Medical Vision Seminar

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FedDG: Federated Domain Generalization on Medical Image Segmentation via Episodic Learning in Continuous Frequency Space

Quande Liu, Cheng Chen, Jing Qin, **Qi Dou**, Pheng-Ann Heng Department of Computer Science and Engineering, The Chinese University of Hong Kong

目录

- •问题定义
- 背景
- 主要贡献
- 动机
- 方法
- 实验结果

问题定义

▶模型输入

来自不同客户端的数据

▶模型训练

- 1.初始化全局参数,数据本地训练
- 2.汇聚(FedAvg)在本地训练得到的局部参数,得到全局 参数

▶模型输出

在未知域(客户端)上进行推理/预测

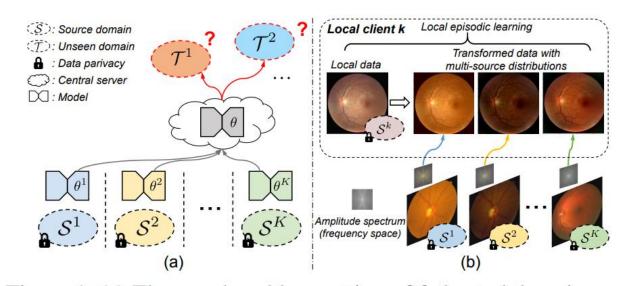


Figure 1. (a) The novel problem setting of federated domain generalization (FedDG), which aims to learn a federated model from multiple decentralized source domains such that it can directly generalize to completely unseen target domains. (b) Our main idea to tackle FedDG by transferring distribution information in frequency space and episodic learning at each local client.

背景

▶联邦学习(Federated Learning)

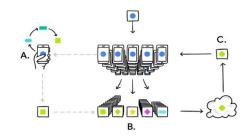
DNN需要大量数据参与训练才容易取得较好的性能,但由于客户隐私或商业利益问题,客观上给数据收集带来了障碍,造成了一个个数据孤岛。

联邦学习为多客户端数据协作提供了一种有前途的隐私保护解决方案,它通过聚合每个本地客户端的参数同时将数据保留在本地,从分散的数据集开发了一个全局模型。

➤联邦领域泛化(Federated Domain Generalization)

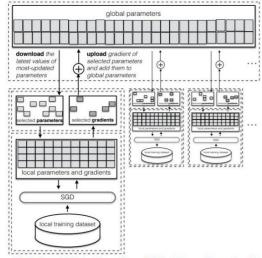
在实际场景中,由于每个客户端由于所处的环境不同、采集设备不同等问题会造成不同站点采集的数据存在一定差异(域偏移),尤其在医疗图像领域,这个问题更为突出因此,联邦域泛化就被提出用来解决这个问题,它主要通过在多个域同时学习,训练得到更具泛化性的模型。

联邦学习 (Federated Machine Learning)



- H. Brendan McMahan et al, Communication-Efficient Learning of Deep Networks from Decentralized Data, Google, 2017
- 手机终端,多个用户,1个中心
- 所有数据特征维度相同
- 本地训练
- 选择用户训练

WeBank



Reza Shokri and Vitaly Shmatikov. 2015. *Privacy-Preserving Deep Learning*. In Proceedings of the 22nd ACM SIGSAC Conference or Computer and Communications Security (CCS '15). ACM, New York, NY, USA, 1310–1321.

• 选择参数更新

И

背景

▶元学习(Meta Learning)

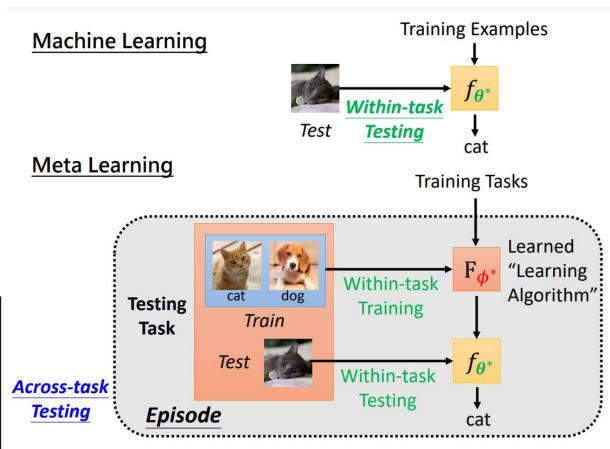
Mate learning: learn to learn, Meta Learning希望使得模型获取一种"学会学习"的能力,使其可以在获取已有"知识"的基础上快速学习新的任务。

