# Computer- and robot-assisted Surgery





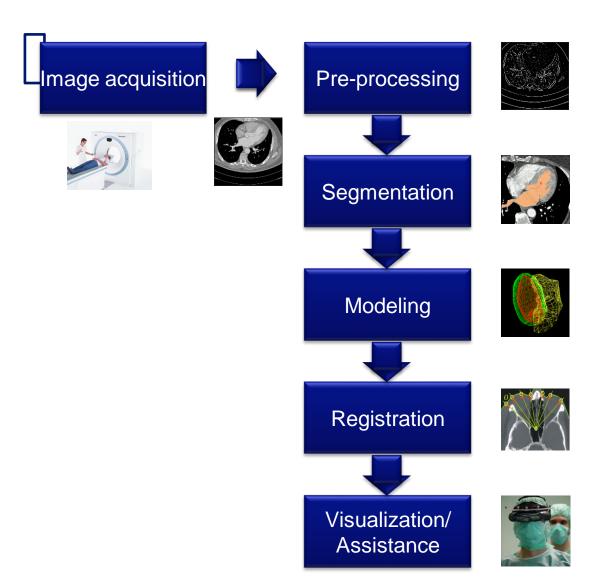
Lecture 7
Basics of Computer Vision – Part 2

NATIONALES CENTRUM FÜR TUMORERKRANKUNGEN PARTNERSTANDORT DRESDEN UNIVERSITÄTS KREBSCENTRUM UCC

#### getragen von:

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# Process chain computer-assisted surgery





## Interaction and Feedback

<a href="https://pingo.coactum.de">https://pingo.coactum.de</a> -> 392473

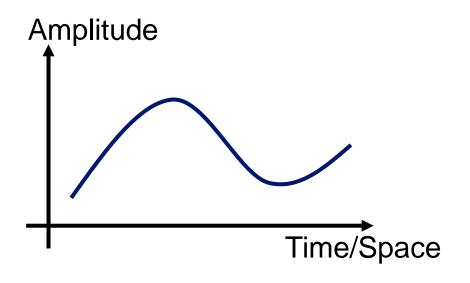


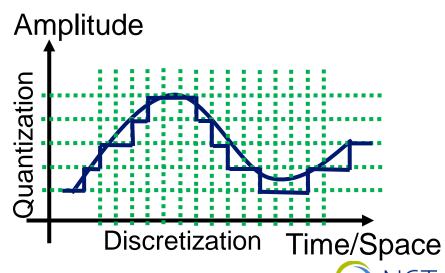


Context:



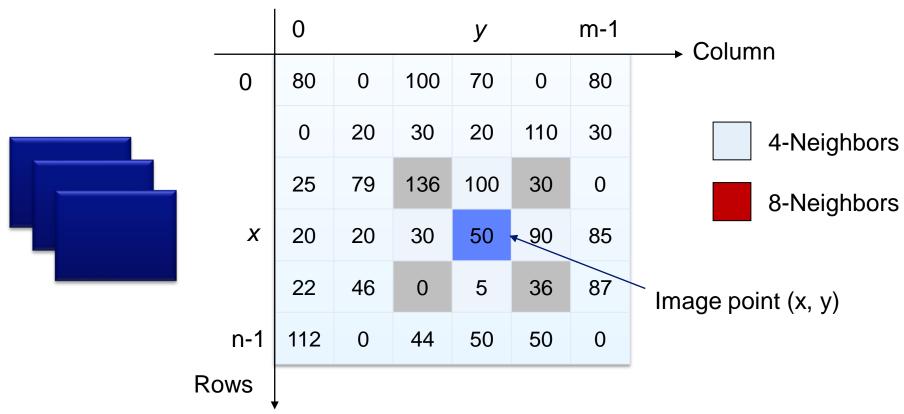
Digitalization: Discretization + Quantization





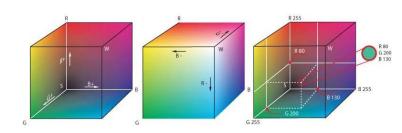
2D grayscale image: Discrete function

Img: 
$$[0..n] \times [0..m] \rightarrow [0..q]$$
  
 $(x, y) \mapsto G(x, y) = g$ 



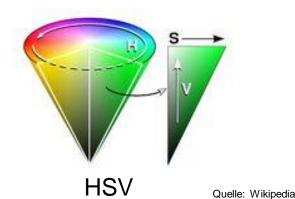


- Color image: different models for different applications
  - B/W: Grayscale
  - RGB-model: specific for screens (Phosphor-crystals), very common
  - CMYK-model: Color printer (subtractive color mix)
  - YCbCr: Breakdown into luminescence Y und two color components Cb, Cr
  - HSV (Hue, Saturation, Value): specific for color segmentation



**RGB** 







RGB-model:

Img: 
$$[0..n] \times [0..m] \rightarrow [0..R] \times [0..G] \times [0..B]$$
  
 $(x, y) \mapsto G(x, y) = (r, g, b)$ 

3 components: red, green and blue usually 256 x 256 x 256 nuances = 16,8 Mio. colors



#### Conversion between different models

• RGB to B/W: 
$$I = \frac{R+G+B}{3}$$

• RGB to HSV: 
$$V = MAX(R, G, B)$$
 or  $V = \frac{R+G+B}{3}$ 

$$S = 1 - \frac{MIN(R,G,B)}{V} \text{ or } S = \begin{cases} \frac{3}{2}(R - V), B + R \ge 2G \\ \frac{3}{2}(V - B), B + R < 2G \end{cases}$$

$$H = \begin{cases} 60^{\circ} (0 + \frac{G - B}{MAX(R,G,B) - MIN(R,G,B)}), & R = MAX(R,G,B) \\ B - R & G \end{cases}$$

