in the hippocampus, we used a detection method consistent with the consensus in the field [38]. We re-referenced~~ A detection method in line with the field consensus [38] was used to identify potential SWR events in the hippocampus. The local field potential (LFP) signals from a region of interest (ROI), such as AHL, were re-referenced by subtracting the average signal outside the ROI (e.g., AHR, PHL, PHR, ECL, ECR, AL, AR) (see Figure 4A). ~~Using these~~ These re-referenced LFP signals ~~we applied were used to apply~~ a ripple-band filter (80–140 Hz) ~~to and~~ isolate SWR-positive (SWR⁺) candidates (see Figure 4B). ~~We performed SWR detection~~ SWR detection was performed using a publicly available tool (https://github.com/Eden-Kramer-Lab/ripple_detection) [39], with ~~some~~ modifications such as a revised bandpass range of 80–140 Hz for human applications [19, 20] ~~as opposed to instead of~~ the original 150–250 Hz range ~~used primarily~~ primarily used for rodents.

For SWR⁺ candidates, ~~we defined~~ SWR-negative (SWR⁻) candidates were defined as control events by shuffling the timestamps of SWR⁺ candidates across all trials and subjects. ~~We visually inspected the~~ The defined SWR⁺/SWR⁻ candidates were visually inspected (see Figure 4).

2.4. Defining SWRs from putative hippocampal CA1 regions

We ~~narrowed down confined~~ SWR candidates within putative CA1 regions to define SWRs. ~~We first identified~~ First, putative CA1 regions were identified as follows. ~~We embedded~~ SWR⁺/SWR⁻ candidates within the hippocampus were embedded into a two-dimensional space based on ~~their~~ superimposed spike counts per unit using UMAP (uniform manifold approximation and projection) [40] in a supervised manner (Figure 4A). The silhouette score [41], a ~~validation metric for measure for validating~~ clustering, was calculated from clustered samples (Table 2). ~~We defined hippocampal regions with~~ Hippocampal regions showcasing an average silhouette score across sessions ~~greater than exceeding~~ the 75th percentile were defined as putative CA1 regions, ~~resulting in the identification of which resulted in~~ five electrode locations identified from five patients (Table 3).

~~We defined~~ SWR⁺/SWR⁻ candidates within putative CA1 regions were marked as SWRs, ~~meaning thereby~~ they were no longer candidates. ~~The SWR duration and ripple band peak amplitude of SWRs followed~~ followed a log-normal ~~distributions distribution~~ (Figure 4C & E). ~~We visually inspected~~ As seen in Figure 4, SWR⁺/SWR⁻ ~~as shown in Figure 4.~~ We divided each SWR period were visually inspected. Each SWR period was divided into pre-SWR (at from -800 to -300 ms from SWR center), mid-SWR (at from -250 to +250 ms), and post-SWR (at from +300 to +800 ms) ~~based on according to~~ the time from the ~~SWR's center center of the SWR.~~

2.5. Statistical Evaluation

~~We conducted the~~ The Brunner–Munzel and Kruskal–Wallis tests were conducted using the scipy package in Python [42]. ~~We performed a correlation analysis~~ A correlation analysis was performed by determining the rank of the observed correlation coefficient ~~within in~~ the set-size-shuffled surrogate dataset, using a custom Python script. ~~Additionally, we executed~~ Moreover, a bootstrap test was executed using a homemade Python script.

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3. Results

3.1. iEEG recording and neural trajectory in MTL regions during a Sternberg task

We utilized a publicly accessible dataset [35] for this analysis, which consists of LFP signals (Figure 1A) from MTL regions (Table 11) obtained during a modified Sternberg task. SWR⁺ candidates were detected within all hippocampal regions from the LFP signals, filtered by the ripple band (80–140 Hz) (Figure 1B), whereas SWR⁻ candidates were defined at identical timestamps as SWR⁺ candidates but shuffled across separate trials (Figure 1). The dataset also encompasses the multiunit spikes (Figure 1C) were also included in the dataset, identified by implementation, which were specified through the application of a spike sorting algorithm [37]. Relying on the 50-ms binned multiunit activity devoid of overlaps, we applied GPFA [36] to elucidate the neural trajectory (or factors) of MTL regions by session and region (Figure 1D). Each factor was z-normalized by session and region (an instance example being session #2 in AHL of subject #1). The Euclidean distance from the origin (*O*) was subsequently then calculated (Figure 1E).

3.2. Hippocampal neural trajectory correlation with a Sternberg task

Figure 2A delineates the median neural trajectories of 50 trials as point clouds within the three primary principal factor space. The optimal Using the elbow method, we established that the ideal embedding dimension for the GPFA model, determined by employing the elbow method, was found to be was three (Figure 2B). The trajectory distance from the origin (*O*) ($\|g_F\|$, $\|g_E\|$, $\|g_M\|$, and $\|g_R\|$) was larger in the hippocampus than in the EC and amygdala (Figure 2C & D).¹

Similarly, the distances among between geometric medians of the four phases: $\|g_{FGE}\|$, $\|g_{FGM}\|$, $\|g_{FGR}\|$, $\|g_{EGM}\|$, $\|g_{EGR}\|$, and $\|g_{MGR}\|$ were calculated, displaying

¹Hippocampus: Distance = 1.11–1.01, median IQR, $n = 195,681$ timepoints; EC: Distance = 0.94–1.10, median IQR, $n = 133,761$ timepoints; Amygdala: Distance = 0.78–0.88, median IQR, $n = 165,281$ timepoints.

were computed. It was observed that the hippocampus demonstrated larger exhibited greater distances among the phases compared to both the EC and amygdala.¹

3.3. Memory load-dependent neural trajectory distance between the encoding and retrieval states in the hippocampus

Considering With consideration given to the memory load of the Stenberg task, Sternberg task, it was observed that the correct trial rate and set size (= equalling the number of alphabet letters letter to encode) were negatively correlated (Figure 3A).¹ Likewise, Similarly, a positive correlation was evident between response time and set size displayed a positive correlation (Figure 3B).¹ FurtherAlso, the set size and the trajectory distance between the encoding and retrieval phases ($\log_{10}\|g_{EGR}\|$) exhibited a positive correlation showed a positive relationship (Figure 3C).¹, while However, distances between other phase combinations did not note any exhibited no significant correlations (Figures 3D & S2).

3.4. Detection of hippocampal SWR from putative CA1 regions

With the intent of improving the accuracy To enhance the precision of recording sites and SWR detection, we attempted to estimate electrodes in CA1 regions of the hippocampus by observing distinct multiunit spike patterns during SWR occurrences incidents. For each

¹Hippocampus: Distance = 0.60–0.70, median IQR, $n = 8,772$ combinations; EC: Distance = 0.28–0.52, median IQR, $n = 5,017$ combinations ($p < 0.01$; Brunner–Munzel test); Amygdala: Distance = 0.24–0.42, median IQR, $n = 7,466$ combinations ($p < 0.01$; Brunner–Munzel test).