Meta-train 学习元知识

Meta-test 验证元知识

在meta-test过程时,我们便可以将学到的元知识应用于meta-test数据来训练我们真正的任务模型。

目的	输入	函数	输出	流程
通过 训练数据, 学习到	Χ	f	Υ	1. 初始化 f 参数
输入 X 与输出 Y 之间				2. 喂数据 <x,y></x,y>
的映射,找到函数 f				3. 计算 loss,优化 f 参数
				4. 得到:y = f(x)
通过 (很多) 训练任务	(很多)	F	f	1. 初始化 F 参数
T 及对应的 训练数据	训练任			2. 喂训练任务 T 及对应的
D, 找到函数 F。F 可以	务 及 对			训练数据 D,优化 F 参数
输出一个函数 f, f 可用	应的训			3. 得到:f=F*
于新的任务	练数据			4. 新任条中: v=f(x) 知事 @原爽的安迪
	通过 训练数据, 学习到输入 X 与输出 Y 之间的映射,找到函数 f 通过 (很多) 训练任务 T 及对应的 训练数据 D, 找到函数 F。F可以输出一个函数 f, f 可用	通过 训练数据, 学习到 X 输入 X 与输出 Y 之间的映射,找到函数 f	通过 训练数据, 学习到 X f 输入 X 与输出 Y 之间的映射,找到函数 f (很多) 训练任务	通过 训练数据, 学习到 X f Y 输入 X 与输出 Y 之间的映射,找到函数 f (很多) 训练任务 (很多) F f T 及对应的 训练数据 训练任 为 及对输出一个函数 f, f 可用 应的 训



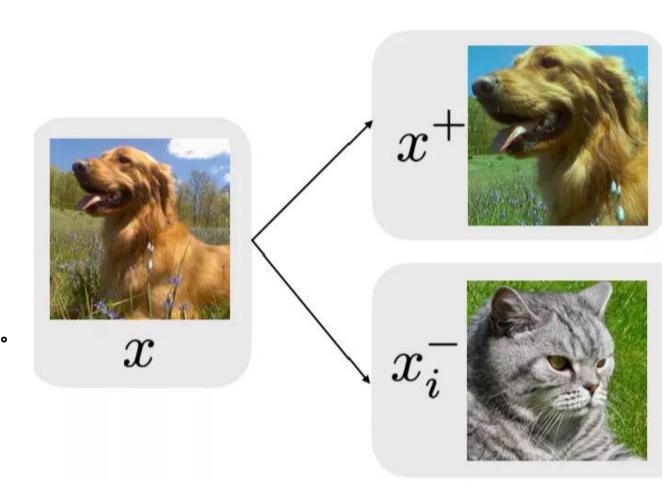
背景

➤对比学习(Contrastive learning)

对比学习是一种基于对比思想的判别式表示学习框架,主要用来做无监督(自监督)的表示学习。

对比学习的主要思想是将样例与与它语义相似的例子(正样例)和与它语义不相似的例子(负样例)进行对比,希望通过设计模型结构和对比损失,使语义相近的例子对应的表示在表示空间更接近,语义不相近的例子对应的表示距离更远,以达到类似聚类的效果。

以图像为例,对比学习期望通过使同一类狗不同角度照片的表示相近,而不同种类动物对应的表示距离相远,使得学到的表示可以忽略掉角度(或光影等)变换带来的细节变动,进而学习到更高维度、更本质的特征(语义)信息。



主要贡献

- 提出了新颖且实际的联邦领域泛化问题,这是第一个在未见域上的联邦学习模型中提升泛化性的工作。
- 2. 提出了一个隐私保护的策略来提高联邦学习模型的泛化性,通过高效的连续频域插值 算法。
- 3. 提出了新颖的<mark>边界介导的情景学习</mark>,在单个client的局部训练中,使用边界优化loss去处理域迁移问题,提高在模糊边界上的模型泛化能力。
- 4. 在两个经典的医学图像分割任务上进行实验,<mark>眼底图分割</mark>和前列腺MRI图像分割,表现sota。

前人工作

◆医学成像中的联邦学习(Federated Learning in Medical Imaging)

现有工作都集中在提高内部客户端的性能上,而没有考虑联邦之外未见域的泛化问题。

◆领域泛化(Domain Generalization)

在现有中,一些方法旨在通过最小化多个源域之间的域差异来学习域不变表示。

- 1.利用对比损失最小化来自同一类别但不同client的样本之间的距离。
- 2.基于元学习(meta learning),这是一种情景训练范式,通过在每次迭代中创建meta-train和meta-test来学习域迁移 (domain shift)。然而,已有方法通常需要将多个领域的数据集中在一个地方进行学习,这违反了分散数据集的联邦学习环境下的隐私保护。
- 3.通过设计深度神经网络结构、利用自监督、设计训练启发式算法或进行数据增广来处理领域泛化的其他方法。这些方法不需要数据集中化,但很难利用丰富的跨域数据分布。