$$G = MAX(R,G,B)$$

$$R - G$$

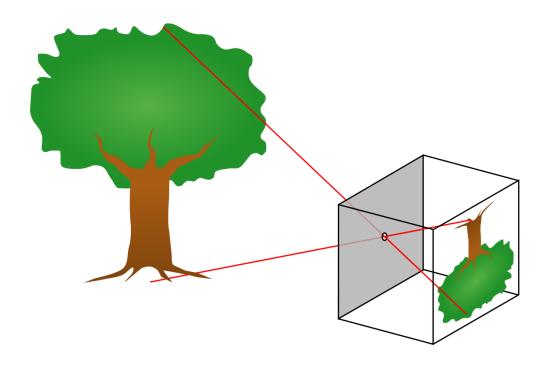
$$G = MAX(R,G,B)$$

$$R - G$$



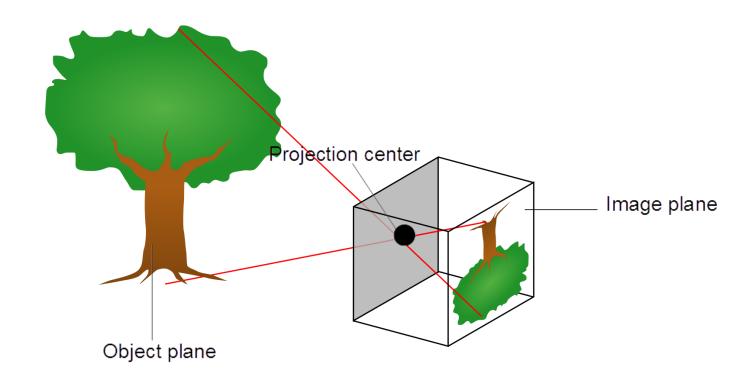
## Pinhole camera model

- Describes mathematical relationship between coordinates in 3D and their projection on a 2D plane
  - Simple model
  - No modeling of lens
  - No world coordinate system



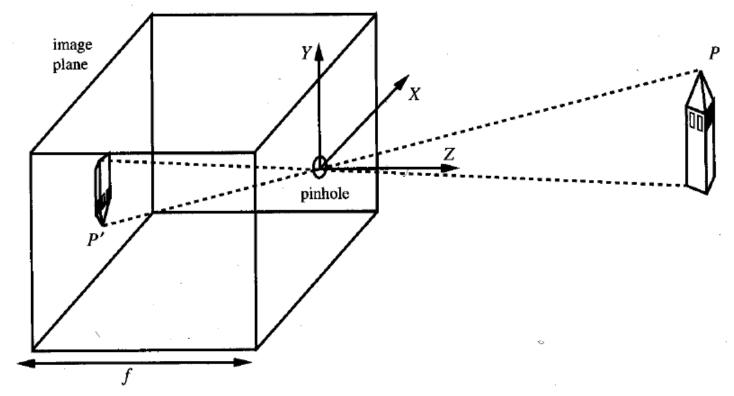


## Pinhole camera model





#### Pinhole camera model



Projection of 3D point P = (x, y, z) onto an image point p = (u, v, w) with focal length f:

$$-\frac{u}{f} = \frac{x}{z} \qquad -\frac{v}{f} = \frac{y}{z} \qquad w = -f$$

$$p = \begin{pmatrix} u \\ v \\ w \end{pmatrix} = \begin{pmatrix} u \\ v \\ -f \end{pmatrix} = -\frac{f}{z} \begin{pmatrix} x \\ y \\ z \end{pmatrix} = -\frac{f}{z} P$$

$$x = -\frac{uz}{f} \qquad y = -\frac{vz}{f}$$

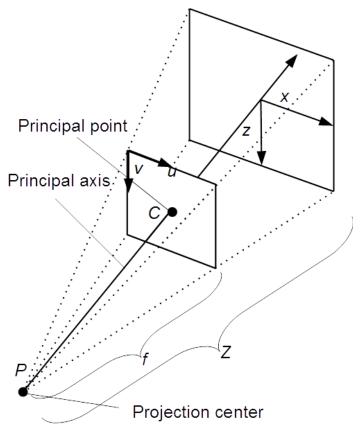
**Back projection** 



- Pinhole camera model strongly simplifies reality
  - Image origin identical with principle point
  - Pixels are square
  - No lens distortion
  - No world coordinate system
- Therefore in practice, extensions are used
- A few definitions:
  - Principal axis: Line through the projection center, orthogonal to image plane
  - Principal point C: Point of intersection of principal axis and image plane
  - Image coordinate system: 2D, unit [pixels]. Origin in the upper left corner uaxis to the right, v-axis to the bottom
  - Camera coordinate system: 3D, unit [mm]. Origin in the projection center, axis
    parallel to those of the image coordinate system (x to u, y to v and z away
    from the projection center)
  - World coordinate system: 3D, unit [mm]. Origin arbitrary, anywhere in space possible



Common variant: Pinhole camera model in positive position



$$\begin{pmatrix} u \\ v \\ w \end{pmatrix} = -\frac{f}{z} \begin{pmatrix} x \\ y \\ z \end{pmatrix} \quad \Longrightarrow \quad \begin{pmatrix} u \\ v \\ w \end{pmatrix} = \frac{f}{z} \begin{pmatrix} x \\ y \\ z \end{pmatrix}$$

- Projection center behind image plane
- No mirroring (negative signs are omitted)



#### Intrinsic parameters

- Focal length f
  - In practice, the conversion from [mm] to [pixel] is incorporated into the focal length
  - As we assume non-quadratic but rectangular pixels, there is a parameter for each direction:  $f_x$ ,  $f_y$
  - Since product of actual focal length [mm] and conversion factor [pixel/mm] they have the unit [pixel]
- Principal point  $c(c_x, c_y)$ 
  - · Point of intersection of principle axis and image plane
  - Has to be taken into consideration when moving origin of image plane

$$\begin{pmatrix} u \\ v \\ w \end{pmatrix} = \frac{f}{z} \begin{pmatrix} x \\ y \\ z \end{pmatrix} \qquad \Longrightarrow \qquad \begin{pmatrix} u \\ v \end{pmatrix} = \frac{1}{z} \begin{pmatrix} f_x \cdot x \\ f_y \cdot y \end{pmatrix} + \begin{pmatrix} c_x \\ c_y \end{pmatrix}$$



# Which of the following coordinate systems is NOT in 3D?

- A: Image coordinate system
- B: Camera coordinate system
- C: World coordinate system
- D: None of the above



## Homogenous coordinates

$$\binom{u}{v} = \frac{1}{z} \binom{f_x \cdot x}{f_y \cdot y} + \binom{c_x}{c_y} \text{can be expressed better}$$

- Homogenous coordinates
- mogenous coordinates
  Add a new dimension with value of 1 to vector, e.g.:  $\begin{pmatrix} x \\ y \\ z \end{pmatrix} \rightarrow \begin{pmatrix} x \\ y \\ z \end{pmatrix} \quad \begin{pmatrix} u \\ v \end{pmatrix} \rightarrow \begin{pmatrix} u \\ v \end{pmatrix}$
- Allows expression of certain operations with matrix multiplication

$$\binom{u}{v} = \frac{1}{z} \binom{f_x \cdot x}{f_y \cdot y} + \binom{c_x}{c_y} \to \binom{u \cdot w}{v \cdot w} = \binom{f_x}{0} \quad \binom{0}{f_y} \quad \binom{c_x}{0} \\ 0 \quad 0 \quad 1 \\ \end{pmatrix} \cdot \binom{x}{y}$$

