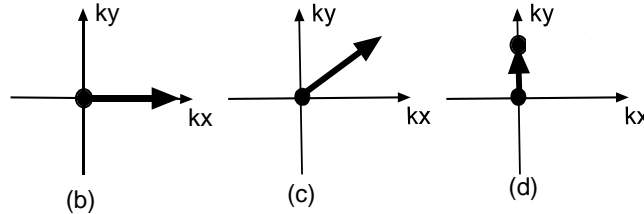


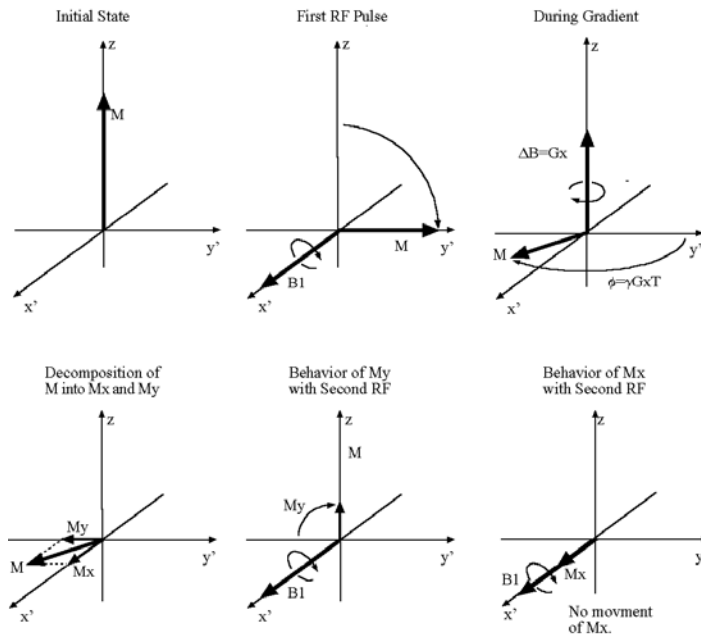
Solutions, Homework #5

1.

- $M_0(u,v) = XY \text{sinc}(Xu) \text{sinc}(Yv)$
- $k_x(t) = \gamma At/(2\pi)$, $k_y(t) = 0$. Assuming that the scaling constant is 1, then $s(t) = XY \text{sinc}(X\gamma At/(2\pi))$
- $k_x(t) = \gamma at/(2\pi X)$, $k_y(t) = \gamma at/(2\pi Y)$. $s(t) = XY \text{sinc}^2(\gamma at/(2\pi))$.
- For $t \in [0, T]$, $k_x(t) = 0$, $k_y(t) = \gamma at/(2\pi Y)$. $s(t) = XY \text{sinc}(\gamma at/(2\pi))$
For $t > T$, $k_x(t) = 0$, $k_y(t) = \gamma aT/(2\pi Y) = 2/Y$.
 $s(t) = XY \text{sinc}(0) \text{sinc}(2) = 0$.



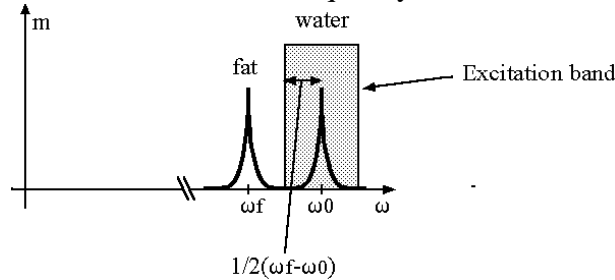
- First of all, $m_0(x) = 1$ implies that the magnetization is uniform everywhere. The first RF pulse tips the magnetization into the transverse plane. Looking in the rotating frame, \mathbf{M} lies along the y' -axis. We then apply a gradient that makes the resonant frequency vary as a function of spatial position $\omega(x) = \omega_0 + \gamma Gx$. In the rotating frame, the resonant frequency is $\omega_{\text{rot}}(x) = \gamma Gx$. Assuming that the gradient is turned on for length of time, T , then the phase that accumulates (as a function of spatial position) is $\phi_{\text{rot}}(x) = \gamma GxT$. We can decompose the magnetization vector into two components $M_{x,\text{rot}} = \sin(\phi)$ and $M_{y,\text{rot}} = \cos(\phi)$. During the second RF pulse $-M_{y,\text{rot}}$ is rotated up to M_z and $M_{x,\text{rot}}$ does not change. Ultimately, we end up with a sinusoidal variation with x of the x - and z -components of the magnetization.



- $m_{xy,\text{rot}}(x) = 0$; $m_z(x) = m_0$
- $m_{xy,\text{rot}}(x) = i m_0$; $m_z(x) = 0$
- $m_{xy,\text{rot}}(x) = i m_0 \exp(-i \gamma GxT) = i m_0 \cos(\gamma GxT) + m_0 \sin(\gamma GxT)$; $m_z(x) = 0$
- $m_{xy,\text{rot}}(x) = m_0 \sin(\gamma GxT)$; $m_z(x) = -m_0 \cos(\gamma GxT)$

3.