动机

1.图像

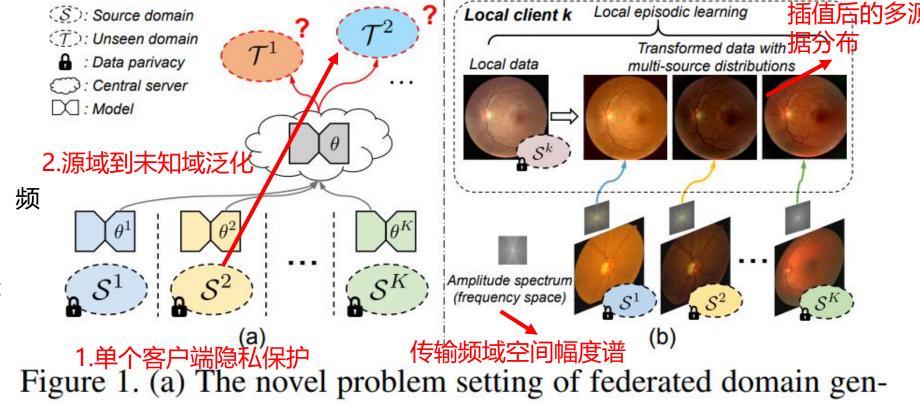


Figure 1. (a) The novel problem setting of federated domain generalization (FedDG), which aims to learn a federated model from multiple decentralized source domains such that it can directly generalize to completely unseen target domains. (b) Our main idea to tackle FedDG by transferring distribution information in frequency space and episodic learning at each local client.

- 低级分布(e.g.风格):频 率空间幅度谱

高级语义(e.g.物体): 频率空间相位谱

动机

2.在联邦以外的未见领域的分割结果差的原因主要来自分割边界的模糊性。 因此设计了一个边界介导的loss来提高域无关(domain invariant)的边界描绘。

所有客户端

本地客户端k与外部客户端n插值产生的新的幅度谱

连续频域插值算法

 $\mathcal{A}_{i,\lambda}^{k\to n} = ((1-\lambda)\mathcal{A}_i^k + \lambda\mathcal{A}_j^n) * \mathcal{M} + \mathcal{A}_i^k * (1-\mathcal{M}). \tag{2}$

 $\mathcal{M}=\mathbb{1}_{(h,w)\in[-\alpha H:\alpha H,-\alpha W:\alpha W]}$

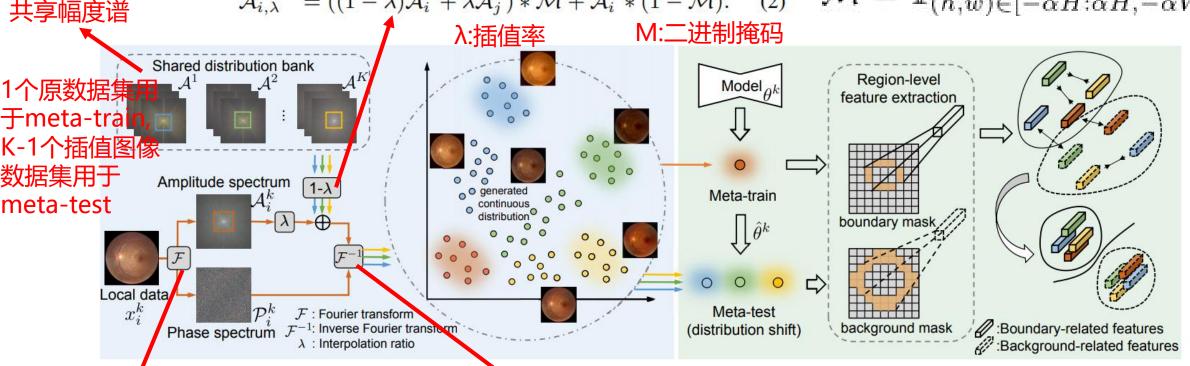


Figure 2. Overview of our proposed episodic learning in continuous frequency space (ELCFS). The distribution information is exchanged across clients from frequency space with an continuous interpolation mechanism, enabling each local client to access the multi-source distributions. An episodic training paradigm is then established to expose the local optimization to domain shift, with explicit regularization to promote domain-independent feature cohesion and separation at the ambiguous boundary region for improving generalizability.