Afterwards, normalize so the "additional" dimension becomes 1:

$$\frac{1}{w} \cdot \begin{pmatrix} u \cdot w \\ v \cdot w \\ w \end{pmatrix} = \begin{pmatrix} u \\ v \\ 1 \end{pmatrix} \to \begin{pmatrix} u \\ v \end{pmatrix}$$



#### Intrinsic parameters

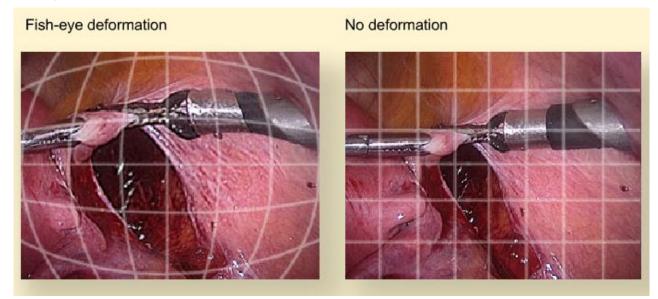
- Focal length f
  - In practice, the conversion from [mm] to [pixel] is incorporated into the focal length
  - As we assume non-quadratic but rectangular pixels, there is a parameter for each direction:  $f_x$ ,  $f_y$
  - Since product of actual focal length [mm] and conversion factor [pixel/mm] they have the unit [pixel]
- Principal point  $c(c_x, c_y)$ 
  - Point of intersection of principal axis and image plane
  - · Has to be taken into consideration when moving origin of image plane
- Contained in the camera matrix K

$$K = \begin{pmatrix} f_{\mathcal{X}} & 0 & c_{\mathcal{X}} \\ 0 & f_{\mathcal{Y}} & c_{\mathcal{Y}} \\ 0 & 0 & 1 \end{pmatrix}$$



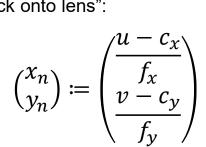
#### Lens distortion

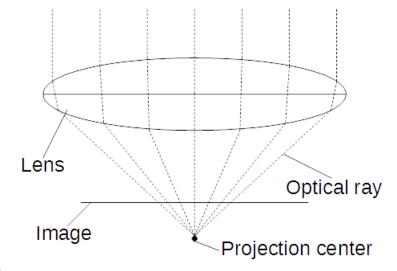
- Wide angle lenses (often encountered in endoscope) can significantly distort the image
  - Radial distortion
    - Symmetric from principle point
  - Other types of distortion are possible





- Intrinsic parameters
  - Radial lens distortion
    - · Project points "back onto lens":



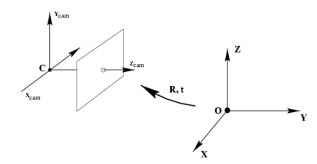


- Distortion is proportional to distance from principle point  $r \coloneqq \sqrt{x_n^2 + y_n^2}$
- The distorted coordinate can then be computed from a distortion model
- Often approximated using first two or three terms of a Taylor polynomial

$${\chi_d \choose y_d} = (1 + \boldsymbol{d_1}r^2 + \boldsymbol{d_2}r^4 + \cdots) {\chi_n \choose y_n}$$

Images can be "undistorted" by using a lookup table and interpolation





- Extrinsic parameters
  - Offset camera to world coordinate, e.g. when using multiple cameras or a robot
  - Transformation from world to camera coordinate system
  - Defined through a coordinate transform consisting of
    - Rotation matrix R

$$R = R_z(\gamma)R_v(\beta)R_x(\alpha)$$

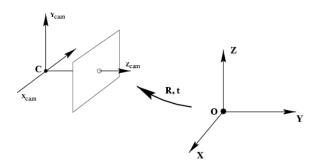
$$R_{x}(\alpha) = \begin{pmatrix} 1 & 0 & 0 \\ 0 & \cos(\alpha) & -\sin(\alpha) \\ 0 & \sin(\alpha) & \cos(\alpha) \end{pmatrix} R_{y}(\beta) = \begin{pmatrix} \cos(\beta) & 0 & \sin(\beta) \\ 0 & 1 & 0 \\ -\sin(\beta) & 0 & \cos(\beta) \end{pmatrix}$$

$$R_{z}(\gamma) = \begin{pmatrix} \cos(\gamma) & -\sin(\gamma) & 0\\ \sin(\gamma) & \cos(\gamma) & 0\\ 0 & 0 & 1 \end{pmatrix}$$

Translation vector t

$$t = \begin{pmatrix} t_x \\ t_y \\ t_z \end{pmatrix}$$





- Extrinsic parameters
  - Offset camera to world coordinate, e.g. when using multiple cameras or a robot
  - Transformation from world to camera coordinate system
  - Defined through a coordinate transform consisting of
    - Rotation matrix R
    - Translation vector t

$$x_c = R \cdot x_w + t$$

• In homogenous coordinates:

$$\begin{pmatrix} x_c \\ 1 \end{pmatrix} = \begin{pmatrix} & & R & & t \\ 0 & 0 & 0 & 1 \end{pmatrix} \begin{pmatrix} x_w \\ 1 \end{pmatrix}$$

 Projection matrix P: 3x4 matrix containing both intrinsic and extrinsic parameters

$$\begin{pmatrix} u \cdot w \\ v \cdot w \\ w \end{pmatrix} = P \begin{pmatrix} x \\ y \\ z \\ 1 \end{pmatrix} \qquad P = (KR|Kt)$$



# Which of the following is NOT contained in the projection matrix?

- A: Principal point
- B: Focal length
- C: Lens distortion parameters
- D: Translation to world coordinate system



#### Camera calibration

- Process of determining intrinsic and extrinsic parameters
- Intrinsic parameters should remain constant for different setups unless zoom or focus of a camera changes
- Extrinsic parameters are dependent on the selection of world coordinate system and change depending on setup
- Once calibrated, a function f is know that maps points in world coordinate system onto the image coordinate system  $f: \mathbb{R}^3 \to \mathbb{R}^2$
- f is defined through the projection matrix P and normalizing of the homogenous coordinates
- The inverse function maps a point of the image coordinate system onto a straight line in world coordinate system that runs through the projection center

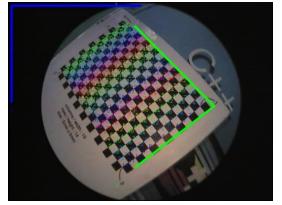


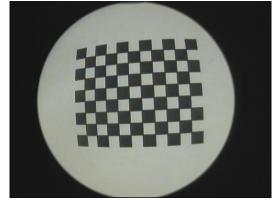
#### Camera calibration

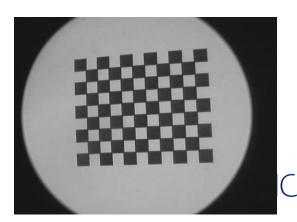
#### Wanted:

P is a  $3\times4$ -Matrix => 12 unknown variables

- Process calibration:
  - 1. Locating a number of 3D/2D point correspondences
  - 3D points are known from usage of an appropriate calibration object or pattern
  - 3. 2D points are located through computer vision methods
  - 4. Estimation of P
  - 5. Estimation of distortion parameters from backprojection error
  - 6. Undistort 2D points and repeat from 4.