- a. $\gamma/2\pi = 42.58 \text{ MHz/T}$, so $f_0 = (42.58 \text{ MHz/T})(1.5 \text{ T}) = 63.87 \text{ MHz}$ and $\Delta f = f_0 - f_f = \gamma/2\pi B_0 \delta_f = (42.58 \text{ MHz/T})(1.5 \text{ T})(3.5 \times 10^{-6}) = 223.5 \text{ Hz}$.
- b. As shown in the drawing below, one possible excitation pulse will be centered at the frequency of water, f_0 , and will have a rectangular frequency profile with a half-bandwidth of $1/2$ of the difference in water and fat frequencies. The water excitation pulse, therefore, will have a center frequency of f_0 and a bandwidth of $\Delta f = f_0 - f_f$.



which has a spectrum $\text{rect}((f-f_0)/\Delta f)$. The RF pulse will then be similar to the IFT of this function – $B_{1,\text{rot}}(t) = A \text{ sinc}(t/T)$ (perhaps truncated with a rect or hanning window), where $1/T = \Delta f = 223.5 \text{ Hz}$ or $T = 4.47 \text{ ms}$. The integrated areas under this RF pulse is $\gamma A T$, which for a 90 degree flip angle, should be set equal to $\pi/2$. Thus, $A = \pi/(2\gamma T)$. The carrier frequency at which it is applied will be $f_0 = 63.87 \text{ MHz}$. The RF pulse will now look like: $B_{1,xy}(t) = A \text{ sinc}(t/T) \exp(-i2\pi f_0 t)$. (Recall that spins in MRI go in the negative frequency direction.)

4.

- a. $\text{FOV}_z = 1/\Delta k_z$ and $\Delta k_z = \gamma/2\pi T_z \Delta G_z$, thus $\Delta G_z = 2\pi/(\gamma T_z \text{FOV}_z) = 0.023 \text{ mT/m}$.
- b. $\Delta z = 1/(2k_{z,\text{max}})$ and $k_{z,\text{max}} = \gamma/2\pi T_z G_{z,\text{max}}$, thus $G_{z,\text{max}} = 2\pi/(\gamma T_z 2 \Delta z) = 0.47 \text{ mT/m}$.
- c. $\text{FOV}_y = 1/\Delta k_y$ and $\Delta k_y = \gamma/2\pi T_y \Delta G_y$, thus $\Delta G_y = 2\pi/(\gamma T_y \text{FOV}_y) = 0.023 \text{ mT/m}$.
- d. $\Delta y = 1/(2k_{y,\text{max}})$ and $k_{y,\text{max}} = \gamma/2\pi T_y G_{y,\text{max}}$, thus $G_{y,\text{max}} = 2\pi/(\gamma T_y 2 \Delta y) = 1.17 \text{ mT/m}$.
- e. $\Delta x = 1/W_{kx}$ and $W_{kx} = \gamma/2\pi T_{\text{read}} G_{\text{read}}$, thus $G_{\text{read}} = 2\pi/(\gamma T_{\text{read}} \Delta x) = 1.17 \text{ mT/m}$.
- f. $\text{FOV}_x = 1/\Delta k_x$ and $\Delta k_x = \gamma/2\pi \Delta t G_{\text{read}}$ and $G_{\text{read}} = 2\pi/(\gamma T_{\text{read}} \Delta x)$, thus $\Delta t = T_{\text{read}} \Delta x / \text{FOV}_x = 0.1 \text{ ms} (100 \mu\text{s})$.

5. Let the signal strength (as a function of x) is equal to sensitivity $S(x)$ and the noise is equal to σ . The signal to noise ratio is then $S(x)/\sigma$. For the volume coil $S_v(x) = 1$ and $\sigma_v = 1$, therefore $SNR_v = 1$. For the surface coil, the SNR is

$$SNR_s = \frac{1}{(0.1 \cdot a)^{3/2} \left(1 + \left(\frac{x}{a}\right)^2\right)^{3/2}} = \frac{1}{\left((0.1 \cdot a) \left(1 + \left(\frac{x}{a}\right)^2\right)\right)^{3/2}}$$

To find the region where $SNR_s > SNR_v$, we merely need to find for which x that $SNR_s > 1$.

- a. $a = 5$ cm, $SNR_s > SNR_v$, for $x < 5$ cm, that is if we are interested in a structure closer to the coil than 5 cm, it is preferred (from the SNR standpoint) to use the surface coil, otherwise the volume coil is better.

$$\begin{aligned} SNR_s &= \frac{1}{\left(0.5 \left(1 + \left(\frac{x}{5}\right)^2\right)\right)^{3/2}} > 1 \\ 0.5 \left(1 + \left(\frac{x}{5}\right)^2\right) &< 1 \\ \left(\frac{x}{5}\right)^2 &< 1 \\ x &< 5 \end{aligned}$$

- b. $a = 10$ cm, $SNR_v > SNR_s$, for all non-zero values of x , therefore, the volume will always have better SNR. (No values of x satisfy the below relationship.)

$$\begin{aligned} SNR_s &= \frac{1}{\left(1 \left(1 + \left(\frac{x}{10}\right)^2\right)\right)^{3/2}} > 1 \\ \left(1 + \left(\frac{x}{10}\right)^2\right) &< 1 \\ \left(\frac{x}{10}\right)^2 &< 0 \\ x^2 &< 0 \end{aligned}$$