快速傅里叶变换

$$\mathcal{F}(x_i^k)(u,v,c) = \sum_{i=1}^{H} \sum_{i=1}^{H} x_i^k(h,w,c) e^{-j2\pi(\frac{h}{H}u + \frac{w}{W}v)}.$$

傅里叶反变换

$$x_{i,\lambda}^{k\to n} = \mathcal{F}^{-1}(\mathcal{A}_{i,\lambda}^{k\to n}, \mathcal{P}_i^k), \tag{3}$$

边界介导的情景学习(Boundary-oriented Episodic Learning)

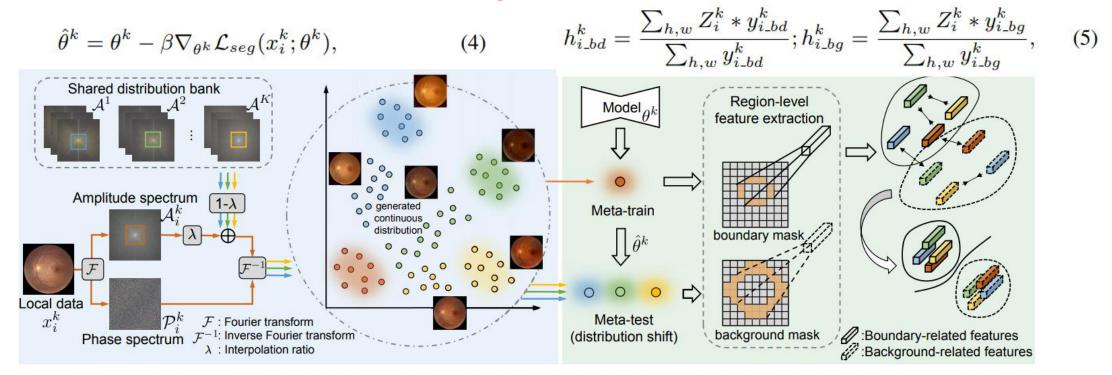


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$$\ell(h_m, h_p) = -log \frac{exp(h_m \odot h_p/\tau)}{\sum_{q=1, q \neq m}^{2K} \mathbb{F}(h_m, h_q) \cdot exp(h_m \odot h_q/\tau)}, \qquad \mathcal{L}_{boundary} = \sum_{m=1}^{2K} \sum_{p=m+1}^{2K} \frac{(1 - \mathbb{F}(h_m, h_p)) \cdot \ell(h_m, h_p)}{B(K, 2) \times 2}, \qquad (7)$$

$$\mathcal{L}_{meta} = \mathcal{L}_{seg}(t_i^k; \hat{\theta}^k) + \gamma \mathcal{L}_{boundary}(x_i^k, t_i^k; \hat{\theta}^k), \qquad (8) \qquad \underset{r}{\text{arg min }} \mathcal{L}_{seg}(x_i^k; \theta^k) + \mathcal{L}_{meta}(x_i^k, t_i^k; \hat{\theta}^k). \qquad (9)$$

方法 Meta Learning

1. meta-train: Dice loss Lseq

$$\hat{\theta}^k = \theta^k - \beta \nabla_{\theta^k} \mathcal{L}_{seg}(x_i^k; \theta^k), \tag{4}$$

- β: learning rate for the inner-loop update
- 2. meta-test: new loss Lmeta

$$\mathcal{L}_{meta} = \mathcal{L}_{seq}(t_i^k; \hat{\theta}^k) + \gamma \mathcal{L}_{boundary}(x_i^k, t_i^k; \hat{\theta}^k), \quad (8)$$

Boundary-oriented meta optimization

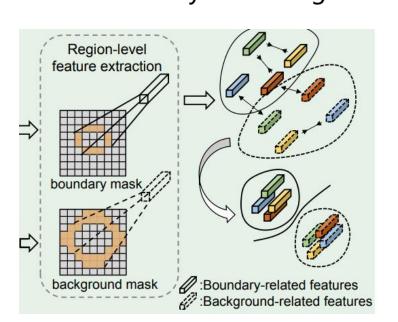
3. extract the boundary-related and background-related features for the input samples.对标签 y_i^k 做形态学操作得到两个新mask:

Binary boundary mask: $y_{i_bd}^k$

Binary background mask: $y_{i\ dg}^{k}$,只包含边界附近的背景,而不是整张图

$$h_{i_bd}^{k} = \frac{\sum_{h,w} Z_{i}^{k} * y_{i_bd}^{k}}{\sum_{h,w} y_{i_bd}^{k}}; h_{i_bg}^{k} = \frac{\sum_{h,w} Z_{i}^{k} * y_{i_bg}^{k}}{\sum_{h,w} y_{i_bg}^{k}}, \quad (5)$$

 Z_i^k :denote the activation map extracted from layer I, which is interpolated with bilinear interpolation to keep consistent dimensions as y_i^k .产生的 $h_{i_bd}^k$ 和 $h_{i_bg}^k$ 都是一维向量。representing the averaged region-level features of the boundary and background pixels.