### **Direct Linear Transformation**

 Standard method for computation of projection matrix P is the Direct Linear Transformation (DLT)

$$\begin{pmatrix} x \cdot w \\ y \cdot w \\ w \end{pmatrix} = P \begin{pmatrix} X \\ Y \\ Z \\ 1 \end{pmatrix} \quad P = (K R \mid K \mathbf{t}) = \begin{pmatrix} p_1 & p_2 & p_3 & p_4 \\ p_5 & p_6 & p_7 & p_8 \\ p_9 & p_{10} & p_{11} & p_{12} \end{pmatrix}$$

$$\Rightarrow x = \frac{p_1 X + p_2 Y + p_3 Z + p_4}{p_9 X + p_{10} Y + p_{11} Z + p_{12}} \text{ One parameter can be normalized.}$$

$$y = \frac{p_5 X + p_6 Y + p_7 Z + p_8}{p_9 X + p_{10} Y + p_{11} Z + p_{12}}$$



#### **Direct Linear Transformation**

$$\Rightarrow \begin{array}{l} p_1X + p_2Y + p_3Z + p_4 = xp_9X + xp_{10}Y + xp_{11}Z + x \\ p_5X + p_6Y + p_7Z + p_8 = yp_9X + yp_{10}Y + yp_{11}Z + y \end{array}$$

• Formulation as a linear system Ax = b with  $n \ge 6$  point correspondences



## 3D cameras

Until now: 2D vision

 Spatial information only secondary (experience)

Goal: Computer-assistance via 3D model

- Navigation
- Augmented reality



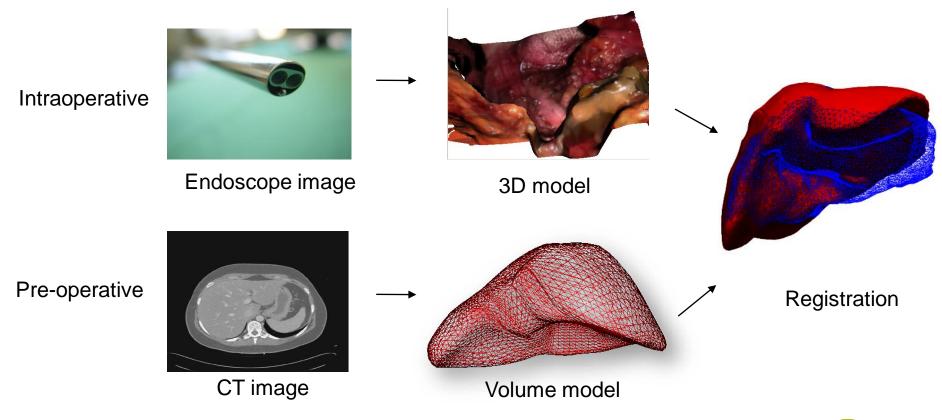






## 3D endoscopy

- Goal: Navigation, augmented reality
  - Create intraoperative model with the endoscope
  - Registration with pre-operative model





## 3D endoscopy

- Applications without 3D reconstruction
  - E.g. Shutter glasses
  - Accessories required (Glasses, ...)
- Applications with 3D reconstruction
  - Active or passive methods:
    - Stereo endoscopy
    - Structure from Motion
    - Time-of-Flight
    - Structured Light
  - Different endoscope types





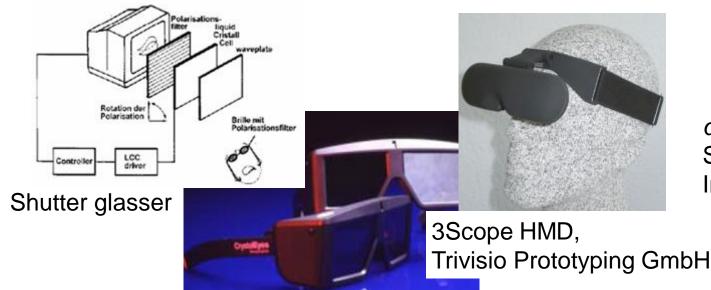


#### Methods without 3D reconstruction

No computer-support

Depth perception is a result from the natural stereo vision of

the viewer



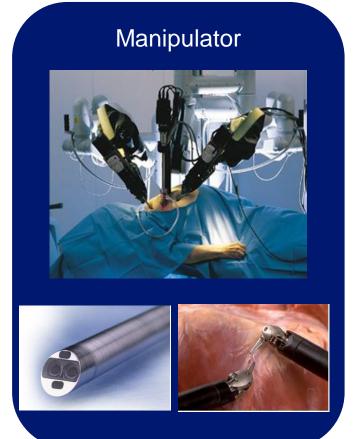


da Vinci<sup>®</sup>
Surgical robot,
Intuitive Surgical, Inc.



## DaVinci





Quelle: Intuitive Surgical



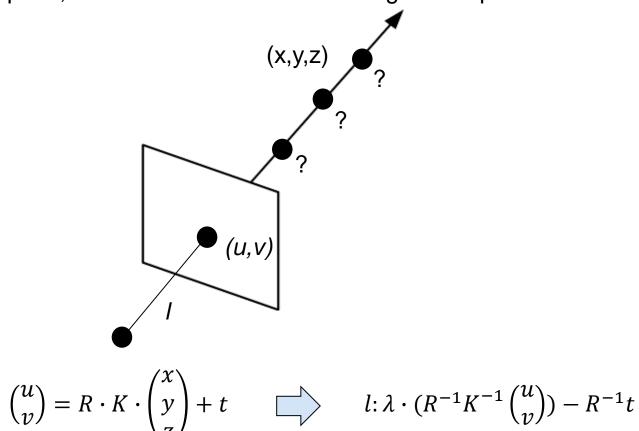
# DaVinci





## 2D to 3D

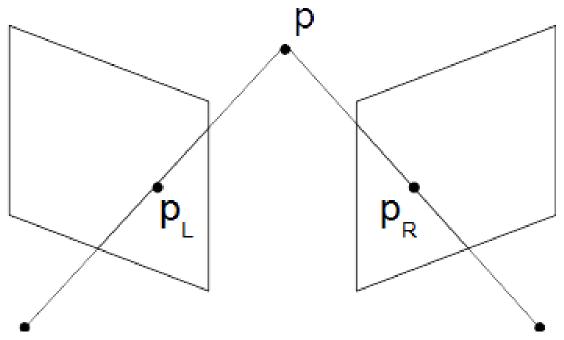
Given a 2D point, how do we reconstruct the original 3D point?