¹Correct rate: set size four (0.99–0.11, mean SD; $n = 333$ trials) vs. set size six (0.93–0.26; $n = 278$ trials) and set size eight (0.87–0.34; $n = 275$ trials; $p < 0.05$; Brunner–Munzel test with Bonferroni correction). Overall, $p < 0.001$ for Kruskal–Wallis test; correlation coefficient = -0.20 , $p < 0.001$.

¹Response time: set size four (1.26–0.45 s; $n = 333$ trials) vs. set size six (1.53–0.91 s; $n = 278$ trials) and set size eight (1.66–0.80 s; $n = 275$ trials). All comparisons $p < 0.001$, Brunner–Munzel test with Bonferroni correction; $p < 0.001$ for Kruskal–Wallis test; correlation coefficient = 0.22 , $p < 0.001$.

¹Correlation between set size and $\log_{10}(\|g_{EGR}\|)$: correlation coefficient = 0.05 , $p < 0.001$. Specific values: $\|g_{EGR}\| = 0.54–0.70$ for set size four trials, $n = 447$; $\|g_{EGR}\| = 0.58–0.66$ for set size six trials, $n = 381$; $\|g_{EGR}\| = 0.61–0.63$ for set size eight trials, $n = 395$.

session and hippocampal region, SWR⁺/SWR⁻ candidates were embedded into a two-dimensional space using UMAP (Figure 4A).¹ The silhouette score was ~~calculated~~ determined as a measure of clustering quality (Figure 4B & Table 2). Recording sites with an average silhouette score across sessions ~~exceeding more~~ significant than 0.6 were recognized as putative CA1 regions [40, 41]¹ (Tables 2 & 3). Hence, ~~Thus~~, we identified five putative CA1 regions, four of which were not previously ~~labeled as labelled~~ seizure onset zones (Table 1). ~~Subsequently, we labeled~~

~~Next, we marked~~ SWR⁺/SWR⁻ candidates within these putative CA1 regions as SWR⁺ and SWR⁻, respectively¹ (Table 3). Both SWR⁺ and SWR⁻ ~~exhibited~~ showed the same duration¹ (Figure 4C) ~~as per their definitions, following a log-distribution profile. A notable uptick. A significant increase in SWR⁺ incidence appeared emerged during the initial 400 ms of the retrieval phase¹ (Figure 4D). Besides, Furthermore,~~ the peak ripple band amplitude of SWR⁺ ~~exceeded~~ was higher than that of SWR⁻, following a log-normal distribution (Figure 4E).¹

3.5. Transient change in neural trajectory in the hippocampus during SWR

We analyzed the *distances* of the trajectory from origin (*O*) during SWR events in both encoding and retrieval phases (Figure 5A). ~~Given Upon observing the increase in distance during SWR, as shown in (Figure 5A, we classified), we categorized~~ each SWR into three ~~stages~~ states: pre-, mid-, and post-SWR. ~~Thereafter, the distances from *O* during these SWR periods are represented as $\|\text{pre-eSWR}^+\|$, $\|\text{mid-eSWR}^+\|$, and so forth. $\|\text{mid-eSWR}^+\|$ was larger than $\|\text{pre-eSWR}^+\|$~~

¹For illustrative purposes, consider the AHL in session #1 of subject #1.

¹The regions identified were: AHL of subject #1, AHR of subject #3, PHL of subject #4, AHL of subject #6, and AHR of subject #9.

¹Defining them resulted in equal counts for both categories: SWR⁺ ($n = 1,170$) and SWR⁻ ($n = 1,170$).

¹Defining them resulted in identical duration for both categories: SWR⁺ (93.0-65.4ms) and SWR⁻ (93.0-65.4ms).

¹SWR⁺ increased against the bootstrap sample; 95th percentile = 0.42 Hz; $p < 0.05$.

¹SWR⁺ (3.05-0.85SD of baseline, median IQR; $n = 1,170$) vs. SWR⁻ (2.37-0.33SD of baseline, median IQR; $n = 1,170$; $p < 0.001$; Brunner-Munzel test).

¹1.25-1.30, median IQR, $n = 1,281$, in Match-IN task; 1.12-1.35, median IQR, $n = 1,163$, in Mismatch-OUT task

¹, and $\|\text{mid-rSWR}^+\|$ was larger than $\|\text{pre-rSWR}^+\|$ in both Match-IN and Mismatch-OUT tasks.¹

3.6. Visualization of hippocampal neural trajectory during SWR in two-dimensional spaces

~~Given Based on~~ our observations of ~~the~~ neural trajectory 'jump' during SWR (Figure 5), we visualized the three-dimensional trajectories of pre-, mid-, and post-SWR events during the encoding and retrieval phases (Figure 6), ~~the distance between which was dependent on memory-load (Figure 3). We accomplished the visualization in two-dimensional spaces by linearly aligning peri-SWR trajectories, positioning.~~ For this visualization, we positioned \mathbf{g}_E at the origin (0, 0) and \mathbf{g}_R at the coordinate ($\|\mathbf{g}_{ER}\|$, 0). ~~These aligned trajectories were then rotated around the \mathbf{g}_{ER} axis (= x-axis), ensuring conservation of distances from the origin *O* and angles between \mathbf{g}_{ER} in the original three-dimensional spaces in the two-dimensional spaces. The scatter plot in these in two-dimensional spaces portrays the distinctive distributions of by linearly aligning peri-SWR trajectories based on phases and task types. For instance, one can distinguish that $\|\text{mid-eSWR}^+\|$ is larger than $\|\text{pre-eSWR}^+\|$ (Figure 6B), consistent with our earlier findings (Figure 5).~~

3.7. Fluctuating hippocampal neural trajectories between encoding and retrieval states

~~Following this~~ Subsequently, we inspected the trajectory *directions* based on \mathbf{g}_{ER} . Directions of SWRs were identified by the neural trajectory at -250 ms and +250 ms from their center (i.e., eSWR^+). ~~We From this data, we~~ computed the density of $\text{eSWR}^+ \cdot \mathbf{g}_{ER}$, $\text{rSWR}^+ \cdot \mathbf{g}_{ER}$, and $\text{eSWR}^- \cdot \text{rSWR}^-$ (Figure 7A-D). ~~$\text{rSWR}^- \cdot \mathbf{g}_{ER}$ exhibited biphasic distributions. By comparing the distribution of $\text{rSWR}^+ \cdot \mathbf{g}_{ER}$ (Figures 7A & B) with those of $\text{rSWR}^- \cdot \mathbf{g}_{ER}$ (Figures 7C & D), we calculated the contributions of SWR (Figures 7E & F), which unveiled a shift in the direction of \mathbf{g}_{ER}~~