方法 Boundary-oriented meta optimization

4.对剩下的K-1个插值数据集使用同样操作。获得K个boudary-related和background-related features. (共2*K个数据集)

5.使用InfoNCE loss: InfoNCE 主要用在自监督学习中作为一个对比损失函数,只要构建好正负样本对,然后利用InfoNCE 的优化过程,就可以做到使正样本对之间的互信息最大,使负样本对之间的互信息最小。

 (h_m, h_p) : a pair of features, which is a positive pair if h_m and h_p are of the same class (both boundary-related or background-related) and otherwise negative pair.

$$\ell(h_m, h_p) = -\log \frac{\exp(h_m \odot h_p/\tau)}{\sum_{q=1, q \neq m}^{2K} \mathbb{F}(h_m, h_q) \cdot \exp(h_m \odot h_q/\tau)},$$
(6)

 $\mathcal{L}_{boundary} = \sum_{m=1}^{2K} \sum_{p=m+1}^{2K} \frac{(1 - \mathbb{F}(h_m, h_p)) \cdot \ell(h_m, h_p)}{B(K, 2) \times 2}, \quad (7)$

$$\mathcal{L}_{meta} = \mathcal{L}_{seg}(t_i^k; \hat{\theta}^k) + \gamma \mathcal{L}_{boundary}(x_i^k, t_i^k; \hat{\theta}^k), \quad (8)$$

$$\underset{ok}{\operatorname{arg\,min}} \mathcal{L}_{seg}(x_i^k; \theta^k) + \mathcal{L}_{meta}(x_i^k, t_i^k; \hat{\theta}^k). \tag{9}$$

1.InfoNCE的loss:一对输入,两个h分别由activation map得到的一维向量。分子,二者点乘,计算cos相似度,分母中F正对时为0,负对时为1。正对表示属于两张图属于同一类(同为boundary或同为background),τ为温度常数

2.B(K,2)代表组合数,从K个数据集中任选两个。正对时,F为0,存在边界损失。负对时,F为1,边界损失为0

3.最终的meta loss由dice loss和 boundary loss组成

在单个client完成inner-loop的meta-learning后,通过FedAvg方法汇聚局部模型的参数到全局模型

$$\theta = \sum_{k=1}^{K} \frac{N^k}{N} \theta^k$$
 $N = \sum_{k=1}^{K} N^k$

实验结果

数据集分布,眼底图4 个,前列腺MRI6个

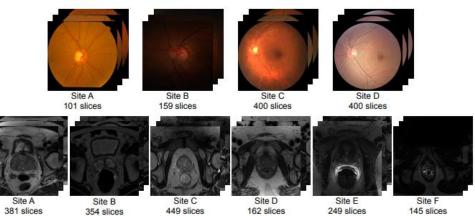


Figure 3. Example cases and slice number of each data source in fundus image segmentation and prostate MRI segmentation tasks.

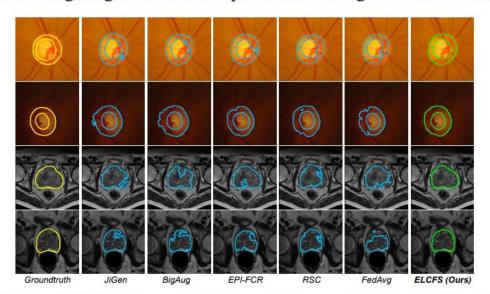


Figure 4. Qualitative comparison on the generalization results of different methods in fundus image segmentation (top two rows) and prostate MRI segmentation (bottom two tows).

Base Network:2D UNet

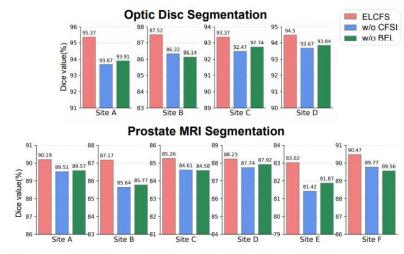
Table 1. Comparison of federated domain generalization results on Optic Disc/Cup segmentation from fundus images.