 $\lambda$  variable describing position on line l



## Stereo camera system - Triangulation



Given two calibrated cameras, each containing a projection  $(p_1, p_2)$  of point p, two lines can be computed:

$$l_L(\lambda_L) = \lambda_L \cdot (R_L^{-1} K_L^{-1}) - R_L^{-1} t_L$$
  
$$l_R(\lambda_R) = \lambda_R \cdot (R_R^{-1} K_R^{-1}) - R_R^{-1} t_R$$

Solve for  $\lambda_L$ ,  $\lambda_R$  so that  $l_L(\lambda_L) = l_R(\lambda_R)$ , reconstructing point p



## Stereo endoscopy

**Used endoscope:** Stereo endoscope (two channels)

**Reconstruction:** Triangulation with known

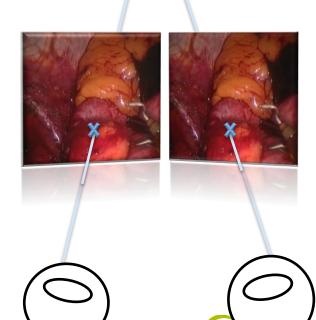
relationship between the two

cameras

**Pro:** known stereoscopic basis

**Cons:** greater diameter

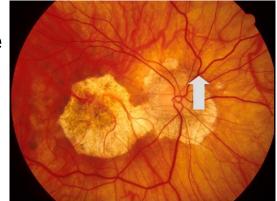
more expensive endoscope

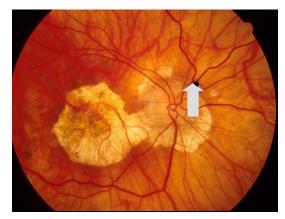


## **Problem Stereo**

• Correspondence:

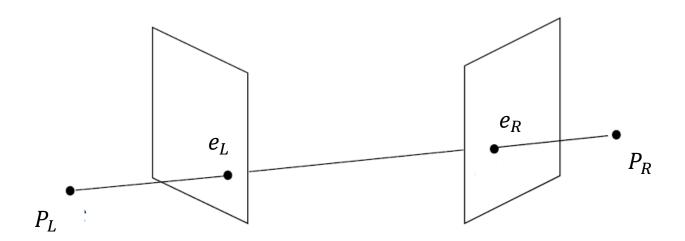
Which point in the left image belongs to which point in the right image?





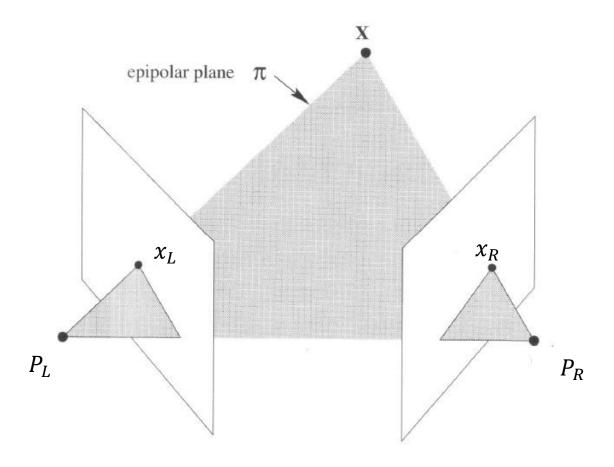


- Relationship between two cameras is described through *Epipolar geometry*
- The points of intersection,  $e_L$ ,  $e_R$ , of the line between the projection centers,  $P_L$ ,  $P_R$ , are called *epipoles*



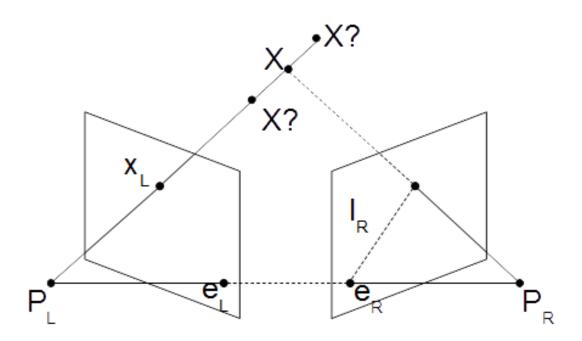


- Epipolar plane  $\pi(X)$ :
  - Plane created through a 3D point X in the scene and the two projection centers  $P_L$ ,  $P_R$



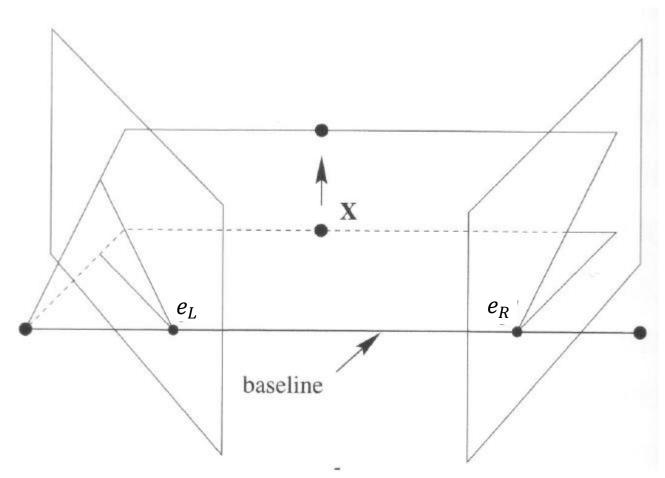


- Epipolar line  $l_R(x_L)$ : line of intersection of  $\pi(X)$  and image plane
  - All 3D points X that could be projected onto  $x_L$  in the left image, are mapped onto a line  $l_R(x_L)$  in the right image





• All epipolar lines of a stereo camera system intersect in the epipoles  $e_L$ ,  $e_R$ 





#### Usage:

- Reduction of the correspondence problem from two dimensions onto one dimension, as only points on an epipolar line have to be considered:
  - Higher robustness (less wrong correspondences)
  - Higher efficiency