¹1.08-1.07, median IQR, $n = 1,149$, in Match-IN task; 0.90-1.12, median IQR, $n = 1,088$, in Mismatch-OUT task

¹1.32-1.24, median IQR, $n = 935$, in Match-IN task; 1.15-1.26, median IQR, $n = 891$, in Mismatch-OUT task

¹1.19-0.96, median IQR, $n = 673$, in Match-IN task; 0.94-0.88, median IQR, $n = 664$, in Mismatch-OUT task

(Figures 7E & F; see *red rectangles*). Additionally, only in the Mismatch OUT task was $\overrightarrow{\text{eSWR}} \rightarrow \overrightarrow{\text{rSWR}}$ less than that of $\overrightarrow{\text{eSWR}} \rightarrow \overrightarrow{\text{rSWR}}$ (baseline periods) (Figure 7F; see *pink circles*); stated differently, eSWRs and rSWRs directed in the opposing direction exclusively in the Mismatch OUT task but not in the Match IN task (Figure 7E; see *pink circles*).

4. Discussion

This study ~~posited~~ hypothesized that hippocampal neurons ~~demonstrate unique~~ express distinct representations, or trajectories, in low-dimensional spaces during a working memory (WM) task in humans, specifically during sharp-wave ripple (SWR) periods. Initially, we projected the multiunit spikes from medial temporal lobe regions during a Sternberg task onto three-dimensional spaces using Gaussian-process factor analysis (GPFA) (Figure 4D–E and Figure 2A) [36]. The trajectory distance ~~among~~ amongst WM phases ($\|\mathbf{g}_{FGE}\|$, $\|\mathbf{g}_{FGM}\|$, $\|\mathbf{g}_{FGR}\|$, $\|\mathbf{g}_{EGM}\|$, $\|\mathbf{g}_{EGR}\|$, and $\|\mathbf{g}_{MGR}\|$) was larger in the hippocampus than in the entorhinal cortex (EC) and amygdala (Figure 2E), indicating more dynamic suggesting increased neural activity in the hippocampus during the WM task. Moreover, the trajectory distance between the encoding and retrieval phases in the hippocampus ($\|\mathbf{g}_{FGE}\|$) positively correlated displayed a positive correlation with memory load (Figure 3C–D), ~~thereby marking it as a reflection of~~ indicating that it reflects WM processing. The neural trajectory in the hippocampus also ~~exhibited~~ showed a transient increase during SWRs (Figure 5). ~~Lastly~~ Finally, the hippocampal neural trajectory ~~fluctuated~~ alternated between encoding and retrieval states, transitioning from encoding to retrieval during SWR events (Figure 7). Overall, these findings highlight emphasize the role of hippocampal neural activity in a WM task in humans [31, 32, 33].

We ~~discovered that the neural trajectory's distance~~ found that the distance of the neural trajectory among the four phases was longer in the hippocampus compared to the EC and amygdala, even when adjusting for the distance from origin O ($\|\mathbf{g}_F\|$, $\|\mathbf{g}_E\|$, $\|\mathbf{g}_M\|$, and $\|\mathbf{g}_R\|$) in those regions (Figure 2C–E). These findings ~~corroborate the role of the hippocampus in the WM task,~~ which aligns with previous align with existing reports of hippocampal persistent firing in the maintenance phase

[3] [4] [5] [6]. ~~However,~~ reinforcing the role of the hippocampus in the WM task. Notably, by applying GPFA to multiunit activity during a one-second level resolution of resolution WM task, we ~~found that the~~ observed that the neural trajectory in low dimensional space ~~neural trajectory~~ exhibits a memory-load dependency between the encoding and retrieval phases, represented as $\|\mathbf{g}_{EGR}\|$ (Figure 3). These results reaffirm the association between the hippocampus and WM processing [?].

The reliability of our analysis, ~~restricted~~ confined to presumed CA1 regions (Figure 4), is supported by several ~~contributing~~ factors. This focused approach is grounded in consistent ~~observations~~ reports that SWRs are synchronous with spike bursts of interneurons and pyramidal neurons [43] [44] [29] [45], potentially within a 50 μm radius of the recording site [46]. In this study, we ~~observed~~ noted an increase in SWR occurrences at 0–400 ms of the retrieval phase (Figure 4D), aligning with prior paralleling previous studies demonstrating increased SWR occurrences before spontaneous verbal recall [19] [20]. This finding not only corroborates ~~but broadens the observation~~ earlier observations, but also broadens them by extending to a triggered retrieval condition stage. Additionally, the log-normal distributions of SWR duration and ripple band peak amplitude observed in this study (Figure 4C–E) correlate are consistent with the consensus in ~~this the~~ this field [38]. ~~Hence~~ Therefore, our approach of ~~confining~~ restricting recording sites to probable CA1 regions likely improved the precision enhanced the accuracy of SWR detection. It ~~should be noted that an~~ is essential to mention that the increase in trajectory distance from origin O during SWR (Figure 5) may ~~have been skewed to a greater extent~~ be slightly skewed due to the channel selection; however, this does not ~~dramatically~~ severely impact our primary findings.

Interestingly, trajectory directions in the retrieval phase ~~oscillated~~ alternated between encoding and retrieval states ~~both in in both~~ both in in both baseline and SWR periods (Figure 7C & D). ~~Furthermore,~~ the balance of Moreover, these fluctuations transitioned from encoding to retrieval states during SWR (Figure 7E & F). These findings concur with previous ~~studies suggesting~~ SWR's working theories suggesting SWR's role in memory recall [19] [20]. Our results add ~~another layer of to~~ this understanding, specifying that SWRs occur when

the hippocampal representation transitions from encoding to retrieval states. ~~Therefore~~Hence, our findings ~~offer new~~provide novel insights into hippocampal representations: (i) neural fluctuations between encoding and retrieval states during a WM task and (ii) SWR as a mechanism ~~facilitating~~enabling the transition from encoding to retrieval states [47].

Additionally, our ~~research reveals~~study uncovers WM-task-specific directions between encoding and retrieval SWRs (Figure 7E–F). ~~Particularly~~Notably, encoding SWR and retrieval SWR pointed in opposing directions not ~~in during~~ a Match IN but ~~in during~~ a Mismatch OUT task. These ~~results might~~findings may align with the memory engram theory [48]. Indeed, the Match In task ~~showed subjects a once-seen~~presented subjects with a previously seen letter, while the Mismatch OUT task ~~presented a novel letter not introduced~~introduced a new letter not shown in the encoding phase. These ~~outcomes~~results suggest that SWR relates to the working cognitive processes in humans.