	Task	O	ptic Di	sc Segr	nentatio	on	O	ptic Cu	p Segn	nentatio	n	Overall	Optic Disc Segmentation Optic Cup Segmentation								n	Overall	
85	Unseen Site	A	В	C	D	Avg.	A	В	C	D	Avg.	Overall	A	В	C	D	Avg.	A	В	C	D	Avg.	Overall
		Dice Coefficient (Dice) ↑								Hausdorff Distance (HD)↓													
ľ	JiGen [3]	93.92	85.91	92.63	94.03	91.62	82.26	70.68	83.32	85.70	80.47	86.06	13.12	20.18	11.29	8.15	13.19	20.88	23.21	11.55	9.23	16.22	14.71
ı	BigAug [60]	93.49	86.18	92.09	93.67	91.36	81.62	69.46	82.64	84.51	79.56	85.46	16.91	19.01	11.53	8.76	14.05	21.21	23.10	12.02	10.47	16.70	15.39
1	Epi-FCR [25]	94.34	86.22	92.88	93.73	91.79	83.06	70.25	83.68	83.14	80.03	85.91	13.02	18.97	10.67	8.47	12.78	19.12	21.94	11.50	10.86	15.86	14.32
L	RSC [17]	94.50	86.21	92.23	94.15	91.77	81.77	69.37	83.40	84.82	79.84	85.80	19.44	19.26	13.47	8.14	15.08	23.85	24.01	11.38	9.79	17.25	16.16
	FedAvg [36]	92.88	85.73	92.07	93.21	90.97	80.84	69.71	82.28	83.35	79.05	85.01	17.01	20.68	11.70	9.33	14.68	20.77	26.01	11.85	10.03	17.17	15.93
	ELCFS (Ours)	95.37	87.52	93.37	94.50	92.69	84.13	71.88	83.94	85.51	81.37	87.03	11.36	17.10	10.83	7.24	11.63	18.65	19.36	11.17	8.91	14.52	13.07

Table 2. Comparison of federated domain generalization results on prostate MRI segmentation.

Unseen Site	A	В	C	D	Е	F	Average	A	В	C	D	E	F	Average		
		Dice Coefficient (Dice) ↑								Hausdorff Distance (HD)↓						
JiGen [3]	89.95	85.81	84.06	87.34	81.32	89.11	86.26	10.51	11.53	11.70	11.49	14.80	9.02	11.51		
BigAug [60]	89.63	84.62	83.86	87.66	81.20	88.96	85.99	10.68	11.78	12.07	10.66	13.98	9.73	11.48		
Epi-FCR [25]	89.72	85.39	84.97	86.55	80.63	89.76	86.17	10.60	12.31	12.29	12.00	15.68	8.81	11.95		
RSC [17]	88.86	85.56	84.36	86.21	79.97	89.80	85.80	10.57	11.84	14.76	13.07	14.79	8.83	12.31		
FedAvg [36]	89.02	84.48	84.11	86.30	80.38	89.15	85.57	11.64	12.01	14.86	11.80	14.90	9.30	12.42		
ELCFS (Ours)	90.19	87.17	85.26	88.23	83.02	90.47	87.39	10.30	11.49	11.50	11.57	11.08	8.31	10.88		

消融实验



证明两个模块 (连续频域插值 边界介导的情景 学习)都对模型 有重要贡献

Figure 5. Ablation results to analyze the effect of the two components (i.e. CFSI and BEL) in our method.

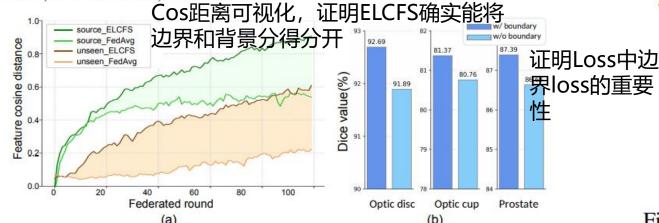


Figure 7. (a) Cosine distance between the boundary-related and background-related features; (b) Generalization performance of our method with or without the boundary-oriented meta objective.

用t-SNE分析可视化连 续频域插值对数据分布

对插值率λ的分析,证

Figure 6. (a) Visualization of t-SNE [34] embedding for the original fundus images at a local client (pink points) and the corresponding transformed images with amplitude spectrum from different clients (green, yellow, and blue points); (b) Generalization performance on optic disc segmentation under different settings of interpolation ratio λ , with fixed value or continuous sampling from different ranges (with error bar from three independent runs).

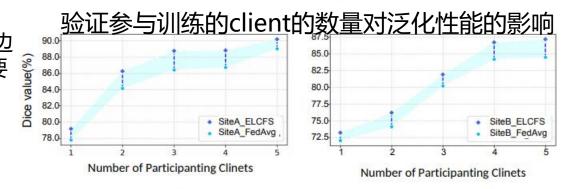
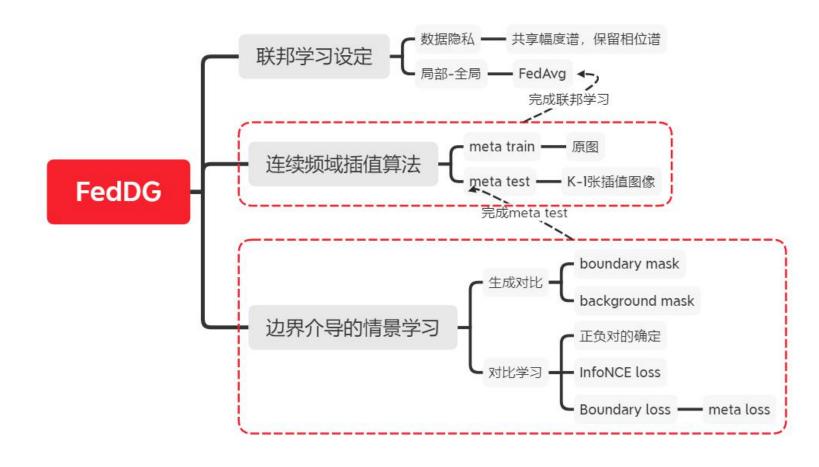