Quelle: Multiple View Geometry



#### Fundamental matrix

- Mathematical description of the epipolar geometrie
- Properties of the Fundamental matrix F
  - 3x3 matrix
  - Has rank of 2
  - For all corresponding points  $x_L$ ,  $x_R$ :
    - $x_L^T F x_R = 0$  ( $x_L$ ,  $x_R$  are image points in homogenous form with w = 1



#### Fundamental matrix

- Can be used to compute epipolar lines:
  - $l_L(x_R) = F^T x_R$
  - $l_R(x_L) = Fx_L$
- For the epipoles:
  - $F^T e_R = 0$
  - $Fe_L = 0$
- $l_L$  ( $l_R$  analog) describes a 2D line in the following manner:
  - $l_L x = 0$  for all x (in homogenous form with w = 1) that lie on this line
- Fundamental matrix can be compute in multiple ways
  - Using known image correspondences in the left and right images
  - When intrinsic and extrinsic parameters are known, directly using  $K_L$  and  $K_R$  and the Essential matrix E, which contains the extrinsic parameters



#### Fundamental matrix

- Computation with know intrinsic and extrinsic parameters
  - Assumption extrinsic parameters
    - Left camera (I|0) as transformation, i.e. identity
    - Right camera (R|t) as transformation
  - Essential matrix *E* can be computed in the following manner:

• 
$$E = [t]_{\mathcal{X}} \cdot R = \begin{pmatrix} 0 & -t_z & t_y \\ t_z & 0 & -t_x \\ -t_y & t_x & 0 \end{pmatrix} R$$

• Fundamental matrix *F* can then be composed:

• 
$$F = K_R^{-T} \cdot E \cdot K_L^{-1}$$

 If the Fundamental matrix has been computed from point correspondences and the intrinsic parameters are known, the Essential matrix can be computed:

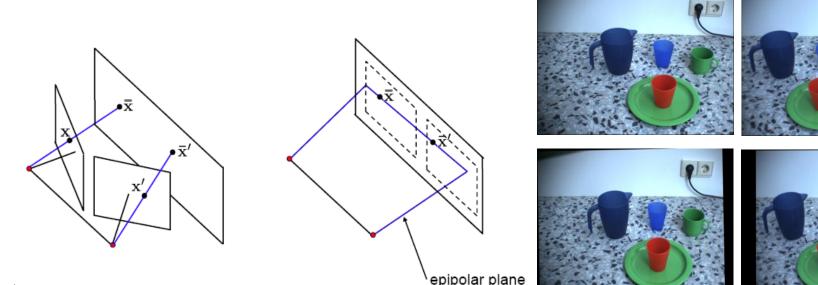
• 
$$E = K_R^T \cdot F \cdot K_L$$



#### Rectification

- If the epipolar geometry is know, images can be rectified:
  - Epipolar lines are parallel to the horizontal axis in a rectified image pair
  - Search for correspondences is restricted on a horizontal direction

Corresponding points share same y-coordinate,
 difference in x-coordinate is called disparity d



#### Rectification

 Rectified images have the benefit that optimized algorithms for correlation can be used to find correspondences

#### Cons:

- Interpolation necessary for rectifying images
- Depending on setup, images can be highly distorted



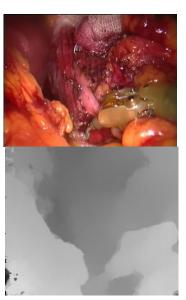
# Rectification Which statement is incorrect?

- A: only possible with calibration
- B: reduces image quality
- C: improves runtime
- D: reduces dimensionalty during correspondence analysis

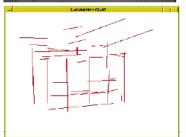


## Correspondence analysis

- Classification into 2 types:
  - Correlation-based approaches
    - Correspondence for each pixel
    - Dense depth map
    - Application: Textured scene
  - Feature-based approaches:
    - Correspondence only for certain features
    - Sparse depth map
    - Application: Structured scene (Indoor)



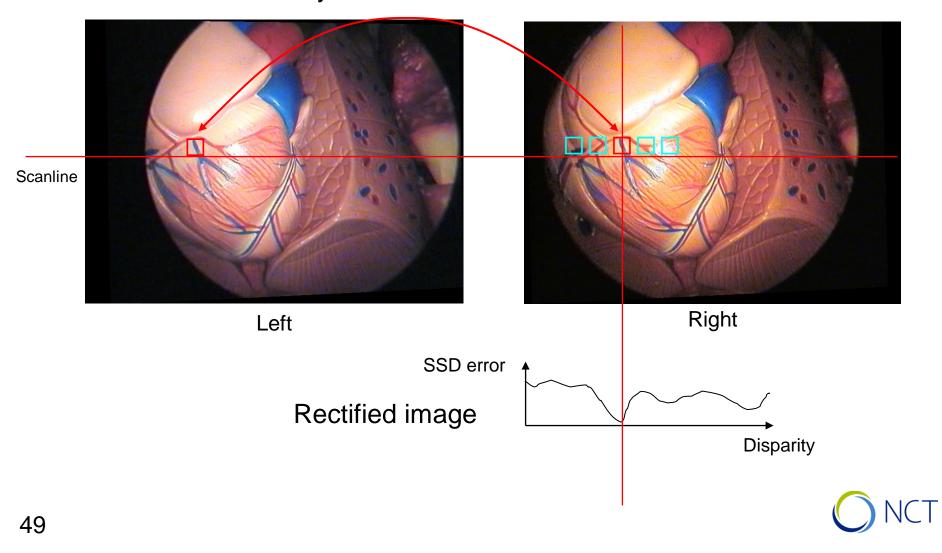






## Correspondences via correlation

- Corresponding elements are image windows
- Correlation as similarity measure



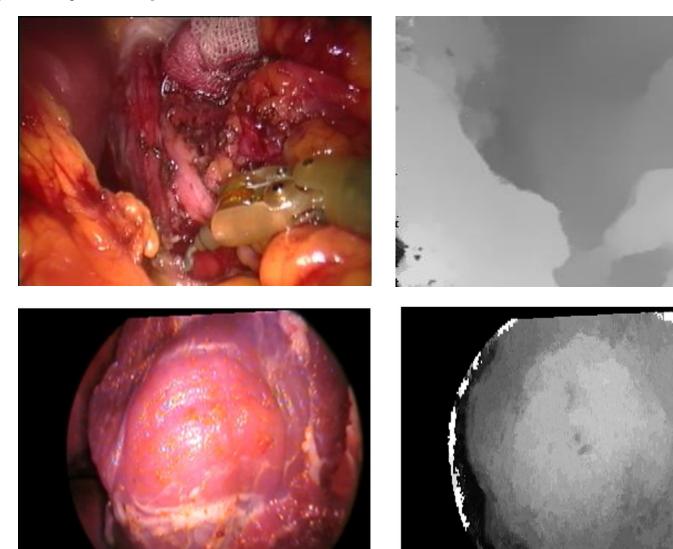
#### Normalization

- Images from different cameras can very due to varying lighting conditions
- Differing sensitivity of the sensors
- → Normalization of pixels in each search window

$$\bar{I} = \frac{1}{|W_m(x,y)|} \sum_{(u,v) \in W_m(x,y)} I(u,v)$$
 Average 
$$\|I\|_{W_m(x,y)} = \sqrt{\sum_{(u,v) \in W_m(x,y)}} [I(u,v)]^2$$
 Magnitude 
$$\hat{I}(x,y) = \frac{I(x,y) - \bar{I}}{\|I - \bar{I}\|_{W_m(x,y)}}$$
 Normalization