In conclusion, our study has demonstrated that hippocampal activity ~~fluctuates~~oscillates between encoding and retrieval states during a WM task and ~~undergoes~~a significant shift ~~shifts significantly~~ from encoding to retrieval during SWR periods.

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Contributors

Y.W. and T.Y. conceptualized the study; Y.W. performed the data analysis; Y.W. and T.Y. wrote the original draft; and all authors reviewed the final manuscript.

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Declaration of Interests

The authors declare that they have no competing interests.

Data and code availability

The data is available on G-Node (<https://doi.gin.g-node.org/10.12751/g-node.d76994/>). The source code is available on GitHub (<https://github.com/yanagisawa-lab/hippocampal-neural-fluctuation-during-a-WM-task-in-humans>).

Inclusion and Diversity Statement

We support inclusive, diverse, and equitable conduct of research.

Declaration of Generative AI in Scientific Writing

The authors employed ChatGPT, provided by OpenAI, for enhancing the manuscript's English language quality. After incorporating the suggested improvements, the authors meticulously revised the content. Ultimate responsibility for the final content of this publication rests entirely with the authors.

Tables

Subject ID	of sessions	AHL	AHR	PHL	PHR	ECL	ECR	AL	AR	SOZ
1	4	o	x	o	o	o	x	o	x	"AHR, LR"
2	7	o	o	o	o	o	o	o	o	"AHR, PHR"
3	3	o	o	o	o	o	o	o	x	"AHL, PHL"
4	2	o	o	o	o	o	o	o	o	"AHL, AHR, PHL, PHR"
5	3	o	x	x	o	x	x	o	x	DRR
6	6	o	o	o	o	o	o	o	o	"AHL, PHL, ECL, AL"
7	4	o	o	o	o	o	o	o	o	"AHR, PHR"
8	5	o	o	o	o	o	o	o	o	ECR
9	2	o	o	o	o	o	o	o	o	"ECR, AR"

Table 1 – Electrode Positions in the Dataset

Annotation of electrode This figure annotates the positions of the electrodes and the seizure onset zones: regions depicted. Regions marked with an "o" symbol are included, while whereas those marked with designated by an "x" (navy) are omitted from the dataset. **Abbreviations** The following abbreviations are used: AHL denotes refers to the left hippocampal head; AHR represents to the right hippocampal head; PHL signifies to the left hippocampal body; PHR indicates to the right hippocampal body; ECL refers to the left entorhinal cortex; ECR implies to the right entorhinal cortex; AL refers to the left amygdala; AR stands for to the right amygdala; and SOZ pertains to the seizure onset zone [35].

Subject	AHL	AHR	PHL	PHR
1	0.60 ± 0.14	n.a.	n.a.	0.1 ± 0
2	0.21 ± 0.16	0.17 ± 0.21	0.18 ± 0.22	0.20 ± 0.15
3	0.40 ± 0.42	0.83 ± 0.12	n.a.	n.a.
4	0.10 ± 0.00	0.10 ± 0.00	0.90 ± 0.00	0.10 ± 0.14
5	n.a.	n.a.	n.a.	n.a.
6	0.63 ± 0.06	n.a.	n.a.	0.27 ± 0.06
7	0.10 ± 0.00	0.35 ± 0.35	0.37 ± 0.47	0.10 ± 0.00
8	0.13 ± 0.10	n.a.	0.28 ± 0.49	n.a.
9	n.a.	0.85 ± 0.07	0.15 ± 0.07	n.a.

Table 2 – Silhouette score comparison of UMAP clustering between SWR^+ candidates and SWR^- candidates- Comparative Analysis of Silhouette Scores in UMAP Clustering of SWR^+ and SWR^- Candidates

The We measured the silhouette scores (mean ± SD across sessions ~~by subject~~for individual subjects) of UMAP clustering for both SWR^+ candidates and SWR^- candidates (Figure 4A) were in UMAP clustering, derived from their underlying multiunit spike patterns multispikes (Figure 4A). The mean values were recorded score was registered as 0.205 (SD = 0.285), with a and the median fell within an interquartile inter-quartile range (IQR; Figure 4B) [40, 41].

Subject ID	of sessions	of trials	ROI	of SWRs	SWR incidence [Hz]
1	2	100	AHL	274	0.34
3	2	97	AHR	325	0.42
4	2	99	PHL	202	0.26
6	2	100	AHL	297	0.37
9	2	97	AHR	72	0.09
Total = 10	Total = 493	"Total = 1,170"	0.30 ± 0.13 (mean ± SD)		

Table 3 – ~~Count of Identified SWR Events~~ Number of Identified SWR Events

The table ~~displays the~~ presents summary statistics ~~of~~ for the ~~presumptive~~ putative CA1 regions and SWRs. To ~~mitigate~~ reduce sampling bias, ~~solely~~ only the ~~initial~~ first two sessions (sessions 1 and 2) from each subject were ~~employed~~ used.