Figure 8. Curves of generalization performance on two unseen prostate datasets (i.e., site A and B) as the number of participating clients increases, using our proposed approach and FedAvg.

总结

Federal learning+domain generalization+meta learning+contrastive learning



(ISBI2020)

ASCNet: Adaptive-Scale Convolutional Neural Networks for Multi-Scale Feature Learning

HengMo Zhang, Jie Zhao, Xiang Li, Li Zhang, Quanzheng Li Peking University, Harvard Medical School

动机

• CNN在实现多尺度信息提取时遇到了困难,扩展卷积核会带来较高的计算代价,使用max pooling会牺牲图像信息。

前人工作

- 前人提出利用扩张卷积来增大感受野的大小。第一种是任意指定 每个卷积层的扩张率。第二类是使用膨胀卷积的金字塔结构来融 合来自多个尺度的信息。
- 虽然前述方法表明扩展卷积是有效的,但它有两个主要局限性
- 1)训练一个扩展的CNN需要额外调整扩张率
- 2)手动设计的扩张率只提供一个固定大小的接受场,这可能不适用于同一图像中的不同对象

Classic convolution

$$\mathbf{x}(\mathbf{p}) = \sum_{\mathbf{q}} f_{int}(\mathbf{q}, \mathbf{p}) \cdot \mathbf{x}(\mathbf{q}),$$
 (4)

从旁边的整数点坐标进行双线性插值

$$\mathbf{y}(\mathbf{p}_0) = \sum_{\mathbf{p}_n \in \mathcal{R}} \mathbf{w}(\mathbf{p}_n) \cdot \mathbf{x}(\mathbf{p}_0 + \mathbf{p}_n), \tag{1}$$
Dilated convolution

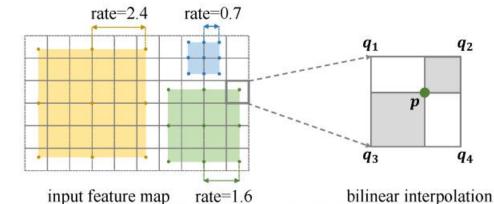
$$\mathbf{y}(\mathbf{p}_0) = \sum_{\mathbf{p}_n \in \mathcal{R}} \mathbf{w}(\mathbf{p}_n) \cdot \mathbf{x}(\mathbf{p}_0 + r \cdot \mathbf{p}_n),$$
 整数

(2)
$$f_{int}(\mathbf{q}, \mathbf{p}) = max(0, 1 - |q_x - p_x|) \cdot max(0, 1 - |q_y - p_y|),$$
 (5)

Adaptive-scale convolution

$$\mathbf{y}(\mathbf{p}_0) = \sum_{\mathbf{p}_n \in \mathcal{R}} \mathbf{w}(\mathbf{p}_n) \cdot \mathbf{x}(\mathbf{p}_0 + r(\mathbf{x}_0, \theta) \cdot \mathbf{p}_n), \tag{3}$$

(3)
$$\mathbf{y}(\mathbf{p}_0) = \sum_{\mathbf{p}_n \in \mathcal{R}} \mathbf{w}(\mathbf{p}_n) \cdot \mathbf{x}(\mathbf{p}_0 + r(\mathbf{x}, \theta) \cdot \mathbf{p}_n) = \sum_{\mathbf{p}_n \in \mathcal{R}} \mathbf{w}(\mathbf{p}_n) \cdot \sum_{\mathbf{q}} f_{int}(\mathbf{q}, \mathbf{p}) \cdot \mathbf{x}(\mathbf{q}).$$
(6)



自适应尺度卷积(ASC):

- 1)扩张率r是从原始数据中学习的,而不是人工分配 的
- 2)特征图上的不同像素使用自适应扩张率,而不是 相同的扩张率
- 3)扩张率r是浮点值,而不是整数

Fig. 1: The sampling process of ASC module. In the left panel, the colored dots represent the sampling locations of the ASC kernel. In the right panel, a bilinear interpolation is adopted when the dilation rate is a float number.