# Disparity maps





# Disparity map A dark pixel in the disparity map implies:

- A: Point close to the camera
- B: Point far from the camera
- C: Point not defined
- D: Point has many correspondences



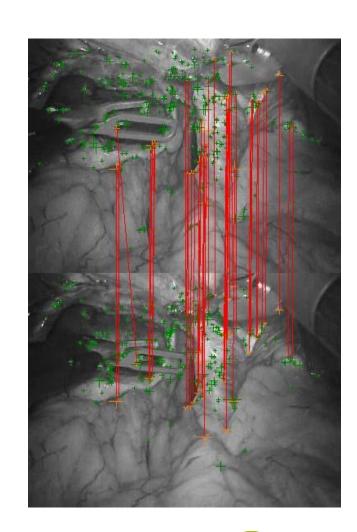
# Disparity map A dark pixel in the disparity map implies:

- A: Point close to the camera
- B: Point far from the camera
- C: Point not defined (when completely black)
- D: Point has many correspondences



## Correspondences via features

- Search restricted to few local point features
- Properties:
  - No occlusions, reproducible in different views, can be re-detected
  - Invariant against: Scaling, rotation, lighting
  - Neighborhood contains information
- Pixel feature: (2n+1)×(2n+1)-Pixel-Block around Pixel p
- Computation is divided into detection and descriptor

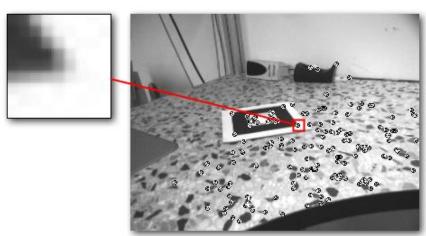




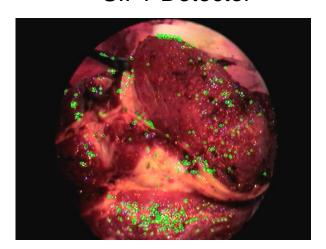
# Correspondences via features

- Detection: Locating stable, transformation invariant key points
- Depending on the algorithm due points different in localization, scale and structure
- Descriptor: Robust, unique characterization of the local neighborhood, e.g. through gradient information or frequency spectrum
- Examples:

Harris Corner Detector



SIFT-Detector





## Correspondences via features

Example: Harris-Corner-Detector:

If the Eigenvalues of the matrix

$$A = \begin{pmatrix} \left(\frac{\partial \operatorname{Img}(x,y)}{\partial x}\right)^2 & \frac{\partial \operatorname{Img}(x,y)}{\partial x} \frac{\partial \operatorname{Img}(x,y)}{\partial y} \\ \frac{\partial \operatorname{Img}(x,y)}{\partial x} \frac{\partial \operatorname{Img}(x,y)}{\partial y} & \left(\frac{\partial \operatorname{Img}(x,y)}{\partial y}\right)^2 \end{pmatrix}$$

are large, a small step in any direction will cause a large change in gray value.

Finding corner through looking for local maxima in:

$$R = \det A - k \cdot \operatorname{trace}(A)^2, k \approx 0.04$$



# Problems/Comparison

- Problems:
  - Occlusion
  - Limited field of view
  - Specularities, changes in light conditions
  - Surface structure: Sparse texture / repeating texture

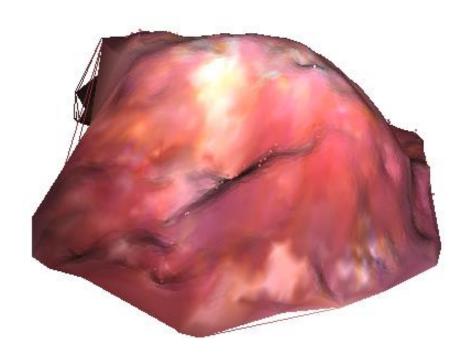
#### Comparison:

Correlation-based	Feature-based
Dense depth map	Sparse depth map
Only for textured scenes	
Prone to errors from changes in	Prone to errors from wrong
direction	correspondences

Specific pros and cons have to be weighted for each use case



# 3D-model





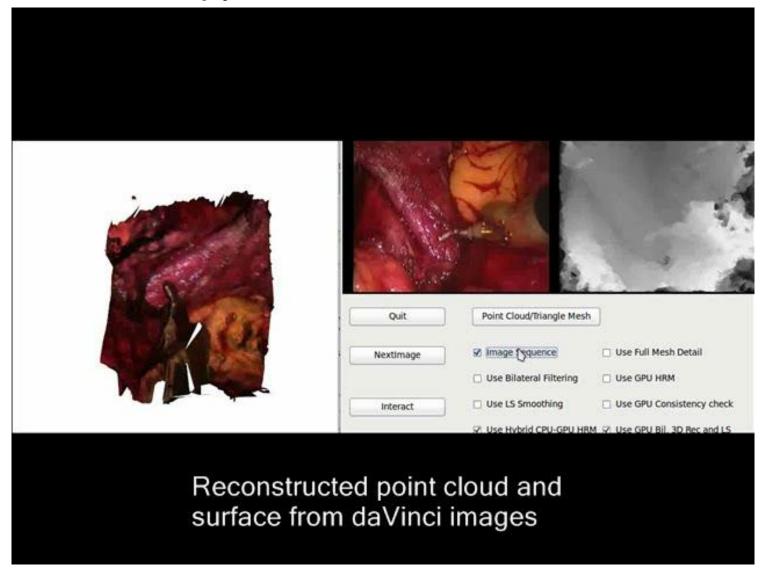


#### Stereo endoscopy

- Given:
  - two calibrated cameras (Projection matrices given)
- 3D-Reconstruction:
  - Rectification
  - Correspondence search:
    - Correlation-based or feature-based
      - Optional: Left/Right check
      - Optional: Detection of wrong correspondences
  - Triangulation
- Net generation
  - Texturizing of net