Figures

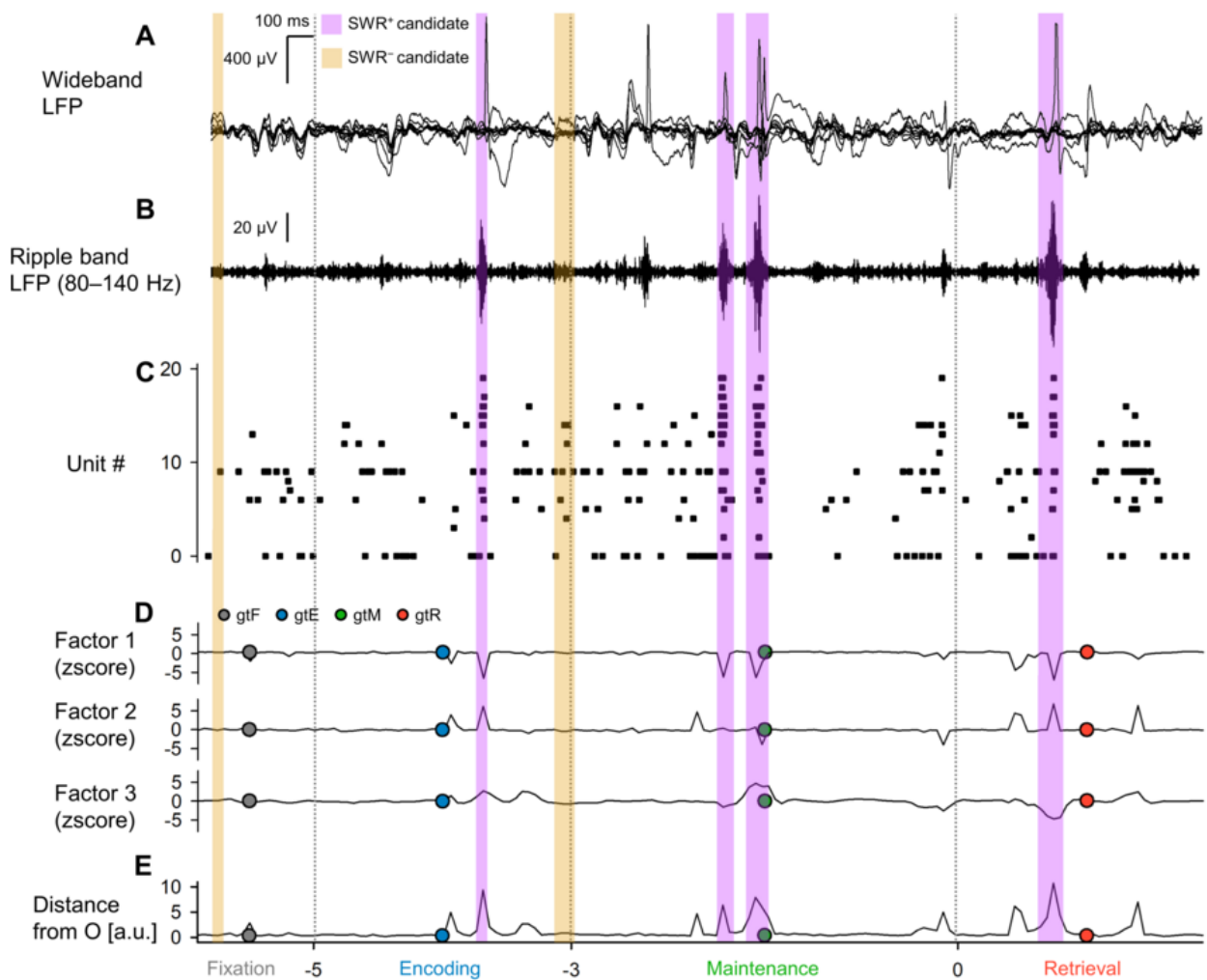


Figure 1 – Local field potential (LFP), multiunit activity, and neural trajectory of the hippocampus during a modified Sternberg task Local Field Potential (LFP), Multiunit Activity, and Neural Trajectory of the Hippocampus during a Modified Sternberg Task [8? , 9]

A. **Representative** Shown here are representative wideband LFP traces from iEEG signals recorded in, recorded from the left hippocampal head. These were attained while the subject performed a modified Sternberg working memory task, consisting. The task consisted of fixation (1 s, gray), encoding (2 s, blue), maintenance (3 s, green), and retrieval (2 s, red) [8? , 9]. B. The corresponding Displayed are the associated ripple band LFP traces [46, 21, 22]. C. The This is the raster plot of multiunit spikes, derived from the LFP traces using utilizing a spike sorting algorithm [37]. D. Neural trajectory The neural trajectory, determined by GPFA on the basis of, is based on the spike counts per unit with 50-ms bins [36]. The dot eircles represent dotted circles symbolize the geometric median coordinates for each phase. E. Trajectory distance from the The trajectory distance from origin O. Please note that is shown. Note, the purple and yellow rectangles indicate highlight the timings for SWR⁺ candidates and SWR⁻ candidates (controls for SWR⁺), respectively [49, 1, 39, 50, 10, 11, 12].

Figure 2 – State-dependent hippocampal neural trajectory

A. The figure illustrates the neural trajectory in the first three-dimensional factors three dimensions computed using the Gaussian Process Factor Analysis (GPFA is illustrated). Smaller dots represent the Each smaller dot represents coordinates of 50-ms neural trajectory bins, while whereas larger dots outlined in black denote the symbolize geometric medians for subsequent of consecutive phases in the Sternberg working memory task: fixation (*gray*), encoding (*blue*), maintenance (*green*), and retrieval (*red*)[36]. B. This figure demonstrates The graph reveals the log-likelihood of GPFA models in conjunction with relation to the number of dimensions employed to embed for embedding multi-unit spikes in medial temporal lobe (MTL) regions. Significantly, the dimensionality's optimal dimension value was determined to be identified as three, ascertained through the use of determined using the elbow method[42]. C. In this segment, This portion maps the distance of the neural trajectory is mapped from the origin (*O*) for the hippocampus (Hipp.), entorhinal cortex (EC), and amygdala (Amy.), and is plotted in relation to the plots it against time from the probe's commencement initiation [35]. D. The following subsequent graph illustrates showcases the trajectory's distance from *O* within across MTL regions, whereby with the hippocampus exhibits demonstrating the greatest distance, succeeded followed by the EC and the Amygdala[16]. E. The subsequent final representation indicates inter-phase trajectory distances within the MTL regions[38]. Abbreviations:

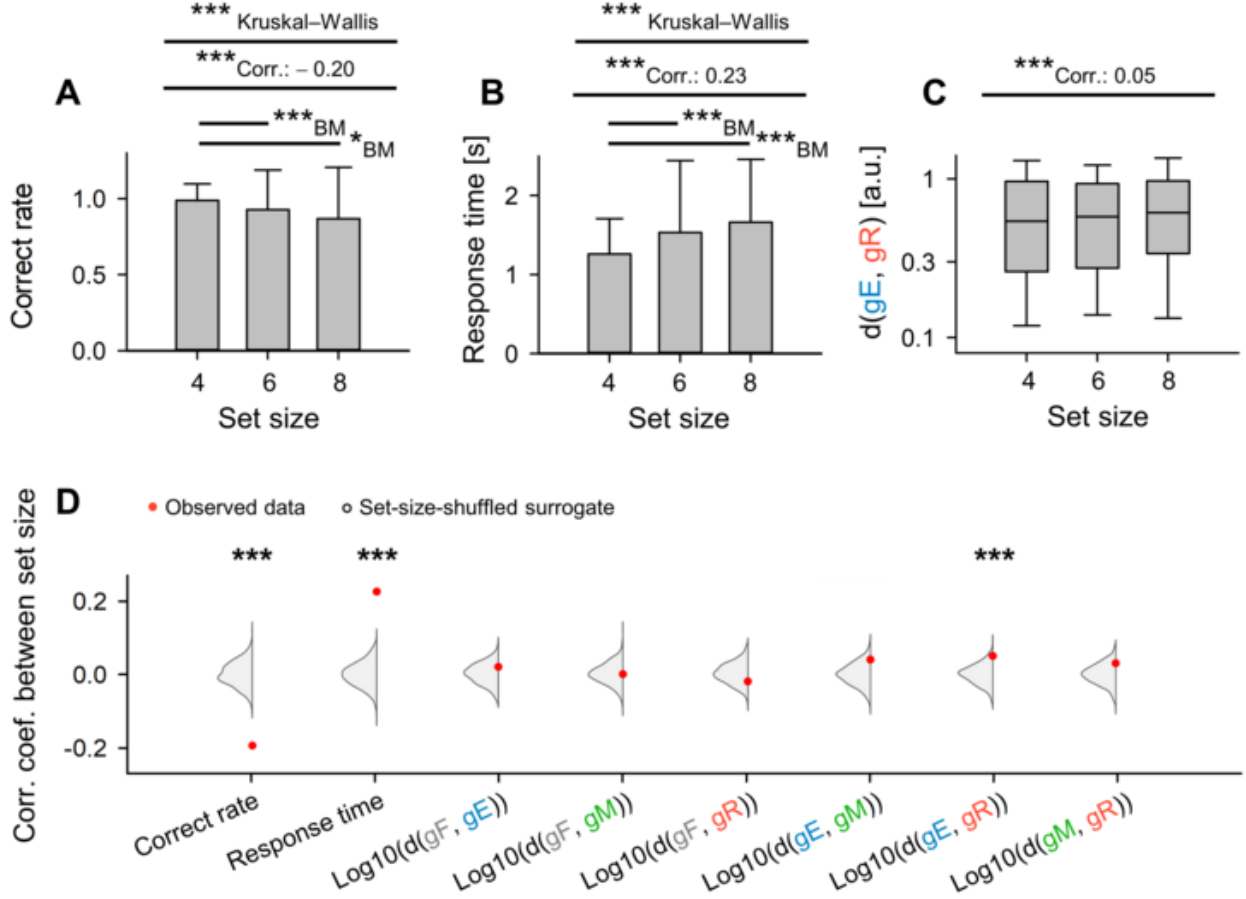


Figure 3 – Dependence of Trajectory Distance on Memory Load Between Encoding and Retrieval States in the Hippocampus

A. Set There is a significant correlation between set size (the number of letters to encode) and correct rate in the WM task (coefficient = -0.20, *** $p < 0.001$) [49, 8, 7]. **B.** Set size and response time are also significantly correlated (coefficient = 0.23, *** $p < 0.001$) [9]. **C.** Set size and the inter-phase distances between encoding and retrieval phases ($\|g_{EgR}\|$) are correlated as well, although less significantly (correlation coefficient = 0.05) [8]. **D.** Red dots illustrate experimentally observed correlations between set size and the following-mentioned parameters: correct rate, response time, $\log_{10} \|g_{FgE}\|$, $\log_{10} \|g_{FgM}\|$, $\log_{10} \|g_{FgR}\|$, $\log_{10} \|g_{EgM}\|$, $\log_{10} \|g_{EgR}\|$, and $\log_{10} \|g_{MgR}\|$. The gray kernel density plot indicates the corresponding set-size-shuffled surrogate measurements ($n = 1,000$) (*** $ps < 0.001$) [22, 45].

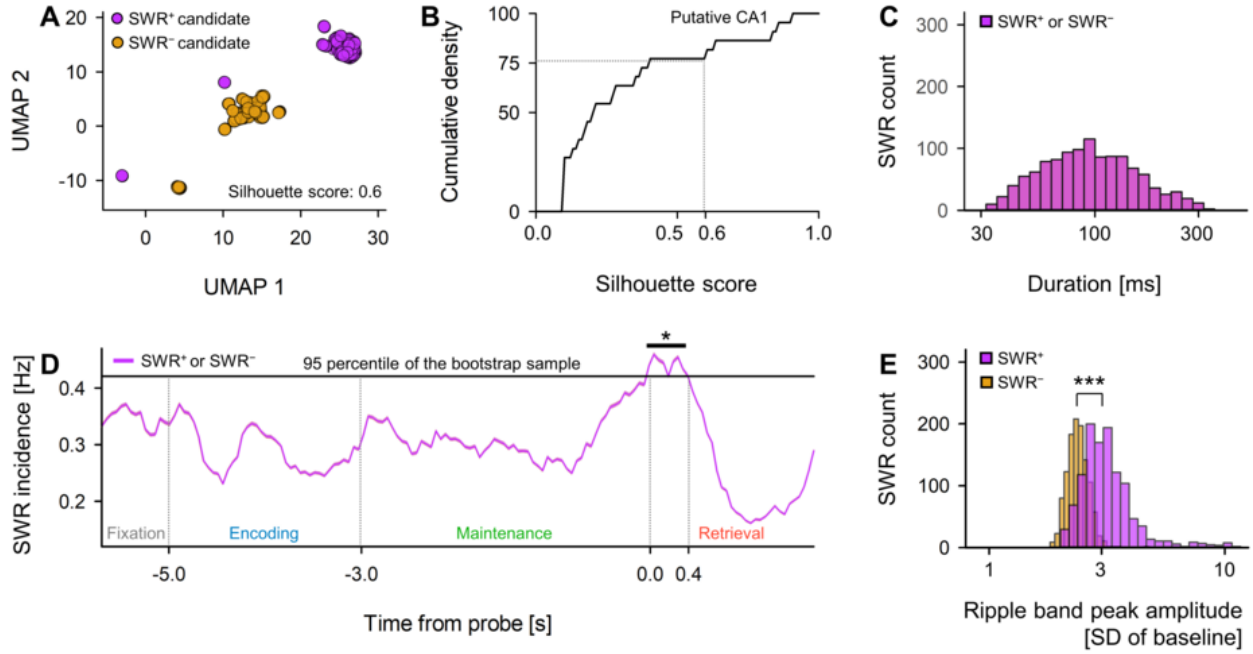


Figure 4 – Detection of SWRs in Presumed CA1 Regions- Detection of SWRs in Assumed CA1 Regions

A. Two-dimensional UMAP (uniform manifold approximation and projection) projection of multi-unit spikes during candidates for possible SWRs (purple) and non-SWRs (yellow) periods is presented [40]. B. Cumulative density plot of silhouette scores, utilized as a gauge for which measure the quality of UMAP clustering quality, for the various hippocampal regions is plotted (refer to see Table 2). Lands exceeding Areas with a silhouette score of above 0.60 (equating corresponding to the 75th percentile) were classified-identified as probable CA1 regions. Candidates for SWRs-SWR and non-SWRs-identified-non-SWR periods in these hypothetical potential CA1 regions were defined as SWRs and non-SWRs, respectively ($n_s = 1,170$), respectively [41]. C. The distribution of durations for both SWRs (purple) and non-SWRs (yellow) are congruently shown, given considering their respective definitions (93.0 [65.4] ms, median [IQR]) [14][20]. D. SWR incidence for The occurrence rate of SWRs (purple) and non-SWRs (yellow) over time from probing, represented since stimulation initiation is illustrated as a mean value \pm 95% confidence interval. Despite their singular character, It is important to note that due to the close intervals, visualization may not be visible due to their narrowness difficult. Note that Also, a significant uptake-increase in SWR incidence-occurrence was perceived detected during the first 400 ms of the retrieval phase (0.421 [Hz], $*p < 0.05$, bootstrap test) [47][15][16]. E. The distributions Distributions of ripple band peak amplitudes are presented-provided for non-SWRs (yellow; 2.37 [0.33] SD of baseline, median [IQR]) and SWRs (purple; 3.05 [0.85] SD of baseline, median [IQR]). Significant differences were observed ($***p < 0.001$, utilizing-using the Brunner-Munzel test) [19][51][38].