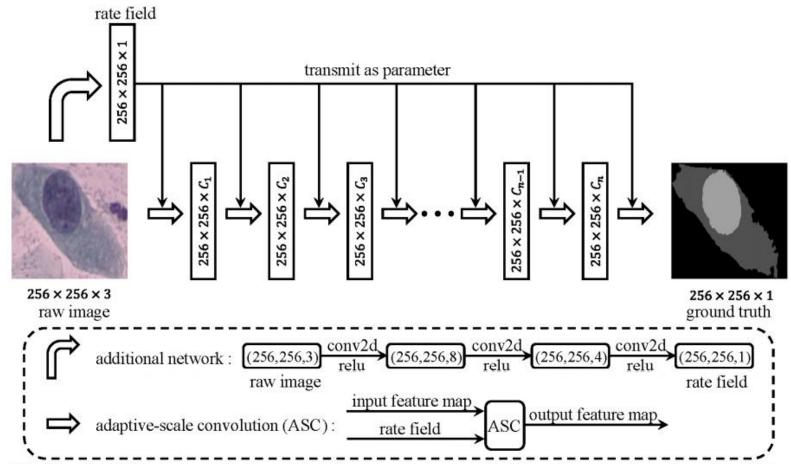


Fig. 2: Architecture of the adaptive-scale convolutional neural network. Note that raw image, rate field and intermediate feature maps have the same spatial dimensions.

实验结果

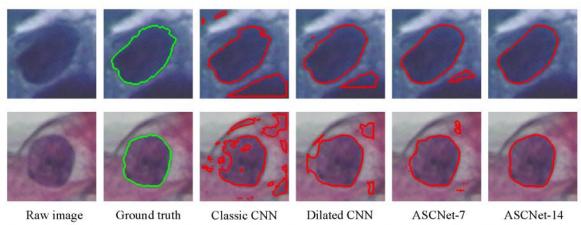


Fig. 3: Two examples of the segmentation results of the different models on the Herley dataset.

Herlev数据集:917幅宫颈细胞图像(562-训练,171-验证,184-测试)

SCD RBC数据集: 5个镰刀细胞的314个显微图像(250-训练,64-测试)

Table 1: Quantitative analysis of different methods in cell segmentation.

	The	Herlev da	taset	SCD RBC dataset					
	Dice	Precision	Recall	Dice	Precision	Recall			
Classic CNN	0.745	0.765	0.767	0.958	0.967	0.949			
Dilated CNN	0.824	0.817	0.890	0.956	0.960	0.953			
ASCNet-7	0.857	0.863	0.891	0.959	0.960	0.958			
U-Net [13, 14]	0.869	0.897	0.879	0.957	0.955				
ASCNet-14	0.906	0.909	0.925	0.967	0.973	0.961			

- 1)Classic CNN:7个标准卷积组成,前6个卷积的通道数设为8,最后一层的通道数与分类数一致,以生成分割结果
- 2)Dilated CNN:包含7个膨胀率分别为1、1、2、
- 4、8、16和1的膨胀卷积
- 3)U-Net
- 4)ASCNet-7:7个自适应尺度卷积,通道数设置与 classic CNN相同
- 5)ASCNet-14: 14个自适应尺度卷积,其中前13个卷积的通道数设置为32,最后一层的通道数与分类数一致

实验结果

通过可视化发现,最优扩 张率与分割目标的大小呈 正相关

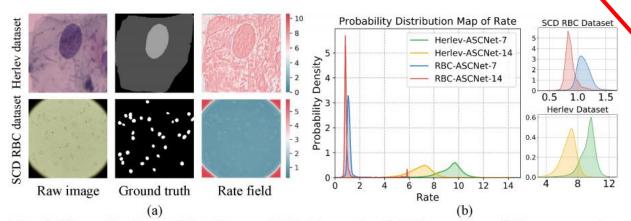


Fig. 4: Visualization of the learned dilation rate. (a) Examples of the segmentation labels and learned rate fields. Top row: Herlev dataset; Bottom row: SCD RBC dataset. (b) An illustration of the distributions of the learned dilation rates. The red spike at approximately 6 is caused by the learned rates of image background in the four corners.

- 1.对于Herlev数据集,宫颈细胞以高倍率成像。 因此,ASCNet相应地产生更大的扩张率,这更 能够聚集大对象的全局信息。
- 2.对于SCD RBC数据集,红细胞是以低放大倍数成像的,因此ASCNet选择通过产生较小的扩张率来捕捉更多局部和精细细节。
- 3.ASCNet-14产生的扩张率比ASCNet-7产生的扩张率小,由于ASCNet中的所有卷积都共享相同的扩张率场,较深的感受场被线性放大更多倍,因此每一卷积层需要较小的扩张率。