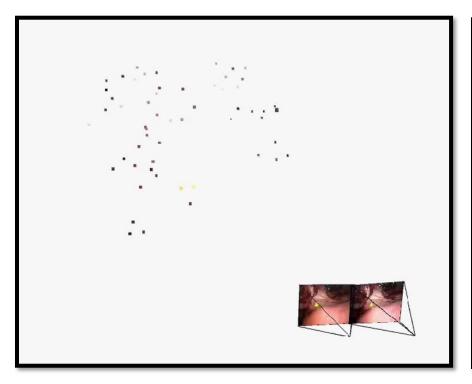


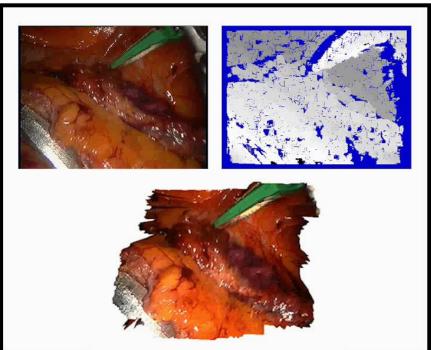
# Stereo endoscopy





# Stereo endoscopy





Stoyanov et al.: "Real-time Stereo Reconstruction in Robotic Assisted Minimally Invasive Surgery", MICCAI 2010



## Stereo endoscopy - Evaluation

#### Pros

- High accuracy with good correspondences
- No additional hardware (e.g. Tracking system, special light source) besides camera necessary
- Dense depth map with correlation-based approaches

#### Cons

- Expensive hardware
- Accuracy decreases with lower distances between cameras
- Very accurate calibration necessary
- For feature-based approaches:
  - Potentially fewer points on surface
  - Prone to wrong correspondences
- Occlusions, shadows
- Problems through weakly textured surface, smoke, blood, etc.



#### Structure-from-Motion

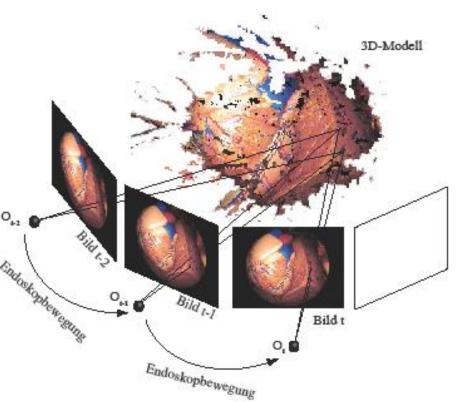
#### Problem:

One channel endoscope

 Computation of scene structure and camera movement from images

 Image either simultaneously or sequential, scenes are geometrically equivalent

 Position of camera not know: has to be estimated from correspondences





# Motion Compensated SLAM (MC-SLAM)

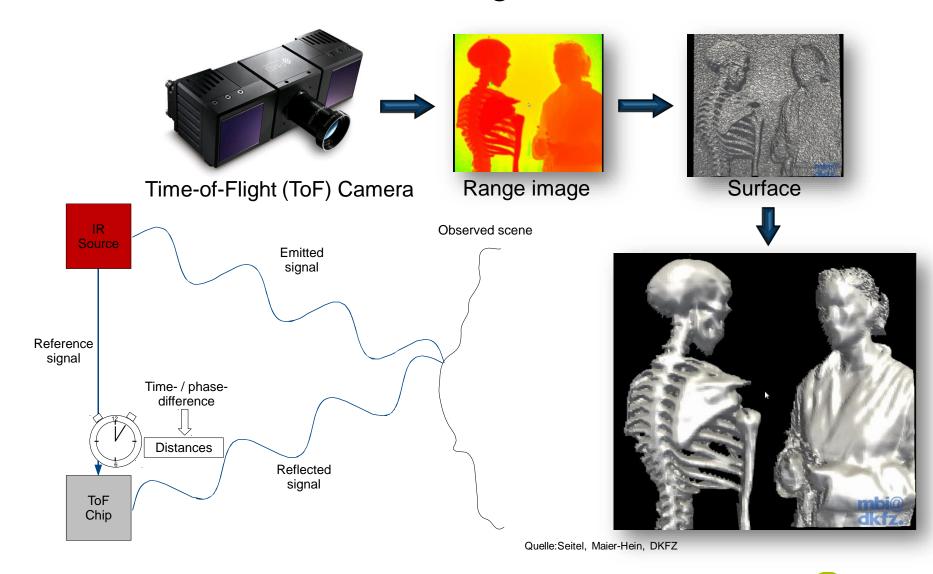


#### Structure from Motion - Evaluation

- Pros
  - High accuracy with good correspondences
  - Relative low hardware cost in comparison to other methods
- Cons
  - Potentially few features
  - Prone to correspondence errors
  - Occlusions, shadows
  - Problems from sparsely textured surfaces, specularities, smoke etc.
  - Often requires tracking
  - Difficult with fast moving objects



# Further methods: Time-of-Flight





#### ToF - Evaluation

- Pros
  - No features required
  - Dense depth map
  - No shadow effects
  - No image processing necessary
- Cons
  - No color image
  - Low resolution
  - Systematic errors
  - Can't deal with transparent structures



# Further methods: Structured light

Through projection of a known pattern, we can draw conclusion on an objects 3D Example shape frequency coding Pattern **Color identifies the stripe** 

## Structured light - Evaluation

- Pro
  - No need to rely on features
  - Density of correspondence selectable
  - Less complex correspondence search
  - Works well for homogenous surfaces
- Cons
  - Additional hardware
  - Projected light can be bothersome
  - Sensitive against reflections and transparencies
  - Difficult: Segmentation of symbols/correct detection of color values



#### Literature

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- Hartley, Zisserman: "Multiple View Geometry"
- Vogt. et al.: "Bildverarbeitung in der Endoskopie des Bauchraums". BVM 2001
- Zimmerman et al.: "Automatic Detection of Specular Reflections in Uterine Cervix Images". SPIE Medical Imaging 2006
- Wengert et al.: "Markerless Endoscopic Registration and Referencing". MICCAI 2006
- Stoyanov et al.: "Soft-Tissue Motion Tracking and Structure Estimation for Robotic Assisted MIS Procedures". MICCAI 2005
- Mountney et al.: Motion Compensated SLAM (MC-SLAM) for Image Guided Surgery

Dillmann et al.: Lecture Robotik III, KIT