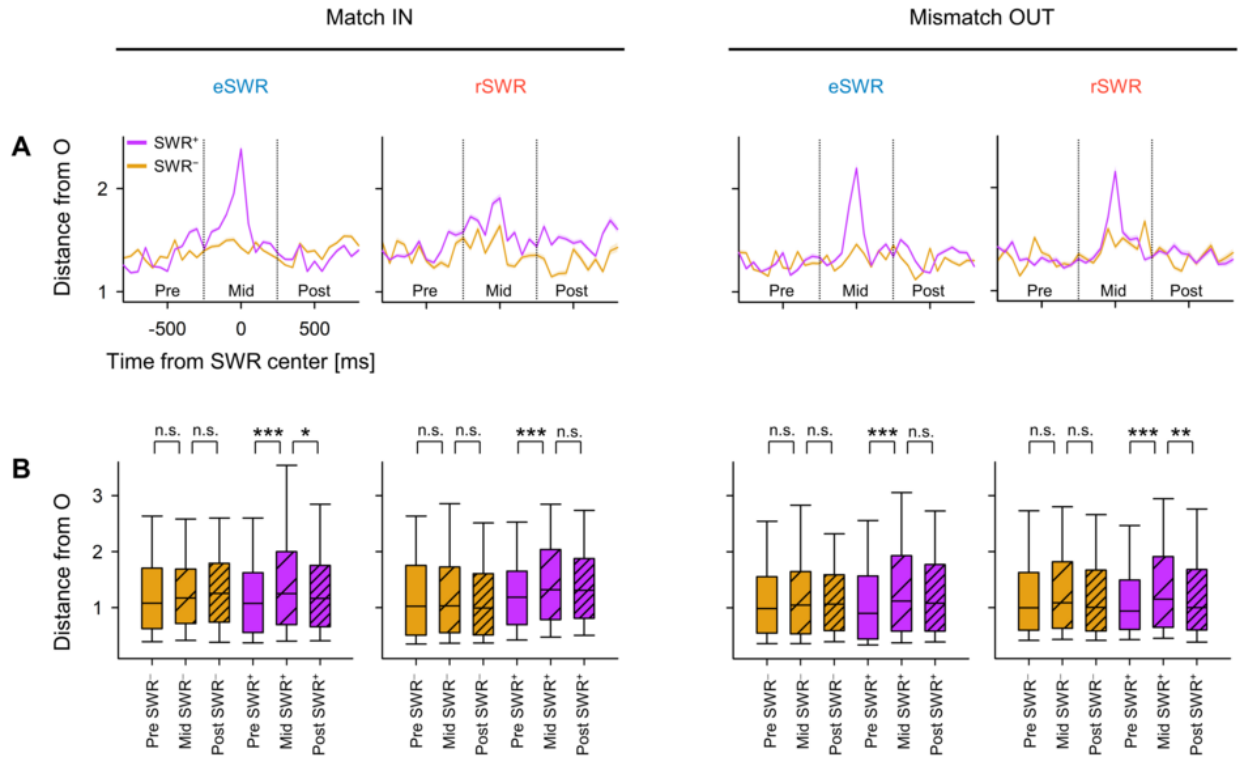


Figure 5 – Transient Alterations in Neural Trajectory During SWR

A. Represents the mean distance from the origin (O) of the peri-sharp-wave-ripple (SWR) trajectory expressed as the mean, which is accompanied by a 95% confidence interval, which may not be visible owing to its narrow range [14, 19, 47]. **B.** Illustrates the distance from the origin (O) during the pre-, mid-, and post-SWR periods (* $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$; according to the Brunner–Munzel test [3]). Abbreviations detailed as Definitions included are: SWR, sharp-wave ripple events; eSWR, SWR occurring in the encoding phase; rSWR, SWR happening during the retrieval phase; SWR⁺, a SWR event; SWR⁻, the control events for paired with SWR⁺; pre-, mid-, or post-SWR, the time intervals from -800 to -250 ms, from -250 to +250 ms, or from +250 to +800 ms, respectively, each relative to the SWR center.

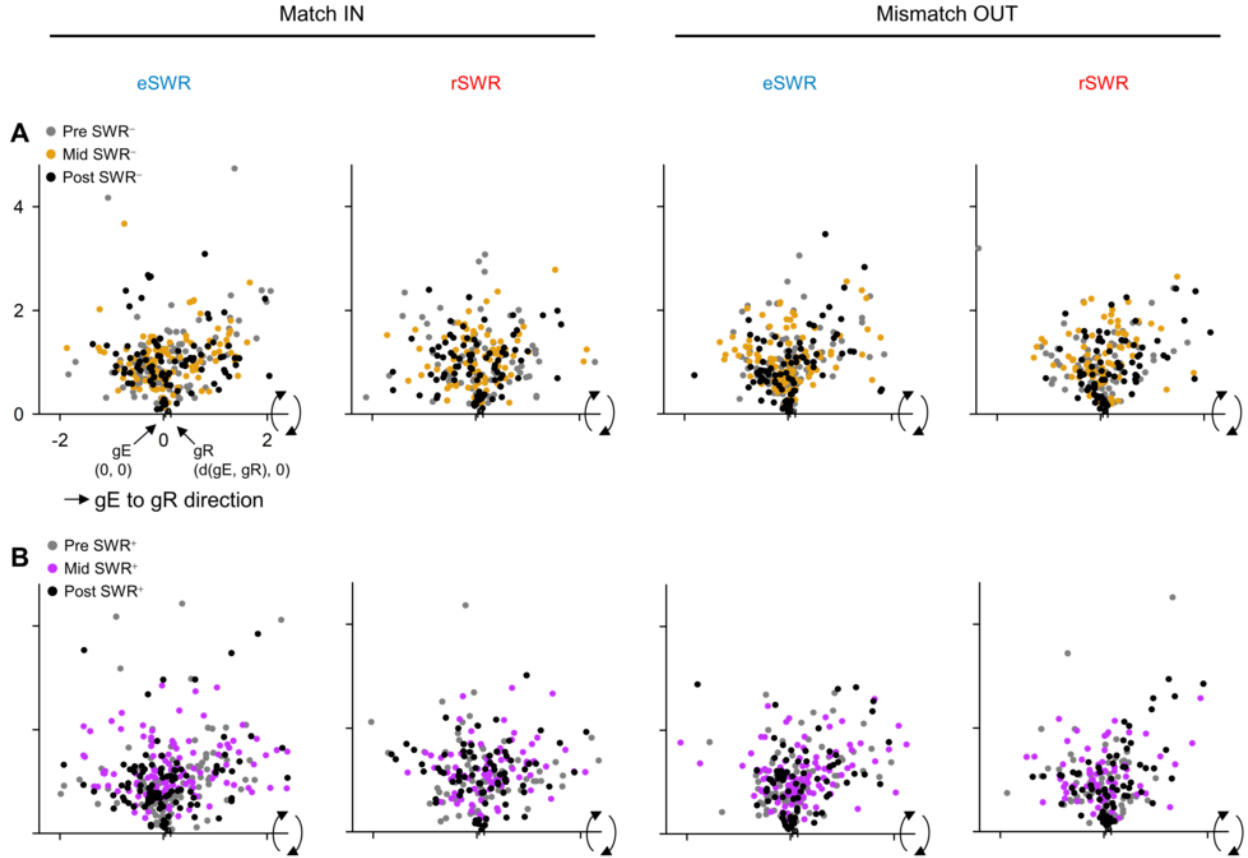


Figure 6 – Visualization of Neural Trajectory During SWR in Two-Dimensional Space Visualizing Neural Trajectory During SWR in Two-Dimensional Space

Featured are The presented neural trajectories within the hippocampus pertain to hippocampal activity during Sharp-Wave Ripple (SWR) events, represented shown in a two-dimensional space. **A.** Trajectories during representative of pre- (gray), mid- (yellow), and post-SWR⁻ (black) phases of an SWR event [47]. **B.** Corresponding trajectories for Trajectories corresponding to SWR⁺ scenarios as opposed in contrast to SWR⁻ [16]. The magnitude of $\|g_E g_R\|$ fluctuates exhibits fluctuations within sessions [38]. The projection projecting protocol went is as follows: initially, g_E was placed situated at the origin $O(0,0)$, and g_R at $(\|g_E g_R\|, 0)$ via linear transformation [17]. Subsequently, the point cloud was rotated around the $g_E g_R$ axis (the x-axis) for compatibility to be compatible with a two-dimensional environment [36]. Consequently Thus, both the distances from O and the angles with respect to the $g_E g_R$ axis were kept intact remained unaltered from their original three-dimensional arrangement configuration [40]. Abbreviations: SWR denotes represents Sharp-Wave Ripples; eSWR refers to denotes SWR during the encoding phase; rSWR indicates signifies SWR during the retrieval phase; SWR⁺ represents typifies an SWR event; SWR⁻ designates signals the control events for SWR⁺; pre-SWR, mid-SWR, or post-SWR specify refer to the time interval from -800 to -250 ms, from -250 to $+250$ ms, or from $+250$ to $+800$ ms from the center of the SWR, respectively [30].

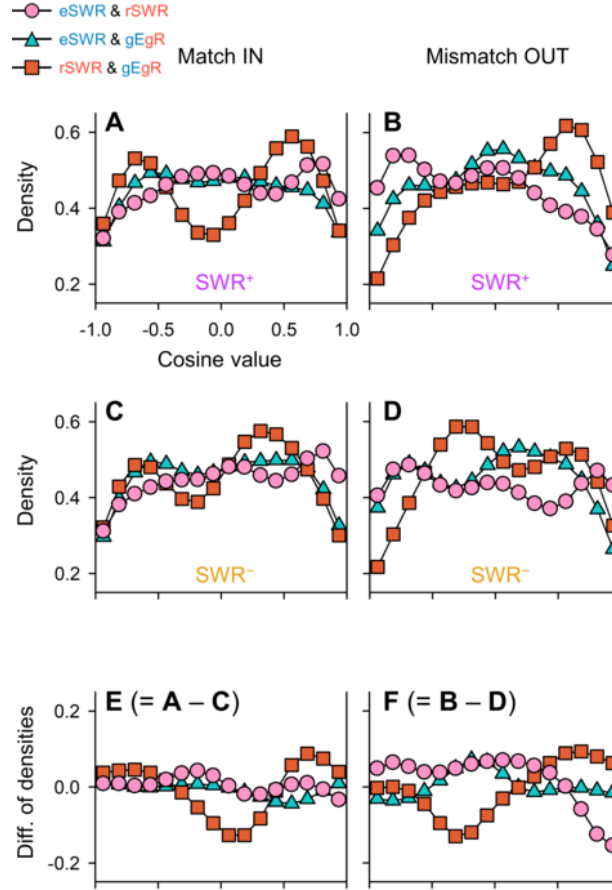


Figure 7 – Neural Trajectory Directions of SWR-based on Encoding and Retrieval States– Directionality of Neural Trajectories in SWR based on Encoding and Retrieval States

A–B The Kernel Density Estimation (KDE) distribution of $\overrightarrow{eSWR} \cdot \overrightarrow{rSWR}^+$ (pink circles), $\overrightarrow{eSWR} \cdot \overrightarrow{gEgR}$ (blue triangles), and $\overrightarrow{rSWR} \cdot \overrightarrow{gEgR}$ (red rectangles) in the Match IN (A) and Mismatch OUT tasks (B) are presented [8]. **C–D** The corresponding distributions of $\overrightarrow{eSWR} \cdot \overrightarrow{rSWR}^-$ (pink circles), $\overrightarrow{eSWR} \cdot \overrightarrow{gEgR}$ (blue triangles), and $\overrightarrow{rSWR} \cdot \overrightarrow{gEgR}$ (red rectangles) in the Mismatch OUT task (D) are presented [9]. **E–F** The differences in-between the distributions of SWR⁺ and SWR⁻, emphasizing accentuate the SWR components ($E = C - A$; $F = D - B$). Notice, with the biphasic distributions of $\overrightarrow{rSWR} \cdot \overrightarrow{gEgR}$, underseering emphasizing the neural fluctuations between encoding and retrieval states during the Sternberg task [7]. Conversely, On the other hand, in the Mismatch OUT task, showed inverse directionality between \overrightarrow{eSWR}^+ and \overrightarrow{rSWR}^+ (pink circles) which was identified, but not observed in the Match IN task (E–F) [31, 32]. Lastly, observed transitions from retrieval to encoding states were observed state for the SWR components occurred in both Match IN and Mismatch OUT tasks (red rectangles in E–F) [37, 46].